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## Advances in Imaging Mass Spectrometry for Biomedical and Clinical Research

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### Abstract

Imaging mass spectrometry (IMS) allows for the untargeted mapping of biomolecules directly from tissue sections. This technology is increasingly integrated into biomedical and clinical research environments to supplement traditional microscopy and provide molecular context for tissue imaging. IMS has widespread clinical applicability in the fields of oncology, dermatology, microbiology, and others. This review summarizes the two most widely employed IMS technologies, matrix-assisted laser desorption/ionization (MALDI) and desorption electrospray ionization (DESI), and covers technological advancements, including efforts to increase spatial resolution, specificity, and throughput. We also highlight recent biomedical applications of IMS, primarily focusing on disease diagnosis, classification, and subtyping.

### Keywords

Imaging Mass Spectrometry; Clinical Mass Spectrometry; Matrix-Assisted Laser Desorption Ionization; Desorption Electrospray Ionization; Direct Tissue Analysis

## 1. Introduction

Mass spectrometry (MS) is an invaluable analytical tool for biomedical research and clinical applications due to its high chemical specificity and unparalleled sensitivity.<sup>1</sup> When coupled to chromatography, including liquid (LC) and gas chromatography (GC), MS is routinely

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#### Declaration of interests

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used to characterize biofluids, such as blood, urine, and plasma.<sup>2,3</sup> While these analyses are regarded as the gold standard for guiding modern patient care, they require rigorous sample preparation and pre-treatment, as well as lengthy analysis time. This presents a challenge to accommodate the growing need for real-time assessment of biological specimens in clinical practice. Additionally, traditional chromatography-based MS analyses lack spatial awareness, often critical for tissue-based diagnostics.<sup>2,3</sup>

Spatially driven MS technologies, such as imaging mass spectrometry (IMS), can be used to visualize molecular distributions within tissue sections in an untargeted manner.<sup>4</sup> Many IMS approaches follow a similar workflow to traditional histology, allowing IMS to be easily integrated into pathology-related research for deeper molecular insight.<sup>5</sup> This review summarizes recent advances in IMS instrumentation and methods to increase spatial resolution, specificity, throughput, and analyte coverage. We also highlight current biomedical and clinical applications of IMS, with a primary focus on studies intended to supplement histopathological analyses, including advances in disease diagnosis, classification, and subtyping.

## 2. Advances in Modern IMS

In recent years, numerous IMS surface sampling technologies have been advanced for improved spatial interrogation of tissue samples (Table I). These technologies differ in instrumental features, such as ionization source and operation principles; however, their workflows remain similar. A typical IMS experiment begins with tissue sectioning and mounting onto a substrate (typically a glass slide) followed by sample preparation, which is unique to each imaging platform and analysis type but can include tissue washing, application of reagents (e.g., enzymes or derivatization reagents), and matrix application. Advancements in IMS technology for biomedical research have focused on improving spatial resolution, increasing throughput, and enhancing molecular coverage. With improved analytical capabilities, parallel efforts to computationally link IMS and histological information have emerged. Herein, recent examples of how machine learning is guiding the translation of IMS technologies into clinical workflows will be highlighted. Finally, while improvements in sample preparation and matrix selection have also been integral to modern IMS,<sup>6,7</sup> we will focus on instrumental advances which have improved image quality, reproducibility, and throughput.

### Spatial Resolution and Throughput

Matrix-assisted laser desorption/ionization (MALDI) and desorption electrospray ionization (DESI) IMS have extensively been applied to clinical tissue analysis.<sup>8–10</sup> MALDI utilizes a focused UV laser for the desorption/ionization of matrix-coated tissue samples, offering an unparalleled combination of molecular coverage and spatial resolution for IMS enabling analysis of molecular classes ranging from small metabolites and lipids to peptides, glyfvcans, and proteins.<sup>10</sup> MALDI IMS can routinely achieve high spatial resolutions, which is crucial for the interrogation of small clinical samples, such as needle biopsies, and for linking IMS data to specific cellular features. MALDI IMS is rapidly approaching single-cell imaging capabilities, with recent publications reporting <10  $\mu\text{m}$  spatial resolutions.

