



HHS Public Access

Author manuscript

J Thromb Haemost. Author manuscript; available in PMC 2024 September 01.

Published in final edited form as:

J Thromb Haemost. 2023 September ; 21(9): 2339–2353. doi:10.1016/j.jtha.2023.06.010.

Why Platelet Mechanotransduction Matters for Hemostasis and Thrombosis

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Abstract

Mechanotransduction is the ability of cells to “feel” or sense their mechanical microenvironment and to integrate and convert these physical stimuli into adaptive biochemical cellular responses. This phenomenon is vital for the physiology of numerous nucleated cell types to affect their various cellular processes. As the main drivers of hemostasis and clot retraction, the platelet also possesses this ability to sense the dynamic mechanical microenvironments of the circulation and convert those signals into biological responses integral to clot formation. Like other cell types, platelets leverage their “hands” or receptors/integrins to mechanotransduce important signals responding to vascular injury to achieve hemostasis. The clinical relevance of cellular mechanics and mechanotransduction is imperative as pathological alterations or aberrant

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OO and SA wrote the manuscript. JL and OO created the figures. WL and JL critically reviewed the manuscript. All authors read and commented on the paper and approved submission.

Conflict of interest

None of the authors declare any conflict of interest with regards to this review.

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mechanotransduction in platelets has been shown to lead to bleeding and thrombosis. As such, the aim of this review is to provide an overview of the most recent research related to platelet mechanotransduction, from platelet generation to platelet activation within the hemodynamic environment and clot contraction at the site of vascular injury, thereby covering the entire “life cycle” of the platelet. Additionally, we describe the key mechanoreceptors in platelets and discuss the new biophysical techniques that have enabled the field to understand how platelets sense and respond to their mechanical microenvironment via those receptors. Finally, the clinical significance and the importance of continued exploration of platelet mechanotransduction is discussed, as the key to better understanding both thrombotic and bleeding disorders lies with a more complete mechanistic understanding of platelet function by way of mechanotransduction.

Keywords

biomechanics; blood platelets; hemostasis; mechanotransduction; thrombosis

Introduction:

Mechanotransduction is the ability of cells to “feel”, sense, interact and convert mechanical stimuli from the physical microenvironment to biochemical signals that elicit adaptive cellular response. Over the last two decades, the field of mechanobiology has made substantial progress investigating how nucleated cells respond to their mechanical microenvironment. Specifically, how cells respond to the elastic (1, 2), viscous (3) and viscoelastic microenvironments(4-6). Studies have shown that mechanotransduction of the signals from these microenvironments effect cell adhesion(3), spreading (7), stem cell fate(1, 6) and cell migration(8). Most importantly it has been shown that mechanobiology and mechanotransduction in various cells have important clinical relevance (9, 10). Like nucleated cells, although less studied, platelets mechanotransduce signals from the mechanical microenvironment to adapt to their microenvironment, however, again like nucleated cells the challenge of translation is in creating tools able to closely mimic the *in vivo* microenvironment to undergo biomechanical studies with physiological relevance.

Hemostasis is a complex and inherently mechanical process involving both the coagulation cascade and platelets to form a clot at the site of injury to promote wound closure (11). Platelets in circulation are recruited to sites of vascular injury and activated through means of biochemical and biomechanical cues. Mechanically, during primary hemostasis, shear, and injury to endothelial cells on the blood vessel wall exposes the subendothelium, consequently allowing platelets to adhere to various proteins, such as collagen with the receptor GPVI and the integrin $\alpha_2\beta_1$ and additionally adhere to von Willebrand Factor (vWF) with the receptor GP1b complex. Platelets then begin to accumulate and aggregate to each other with their surface integrin $\alpha_2\beta_3$ (GPIIb/IIIa) to form a platelet plug. Simultaneously, during secondary hemostasis, thrombin produced by the coagulation cascade converts fibrinogen to fibrin polymers while additionally further activating platelets, causing platelets to spread and contract, which reinforces and stabilizes the developing clot. As such, it is evident that the ability of platelets to sense and respond cues is of vital importance for thrombus formation.

Many biophysical technologies have recently been developed that enable the investigation of these processes with quantitative rigor (Figure 1). One example is microfluidic devices that have been leveraged to experimentally mimic *in vivo* conditions of vascular flow. Numerous microfluidic technologies have led to key insights into platelet physiology as they allow for complete control of not only the biochemical microenvironment but the mechanical one as well. Because it is possible to control flow rate and shear conditions with these techniques, it has been shown these biophysical parameters are essential for thrombus formation and discoid platelet aggregation (12) and because it is possible to integrate various protein substrates that are expressed on the surface of the vascular endothelium, closely mimicking the *in vivo* microenvironment becomes possible(13) (Figure 1). Additionally, microfluidics allow for complete control of the geometry that platelets are exposed to and can be varied in order to mimic different blood vessels in the body, such as valves within the venous system(14) and stenosed blood vessels (15). The added ability to directly culture endothelial cells themselves (16, 17) within these devices has allowed for proper investigation into how platelets respond to blood vessel injury (18, 19). In regard to understanding platelet contraction and the final clot microenvironment, atomic force microscopy (AFM) has been used to measure cell length and force to characterize biomechanics of platelet contraction force and dynamics (20). Using AFM, it has been observed that platelets contract rapidly and generate high contraction and adhesive forces in a stiffness-dependent manner (Figure 1). This is suggestive of heterogeneity, with higher density of fibrin exhibiting higher stiffness. Platelet contraction may result in increases of force in such areas of increased stiffness (21). Consequently, it is evident that the development of *in vitro* technologies and methodologies are imperative for continued understanding of platelet mechanotransduction.

As such, the objective of this review is to 1) discuss how mechanical forces and the mechanical microenvironment influence the initiation, propagation, and the stability of a developing clot, 2) discuss the mechanisms of how platelets leverage key receptors and integrins on their surface to sense and respond to their mechanical microenvironment 3) explore the new technologies and techniques that have enabled bulk and single cell investigations of these phenomena and 4) most importantly discuss why this matters, by highlighting the clinical relevance of platelet mechanotransduction for hemostasis and thrombosis.

Section 1: Platelet biomechanics spanning over the lifespan of the cell

1.1: Platelet production and circulation—With an average lifespan of 7-9 days and in a tightly controlled manner, 1 trillion platelets circulate the blood stream (22, 23). Although not as well characterized, mechanics not only play an imperative role in platelet response to the microenvironment within a growing thrombus, but also in the production of platelets themselves. Biochemically, it has been shown that agonists such as thrombopoietin(23), IL- α (24), CCL5(25) and many chemokine mediators(26) induce megakaryocyte production and/or thrombopoiesis. Mechanically, it has been made clear that the cytoskeleton, specifically microtubules play an essential role in the thrombopoietic process(27). More recently, it has been established that megakaryocytes are mechanically responsive and take in cues from the mechanical microenvironment to produce platelets.

