#### **ORIGINAL ARTICLE**



# Cerebellar Transcranial Alternating Current Stimulation in Essential Tremor Patients with Thalamic Stimulation: A Proof-of-Concept Study

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#### Abstract

Essential tremor (ET) is a disabling condition resulting from a dysfunction of cerebello-thalamo-cortical circuitry. Deep brain stimulation (DBS) or lesion of the ventral-intermediate thalamic nucleus (VIM) is an effective treatment for severe ET. Transcranial cerebellar brain stimulation has recently emerged as a non-invasive potential therapeutic option. Here, we aim to investigate the effects of high-frequency non-invasive cerebellar transcranial alternating current stimulation (tACS) in severe ET patients already operated for VIM-DBS. Eleven ET patients with VIM-DBS, and 10 ET patients without VIM-DBS and matched for tremor severity, were included in this double-blind proof-of-concept controlled study. All patients received unilateral cerebellar sham-tACS and active-tACS for 10 min. Tremor severity was blindly assessed at baseline, without VIM-DBS, during sham-tACS, during and at 0, 20, 40 min after active-tACS, using kinetic recordings during holding posture and action ('nose-to-target') task and videorecorded Fahn-Tolosa-Marin (FTM) clinical scales. In the VIM-DBS group, active-tACS significantly improved both postural and action tremor amplitude and clinical (FTM scales) severity, relative to baseline, whereas sham-tACS did not, with a predominant effect for the ipsilateral arm. Tremor amplitude and clinical severity were also not significantly different between ON VIM-DBS and active-tACS conditions. In the non-VIM-DBS group, we also observed significant improvements in ipsilateral action tremor amplitude, and clinical severity after cerebellar active-tACS, with a trend for improved postural tremor amplitude. In non-VIM-DBS group, sham- active-tACS also decreased clinical scores. These data support the safety and potential efficacy of high-frequency cerebellar-tACS to reduce ET amplitude and severity.

Keywords Essential tremor · Transcranial alternating current stimulation · Cerebellum · Deep brain stimulation · Motion capture

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# Introduction

Essential tremor (ET) is a frequent and disabling disorder with progressive worsening postural tremor of the arms, which seriously affects quality of life [1]. ET has been associated with pathological changes in the cerebellum [2], reduced function of the cerebellar cortex and abnormal

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oscillations within the cerebello-thalamo-cortical (CTC) network [2-10]. High-frequency deep brain stimulation (DBS) of the ventral intermediate nucleus of the thalamus (VIM), which receives afferent inputs from the cerebellar deep nuclei, is very effective in improving ET [11-13]. It can decrease tremor amplitude by up to 40-80%, by disrupting the abnormal rhythmic activity within the CTC network with low- and high-frequency thalamic oscillation reduction [14-16]. Although effective and well-tolerated [16], this technique is an invasive neurosurgical procedure, and decreasing responsiveness and the occurrence of side-effects could impact its benefits in the long-term [17, 18]. Recently, VIM lesioning using focused ultrasound has been reported to drastically improve ET symptoms with good tolerance [19, 20]. However, both treatments are of high cost with potential adverse events.

Non-invasive brain stimulation (NIBS) techniques targeting the cerebellum, such as repetitive transcranial magnetic stimulation (rTMS), theta burst stimulation (TBS) or transcutaneous direct current stimulation (tDCS), have also been tested in a few studies to manage ET [21-26]. Open-label studies and a recent meta-analysis suggested positive therapeutic effects of cerebellar NIBS for ET [21, 23], although double-blind proof-of-concept studies mainly failed to demonstrate its therapeutic interest of NIBS [24, 27, 28]. In two recent controlled trials, low-frequency rTMS applied over the cerebellum induced a significant improvement in tremor severity immediately after [25, 29]. Recently, transcranial alternating current stimulation (tACS) has emerged as a NIBS technique to manipulate intrinsic neuronal oscillations with externally applied rhythmic electrical frequencies, with after-effects that can persist over 1 h after current offset [30]. When applied over the cerebellum at 5 Hz or 300 Hz in healthy subjects, it led to an increase in cerebellar-brain inhibition (CBI), with no changes in the short-intracortical inhibition and short-afferent inhibition [31, 32]. Applied at 50 Hz it induced no changes [31] or a CBI weakening with better sequential tapping adaptation [32]. Lastly, phase-locked cerebellar tACS has also been shown to decrease tremor amplitude in a small sample of patients with ET [33] or with non-jerky dystonic tremor [34]. Finally, the fact that: 1) all these previous data highlight the potential benefits of cerebellar tACS in modulating CTC network functioning; 2) ET patients exhibited various abnormal neuronal oscillations within the CTC network, including very low and high frequency oscillations, which may reflect altered Purkinje cells GABAergic neurotransmission [35, 36, 37]; 3) high-frequency thalamic DBS dramatically improves ET severity in correlation with increased activation within the whole CTC network, intra-regional inhibition with decreased neuronal oscillations [17], strongly support the potential value of cerebellar tACS for ET management.

Here, we hypothesise that high-frequency tACS could improve tremor severity similarly to high-frequency VIM-DBS, by increasing GABAergic inputs to deep cerebellar nuclei, and subsequently modulate the CTC network excitability and neuronal oscillations. To test this hypothesis, we first studied the effects of high-frequency VIM-DBS and cerebellar tACS applied at the same frequency in ET patients previously treated by VIM-DBS. We also tested the effects of high-frequency cerebellar tACS in a group of ET patients not previously operated for VIM-DBS and matched for tremor severity.