Higher spatial resolutions ( $<1\ \mu\text{m}$ ) have been demonstrated with the optimization of custom front-side laser systems<sup>11</sup> and the development of transmission geometry<sup>12</sup>, which redirects the laser path to irradiate the tissue through the back of the slide. The sampled area per pixel decreases with higher spatial resolution, therefore decreasing the number of molecules sampled in a given pixel. To overcome this, instrumental approaches, such as continuous accumulation of selected ions (CASI), which enriches ions in a narrow mass window, and MALDI-2, which uses a second laser for postionization of the MALDI plume, can be used to enhance signal intensity.<sup>26</sup> Studies combining transmission geometry and MALDI-2 have achieved imaging at subcellular resolution ( $<1\ \mu\text{m}$ ) and have been applied to study clinically relevant samples.<sup>27</sup> DESI deflects a spray of charged droplets onto the tissue surface to extract analytes for detection by mass spectrometry.<sup>28</sup> It is appealing for clinical applications because it can utilize nondestructive extraction solvents, such as water, and can be performed under atmospheric pressure without any sample preparation. Solvent-based IMS techniques like DESI require a liquid droplet deposition on the sample, limiting achievable spatial resolution to 50 – 250  $\mu\text{m}$  in most cases.<sup>29</sup> Optimization of solvent flow rates, composition, spray-to-sample distance, and other parameters have been explored to improve spatial resolutions.<sup>29</sup> In one example, modifications to the DESI sprayer design included the addition of a capillary positioning device, a gas nozzle with an aperture of 400  $\mu\text{m}$ , and a solvent capillary with a tapered tip and a larger outer-to-inner diameter ratio – 360  $\mu\text{m}$  – 40  $\mu\text{m}$ , as compared to 150  $\mu\text{m}$  – 50  $\mu\text{m}$ .<sup>30</sup> They report improved spray focusing and stability, enabling 20  $\mu\text{m}$  spatial resolution imaging. Nano-DESI is a similar liquid extraction-based IMS approach in which analytes are desorbed from the tissue surface via a continuous liquid junction maintained between two capillaries. Ions are subsequently introduced to the mass spectrometer via electrospray ionization.<sup>31</sup> This approach has allowed higher spatial resolution and throughput imaging under ambient conditions. Recently, Laskin and coworkers have achieved  $\sim 10\ \mu\text{m}$  spatial resolutions with nano-DESI using an improved microfluidic probe, forming a smaller liquid bridge on the tissue's surface.<sup>16</sup>

Increased IMS spatial resolution has also motivated development efforts for improved image acquisition speed. Instrument improvements to enhance throughput include modifications to stage mechanics, development of lasers with high repetition rates, implementation of continuous raster sampling for MALDI-TOF instruments, and optimized sample preparation and data generation workflows. Improvements in stage mechanics and laser optics have led to the development of commercial platforms capable of high acquisition rates, such as the RapifleX Tissue typer (Bruker Daltonics), which utilizes a 10 kHz laser and is capable of acquiring  $>25$  pixels/sec. Modified workflows using this instrument have been demonstrated to approach  $\sim 50$  pixels/sec.<sup>32,33</sup> Others have developed high throughput IMS instruments that utilize continuous raster sampling where the sample stage is moved continuously while sampling with either a laser or liquid droplet. Spatial resolution is defined by the sampling rate, the sample stage velocity, and the distance between line scans. Continuous raster sampling by MALDI has been shown to generate up to 50 pixels/sec.<sup>33,34</sup> More recently, a laser scanning technique has been used to achieve 100 pixels/sec.<sup>35</sup> Most DESI imaging experiments are performed as continuous raster experiments with data acquisition rates of 30 pixels/sec routinely achievable.<sup>36</sup> These technologies and similar advances to increase

throughput are critical for large-scale biomedical research projects and for incorporating IMS into clinical settings for real-time tissue interrogation.