Specifically, megakaryocytes respond to shear (28, 29) as well as turbulent energy (30) in order to produce new platelets into circulation.

Once produced and in circulation, platelets experience mechanical forces from their surrounding microenvironment and throughout thrombus formation. Fluid shear stress is the most relevant force in platelet-mediated hemostasis and thrombosis (31) (Figure 1). In blood vessels, fluid shear stress is influenced by mechanical forces produced by pressure changes and influenced by the size of the microvasculature, fluid flow rate, and other rheological properties of blood (32). Inactivated platelets in circulation are subjected to these same mechanical forces under flow conditions in blood vessels. Platelets in circulation are pushed towards the periphery of flow nearer to maximal shear stresses generated at the vessel wall (Figure 2)(33).

1.2: Platelets at the site of vascular injury—During vascular injury, convection and diffusion drive platelets to collide with the vascular surface, enabling interactions with the exposed subendothelium (Figure 2). Plasma vWF is immobilized onto the exposed subendothelial matrix and in doing so, vWF becomes a ligand for mechanopresentation binding to the mechanoreceptor GPIb(34). Under high shear rate flow conditions, vWF binds to its platelet receptor, GPIb-IX to form a “catch bond”. This bond allows transient platelet adhesion under high shear stress present in arteries and arterioles (35-37) (Figure 2).

Platelets express integrins that transduce signals from within the platelet and from the mechanical microenvironment. Under shear stress, vWF binds on both the platelet GPIb-IX-V complex and $\alpha 2b\beta 3$ (GPIIb/IIIa) to mediate aggregation (31). Shear-activated platelets release stored vWF to promote thrombus formation. The growth of the thrombus is further influenced by increasing shear rate as platelets on the surface of the thrombus are subject to greater activation and aggregation than those platelets within the core (38, 39). This demonstrates the effect of blood rheology in thrombus development as alterations in the microenvironment influence platelet adhesiveness onto thrombogenic surfaces and the rate of thrombus growth (40).

Stable platelet adhesion to the vessel wall is an essential first step in thrombus formation in response to vascular injury (41). Additionally, at sites of vascular injury and in response to changes in vessel geometry, it has been found that discoid platelets form aggregates due to rapid changes in the hemodynamic environment(12). To undergo this, platelets mechanosense shear microgradients by sensing sudden accelerations and decelerations in shear that lead to the formation and restructuring/strengthening of GPIb and $\alpha 2b\beta 3$ (GPIIb/IIIa) membrane tethers (42). These discoid platelet aggregates are then converted to stable platelet aggregates by the release of soluble platelet agonists such as ADP(42). Similarly, platelet activation mediated by GPVI and GPIb and subsequent biochemical secretion of platelet agonists reinforce $\alpha I I b \beta 3$ -dependent platelet aggregation. Fibrinogen is critical for formation of a stable thrombus and once the thrombus is formed, platelets within interact with a fibrin meshwork. Subsequent stable thrombus formation and clot retraction is driven by biochemical transduction mediated by integrin $\alpha I I b \beta 3$ through outside-in signals following fibrinogen binding (43). Importantly, platelets mechanosense the stiffness of fibrin and fibrinogen as the fibrin meshwork forms in thrombus formation.

The capability of platelets to mechanosense stiffness in the microenvironment in a growing thrombus allows for platelet mechanotransduction into further platelet aggregation and activation (20). Platelets are activated nonuniformly within the developing clot(44). As platelets contract and pull fibrin fibers together, secondary aggregates of platelets form, thereby remodeling the fibrin network and increasing the density and clot stiffness. Platelet contraction mechanically remodels the fibrin network of the clot over the course of clot contraction (45) (Figure 2).

Section 2: Overview of the mechanoreceptors in platelets

As noted previously mechanical forces play a major role in thrombus formation to stem bleeding. These processes all require platelet integrins or glycoproteins aka “hands” to interact, grab, and hold onto various proteins in the microenvironment such as vWF, collagen and fibrinogen (Figure 3). The major mechanoreceptors that we will discuss are the vWF receptor GPIb-IX complex, the fibrin(ogen) receptor $\alpha 2b\beta 3$ (GPIIb/IIIa) and the collagen receptors GPVI and $\alpha 2\beta 1$.

2.1: Overview of GPIb-IX complex and mechanotransduction signaling mechanisms

—The GPIb-IX complex, with approximately 25,000 copies (46) is an essential platelet glycoprotein, where dysfunction and/or absence of this receptor leads to Bernard-Soulier syndrome, in which patients have a propensity to bleed(47). The GPIb-IX complex allows for platelets to sense mechanical force while responding to vascular injury through a mechanosensory domain (MSD) within the complex (Figure 3) (48). The MSD within GPIb acts as the mechanoreceptor, mechanotransmitter and mechanotransducer upon presentation of the vWF A1 domain. In physiological flow conditions, A1 is shielded in vWF and will undergo morphological changes under shear stress(49). For vWF to expose its A1 domain, it mechanosenses fluid shear to straighten the folded globular conformation of a vWF multimer. The MSD in GPIb is in a folded state until unfolded by vWF-mediated pulling which occurs in the presence of shear flow. Binding of vWF to MSD propagates force along the GPIb macroglycopeptide stalk to transmit platelet intracellular biochemical signaling by enhancing calcium triggering in platelets. Intracellular calcium triggering activates integrin $\alpha 2b\beta 3$ (GPIIb/IIIa) (49). Additionally, the MSD also plays a critical role in mechanotransduction via GPIb to induce a biomechanical pathway of integrin $\alpha 2b\beta 3$ (GPIIb/IIIa) affinity maturation and thrombus development which we will discuss further when discussing the integrin $\alpha 2b\beta 3$ (GPIIb/IIIa) (50).

The structure of GPIb-IX complex consists of GPIb α , GPIb β and GPIX subunits (51). The GPIb α subunit N-terminal domain associates with vWF A1 domain via catch-bond to facilitate platelet tethering. There is a leucine-rich repeat domain (LRRD) within N-terminal domain of the ligand binding domain of GPIb α that is unfolded by this interaction with vWF (52). This ligand-receptor engagement further strengthens the vWF-A1 bond to prolong the bond lifetime and increases the likelihood of unfolding the MSD (53, 54) Fluorescence biomembrane force probe has enabled single-cell analysis of ligand binding kinetics to demonstrate the role of MSD unfolding in GPIb mechanosensing and has shown LRRD unfolding prolongs the bond vWF-A1 bond lifetime (55, 56). The C-terminal domain of

GPIb α also plays an essential role by interacting with Filamin, an actin binding protein, and promoting vWF induced platelet activation(57, 58).

Several studies elucidated the mechanism by which MSD enables platelet mechanosensing. The use of optical tweezers enabled pulling of the N-terminal domain within GPIb α with recombinant vWF-A1 (48). This induced unfolding of a domain in the juxtamembrane stalk of GPIb α and thereby identified the MSD. Furthermore, it was identified that forces ranging from 5 to 20 pN were required to unfold the MSD which is comparable to the forces that induce catch-bonds in forming the complex of vWF-A1 with GPIb α . This unfolding force is lower than the drag force exerted on a platelet under physiologic shear conditions in circulation (49).

