

Original Research

Identifying Consistent Metrics from the Force-Time Curve of the Countermovement Jump in Combat Fighters and Physically Active Men.

ALEXANDRE R. P. FERREIRA†1, VICTOR O. C. MACEDO†1, DANIEL BOULLOSA‡2, and AMILTON VIEIRA‡1

¹College of Physical Education, University of Brasília, Brasília, DF, BRAZIL; 2Integrated Health Institute, Federal University of Mato Grosso do Sul, Campo Grande, MT, BRAZIL

*Denotes undergraduate student author, †Denotes graduate student author, ‡Denotes professional author

ABSTRACT

International Journal of Exercise Science 16(4): 1038-1051, 2023. We investigated the consistency of metrics obtained from the unweighting, braking, propulsive, and landing phases of the countermovement (CMJ) force-time curve in combat fighters and physically active men. Combat fighters (n=21) and physically actives (n=21) were tested for three days (2-7 days apart). Participants performed four maximal CMJ separated by 1-min for between-day comparisons. From force-time recording, the consistency of 16 CMJ metrics (peak and mean ground reaction forces (GRF), net impulse, and duration from each phase) was investigated using the intraclass correlation coefficient (ICC) and typical error (CVTE). We considered as "consistent" those metrics showing no systematic differences, ICC ≥ 0.75, and CV_{TE} ≤ 10%. We further compared the CV_{TE} between groups and pairs of trials (days). Participants demonstrated more consistency in the braking and propulsive phases, while the unweighting phase did not show any consistent metric. There was no evidence of a learning effect (systematic changes), but analysis appointed more consistency on days 2-3 than on days 1-2 (18 metrics presented lower CV_{TE} while 11 presented higher). We identified braking and propulsive GRF (peak and mean) and propulsive impulse as consistent metrics for combat fighters, while only propulsive impulse for physically actives. The between-group analyses showed that 24 comparisons favored the combat fighters against only five favoring the physically actives. In conclusion, forcetime metrics related to jumping strategy, like phase duration, are less consistent than those related to driven forces and jump output, probably because participants changed their jump strategy during testing days.

KEY WORDS: Exercise test, vertical jump testing, force platform, muscular fitness, reliability

INTRODUCTION

The countermovement jump (CMJ) is primarily used to assess lower-body neuromuscular function (20,38,56,62,63). The CMJ testing has been applied to an extensive range of individuals, from sedentary to elite athletes of all age groups (35), including individuals with musculoskeletal disorders (6) and obesity (46). The CMJ is popular because it is practical and non-fatiguing, can be quickly performed, and provides valuable information on neuromuscular adaptations induced by training regimens and exercise-induced neuromuscular fatigue

(4,7,31,54). Furthermore, researchers have pointed out that the CMJ allows for discrimination between athletes with distinct competitive levels (11,19,20,56,63) and training backgrounds (24,26,30,45,58,63).

Force platforms are considered the gold standard device for CMJ testing (9,29). A force platform allows a comprehensive assessment of the constituent phases of the CMJ, providing metrics expressing the jump output (e.g., net propulsive impulse), the driven forces of the jump (e.g., peak and mean ground reaction forces), and movement strategy (e.g., phase durations). Although there are arguments that force platforms are not accessible due to their high cost and lack of portability, the technology advance has allowed the commercialization of low-cost force platforms (27). In addition, recent publications have provided inexpensive software for CMJ force-time curve analysis (5), suggesting that the use of force platforms will likely grow.

To improve understanding and application of the CMJ data, researchers (5,39) have proposed that force-time data from CMJ testing should be segmented in phases (e.g., unweighing, braking, propulsion, and landing). Indeed, several studies have been published applying this method for CMJ phase segmentation (2,10,13,36,55). However, the segmentation of the CMJ in phases requires multiple calculations (e.g., differentiation, integration) and the identification of thresholds (e.g., integration start and take-off), which may increase the chance of computational error. In addition, errors can also arise from participants (e.g., learning, motivation, fatigue). Each potential source of error (computational and biological) may substantially affect the measurement's quality. Whether metrics deriving from CMJ phases are consistent across testing sessions is still being determined.

It is established that the jump height (estimated from flight time or takeoff velocity) and ground reaction forces produced during a CMJ vary little from day to day (52). However, this may not be the case for metrics related to jumping strategy since an individual can change the movement strategy (e.g., applying less force for longer duration) while keeping consistent the jump height $(12,37)$.

The usefulness of the CMJ to assess neuromuscular function, especially to monitor exerciseinduced small changes in performance (e.g., pre- vs. post-training), depends on data consistency. Consistent metrics increase the likelihood of observing true changes in performance (15). The typical error (expressed as coefficient of variation - CV_{TE}) and intraclass coefficient of correlation (ICC) are often evaluated together to determine consistency. It is generally accepted that a metric is consistent if the ICC \geq 0.75 and the CV_{TE} \leq 10% (1,22,57). However, these scores are estimates and should be interpreted considering the 95% confidence interval (22).