### Analyte Coverage, Identification, and Quantitation

Molecular coverage, specificity, and quantitation are critical for robust MS analysis. Time-of-flight (TOF) and quadrupole time-of-flight (qTOF) are the most used mass analyzers in IMS today. TOF instruments offer the widest detectable mass range ( $>100$  kDa)<sup>37</sup>, while qTOF instruments provide resolving powers of  $\sim 50\,000$  and  $<5$  ppm mass accuracy.<sup>38</sup> Both systems enable high throughput molecular imaging (30–100 pixels/sec). Fourier transform mass spectrometers, such as Fourier transform ion cyclotron resonance (FT-ICR) MS<sup>39</sup> and orbitrap MS, offer much higher resolving powers ( $>100\,000$ ) and improved accurate mass ( $<1$  ppm) and are increasingly used for clinical sample analysis.<sup>3</sup> These platforms are ideal for separating and identifying analytes with similar  $m/z$  values; however, they remain costly and have lengthy data acquisition times.<sup>40</sup> Alternatively, incorporating orthogonal separation techniques, such as ion mobility spectrometry that provides a gas-phase separation of ions, can increase sensitivity and specificity in IMS experiments.<sup>41,42</sup> For example, high-field asymmetric ion mobility spectrometry (FAIMS) has been integrated with DESI IMS to decrease chemical noise and improve signal-to-noise ratios.<sup>41,43</sup> Higher resolution ion mobility devices, such as traveling wave ion mobility spectrometry (TWIMS) and trapped ion mobility spectrometry (TIMS), have also been used with imaging mass spectrometry to elucidate isobaric/isomeric species in direct tissue analyses.<sup>41,42,44</sup> Furthermore, collision cross section (CCS) values, a descriptor of the structure and three-dimensional conformation of the gas phase ions, can be derived with ion mobility, aiding in more accurate analyte identification. Finally, tandem MS ( $MS^n$ ) can be performed directly on tissue to provide analyte structural information based on detected fragments.<sup>45</sup> More advanced fragmentation techniques, such as ultraviolet photodissociation<sup>46</sup> and ozone-induced dissociation<sup>47,48</sup>, can also provide detailed structural information, such as double bond position and stereochemistry, making these techniques more suitable for targeted analyses.<sup>45</sup>

Although relative quantitation in IMS is routine, absolute quantitation has been a significant challenge in the field of IMS, owing to the high pixel-to-pixel variability, differences in analyte extraction efficiencies, and ion suppression effects.<sup>49</sup> Absolute quantitation is most commonly achieved using internal standards against which analyte signals are calibrated.<sup>50</sup> Internal standards can be sprayed, spotted, or otherwise deposited onto the tissue surfaces.<sup>51</sup> In MALDI IMS workflows, this can be done prior to (or with) the matrix application. The internal standard can also be included in the extraction solvent in DESI IMS applications.<sup>52</sup> There are numerous ways of incorporating standards, such as using a single standard and constructing an on-tissue calibration curve; however, mixtures of internal standards are often preferred for quantitation, as they are selected to be structurally similar to various analytes of interest. Alternatively, computational approaches for quantitation have been explored, including calculating matrix correction factors and normalizing against other quantitative approaches.<sup>49,52</sup> Despite significant progress, quantitation remains one of the most significant limitations of IMS; a more in-depth exploration of the topic can be found elsewhere.<sup>49,52,53</sup>

IMS can be used to study a wide range of analytes, including small metabolites, lipids, peptides, glycans, and proteins. MALDI and DESI efficiently ionize metabolites and lipids without significant sample preparation or instrument modifications.<sup>54</sup> Untargeted imaging of larger molecules, such as proteins and glycans, is more challenging and requires additional sample preparation steps.<sup>55–57</sup> Aberrant protein glycosylation has been linked to numerous health conditions; therefore, characterizing the glycome with spatial specificity is an active area of interest for clinical and pharmaceutical applications alike. This topic is covered in more detail in the following reviews.<sup>58,59</sup> Similarly, spatial interrogation of proteins, protein-ligand complexes, proteoforms, and various modifications can provide critical insight into numerous biological processes.<sup>60</sup> Intact MS-based protein imaging was first achieved with MALDI IMS.<sup>61</sup> This approach offers a broad mass range of approximately 500 Da to over 80 kDa<sup>62</sup>, depending on the instrument platform. However, MALDI-generated ions have lower charge states ( $\leq 3$ ), greatly reducing gas-phase fragmentation efficiency and hindering direct top-down protein identification.<sup>60,63</sup> Extraction-based approaches like DESI and nano-DESI generate higher charge-state ions and are particularly well suited for intact protein analysis. In a recent example, nano-DESI was used to map proteins in rat brain tissue at  $<10\mu\text{m}$  spatial resolution with oversampling.<sup>64</sup>

