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Multi-modal MRI measures reveal sensory abnormalities in major depressive disorder patients: A surface-based study

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ABSTRACT

Background: Multi-modal magnetic resonance imaging (MRI) measures are supposed to be able to capture different brain neurobiological aspects of major depressive disorder (MDD). A fusion analysis of structural and functional modalities may better reveal the disease biomarker specific to the MDD disease.

Methods: We recruited 30 MDD patients and 30 matched healthy controls (HC). For each subject, we acquired high-resolution brain structural images and resting-state fMRI (rs-fMRI) data using a 3 T MRI scanner. We first extracted the brain morphometric measures, including the cortical volume (CV), cortical thickness (CT), and surface area (SA), for each subject from the structural images, and then detected the structural clusters showing significant between-group differences in each measure using the surface-based morphology (SBM) analysis. By taking the identified structural clusters as seeds, we performed seed-based functional connectivity (FC) analyses to determine the regions with abnormal FC in the patients. Based on a logistic regression model, we performed a classification analysis by selecting these structural and functional cluster-wise measures as features to distinguish the MDD patients from the HC.

Results: The MDD patients showed significantly lower CV in a cluster involving the right superior temporal gyrus (STG) and middle temporal gyrus (MTG), and lower SA in three clusters involving the bilateral STG, temporal pole gyrus, and entorhinal cortex, and the left inferior temporal gyrus, and fusiform gyrus, than the controls. No significant difference in CT was detected between the two groups. By taking the above-detected clusters as seeds to perform the seed-based FC analysis, we found that the MDD patients showed significantly lower FC between STG/MTG (CV's cluster) and two clusters located in the bilateral visual cortices than the controls. The logistic regression model based on the structural and functional features reached a classification accuracy of 86.7% (*p <* 0.001) between MDD and controls.

Conclusion: The present study showed sensory abnormalities in MDD patients using the multi-modal MRI analysis. This finding may act as a disease biomarker distinguishing MDD patients from healthy individuals.

1. Introduction

Major depressive disorder (MDD) is a severe psychiatric disorder that severely impacts individual life quality and has a high worldwide prevalence [\(Malhi and Mann, 2018](#page-7-0)). As ranked by World Health Organization (WHO), depression has been one of the leading causes of the global burden of disease ([WHO, 2008](#page-7-0)). The 12-month and prevalence lifetime prevalence for MDD were observed to be 6.6% and 16.2% respectively. Moreover, MDD was more commonly reported in women compared to men, indicating a twice higher occurrence rate ([Kupfer](#page-6-0) [et al., 2012\)](#page-6-0). Several hypotheses involving the monoamine, hypothalamic–pituitary–adrenal axis, inflammation, neuroplasticity, genes, and brain structural/functional changes have been proposed to understand the pathophysiology of depression [\(Jeon and Kim, 2016; Kennis et al.,](#page-6-0)

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[2020; Kupfer et al., 2012; Malhi and Mann, 2018; Miller and Raison,](#page-6-0) [2016; Price and Drevets, 2012](#page-6-0)). Among them, neuroimaging techniques comprise a powerful method to detect brain structural and functional changes. Many studies have already analyzed neuroimaging biomarkers specific to depression and subtypes of depression (Cohen et al., 2021; [Kube et al., 2020; Sui et al., 2020\)](#page-6-0). However, despite extensive research, the lack of spatially converged findings across modalities in MDD still poses challenges to its diagnosis and treatment and calls for more investigation ([Cash et al., 2023; Gray et al., 2020; Malhi and Mann,](#page-5-0) [2018; Müller et al., 2017](#page-5-0)).