Although studies have been published reporting consistency of metrics obtained from key phases of the CMJ, mainly from the propulsive phase (aka concentric phase) (12,14,28,32,40– 42,44,48,51,61), some information is still missing. For example, Warr et al. (61) and Heishman et al. (14) recently performed a reliability study on male athletes, but no information was provided about the landing phase of the CMJ. Others have not fully described data consistency since their analysis was only part of the main study (40,51) or have been focused on a few propulsive phase metrics (12,42,44,48). Furthermore, some have performed intraday analysis (28,32,41), which has limited application for those interested in monitoring exercise-induced changes in performance.

This study aimed to investigate the consistency of metrics obtained from the unweighting, braking, propulsive, and landing phases of the CMJ in combat fighters and physically active men. It is interesting to know if the training background would play a role in metrics consistency since it is recognized that athletes may present a greater movement consistency, which would reflect lower CV_{TE} (60). For this reason, we have included a group of physically active men serving as a control group. We hypothesized that (I) net propulsive impulse and ground reaction forces would be more consistent than metrics related to movement strategy (phase duration). (II) Combat fighters would be more consistent in their performance than physically actives, and (III) adding a third testing day would improve consistency.

METHODS

Participants

The sample size was estimated a priori (G*Power, version 3.1.9.6, Germany), under the assumption that combat fighters would exhibit greater propulsive impulse during the CMJ than physically active men (Cohen's *d* = 1.19 (58)) as well as 0.05 of alpha error, 0.90 of power. These assumptions indicated that a sample size of at least 32 individuals would reach sufficient power to avoid type II error. Combat fighters ($n = 21$) and physically active men ($n = 21$) participated in this study. The combat fighters (tier 2: trained/developmental (34)) had to be engaged in any combat sport for a minimum of three days per week for at least two years. This sample included athletes from karate (n = 5), wrestling (n = 2), taekwondo (n = 3), Brazilian jiu-jitsu (n = 8), and judo (n = 2). The sample of physically active (tier 1: recreationally active (34)) was composed of men engaged in at least 150-min moderate-intensity activities and/or 75-min of vigorous activities per week (e.g., resistance training, walking, jogging, running). Fourteen participants were classified as "very active", while seven as "active" (8). To avoid confounding, we did not included participants reporting less than the minimum criteria to be part of the group of combat fighters (e.g., engaged in combat sports for less than 2 yrs.) in the group of physically actives. We instructed the participants to avoid any vigorous activity 48 hours before testing. They reported being free from any chronic disease or injury that could compromise jump performance and were informed about the risks and benefits of their participation before signing informed consent. This study was approved by the UDF – University Center Ethical Committee (number 2.878.364). This research was carried out fully in accordance to the ethical standards of the International Journal of Exercise Science (43).

Protocol

The participants were tested on three separate days (2 to 7 days apart) at approximately the same time of day (±1 hour), and a single investigator performed all testing procedures. A video of the CMJ protocol was viewed prior to testing. During the first testing day, body mass and stature were taken, and physical activity and health questionnaires were filled out. Before all

testing sessions, participants performed a standardized warm-up protocol consisting of 2 sets of overloaded (50% of body mass) back squats and five CMJs with progressive effort (20, 40, 60, 80, and 100% of perceived effort). They performed just one jump at each perceived effort, including a jumping maximally to increase the readiness for testing.

Variable	Combat Fighters	Physically Active	p-value
Age (years)	25 ± 5	22 ± 2	0.10
Body mass (kg)	80 ± 10	77 ± 17	0.53
Stature (cm)	177 ± 5	176 ± 9	0.68
BMI (kg m-2)	25 ± 3	25 ± 4	0.48
CMJ height (cm)	44 ± 5	$39 \pm 7*$	0.02

Table 1. Participant's characteristics.

* Less than Combat Fighters. BMI, body mass index; CMJ, countermovement jump.

CMJ testing was performed on a force platform with a sampling rate set at 1000 Hz (Accupower Portable Force Plate, AMTI, Watertown, MA, USA). Participants stood still for approximately three seconds with hands akimbo and then performed their maximum effort to jump following the command "3, 2, 1, jump". We instructed the participants to jump "as fast and as high as possible" to minimize the duration of the transition between the descending and ascending part of the movement and to land with feet extended (ankle plantarflexed). The countermovement depth was self-selected, and they were instructed to take-off and land with the same body posture (i.e., hands akimbo while keeping their hip, knee, and ankle joint fully extended). On landing, participants were instructed to absorb the forces by flexing their hips, knees, and ankles achieving your preferred squat depth. They also were instructed "to land softly, without noise". Participants performed four valid CMJs with maximum effort separated by a 1-min rest interval (21,52). However, ten participants from both groups were required to perform from one to three more attempts because the jump height difference exceeded 1 cm.

