



The neurovascular unit in healthy and injured spinal cord

Rubing Zhou^{1,2,*}, Junzhao Li^{2,*}, Ruideng Wang¹,
Zhengyang Chen¹ and Fang Zhou¹

Abstract

The neurovascular unit (NVU) reflects the close temporal and spatial link between neurons and blood vessels. However, the understanding of the NVU in the spinal cord is far from clear and largely based on generalized knowledge obtained from the brain. Herein, we review the present knowledge of the NVU and highlight candidate approaches to investigate the NVU, particularly focusing on the spinal cord. Several unique features maintain the highly regulated microenvironment in the NVU. Autoregulation and neurovascular coupling ensure regional blood flow meets the metabolic demand according to the blood supply or local neural activation. The blood–central nervous system barrier partitions the circulating blood from neural parenchyma and facilitates the selective exchange of substances. Furthermore, we discuss spinal cord injury (SCI) as a common injury from the perspective of NVU dysfunction. Hopefully, this review will help expand the understanding of the NVU in the spinal cord and inspire new insights into SCI.

Keywords

Blood–spinal cord barrier, neurovascular coupling, neurovascular unit, spinal cord, spinal cord injury

Received 4 September 2022; Revised 9 February 2023; Accepted 24 March 2023

Introduction

Proper structural and functional homeostasis of the central nervous system (CNS) requires precise regulation of blood perfusion, oxygen delivery, and energy supply.^{1,2} The CNS has two unique vascular features to maintain homeostasis: the neurovascular unit (NVU) ensures adequate blood supply according to neural activation and metabolic waste removal, and the blood–central nervous system barrier (BCNSB) partitions the circulating blood from the parenchyma to permit the selective exchange of substances.³ The blood–brain barrier (BBB) and blood–spinal cord barrier (BSCB) have similar barrier abilities and are sometimes referred to as BCNSB.⁴ These key features in the NVU are maintained by the highly coordinated activity of multiple cell types.^{5–7} The NVU has attracted enthusiastic interest in the scientific community for its status in brain function. However, the spinal cord, another essential organ in the CNS, has received less attention. The current understanding of the NVU in the spinal cord typically has to follow the paradigm obtained from the brain.

It has been widely accepted that BCNSB disruption contributes to neurological deficits.^{2,8,9} Extreme alterations

of the NVU are thought to result in tissue ischemia and energy supply deficits, further promoting neurological disorders.¹⁰ Diverse immune cells are strategically distributed within the NVU and associated with neuro-inflammatory response in diseases.¹¹ Thus, studies of the BCNSB and NVU can help in understanding the mechanisms of neurological disorders and may provide novel treatments for these diseases, such as ischemic stroke, traumatic brain injury, and vascular dementia.^{12–14} However, to date, interpretation of the mechanisms of the NVU and BSCB are insufficient in injured spinal cord. Spinal cord injury (SCI) is a devastating injury that causes long-term disability.

¹Department of Orthopedics, Peking University Third Hospital, Beijing, China

²Neuroscience Research Institute and Department of Neurobiology, School of Basic Medical Sciences, Peking University Health Science Center, Beijing, China

*Rubing Zhou and Junzhao Li contributed equally.

Corresponding author:

Fang Zhou, Department of Orthopedics, Peking University Third Hospital, Beijing 100191, China.
Email: zhouf@bjmu.edu.cn

The primary insult initiates a sustained impairment cascade called secondary injury, which continues to exacerbate the degree of SCI.¹⁵ Insults to the spinal cord can disrupt the functional or structural integrity of the NVU and BCSB, thus playing a vital role in secondary injury.^{16,17} Therefore, we will discuss the status of the research on the NVU and BCSB dysfunction in SCI.

The neurovascular unit

It was observed that the blood supply to the CNS was not exclusively controlled by systemic circulation; the brain could regulate its blood supply and metabolic needs in active brain regions by neural activity. The concept of the NVU was proposed to study the pathological mechanisms of stroke by the National Institute of Neurological Disorders and Stroke Progress Review Group in 2001, emphasizing the unique relationship between brain cells and cerebral vasculature.¹⁰ This concept emerged as a new paradigm for investigating physiology and pathology in the CNS.

Today's view of the NVU has been broadly amplified. BCNSB is currently preferred as the main functional configuration of the NVU.¹ In addition to its barrier function which preserves the normal function of the CNS, the BCNSB also actively serves as a communication interface for the NVU between the periphery and the CNS. In contrast, interactions in the NVU are critical for the formation and maintenance of the BCNSB.^{5,10} The role of the NVU in regulating cerebral blood flow has been broadly categorized as (1) autorregulation, the response of the cerebral vasculature to changes in perfusion pressure;^{18,19} (2) neurovascular coupling, the local blood flow response to changes in neural activity;^{3,20} (3) vascular reactivity to metabolic stimuli, such as pH or CO₂ content;²¹ and (4) endothelium-dependent responses, such as hemodynamic stimuli (e.g., shear stress), neurotransmitters, and pharmacological agents.²² Nevertheless, some functions of the NVU are difficult to distinguish clearly in experiments and therefore are often misidentified in studies.

At different levels of the vascular network, diverse types of cells and associated structures play diverse roles in cerebrovascular function and homeostasis synergistically throughout the CNS.²³ Collectively, the BCNSB comprises endothelial cells (ECs), basement membrane (BM), pericytes, smooth muscle cells (SMCs), and glia limitans. Interactions among these different vascular cells with neurons and astrocytes refine the functions of the BCNSB and act as a whole NVU (Figure 1).²⁴ In the following section, we discuss the common features of cells in the NVU, supplemented by available studies from the perspective of the brain.

Neurons

Neurons are protected by the BCNSB to ensure normal function.² Neurons can regulate nearby blood vessels by generating signals directly or via interposed cells based on their oxygen or metabolic demands. Neuron terminals can trigger calcium signaling in astrocyte processes via several mechanisms, thus preceding the onset of vascular responses.²⁵ Classically, neurons release glutamate to activate the ionotropic and metabotropic glutamate receptors on astrocytes, evoking Ca²⁺ release from internal stores and increasing the intracellular Ca²⁺, leading to activation of downstream Ca²⁺-dependent enzymes and generation of vasodilatory substances.²⁶ Thus, astrocytes take over to adjust the blood supply by modulating local vascular cells.

Moreover, studies have shown that neurons release various neurotransmitters directly or indirectly via astrocytes and pericytes to mediate vascular changes in the brain.²⁷ Diverse signaling cascades may involve this process at the capillary or arteriole levels.²⁶ Neuronal activity-induced capillary dilation classically relies on glutamate receptor (mainly metabotropic) activated Ca²⁺-dependent signaling in astrocytes. In contrast, neurovascular coupling-evoked arteriole dilation in the brain depends on NMDA receptor activation and Ca²⁺-dependent NO generation by interneurons.²⁶ Different types of interneurons have been suggested to control local blood flow responses differently.²⁷ More information is needed to identify the exact function of these neurotransmitter signals in the NVU at the level of the spinal cord.

Astrocytes

Small arteries penetrating the neural parenchyma are completely enveloped by astrocytic endfeet, which occupy a larger surface area of the microvasculature than the neural processes.²⁸ Astrocytes also ensheath capillaries to constitute the most abluminal layer in the NVU.²⁹ In the human cortex, a single astrocyte might sense the activity of more than one million neuronal synapses in its domain by the fine endfeet.³⁰ Moreover, each astrocyte has at least one process with its endfeet surrounding the cerebral blood vessel.³¹ Characterized by highly ramified processes contacting the neural processes and microvessels, astrocytes are well positioned to link neural activity to microvascular function.³² Astrocytes are expected to modulate local perfusion by neuron-to-astrocyte signaling.³³ In vivo imaging has verified a frequency-related correlation between neuronal activity, Ca²⁺ transients in astrocytes, and vasomotility.³⁴ Astrocytic Ca²⁺ transients are less synchronized with low-frequency neuronal Ca²⁺ transients and do not seem to contribute to low-frequency

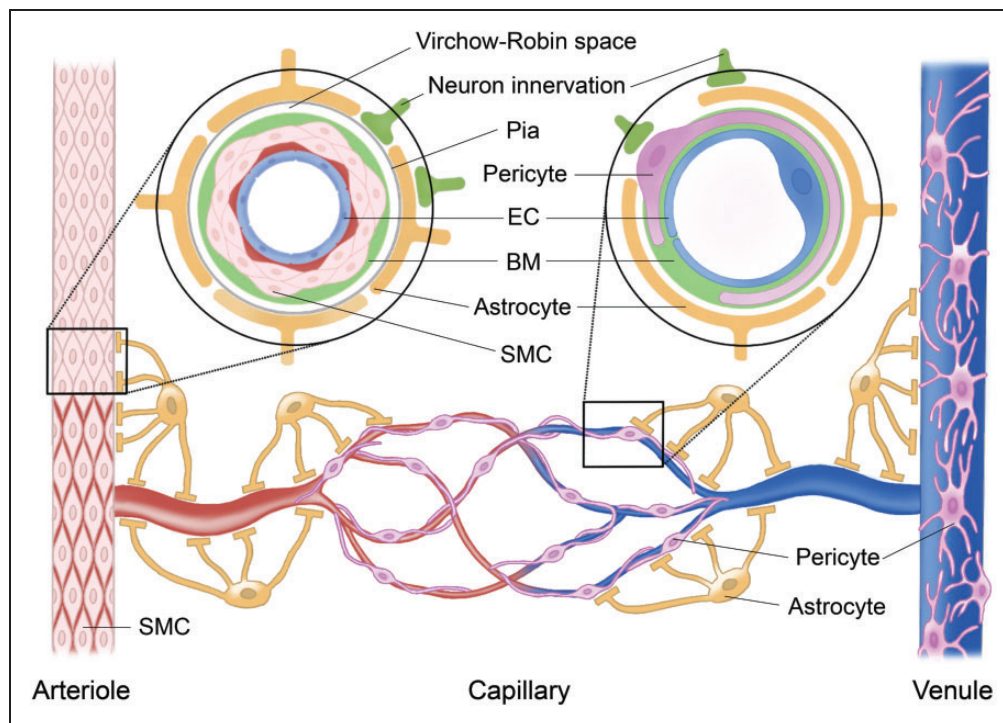


Figure 1. The typical components of the neurovascular unit (NVU) in the central nervous system (CNS). The NVU comprises (1) vascular cells, including endothelial cells (ECs) and mural cells, such as pericytes on capillaries and venules, or smooth muscle cells (SMCs) on arterioles and small arteries; (2) neuroglial cells, such as astrocytes; and (3) neurons. ECs form the luminal layer of the vessel wall. The space between adjacent ECs is held by paracellular junctions. The expression of some junctional proteins (including claudin-11, ZO-1, occludin, catenin, and VE-cadherin) is lower in the BSCB than in the BBB. At the arteriolar level (left inset), the basement membrane (BM) and SMC envelope endothelium. Astrocytic endfeet insert into the BM to regulate SMCs through the pia and the glia limitans. The capillary and venule (right inset) lack SMCs, where pericytes embed in the BM and wrap around the ECs on the abluminal side. The astrocytic endfeet attach to the pericytes at both venules and capillaries. Pericyte coverage is less on the BSCB than on the BBB. SMCs, pericytes, and astrocytes all receive neuronal innervation to control their function. In addition, these conformations of cells are also the major cellular structure of the blood–central nervous system barrier.

hemodynamic changes. However, under high-frequency-stimulated neuronal Ca^{2+} responses, astrocytic Ca^{2+} transients are cumulative and temporarily correlated with vasoconstriction.³⁵ In the CNS, astrocytes can detect changes in both blood and neurons through several neurotransmitters, mainly glutamate and γ -aminobutyric acid, and evoke downstream calcium signaling.³⁶ These calcium signals can activate smooth muscle cells via potassium signaling and the Na^+/K^+ ATPase,³⁷ causing local vasodilation and then propagating away to induce vasomotion in adjacent arterioles.^{32,38} Moreover, astrocytes also produce and release various molecular mediators, such as prostaglandins, nitric oxide (NO), and arachidonic acid, to regulate local blood flow in a coordinated manner.^{39,40}

Astrocytes alone are not to determine barrier properties because astrocytes appear postnatally in the brain, well after the BBB has already been sealed.⁴¹ Nevertheless, astrocytes still contribute to BBB properties by releasing molecules to promote BBB repair, restrict peripheral immune cells, and assist in the

resolution of inflammation.⁴² Astrocyte-derived factor induces endothelial polarization and produces glycocalyx on the CNS endothelium.²⁹ Astrocyte-derived Sonic hedgehog signaling stimulates the expression of tight junction (TJ) proteins such as claudin-5 and occludin in the CNS endothelium.⁴³ In addition, astrocytes can also generate and release vascular endothelial growth factor, which downregulates claudin-5 and occludin through activation of endothelial nitric oxide synthase (NOS) and increases BBB permeability.⁴⁴

Endothelial cells and smooth muscle cells

The ECs lining the lumen of vessels are the core anatomical unit of the barrier directly facing the blood flow, regulating transportation and communication between the CNS and blood circulation. Many features of ECs contribute to the barrier property. The paracellular junctions, mainly including tight junctions (TJs) and adherens junctions, hold the space between adjacent ECs and limit the paracellular flux of solutes.⁴⁵

These paracellular junctions primarily confer low paracellular permeability and high electrical resistance to the barrier in the CNS.^{6,46} The majority of the regulated transportation occurs through the paracellular route.⁴⁷ In addition, the ECs in BCNSB offer low-rate vesicle-mediated transportation across the endothelium, called transcytosis.^{45,48} This form of transportation is designed to transport macromolecules mediated by specialized structures, including clathrin, caveolae, and vesiculo-vacuolar-organelles.⁴⁹ Vesicles are likely to be a highly efficient and economical way of exchanging information across the BBB.⁵⁰ However, transcytosis is understudied in the spinal cord.