Magnetic resonance imaging (MRI) has been widely used to delineate brain structural and functional properties *in vivo*. Brain structural and resting-state functional MRI techniques are largely used to explore neuroimaging biomarkers specific to MDD [\(Pilmeyer et al., 2022\)](#page-7-0). The structural MRI (sMRI) modality enables the depiction of neuroanatomical morphological changes, and the resting-state fMRI (rs-fMRI) modality enables the measurement of brain functional abnormalities, like abnormal functional relationships between brain regions. The voxelbased morphometry (VBM) [\(Good et al., 2001\)](#page-6-0), surface-based morphometry (SBM) [\(Pantazis et al., 2004](#page-7-0)), and rs-fMRI functional connectivity (FC) [\(Mulders et al., 2015](#page-7-0)) are commonly used to analyze brain anatomical and functional characteristics in MDD. These methods have revealed large-scale alterations in brain regions associated with cognitive and affective functions [\(Dichter et al., 2015; Disner et al.,](#page-6-0) [2011; Wang et al., 2012\)](#page-6-0). Previous sMRI studies ([Arnone et al., 2012;](#page-5-0) [Bora et al., 2012; Du et al., 2012; Koolschijn et al., 2009; Li et al., 2020;](#page-5-0) [Zhang et al., 2016; Zhao et al., 2014; Zhu et al., 2022](#page-5-0)) reported abnormal gray matter (GM) volume and thickness in MDD in regions of the prefrontal cortex, orbitofrontal cortex, temporal cortex, insular cortex, cingulate cortex, hippocampus, striatum, amygdala, and thalamus. In addition, previous rs-fMRI studies ([Briley et al., 2022; Jav](#page-5-0)[aheripour et al., 2021; Long et al., 2020; Mulders et al., 2015; Veer et al.,](#page-5-0) [2010\)](#page-5-0) frequently reported resting-state FC abnormalities in regions involved in the default mode network, salience network, dorsal attention network, visual network, and somatosensory network. Although promising progress has been made in MDD research, the findings from different MRI modalities are not well-converged ([Cash et al., 2023; Gray](#page-5-0) [et al., 2020; Müller et al., 2017](#page-5-0)). The spatially heterogeneous distribution of these findings across multiple MRI modalities ([Liu et al., 2016;](#page-6-0) [Zhang et al., 2022\)](#page-6-0) may limit the knowledge of neuroimaging markers for diagnoses and treatments of MDD ([Zhuo et al., 2019\)](#page-7-0).

A considerable solution for this heterogeneity is to include multidisciplinary technologies such as multimodality MRI and artificial intelligence approaches ([Zhuo et al., 2019](#page-7-0)). Multi-modal MRI measures can capture different aspects of brain structural and functional properties ([Glasser, Coalson, et al., 2016\)](#page-6-0), and a fusion analysis of them can be powerful in identifying the disease markers ([Calhoun and Sui, 2016; Liu](#page-5-0) [et al., 2018; Meng et al., 2017; Sui et al., 2015; Sui et al., 2018](#page-5-0)). To detect confirmative imaging results, previous studies overlapped regions showing between-group differences across measures ([Hong et al., 2017;](#page-6-0) [Liu et al., 2016\)](#page-6-0) and used multivariate algorithms such as the canonical correlation analysis [\(Liu et al., 2018; Meng et al., 2017; Sui et al., 2015;](#page-6-0) [Sui et al., 2018](#page-6-0)) to characterize the association between brain structural/functional properties and clinical symptoms and behaviors.

Surface-based analysis (SBA) is considered to provide a better framework to analyze multi-modal measurements than volume-based analysis ([Glasser et al., 2013](#page-6-0)) for two main reasons. First, the SBA approach enables simultaneously analyzing multiple structural measures such as cortical thickness (CT), surface area (SA), and cortical volume (CV) ([Peng et al., 2015\)](#page-7-0). Second, due to subject-wise variabilities in cortical folding patterns ([Glasser, Smith, et al., 2016](#page-6-0)), the SBA approach may provide better cortical spatial localizations ([Coalson](#page-6-0) [et al., 2018; Glasser, Smith, et al., 2016](#page-6-0)), alignments [\(Glasser, Smith,](#page-6-0) [et al., 2016; Robinson et al., 2018; Van Essen, 2004](#page-6-0)), morphological identification and visualization [\(Dale et al., 1999; Xu et al., 2016\)](#page-6-0) relative to the voxel-based analysis (VBA). A recent study ([Brodoehl](#page-5-0)

[et al., 2020](#page-5-0)) suggested that the surface-based smoothing process reduced signal contamination and enhanced brain activity and FC results compared to the volumetric smoothing process. Hence, we were motivated to perform a surface-based multi-modal fusion analysis, involving the detection of the structural alteration and the FC alterations based on structural findings in MDD.