#### Methods

#### **Study Design and Patients**

In this double-blind trial, we recruited patients from the Salpêtrière Hospital, Paris, France. All patients were assessed at the Paris Brain Institute. Two groups of patients were included. All patients were eligible for inclusion if they fulfilled ET diagnosis criteria according to the Task Force on tremor of the International Parkinson and Movement Disorders Society [38], were aged 18 to 75 years, had no other causes of tremor or neurological disorders, were affiliated to the French national health insurance or similar scheme, agreed to participate and provided written informed consent. An additional inclusion criterion was unilateral VIM-DBS for more than 6 months prior to this study for patients in the VIM-DBS group. This study received approval from the local ethics committee of Paris VI University and the French Ministry of Health. All patients gave written informed consent. The study was performed according to the Declaration of Helsinki and Good clinical practice guidelines, and was sponsored by the INSERM (C14-44). Clinical trial.gov registration: NCT02346409.

#### Procedures

Patients with VIM-DBS were first assessed with unilateral VIM-DBS ON with their usual stimulation parameters, and the DBS was then switched OFF for 3 h to avoid rebound effects due to sudden neurostimulation cessation. Then, all patients were assessed without treatment, OFF VIM-DBS for patients previously operated (baseline assessment). Then, each patient first received sham-tACS followed by active high-frequency tACS for 10 min each, without being informed of the order of application, and at 0, 20 and 40 min after current offset (Fig. 1). Anti-tremor drugs were stopped 7 days before the assessment in both groups, except for propranolol which was stopped the day before.

We performed assessments of tremor severity by using the Fahn-Tolosa-Marin (FTM) scale [39], and kinetic



Fig. 1 Study design. For VIM-DBS patients (upper panel, left part), assessments were performed first ON-VIM DBS, then after ceasing VIM-DBS for 3 h (OFF DBS/baseline). In the OFF-DBS condition, sham-tACS was applied for 10 min followed by active-cerebellar tACS for 10 min. Patients were assessed during sham-tACS, during active-tACS and at 0, 20 and 40 min following current offset. The same protocol was applied for the patients not previously oper-

ated for VIM-DBS, i.e. No-DBS Group (lower panel, left part). We measured tremor amplitude using kinematic arm recordings using the VICON® 3D motion capture system with 29 reflective markers positioned bilaterally on the arms, head and trunk during posture holding and action with the 'nose-to-target' task (right part, lower and upper panels, respectively)

recordings of arm tremor using a VICON® 3D motion capture system with 29 reflective markers positioned bilaterally on the arms, head and trunk (Fig. 1).

Cerebellar tACS was administrated to patients at rest, seated in a chair, and positioned in front of a table. tACS was delivered by a battery-driven stimulator (NeuroConn, DC-Stimulator Plus, CE) connected to a pair of saline-soaked square-shaped sponge electrodes (9  $\text{cm}^2$ ). One electrode was positioned over the posterior cerebellum (3 cm lateral to the inion), contralateral to VIM-DBS, whereas the return electrode was positioned over the contralateral cheekbone. Electrodes were fixed by elastic bands. For the control group, we applied cerebellar tACS ipsilaterally to the most severe side with a similar set-up. During active stimulation, tACS was delivered at a frequency of 130 to 180 Hz matched to the chronic VIM-DBS stimulation frequency in the VIM-DBS group; and at 130 Hz in the No-DBS group. The stimulation intensity was set at 1 mA and was applied over a 10-min period resulting in a current density of 0.11 mA/cm<sup>2</sup> [40] and a delivered total charge of 0.066 C/cm<sup>2</sup>. Sham-tACS was also applied for a 10 min period starting with delivery of a 1 mA current but for 10 s only. All patients reported a moderate local paraesthesia at the beginning of both shamand active-tACS and they were unable to differentiate the two conditions.

#### **Randomization and Masking**

This proof-of-concept trial was double-blind and shamcontrolled (Fig. 1). All the assessments were recorded and videorecorded, and rated in random order by two blinded investigators at the end of the study (ZK performed the clinical scale rating and OC the kinetics analysis), all sequences having been previously coded by a blinded clinical research assistant.

#### Outcomes

The predefined primary outcome was tremor amplitude, as assessed by the displacements of the markers positioned on

the arms during a 5 s holding posture (arms folded, wrists slightly extended, fingers apart). Secondary endpoints included: i) the movement duration for performance of the 'nose-to-target' task with a marker placed on a support on the table at a fixed position with 5 round trips (Fig. 1), and the displacement of the finger marker within a 2cm<sup>2</sup> area around the target (reflecting the pointing precision); ii) the clinical severity with the total score of the FTM scale, with part A rating the tremor severity of each body part in different posture and action tasks and part B rating the tremor severity during handwriting, drawing and pouring (we did not assess orthostatic tremor in part A, nor pouring in part B); and iii) the safety and tolerance of the procedure, as assessed by the occurrence of adverse events, serious adverse events or discomfort.

#### **Statistical Analysis**

In this study, we aimed to examine the changes in tremor severity with active cerebellar high frequency tACS. In line with previous data obtained after cerebellar NIBS [21, 23, 25], we expected a decrease of 25% (SD 15%) in the tremor amplitude during active tACS with respect to baseline. With this assumption, our 10 patients should enable us to have a power of 90% with an alpha error rate of 5% (Wilcoxon signed-rank test).