ECs and SMCs are major vasomotion effectors in the NVU that regulate blood flow in response to signals from neurons and astrocytes. ECs are equipped with a repertoire of voltage-gated ion channels, ligand-gated ion channels, and G-protein-coupled receptors, which provide the ability to respond to multiple physiological inputs in the CNS.^{3,51} Diverse bioactive molecules can elicit endothelial functions to regulate hemodynamics in the brain, and many of them are autocrine, such as adrenomedullin, angiotensin, NO, prostanoids, and several others.⁵² ECs also propagate vasomotor responses to regulate blood flow in the CNS in response to both chemical and mechanical signals from the luminal side.⁵³ Shear stress evoked by flowing blood and impinging on the endothelial surface can induce the release of dilatory NO.⁵³ Therefore, there is likely a positive feedback mechanism in which dilatation increases the blood flow at arterioles; thus, increased shear stress and release of NO can cause further vascular dilatation downstream.⁵⁴ The mechanosensory effect of shear force is probably mediated by the endothelial glycocalyx with changing oncotic pressure gradients at the endothelium surface,⁵⁵ transmitted by the pathway platelet endothelial cell adhesion molecule-1, vascular endothelial cell cadherin, and PI3 kinase.⁵⁶ Alternatively, the mechanosensory effect may be directly transduced by mechanosensitive ion channels, such as inwardly rectifying potassium channels (KIRs) and transient receptor potential cation channels V4 and Piezo-1.⁵⁷

The primary function of SMCs is to maintain the vascular tone or narrow vessel diameter to increase intravascular pressure,⁵⁸ by receiving signals from ECs, tissue metabolism, humoral stimuli, and neural stimuli.⁵⁹ ECs can directly affect SMCs via several mechanisms, including the release of signaling molecules such as NO, or electrical signals via myoendothelial gap junctions between ECs and SMCs.⁶⁰ In addition to directly responding to neurotransmitters released by neurons, the SMC also responds to the modulated signaling within astrocytes in the CNS. Neuronal activity can promote a calcium signal in

astrocytic endfeet decoded by Ca²⁺-sensitive K⁺ channels, which locally release K⁺ into the perivascular space to activate SMC inward rectifier K⁺ channels and cause vasodilation.³⁷ ATP from both neurons and astrocytes can activate purinergic receptors on SMCs. The activation of purinergic receptors P2X and P2Y in SMCs has been shown to cause an increase in Ca²⁺, thus causing SMC contraction.⁶¹ The influx of Ca²⁺ across the plasmalemma or the release of Ca²⁺ stores from the sarcoplasmic reticulum in SMCs could activate contractile proteins and narrow the vascular diameter.⁵⁸ In capillaries and postcapillary venules that lack SMCs, pericytes are thought to be the major regulators that replace SMCs.⁶² However, vessel dilation in capillaries occurs seconds prior to arterioles mediated by neurovascular coupling in the cerebral cortex.³⁴ Whether there is a functional relationship between SMCs and pericytes remains unclear. Furthermore, the contraction and relaxation of SMCs are simultaneously governed by multiple mechanisms from different cells in the NVU, which appears redundant and inconvenient, yet the physiological significance of this type of overlapping control on SMCs is not well understood.

Pericytes

Pericytes are embedded in the basement membrane at the capillary abluminal side.²⁹ Several neurovascular functions necessary for CNS homeostasis are regulated by pericytes, including BCNSB maintenance, vascular angioarchitecture, vesicle trafficking, and neurovascular coupling.^{63,64} Recruitment of pericytes to the capillary wall is a critical marker for maturity of the BCNSB.⁵ The pericyte synthesizes many elements of the basement membrane, such as proteoglycans and laminal proteins, which are thought to be critical in the differentiation of BCNSB.⁶⁵ Unlike astrocyte endfeet, pericyte remodeling is likely nonexistent in the brain.⁶⁶ This property may be essential in restoring capillary flow in injury or aging but has not been verified in the spinal cord. Pericytes regulate the function of BCNSB in at least two ways: regulating BCNSB-specific gene expression in ECs and inducing polarization of astrocyte endfeet surrounding blood vessels.⁶⁷ Pericytes probably control the expression of endothelial paracellular junctions, the alignment of TJs, and bulk flow transcytosis of vesicles across the BCNSB.⁶⁸ Coculture of pericytes with ECs has shown enhanced barrier function with increased expression of TJs and decreased permeability under healthy and hypoxic conditions.⁶⁹ Pericyte-deficient mouse models have increased permeability of the BBB,^{64,67} and reduced TJ proteins expression.⁷⁰

Pericytes are major regulators that adjust blood flow in the capillaries and postcapillary venules,⁶² by vasomotion according to neuronal activity changes in the CNS.³⁴ Pericytes possess contractile proteins, including the mesenchymal intermediate filament proteins vimentin and microfilaments that are assembled to actin and myosin, and to the contraction-related proteins tropomyosin and desmin.⁷¹ Pericytes have a Ca^{2+} -dependent contraction in response to neurotransmitters, neuronal activity, or electrical stimulation in neurovascular coupling.^{27,72} Neurotransmitters such as norepinephrine cause pericyte contraction, while gamma-aminobutyric acid, adenosine, glutamate, and dopamine cause pericyte relaxation.⁶⁸ These signals activate purinergic receptors or voltage-gated Ca^{2+} channels expressed on pericytes to increase intracellular Ca^{2+} and cause pericyte contraction.^{68,73} Activating K^+ channels decreases Ca^{2+} influx and causes pericyte relaxation in response to high lactate and carbon dioxide levels.^{27,40,74} Moreover, capillary dilation is reduced by blocking NOS, suggesting a role for NO in pericyte-induced capillary dilation and contraction.⁶² Such signals in neurovascular coupling for contraction can propagate between pericytes in the brain, probably transmitting through gap junctions between pericytes or ECs.⁴⁰ Hence, it has been theorized that the vascular responses may be initiated by pericytes in capillaries and then propagated to upstream arterioles, because pericytes are closer to the active neurons than arterioles in the brain, and the neuronal activity activates an outward membrane current in pericytes that dilate capillaries before the arterioles.^{40,62}

In pericyte-deficient mice with decreased pericyte coverage, cerebral microcirculation perfusion, oxygenation levels, and neurovascular coupling are diminished,⁷² and the BBB is dysfunctional resulting in an accumulation of neurotoxic substances in the brain.⁷⁰ Physiologically, the number of pericytes and their capillary coverage in the spinal cord are lower than those in the brain,⁷⁵ probably indicating that the regulating ability of capillaries is weaker in the spinal cord. In chronic SCI, the paradoxical excess activity of monoamine receptors on pericytes causes local capillaries to constrict abnormally and reduce blood flow.⁷⁶

Basement membrane

The BM is an essential accessory structure to seal the BCNSB, provide structural support and allow intercellular signaling communication in the NVU.²⁹ The space of discontinuous pericyte coverage and the space between astrocytes and endothelium are padded by BM. The BM is an extracellular matrix that in itself does not prevent small molecules from entering the CNS. Instead, it probably serves to restrict the passage of immune cells and provides a specific perivascular

microenvironment for substance exchange and signaling communication.⁷⁷ Disruption of the BM can lead to alterations in the cytoskeleton of the endothelium, in turn affecting TJ proteins and barrier integrity.⁶⁵

The BM in the CNS is mainly comprised of type IV collagen, fibronectin, laminins, and other glycoproteins. Collagen IV and fibronectin are secreted by multiple cells in the NVU, while deletion of either one is embryonic lethal.⁷⁸ Laminin contributes to BCNSB regulation and pericyte differentiation,²⁹ in addition to repairing BBB after ischemic brain injury.⁷⁹ Conditional deficiency of laminin leads to compromised BBB integrity with decreased pericyte coverage, diminished aquaporin-4 and TJs expression, and enhanced transcytosis.⁸⁰ Two main families of ECM receptors predominate in the BM, including dystroglycans and integrins. Laminin $\alpha 2$ -dystroglycan receptor interactions regulate the maturation and function of the BBB.⁸¹ Integrin $\beta 1$ is indispensable for proper VE-cadherin signaling and paracellular junction organization in the BBB.⁸² The degradation of the BM opens a conduit that enhances the migration of inflammatory cells into the parenchyma to aggravate the secondary injury.⁸³

Multiple proteases regulate the extracellular matrix (ECM) in the BM, such as matrix metalloproteinases (MMPs).⁸⁴ Currently, twenty-four human MMP homologs have been categorized into six subfamilies: collagenases, gelatinases, stromelysins, matrilysins, membrane-type metalloproteinases, and others.⁸⁵ MMPs are typically maintained at low expression levels in the adult CNS, which is necessary for maintaining normal functions of the ECM and is modified in pathological conditions.^{85,86} Some MMPs, such as MMP-1, -2, -3, -7, and -9, have been found to upregulate and break the BM in CNS injury.⁸⁷ These MMPs cleave the ECM, diminish signaling in the ECM, and degrade the paracellular junction proteins, thus disrupting BCNSB.⁸⁸ MMP-2 and MMP-9 can cleave dystroglycan to break the anchors of astrocyte endfeet.⁸⁹ MMP-8 and MMP-13 are also reported to be upregulated during neuroinflammation and are associated with BBB damage.⁹⁰ In addition, increased MMP-12 regulates ECM remodeling by inactivating some proteases, which is correlated with the development and myelination of the CNS.⁸⁴ The upregulation of MMPs has been widely reported to deteriorate the BSCB in SCI,^{9,16} mainly including MMP-2, -3, and -9.⁹¹ MMP-9 is the main contributor to disrupting the BSCB after SCI because MMP-9 inhibition or deficiency can reduce barrier disruption.⁹² However, MMP-2 and MMP-9 likely support tissue repair by ECM remodeling to facilitate angiogenesis and glial scar formation in chronic SCI.⁹³ MMP-2 deficiency leads to vascular instability, a decline in vascular-ity, and prolonged MMP-9 upregulation in SCI.⁹⁴

Moreover, MMP-12 knockout mice showed reduced permeability of the BSCB and improved functional recovery after SCI.⁹²

Other cells

Oligodendrocytes and microglia constantly reside around the NVU but are not traditionally considered part of it. The role of oligodendrocytes or oligodendrocyte precursor cells in the NVU is partially conclusive. Oligodendrocytes ensheath axons and are adjacent to astrocytes, pericytes, and endothelial cells in cerebral white matter.⁹⁵ The possible role of oligodendrocytes in the NVU may be to engage in cerebral vascular remodeling or regeneration through Wnt or Nogo signaling and release matrix metalloproteinase.⁹⁶ Perivascular microglia are immune cells in the CNS that inhabit the NVU and respond to changes in the NVU in disease. These microglia probably have dual-directional effects on the NVU, protecting NVU integrity in acute injury but engulfing astrocytic end-feet and increasing barrier permeability in chronic injury.⁹⁷ In addition, microglia probably have an unrecognized role in modulating blood flow and neurovascular coupling in the brain through P2RY12 signaling to interact with other cellular components in the NVU.^{98,99}