The ‘trigger’ model of GPIb-IX signaling further explained the shear requirement of the MSD to be induced and unfold from its resting folded state (49). The MSD was further established by studies altering the MSD regions in GPIb mutants and it was shown that no other region of the molecule served as an alternative mechanotransducer (59). Further it was identified that the unfolded MSD can refold with or without applied forces and is relatively unstable. Therefore, the MSD can refold and turn off the mechanosensory signaling of GPIb. The MSD requires a continuous pulling force of >15pN to fully active GPIb-IX (60). Thus, the microenvironment influences the conformation and stability of the MSD with downstream implications of platelet mechanotransduction. Pathologically, the clearance of platelets has more recently been linked to the MSD in type 2B von Willebrand’s Disease, where binding of vWF under physiological shear induces MSD unfolding and thereafter intracellular signaling that eventually leads to the exposure of β -galactose on the surface of the platelet causing enhanced clearance and thrombocytopenia(49).

Although the mechanotransductory mechanisms of the GPIb-IX complex are well characterized, one additional signaling mechanism that remains elusive and controversial is the role of GPIb-IX in thrombin induced platelet activation. Although some studies have shown little evidence that the GPIb-IX complex is associated with thrombin induced platelet activation(61), it has been shown that GPIb is necessary for full activation of platelets essentially working synergistically with protease-activated receptor (PAR)-1 as a co-receptor (62), but not PAR-4(63) (two key thrombin receptors). More recently, it has been shown that thrombin actually induces an independent pathway of signaling in GPIb(64) that works cooperatively with the PAR receptors leading to enhanced platelet activation(65). It is common for biological pathways to be redundant to intensify and strengthen a processes like hemostasis and as such, further investigation is necessary to determine the role of GPIb-IX complex in thrombin induced platelet activation.

2.3: Overview of α 2b β 3 (GPIIb/IIIa) signaling and mechanotransduction

mechanisms—The integrin α 2b β 3 (GPIIb/IIIa), with approximately 80,000 copies per platelet, is the most abundant receptor on the platelet surface(66) and binds to arginine-glycine-aspartic acid (RGD) sites on fibrinogen, fibrin, vWF and fibronectin. The clinical relevance and the importance of α 2b β 3 (GPIIb/IIIa) in hemostasis was established by the discovery of Glanzmann’s thrombasthenia, an autosomal recessive bleeding disorder that is caused by impaired synthesis and/or function of α 2b and/or β 3 subunits leading to impaired

platelet function(67, 68). The conformation and affinity of $\alpha 2b\beta 3$ (GPIIb/IIIa) is tightly regulated and in resting platelets $\alpha 2b\beta 3$ (GPIIb/IIIa) adopts the inactive or bent conformation and upon activation this low affinity integrin conformation adopts an active or extended conformation, possessing enhanced binding efficiency to fibrin(ogen)(69). Like other integrins, $\alpha 2b\beta 3$ (GPIIb/IIIa) bears a mechanical load to undergo mechanotransduction. This load can originate intracellularly from the acto-myosin machinery or inputs from the extracellular mechanical microenvironment (Figure 3). As such the signaling of $\alpha 2b\beta 3$ (GPIIb/IIIa) is bidirectional from either inside-out signaling and/or outside-in signaling with the end product leading to increased engagement of $\alpha 2b\beta 3$ (GPIIb/IIIa) to fibrin(ogen) and clot retraction. Inside-out signaling is a very redundant process as it can progress through vWF and/or collagen binding to glycoproteins at the site of injury, thrombin generated during secondary hemostasis, and/or ADP and TXA2 released granules within the platelet. The numerous signaling receptors that bind to these agonists cause triggering of downstream events leading to the activation of Rap1 (small GTPase) and recruitment of the mechanosensitive proteins talin and kindlin(70) which bind to the cytoplasmic tail of $\beta 3$. This consequently causing a conformational change of $\alpha 2b\beta 3$ (GPIIb/IIIa) from the inactive bent conformation to the activated extended open conformation, allowing for connections between the intracellular cytoskeleton (acto-myosin machinery) and the extracellular matrix. This enabling strong interactions between $\alpha 2b\beta 3$ (GPIIb/IIIa) and fibrin(ogen), allowing for force generation. Deficiencies in either talin or kindlin have been shown to be associated with bleeding diathesis and as such both proteins are essential for sufficient signaling and activation of $\alpha 2b\beta 3$ (GPIIb/IIIa) (71, 72). Additionally, it has been shown that the cytosolic protease, calpain, cleaves talin in order to increase platelet contraction of fibrin(73).

Recent advances in single platelet biophysical techniques have recognized a distinct intermediate state of $\alpha 2b\beta 3$ (GPIIb/IIIa) and as such a biomechanical pathway of inside-out signaling that is slightly different than what is known biochemically. Using biomembrane force probes (BFP)(50) it was shown that when triggered by mechanical stimulation, GPIIb induces intracellular calcium release thereby promoting the intermediate state of $\alpha 2b\beta 3$ (GPIIb/IIIa), a state with affinity and bond lifetimes that are intermediate of both the inactive and active conformations. This in turn leading to outside-in signaling allowing for platelet aggregation and thrombus development(50) (Figure 4). Outside-in signaling occurs when $\alpha 2b\beta 3$ (GPIIb/IIIa) binds to and interacts with fibrin(ogen), here substrate stiffness plays an essential role as soft substrates result in weak $\alpha 2b\beta 3$ (GPIIb/IIIa) interactions with fibrinogen, while stiffer substrates lead to increased outside-in signaling, consequently causing increased platelet activation (Phosphatidyl serine exposure, granule release etc), adhesion, spreading and contraction(74, 75). This increased biophysical input from outside-in signaling alongside the biochemical input from inside-out signaling synergistically drive platelet aggregation and contraction. Similarly, utilizing subcellular techniques to investigate platelet integrin response to the mechanical microenvironment, it was shown that platelet integrins respond to tangential tension from the mechanical microenvironment (76) and that low level integrin tension is produced during adhesion while high level integrin tension is produced during contraction(77).

Unlike the GPIIb-IX complex, the mechanosensitive domains/epitopes of $\alpha 2b\beta 3$ (GPIIb/IIIa) are not as well characterized. What is known is that structurally, the domains of integrins

are highly conserved within the integrin family(78). One example of a mechanosensitive domain is the plexin-semaphorin-integrin (PSI) domain, located on the β subunit of $\alpha 2\beta 3$ (GPIIb/IIIa). It has been shown to be an important domain for integrin transition from the inactive to the active state(79) similar to its role in activation for the $\beta 2$ subunit of other integrins(80). Although there is evidence that this domain shows some importance in the transition from the inactive to active confirmation, other domains of $\alpha 2\beta 3$ (GPIIb/IIIa) need to be explored in order to determine the epitopes essential for affinity maturation.