The present study aimed at detecting brain abnormalities in MDD patients using surface-based multi-modal MRI analysis. We used 30 MDD patients and 30 age-, sex- and education-level-matched healthy controls (HC). We first detect the clusters with significant differences in the CV, CT, and SA measures between the MDD and HC groups. We then determined brain FC alterations associated with structural changes that we found in MDD patients. Finally, we investigated whether these structural and functional abnormalities can successfully distinguish MDD from HC or not by using a logistical regression model.

2. Materials and methods

2.1. Subjects

Thirty patients with MDD and thirty age-, gender- and educationmatched HCs were recruited from the Department of Psychiatry at the Affiliated Brain Hospital of Guangzhou Medical University. All subjects who qualified for this study were right-handed and aged from 18 to 60 years. All MDD patients were clinically diagnosed according to the Structured Clinical Interview for DSM-IV Patient Edition [\(Glasofer et al.,](#page-6-0) [2017\)](#page-6-0) and none of them had any other comorbid psychotic or neurological diseases. The severity of depression was evaluated using the 24 item Hamilton Depression Rating Scale (HDRS) [\(Williams, 1988](#page-7-0)) and each of the MDD patients had at least 21 scores on HDRS. In this study, 26 MDD patients never received antidepressant treatment (i.e., medication-free), and the other 4 MDD patients took no medication for three months before participating in this study (i.e., medical-naive). The healthy subjects were screened with the DSM-IV Non-Patient Edition to confirm the lifetime absence of Axis I illnesses and had no history of psychiatric illness in any two lines of first- to third-degree biological relatives. All the MDD patients and healthy controls reported no lifetime history of seizures, head trauma, serious medical or surgical illness, substance abuse or dependence, or contraindications for MRI. Moreover, none of the subjects had abnormal MRI signals in the brain checked based on the clinical T1-weighted and T2-weighted FLAIR MRI images. The study protocol was approved by the Ethics Committee of Affiliated Brain Hospital of Guangzhou Medical University, and all subjects gave their written informed consent.

2.2. MRI data acquisition

All MRI data were acquired from a 3.0 Tesla MRI system (Achieva Xseries scanner; Philips, Medical Systems, Best, Netherlands) with an 8 channel phased-array head-coil at the Department of Radiology in the Affiliated Brain Hospital of Guangzhou Medical University. Tight but comfortable foam padding was used to reduce head motion, and earplugs were provided to muffle scanner noise.

The high-resolution brain structural images were obtained with T1 weighted (T1w) 3D turbo field-echo (TFE) and T2-weighted (T2w) 3D turbo spin-echo (TSE) sequences. The T1w TFE sequence parameters were as follows: TR = 8.2 ms, TE = 3.7 ms, flip angle = 7° , the field of view (FOV) = 256×256 mm², data matrix = 256×256 , slice thickness $= 1$ mm, voxel size $= 1.0$ mm³, and 188 sagittal slices. The T2w TSE sequence parameters were: $TR = 2,500$ ms, $TE = 250$ ms, flip angle = 90°, FOV = 256 \times 256 mm², data matrix = 256 \times 256, slice thickness = 1 mm, voxel size $= 1.0$ mm³, and 188 sagittal slices. The rs-fMRI was obtained with a gradient-echo echo-planar-imaging (EPI) sequence with the following parameters: $TR = 2,000$ ms, $TE = 30$ ms, flip angle = 90° , $FOV = 220 \times 220$ mm², data matrix = 64 \times 64, slice thickness = 4 mm with interslice gap = 0.6 mm, voxel size = 3.4 mm \times 3.4 mm \times (4.0 +

0.6 mm), and 33 axial interleaved slices. The rs-fMRI scanning lasted about 8 min and acquired 240 time points for each subject. During the rs-fMRI scanning, subjects were instructed to relax with their eyes closed and not to sleep or think about things in particular. All of the images were acquired in the same session for each subject.