Autoregulation

Autoregulation is a self-adjusted mechanism involving constriction or dilation of cerebral resistance vessels to maintain constant tissue perfusion within a range of systemic mean arterial blood pressure (MAP). The vessels in the CNS constrict autonomically to impede blood flow when MAP increases, or dilate to facilitate blood flow when MAP decreases or the partial pressure of CO₂ increases.²³ This buffering system in the CNS is designed to stabilize blood perfusion to match metabolic need and maintain neural function during systemic blood pressure fluctuations. Lassen et al. first proposed this concept and described a plateau region wherein cerebral blood flow remains relatively stable across a range of MAP (60–150 mmHg).¹⁰⁰ Interestingly, Birch et al. identified that the relative capacity to buffer changes in cerebral blood flow is strongly dependent on the speed of changes in MAP. The slower the change in MAP, the smaller the impact on cerebral blood flow, to a point where cerebral blood flow becomes almost unaffected.¹⁰¹ Autoregulation ability of the spinal cord mirrors that of the brain, providing a similar mechanism for maintaining balance for spinal cord blood flow (SCBF).¹⁰²

However, the mechanism of autoregulation in the spinal cord seems more complicated. The autoregulation is still preserved after operationally sacrificing the

segmental arteries of the spinal cord.¹⁰³ Autoregulation remains intact in the thoracic spinal cord after the high cervical spinal cord is completely severed.¹⁰⁴ SCBF and local field potentials are not significantly affected and remain coupled in the preserved spinal cord segments, indicating that spinal cord autoregulation allows a potent adaptation when significant fluctuation in MAP occurs or supraspinal control is lost.¹⁰⁵

Autoregulation in the CNS is now divided into two categories: “static” and “dynamic” autoregulation.^{18,21} The former refers to blood perfusion or blood flow in the CNS maintaining a relatively steady state when MAP varies under physiological conditions.¹⁰⁶ Dynamic autoregulation refers to the ability of autoregulation to respond to rapid changes in blood pressure from seconds to minutes. The effectiveness of static autoregulation can be even more prominent with lower frequency changes in MAP. The progressively slower changes in MAP result in more minor changes in cerebral blood flow.¹⁸ Therefore, the MAP and cerebral blood perfusion are usually measured and averaged over longer time intervals (10 min or more) in experiments to make the resulting values adequately represent static autoregulation.¹⁸ In contrast, dynamic autoregulation requires high temporal resolution techniques to measure the fast changes in blood flow.¹⁰⁷ During more rapid changes in MAP, there is much greater variability in cerebral blood flow than the assumption based on Lassen’s concept of static autoregulation.¹⁸

The relationship between static and dynamic autoregulation has not been clearly identified. Tiecks et al. reported a robust linear relationship between static and dynamic autoregulation in the brain, probably denoting that static autoregulation is additionally maintained based on the constant and rapid adjustment of dynamic autoregulation.¹⁰⁸ Otherwise, they are opposite types of adaptive responses. As de Jong et al. suggested, there is a weak relationship between static and dynamic autoregulation in the brain, which has significant variability between individuals and sex.¹⁰⁹ In addition, after high-level SCI, static autoregulation is well maintained, while dynamic cerebral autoregulation is markedly altered, supporting the view that static and dynamic autoregulation are separated.¹¹⁰

Anatomical basis of spinal cord autoregulation

In humans, the parenchyma of the spinal cord is supplied by branches of several major arteries, including the vertebral and posterior-cerebellar arteries. The anterior radicular artery enters the spinal cord

bilaterally, with each anterior root joining the anterior spinal artery, which descends on the ventral surface of the spinal cord. Small branches of the vertebral or posterior-inferior cerebellar arteries continue caudally over the dorsal spinal cord, usually forming two small trunks known as the posterior spinal arteries (Figure 2). While the venous drainage of the spinal cord may be variable, its anatomic pattern often runs parallel to the paired artery.

Cardiac pulsatile flow can cause fluctuating hemodynamic changes in the arterial vessels of the spinal cord. Moreover, the vessels entering the spinal cord lack the siphon structure seen in the brain (such as the internal carotid artery siphon) to attenuate pulsatile variation of blood velocity and pressure.¹¹¹ How autoregulation of the spinal cord adjusts to these pulsatile hemodynamic changes is unclear. Theoretically, the pulsatile pressure load from blood flow in the spinal cord is supposed to be alleviated by large elastic arteries, as the arteries distend when the blood pressure rises during systole and recoil when the blood pressure falls during diastole, called Windkessel effect.¹¹² There is also a novel hypothesis that an extensive array of highly innervated arteriovenous glomeruli found in the spinal cord might be involved in the autoregulation of SCBF, because these arteriovenous anastomoses are similar in the pads of mammalian extremities or penis

to bypass the capillaries,¹¹³ but more data are needed to prove this hypothesis.

Signal transmission in autoregulation

Autoregulation in the CNS is considered to operate through multiple mechanisms including myogenic, metabolic, neurotransmitter-mediated, neurogenic, and systemic control (Figure 3).^{20,51} The myogenic mechanism encompasses the direct reflex response of vessels to variations in mechanical force caused by blood flow, such as perfusion pressure, shear force, and stretch force, which dictate the responses of ECs and SMCs.⁵¹ The metabolic mechanism of blood flow control in the CNS involves metabolic byproducts, such as lactate or CO₂, to regulate blood perfusion.⁵¹ Accumulating extracellular lactate can induce vessel relaxation which adjusts to the metabolic needs of neurons.¹¹⁴ Gap junction-coupled astrocytes can remove lactate from the extracellular fluid and discharge it through their endfeet into the perivascular fluid.¹¹⁵ The released lactate then causes vasodilation by some different mechanisms, either by releasing endothelial vasoactive substances such as NO and hindering the transport of extracellular prostaglandin,^{27,40} or by interfering with the metabolism of surrounding cells via the lactate/pyruvate ratio to release vasoactive substances.^{74,115}

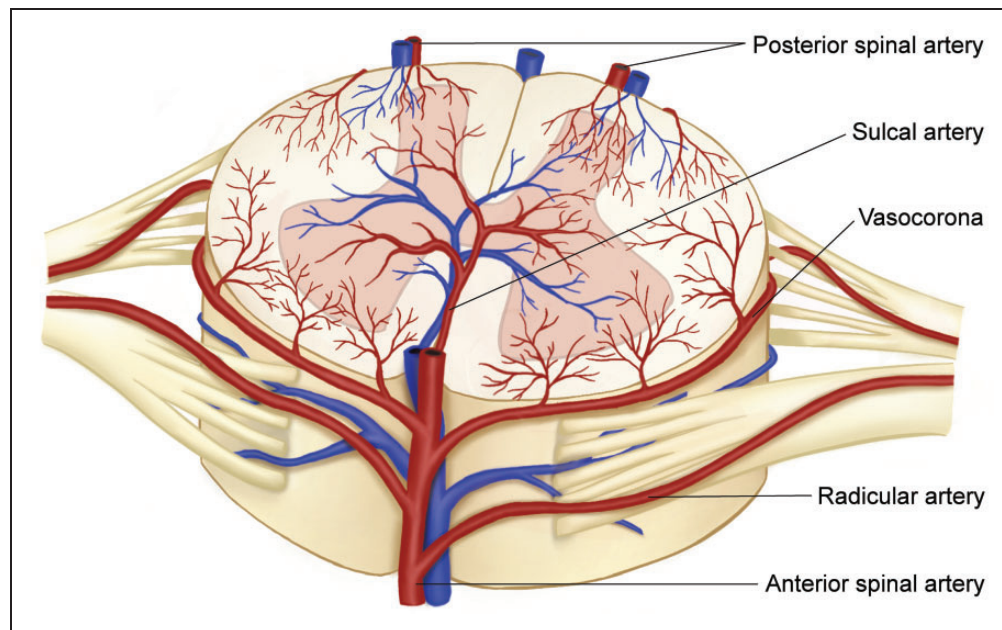


Figure 2. A dorsal view of the vascular anatomy of the spinal cord. The spinal cord is supplied by a net-like anastomosing vascular system from the branches of longitudinal anastomotic trunks: one anterior spinal artery and two posterolateral spinal arteries. The pattern of venous return is often parallel to the anatomic arteries. The spinal arteries are supplied by the aorta and lack the siphon structure as in the brain to attenuate cardiac pulsatile blood flow variation. The blood flow direction can change in the median spinal vessels and vasocorona due to multiple traffic branches. Theoretically, there is a dead point where the opposing pressures stop the blood flow. The location of the dead point is constantly changing due to physical activity or blood pressure fluctuation, indicating that autoregulation in the spinal cord is more sophisticated than in the brain.

The vasculature in the CNS is known to be innervated by (1) sympathetic nerves, (2) parasympathetic nerves, and (3) sensory nerves.¹¹⁶ Sympathetic control plays a vital role in the neurogenic autoregulation of the spinal cord. Autoregulation can be eliminated in animals receiving paravertebral sympathectomies, causing the SCBF to vary in a linear relationship with the changes in MAP.¹¹⁷ The neurotransmitter theory of autoregulation is very complicated. Neurons can release multiple neurotransmitters from nerve endings via the nervi-vasorum,⁵¹ or hierarchically through astrocytes and pericytes,^{32,118} to adjust vascular reactivity to control vascular reactivity.¹¹⁹ Several independent studies have reported that many neurotransmitters are involved

in autoregulation (Figure 3). Some neurotransmitters are directly vasoactive, such as adenosine, acetylcholine, catecholamines, and neuropeptides;³⁷ other neurotransmitters are not vasoactive but stimulate the production of vasodilators, including NO, metabolites of cyclooxygenase-2 (COX-2) and P450 epoxygenases, through downstream enzymatic activation in astrocytes and vascular cells.^{33,119}

However, it is difficult to discern the independent autoregulation mechanism in the CNS through inhibition or activation in experimental investigations because overlapping effects in the NVU provide redundant or synergistic effects in autoregulation.²⁰ Moreover, despite their sound theoretical background,