2.4: Overview of mechanotransduction on collagen surfaces—One of the most abundant subendothelial proteins for platelet adhesion and aggregation at the injured vessel wall is collagen. Consequently, on their surface, platelets express two collagen receptors, GPVI and the integrin $\alpha 2\beta 1$ in order to trigger platelet activation and aid in thrombus formation. GPVI has been thought to be the main receptor involved in platelet activation, weak adhesion to collagen by activating the integrin $\alpha 2\beta 1$ to promote strong platelet adhesion to collagen (81) and activating the integrin $\alpha 2\beta 3$ (GPIIb/IIIa) further leading to platelet activation (82). As such, clinically speaking absence of these receptors is known to cause a mild bleeding phenotype(83). Although GPVI has been known to bind collagen leading to platelet activation, recent evidence has indicated that GPVI also plays an important role in platelet aggregation and development of a thrombus through its interactions with both fibrinogen and fibrin(84) leading to thrombin generation(85). GPVI specifically interacts with fibrinogen in its dimeric form(84) close to its collagen binding site(86) to further support adhesion and enhance platelet activation. Fibrin formation then leads to increased avidity of GPVI and further promotes platelet activation and platelet spreading through mechanisms independent of $\alpha 2\beta 3$ (GPIIb/IIIa)(87).

Like $\alpha 2\beta 3$ (GPIIb/IIIa), the true mechanotransductive domains of these receptors have not been well characterized, but our group specifically has shown that platelets do mechanosense collagen surfaces of different stiffnesses and spread further on stiffer substrates (Figure 3)(88) and this mechanotransduction is mediated through actin polymerization and the myosin light chain kinase (MLCK), similar to platelet response on fibrinogen coated surfaces(75). Together, knowing GPVI is thought to be involved in early platelet adhesion to collagen(82) and studies showing no difference in the intensity of $\alpha \text{I} \text{I} \beta 3$ activation on collagen substrates of different stiffnesses, it was postulated that $\alpha \text{I} \text{I} \beta 3$ activation is mediated through initial binding of GPVI to collagen thereby activating $\alpha \text{I} \text{I} \beta 3$, while increased spreading area on collagen coated surfaces of different stiffnesses is mediated by $\alpha 2\beta 1$ through outside-in mechanisms(88). Additionally, other studies have elucidated the fact that platelets reorganize their cytoskeleton on collagen surfaces to regulate their spreading behavior depending on the surrounding geometric constraints further highlighting the ability of platelets to “feel” and mechanosense their microenvironment on collagen surfaces (89, 90).

Section 3: Investigating platelet response to the mechanical microenvironment

When thinking of the platelet mechanical microenvironment, it is imperative to discuss whole blood clot contraction and platelet interactions with fibrin(ogen). In brief, during clot contraction, thrombin produced by the coagulation cascade converts fibrinogen to form

fibrin polymers and platelets perform many different biophysical actions during this process, they adhere to, they spread to, and contract these fibrin polymers, dramatically stiffening the clot (91, 92). Like most biological tissues, the clot in itself is viscoelastic containing both viscous and elastic properties (93), and this viscoelasticity can vary greatly during the clotting process(94). Historically, research has focused on understanding macroscale platelet mechanical behavior by measuring bulk clot forces(95) and clot viscoelasticity(96). The challenge however with understanding mechanotransduction and single platelet biomechanical behavior with bulk clot assays lies within the complexity of its components and the constantly changing mechanical microenvironment (97). This consequently, making it nearly impossible to decouple the influence of individual components. Additionally, although a necessary step, an issue with decoupling individual components lies with simplifying complex interactions that might influence behavior. Substantial progress has been made to decouple the role of fibrin in this process (96, 98), and more recently progress has been made on the influence the mechanical microenvironment has on platelets due to new single platelet technologies. For example, decoupling the viscous component or fluidity of a developing blood clot and focusing on the contributions of the elastic component of a stiffening clot, single platelet assays have provided key information regarding how single platelets respond to increased and decreased stiffness using standard adhesion assays on hydrogels of varying stiffness (75) and how they respond to different geometries(89) in order to spread and release granules(90).

Understanding how individual platelets integrate into the myriad of the clot environment and generate platelet forces has been a more recent and important area of exploration. Although low throughput, our own lab has leveraged atomic force microscopy (AFM) to measure the contractile forces of single platelets (21) which allowed for the force measurements of platelets in various mechanical microenvironments. Building on this work we developed a microfluidic system, coined the “Platelet Contraction Cytometer” that has increased the throughput of the measurements of single platelet forces from tens to hundreds of platelets(74). This recent advance in our single platelet contraction technology has allowed for a more thorough investigation into platelet biomechanical behavior to different substrates, consequently allowing for key insights into how platelet force is influenced by the stiffness of the mechanical microenvironment (74). Mechanistically our system showed that the Rho kinase and not the Myosin Light Chain Kinase pathway (MLCK) is required for mechanosensitive platelet contraction in various mechanical microenvironments. This was mechanistically interesting as our group had previously shown that other biophysical parameters such as adhesion and spreading were primarily associated with the MLCK pathway(75, 88). This eluding to the concept that different biophysical parameters are associated with different mechanistic pathways.

Although our group has focused its efforts on leveraging fibrin(ogen) as the protein of choice for both our AFM and microfluidic systems, other groups have used collagen or vWF as the protein of choice for their platelet contraction systems and have provided key insights on how platelets behave on these surfaces. Using microfluidics and high shear gradients, it was found that platelet forces of a growing platelet aggregate are sensitive to various platelet inhibitors (99). Similarly, one common technique many groups have utilized to measure platelet forces at the single cell level is traction force microscopy. Mechanistically

these techniques have been beneficial by showing the importance of the GPIb complex interactions with the A1 domain of vWF for platelet force generation and highlighted the protein filamin as the intermediary that transmits forces from the cytoskeleton within the platelet to vWF (Figure 3) (100). Additionally, we know from previous work that within a clot, the platelet population is heterogenous and this heterogeneity is advantageous (44) and it is known that the forces a single platelet can generate has a wide range from 1 nN – 100 nN(74, 92, 97), however another elusive question is what makes one platelet highly contractile while another weakly contractile. Recently, using traction force microscopy one group has begun to answer this question, they showed that highly contractile platelets exhibit increased spreading area, and are morphologically more circular with uniformly distributed F-actin(101). As such, it is evident that single platelet biophysical assays especially regarding contraction have provided key mechanistic insights and as such have shown the importance of investigating cellular mechanics at the single cell. More recently, leveraging our knowledge of platelet mechanical behavior at the bulk clot level and the more recent developments of how platelets behave at the single platelet level, computational models have aided in connecting the macroscale to the microscale (44, 97) by helping us understand the importance of platelet heterogeneity in isovolumetric contraction (44) and the connection between single platelet force and bulk clot force(97). Although substantial progress has been made, more work is necessary to definitively translate platelet behavior at the single cell level to collective platelet behavior at the bulk clot level, an area complicated by the complexity of the microenvironment.