Figure 1 depicts the 16 CMJ metrics (i.e., 4 metrics: peak and mean ground reaction forces, net impulse, and duration from 4 CMJ phases: unweighting, braking, propulsive, and landing). The metrics were extracted from vertical ground reaction forces (GRF) using a custom-made Python script based on previous recommendations (39). The signal was visually inspected and filtered using a fourth-order low pass Butterworth filter with a cutoff frequency of 30 Hz. This low pass threshold was determined based on previous studies successfully applying this cutoff frequency (50,53,59). The offset was adjusted by subtracting the mean residual force measured during the flight phase of the jump, guaranteeing a zeroed measure. Bodyweight and mass were measured during the one second period of the weighing phase with a lower standard deviation (SD). The start of the CMJ was identified as the instant when the force signal reached the threshold of $5 \times$ SD of the bodyweight minus 30 ms (49). Acceleration was obtained by dividing the net forcetime signal by the participant's body mass. Then velocity and displacement were calculated by numerically integrating acceleration-time and velocity-time using the trapezoidal rule. The unweighting phase was delimited from the onset of countermovement until the instant when velocity reached a minimum value. The braking phase was delimited from the end of the

unweighting phase until displacement reached a minimum value. The propulsive phase was delimited from the end of the braking phase until take-off. Take-off and landing were identified when the force signal reached the threshold of $5 \times SD$ of the flight force (platform unloaded) (47). Flight force was sampled from the middle portion of the flight interval with half of its duration. The end of the landing phase was identified when acceleration first crossed zero or at its minimum (when the signal did not reach zero).

Figure 1. Typical vertical ground reaction force-time (vGRF) recording from countermovement jump (CMJ). A-D are depicting the key phases of the CMJ: A) unweighting; B) braking; C) propulsive; D) landing**.**

Statistical Analysis

Data distribution was inspected, and outliers were removed $(1.2 \times SD)$ below or above the average for within- or 2 × SD for between-participants). At least two valid data from each metric (variable) were averaged and further analyzed; otherwise, the participant was excluded from that specific analysis. Table 2 describes the number of participants analyzed in each group and day. The Wilcoxon test with Bonferroni correction was used for test-retest comparisons utilizing The Statistical Package for the Social Sciences (SPSS version 23.0). Significant differences (*p* ≤ 0.017) were interpreted using Hedge's g effect size (ES), with the threshold of < 0.2 for trivial; 0.2 – 0.6 for small; 0.6 – 1.2 for moderate; and 1.2 – 2.0 for large (17). The intraclass correlation coefficient (ICC) and typical error of measurement as a coefficient of variation (CV_{TE}) were calculated using a custom-made spreadsheet (16). CV_{TE} were interpreted as very large ($> 15\%$), large (10 to 15%), moderate (5 to 10%) and low (< 5%) (57), while ICC were interpreted as poor (< 0.50), moderate (0.50 to 0.75), good (0.751 to 0.90) and excellent (> 0.90) (22). We further compared the magnitude of the CV_{TE} between groups (CV ratio = CV combat fighters ÷ CV physically active) and days (CV ratio = CV days 2 and $3 \div$ CV days 1 and 2). CV ratios exceeding

0.87 or 1.15 indicated a substantial difference (48,57). We considered as "consistent" those metrics showing ES < 0.2, ICC \geq 0.75, and CV \leq 10%, including their 95% confidence intervals, meaning that there was a 95% chance that the true score was \geq 0.75 and \leq 10%. These conditions must be met on all three testing days.

RESULTS

Tables 2 and 3 show results from force-time metrics and the ICC and CV_{TE} obtained during CMJ in combat fighters and physically active men, respectively. Combat fighters demonstrated consistent values of peak and mean GRF from braking and propulsive phases and propulsive impulse, while physically actives only demonstrated it for the landing impulse. The unweighting was the single CMJ phase not showing any consistent metric. No systematic differences were observed between testing days (i.e., learning effect), except the GRF_{PEAK} was lesser on day 2 than on day 1 in the unweighting phase of the combat fighters. Overall, the between-day comparisons using the CV ratio appointed more consistency on days 2 and 3 than on days 1 and 2 (i.e., 18 metrics presented lower CV_{TE} while 11 presented higher). The betweengroup comparisons showed that combat fighters demonstrated a superior number of metrics presenting lower CV_{TE} than physically actives (i.e., 24 comparisons favoring combat fighters against five for physically actives).

Metric	Group	Day 1	Day 2	Day 3
Unweighting phase				
Duration (ms)	PA	298 (221, 375) ^[21]	289 (241, 323)[18]	287 (207, 365) ^[21]
	CF	305 (262, 340) ^[21]	290 (255, 326) ^[20]	290 (252, 316) ^[20]
$\mathrm{GRF_{PEAK}}$ (N)	PA	199 (28, 395)[20]	155 (7, 315)[19]	185 (41, 394) ^[21]
	CF	114 (58, 204)[17]	83 (23, 138) ^{[18] a}	66 (30, 129)[18]
$\mathrm{GRF}_{\mathrm{MEAN}}$ (N)	PA	468 (302, 660)[19]	450 (236, 635)[21]	424 (233, 578)[20]
	CF	410 (295, 505) ^[21]	392 (307, 483)[19]	390 (268, 495)[21]
Impulse (Ns)	PA	93 (48, 119)[19]	85 (59, 115)[19]	89 (56, 125)[20]
	CF	112 (90, 136) ^[21]	112 (88, 140) ^[20]	116 (91, 140) ^[21]
Braking phase				
Duration (ms)	PA	115 (98, 204) ^[21]	160 (98, 213)[21]	161 (98, 222)[20]
	CF	168 (138, 192)[19]	160 (130, 193) ^[20]	167 (130, 205) ^[20]
$\rm GRF_{PEAK}$ (N)	PA	1754 (1204, 2243)[19]	1780 (1276, 2342) ^[20]	1759 (1164, 2310) ^[20]
	CF	1913 (1503, 2318)[21]	1951 (1470, 2417)[21]	1931 (1489, 2287)[21]
$GRFMEAN$ (N)	PA	1285 (935, 1661) ^[20]	1297 (929, 1632) ^[20]	1273 (846, 1619) ^[20]
	CF	1415 (1160, 1724) ^[21]	1461 (1150, 1837) ^[21]	1448 (1185, 1766) ^[21]
Impulse (Ns)	PA	80 (43, 116) ^[20]	83 (57, 120) ^[20]	85 (49, 121)[20]
	CF	108 (86, 141)[21]	108 (82, 131)[20]	110 (87, 134) ^[21]
Propulsive phase				
Duration (ms)	PA	259 (200, 330) ^[20]	256 (160, 330) ^[21]	261 (170, 340) ^[21]
	CF	296 (241, 372)[21]	292 (252, 345)[19]	300 (277, 319)[17]
$\mathrm{GRF_{PEAK}}$ (N) PA		1859 (1241, 2411)[19]	1887 (1343, 2438)[19]	1901 (1309, 2455) ^[20]