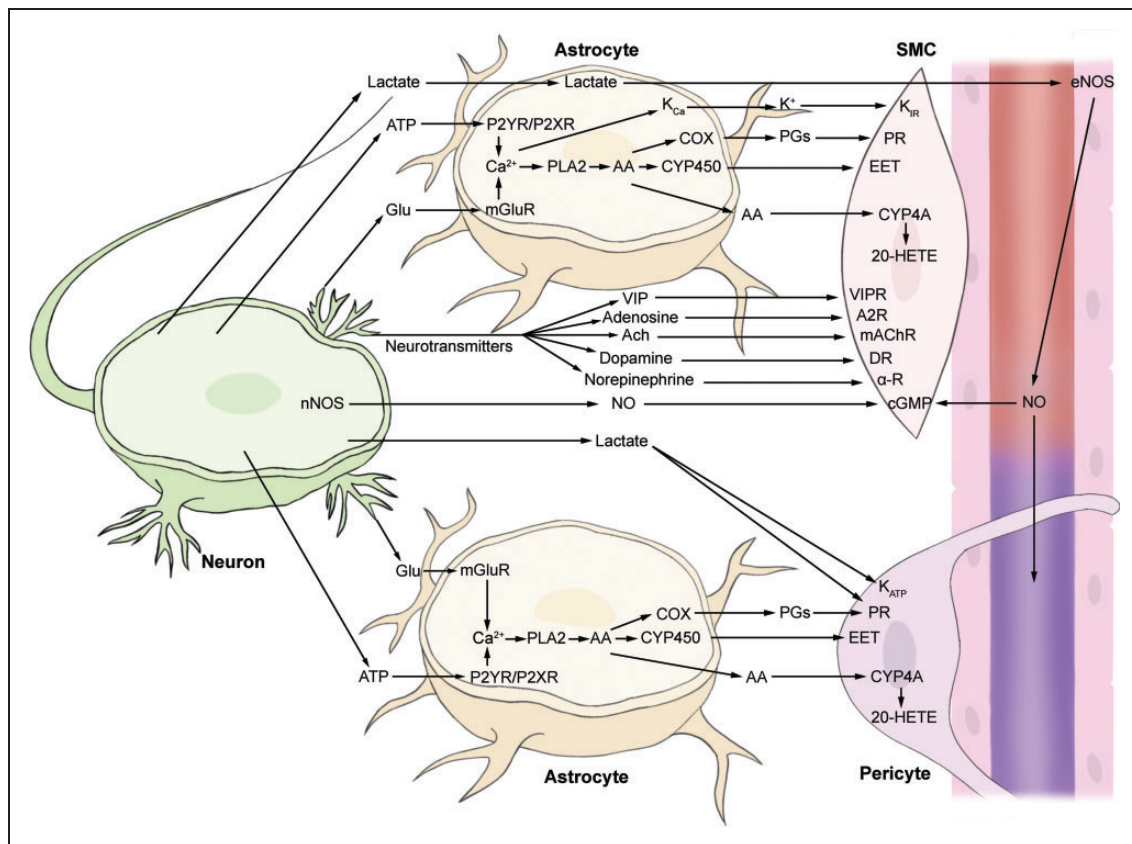


Figure 3. Simplified schematic diagram of the major pathways that regulate blood flow in the cerebral NVU. Neuronal presynaptic release of glutamate (Glu) is taken up by astrocytic processes and acts on metabotropic glutamate receptors (mGluR) to raise $[Ca^{2+}]$, inducing the generation of arachidonic acid (AA) from phospholipase A2 (PLA2). The ionotropic glutamate receptors seem less important in controlling blood flow in the spinal cord, and this signaling is not shown in the figure. AA can be converted to multiple prostaglandins (PGs) (by cyclooxygenase, COX), epoxyeicosatrienoic acid (EET) (by cytochrome P450 epoxygenase, CYP450) to dilate vessels, or 20-hydroxyeicosatetraenoic acid (20-HETE) (by ω -hydroxylase, CYP4A) to constrict vessels. Raised $[Ca^{2+}]$ in astrocyte endfeet may activate Ca^{2+} -gated K^+ channels (K_{Ca}) to release K^+ and activate inward rectifier K^+ channels (K_{IR}) on SMCs. The metabolic process of neurons releases adenosine triphosphate (ATP) acting on metabotropic purinergic receptors (P2XR or P2YR) on astrocytes to increase intracellular Ca^{2+} . The metabolic byproducts adenosine (to adenosine 2 receptor, A2R) and lactate activate ATP-sensitive potassium (K_{ATP}) channels, causing vessel relaxation; lactate inhibits PG transporters to cause PG accumulation or activate endothelial nitric oxide synthase (NOS) to release nitric oxide (NO), subsequently causing vasodilation. Neurons release diverse vasoactive neurotransmitters to control the NVU directly, such as vasoactive intestinal peptide (VIP) (to VIP receptor, VIPR), acetylcholine (ACh) (to muscarinic acetylcholine receptor, mAChR), dopamine (to dopamine receptor, DR), norepinephrine (to α -adrenoceptor, α -R), and NO (to cyclic guanosine monophosphate, cGMP).

these signaling molecules have broad communication and sometimes are able to activate each other. Thus, no single method has been universally accepted as a gold standard.¹⁹ In addition, side effects may interfere with results in different pharmacological experiments,²¹ easily disrupting the precise balance and confusing the understanding of this autocontrol mechanism in the NVU.

Neurovascular coupling

One vital role in the prototypical functions of the NVU is neurovascular coupling, previously called functional hyperemia.¹⁰ neurovascular coupling refers to the link between neural activity and blood flow, resulting in a rapid dilatation of blood vessels and blood flow acceleration near the activated neurons with high spatial and temporal correspondence.^{3,20,23} In animal models, focal spinal cord perfusion was observed to increase markedly during peripheral nerve stimulation.¹²⁰ These results suggest that neurovascular coupling in response to increased metabolic demands of neurons also exists in the spinal cord.

Neurovascular coupling is mainly regulated by neuron-astrocytic interactions in the NVU. Neurons release glutamate to activate metabotropic glutamate receptors on astrocytes and release Ca^{2+} , leading to the activation of downstream Ca^{2+} -dependent enzymes and the generation of vasodilatory substances.²⁶ In addition, ionotropic NMDA glutamatergic receptors activate NOS and release NO to regulate blood flow.²³ However, pharmacologically inhibiting NMDA receptors does not significantly affect blood flow in the spinal cord, indicating that these signals are not predominant in the spinal cord.¹²¹ Moreover, neurovascular coupling probably induces a remote response transmitted upstream where multiple cells release mediators to engage signaling pathways and activate effectors across the NVU network in a highly orchestrated manner.^{10,23} These signaling pathways in neurovascular coupling probably involve a feed-forward mechanism, resulting in the release of vasoactive substances, such as extracellular K^+ , NO, and prostanoids in the brain,^{34,40} but there is still not enough data to support its existence.^{10,20} There could also be a relationship between neurovascular coupling and dynamic autoregulation.¹²² The activity-induced retrograde propagation of vasodilation may also involve the dynamic autoregulation of the intravascular pressure changes induced by downstream vasodilatation in the brain,²³ but more data are needed to support this possibility.

The data regarding neurovascular coupling in the spinal cord are insufficient. Some reports have shown that task-related or peripheral nerve electrical stimulation can induce a noticeable increase in SCBF.¹²³

Interestingly, SCBF monitored by fMRI still remains coupled with local field potentials after spinal transection to abolish the changes in MAP.¹⁰⁵ Some BOLD-fMRI reports have detected neuronal activity-related blood flow changes in the spinal cord using averaged values per unit time or the flow-rephasing compensation method to eliminate the influence of pulsatile variation in blood flow.¹²⁴ However, these methods may not be suitable for detecting rapid blood flow changes, such as those in functional neurovascular coupling, because these averaged values may reflect the changes caused by dynamic autoregulation.

In addition, various methods quantifying the efficacy of NVU mechanisms accompany their respective limitations, contributing to results that sometimes appear conflicting.¹⁸ New imaging methods have recently provided in vivo evidence that neurovascular coupling exists in the spinal cord. Functional ultrasound imaging detects hemodynamic changes responding to electrical epidural stimulation that reflect neurovascular coupling in the spinal cord.¹²⁰ Intrinsic optical signals and light reflectance spectroscopy reveal that the light scattering of vessels and hemoglobin oxygen saturation in the lumbar spinal cord change simultaneously with peripheral electrical stimulation.¹²⁵ These results confirm that neurovascular coupling exists in the spinal cord.

Blood–central nervous system barrier

The modern concept of BCNSB was described by Davson et al. as limiting the entrance of plasma components, red blood cells, leukocytes, and foreign pathogens into the neural parenchyma in healthy conditions.¹²⁶ Moreover, the CNS parenchyma is thought to lack a potent innate immune response related to this barrier function, termed “immune privilege”. Pathogens introduced directly into the CNS parenchyma evade systemic immunological recognition.¹²⁷ Local cell death in the CNS parenchyma does not elicit a stereotypic response of myelomonocytic cells.¹²⁸ Despite some controversy regarding whether CNS parenchyma lacks humoral immunity surveillance,¹²⁹ the immune privilege or immunologically unique property of the CNS is primarily due to the BCNSB.¹²⁸

More functions have been subsequently found in the BCNSB. The BCNSB responds to stimuli that arise within both the CNS parenchyma and blood compartments.¹³⁰ In addition, the BCNSB serves as a key homeostatic site for the NVU to regulate nervous tissue perfusion,^{2,3,5} and a relay station for immune signaling between the blood and CNS via cytokines.²⁴ Furthermore, the BCNSB acts as both a secretory and endocrine target tissue with endocrine-like properties to enable substance exchange control

and communication.¹³¹ The BCNSB releases hormones and neuropeptides into the blood or the interstitial fluid,¹³² and is also a target for some hormones, such as leptin and insulin, to regulate glucose metabolism.¹³³

The endothelium in the CNS lacks membrane fenestrations and pinocytotic vesicles (transcellular pathway) when compared to peripheral organs and has extensive paracellular junctions to limit the flux between ECs (paracellular pathway).⁶⁵ The paracellular pathway is occupied by paracellular junctions, including TJs, to regulate barrier permeability and provide mechanical stability.^{2,6,45} The majority of trans-endothelium transport occurs through the paracellular route.⁴⁷ TJs are comprised of the claudin family, zonula occludens (ZO) family, TJ-associated MARVEL domain-containing proteins (TAMPs), and junctional adhesion molecules (JAMs).^{6,46} Claudins comprise TJ strands and play pivotal roles in regulating paracellular permeability.¹³⁴ Claudins interact with ZO proteins, which are scaffolding proteins with a cytoplasmic region that anchor to the cytomembrane and are essential for TJ assembly.⁶ In addition to TAMPs (including occludin and tricellulin), other members of the immunoglobulin superfamily, such as JAMs, endothelial cell-selective adhesion molecule (ESAM), and nectins, are also associated with TJs.¹³⁰ Adherens junctions involve the cadherin family and platelet endothelial cell adhesion molecules.⁸ These endothelial junctions impose a high trans-endothelial resistance of 1500–6000 Ω/cm^2 in cerebral capillaries and 20–50 Ω/cm^2 in the placental barrier.¹³⁵ In addition, the barrier has a negative surface charge to repulse anionically charged compounds,⁶⁵ which mainly come from the glycocalyx, a negatively charged dense layer of carbohydrates on the luminal side, acting as the first line of barrier and preventing immune cell entry.^{29,136} Some early studies utilized the loss of anionic charge to reflect BSCB disruption in SCI.¹³⁷ However, the disruption of the BCNSB still lacks a direct detection method.¹³⁸ In many studies, the common method used to evaluate BCNSB function is to measure the entry of serum proteins or intravenously injected tracers into the CNS.¹³⁰

The BCNSB contains multiple substrate-specific transport systems that control the transport of nutrients, energy metabolites, and other essential molecules transported between the interstitial fluid in the CNS and the blood,⁵ through passive diffusion, facilitated diffusion, and active transport.²⁴ The forms of exchanges interact broadly with hemodynamic changes and NVU functions.⁴⁷ The intravascular pressure gradient between arterioles and venules is the primary regulator of luminal flow.¹³⁵ Dilation of upstream resistance arterioles increases the pressure gradient, thus increasing blood flow in the capillary, which is critical for regulating transportation across the barrier.¹³⁵ The physiological

shear force corresponding to the increased blood flow in capillaries maintains the barrier phenotype through regulation of junctional protein and substance transportation.¹³⁵ BCNSB dysfunction-related blood flow reductions can further contribute to neurological deficits.²

Comparison of the BSCB and BBB

Traditionally, the characteristics of the BSCB are believed to be similar to the BBB,^{4,139} despite several minor structural and functional differences.¹⁷ The number of pericytes covering the BSCB is less than that covering the BBB.⁷⁵ The large superficial vessels in the spinal cord contain more glycogen deposits, which are not generally seen in the brain.¹⁴⁰ Compared to the BBB, the permeability of the BSCB is considered to be higher in the physiological state because the spinal cord generally takes up more tracers than the brain.¹⁴¹ In multiple sclerosis or experimental allergic encephalomyelitis affecting both the brain and spinal cord, more blood-derived interferons and tumor necrosis factors reach the spinal cord.¹³⁹ Compared to conditioned brain injury, the duration of the BSCB remains highly permeable after conditioned SCI, and the area of BSCB leakage is 2–3 times greater than that of BBB leakage.¹³⁹ These differences between the BBB and BSCB may be due to lower expression of TJ proteins (claudin-11, ZO-1, and occludin), adherens junction-associated proteins (beta-catenin and VE-cadherin), or efflux transporters (such as P-glycoprotein) in the spinal cord vasculature compared to the brain.^{142,143}

Advanced approaches to study the NVU in the spinal cord

The first quantitative study to calculate blood perfusion in the spinal cord with an autoradiographic technique by computing the intracardiac injected microspheres lodging in the spinal cord in proportion to the cardiac output.¹⁴⁴ Similar measurements using fluorescent or radioactive microspheres have reported the autoregulation ability in the spinal cord.¹⁴⁵ Later, various methods were developed to measure the SCBF, such as the hydrogen electrode technique, radioactivity or fluorometric angiography technique, Doppler flowmetry, and magnetic resonance imaging (MRI). However, these methods have a common drawback that is inappropriate for measuring NVU elements at high resolution. Some technological advances with high spatial and temporal resolution have recently been applied to measure neuronal and vascular dynamics in the brain,¹⁴⁶ but they have scarcely been used for investigating the spinal cord. Next, we review the methods that can be applied to monitoring NVU changes:

- (1) Intrinsic optical signal (IOS) imaging. The first intraoperative IOS imaging of the human brain was reported by Haglund's group to monitor stimulation-evoked epileptiform discharges and cognitively evoked functional activity in the cerebral cortex.¹⁴⁷ IOS detects changes in light reflectance and the absorption rate of oxyhemoglobin and deoxyhemoglobin to provide information about SCBF, oxygenation, and metabolism. In particular, IOS is commonly used *in vivo* to provide hemodynamic information in response to simultaneous neuronal activity changes through neurovascular coupling. After electrically stimulating the peripheral nerves, changes in optical reflectance can be recorded simultaneously in the dorsal spinal cord.¹⁴⁸ The responses in the spinal cord increase gradually as the current intensity of the peripheral stimulus increases. Whereas the stimulus intensity has a maximal level, the relationship between stimulus and response is nonlinear out of this range.¹⁴⁹
- (2) BOLD-fMRI. The most common form of functional MRI relies on detecting changes in different magnetic properties of oxyhemoglobin and deoxyhemoglobin, called the blood oxygenation level-dependent (BOLD) signal. BOLD-fMRI provides indirect measurements of functional activation of neuronal networks through neurovascular coupling via direct measurement of transient changes in tissue perfusion, blood-volume changes, or oxygen concentration.¹⁵⁰ MRI is the most preferred noninvasive method applied clinically for the spinal cord, as gray and white matter and adjacent structures in the spinal cord can be visualized. Task-related or peripheral stimuli-related functional responses in the spinal cord can be observed under BOLD-fMRI in humans, which can be used to predict motor and sensory recovery after SCI.¹²³ However, spinal BOLD-fMRI has low spatial specificity because of physiological motion, such as breathing and heartbeat, and predominantly draining veins on the surface of the spinal cord.¹⁵¹
- (3) Optical coherence tomography (OCT). An intrathecal OCT catheter can be used to observe the parenchyma, subarachnoid space, epidural vessels, dentate ligaments, and rootlets with an excellent minimally invasive visualization. Based on the interference pattern of low-coherence broadband light backscattered off the neural tissue, OCT can monitor the moving red blood cells as intrinsic contrast agents to directly measure SCBF. Furthermore, Doppler or speckle variance OCT imaging enables real-time visualization of SCBF in the posterior spinal venous vessels. OCT employing diffuse optical and correlation spectroscopies can also record the SCBF and oxygenation of the spinal cord in real time under various conditions.¹⁵²
- (4) Laser speckle contrast imaging (LSCI). LSCI detects the speckle contrast signals induced by the movement of red blood cells. This technique can monitor SCBF changes with an excellent spatial and temporal resolution by an ultrafast detector in a noncontact CCD camera. This wide-angle scanning technique can monitor spinal cord blood perfusion after SCI in animal models and patients in a full vision field intraoperatively.¹⁵³
- (5) Photoacoustic microscopy (PAM). PAM is a hybrid imaging technique based on the photoacoustic effect, combining the advantages of optical and ultrasound techniques and providing high ultrasonic spatial resolution.¹⁴⁶ A photoacoustic signal is generated after inducing pulsed laser energy, causing transient thermoelastic expansion of biological tissue that consequently emits high-frequency acoustic waves detectable by an ultrasound transducer. Imaging of blood optical absorption by PAM at multiple appropriately selected wavelengths can probe changes in hemoglobin concentration, blood volume, and hemoglobin oxygen saturation, along with functional hemodynamic responses to peripheral stimulation.¹⁵⁴ This method can also be utilized to assess tissue loss, guide microinjection, or trace exogenous contrast agents in the spinal cord.
- (6) Functional ultrasound imaging (fUSI). fUSI is a recently developed Doppler ultrasound method using a single plane-wave emission as one focused beam to obtain centimeter-level images and coherently sum the set of images from tilted planar illuminations. This 'compound' ultrasonic image has better resolution and lower noise than other functional imaging. This device can image the microvascular topology and cerebral hemodynamics *in vivo* with 100 μm resolution, tens of frames per second, and a penetration depth of approximately 8–9 mm in the rodent brain.¹⁵⁵ The fUSI can record the hemodynamic response to neuronal activation induced by peripheral natural or electrical stimulations at a restricted area of approximately 1 mm in the contralateral dorsal horn of the spinal cord.¹⁵⁶
- (7) Two-photon fluorescent laser scanning microscopy (2PLSM). 2PLSM is based on the nonlinear excitation of a single fluorescent molecule by two nearly coincident photons, having a great advantage over single-photon fluorescence microscopy. Because of the longer wavelength and lower energy of exciting light, 2PLSM has less laser-induced damage to the tissue and less photobleaching of the imaged fluorophores. In addition, longwave

length and low-frequency light is less scattered in the tissue, which enables deeper tissue penetration. One major limitation of 2PLSM is that the observed object needs fluorescence labeling. By probes or transgenic labeling, the electrical activity of neurons can be monitored directly with voltage-sensitive indicators or indirectly with calcium-sensitive and neurotransmitter-sensitive indicators.¹⁴⁶ Methodologically, measurement of hemodynamic change can be classified into two main categories: changes in perfusion or oxygenation. 2PLSM can fulfill the measurement of blood flow velocity and vascular parameters by intravenously injected fluorescence dye (such as Q-dot or fluorescence-labeled dextran) or the measurement of oxygen saturation by a phosphorescent probe (such as PtP-C343).¹⁵⁷ 2PLSM can acquire information from fluorescently labeled elements of the NVU in the spinal cord with a very high spatial and temporal resolution, such as the velocity of a single red blood cell. A two-photon-excitable oxygen sensor probe, such as PtP-C343, can be injected intravenously and imaged under 2PLSM to enable quantitative measurement of oxygen metabolism changes in neurovascular coupling.¹⁵⁸

All these methods have advantages and disadvantages and need to be chosen accordingly. Although having an unsurpassed spatial resolution, the 2PLSM can only image the dorsal spinal cord for limited penetration depth and relatively small imaging volume. PAM or fUSI provides deeper tissue penetration to reach the ventral side, so they are suitable for imaging cord-wide changes in NVU activity. MRI cannot provide sufficient spatial resolution to study individual vascular events. BOLD-fMRI is suitable for monitoring organic variation in blood perfusion but is limited by the long delays between sequential images.¹⁵⁷ 2PLSM can directly measure the changes in blood velocity or microvascular diameter and is therefore better for surveying neurovascular coupling. However, except for the LSCI and BOLD-fMRI, which give specific values that can be used to reference the changes in blood perfusion, the results detected by other methods require the assistance of formulas (Poiseuille's law) to estimate changes in blood perfusion.

NVU dysfunction in SCI

After SCI, the normal communication patterns within the NVU can be severely altered. The interruption of metabolism and angioarchitecture after injury can disturb the integrity of NVU function, leading to inappropriate blood perfusion changes⁷ and BSCB disruption.¹⁷ Amending NVU dysfunction after SCI, such as BSCB

disruption and ischemia, is crucial in the secondary injury mechanism.¹⁵⁰

Furthermore, assessment of small vessel disease in the spinal cord demonstrated a relationship between barrier impairment and lower tissue perfusion, suggesting that defects in functional elements in the NVU can affect each other.¹⁵⁹ Evidence shows that amyotrophic lateral sclerosis is a neurovascular disease, characterized by BSCB disruption, microhemorrhage, and microcirculation hypoperfusion,¹⁶⁰ similar to the secondary injury in SCI. However, NVU dysfunction in SCI may be more complicated, but related investigations are scarce.

Blood supply dysregulation in SCI

Disrupted autoregulation has been observed in early SCI reports.¹⁶¹ However, whether this "autoregulation of blood perfusion" is an organic level autogenous perfusion control or managed by the NVU has not been confirmed. The systemic blood circulation deficiency after injury could overwhelm the autoregulation of the spinal cord, covering up the changes in this regulatory mechanism. Generally, despite traumatic blood loss, there is a transient state of spinal shock characterized by paralysis of the muscle pump and denervation of the cardiac pump to reduce effective blood circulation.¹⁵ Severe systemic hypotension occurs with evident autonomic dysfunction and attenuated cardiopulmonary output, especially after cervical injuries, termed autonomic dysreflexia.¹¹⁰ It is characterized by loss of supraspinal sympathetic control on the heart and decreased cardiac pump function. Systemic vasodilation secondary to loss of sympathetic tone further causes low effective circulating blood volume.¹⁶² Profound hypotension leads to MAP failing to maintain autoregulation, continuously aggravating NVU dysfunction. SCI patients sometimes suffer cognitive impairments probably induced by NVU dysfunction caused by cerebral hypoperfusion, which could be reversed by increasing blood pressure.¹⁶³

In addition to these systemic effects, the impaired autoregulatory capacity in spinal vasculature can further render the spinal cord vulnerable to systemic hypotension and contribute to ongoing ischemia.¹⁵ Posttraumatic spinal cord ischemia worsens progressively after several hours and persists for weeks in SCI.¹⁵³ Hence, medical evidence-based guidelines suggest a level III recommendation to maintain the MAP between 85 and 90 mmHg for the first seven days following SCI.¹⁶⁴ Regardless of spontaneous neurologic recovery after spinal shock, management of MAP alone cannot provide a stable curative effect on the neurological prognosis of SCI patients,¹⁶⁵ making this issue more inexplicable.

Diverse mechanisms can affect blood flow in the spinal cord, including intraspinal cord pressure, which can even change the blood flow direction in venous vessels.¹⁶⁶ Given that the spinal cord is enveloped in the nonelastic dura and bony canal, it may obey the Monro-Kellie doctrine as in the brain.¹⁶⁷ Namely, the total volume of neural tissues, cerebrospinal fluid, and intraspinal blood are fixed. Increased intraspinal cord pressure after SCI caused by tissue swelling or bleeding may exhaust this compensatory ability. The higher the pathological intraspinal cord pressure is, the more deranged the autoregulation of the spinal cord. The intraspinal cord pressure increases significantly after SCI,¹⁶⁸ and the blood flow perfusion and oxygenation metabolism plummets after SCI and remains chronically diminished.¹⁶⁹

Theoretically, when autoregulation is disturbed in SCI, the arterioles are maximally dilated due to local acidosis and hypoxia, and the perfusion of the spinal cord is directly proportional to the systemic blood pressure.¹⁴⁴ However, autoregulation in the injured spinal segment can be preserved for 1–2 hours after SCI.^{113,161} During this period, a pathological hemodynamic change characterized as a significant blood flow acceleration in venous vessels occurs quickly after SCI and is maintained for approximately 1–2 hours. The pharmacologically elevating MAP only increases blood perfusion for one more hour before ischemia occurs, while for 4 hours, it is accompanied by cerebrospinal fluid drainage.¹⁷⁰ The time course of autoregulation dysfunction in SCI still needs to be elucidated.

Due to the distribution of radicular arteries, blood flow can ascend or descend within the spinal cord, creating numerous watershed areas of blood supply where opposing vascular currents meet. Watershed areas are more susceptible to ischemia.¹⁶⁶ Perfusion in the injured spinal cord is usually a patch-like pattern intersected by regions of low, intermediate, and high blood flow.¹⁵³ However, many reports find that hyperperfusion management by vasoconstriction agents after SCI has no benefit.¹⁴⁵ Some parts of the injury site were only perfused in the systolic period¹⁵³ and reversely exacerbated hemorrhage and tissue edema.¹⁶⁷ Despite the unfavorable systemic hypotension, vasodilatation agents can dilate the neighboring nondilated arterioles in the well-perfused regions and steal blood from the injured spinal cord (steal-phenomenon).¹⁵³ Interestingly, when a calcium channel blocker (nimodipine), which inhibits the contraction of vascular SMCs, is additionally administered for hyperperfusion management after SCI, local perfusion and electrophysiological output both improve.¹⁷¹ These studies showed that autoregulation in SCI is far from understood, and the potential pharmacological treatment still needs further testing in SCI.

BSCB disruption in SCI

The BSCB disruption permits proinflammatory substances to enter the spinal parenchyma to amplify the pathophysiological cascades and magnify additional damage.¹⁷ In the murine model, BSCB disruption in the acute SCI usually has biphasic peaks: immediate leakage at the epicenter and adjacent site within several hours and a delayed permeability increment with longer duration.¹⁴¹ After mechanical impact, BSCB leakage generally starts in 5–15 min at the epicenter^{17,47} and gradually appears in segments away from the epicenter, even along the whole spinal cord in some cases.¹³⁰ The murine models show that the segment located 1 cm away from the epicenter suffered BSCB leakage in 30 minutes and 2 cm away in approximately 3 hours.¹⁷² The caudal segments seem more vulnerable to BSCB disruption than the rostral segments.¹⁴⁰ These phenomena suggest that the mechanism of BSCB disruption may be more complex in SCI. Moreover, the barrier disruption is difficult to quantitate except for measuring the leakage of hematogenous tracers where bleeding could also occur,⁴⁷ combining hemorrhage and BSCB disruption together to confuse matters. Some data indicate that BSCB disruption in the early period of SCI is a secondary change after mechanical damage. Pathological hemodynamic changes and leukocyte transmigration disrupt the BSCB after SCI and inhibiting these processes can also attenuate BSCB disruption. Much work is needed to clarify the mechanism of BSCB disruption in SCI according to the current view.