To improve protein coverage in IMS experiments, protein imaging can also be accomplished by bottom-up proteomics following on-tissue digestion.<sup>65</sup> In an imaging context, simultaneously achieving robust protein identification, high protein coverage, and high spatial resolutions with either approach remains challenging. Spatial profiling techniques, such as laser capture microdissection (LCM)<sup>66</sup> and liquid-extraction surface analysis (LESA)<sup>67</sup> can be used to probe specific tissue locations for in-depth protein analyses.<sup>63</sup> Once proteins are extracted, the sample can be subjected to either bottom-up or top-down workflows compatible with downstream LC-MS/MS.<sup>68</sup> These approaches offer high molecular coverage and robust quantitation but at limited spatial information. More recently, nanodroplet processing in One Pot for Trace Samples (NanoPOTS) has emerged as a technique for working with smaller sample amounts, allowing the mapping of protein abundance with improved sensitivity and at higher spatial resolutions with LCM LC-MS/MS workflows.<sup>69</sup> IMS and spatial profiling approaches can be used in parallel to maximize information gleaned from precious tissue samples. Modern multimodal imaging workflows can use IMS data to drive spatial omics (proteomics, glycomics, transcriptomics, *etc.*) data collection from specific areas of interest to better understand localized molecular biology within tissue microenvironments.

## Tissue Processing and Sample Preparation

In addition to instrumental considerations, the information gleaned from a biological system is dictated by the nature of the sample itself and how the specimen is prepared. Surgical samples are used for intraoperative diagnosis, stored for post-surgical analysis, and for developing and validating new diagnostic methods. Common clinical tissue samples include biopsies (needle, wedge), excised tumors, smears, and whole organs.<sup>40</sup> Upon excision, samples can be fixed or flash frozen and embedded to preserve tissue morphology and aid in their handling. Both tissue fixation and embedding can affect postoperative IMS analysis and profoundly impact data quality.<sup>40,70</sup> For example, fixation materials, such as formalin

and paraformaldehyde, alter the chemical composition of the samples through reactions such as cross-linking and denaturing.<sup>70</sup> Similarly, common embedding materials, such as paraffin and optimal cutting temperature (OCT) gel, can introduce ion suppression effects in IMS analysis.<sup>71</sup> Formalin-fixed paraffin-embedded (FFPE) tissue blocks have long been used for immunohistochemical analysis and are ideal for spatial proteomics and glycomics; however, this embedding material and the washing steps required for deparaffinization significantly hinder lipid and small metabolite detection in MALDI IMS. In addition to the sample procurement and preservation, sample preparations vary by the instrument employed and the target analyte class. These considerations range from the mounting substrate to sample pre-treatment, such as washing, chemical derivatizations, and type of matrix employed, if any.<sup>9</sup> For example, protein imaging requires a series of washes to remove salts and lipids that introduce ionization suppression, and some approaches also require on-tissue enzymatic digestion.<sup>60</sup> Similarly, glycan imaging requires lengthy sample preparation, including antigen retrieval and enzymatic digestion.<sup>58</sup> Comprehensive reviews of sample preparation considerations and their impact on IMS analysis can be found elsewhere.<sup>1,6,7,40</sup>

### 3. Multimodal Data Integration and Visualization

Histology uses numerous stains and dyes to reveal the morphological and cellular composition of tissues. While these approaches are highly informative and routinely used by pathologists for diagnosis in clinical settings, they provide only limited molecular information.<sup>5,72</sup> For example, immunohistochemistry (IHC) and fluorescence *in situ* hybridization (FISH) are targeted approaches to map the spatial distributions of specific protein or RNA markers in tissue sections.<sup>73,74</sup> Untargeted molecular investigations, such as with IMS, can reveal spatially resolved molecular features but do not provide information on cellular and morphological structures. When collectively employed in multimodal imaging experiments, these integrated approaches greatly increase the information obtained from biological systems, enabling molecular histology and furthering next-generation molecular pathology practices.<sup>5,72</sup>