Section 4: Clinical Implications of Platelet Biomechanics and Mechanotransduction

Our understanding of platelet mechanics and how the mechanical microenvironment shapes platelet behavior has improved with the advancement of tools such as in-vitro flow-based microfluidics, volumetric bulk clot contraction assays, single platelet assays and assays investigating subcellular integrin mechanics in addition to the improved imaging techniques to further allow single and aggregate platelet exploration(102). Numerous bulk, aggregate and single platelet experimental techniques have linked platelet mechanics to not only hematological clinical disorders but numerous others (Table 1). Leveraging volumetric bulk clot contraction assays it has been shown that impaired bulk clot contraction is implicated in numerous disease states such as Sickle Cell Disease (103), asthma (104), lupus(105), stroke(106) and trauma(107) to name a few (Figure 5). Similarly in microclots, patients with von Willibrand's Disease show impaired clot contraction(108). However enhanced clot contraction has been implicated in disorders such as in Thromboangiitis obliterans(109), Polycythemia Vera(110), severe coronary artery disease(111) and chest pain associated coronary artery disease (112). The difficulty however is in understanding whether these changes at the bulk clot contraction are due to the platelets themselves or due to changes in the biochemical or mechanical microenvironments. Specifically, in these disease states is this impairment or enhancement of contraction due to increases in platelet count, alterations in the fibrin content or stiffness, and/or due to abnormal concentrations of coagulation factors. As such, new single and aggregate platelet technologies have started to decouple disorders that are due to impaired platelet mechanics. As a start, and unsurprisingly measuring single platelet, we and other groups have shown that patients with cytoskeletal disorders such as May Hegglin Disorder(74, 113) and Wiskot Aldrich Syndrome(74)

have impaired single platelet contraction forces. Additionally with our high throughput single platelet contraction system, we showed that patients with symptomatic bleeding but completely normal clinical hemostatic tests have impaired platelet contraction force, this in turn connecting impaired platelet nanomechanics to a bleeding phenotype(74) (Figure 5).

Leveraging our knowledge of platelet contraction, our group has leveraged the ability of platelets to generate forces to break open fibrinogen coated microcapsules to deliver hemostatic agents with implications for patients with hemophilia(116). Additionally, decreased platelet aggregate forces have been shown to be found in trauma patients that require blood transfusions (99). This further highlighting the clinical importance of decoupling platelet mechanical behavior from bulk clots. Not only have these systems allowed for advancements in our knowledge of platelet influence on disease pathophysiology, but also on how various drugs can alter platelet mechanics such as in patients taking aspirin and abciximab(99). More recently, the importance of Piezo receptors (117) as a mechanosensitive ion channel that responds to stretching and shear stress has shown to have relevance in platelets(118, 119) particularly clinical relevance. Specifically, Piezo1 has been shown to mediate a thrombotic pathway in the platelets of patients suffering from diabetes(120) as well as in hypertension(121). As such, it is evident that new platelet mechano-pathways need to be explored as they may have important clinical relevance. Additionally and important to note when interpreting results from animal disease models and anti-platelet drugs, that platelet biophysical behavior varies between animal species, noting that each species possess a unique single platelet biophysical signature (92).

Concluding Remarks

Platelets demonstrate biomechanical properties that are integral to hemostasis and thrombosis. The platelet microenvironment is influenced by rheological properties that platelets sense through biomechanical cues of the surrounding milieu. Altered hemodynamic forces, shear stress, vascular injury, stiffness of the microenvironment and receptor/integrin and matrix protein interactions influence how platelets sense and respond to their mechanical microenvironment. Although we have made substantial progress in how individual platelets integrate in the myriad of the clot environment, sense their surroundings, and contract to restore hemostasis, many questions remain unanswered. Several groups have shown that platelet force ‘correlates’ with bleeding and/or thrombosis and as such are linking clinical symptomology to mechanics (Table 1, Figure 4). However, what is important to confirm is whether impaired platelet force is correlated to bleeding or is actually causing symptomatic bleeding and what are the mechanisms behind the impairment in cellular force.

Another area of important exploration is the role of viscosity in a developing clot, the field has made substantial progress on how platelets respond to varying elasticity but the role of viscosity in the viscoelastic clot microenvironment remains poorly explored. What key advantage does the continuously changing viscosity give to a developing clot and how are platelets responding to these changes? This will be important to investigate and will lead to a more accurate understanding of how platelets are interacting with a viscoelastic microenvironment that is constantly changing/remodeling. Additionally, and subcellularly, the identification of the biomechanical pathway leading to the intermediate

state of the integrin $\alpha 2\beta 3$ (GPIIb/IIIa) has provided us with an initial understanding of integrin affinity maturation, however further studies are necessary to help us understand the biological and clinical importance of this intermediate state. Are integrin conformation states affected or altered in clinical disorders? Knowing that antibodies and platelet inhibitors can stabilize integrins into specific conformations(122) and that termination of integrin $\alpha 2\beta 3$ (GPIIb/IIIa) tension is coupled with the exposure of phosphatidylserine and cessation of contraction(76), do certain disorders stabilize integrin conformations and do these stabilized conformations lead to impaired platelet function and aberrant mechanotransduction? Finally, in every contractile cell including platelets, the role of MLCK and Rho kinase pathways has been well characterized, but platelets still produce contraction forces and still adhere to matrix protein coated surfaces while these pathways are inhibited, and as such these pathways are not telling the complete story. Similarly to the recent Piezo1 discoveries (118, 119), it will be important to investigate what other pathways are driving the initiation and propagation of platelet contraction and mechanics.

Taken collectively, investigations into platelet mechanotransduction will provide important insights into numerous clinical and biological phenomena. Specifically, further investigation at not only the single cell level, but the subcellular integrin level will improve our knowledge of the pathways that govern mechanical translation, the clinical disorders that are affected by aberrant mechanotransduction, the link between single platelet biomechanics and the mechanics that are occurring within the bulk clot microenvironments.

Acknowledgements

The authors are grateful to colleagues and collaborators for critical comments on this review and contributions to concepts presented. Financial support for this work was provided by a National Institutes of Health grant F31HL160210 (to O.O.), a National Institutes of Health grants T32HL139443-3 (to S. A.), R01 HL130918 (to W.A.L.), and R35HL145000 (to W.A.L.)