2.3. Structural MRI data pre-processing

The structural MRI (sMRI) data, including T1w and T2w images, were visually inspected and rated on a four-point quality scale (poor, fair, good, and excellent) by a neuroradiologist (HW). Only the "good" or "excellent" images were included in this study. No imaging datasets were excluded according to this threshold. All the eligible images were preprocessed by using the structural Human Connectome Project (HCP) pipeline (version 3.27) ([Glasser et al., 2013\)](#page-6-0).

The sMRI data were preprocessed by following partial sessions of HCP structural pipelines which involved the PreFreeSurfer and Free-Surfer. In the PreFreeSurfer section, the T1w images were cropped, AC-PC aligned, and brain extracted. PreFreeSurfer produced an undistorted "native" structural volume space for each subject, aligned the T1w and T2w images, performed a bias field correction, and registered the subject's native structural volume to the MNI space. Due to the lack of structural field maps, the gradient nonlinearity correction was not included. In the FreeSurfer section, we conducted the procedures of the auto-recon pipeline of FreeSurfer, which used the brain mask from PreFreeSurfer as an input, performed brain extraction, brain segmentations, surface tessellation, spheric registration, and morphometric measurements. From these procedures, we obtained the cortical measurements of the CT, SA, and CV.

2.4. Resting-state fMRI preprocessing

The rs-fMRI data were preprocessed with the pipeline of DPABI [\(http](https://rfmri.org/dpabi) [s://rfmri.org/dpabi](https://rfmri.org/dpabi)). The pipeline included the following steps: exclusion of the first 10 volumes, slice-timing and head motion correction, detrend, regression of Friston-24 motion parameters and signals of the white matter and cerebrospinal fluid, and temporal filtering (0.01–0.1 Hz). In the preprocessing, we set the threshold of the rs-fMRI images as the head movement < 1.5 mm in any plane or rotation $< 1.5^\circ$ in any axis. No subject was excluded according to this threshold.

2.5. Cortical measurement generation

We first extracted three structural morphological measures including the cortical thickness (CT, lh/rh.thickness), surface area (SA, lh/rh. area), and cortical volume (CV, lh/rh.volume) from the FreeSurfer section described above. Then, we took a surface-based down-resampling procedure to normalize these measures. The normalization steps ([Glasser et al., 2013; Zhang et al., 2022](#page-6-0)) were as follows: (1) individual midthickness surfaces were averaged from white matter (WM) and pial surfaces and were resampled to the fs_LR 164 k surface and then to the fs_LR 32 k surface (2-mm vertex spacing), (2) CT, SA, and CV were separately resampled to fs_LR 32 k surface via the fs_LR 164 k surface, and (3) all measures were smoothed [\(Glasser et al., 2013; Liu et al.,](#page-6-0) [2016; Zhang et al., 2022](#page-6-0)) with a Gaussian kernel of full-width-at-halfmaximum (FWHM) = 10 mm (σ = 4.25 mm, FWHM = $\sigma\sqrt{8\ln 2}$) for keeping a consistency in smoothing effects. Finally, we examined the differences in each of these measures between MDD and HC groups, which were denoted as structural alterations, and the significant clusters were used as seeds in the following functional analysis.

After the identification of structural alterations, we performed the seed-based FC analysis on the cortical surface with the following steps: (a) the functional images (timeseries) were co-registered to the cortical surface using a boundary-based registration (BBR). Individual mean functional images were registered to the preprocessed structural images

to generate transformation matrices. The other functional images were projected to the cortical surface by sampling along the midthickness surface using the BBR transformation matrix. (b) The projected functional images were resampled to fs_LR 32 k surface via fs_LR 164 k, and smoothed with a Gaussian kernel of 10-mm FWHM. (c) The FC between the seed region and rest vertices of bilateral surfaces were calculated by taking each structural cluster as the seed (*wb_command -cifti-average-roicorrelation*). Finally, we examined the difference in the seed-based FC between MDD and HC groups.