Table 2. Force-time metrics obtained during countermovement jump in combat fighters (CF) and physically active men (PA). Data are presented as mean (95% confidence intervals), and [*n*] describes the number of participants analyzed.

a less than day 1 ($p = .006$; ES = 0.88).

Table 3. Intraclass Correlation Coefficient (ICC) and Coefficient of Variation (CV_{TE}) of force-time metrics obtained during countermovement jump in combat fighters (CF) and physically active men (PA). Data are presented as mean (95% confidence intervals).

Metric	Group	Days 1 and 2		Days 2 and 3	
		CV_TE	ICC	CV _{TE}	ICC
Unweighting phase					
Duration (ms)	PA	10.0 (7.5, 15.4) $*$	0.33 (-0.18, 0.69)	12.3(9.1, 19.0)	0.19 (-0.32 , 0.59)
	CF	$6.7(5.0, 9.9)^{*}$	0.34 (-0.12, 0.68)	6.1 (4.6, 9.0) $^{\#}$	0.28 (-0.18 , 0.64)
$\mathrm{GRF_{PEAK}}$ (N)	PA	91.1 (63.1, 160.6) $*$	0.34 (-0.14, 0.68)	115.8 (78.8, 211.9)	0.06 (-0.42, 0.49)
	CF	33.0 (23.7, 54.4) **	0.44 (-0.04 , 0.76)	56.7 (40.1, 96.1) #	$-0.11 (-0.54, 0.37)$
GRF_{MEAN} (N)	PA	30.6(22.3, 48.3)	-0.23 $(-0.65, 0.26)$	26.4 (19.5, 40.7) $*$	0.13 (-0.33 , 0.53)
	CF	19.4 (14.3, 29.9) **	-0.24 $(-0.66, 0.25)$	22.6 (16.7, 35.2) #	$-0.41 (-0.77, -0.05)$
Impulse (Ns)	PA	15.2 (11.3, 23.3)	0.58(0.18, 0.81)	11.1 $(8.3, 16.9)$ *	0.79(0.54, 0.91)
	CF	$8.1(6.1, 12.3)$ #	0.66(0.29, 0.85)	6.8 (5.1, 10.3) $**$	0.77(0.50, 0.90)
Braking phase					
Duration (ms)	PA	7.0 (5.3, 10.2) **	0.91(0.79, 0.96)	16.3 (12.1, 24.7)	0.52(0.11, 0.78)
	CF	8.4 (6.3, 12.6)	0.51(0.08, 0.78)	6.9 (5.2, 10.3) *#	0.71 $(0.40, 0.87)$
$\mathrm{GRF_{PEAK}}$ (N)	PA	21.8 (16.0, 33.8)	-0.21 $(-0.62, 0.27)$	6.6 (5.0, 9.7) $*$	0.90(0.77, 0.96)
	CF	4.0 (3.0, 5.8) $*$	0.94(0.86, 0.98)	2.8 (2.2, 4.1) **	0.97(0.93, 0.99)
GRF_{MEAN} (N)	PA	6.1(4.6, 9.1)	0.87(0.70, 0.95)	4.3 $(3.2, 6.3)$ *	0.95(0.87, 0.98)
	CF	4.5 (3.4, 6.5) $*$	0.89(0.76, 0.96)	3.0 $(2.3, 4.3)$ **	0.95(0.89, 0.98)
Impulse (Ns)	PA	15.1 (11.3, 22.8)	0.66(0.33, 0.85)	7.8 (5.9, 11.6) $*$	0.90(0.78, 0.96)
	CF	8.6 (6.4, 12.7) $*$	0.63(0.27, 0.83)	6.9 (5.3, 10.3) $*$	0.77(0.51, 0.90)
Propulsive phase					
Duration (ms)	PA	18.9 (14.1, 26.8)	-0.13 $(-0.55, 0.33)$	5.8 (4.4, 8.5) $*$	0.91(0.80, 0.96)
	CF	10.5 (7.9, 16.0) $*$	0.05 (-0.44 , 0.49)	5.6 (4.2, 8.7) $*$	0.34 (-0.17, 0.69)
$\mathrm{GRF_{PEAK}}$ (N)	PA	5.4 (4.0, 8.0) $*$	0.93(0.83, 0.97)	22.8 (16.8, 35.5)	-0.14 $(-0.56, 0.33)$
	CF	3.5 (2.7, 5.1) $*$	0.95(0.89, 0.98)	2.8 (2.1, 4.0) **	0.97(0.93, 0.99)
GRF _{MEAN} (N)	PA	$3.8(2.9, 5.7)$ *	0.96(0.90, 0.98)	19.2 (14.2, 29.7)	0.03 (-0.44 , 0.46)
	CF	3.3(2.5, 4.8)	0.95(0.89, 0.98)	2.8 (2.1, 4.0) *#	0.97(0.92, 0.99)