The main outcome criterion was the sum of the displacements of the arm markers during posture holding (postural tremor) at the different timepoints. Secondary outcomes were the time required to perform the 'nose-to-target' task (action tremor) and the precision of targeting (measured by the displacements of the finger markers in the  $2 \text{ cm}^2$  area around the target, Fig. 1), and the FTM scores. For this purpose, we modelled each outcome using a linear mixed model. We included the treatment condition (baseline or OFF VIM-DBS, ON VIM-DBS, during sham-tACS, during and 0, 20, 40 min after active-tACS) and patient intercepts as random effects. We used R (R, version 3.3.1, R Core Development Team, FactoMineR package) for statistical analyses, with the LmerTest package for the linear mixed-effect model computation. We used a significance threshold of 0.05 with Bonferroni correction and p-values were adjusted using the false-discovery-rate method.

# Results

# **Patient Characteristics**

Between February 2015 and July 2018, we included 11 patients with ET previously operated for VIM-DBS (3F/8 M) and 10 patients with ET not previously operated for VIM-DBS (2F/8 M) that were not significantly different for age (p=0.24), disease duration (p=0.48) or tremor severity (p=0.95, Tables 1).

# Effects of Cerebellar tACS on ET Severity in the VIM-DBS Group

#### **Postural Tremor Amplitude**

In the active-tACS *vs* OFF-VIM-DBS condition, the postural tremor amplitude decreased significantly during and at 0, 20 and 40 min following stimulation (p=0.02, p=0.03, p=0.04 and p=0.04, respectively, Fig. 2, see supplementary video). There was no significant difference in postural tremor amplitude during active-tACS *vs* ON VIM-DBS condition (p=0.26, Fig. 2), nor during sham-tACS *vs* OFF VIM-DBS (p=0.26). Comparing the effects of active-tACS between arms, we found that the effects of active-tACS were only significant for the ipsilateral arm during and at 0 min following active-tACS relative to OFF VIM-DBS (p=0.02and p=0.02, respectively), and relative to sham-tACS (p=0.03), with no significant difference for the contralateral arm (Fig. 2, see supplementary video).

#### **Action Tremor Amplitude**

In the active-tACS vs OFF-VIM-DBS condition, finger displacement within the  $2\text{cm}^2$  area around the target during the 'nose-to-target' task was significantly lower at 0 and 20 min following stimulation (p=0.04 and p=0.008, respectively), with a trend during and at 40 min following stimulation (p=0.05). These effects were only significant for the ipsilateral arm during, at 0, 20 and 40 min following stimulation (p=0.002, p=0.045, p=0.005 and p=0.008, respectively, Fig. 2). Finger displacement of the ipsilateral arm was also significantly lower with active-tACS vs shamtACS (p=0.02, Fig. 2). Finger displacement was not significantly different between active tACS vs the ON VIM-DBS condition (p=0.32), and between sham-tACS vs the OFF VIM-DBS condition (p=0.26, Fig. 3).

The task duration was also significantly lower in the active-tACS vs OFF-VIM-DBS condition (p = 0.012,  $p < 10^{-4}$ ,  $p < 10^{-4}$ ,  $p < 10^{-4}$ ,  $p < 10^{-4}$ , respectively for during-stimulation and at 0, 20 and 40 min after, not shown), but only in the ipsilateral arm (p = 0.003,  $p < 10^{-4}$ ,  $p < 10^{-4}$ ,  $p < 10^{-4}$  ipsilaterally; contralaterally the respective values were p = 0.88, p = 0.05, p = 0.20, p = 0.20).

#### **Clinical ET Severity**

The FTM total score (blinded video scoring) was significantly lower during active-tACS and after 0, 20, 40 min *vs* both OFF VIM-DBS (p = 0.006, p = 0.010, p = 0.007, p = 0.02, respectively, Fig. 4) and sham tACS (p = 0.006,

Table 1 Baseline demographic and clinical characteristics of patients with Essential tremo	r
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	Patient	Sex, age (yrs)	Disease duration (yrs)	Time since surgery for VIM-DBS (months)	FTM total score (baseline) <sup>a</sup>	Medication (dosage/day)	tACS frequency (Hz)	VIM-DBS settings (contact/pulse width/amplitude)
ET with VIM- DBS	01	M, 61	10	48	41	-	180	1–2-C+/ 60 μs/3.8 V
	02	M, 73	18	26	35	Propanolol 100 mg	130	1–2+/120 µs/3.5 V
	03	M, 67	12	24	26	Topiramate 50 mg, Primidone 250 mg	130	1-C+/60 µs/3.7 V
	04	F, 47	27	15	11	Propanolol 80 mg, Gabapentin 300 mg	130	2-C+/60 µs/3.0 V
	05	M, 56	40	12	19	_	180	0–1+/90 µs/4 V
	06	M, 29	12	10	17	-	130	0-C+/60 μs us/3.0 V
	07	M, 69	49	30	36	_	130	2-C+/60 µs/2.8 V
	08	M, 69	22	93	18	_	180	1–0+/60 µs/4.0 V
	09	F, 41	26	12	28	Propanolol 40 mg, Topiramate 25 mg, Gabapentin 300 mg	130	0-C+/60 μs/2.8 V
	10	F, 72	16	55	26	-	130	1–2+/60 µs/3.6 V
	11	M, 44	34	36	42	Topiramate 50 mg	180	1-C+/60 µs/3.9 V
	Mean (SD)	57.1 (14.8)	24.2 (12.6)	32.8 (24.9)	27.2 (10.3)			
ET without VIM-DBS	12	M, 68	46	-	34	Propanolol 120 mg, Gabapentin 600 mg	130	
	13	M, 70	12	-	26	Propanolol 100 mg	130	
	14	M, 74	46	-	23	Topiramate 50 mg, Primidone 50 mg	130	
	15	M, 66	52	_	28	_	130	
	16	M, 52	12	-	21	Propanolol 60 mg	130	
	17	M, 71	17	-	19	Propanolol 40 mg	130	
	18	M, 71	42	-	29	Propanolol 40 mg	130	
	19	F, 71	15	-	23	Propanolol 100 mg	130	
	20	M, 61	53	-	32	Propanolol 80 mg	130	
	21	F, 42	12	_	33	-	130	
	Mean (SD)	64.6 (10.2)	30.7 (18.3)	-	26.8 (5.2)			