2.6. Statistical analyses

2.6.1. Demographical statistics

We assessed group differences in gender, age, and education years between MDD and HC groups. In the demographical statistics, a *χ*2 test was used for comparing the gender differences, while independent *t*tests were used for comparing age and years of education between the two groups. The significance level was set at *p <* 0.05.

2.6.2. Multidimensional structural analyses

To assess structural morphological differences between the MDD and HC groups, we applied the Permutation Analysis of Linear Models (PALM) ([Winkler et al., 2016](#page-7-0)), a tool that allows inference using permutation methods, to the structural measures of the left- and righthemisphere surfaces separately. In specific, we calculated betweengroup differences in each structural measure on each vertex by using the PALM (5,000 permutations) with gender, age, and educational level as covariates. Cluster-forming threshold (cluster) and family-wise error (FWE) methods were applied for the multiple-comparison correction (*p*cluster+FWE *<* 0.05). To determine the significant clusters of each measure after the corrections, we split measure-specific results into independent clusters by using Workbench/*wb_command -cifti-find-clusters*. These clusters were reported based on the Desikan-Killiany atlas [\(Desi](#page-6-0)[kan et al., 2006](#page-6-0)).

2.6.3. Seed-based FC analyses

To detect brain FC alterations associated with structural alterations in MDD patients, we used clusters showing significant differences between MDD and HC groups in the Multidimensional structural analyses as seed regions. We then applied PALM (5,000-time permutations) with seed-based FC as the dependent variable, group as the independent variable, and gender, age, and educational level as the covariates. Afterward, the seed-based FC results were thresholded by a clusterforming FWE method (*p*cluster+FWE *<* 0.05) and split into the clusters using the Workbench. FC results after multiple-comparison corrections were reported based on the network parcellation atlas [\(Yeo et al., 2011](#page-7-0)).

2.6.4. Classification analysis

To distinguish MDD from controls based on our multi-modal results, we applied a cross-validated logistic regression model by using the classification module of Matlab 2020a. The steps were as follows. (1) Feature selection: The cluster-wise averaged values from both structural morphological and seed-based FC analyses were taken as features. (2) Model selection: A logistic regression model was used to detect the model classification based on both structural and functional features. (3) A *k*-fold cross-validation: A 10-fold cross-validation procedure was applied to evaluate the accuracy of the logistic regression model. In each of the cross-validation iterations, 90% of the subjects were selected as the training set, while the rest 10% of the subjects were selected as the test set. (4) Statistical significance: For confirming the significance of our model and its probability distance to the chance level, a labelshuffled permutation was applied (5,000 times). In each permutation loop, the group labels (MDD/HC) of subjects were randomly assigned and re-entered into the model space to compute the classification accuracy. After all permutation loops (5,000 times), the null accuracy distribution based on the label-shuffled permutation was calculated and then the model performance was identified by seeking the position of the accuracy gotten from our model in the generated null accuracy distribution.

To assess the performance of the logistic regression model, we generated classification accuracy and statistical significance. For the model performance, a confusion matrix and a receiver-operating characteristics (ROC) plot were created to show the model's classification accuracy and sensitivity.

3. Results

3.1. Demographics

Table 1 lists the demographical information of the MDD and HC groups. No significant difference was found in gender, age, and educational level between MDD and HC groups.

3.2. Surface-based structural properties

To detect the abnormal brain structure in MDD, we compared the morphological properties between the two groups. We found that the MDD patients had significantly lower cortical volume (CV) and surface area (SA) in the temporal and occipital cortices than the HC (Fig. 1, *p*cluster+FWE *<* 0.05). However, no significant between-group difference was found in the cortical thickness (CT). Fig. 1A shows that the MDD patients had significantly lower CV than the HC group in a cluster, involving the superior temporal gyrus (STG) and middle temporal gyrus (MTG). Fig. 1B shows that the MDD patients had significantly lower SA in three clusters than the HC group. The first cluster involves vertices of the left inferior temporal lobe (ITG), STG, temporal pole gyrus (TPG), entorhinal cortex (EC), and fusiform gyrus (FG). The second cluster includes vertices of the left FG and ITG. The third cluster involves vertices of the right STG, TPG, and EC. The detailed information for these clusters is listed in Table 2.