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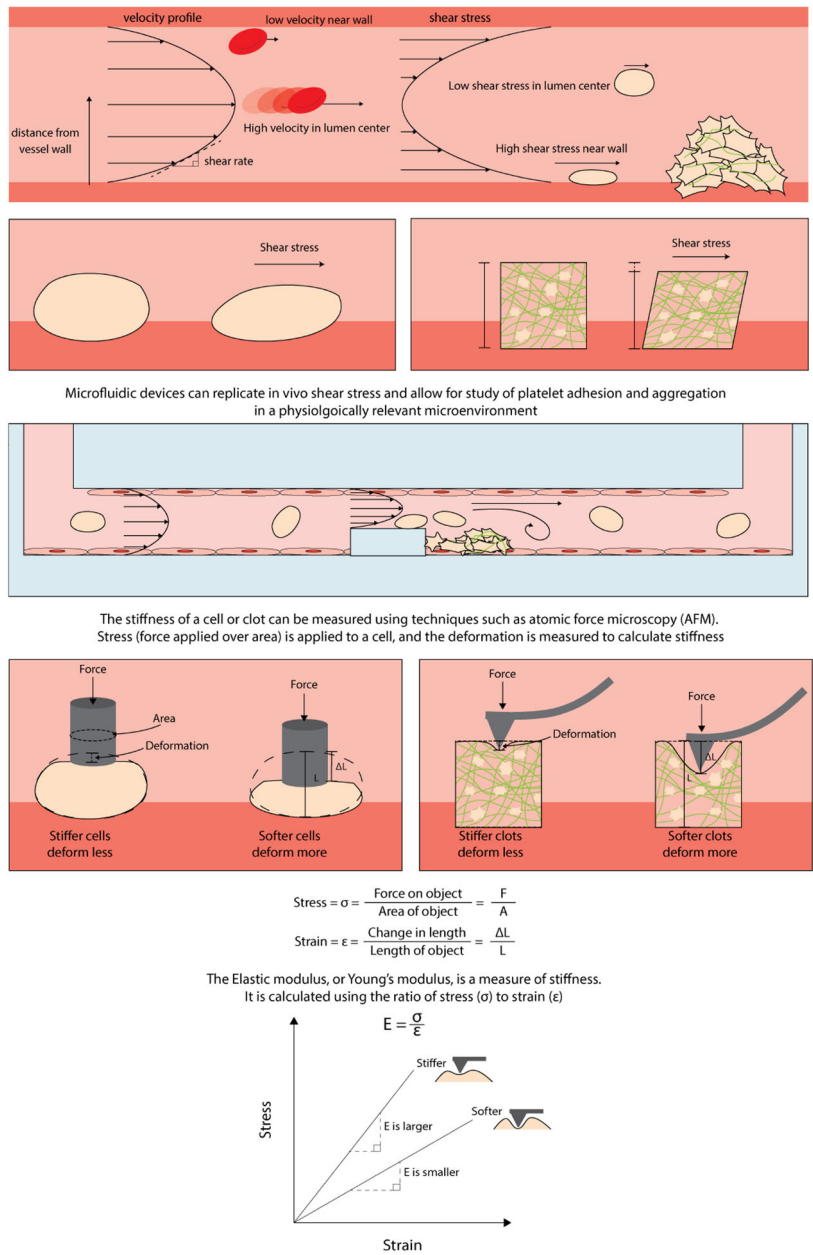
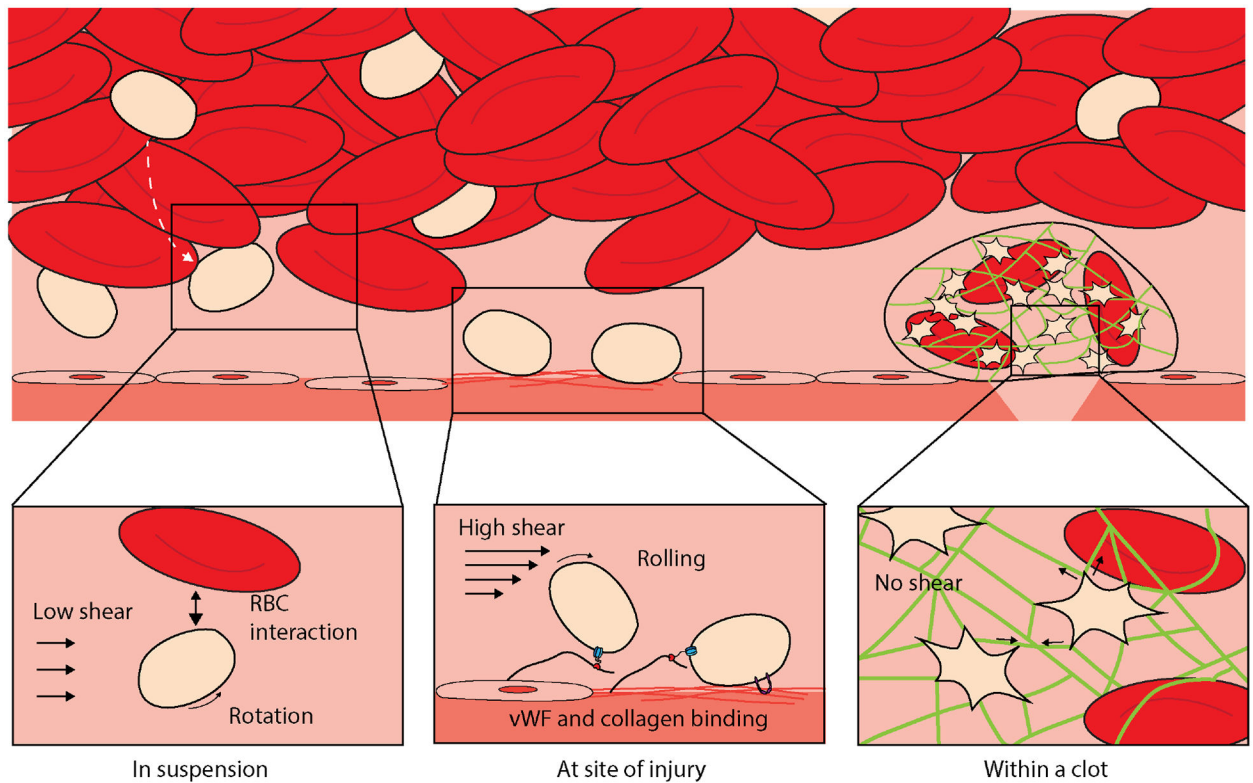


FIGURE 1.

Biophysics of shear flow and cell stiffness. Fluid flowing through a blood vessel reaches a steady state with a parabolic velocity profile. Shear rate is the change in velocity as the fluid distance from the vessel wall increases. Shear stress is a measure of how much force is acting on an object and is proportional to shear rate and fluid viscosity. Platelets aggregate with fibrin to form a network to develop a clot. The ability to control geometric constraints and endothelialize microfluidics has enabled *in vitro* studies that closely mimic the *in vivo* microenvironment. Clot stiffness changes over the course of contraction and deforms as platelets mechanically remodel the fibrin network.