GRF = ground reaction force. **Bold numbers** identify consistency. A substantial difference was defined as a CV ratio < 0.87. Symbols stand for less CV_{TE} for *trials and #groups.

DISCUSSION

We investigated the consistency of the duration, GRF, and net impulse produced during the unweighting, braking, propulsive, and landing phases of the CMJ in combat fighters and physically active men. Our study design considered three testing days allowing two pairwise comparisons (days 1 vs. 2 and days 2 vs. 3) and the comparisons between two groups with a distinct training background, where the physically actives served as a control. Our results demonstrated that from 32 metrics investigated, six metrics (5 from combat fighters) were considered consistent on days 1 - 2 and days 2 - 3. Four other metrics reached acceptable scores only on days 1 - 2, while three were only on days 2 - 3. Furthermore, adding a third testing day substantially reduced the typical error in 7 out of 8 metrics of the braking phase (Table 3).

We hypothesized that GRF (peak and mean) and net propulsive impulse (usually converted to jump height applying the impulse-momentum theorem) would be more consistent than phase durations related to movement strategy. Our hypothesis was partially confirmed with the combat fighters showing consistent GRF_{PEAK} and GRF_{MEAN} on braking and propulsive as well as the net propulsive impulse. At the same time, the physically actives were less consistent in these metrics, which follows our second hypothesis that combat fighters would be more consistent than physically actives. Previous studies support that individuals with superior training backgrounds may demonstrate more consistency (18,60). Furthermore, we hypothesized that adding a third testing day would improve performance consistency since some learning could be expected from the previous trial. However, our results showed no systematic changes in the mean of almost all metrics of both groups (Table 2), and 11 metrics showed a higher typical error on days 2 - 3 than on days 1 - 2.

Although several metrics can be readily obtained from CMJ phases, our results suggest that more attention should be given to data consistency. We observed inconsistent results from the unweighting phase for both groups. This result corroborates with a previous study (61) reporting CV ranging from 19 to 40% in the unweighting. Furthermore, even metrics obtained from braking and propulsive phases, which indicated more consistent results, should be seen carefully since some inconsistencies were found. We and others (14,61) have observed that metrics related to jumping strategy are less consistent, indicating between days changes in jumping strategy while keeping jumping output consistent. It is important to note that our testing procedure focused on jump height consistency (jump height within 1 cm variation) since jump height is usually the metric of primary interest. Our results suggest that more than this approach is needed for other metrics beyond jump height. A previous study demonstrated that individuals might maintain the jump height output while adopting different strategies (e.g., expending a longer time to perform the countermovement) under symptoms of high-intensity exercise-induced fatigue (12). Therefore, our findings suggest that the protocol applied in the current investigation needs to be revised for those interested in monitoring time-based metrics (e.g., phase durations). Further studies might find better consistency in performing "real-time" monitoring of the metrics of interest. For example, suppose the metric of interest is the propulsion duration, related to neuromuscular fatigue (3). In that case, its variability (e.g., change in mean or coefficient of variation) should be monitored during the testing. In this case, we also recommend monitoring countermovement depth since the athlete may perform a deeper squat (i.e., negative displacement) in the countermovement, resulting in a longer propulsion duration. We also might suggest that the verbal instruction should be more phasespecific. Previous literature (33) has indicated that maximal force and the rate of force (force over time) should not be measured in the same trial since verbal instruction may influence metrics magnitude. Furthermore, a recent study (25) demonstrated that verbal cues might affect the magnitude of phase-specific jump variables (e.g., braking time and force) in recreationally active individuals. Taking it together, we recommend that practitioners consider performing two separate jump tests with foci of attention on specific phases of the jump when interested in both jump output and time-related metrics.

To our knowledge, this is the first study investigating the consistency of metrics obtained during the CMJ landing phase. Our results partially agreed with a previous study (28), demonstrating consistent impulse and net mean force while reporting inconsistent landing duration. However, an interesting result was that the physically actives demonstrated consistent landing impulses, while combat fighters only demonstrated it on days 1 - 2. We might speculate that physically actives had to put less effort into the landing to stabilize their center of mass since they jumped on average 5 cm less (\downarrow 11%) and had 3 kg less (\downarrow 4%) body mass than combat fighters. Although we did not aim to compare the jump mechanics between phases, we noticed that the magnitude of the landing impulse is slightly greater on landing (238 - 288 Ns) than on the propulsive phase (195 - 222 Ns). This difference may be related to the way the landing impulse was measured. The landing phase integration was ended when the center of mass acceleration first crossed zero, but integration drift or any change in strain gages properties might have occurred. Although this issue may have affected the magnitude of the landing impulse, it did not affect our results since it would have affected both groups equally during the three testing days.