Some early studies suggested that BSCB leakage after SCI is caused by vesicular transport.¹⁷² Electron microscopy showed that large numbers of vesicles appeared in the swollen ECs in capillaries and venules within 6 to 10 min after SCI, but without widening of the paracellular junctions.¹⁷³ Several forms of vesicle-based transcytosis exist and allow particular macromolecules to cross the endothelium, which can be classified into two categories: clathrin-mediated and caveolae-mediated.⁴⁷ The former is receptor-mediated to transfer insulin and transferrin; the latter is adsorptive transcytosis, where charged interactions between the molecule and plasma membrane facilitate its entry.¹⁷⁴ However, vesicular transport abnormalities seem not to be primarily responsible for BSCB disruption after SCI. Because transcytosis as an active transport process is low-rate, selective, and energy dependent,⁴⁸ it seems not to correlate with the extensive BSCB leakage of nonselective tracers of varied size in SCI.¹⁷ Nevertheless, there are no further data to prove whether these vesicles are influx or efflux because vesicles are bidirectionally transported or whether these vesicles are caveolae,¹⁷⁵ which is closely related to neurovascular

coupling.¹⁷⁶ A recent report found many junctional discontinuities emerging on TJs 15 minutes after SCI, and reducing these junctional discontinuities can decrease BSCB leakage. Combined with the previous electron microscopy data demonstrating no widening of the paracellular junctions,¹⁷³ these results probably indicate that not all paracellular junctions are disintegrated in the BSCB leakage after SCI.

Many groups have suggested the degeneration of TJs as the reason for BSCB disruption in SCI, using the expression level of TJs as the indicator for BSCB function.¹⁷⁷ However, most results report that TJs are downregulated at approximately 12–24 h after SCI.¹⁷⁸ The expression of TJs remains unchanged in the early period of SCI when BSCB disruption occurs. Sometimes, a decrease in TJs expression may reflect that BSCB damage is more severe than paracellular leakage, such as whole endothelial cell loss.¹³⁰ Therefore, the related treatment to reverse the downregulation of TJs requires more caution when applied to clinical trials, especially in the acute period of SCI.

Conclusion and future directions

Today's view of the NVU has been broadly amplified. The BCNSB is constantly regarded as a functional configuration in the NVU. Despite the significant similarity of the NVU between the brain and spinal cord, investigation of the NVU in the spinal cord lags far behind that in the brain. Minor differences can be observed in the major elements of the NVU from the limited data available. The vascular anatomy of the spinal cord is markedly different from that of the brain, and the blood flow in the spinal cord is more variable and fluctuating, indicating a more sophisticated autoregulation mechanism in the spinal cord. NMDA receptor-mediated neurovascular coupling is less predominant in the spinal cord. Moreover, the permeability of the BSCB is physiologically higher than that of the BBB, probably because the coverage of pericytes and the expression of some paracellular junctional proteins are inherently lower than those of the BBB. More studies are needed to explore the spinal cord NVU.

Further, in SCI, impaired NVU function could be involved in secondary injury and exacerbate severity. Models of SCI should be weighed to explore the underlying mechanisms contributing to NVU dysfunction. The development of therapies to prevent and treat NVU dysfunction in SCI requires targeted exploration of the injury mechanisms of the NVU.

Funding

The author(s) disclosed receipt of the following financial support for the research, authorship, and/or publication of this

article: This work was supported by the National Natural Science Foundation of China (81971160) and the Peking University Medicine Seed Fund for Interdisciplinary Research (BMU2018MX021).

Declaration of conflicting interests

The author(s) declared no potential conflicts of interest with respect to the research, authorship, and/or publication of this article.

ORCID iD

Fang Zhou  <https://orcid.org/0000-0002-7775-069X>

References

1. Zlokovic BV. Neurovascular pathways to neurodegeneration in Alzheimer's disease and other disorders. *Nat Rev Neurosci* 2011; 12: 723–738.
2. Sweeney MD, Zhao Z, Montagne A, et al. Blood-brain barrier: from physiology to disease and back. *Physiol Rev* 2019; 99: 21–78.
3. Kaplan L, Chow BW and Gu C. Neuronal regulation of the blood-brain barrier and neurovascular coupling. *Nat Rev Neurosci* 2020; 21: 416–432.
4. Reinhold AK and Rittner HL. Barrier function in the peripheral and central nervous system – a review. *Pflugers Arch* 2017; 469: 123–134.
5. Zhao Z, Nelson AR, Betsholtz C, et al. Establishment and dysfunction of the blood-brain barrier. *Cell* 2015; 163: 1064–1078.
6. Zlokovic BV. The blood-brain barrier in health and chronic neurodegenerative disorders. *Neuron* 2008; 57: 178–201.
7. Sandsmark DK, Bashir A, Wellington CL, et al. Cerebral microvascular injury: a potentially treatable endophenotype of traumatic brain injury-induced neurodegeneration. *Neuron* 2019; 103: 367–379.
8. Liebner S, Dijkhuizen RM, Reiss Y, et al. Functional morphology of the blood-brain barrier in health and disease. *Acta Neuropathol* 2018; 135: 311–336.
9. Tran AP, Warren PM and Silver J. The biology of regeneration failure and success after spinal cord injury. *Physiol Rev* 2018; 98: 881–917.
10. Iadecola C. The neurovascular unit coming of age: a journey through neurovascular coupling in health and disease. *Neuron* 2017; 96: 17–42.
11. Candelario-Jalil E, Dijkhuizen RM and Magnus T. Neuroinflammation, stroke, blood-brain barrier dysfunction, and imaging modalities. *Stroke* 2022; 53: 1473–1486.
12. Wang L, Xiong X, Zhang L, et al. Neurovascular unit: a critical role in ischemic stroke. *CNS Neurosci Ther* 2021; 27: 7–16.
13. Li C, Wang Y, Yan XL, et al. Pathological changes in neurovascular units: lessons from cases of vascular dementia. *CNS Neurosci Ther* 2021; 27: 17–25.
14. Xie L, Lu B, Ma Y, et al. The 100 most-cited articles about the role of neurovascular unit in stroke

- 2001–2020: a bibliometric analysis. *CNS Neurosci Ther* 2021; 27: 743–752.
15. Ahuja CS, Wilson JR, Nori S, et al. Traumatic spinal cord injury. *Nat Rev Dis Primers* 2017; 3: 17018.
 16. Kumar H, Ropper AE, Lee SH, et al. Propitious therapeutic modulators to prevent blood-spinal cord barrier disruption in spinal cord injury. *Mol Neurobiol* 2017; 54: 3578–3590.
 17. Bartanusz V, Jezova D, Alajajian B, et al. The blood-spinal cord barrier: morphology and clinical implications. *Ann Neurol* 2011; 70: 194–206.
 18. Claassen J, Thijssen DHJ, Panerai RB, et al. Regulation of cerebral blood flow in humans: physiology and clinical implications of autoregulation. *Physiol Rev* 2021; 101: 1487–1559.
 19. Claassen JA, Meel-van den Abeelen AS, Simpson DM, et al. Transfer function analysis of dynamic cerebral autoregulation: a white paper from the international cerebral autoregulation research network. *J Cereb Blood Flow Metab* 2016; 36: 665–680.
 20. Phillips AA, Chan FH, Zheng MM, et al. Neurovascular coupling in humans: physiology, methodological advances and clinical implications. *J Cereb Blood Flow Metab* 2016; 36: 647–664.
 21. Willie CK, Tzeng YC, Fisher JA, et al. Integrative regulation of human brain blood flow. *J Physiol* 2014; 592: 841–859.
 22. Chatterjee S, Fujiwara K, Perez NG, et al. Mechanosignaling in the vasculature: emerging concepts in sensing, transduction and physiological responses. *Am J Physiol Heart Circ Physiol* 2015; 308: H1451–1462.
 23. Schaeffer S and Iadecola C. Revisiting the neurovascular unit. *Nat Neurosci* 2021; 24: 1198–1209.
 24. Mastorakos P and McGavern D. The anatomy and immunology of vasculature in the central nervous system. *Sci Immunol* 2019; 4: eaav0492.
 25. Otsu Y, Couchman K, Lyons DG, et al. Calcium dynamics in astrocyte processes during neurovascular coupling. *Nat Neurosci* 2015; 18: 210–218.
 26. Mishra A, Reynolds JP, Chen Y, et al. Astrocytes mediate neurovascular signaling to capillary pericytes but not to arterioles. *Nat Neurosci* 2016; 19: 1619–1627.
 27. Kisler K, Nelson AR, Montagne A, et al. Cerebral blood flow regulation and neurovascular dysfunction in Alzheimer disease. *Nat Rev Neurosci* 2017; 18: 419–434.
 28. Mathiisen TM, Lehre KP, Danbolt NC, et al. The perivascular astroglial sheath provides a complete covering of the brain microvessels: an electron microscopic 3D reconstruction. *Glia* 2010; 58: 1094–1103.
 29. Langen UH, Ayloo S and Gu C. Development and cell biology of the Blood-Brain barrier. *Annu Rev Cell Dev Biol* 2019; 35: 591–613.
 30. Koehler RC, Roman RJ and Harder DR. Astrocytes and the regulation of cerebral blood flow. *Trends Neurosci* 2009; 32: 160–169.
 31. Simard M, Arcuino G, Takano T, et al. Signaling at the gliovascular interface. *J Neurosci* 2003; 23: 9254–9262.
 32. MacVicar BA and Newman EA. Astrocyte regulation of blood flow in the brain. *Cold Spring Harb Perspect Biol* 2015; 7: a020388.
 33. Zonta M, Angulo MC, Gobbo S, et al. Neuron-to-astrocyte signaling is central to the dynamic control of brain microcirculation. *Nat Neurosci* 2003; 6: 43–50.
 34. Grutzendler J and Nedergaard M. Cellular control of brain capillary blood flow: in vivo imaging veritas. *Trends Neurosci* 2019; 42: 528–536.
 35. Gu X, Chen W, Volkow ND, et al. Synchronized astrocytic Ca(2+) responses in neurovascular coupling during somatosensory stimulation and for the resting state. *Cell Rep* 2018; 23: 3878–3890.
 36. Jukkola P, Guerrero T, Gray V, et al. Astrocytes differentially respond to inflammatory autoimmune insults and imbalances of neural activity. *Acta Neuropathol Commun* 2013; 1: 70.
 37. Filosa JA, Bonev AD, Straub SV, et al. Local potassium signaling couples neuronal activity to vasodilation in the brain. *Nat Neurosci* 2006; 9: 1397–1403.
 38. Mulligan SJ and MacVicar BA. Calcium transients in astrocyte endfeet cause cerebrovascular constrictions. *Nature* 2004; 431: 195–199.
 39. Petzold GC and Murthy VN. Role of astrocytes in neurovascular coupling. *Neuron* 2011; 71: 782–797.
 40. Attwell D, Buchan AM, Charkpak S, et al. Glial and neuronal control of brain blood flow. *Nature* 2010; 468: 232–243.
 41. Chow BW and Gu C. Gradual suppression of transcytosis governs functional blood-retinal barrier formation. *Neuron* 2017; 93: 1325–1333.e3.
 42. Sanmarco LM, Polonio CM, Wheeler MA, et al. Functional immune cell-astrocyte interactions. *J Exp Med* 2021; 218
 43. Alvarez JI, Dodelet-Devillers A, Kebir H, et al. The hedgehog pathway promotes blood-brain barrier integrity and CNS immune quiescence. *Science* 2011; 334: 1727–1731.
 44. Argaw AT, Asp L, Zhang J, et al. Astrocyte-derived VEGF-A drives blood-brain barrier disruption in CNS inflammatory disease. *J Clin Invest* 2012; 122: 2454–2468.
 45. Daneman R and Prat A. The blood-brain barrier. *Cold Spring Harb Perspect Biol* 2015; 7: a020412.
 46. Otani T and Furuse M. Tight junction structure and function revisited. *Trends Cell Biol* 2020; 30: 805–817.
 47. Wettschureck N, Strlic B and Offermanns S. Passing the vascular barrier: Endothelial signaling processes controlling extravasation. *Physiol Rev* 2019; 99: 1467–1525.
 48. Conner SD and Schmid SL. Regulated portals of entry into the cell. *Nature* 2003; 422: 37–44.
 49. Doherty GJ and McMahon HT. Mechanisms of endocytosis. *Annu Rev Biochem* 2009; 78: 857–902.
 50. van der Pol E, Boing AN, Harrison P, et al. Classification, functions, and clinical relevance of extracellular vesicles. *Pharmacol Rev* 2012; 64: 676–705. DOI: 10.1124/pr.112.005983.
 51. Zeiler FA, Thelin EP, Donnelly J, et al. Genetic drivers of cerebral blood flow dysfunction in TBI: a speculative synthesis. *Nat Rev Neurol* 2019; 15: 25–39.