VIM-DBS: Ventral Intermediate Thalamic Deep Brain Stimulation, F: female, M: male

<sup>a</sup>OFF VIM-DBS for at least 3 h for patients with VIM DBS

	ON VIM-DBS <sup>a</sup>	Baseline (OFF VIM- DBS <sup>a</sup> )	Sham-tACS	Active-tACS	Change between baseline and Sham-tACS	Change between baseline and Active-tACS	Change between Active and Sham- tACS
FTM score A							
VIM-DBS group	5.6 (3.0)*	11.5 (.8)	11.3 (4.3)	8.1 (3.8)	-0.2 (3.0)	-3.4 (3.4)*	-3.2 (2.2)**
No-DBS group	_	11.2 (3.6)	9.5 (4.3)	8.1 (3.8)	-1.7 (2.8)*	-3.1 (2.1)*	-1.4 (1.6)
FTM score B							
VIM-DBS group	11.6 (5.2)	15.6 (6.4)	14.5 (8.1)	13.6 (6.9)	-1.0 (3.3)	-1.9 (2.5)	-0.9 (3.7)
No-DBS group	_	15.6 (3.4)	15.3 (3.3)	14.0 (3.9)	-0.3 (1.8)	-1.6 (2.1)	-1.3 (2.3)
FTM total score							
VIM-DBS group	17.2 (7.7)*	27.2 (10.3)	26.7 (10.1)	21.5 (9.0)	-0.5 (1.2)	-5.6 (5.1)*	-5.2 (3.6)**
No-DBS group	_	26.8 (5.3)	24.8 (5.9)	22.1 (5.3)	-2.0 (2.9)	-4.7 (3.2)*	-2.7 (3.2)**

Table 2 Effects of high-frequency VIM-DBS, active-tACS and sham-tACS of the cerebellum on clinical tremor severity in patients with Essential Tremor

Values are mean (SD); FTM=Fahn-Tolosa-Marin score

<sup>a</sup>for patients of the VIM-DBS group only

\*p < 0.05 relative to Baseline (OFF VIM-DBS) condition; \*\*p < 0.05 between Sham- and Active-tACS condition (linear mixed model)

p = 0.010, p = 0.007, p = 0.02, respectively, Fig. 4) conditions (Table 2). There was no significant difference in the FTM total score during active-tACS vs the ON VIM-DBS condition (p = 0.10, Fig. 4), nor during sham-tACS vs the OFF VIM-DBS condition (p = 1.0, Fig. 4).

The subscore A (tremor severity) was significantly lower during active tACS and after 0, 20 min vs OFF-VIM-DBS (p=0.003, p=0.005, p=0.045, respectively), and during activetACS vs sham-tACS (p=0.003, Fig. 4 and Table 2) conditions. The subscore A did not change significantly during shamtACS vs the baseline (p=0.90, Fig. 4). We found no significant changes in the subscore B (writing, drawing) with sham or active-tACS vs OFF VIM-DBS (all p values>0.35, Table 2).

# Effects of Cerebellar tACS on ET Severity in the No-DBS Group

#### **Postural Tremor Amplitude**

The postural tremor amplitude did not change significantly during and after active-tACS relative to both baseline (p=0.15) and sham-tACS conditions (p=0.15), and in the two arms (Fig. 2).

#### **Action Tremor Amplitude**

In the active-tACS vs baseline condition, finger displacement within the 2 cm<sup>2</sup> area around the target assessed during the 'nose-to-target' task was significantly lower during and 0, 20 and 40 min after stimulation, but on the ipsilateral side only ( $p < 10^{-4}$ , p = 0.02, p = 0.01, p = 0.04, for during, and 0, 20 and 40 min after active tACS, respectively, Fig. 3), with a trend in comparison to the sham-tACS (p = 0.10). We found no significant change in finger displacements with sham-tACS vs baseline condition, regardless of the arm considered (Fig. 3, p = 0.13 and p = 0.71 for ipsilateral and contralateral arms, respectively, Fig. 3).

The 'nose-to-target' task duration was also significantly lower during active-tACS and at 0, 20, 40 min following stimulation vs baseline ( $p < 10^{-4}$ ,  $p < 10^{-4}$ ,  $p < 10^{-4}$ , and  $p < 10^{-4}$ , respectively). This effect was significant for both sides (not shown), and relative to sham-tACS for the ipsilateral arm (p = 0.04, and p = 0.11 for the contralateral arm, not shown).