Although this study provides some relevant information about consistency of metrics obtained from key phases of the CMJ in combat fighters and physically active men, it is not free of limitations. Three testing days were insufficient to produce acceptable scores for several forcetime metrics. Therefore, more testing days may have been required until our study participants reach consistency. However, requiring a participant to stay away from their exercise routine is challenging, so we only included three testing days in the present study, completed in one or two weeks. Although we have applied the forward dynamics on force-time recordings to identify CMJ phases, we did not investigate other relevant metrics that could be derived from velocity-time and displacement-time curves. Our decision considered that force-time is the primary data captured from a force platform and would be unappropriated to derive data from a source whose data quality was a priori unknown.

In conclusion, our results indicate that combat fighters (i.e., developmental athletes) are more consistent during the braking and propulsive phases of the CMJ than physically active men. Force-time metrics of the CMJ related to the jumping strategy (e.g., phase duration) are less consistent than driven forces and jump output metrics, probably because our participants changed their jump strategy. Adding a third testing day may improve performance consistency, especially from the braking phase.

ACKNOWLEDGEMENTS

This study was financed in part by the Coordenação de Aperfeiçoamento de Pessoal de Nível Superior - Brasil (CAPES) - Finance Code 001. Fundação de Apoio à Pesquisa do Distrito Federal (FAPDF) and Conselho Nacional de Desenvolvimento Científico e Tecnológico (CNPq), Processo: 438324/2018-8.

REFERENCES

1. Atkinson G, Nevill AM. Statistical methods for assessing measurement error (reliability) in variables relevant to sports medicine. Sports Med 26(4): 217–38, 1998.

2. Bird MB, Mi Q, Koltun KJ, Lovalekar M, Martin BJ, Fain A, et al. Unsupervised clustering techniques identify movement strategies in the countermovement jump associated with musculoskeletal injury risk during US Marine Corps Officer Candidates School. Front Physiol 13: 868002, 2022.

3. Bishop C, Jordan M, Torres-Ronda L, Loturco I, Harry J, Virgile A, et al. Selecting metrics that matter: Comparing the use of the countermovement jump for performance profiling, neuromuscular fatigue monitoring, and injury rehabilitation testing. Strength Cond J Epub doi: 10.1519/SSC.0000000000000772, 2022.

4. Boullosa DA, Tuimil JL, Alegre LM, Iglesias E, Lusquiños F. Concurrent fatigue and potentiation in endurance athletes. Int J Sports Physiol Perform 6(1): 82–93, 2011.

5. Chavda S, Bromley T, Jarvis P, Williams S, Bishop C, Turner AN, et al. Force-time characteristics of the countermovement jump: Analyzing the curve in Excel. Strength Cond J 40(2): 67–77, 2018.

6. Clanton TO, Matheny LM, Jarvis HC, Jeronimus AB. Return to play in athletes following ankle injuries. Sports Health 4(6): 471–4, 2012.

7. Claudino JG, Cronin J, Mezêncio B, McMaster DT, McGuigan M, Tricoli V, et al. The countermovement jump to monitor neuromuscular status: A meta-analysis. J Sci Med Sport 20(4): 397–402, 2017.

8. Craig CL, Marshall AL, Sjöström M, Bauman AE, Booth ML, Ainsworth BE, et al. International physical activity questionnaire: 12-country reliability and validity. Med Sci Sports Exerc 35(8): 1381–95, 2003.

9. Cronin JB, Hing RD, McNair PJ. Reliability and validity of a linear position transducer for measuring jump performance. J Strength Cond Res 18(3): 590–3, 2004.

10. Đurović M, Stojanović N, Stojiljković N, Karaula D, Okičić T. The effects of post-activation performance enhancement and different warm-up protocols on swim start performance. Sci Rep 12(1): 9038, 2022.

11. Floría P, Gómez-Landero LA, Suárez-Arrones L, Harrison AJ. Kinetic and kinematic analysis for assessing the differences in countermovement jump performance in rugby players. J Strength Cond Res 30(9): 2533–9, 2016. 12. Gathercole R, Sporer B, Stellingwerff T, Sleivert G. Alternative countermovement-jump analysis to quantify acute neuromuscular fatigue. Int J Sports Physiol Perform 10(1): 84–92, 2015.

13. González-García J, Aguilar-Navarro M, Giráldez-Costas V, Romero-Moraleda B. Time course of jump recovery and performance after velocity-based priming and concurrent caffeine intake. Res Q Exerc Sport Epub doi: 10.1080/02701367.2022.2041162, 2022.

14. Heishman AD, Curtis MA, Saliba E, Hornett RJ, Malin SK, Weltman AL. Noninvasive assessment of internal and external player load: Implications for optimizing athletic performance. J Strength Cond Res 32(5): 1280–7, 2018.