52. Kis B, Chen L, Ueta Y, et al. Autocrine peptide mediators of cerebral endothelial cells and their role in the regulation of blood-brain barrier. *Peptides* 2006; 27: 211–222.
53. Zhou J, Li YS and Chien S. Shear stress-initiated signaling and its regulation of endothelial function. *Arterioscler Thromb Vasc Biol* 2014; 34: 2191–2198.
54. Jacob M, Chappell D and Becker BF. Regulation of blood flow and volume exchange across the microcirculation. *Crit Care* 2016; 20: 319.
55. Tarbell JM, Simon SI and Curry FR. Mechanosensing at the vascular interface. *Annu Rev Biomed Eng* 2014; 16: 505–532.
56. Tzima E, Irani-Tehrani M, Kiosses WB, et al. A mechanosensory complex that mediates the endothelial cell response to fluid shear stress. *Nature* 2005; 437: 426–431.
57. Baratchi S, Khoshmanesh K, Woodman OL, et al. Molecular sensors of blood flow in endothelial cells. *Trends Mol Med* 2017; 23: 850–868.
58. Knot HJ and Nelson MT. Regulation of arterial diameter and wall [Ca²⁺] in cerebral arteries of rat by membrane potential and intravascular pressure. *J Physiol* 1998; 508: 199–209.
59. Harraz OF, Hill-Eubanks D and Nelson MT. PIP2: a critical regulator of vascular ion channels hiding in plain sight. *Proc Natl Acad Sci U S A* 2020; 117: 20378–20389.
60. Hill-Eubanks DC, Gonzales AL, Sonkusare SK, et al. Vascular TRP channels: performing under pressure and going with the flow. *Physiology (Bethesda)* 2014; 29: 343–360.
61. Pascual O, Casper KB, Kubera C, et al. Astrocytic purinergic signaling coordinates synaptic networks. *Science* 2005; 310: 113–116.
62. Hall CN, Reynell C, Gesslein B, et al. Capillary pericytes regulate cerebral blood flow in health and disease. *Nature* 2014; 508: 55–60.
63. Winkler EA, Bell RD and Zlokovic BV. Central nervous system pericytes in health and disease. *Nat Neurosci* 2011; 14: 1398–1405.
64. Daneman R, Zhou L, Kebede AA, et al. Pericytes are required for blood-brain barrier integrity during embryogenesis. *Nature* 2010; 468: 562–566.
65. Cardoso FL, Brites D and Brito MA. Looking at the blood-brain barrier: molecular anatomy and possible investigation approaches. *Brain Res Rev* 2010; 64: 328–363.
66. Berthiaume AA, Schmid F, Stamenkovic S, et al. Pericyte remodeling is deficient in the aged brain and contributes to impaired capillary flow and structure. *Nat Commun* 2022; 13: 5912.
67. Armulik A, Genove G, Mae M, et al. Pericytes regulate the blood-brain barrier. *Nature* 2010; 468: 557–561.
68. Sweeney MD, Ayyadurai S and Zlokovic BV. Pericytes of the neurovascular unit: key functions and signaling pathways. *Nat Neurosci* 2016; 19: 771–783.
69. Hori S, Ohtsuki S, Hosoya K, et al. A pericyte-derived angiopoietin-1 multimeric complex induces occludin gene expression in brain capillary endothelial cells through tie-2 activation in vitro. *J Neurochem* 2004; 89: 503–513.
70. Bell RD, Winkler EA, Sagare AP, et al. Pericytes control key neurovascular functions and neuronal phenotype in the adult brain and during brain aging. *Neuron* 2010; 68: 409–427.
71. Attwell D, Mishra A, Hall CN, et al. What is a pericyte? *J Cereb Blood Flow Metab* 2016; 36: 451–455.
72. Kisler K, Nelson AR, Rege SV, et al. Pericyte degeneration leads to neurovascular uncoupling and limits oxygen supply to brain. *Nat Neurosci* 2017; 20: 406–416.
73. Rungta RL, Chaigneau E, Osmanski BF, et al. Vascular compartmentalization of functional hyperemia from the synapse to the pia. *Neuron* 2018; 99: 362–375 e364.
74. Gordon GR, Choi HB, Rungta RL, et al. Brain metabolism dictates the polarity of astrocyte control over arterioles. *Nature* 2008; 456: 745–749.
75. Winkler EA, Sengillo JD, Bell RD, et al. Blood-spinal cord barrier pericyte reductions contribute to increased capillary permeability. *J Cereb Blood Flow Metab* 2012; 32: 1841–1852.
76. Li Y, Lucas-Osma AM, Black S, et al. Pericytes impair capillary blood flow and motor function after chronic spinal cord injury. *Nat Med* 2017; 23: 733–741.
77. Carvey PM, Hendey B and Monahan AJ. The blood-brain barrier in neurodegenerative disease: a rhetorical perspective. *J Neurochem* 2009; 111: 291–314.
78. Poschl E, Schlotzer-Schrehardt U, Brachvogel B, et al. Collagen IV is essential for basement membrane stability but dispensable for initiation of its assembly during early development. *Development* 2004; 131: 1619–1628.
79. Nirwane A and Yao Y. Cell-specific expression and function of laminin at the neurovascular unit. *J Cereb Blood Flow Metab* 2022; 42: 1979–1999.
80. Gautam J, Cao Y and Yao Y. Pericytic laminin maintains blood-brain barrier integrity in an age-dependent manner. *Transl Stroke Res* 2020; 11: 228–242.
81. Menezes MJ, McClenahan FK, Leiton CV, et al. The extracellular matrix protein laminin alpha2 regulates the maturation and function of the blood-brain barrier. *J Neurosci* 2014; 34: 15260–15280.
82. Yamamoto H, Ehling M, Kato K, et al. Integrin beta1 controls VE-cadherin localization and blood vessel stability. *Nat Commun* 2015; 6: 6429.
83. Milich LM, Ryan CB and Lee JK. The origin, fate, and contribution of macrophages to spinal cord injury pathology. *Acta Neuropathol* 2019; 137: 785–797.
84. de Almeida LGN, Thode H, Eslambolchi Y, et al. Matrix metalloproteinases: from molecular mechanisms to physiology, pathophysiology, and pharmacology. *Pharmacol Rev* 2022; 74: 712–768.
85. Rempe RG, Hartz AMS and Bauer B. Matrix metalloproteinases in the brain and blood-brain barrier: Versatile breakers and makers. *J Cereb Blood Flow Metab* 2016; 36: 1481–1507.
86. Loffek S, Schilling O and Franzke CW. Series “matrix metalloproteinases in lung health and disease”: biological role of matrix metalloproteinases: a critical balance. *Eur Respir J* 2011; 38: 191–208.

87. Abdul-Muneer PM, Pfister BJ, Haorah J, et al. Role of matrix metalloproteinases in the pathogenesis of traumatic brain injury. *Mol Neurobiol* 2016; 53: 6106–6123.
88. Rosenberg GA. Matrix metalloproteinases and their multiple roles in neurodegenerative diseases. *Lancet Neurol* 2009; 8: 205–216.
89. Agrawal S, Anderson P, Durbeej M, et al. Dystroglycan is selectively cleaved at the parenchymal basement membrane at sites of leukocyte extravasation in experimental autoimmune encephalomyelitis. *J Exp Med* 2006; 203: 1007–1019.
90. Figueiredo CA, Steffen J, Morton L, et al. Immune response and pathogen invasion at the choroid plexus in the onset of cerebral toxoplasmosis. *J Neuroinflammation* 2022; 19: 17.
91. Zhang H, Chang M, Hansen CN, et al. Role of matrix metalloproteinases and therapeutic benefits of their inhibition in spinal cord injury. *Neurotherapeutics* 2011; 8: 206–220.
92. Veeravalli KK, Dasari VR and Rao JS. Regulation of proteases after spinal cord injury. *J Neurotrauma* 2012; 29: 2251–2262.
93. Verslegers M, Lemmens K, Van Hove I, et al. Matrix metalloproteinase-2 and -9 as promising benefactors in development, plasticity and repair of the nervous system. *Prog Neurobiol* 2013; 105: 60–78.
94. Trivedi A, Zhang H, Ekeledo A, et al. Deficiency in matrix metalloproteinase-2 results in long-term vascular instability and regression in the injured mouse spinal cord. *Exp Neurol* 2016; 284: 50–62.
95. Shindo A, Liang AC, Maki T, et al. Subcortical ischemic vascular disease: roles of oligodendrocyte function in experimental models of subcortical white-matter injury. *J Cereb Blood Flow Metab* 2016; 36: 187–198.
96. Niu J, Tsai HH, Hoi KK, et al. Aberrant oligodendroglial-vascular interactions disrupt the blood-brain barrier, triggering CNS inflammation. *Nat Neurosci* 2019; 22: 709–718.
97. Haruwaka K, Ikegami A, Tachibana Y, et al. Dual microglia effects on blood brain barrier permeability induced by systemic inflammation. *Nat Commun* 2019; 10: 5816.
98. Bisht K, Okojie KA, Sharma K, et al. Capillary-associated microglia regulate vascular structure and function through PANX1-P2RY12 coupling in mice. *Nat Commun* 2021; 12: 5289.
99. Dufort C, Wang Y and Hu X. Microglia: Active participants in brain capillary function. *J Cereb Blood Flow Metab* 2022; 42: 2161–2163.
100. Lassen NA. Cerebral blood flow and oxygen consumption in man. *Physiol Rev* 1959; 39: 183–238.
101. Diehl RR, Linden D, Lucke D, et al. Phase relationship between cerebral blood flow velocity and blood pressure. a clinical test of autoregulation. *Stroke* 1995; 26: 1801–1804.
102. Hickey R, Albin MS, Bunegin L, et al. Autoregulation of spinal cord blood flow: is the cord a microcosm of the brain? *Stroke* 1986; 17: 1183–1189.
103. Halstead JC, Wurm M, Etz C, et al. Preservation of spinal cord function after extensive segmental artery sacrifice: regional variations in perfusion. *Ann Thorac Surg* 2007; 84: 789–794.
104. Kobrine AI, Doyle TF, Newby N, et al. Preserved autoregulation in the rhesus spinal cord after high cervical cord section. *J Neurosurg* 1976; 44: 425–428.
105. Piche M, Paquette T and Leblond H. Tight neurovascular coupling in the spinal cord during nociceptive stimulation in intact and spinal rats. *Neuroscience* 2017; 355: 1–8.
106. van Beek AH, Claassen JA, Rikkert MG, et al. Cerebral autoregulation: an overview of current concepts and methodology with special focus on the elderly. *J Cereb Blood Flow Metab* 2008; 28: 1071–1085.
107. Greenfield JC, Jr., Rembert JC and Tindall GT. Transient changes in cerebral vascular resistance during the Valsalva maneuver in man. *Stroke* 1984; 15: 76–79.
108. Tiecks FP, Lam AM, Aaslid R, et al. Comparison of static and dynamic cerebral autoregulation measurements. *Stroke* 1995; 26: 1014–1019.
109. de Jong DLK, Tarumi T, Liu J, et al. Lack of linear correlation between dynamic and steady-state cerebral autoregulation. *J Physiol* 2017; 595: 5623–5636.
110. Phillips AA, Ainslie PN, Krassioukov AV, et al. Regulation of cerebral blood flow after spinal cord injury. *J Neurotrauma* 2013; 30: 1551–1563.
111. van Tuijl RJ, Ruigrok YM, Velthuis BK, et al. Velocity pulsatility and arterial distensibility along the internal carotid artery. *J Am Heart Assoc* 2020; 9: e016883.
112. Belz GG. Elastic properties and windkessel function of the human aorta. *Cardiovasc Drugs Ther* 1995; 9: 73–83.
113. Martirosyan NL, Feuerstein JS, Theodore N, et al. Blood supply and vascular reactivity of the spinal cord under normal and pathological conditions. *J Neurosurg Spine* 2011; 15: 238–251.
114. Pournaras CJ, Rungger-Brandle E, Riva CE, et al. Regulation of retinal blood flow in health and disease. *Prog Retin Eye Res* 2008; 27: 284–330.
115. Diel GA. Brain lactate metabolism: the discoveries and the controversies. *J Cereb Blood Flow Metab* 2012; 32: 1107–1138.
116. Frederiksen SD, Haanes KA, Warfvinge K, et al. Perivascular neurotransmitters: Regulation of cerebral blood flow and role in primary headaches. *J Cereb Blood Flow Metab* 2019; 39: 610–632.
117. Young W. Sympathectomy and spinal cord blood flow. *J Neurosurg* 1992; 77: 654–655.
118. Hartmann DA, Coelho-Santos V and Shih AY. Pericyte control of blood flow across microvascular zones in the central nervous system. *Annu Rev Physiol* 2022; 84: 331–354.
119. Montalbano MJ, Loukas M, Oskouian RJ, et al. Innervation of the blood vessels of the spinal cord: a comprehensive review. *Neurosurg Rev* 2018; 41: 733–735.
120. Tang S, Cuellar CA, Song P, et al. Changes in spinal cord hemodynamics reflect modulation of spinal network with different parameters of epidural stimulation. *Neuroimage* 2020; 221: 117183.