# **Clinical ET Severity**

The FTM total score was significantly lower during active tACS and at 0, 20, 40 min following stimulation *vs* baseline ( $p < 10^{-4}$ , p = 0.03, p = 0.018 and p = 0.003, respectively, Fig. 4), and during active-tACS *vs* sham-tACS (p = 0.045, Fig. 4) conditions (Table 2). During shamtACS *vs* baseline, there was no significant difference in the FTM total score (p = 0.06, Fig. 4). With respect to baseline, the subscore A was significantly lower during and at 0, 20, 40 min following active-tACS ( $p < 10^{-4}$ , p = 0.01, p = 0.02 and p = 0.02, respectively, Fig. 4) and also with sham-tACS (p = 0.02, Fig. 4 and Table 2). We found no significant changes for the subcore B with either sham or active-tACS *vs* baseline (all p values > 0.35, Table 2).



0

Active-tACS

Sham-tACS

Fig. 2 Effects of active- and sham-tACS at high-frequency on postural tremor. Box plots for postural tremor amplitude as measured by the sum of the displacements of the two arm markers (left panels) during posture holding in ET patients with VIM-DBS (upper panels),

Baseline-OFF-DBS

#### Safety and Tolerance of the Procedure

No adverse or serious adverse event occurred during the trial. Both sham and active-tACS were generally welltolerated regardless of the group. Two patients with VIM-DBS described mild transient paraesthesia of the ipsilateral arm occurring at current onset (during both the sham and active tACS conditions), and one patient in the control group described moderate transient paraesthesia under the skull electrode during both sham- and active tACS conditions.

# Discussion

VIM-DBS Group

No-DBS Group

0

ON-VIM-DBS

In this proof-of-concept double-blind sham-controlled study, we assessed for the first time the effects of high-frequency cerebellar tACS on ET patients treated with VIM-DBS; and in ET patients with similar tremor severity with no VIM-DBS, taken as controls. Using objective measurements

and No-DBS patient group (lower panels). Postural tremor amplitude for the contralateral (middle panels) and ipsilateral (right panels) arms. \*P < 0.05 relative to baseline condition; †P < 0.05 relative to sham-tACS

40min post-tACS

Omin post-tACS 20min post-tACS

(kinetic measures using VICON® 3D motion capture) and blind assessments of the FTM scores by independent examiners, we found a significant improvement in kinetic and clinical measures with active-cerebellar tACS. The effects were comparable to those of VIM-DBS for managing posture tremor amplitude and reducing clinical severity, and only present in the ipsilateral arm. In the control group of ET patients not previously treated with VIM-DBS, we also found a significant improvement in the 'nose-to-target' task parameters in the ipsilateral arm, and in tremor clinical severity after active-cerebellar tACS.

Interestingly, we observed variable effects across patients of both groups, with in addition, an absence of decreased tremor severity (total FTM score) with active-tACS in 4 out of our 21 patients (19%), and no change in writing tremor for about one third of patients (score B). Such interindividual variability in cerebellar NIBS has been reported in previous NIBS trials [26], also with individual phase-locked tACS [33]. These variable effects of active-tACS could be



**Fig. 3** Effects of active- and sham-tACS at high-frequency on action tremor. Box plots for action tremor amplitude as measured by the sum of the displacements of the finger in the 2cm2 area around the target, for the two arms (left graphs), the contralateral (middle panels)

due to differences in clinical characteristics, such as disease duration or age [26], features of the tremor movement [33], electrode–skin capacitance, or individual cerebellar-cortex anatomical and functional connectivity at baseline [9, 10].

The physiological effects of non-invasive brain stimulation of the cerebellar cortex are not fully understood. Here, we hypothesised that high frequency tACS would modify cerebellar cortex excitability leading to subsequent changes in the pathological oscillatory activity within the CTC network. The fact that we found similar effects between VIM-DBS and active cerebellar tACS, applied at the same stimulation frequency, would favour this hypothesis. In ET patients, a possible progressive neurodegeneration of Purkinje cells has been reported with reduced activity of these cells [2, 41], leading to a deficit in GABAergic inputs to the deep cerebellar nuclei neurons, and pathological oscillatory activities within the CTC network activity [7]. Previous studies demonstrated an increased theta-alpha band activity and high-frequency oscillations in the VIM of ET

and ipsilateral (right panels) arms, during the 'nose-to-target' task in ET patients with VIM-DBS (upper panel), and No-DBS patient group (lower panel). \*P < 0.05 relative to baseline condition; †P < 0.05 relative to sham-tACS

patients [37, 42, 43], with, in addition, an abnormal thalamocortical low-frequency oscillation phase-amplitude coupling [44, 45], a mechanism mediating movement execution [46]. With high-frequency VIM-DBS, tremor suppression was found to be correlated to decreased thalamic neuronal firing and low-frequency oscillations [47-49], and modulation of both olivocerebellar and thalamocortical circuits with activation of the contralateral cerebellar cortex, deep cerebellar nuclei and motor cortex [17, 50]. These data suggests that VIM-DBS could lead to a partial reestablishment of CTC functioning, and act as a filter to uncouple thalamocortical from cortico-spinal reflex loops [48]. Applied at the cerebellar cortex, 5 Hz tACS has been shown to increase cerebello-cortex inhibition in healthy subjects [31], and low-frequency phase-locked cerebellar tACS has also been reported to decrease tremor amplitude in ET patients [33]. Conversely, cathodal cerebellar tDCS, thought to inhibit cerebellar cortical activity, does not significantly reduce tremor [24]. Lastly, when applied over the cerebellum, 300 Hz tACS