Correlation of IMS data with stained microscopy can be achieved through computational approaches, such as multimodal registration workflows, as demonstrated by Patterson et al.<sup>75</sup> and Race et al.<sup>76</sup> (Figure 1). Patterson et al.<sup>75</sup> used autofluorescence microscopy and computational registration to link IMS and microscopy data. An advantage of this approach is the ability to register serial tissue sections that have undergone different analyses with varying spatial resolutions (Figure 1A). Building on image registration, Van de Plas et al.<sup>77</sup> demonstrated a predictive imaging modality, termed data-driven image fusion, by combining hematoxylin and eosin (H&E) stained microscopy images with IMS using highly multivariate linear regression (Figure 1B). The resulting model enables the prediction of IMS data to higher spatial resolution (*i.e.*, spatial sharpening) and in tissue areas not analyzed by IMS (*i.e.*, out-of-sample prediction). Race et al.<sup>76</sup> combined IMS, histological staining, and deep learning for automatic annotation of histology images and annotation transfer between two modalities. The workflow was demonstrated on data generated from multiple IMS technologies, including MALDI, DESI, and rapid evaporative ionization mass spectrometry (REIMS) (Figure 1C).

A crucial aspect of obtaining biological insight from multimodal data is the development of computational workflows to interpret large datasets. Classification models require “training” datasets to build models and “testing” datasets to evaluate their performance. The performance is measured by the ability to (1) correctly differentiate disease and healthy cases (accuracy), (2) identify the diseased cases correctly (sensitivity), and (3) determine the healthy cases correctly (specificity), where these characteristics are reported in percentages.<sup>78</sup> Pathologists can manually interpret stained sections to annotate important features, such as tumors, tumor margins, and normal tissues. This provides meaningful labels for the training data sets, which can be superimposed onto the molecular data via multimodal image registration.<sup>15,79</sup> In the case of biomarker discovery, mass spectra from tissue regions labeled as “tumor” and “control” are compared to reveal mass spectral differences. Once candidate signals ( $m/z$  values) are detected, statistical tests, such as Student’s t-test and analysis of variance (ANOVA), are performed to determine if the chemical signal significantly differs between the two groups.<sup>5</sup> When building classification models based on multiple mass spectral differences, supervised multivariate analyses, such as least absolute shrinkage and selection operator (LASSO) and partial least squares regression, are performed.<sup>80</sup> These approaches are intended to predict tumor class and tissue labels based on training sets. Recently, Tideman et al.<sup>81</sup> demonstrated automated biomarker discovery by interpreting classification models constructed from IMS data. This approach offers a spatially specific method for determining important molecular features across large cohorts of biological specimens.

The power of integrating molecular and cellular observations has been demonstrated in numerous applications, including in precision medicine, diagnosis, and biomarker discovery.<sup>29,36</sup> For example, recent publications by Schwamborn and coworkers<sup>82,83</sup> used molecular information from MALDI IMS to supplement cellular observations for a more comprehensive understanding of pancreatic tumors. Bollwein et al.<sup>82</sup> used MALDI IMS and machine learning models to differentiate between pancreatic ductal adenocarcinoma and cholangiocarcinoma tumors, which are extremely difficult to distinguish based on morphology alone. The machine learning models, built on tryptic peptide data from tissue microarrays, correctly classified more than 80% of cases. Similarly, Gonçalves et al.<sup>83</sup> identified molecular differences between primary pancreatic ductal adenocarcinoma and distant metastases, the presence of which can affect treatment options for patients. Multiple candidates for protein biomarkers of disease progression and development of distant metastases were identified, and the classification model reported a > 90% accuracy. Both studies showcase the combination of IMS and histological studies for a more comprehensive understanding of disease states.

Building robust prediction models to discern disease states requires significant sample cohorts and rigorous validation with currently employed tissue diagnostic methods. Tissue microarrays and biopsies from large cohorts of diseased and normal patients are ideal for evaluating not only model performance but also the robustness and repeatability of the employed analytical technique. In a recent study, Deininger et al.<sup>84</sup> conducted a multi-site study to examine the reproducibility of MALDI imaging techniques for tissue classification. The study developed a standard operating procedure that included histological annotation and an optimized data pre-processing pipeline designed to remove technical variation while

retaining biological information. The authors report that using the standard procedure increased classification accuracy and overall robustness in multi-site studies. Similar large-scale studies will be needed to fully incorporate spatially oriented mass spectrometry techniques in the clinical setting.