121. Kristensen JD, Karlsten R and Gordh T. Laser-Doppler evaluation of spinal cord blood flow after intrathecal administration of an N-methyl-D-aspartate antagonist in rats. *Anesth Analg* 1994; 78: 925–931.
122. Acharya D, Ruesch A, Schmitt S, et al. Changes in neurovascular coupling with cerebral perfusion pressure indicate a link to cerebral autoregulation. *J Cereb Blood Flow Metab* 2022; 42: 1247–1258.
123. Stroman PW, Khan HS, Bosma RL, et al. Changes in pain processing in the spinal cord and brainstem after spinal cord injury characterized by functional magnetic resonance imaging. *J Neurotrauma* 2016; 33: 1450–1460.
124. Sprenger C, Finsterbusch J and Buchel C. Spinal cord-midbrain functional connectivity is related to perceived pain intensity: a combined spino-cortical fMRI study. *J Neurosci* 2015; 35: 4248–4257.
125. Sharma V, He JW, Narvenkar S, et al. Quantification of light reflectance spectroscopy and its application: determination of hemodynamics on the rat spinal cord and brain induced by electrical stimulation. *Neuroimage* 2011; 56: 1316–1328.
126. Davson H. Review lecture. The blood-brain barrier. *J Physiol* 1976; 255: 1–28.
127. Andersson PB, Perry VH and Gordon S. Intracerebral injection of proinflammatory cytokines or leukocyte chemotaxins induces minimal myelomonocytic cell recruitment to the parenchyma of the Central nervous system. *J Exp Med* 1992; 176: 255–259.
128. Engelhardt B, Vajkoczy P and Weller RO. The movers and shapers in immune privilege of the CNS. *Nat Immunol* 2017; 18: 123–131.
129. Abbott NJ, Pizzo ME, Preston JE, et al. The role of brain barriers in fluid movement in the CNS: is there a ‘glymphatic’ system? *Acta Neuropathol* 2018; 135: 387–407.
130. Erickson MA and Banks WA. Neuroimmune axes of the blood-brain barriers and blood-brain interfaces: bases for physiological regulation, disease states, and pharmacological interventions. *Pharmacol Rev* 2018; 70: 278–314.
131. Banks WA. The blood-brain barrier as an endocrine tissue. *Nat Rev Endocrinol* 2019; 15: 444–455.
132. Ghersi-Egea JF, Strazielle N, Catala M, et al. Molecular anatomy and functions of the choroidal blood-cerebrospinal fluid barrier in health and disease. *Acta Neuropathol* 2018; 135: 337–361.
133. Kastin AJ and Akerstrom V. Glucose and insulin increase the transport of leptin through the blood-brain barrier in normal mice but not in streptozotocin-diabetic mice. *Neuroendocrinology* 2001; 73: 237–242.
134. Zihni C, Mills C, Matter K, et al. Tight junctions: from simple barriers to multifunctional molecular gates. *Nat Rev Mol Cell Biol* 2016; 17: 564–580.
135. Hajal C, Le Roi B, Kamm RD, et al. Biology and models of the blood-brain barrier. *Annu Rev Biomed Eng* 2021; 23: 359–384.
136. Kutuzov N, Flyvbjerg H and Lauritzen M. Contributions of the glycocalyx, endothelium, and extravascular compartment to the blood-brain barrier. *Proc Natl Acad Sci U S A* 2018; 115: E9429–E9438.
137. Mautes AE, Weinzierl MR, Donovan F, et al. Vascular events after spinal cord injury: contribution to secondary pathogenesis. *Phys Ther* 2000; 80: 673–687.
138. Saunders NR, Dreifuss JJ, Dziegielewska KM, et al. The rights and wrongs of blood-brain barrier permeability studies: a walk through 100 years of history. *Front Neurosci* 2014; 8: 404.
139. Zhang B and Gensel JC. Is neuroinflammation in the injured spinal cord different than in the brain? Examining intrinsic differences between the brain and spinal cord. *Exp Neurol* 2014; 258: 112–120.
140. Sharma HS. Pathophysiology of blood-spinal cord barrier in traumatic injury and repair. *Curr Pharm Des* 2005; 11: 1353–1389.
141. Neuwelt E, Abbott NJ, Abrey L, et al. Strategies to advance translational research into brain barriers. *Lancet Neurol* 2008; 7: 84–96.
142. Uchida Y, Sumiya T, Tachikawa M, et al. Involvement of claudin-11 in disruption of blood-brain, -spinal cord, and -arachnoid barriers in multiple sclerosis. *Mol Neurobiol* 2019; 56: 2039–2056.
143. Uchida Y, Yagi Y, Takao M, et al. Comparison of absolute protein abundances of transporters and receptors among blood-brain barriers at different cerebral regions and the blood-spinal cord barrier in humans and rats. *Mol Pharm* 2020; 17: 2006–2020.
144. Mortazavi MM, Verma K, Harmon OA, et al. The microanatomy of spinal cord injury: a review. *Clin Anat* 2015; 28: 27–36.
145. Guha A, Tator CH and Rochon J. Spinal cord blood flow and systemic blood pressure after experimental spinal cord injury in rats. *Stroke* 1989; 20: 372–377.
146. Urban A, Golgher L, Brunner C, et al. Understanding the neurovascular unit at multiple scales: advantages and limitations of multi-photon and functional ultrasound imaging. *Adv Drug Deliv Rev* 2017; 119: 73–100.
147. Haglund MM, Ojemann GA and Hochman DW. Optical imaging of epileptiform and functional activity in human cerebral cortex. *Nature* 1992; 358: 668–671.
148. Sasaki S, Sato K, Shinomiya K, et al. Postnatal changes in intrinsic optical responses to peripheral nerve stimulation in the in vivo rat spinal cord. *Neuroimage* 2003; 20: 2126–2134.
149. Sasaki S, Yazawa I, Miyakawa N, et al. Optical imaging of intrinsic signals induced by peripheral nerve stimulation in the in vivo rat spinal cord. *Neuroimage* 2002; 17: 1240–1255.
150. David G, Mohammadi S, Martin AR, et al. Traumatic and nontraumatic spinal cord injury: pathological insights from neuroimaging. *Nat Rev Neurol* 2019; 15: 718–731.
151. Leitch JK, Figley CR and Stroman PW. Applying functional MRI to the spinal cord and brainstem. *Magn Reson Imaging* 2010; 28: 1225–1233.
152. Mesquita RC, D’Souza A, Bilfinger TV, et al. Optical monitoring and detection of spinal cord ischemia. *PLoS One* 2013; 8: e83370.

153. Gallagher MJ, Hogg FRA, Zoumprouli A, et al. Spinal cord blood flow in patients with acute spinal cord injuries. *J Neurotrauma* 2019; 36: 919–929.
154. Liao LD, Lin CT, Shih YY, et al. Transcranial imaging of functional cerebral hemodynamic changes in single blood vessels using in vivo photoacoustic microscopy. *J Cereb Blood Flow Metab* 2012; 32: 938–951.
155. Martinez de Paz JM and Mace E. Functional ultrasound imaging: a useful tool for functional connectomics? *Neuroimage* 2021; 245: 118722.
156. Claron J, Hingot V, Rivals I, et al. Large-scale functional ultrasound imaging of the spinal cord reveals in-depth spatiotemporal responses of spinal nociceptive circuits in both normal and inflammatory states. *Pain* 2021; 162: 1047–1059.
157. Fumagalli S, Ortolano F and De Simoni MG. A close look at brain dynamics: cells and vessels seen by in vivo two-photon microscopy. *Prog Neurobiol* 2014; 121: 36–54.
158. Lecoq J, Parpaleix A, Roussakis E, et al. Simultaneous two-photon imaging of oxygen and blood flow in deep cerebral vessels. *Nat Med* 2011; 17: 893–898.
159. Wong SM, Jansen JFA, Zhang CE, et al. Blood-brain barrier impairment and hypoperfusion are linked in cerebral small vessel disease. *Neurology* 2019; 92: e1669–e1677.
160. Rule RR, Schuff N, Miller RG, et al. Gray matter perfusion correlates with disease severity in ALS. *Neurology* 2010; 74: 821–827.
161. Senter HJ and Venes JL. Loss of autoregulation and posttraumatic ischemia following experimental spinal cord trauma. *J Neurosurg* 1979; 50: 198–206.
162. Partida E, Mironets E, Hou S, et al. Cardiovascular dysfunction following spinal cord injury. *Neural Regen Res* 2016; 11: 189–194.
163. Phillips AA, Warburton DE, Ainslie PN, et al. Regional neurovascular coupling and cognitive performance in those with low blood pressure secondary to high-level spinal cord injury: improved by alpha-1 agonist midodrine hydrochloride. *J Cereb Blood Flow Metab* 2014; 34: 794–801.
164. Walters BC, Hadley MN, Hurlbert RJ, et al. Guidelines for the management of acute cervical spine and spinal cord injuries: 2013 update. *Neurosurgery* 2013; 60: 82–91.
165. Saadeh YS, Smith BW, Joseph JR, et al. The impact of blood pressure management after spinal cord injury: a systematic review of the literature. *Neurosurg Focus* 2017; 43: E20.
166. Hernandez-Gerez E, Fleming IN and Parson SH. A role for spinal cord hypoxia in neurodegeneration. *Cell Death Dis* 2019; 10: 861.
167. Saadoun S and Papadopoulos MC. Acute, severe traumatic spinal cord injury: monitoring from the injury site and expansion duraplasty. *Neurosurg Clin N Am* 2021; 32: 365–376.
168. Khaing ZZ, Cates LN, Fishedick AE, et al. Temporal and spatial evolution of raised intraspinal pressure after traumatic spinal cord injury. *J Neurotrauma* 2017; 34: 645–651.
169. Meyer BP, Hirschler L, Lee S, et al. Optimized cervical spinal cord perfusion MRI after traumatic injury in the rat. *J Cereb Blood Flow Metab* 2021; 41: 2010–2025.
170. Martirosyan NL, Kalani MY, Bichard WD, et al. Cerebrospinal fluid drainage and induced hypertension improve spinal cord perfusion after acute spinal cord injury in pigs. *Neurosurgery* 2015; 76: 461–468; discussion 468–469.
171. Fehlings MG, Tator CH and Linden RD. The effect of nimodipine and dextran on axonal function and blood flow following experimental spinal cord injury. *J Neurosurg* 1989; 71: 403–416.
172. Noble LJ and Wrathall JR. Distribution and time course of protein extravasation in the rat spinal cord after contusive injury. *Brain Res* 1989; 482: 57–66.
173. Griffiths IR, McCulloch M and Crawford RA. Ultrastructural appearances of the spinal microvasculature between 12 hours and 5 days after impact injury. *Acta Neuropathol* 1978; 43: 205–211.
174. Ayloo S and Gu CH. Transcytosis at the blood-brain barrier. *Curr Opin Neurobiol* 2019; 57: 32–38.
175. Parton RG. Caveolae: Structure, function, and relationship to disease. *Annu Rev Cell Dev Biol* 2018; 34: 111–136.
176. Chow BW, Nunez V, Kaplan L, et al. Caveolae in CNS arterioles mediate neurovascular coupling. *Nature* 2020; 579: 106–110.
177. Jin LY, Li J, Wang KF, et al. Blood-spinal cord barrier in spinal cord injury: a review. *J Neurotrauma* 2021; 38: 1203–1224.
178. Chio JCT, Wang J, Badner A, et al. The effects of human immunoglobulin G on enhancing tissue protection and neurobehavioral recovery after traumatic cervical spinal cord injury are mediated through the neurovascular unit. *J Neuroinflammation* 2019; 16: 141.