Fig. 4 Effects of active- and sham-tACS at high frequency on clinical tremor severity. Box plots for the severity of tremor as measured by the FTM total and by the FTM subscore A in ET patients with

has been shown to increase cerebellum-brain inhibition [32], and 140 Hz tACS applied over M1 to increase cortical excitability [30]. Finally, all these previous studies and our results suggest that high frequency tACS applied over the cerebellum may increase Purkinje cell excitability with, in consequence, a modulation of the CTC network oscillatory activity and tremor reduction.

This study has some limitations. First, we cannot fully exclude the possibility that our findings on VIM-DBS ET patients resulted from an artifact due to the setup used with the cerebellar tACS, since current may have flowed through the DBS electrode. However, the facts that kinetic and functional improvements persisted for up to 40 min after current offset, were also found in non-operated ET patients, and more pronounced for the arm ipsilateral to the stimulated cerebellum do not favour this hypothesis. Second, we had no direct evidence that allowed us to determine which part of the cerebellum could be affected by the tACS nor its physiological effects on cerebellar activity. In our protocol, we positioned stimulating electrodes as recommended

VIM-DBS (upper panels) and No-DBS patient group (lower panels). \*P < 0.05 relative to baseline condition;  $\dagger P < 0.05$  relative to sham-tACS

in previous studies using DC stimulation [51, 52] and the effects observed across patients led us to suppose that the posterior cerebellum was actively modulated. Third, although a strength of the study was the sham-controlled design, sham-tACS was always applied prior to activetACS which may have primed the effects of active-tACS, and we cannot totally rule out the possibility that patients felt some differences between sham-tACS and active-tACS without mentioning it. We chose this experimental design for the comfort of the patients as the anti-tremor drugs were stopped 7 days preceding the assessment for all patients and stimulation was turned OFF for several hours for VIM-DBS patients, with a return to the pre-operative tremor disability. In addition, our primary outcome was the comparison of active-tACS vs VIM-DBS, and not per se sham vs activetACS. We also observed some significant changes in kinetics parameters in our control ET patients group with sham-tACS suggesting a possible placebo effect in these patients, as has been previously reported in ET patients using NIBS [28, 29]. However, the fact that we found significant differences in blinded clinical scores between active and sham-tACS with better effects for the ipsilateral arm, and no effect of sham tACS in the VIM-DBS group, may indicate that active tACS is indeed more efficient than sham-tACS to decrease tremor severity [29].

# Conclusions

Overall, this proof-of-concept study supports the fact that high-frequency cerebellar tACS could modulate the CTC network, with objective changes in the postural and kinetic characteristics of essential tremor. In addition, it demonstrates the safety and potential benefits of high-frequency cerebellar tACS for ET patients. Further studies are needed to assess the value of repeated sessions for long-lasting effects, determine the optimal stimulation settings. This needs to be done in relation to individual tremor characteristics [33] and anatomical and functional cerebellar-cortex connectivity [9, 23], before we can propose this technique for patients with tremor insufficiently controlled by medical treatment.

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**Data Availability** All relevant data are within the article. Requests for anonymized data should be sent to M.L. Welter at the Paris Brain Institute, 75013 Paris, France.

# References

- Louis ED, Ottman R, Hauser WA. How common is the most common adult movement disorder? estimates of the prevalence of essential tremor throughout the world. Mov Disord. 1998;13:5– 10. https://doi.org/10.1002/mds.870130105.
- Louis ED, Faust PL, Vonsattel JP, et al. Neuropathological changes in essential tremor: 33 cases compared with 21 controls. Brain. 2007;130:3297–307. https://doi.org/10.1093/brain/ awm266.
- 3. Deuschl G, Elble RJ. The pathophysiology of essential tremor. Neurology. 2000;54:S14-20.
- Placantonakis DG, Bukovsky AA, Zeng XH, et al. Fundamental role of inferior olive connexin 36 in muscle coherence during tremor. Proc Natl Acad Sci U S A. 2004;101:7164–9. https://doi. org/10.1073/pnas.04003221010400322101[pii].