Unsupervised machine learning strategies can also be employed to extract valuable information from highly dimensional IMS datasets. These strategies are generally explorative and seek to uncover trends and correlations within IMS datasets without *a priori* information (*i.e.*, labels).<sup>85</sup> Unsupervised methods include component analyses and clustering. Briefly, component analyses, such as principal component analysis and non-negative matrix factorization, are intended to reduce multidimensional IMS data and reveal underlying trends in the datasets.<sup>5,15,80</sup> Clustering methods, such as hierarchical clustering and *k*-means, partition pixels based on mass spectral similarities and reveal the molecular ions that drive the resulting groupings.<sup>5,80</sup> Clusters are often color-coded and visualized as image segments. These methods are especially powerful when combined with traditional microscopy techniques, as they enable the discovery of molecular profiles with distinct spatial patterns (*i.e.*, segments) that can be linked to specific morphological features.

There are both commercially available and open-source software solutions capable of analyzing and visualizing IMS data. Commercially available IMS software include SCiLS and FlexImaging (Bruker Daltonics), LipostarMSI (Molecular Discovery), and HDI (Waters). Free, open-source IMS processing solutions include MSIReader<sup>86</sup>, METASPACE<sup>87</sup>, and numerous R packages specific for IMS analysis (Cardinal<sup>88</sup>, MALDIquant<sup>89</sup>, and others<sup>90</sup>). As IMS workflows evolve to incorporate multimodal imaging data, new software solutions for multimodal data analysis and/or registration have emerged. For example, MZ mine 3 is open-source software that supports hybrid datasets, including LC-MS, ion mobility-MS, and IMS datasets.<sup>91</sup> Similarly, several tools for registration and alignment of IMS with other clinically relevant imaging modalities have emerged; these are summarized in recent review papers.<sup>92,93</sup>

#### 4. Clinical Applications of IMS

Perioperatively, histopathology methods, including frozen section analysis and imprint cytology, provide valuable diagnostic information. These strategies are often time-consuming, require expert pathologists for their interpretation, and may introduce unwanted freezing artifacts.<sup>5,94</sup> More advanced analytical approaches, such as IMS, can be integrated to provide complementary information in tumor diagnosis, prognosis, and margin assessment.<sup>29</sup> Beyond the clinical lab, IMS has played a vital role in the pharmaceutical field, aiding drug discovery and development.<sup>95,96</sup> Here, we showcase recent biomedical, clinical, and pharmaceutical applications of IMS, with a primary focus on MALDI and DESI. The reader is directed to the following reviews for a more in-depth look into the techniques not covered in this review.<sup>8</sup>

##### **Matrix-assisted Laser Desorption/Ionization Imaging Mass Spectrometry (MALDI IMS)**

MALDI is the most widespread IMS technology and has been used in numerous biomedical and clinical applications, including biomarker discovery, cancer diagnosis,



therapeutic testing, and microorganism identification.<sup>29</sup> In fact, MALDI MS is routinely employed in clinical microbiology to identify microorganisms in biological isolates, where rapid and precise pathogen identification is critical for selecting appropriate treatment.<sup>97</sup> MALDI MS can detect pathogens on a species level within minutes, offering a high-throughput alternative to conventional identification strategies that require lengthy incubation procedures.<sup>98</sup> Incorporating the spatial dimension with MALDI IMS offers a unique insight into the molecular species implicated at the host-pathogen interface and molecular alterations that occur during the course of an infection.<sup>99,100</sup> Such studies are integral in developing new therapeutics and understanding antibiotic resistance on a molecular level.<sup>5</sup>

MALDI IMS offers broad analyte coverage and is well-suited for the analysis of large biomolecules, such as proteins and glycans. Because of this, numerous studies have investigated alterations of protein and glycan signatures to identify disease states. For example, Capitoli et al.<sup>101</sup> demonstrated MALDI IMS as a complementary tool to cytopathology diagnosis of thyroid nodules based on proteomic signatures. Thyroid fine-needle aspirations were analyzed by MALDI IMS, and the probability of malignancy was mapped on a pixel-by-pixel basis. Although further work is necessary to systematically test these workflows on larger sample cohorts, this introductory study showed promising results in building a MALDI IMS-based proteomic diagnostic tool for thyroid cytopathology. In a more recent example, Ochoa-Rios et al.<sup>102</sup> used MALDI IMS to investigate changes in N-glycan composition in mouse and human liver tissues due to non-alcoholic steatohepatitis. N-glycan changes were detected even in early stages of the disease and could be used to identify progression before tissue damage was pathologically visible.