**FIGURE 2.**

Biomechanical platelet interactions with the microenvironment. When platelets are in suspension in circulation, they not only move in the direction of the flow but also rotate and are subjected to mechanical interactions with red blood cells, which “push” them to the periphery. After vascular injury occurs, the extracellular matrix (collagen, laminin, and fibronectin) is exposed, and platelets in a high-shear environment bind and tether to von Willibrand factor and bind to collagen to begin thrombus formation. Following this, platelet activation and aggregation occur with signaling of mechanical and biochemical pathways. This subsequently leads to platelet plug formation and dot formation to dramatically shrink and stabilize the thrombus.

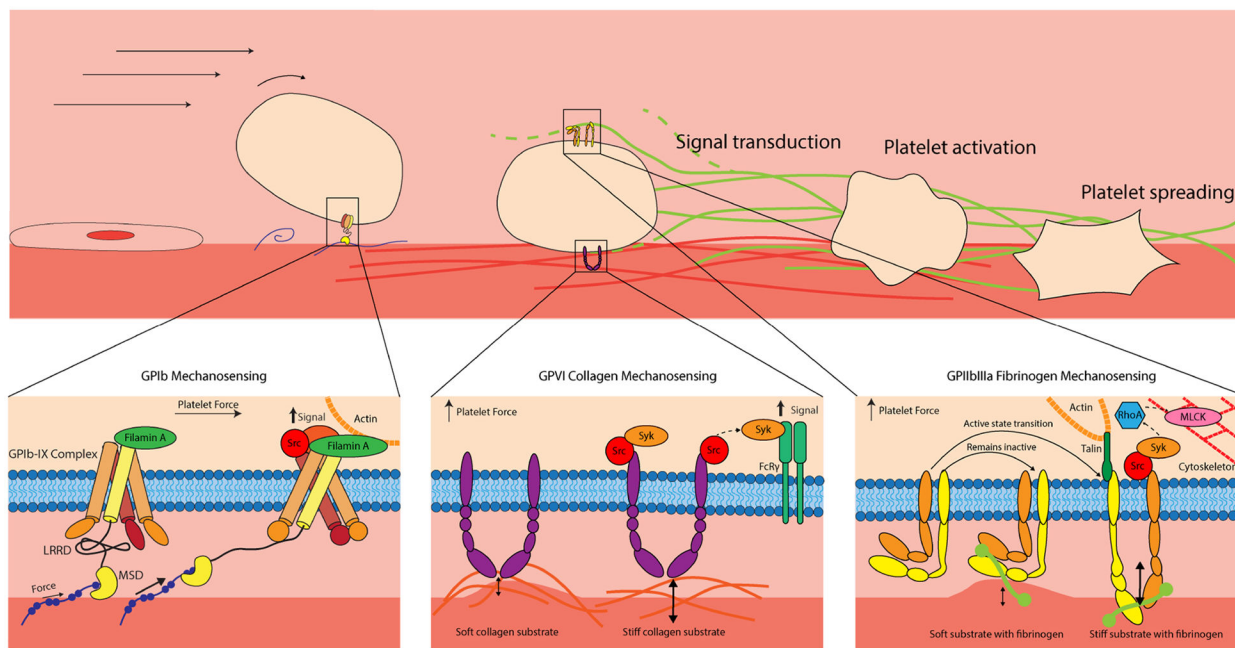


FIGURE 3. Platelet mechanotransduction occurs in all aspects of hemostasis after injury. Glycoprotein (GP)Ib mechanosensing: GPIb binds to von Willibrand factor and leverages its mechanosensory domain to activate platelets. GPVI collagen mechanosensing: GPVI interacts with collagen to activate platelets and support stable adhesion, responding to stiffness in the mechanical microenvironment. GPIIb/IIIa fibrinogen mechanosensing: The integrin $\alpha_{IIb}\beta_3$ (GPIIb/IIIa), the most abundant receptor on platelets, interacts with fibrin(ogen) and responds to changes in the developing clot microenvironment.

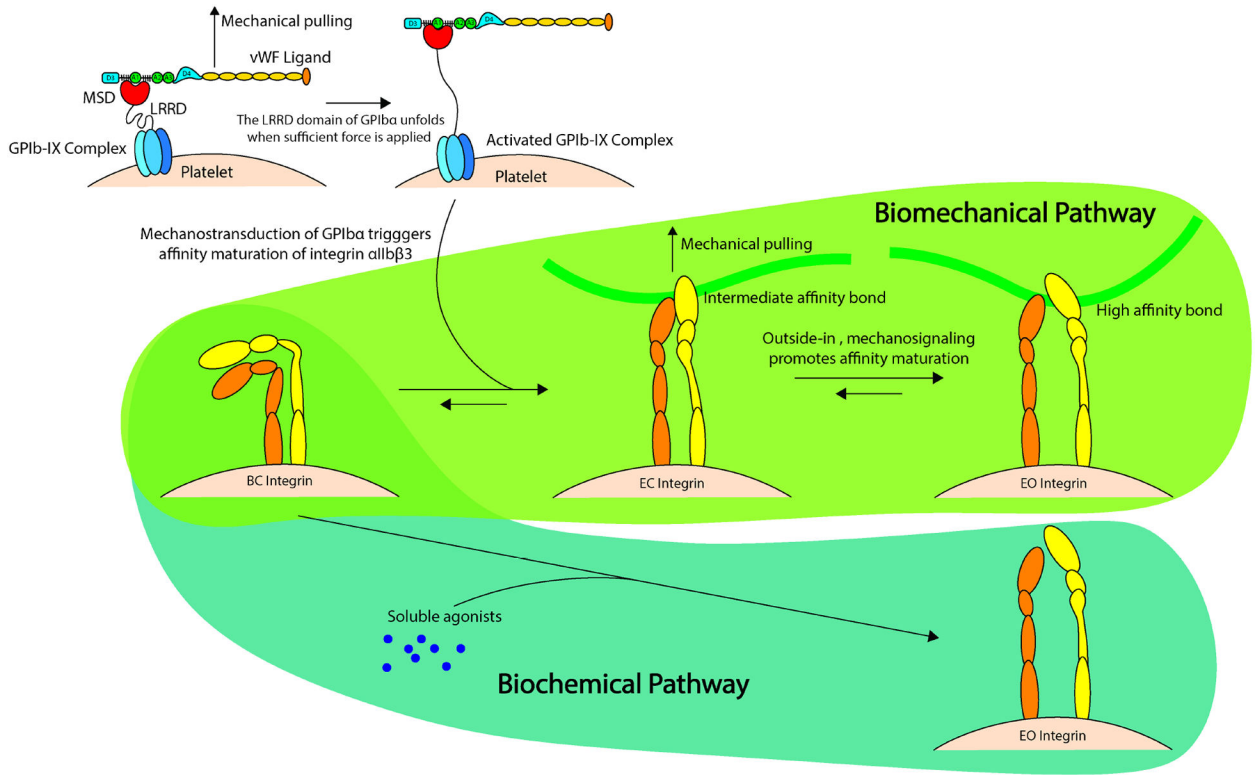


FIGURE 4. Platelet mechanotransduction demonstrated using the “trigger” model of glycoprotein GPIb-IX signaling and integrin $\alpha_{IIb}\beta_3$ affinity maturation. First, mechanoreception occurs by mechanical pulling force applied by von Willibrand factor on GPIba to unfold. Mechanoreception is demonstrated by leucine-rich repeat domain engaging with GPIba. This leads to mechanotransmission along the GPIba macroglycopeptide stalk and transfers this signal via mechanotransduction to induce platelet activation via the biochemical pathway (soluble-agonist dependent) and biomechanical pathway. The biomechanical pathway upregulates integrin $\alpha_{IIb}\beta_3$ from the inactive state (bent closed) to the intermediate state (extended closed). Outside-in signaling further promotes affinity maturation to the high-affinity state (extended open integrin conformation).