- Pedrosa DJ, Reck C, Florin E, et al. Essential tremor and tremor in Parkinson's disease are associated with distinct "tremor clusters" in the ventral thalamus. Exp Neurol. 2012;237:435–43. https:// doi.org/10.1016/j.expneurol.2012.07.002.
- Gallea C, Popa T, García-Lorenzo D, et al. Intrinsic signature of essential tremor in the cerebello-frontal network. Brain. 2015;138:2920–33. https://doi.org/10.1093/brain/awv171.
- Filip P, Lungu OV, Manto M-U, et al. Linking essential tremor to the cerebellum: physiological evidence. Cerebellum. 2016;15:774–80. https://doi.org/10.1007/s12311-015-0740-2.
- Fang W, Chen H, Wang H, et al. Essential tremor is associated with disruption of functional connectivity in the ventral intermediate Nucleus-Motor Cortex–Cerebellum circuit. Hum Brain Mapp. 2016;37:165–78. https://doi.org/10.1002/hbm.23024.
- Hanajima R, Tsutsumi R, Shirota Y, et al. Cerebellar dysfunction in essential tremor. Mov Disord. 2016;31:1230–4. https:// doi.org/10.1002/mds.26629.
- Pinto AD, Lang AE, Chen R. The cerebellothalamocortical pathway in essential tremor. Neurology. 2003;60:1985–7. https://doi.org/10.1212/01.wnl.0000065890.75790.29.
- Deuschl G, Raethjen J, Hellriegel H, et al. Treatment of patients with essential tremor. Lancet Neurol. 2011;10:148–61. https:// doi.org/10.1016/S1474-4422(10)70322-7.
- 12. Kumar R, Lozano AM, Sime E, et al. Long-term follow-up of thalamic deep brain stimulation for essential and parkinsonian tremor. Neurology. 2003;61:1601–4.
- 13. Bardinet E, Belaid H, Grabli D, et al. Thalamic stimulation for tremor: can target determination be improved? Mov Disord. 2011;26:307–12. https://doi.org/10.1002/mds.23448.
- Limousin P, Speelman JD, Gielen F, et al. Multicentre European study of thalamic stimulation in parkinsonian and essential tremor. J Neurol Neurosurg Psychiatry. 1999;66:289–96.
- Schuurman PR, Bosch DA, Bossuyt PM, et al. A comparison of continuous thalamic stimulation and thalamotomy for suppression of severe tremor. N Engl J Med. 2000;342:461–8. https:// doi.org/10.1056/NEJM200002173420703.
- Rehncrona S, Johnels B, Widner H, et al. Long-term efficacy of thalamic deep brain stimulation for tremor: double-blind assessments. Mov Disord. 2003;18:163–70.
- Gibson WS, Jo HJ, Testini P, et al. Functional correlates of the therapeutic and adverse effects evoked by thalamic stimulation for essential tremor. Brain. 2016;139:2198–210. https://doi.org/ 10.1093/brain/aww145.
- Fasano A, Herzog J, Raethjen J, et al. Gait ataxia in essential tremor is differentially modulated by thalamic stimulation. Brain. 2010;133:3635–48. https://doi.org/10.1093/brain/awq267.
- Iorio-Morin C, Yamamoto K, Sarica C, et al. Bilateral focused ultrasound thalamotomy for essential tremor (BEST-FUS Phase 2 Trial). Mov Disord. 2021;36:2653–62. https://doi.org/10.1002/ mds.28716.
- Abe K, Horisawa S, Yamaguchi T, et al. Focused ultrasound thalamotomy for refractory essential tremor: A Japanese multicenter single-arm study. Neurosurgery. 2021;88:751–7. https://doi.org/ 10.1093/neuros/nyaa536.
- Kang N, Cauraugh JH. Does non-invasive brain stimulation reduce essential tremor? A systematic review and meta-analysis. PLoS One. 2017;12:e0185462. https://doi.org/10.1371/journal.pone.0185462.
- Latorre A, Rocchi L, Berardelli A, et al. The use of transcranial magnetic stimulation as a treatment for movement disorders: A critical review. Mov Disord. 2019;34:769–82. https://doi.org/10. 1002/mds.27705.
- Popa T, Russo M, Vidailhet M, et al. Cerebellar rTMS stimulation may induce prolonged clinical benefits in essential tremor, and subjacent changes in functional connectivity: an open label trial. Brain Stimul. 2013;6:175–9. https://doi.org/10.1016/j.brs.2012. 04.009.