Table 1

Demographical information of the Major Depressive Disorder (MDD) and healthy controls (HC) groups.

^aχ²-test. ^btwo-sample *t*-tests.

Abbreviations: HDRS, Hamilton Depression Rating Scale; MDD, Major Depressive disorder; HC, healthy controls; N/A, non-applicable; M, male; F, female.

Fig. 1. Regions with significantly decreased brain structural morphological properties obtained from the surface-based analysis in the MDD group relative to the HC group (MDD *<* HC). (a) Cortical volume, and (b) Surface area. The color bar indicates the vertex-wise *t* values survived under a cluster-forming thresholded family-wise error (FWE) correction (*p <* 0.05).

Table 2

The cortical structural alterations of the Major Depressive Disorder (MDD) group compared with the healthy control (HC) group.

Cluster	MNI			t	Vertices	Brain Areas
	\boldsymbol{x}	y	z			
CV						
C1	60	-4	Ω	-3.33	374	R.STG, R.MTG
SA						
C1	-42	-10	-41	-3.65	297	L.ITG, L.TPG, L.EC, L.FG,
						L STG
C ₂	-40	-48	-20	-3.89	190	L.FG, L.ITG
C ₃	50	2	-12	-3.06	212	R.STG, R.TPG, R.EC

This table lists the MNI coordinates of the clusters and the associated areas showing significantly decreased cortical volume (CV) and surface area (SA) in major depressive disorder (MDD) patients relative to the healthy controls (HC). These clusters were reported based on the Desikan-Killiany atlas [\(Desikan et al.,](#page-6-0) [2006\)](#page-6-0).

Abbreviations: STG, superior temporal gyrus; MTG, middle temporal gyrus; ITG, inferior temporal gyrus; TPG, temporal pole gyrus; EC, entorhinal cortex; FG, fusiform gyrus. C1, C2, and C3 refer the 1st, 2nd, and 3rd cluster, respectively. The MNI coordinates were on the mid-thickness surface (fs_LR 32 k).

Fig. 2. The seed-based functional connectivity (FC) analysis in the MDD group relative to the HC group. (a) The selected seed was the region showing significant between-group differences in the cortical volume. (b) An example of the ROI-based FC maps for an individual. The color bar shows the robust range of Fisher's *r*-to-*z* transformed FC. (c) Clusters showed significantly decreased FC in the MDD group relative to the HC group. The color bar indicates the vertex-wise *t* values survived under a cluster-forming thresholded family-wise error (FWE) correction (*p <* 0.05).

3.3. Seed-based functional connectivity

To determine the FC alterations in the MDD, we took the significant structural clusters as the seeds and compared the seed-based FC between the two groups. Fig. 2 shows that the MDD patients had significantly lower FC in two regions than the controls when we took the cluster at STG/MTG (obtained from CV comparison) as the seed. These regions are mainly distributed in the visual network according to the network parcellation atlas [\(Yeo et al., 2011\)](#page-7-0).

3.4. Classification

The logistic regression model analysis showed an 86.7% classification accuracy in distinguishing the MDD patients from the HC [\(Fig. 3](#page-4-0)). The area under the curve (AUC) was 0.93, the true positive rate (TPR) was 83%, and the false positive rate (FPR) was 10%.

4. Discussion

The present study applied a multi-modal fusion analysis, which included structural analysis and seed-based FC analysis, to detect the cortical morphological vulnerabilities and functional network alterations associated with structural abnormalities in MDD. The MDD patients had significantly lower CV and SA in the temporal and occipital

Fig. 3. The confusion matrix and receiver operating characteristic (ROC) curve of the logistic regression model. (a) The confusion matrix lists the classification performance of the logistic regression model. (b) The area under the curve (AUC) was 0.93, the true positive rate (TPR) was 0.83, and the false positive rate (FPR) was 0.1.

cortices than the controls. The seed-based FC analysis revealed lower FC between STG/MTG and regions in the visual network relative to the controls. In addition, structural values (CV and SA) in those regions and FC between them provided a high classification accuracy in distinguishing MDD patients from controls.