Similarly, recent studies have showcased MALDI IMS as a powerful diagnostic tool for cancer types that are particularly challenging to classify with histopathology alone. For example, Sommella et al.<sup>103</sup> used MALDI IMS to investigate salivary tumor tissues (Figure 2A–D). This tumor type's diverse morphological profile and cell types may not follow traditional observations that allow pathologists to differentiate malignant and benign tumors. Although this tumor type is difficult to characterize with conventional pathology practices, the authors successfully delineated normal and tumor tissue based on metabolomic and lipidomic signatures with a reported 95% accuracy. Janßen et al.<sup>104</sup> applied MALDI IMS and computational classification models to differentiate between the two most common non-small cell lung cancer tumor types – adenocarcinoma and squamous cell carcinoma (Figure 3E & 3F). This study exemplifies a successful transfer of classifiers developed on tissue microarrays to whole lung tissue sections, which are generated in routine clinical practices. These and similar studies not only elucidate molecular alteration due to disease but also pave the way for incorporating MALDI IMS in real-time clinical decision making.

Perioperatively, MALDI IMS can provide complementary diagnostic information. A proof-of-concept study by Calligaris et al.<sup>105</sup> investigated the use of MALDI IMS for near-real time pituitary tumor detection based on proteomic signatures. The authors demonstrated that MALDI IMS could successfully classify tumors by directly detecting excessive hormonal production from functional pituitary adenomas. Their analyses were performed in under 30 minutes, a timeframe compatible with guiding surgical decision making. As MALDI

IMS requires more extensive sample preparation, such as the deposition of the MALDI matrix, this step may lengthen analysis time. New workflows, such as implementing matrix pre-coated slides<sup>106</sup> and simplified sample preparation strategies, have been proposed to increase throughput significantly.<sup>107</sup>

MALDI IMS has also been employed to study drug metabolism, formulation, and delivery, among other pharmaceutical applications.<sup>95</sup> In a recent proof-of-concept study, MALDI IMS was used to determine if an inhaled therapy drug can effectively be delivered to the target therapeutic area within human lungs.<sup>108</sup> In this study, biopsies were taken from patients with confirmed intestinal lung disease after administering a single dose of nebulized ipratropium bromide. Biopsy sections were analyzed with MALDI IMS and histopathology; the data revealed that the drug co-localized with fibrotic regions in the samples, suggesting that drugs designed to treat pulmonary fibrosis could be administered via inhalation. More examples of MALDI IMS applied to pharmaceutical research and drug development can be found in the highlighted review.<sup>95</sup>

### **Desorption Electrospray Ionization Imaging Mass Spectrometry (DESI IMS)**

DESI IMS has been increasingly employed in cancer research for diagnosis, subtyping, staging, and surgical margin evaluation.<sup>29</sup> Target analyte classes for DESI IMS include metabolites, fatty acids, and lipids; however, modification of spray conditions and extraction solvent compositions have expanded this list to include proteins.<sup>109</sup> Robust classification models have been developed for distinguishing gastric cancer<sup>110</sup>, skin cancer<sup>111</sup>, breast cancer<sup>112</sup>, and others<sup>28</sup> to guide real-time surgical decision making. Of note, Vijayalakshmi et al.<sup>113</sup> used DESI IMS and a LASSO predictive model to identify diagnostic metabolomic signatures in clear cell renal cell carcinoma (ccRCC) from human nephrectomy specimens (Figure 3A & 3B). The authors report that combined indicators (baseline LASSO of differentially expressed metabolites and the ratio of glucose to arachidonic acid) can discriminate between cancer and normal tissue with 85.3% accuracy. In a similar study, Santoro et al.<sup>112</sup> used DESI IMS to investigate the metabolomic and lipidomic compositions of molecular subtypes of breast cancer. With similar modeling approaches, the authors could distinguish between invasive breast cancer and adjacent benign tissues, as well as between ductal carcinoma *in situ* and invasive breast cancer. In another recent study, Yang et al.<sup>114</sup> used DESI IMS and machine learning to determine the safe surgical resection distance and margin status of oral squamous cell carcinoma based on diagnostic lipid ions (Figure 3C & 3D). With this method, the authors report an overall prediction accuracy of 92.6%. Moreover, the total data acquisition and analysis procedure can be performed within 30 minutes, which is compatible with perioperative analysis timeframes.