15. Hopkins WG. Measures of reliability in sports medicine and science. Sports Med 30(1): 1–15, 2000.

16. Hopkins WG. Spreadsheets for analysis of validity and reliability. Sportscience 19: 36–45, 2015.

17. Hopkins WG, Marshall SW, Batterham AM, Hanin J. Progressive statistics for studies in sports medicine and exercise science. Med Sci Sports Exerc 41(1): 3–13, 2009.

18. Hopkins WG, Schabort EJ, Hawley JA. Reliability of power in physical performance tests. Sports Med 31(3): 211–34, 2001.

19. James LP, Beckman EM, Kelly VG, Haff GG. The neuromuscular qualities of higher- and lower-level mixedmartial-arts competitors. Int J Sports Physiol Perform 12(5): 612–20, 2017.

20. James LP, Connick M, Haff GG, Kelly VG, Beckman EM. The countermovement jump mechanics of mixed martial arts competitors. J Strength Cond Res 34(4): 982–7, 2020.

21. Kennedy RA, Drake D. Improving the signal-to-noise ratio when monitoring countermovement jump performance. J Strength Cond Res 35(1): 85–90, 2021.

22. Koo TK, Li MY. A guideline of selecting and reporting intraclass correlation coefficients for reliability research. J Chiropr Med 15(2): 155–63, 2016.

23. Kottner J, Audigé L, Brorson S, Donner A, Gajewski BJ, Hróbjartsson A, et al. Guidelines for reporting reliability and agreement studies (GRRAS) were proposed. J Clin Epidemiol 64(1): 96–106, 2011.

24. Kozinc Ž, Žitnik J, Smajla D, Šarabon N. The difference between squat jump and countermovement jump in 770 male and female participants from different sports. Eur J Sport Sci 22(7): 985–93, 2022.

25. Krzyszkowski J, Chowning LD, Harry JR. Phase-Specific Verbal cue effects on countermovement jump performance. J Strength Cond Res 36(12): 3352–8, 2022.

26. Laffaye G, Wagner PP, Tombleson TIL. Countermovement jump height: Gender and sport-specific differences in the force-time variables. J Strength Cond Res 28(4): 1096–105, 2014.

27. Lake J, Mundy P, Comfort P, McMahon JJ, Suchomel TJ, Carden P. Concurrent validity of a portable force plate using vertical jump force-time characteristics. J Appl Biomech 34(5): 410–3, 2018.

28. Lake JP, Mundy PD, Comfort P, McMahon JJ, Suchomel TJ, Carden P. Effect of barbell load on vertical jump landing force-time characteristics. J Strength Cond Res 35(1): 25–32, 2021.

29. Linthorne NP. Analysis of standing vertical jumps using a force platform. Am J Phys 69(11): 1198–204, 2001.

30. Loturco I, Pereira LA, Kobal R, Kitamura K, Cal Abad CC, Nakamura FY, et al. Peak versus mean propulsive power outputs: Which is more closely related to jump squat performance? J Sports Med Phys Fitness 57(11): 1432– 44, 2017.

31. Loturco I, Winckler C, Kobal R, Cal Abad CC, Kitamura K, Veríssimo AW, et al. Performance changes and relationship between vertical jump measures and actual sprint performance in elite sprinters with visual impairment throughout a Parapan American games training season. Front Physiol 6: 323, 2015.

32. Lum D, Comfort P, Barbosa TM, Balasekaran G. Comparing the effects of plyometric and isometric strength training on dynamic and isometric force-time characteristics. Biol Sport 39(1): 189–97, 2022.

33. Maffiuletti NA, Aagaard P, Blazevich AJ, Folland J, Tillin N, Duchateau J. Rate of force development: Physiological and methodological considerations. Eur J Appl Physiol 116(6): 1091–116, 2016.

34. McKay AKA, Stellingwerff T, Smith ES, Martin DT, Mujika I, Goosey-Tolfrey VL, et al. Defining Training and performance caliber: A participant classification framework. Int J Sports Physiol Perform 17(2): 317–31, 2022.

35. McKay MJ, Baldwin JN, Ferreira P, Simic M, Vanicek N, Burns J, et al. Reference values for developing responsive functional outcome measures across the lifespan. Neurology 88(16): 1512–9, 2017.

36. McMahon JJ, Jones PA, Comfort P. Comparison of countermovement jump-derived reactive strength index modified and underpinning force-time variables between Super League and Championship Rugby League players. J Strength Cond Res 36(1): 226–31, 2022.

37. McMahon JJ, Jones PA, Dos'Santos T, Comfort P. Influence of dynamic strength index on countermovement jump force-, power-, velocity-, and displacement-time curves. Sports 5(4): 72, 2017.

38. McMahon JJ, Rej SJE, Comfort P. Sex differences in countermovement jump phase characteristics. Sports 5(1): 8, 2017.

39. McMahon JJ, Suchomel TJ, Lake JP, Comfort P. Understanding the key phases of the countermovement jump force-time curve. Strength Cond J 40(4): 96–106, 2018.