4.1. Structural alterations

The surface-based analyses showed that the values of CV and SA were lower in the regions involving the STG, MTG, EC, FG, ITG, and TPC in the MDD patients than in the HC ([Fig. 1](#page-3-0) and [Table 2\)](#page-3-0). These regions largely overlapped with brain sensory cortices (i.e., visual and auditory cortices). The STG, MTG, ITG, and TPC are located in the lateral temporal cortices, which are believed to be engaged in the auditory, visual, facial cognition, and language-associated functions [\(Acheson and](#page-5-0) [Hagoort, 2013; Cheng et al., 2016; Ishai et al., 1999; Kellogg, 2003;](#page-5-0) [Sakurai et al., 2008](#page-5-0)). The abnormality in these regions was found to be associated with symptom severity and suicidal behaviors in MDD patients ([Cao et al., 2016; Fitzgerald et al., 2008; Hwang et al., 2010;](#page-5-0) [Kocsis et al., 2021; Li et al., 2010; Niu et al., 2017; Pan et al., 2015; Peng](#page-5-0) [et al., 2015; Phillips et al., 2015; Takahashi et al., 2010\)](#page-5-0). The FG is involved in face cognition and social communication ([Haxby et al.,](#page-6-0) [2002; Hoffman and Haxby, 2000](#page-6-0)), and its alteration may influence the vulnerability to depression ([Papmeyer et al., 2015\)](#page-7-0). The EC acts as the gateway between the hippocampus and neocortex, and its volume was found to be decreased in patients with depression ([Furtado et al., 2008](#page-6-0)). Moreover, optogenetic activation in the entorhinal-visual circuit was found to promote depressive behaviors in mice [\(Lu et al., 2022](#page-6-0)). Although depression is not a typical psychiatric disorder characterized by disturbed sensory perception, the sensory abnormality (e.g., visual, auditory, and touching systems) was found to contribute to the anhedonia symptoms and individual emotional experiences in MDD ([Bubl](#page-5-0) [et al., 2012; Fitzgerald, 2013; Qiao et al., 2013; Schwenzer et al., 2012](#page-5-0)). The deficits in auditory and visual perception may potentially lead to attentional and control deficits in MDD patients [\(Grange and Rydon-](#page-6-0)[Grange, 2022; Zweerings et al., 2019](#page-6-0)). Moreover, accumulating evidence reported interactions between sensory perception and depressive symptoms in MDD patients [\(Canbeyli, 2010](#page-5-0); Canbeyli, 2013). For instance, a bidirectional relationship was suggested that sensory stimulation can modulate depression and in turn, depression impairs sensory perception ([Canbeyli, 2022](#page-5-0)).

4.2. Seed-based FC alterations

The present study found decreased FC between the cluster at MTG/ STG and clusters in the bilateral occipital cortices ([Fig. 2](#page-3-0)C). The impaired activity of visual cortices was found to be related to abnormal cognitive and emotional functions in MDD patients [\(Le et al., 2017\)](#page-6-0). A previous study also found that the FC of the visual network may contribute to distinguishing MDD patients from controls ([Zeng et al.,](#page-7-0) [2012\)](#page-7-0). Moreover, repetitive transcranial magnetic stimulation to the visual cortices was reported to alleviate depressive symptoms ([Zhang](#page-7-0) [et al., 2021](#page-7-0)) and its activation was found to correlate with treatment responses in MDD patients [\(Furey et al., 2013](#page-6-0)). Our study reported significantly decreased FC between the STG/MTG and bilateral visual network, suggesting a disrupted connection between the auditory and visual cortices in MDD patients, which is consistent with previous studies [\(He et al., 2016; Lu et al., 2020\)](#page-6-0). Taken together, the structural and functional alterations observed in the present study may suggest a disrupted sensory system in MDD patients.