- Gironell A, Martinez-Horta S, Aguilar S, et al. Transcranial direct current stimulation of the cerebellum in essential tremor: a controlled study. Brain Stimul. 2014;7:491–2. https://doi.org/10. 1016/j.brs.2014.02.001.
- Gironell A, Kulisevsky J, Lorenzo J, et al. Transcranial magnetic stimulation of the cerebellum in essential tremor: a controlled study. Arch Neurol. 2002;59:413–7. https://doi.org/10.1001/ archneur.59.3.413.
- Maas RPPWM, Helmich RCG, van de Warrenburg BPC. The role of the cerebellum in degenerative ataxias and essential tremor: Insights from noninvasive modulation of cerebellar activity. Mov Disord. 2020;35:215–27. https://doi.org/10.1002/mds.27919.
- Bologna M, Rocchi L, Leodori G, et al. Cerebellar continuous theta burst stimulation in essential tremor. Cerebellum. 2015;14:133–41. https://doi.org/10.1007/s12311-014-0621-0.
- Olfati N, Shoeibi A, Abdollahian E, et al. Cerebellar repetitive transcranial magnetic stimulation (rTMS) for essential tremor: A double-blind, sham-controlled, crossover, add-on clinical trial. Brain Stimul. 2020;13:190–6. https://doi.org/10.1016/j.brs.2019. 10.003.
- Shin H-W, Hallett M, Sohn YH. Cerebellar repetitive transcranial magnetic stimulation for patients with essential tremor. Parkinsonism Relat Disord. 2019;64:304–7. https://doi.org/10.1016/j.parkreldis. 2019.03.019.
- Moliadze V, Antal A, Paulus W. Boosting brain excitability by transcranial high frequency stimulation in the ripple range. J Physiol. 2010;588:4891–904. https://doi.org/10.1113/jphysiol. 2010.196998.
- Spampinato D, Avci E, Rothwell J, et al. Frequency-dependent modulation of cerebellar excitability during the application of non-invasive alternating current stimulation. Brain Stimul. 2021;14:277–83. https://doi.org/10.1016/j.brs.2021.01.007.
- Naro A, Leo A, Russo M, et al. Does transcranial alternating current stimulation induce cerebellum plasticity? Feasibility, safety and efficacy of a novel electrophysiological approach. Brain Stimul. 2016;9:388–95. https://doi.org/10.1016/j.brs.2016.02.005.
- Schreglmann SR, Wang D, Peach RL, et al. Non-invasive suppression of essential tremor via phase-locked disruption of its temporal coherence. Nat Commun. 2021;12:363. https://doi.org/ 10.1038/s41467-020-20581-7.
- Nieuwhof F, Toni I, Buijink AWG, et al. Phase-locked transcranial electrical brain stimulation for tremor suppression in dystonic tremor syndromes. Clin Neurophysiol. 2022;140:239–50. https:// doi.org/10.1016/j.clinph.2022.03.020.
- De Zeeuw CI, Hoebeek FE, Schonewille M. Causes and consequences of oscillations in the cerebellar cortex. Neuron. 2008;58:655–8. https://doi.org/10.1016/j.neuron.2008.05.019.
- de Solages C, Szapiro G, Brunel N, et al. High-frequency organization and synchrony of activity in the purkinje cell layer of the cerebellum. Neuron. 2008;58:775–88. https://doi.org/10.1016/j. neuron.2008.05.008.
- Schnitzler S, Hartmann CJ, Groiss SJ, et al. Occurrence of thalamic high frequency oscillations in patients with different tremor syndromes. Clin Neurophysiol. 2018;129:959–66. https://doi.org/ 10.1016/j.clinph.2018.01.073.
- Bhatia KP, Bain P, Bajaj N, et al. Consensus Statement on the classification of tremors. from the task force on tremor of the International Parkinson and Movement Disorder Society. Mov Disord. 2018;33:75–87. https://doi.org/10.1002/mds.27121.
- Fahn S, Tolosa E, Marin C. Clinical rating scale for tremor. In: Jankovic J, Tolosa E, editors. Parkinson's disease and movement disorders. 2nd ed. Baltimore: Williams and Wilkins; 1993. p. 271–80.

- Herzog R, Berger TM, Pauly MG, et al. Cerebellar transcranial current stimulation - An intraindividual comparison of different techniques. Front Neurosci. 2022;16:987472. https://doi.org/10. 3389/fnins.2022.987472.
- Louis ED. From neurons to neuron neighborhoods: the rewiring of the cerebellar cortex in essential tremor. Cerebellum. 2014;13:501–12. https://doi.org/10.1007/s12311-013-0545-0.
- Brodkey JA, Tasker RR, Hamani C, et al. Tremor cells in the human thalamus: differences among neurological disorders. J Neurosurg. 2004;101:43–7. https://doi.org/10.3171/jns.2004. 101.1.0043.
- Kane A, Hutchison WD, Hodaie M, et al. Enhanced synchronization of thalamic theta band local field potentials in patients with essential tremor. Exp Neurol. 2009;217:171–6. https://doi.org/10. 1016/j.expneurol.2009.02.005.
- Pedrosa DJ, Quatuor E-L, Reck C, et al. Thalamomuscular coherence in essential tremor: hen or egg in the emergence of tremor? J Neurosci. 2014;34:14475–83. https://doi.org/10.1523/JNEUROSCI.0087-14. 2014.
- Kondylis ED, Randazzo MJ, Alhourani A, et al. Movement-related dynamics of cortical oscillations in Parkinson's disease and essential tremor. Brain. 2016;139:2211–23. https://doi.org/10.1093/ brain/aww144.
- Opri E, Cernera S, Okun MS, et al. The functional role of thalamocortical coupling in the human motor network. J Neurosci. 2019;39:8124–34. https://doi.org/10.1523/JNEUROSCI.1153-19. 2019.
- Opri E, Cernera S, Molina R, et al. Chronic embedded corticothalamic closed-loop deep brain stimulation for the treatment of essential tremor. Sci Transl Med. 2020;12:eaay7680. https://doi. org/10.1126/scitranslmed.aay7680.
- Milosevic L, Kalia SK, Hodaie M, et al. Physiological mechanisms of thalamic ventral intermediate nucleus stimulation for tremor suppression. Brain. 2018;141:2142–55. https://doi.org/10. 1093/brain/awy139.
- Ferleger BI, Houston B, Thompson MC, et al. Fully implanted adaptive deep brain stimulation in freely moving essential tremor patients. J Neural Eng. 2020;17:056026. https://doi.org/10.1088/ 1741-2552/abb416.
- Molnar GF, Sailer A, Gunraj CA, et al. Changes in cortical excitability with thalamic deep brain stimulation. Neurology. 2005;64:1913–9. https://doi.org/10.1212/01.WNL.0000163985. 89444.DD.
- Parazzini M, Rossi E, Rossi L, et al. Evaluation of the current density in the brainstem during transcranial direct current stimulation with extra-cephalic reference electrode. Clin Neurophysiol. 2013;124:1039–40. https://doi.org/10.1016/j.clinph.2012.09.021.
- Parazzini M, Rossi E, Ferrucci R, et al. Modelling the electric field and the current density generated by cerebellar transcranial DC stimulation in humans. Clin Neurophysiol. 2014;125:577–84. https://doi.org/10.1016/j.clinph.2013.09.039.

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