40. Merino Fernández M, Ruiz-Moreno C, Giráldez-Costas V, Gonzalez-Millán C, Matos-Duarte M, Gutiérrez-Hellín J, et al. Caffeine doses of 3 mg/kg increase unilateral and bilateral vertical jump outcomes in elite traditional Jiu-Jitsu athletes. Nutrients 13(5): 1705, 2021.

41. Merrigan JJ, Stone JD, Hornsby WG, Hagen JA. Identifying reliable and relatable force-time metrics in athletes-Considerations for the isometric mid-thigh pull and countermovement jump. Sports 9(1): 4, 2020.

42. Moir GL, Garcia A, Dwyer GB. Intersession reliability of kinematic and kinetic variables during vertical jumps in men and women. Int J Sports Physiol Perform 4(3): 317–30, 2009.

43. Navalta JW, Stone WJ, Lyons TS. Ethical issues relating to scientific discovery in exercise science. Int J Exerc Sci 12(1): 1–8, 2019.

44. Nibali ML, Tombleson T, Brady PH, Wagner P. Influence of familiarization and competitive level on the reliability of countermovement vertical jump kinetic and kinematic variables. J Strength Cond Res 29(10): 2827–35, 2015.

45. Parker J, Lundgren LE. Surfing the waves of the CMJ; Are there between-sport differences in the waveform data? Sports 6(4): 168, 2018.

46. Pathare N, Haskvitz EM, Selleck M. Comparison of measures of physical performance among young children who are healthy weight, overweight, or obese. Pediatr Phys Ther 25(3): 291–6, 2013.

47. Pérez-Castilla A, Fernandes JFT, Rojas FJ, García-Ramos A. Reliability and magnitude of countermovement jump performance variables: Influence of the take-off threshold. Meas Phys Educ Exerc Sci 25(3): 227–35, 2021.

48. Pérez-Castilla A, Jiménez-Reyes P, Haff GG, García-Ramos A. Assessment of the loaded squat jump and countermovement jump exercises with a linear velocity transducer: Which velocity variable provides the highest reliability? Sports Biomech 20(2): 247–60, 2021.

49. Pérez-Castilla A, Rojas FJ, García-Ramos A. Reliability and magnitude of loaded countermovement jump performance variables: A technical examination of the jump threshold initiation. Sports Biomech 21(5): 622–36, 2022.

50. Samozino P, Morin J-B, Hintzy F, Belli A. A simple method for measuring force, velocity, and power output during squat jump. J Biomech 41(14): 2940–5, 2008.

51. Sole CJ, Mizuguchi S, Sato K, Moir GL, Stone MH. Phase characteristics of the countermovement jump forcetime curve: A comparison of athletes by jumping ability. J Strength Cond Res 32(4): 1155–65, 2018.

52. Souza AA, Bottaro M, Rocha VA, Lage V, Tufano JJ, Vieira A. Reliability and test-retest agreement of mechanical variables obtained during countermovement jump. Int J Exerc Sci 13(4): 6–17, 2020.

53. Street G, McMillan S, Board W, Rasmussen M, Heneghan JM. Sources of error in determining countermovement jump height with the impulse method. J Appl Biomech 17(1): 43–54, 2001.

54. Taylor K-L, Chapman D, Cronin J, Newton M, Gill N. Fatigue monitoring in high performance sport: A survey of current trends. J Aus Strength Cond 20: 12–23, 2012.

55. Thomas C, Jones PA, Dos'Santos T. Countermovement jump force–time curve analysis between strengthmatched male and female soccer players. Int J Environ Res Public Health 19(6): 3352, 2022.

56. Thomas C, Kyriakidou I, Dos'Santos T, Jones PA. Differences in vertical jump force-time characteristics between stronger and weaker adolescent basketball players. Sports 5(3): 63, 2017.

57. Ugliara L, Tufano JJ, Bottaro M, Vieira A. Test-retest reliability of plantar flexion torque generation during a functional knee extended position in older and younger men. J Aging Phys Act 29(4): 626–31, 2021.

58. Ugrinowitsch C, Tricoli V, Rodacki A, Ricard M. Influence of training background on jumping height. J Strength Cond Res 21(3): 848-52, 2007.

59. Vieira A, Ribeiro GL, Macedo V, de Araújo Rocha Junior V, Baptista R de S, Gonçalves C, et al. Evidence of validity and reliability of Jumpo 2 and MyJump 2 for estimating vertical jump variables. PeerJ 11: e14558, 2023.

60. Vieira A, Tufano JJ. Reactive strength index-modified: Reliability, between group comparison, and relationship between its associated variables. Biol Sport 38(3): 451–7, 2021.

61. Warr D, Pablos C, Sánchez-Alarcos J, Izquierdo Velasco J, Redondo JC. Reliability of measurements during countermovement jump assessments: Analysis of performance across subphases. Cogent Soc Sci 6(1): 1843835, 2020.

62. Welsh TT, Alemany JA, Montain SJ, Frykman PN, Tuckow AP, Young AJ, et al. Effects of intensified military field training on jumping performance. Int J Sports Med 29(1): 45–52, 2008.

63. Williams KJ, Chapman DW, Phillips EJ, Ball N. Effects of Athlete-dependent traits on joint and system countermovement-jump power. Int J Sports Physiol Perform Epub doi: 10.1123/ijspp.2018-0050, 2018.