4.3. Classification

The present study showed that the patients had brain structural and functional alterations in regions related to sensory processing functions ([Figs. 1 and 2](#page-3-0)). Based on these multi-modal MRI alterations, we detected a relatively high classification rate (86.7%) in distinguishing the MDD patients from the healthy controls (Fig. 3). These findings indicated sensory processing abnormalities in individuals with MDD, which are consistent with previous studies [\(Bubl et al., 2010; Chen et al., 2022;](#page-5-0) [Fitzgerald, 2013; Gong et al., 2020; Xia et al., 2022; Zweerings et al.,](#page-5-0) [2019\)](#page-5-0).

Furthermore, altered activity and connectivity of sensory areas have been identified as indicators of treatment responses and factors modulating depressive symptoms in individuals with MDD (Canbeyli, 2022; Dichter et al., 2015; Farb et al., 2011; Furey et al., 2013; Gao et al., 2018; Li et al., 2021; Rolle et al., 2020). Although the classification model performance is varied by modalities, cross-validation schemes, sample sizes, and classification algorithms, our classification result aligns with previous research that classified MDD patients from controls or predicted treatment outcomes (Aleem et al., 2022; Cohen et al., 2021; Gao et al., 2018). Previous reviews reported that the overall classification accuracy was 82% [\(Lee et al., 2018\)](#page-6-0) and AUC was 0.84 [\(Cohen](#page-6-0) [et al., 2021](#page-6-0)) for predicting treatments in MDD patients. The classification accuracy between MDD and HC reviewed by ([Gao et al., 2018](#page-6-0)) was discovered to be ranged from 45% to 99% [\(Lord et al., 2012; Sunder](#page-6-0)[mann et al., 2017](#page-6-0)). In line with these studies, our cross-validated logistic regression model has shown a good classification performance, suggesting that sensory processing abnormalities may potentially serve as one of the disease biomarkers in MDD ([Lu et al., 2020; Xia et al., 2022](#page-6-0)).

5. Conclusion

The present study showed that MDD patients had structural and functional alterations in the sensory system that contributed to a high classification accuracy in distinguishing the MDD patients from controls. The findings of structural and functional alterations in the sensory system may act as a neuroimaging biomarker in MDD disease.

6. Limitations

Several limitations should be considered in our study. First, the sample size in the current study is relatively small, which may bias the results and impact the result reproducibility. Future studies should address this issue by employing a larger sample size or including an independent sample for validation. Second, the subcortical areas were not considered in the SBA approach. In fact, the cortico-subcortical (limbic) circuits have been proposed to be involved in the pathophysiology of MDD ([Disner et al., 2011; Kupfer et al., 2012\)](#page-6-0). Future studies should consider the effect of subcortical areas on the mechanisms of MDD. Third, the removal of global signals can reduce physiological noise and alter neural signal distribution, and this approach is still in debate (Aquino et al., 2020; Murphy and Fox, 2017; Power et al., 2017). Future multi-modal MRI studies may also consider the effect of global signals.

8. Data availability statement

Data and code are available from the corresponding author upon reasonable request.

9. Competing interests statement

The authors declare that they have no competing financial interests.

CRediT authorship contribution statement

Shufei Zhang: Conceptualization, Methodology, Formal analysis, Writing – original draft, Writing – review & editing. **Shenglin She:** Conceptualization, Methodology, Data curation, Formal analysis, Writing – review & editing. **Yidan Qiu:** Writing – review & editing. **Zezhi Li:** Data curation. **Xiaoyan Wu:** Writing – review & editing. **Huiqing Hu:** Data curation, Writing – review & editing. **Wei Zheng:** Data curation. **Ruiwang Huang:** Conceptualization, Methodology, Formal analysis, Supervision, Writing – original draft, Writing – review & editing. **Huawang Wu:** Conceptualization, Methodology, Formal analysis, Supervision, Writing – original draft, Writing – review & editing.

Declaration of Competing Interest

The authors declare that they have no known competing financial interests or personal relationships that could have appeared to influence the work reported in this paper.

Data availability

Data will be made available on request.

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