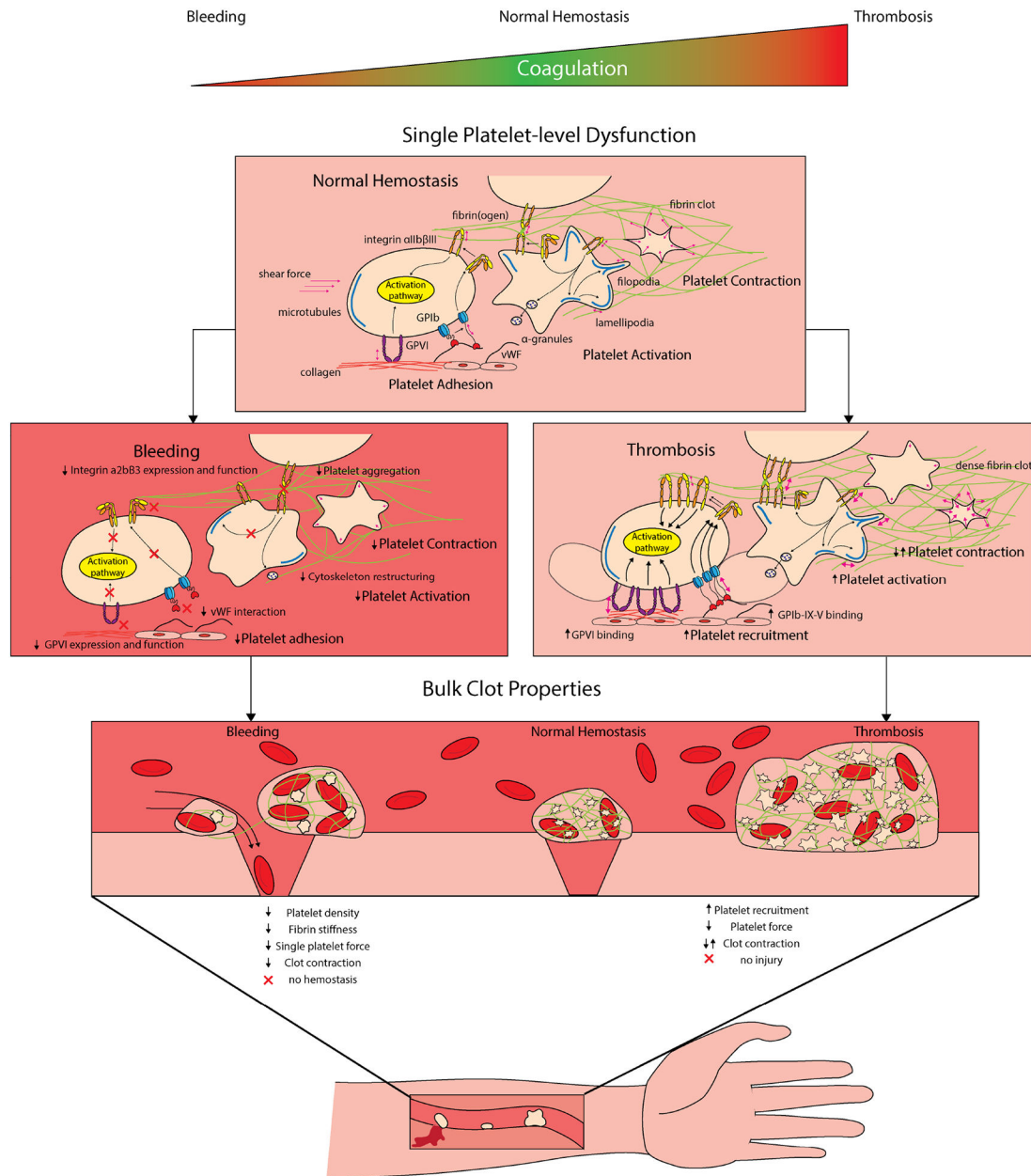


FIGURE 5. Aberrant hemostasis occurs when there is too little clotting (bleeding) or too much clotting (thrombosis), wherein platelet dysfunction can lead to both disease processes. At the single-platelet level, decreased platelet activation or interactions with exposed extracellular matrix proteins can lead to deficiencies at the bulk clot level, causing decreases in platelet density and decreases in contraction force, leading to impaired hemostasis. Alternatively, platelet preactivation leads to enhanced recruitment, leading to thrombosis. Interestingly, both increases and decreases in bulk clot contraction force have been implicated in thrombosis. Consequently, more thorough exploration is necessary to determine the reasoning as to why in some disorders, both increased and decreased forces leads to thrombosis.

Table 1:

Disorders linked to mechanical platelet dysfunction

Disorder	Platelet Mechanical Insights	Reference
Sickle Cell Disease	Decreased bulk contraction force	(103)
Asthma	Decreased bulk contraction force	(104)
Lupus	Decreased bulk contraction force	(105)
Acute ischemic stroke	Decreased bulk contraction force	(106)
Covid-19	Decreased bulk contraction force	(114)
Trauma	Decreased aggregate and bulk contraction force	(99) (107)
Thromboangiitis obliterans	Increased bulk contraction force	(109)
Polycythemia Vera	Increased bulk contraction force	(110)
Severe coronary artery disease	Increased bulk contraction force	(111)
Chest pain associated coronary artery disease	Increased bulk contraction force and increased clot elastic modulus	(112)
May Hegglin Disorder	Decreased single platelet contractile force	(74, 113)
Wiskot Aldrich Syndrome	Decreased single platelet contractile force	(74)
Symptomatic Bleeding	Decreased single platelet contraction force	(74)
type 2B von Willebrand's Disease	Enhanced mechanical activation of GPIb leading to platelet clearance	(49)
Glanzmann's thrombasthenia	Impaired platelet adhesion to fibrinogen	(67, 68)
Bernard-Soulier syndrome	Impaired adhesion to vWF	(47)
GPVI deficiency	Impaired platelet response to collagen	(115)
$\alpha_2\beta_1$ deficiency	Impaired platelet response to collagen	(83)