Growing evidence suggests that intraoperative molecular investigation can provide additional information on surgical margins not revealed by histology. For example, in a study of pancreatic cancer margin detection by Eberlin et al.<sup>115</sup>, several tissue margins diagnosed as non-cancerous by histopathological evaluation were classified as cancerous based on a predictive model built upon metabolomic features. Although the disagreement of classification may be attributed to the error range in the DESI/LASSO analysis, it is possible

that molecular markers of pancreatic cancers could be detected prior to morphological alterations that are typically discerned by histopathology.

DESI IMS is perhaps the most promising IMS technique for translation into the surgical suite because it does not require any sample preparation and can be operated under ambient conditions.<sup>2,94</sup> DESI IMS offers high throughput analysis in applications where spatial resolution is not critical, such as analyzing surgical swabs and smears. For example, Pirro et al.<sup>116</sup> demonstrated DESI IMS for intraoperative diagnosis of glioma from brain tissue swabs from 10 different surgeries. They reported the detection of cancerous tissues with 93% sensitivity and 83% specificity based on lipid and metabolite signals. More recently, Brown et al.<sup>117</sup> monitored 2-hydroxyglutarate ion intensities along with lipid and metabolite profile changes for intraoperative glioma diagnosis. The authors report the sensitivity, specificity, and accuracy of predicting disease status as 63%, 83%, and 74%, respectively. Overall, the authors successfully identified isocitrate dehydrogenase mutation status, glioma diagnosis, and intraoperative estimation of tumor cell infiltration.

The advent of nano-DESI has allowed for higher spatial resolutions and enhanced molecular coverage of extraction-based IMS approaches. Thus, nano-DESI is increasingly used in biomedical applications to study a wide range of analytes, including small metabolites, drugs, and proteins.<sup>118</sup> In a recent application, nano-DESI was used to examine the localization of diclofenac, a widely used nonsteroidal anti-inflammatory drug, and its metabolites in mouse kidney and liver tissues.<sup>119</sup> Nano-DESI has also been applied for high spatial resolution imaging of native proteins in rat kidney<sup>120</sup>, proteoforms in rat brain<sup>64,121</sup> among other applications.<sup>54,122</sup> In a recent application to human samples, nano-DESI IMS was used for direct imaging of proteoforms (<70 kDa) in human kidney samples, where clear localizations to distinct anatomical structures and cellular neighborhoods within the major component of the kidney were demonstrated.<sup>123</sup> Identification was performed on a serial tissue section by top-down MS. These studies pave the way for future application to molecular tissue mapping, biomarker discovery, and disease diagnostics.

Finally, technological improvements in ambient ionization for clinical applications have led to the development of numerous MS-based surgical devices. For example, the MasSpec Pen is a handheld surgical device that operates via a liquid extraction mechanism.<sup>124</sup> The device is intended for *in vivo* surgical use and has shown promising results in clinical applications. Recently, Zhang et al.<sup>125</sup> described the clinical translation of the MasSpec Pen in 100 surgeries performed by seven surgical teams, where tissue analysis was performed during parathyroidectomy, thyroidectomy, breast, and pancreatic surgeries for various clinical indications. Other surgical MS techniques, including laser desorption (SpiderMass), thermal evaporation (REIMS), and solid extraction, have been developed and reviewed in detail elsewhere.<sup>10</sup>

## 5. Conclusions

This review highlights significant technological advances in modern imaging mass spectrometry and showcases recent biomedical and clinical applications. In the future, careful validation of experimental methods and classification models across numerous

centers is necessary to evaluate the reproducibility, robustness, and applicability of the described workflows. As IMS continues to mature as a field, it is increasingly being used in tandem with other technologies for multimodal tissue interrogation. Multi-institution research consortia, such as the Human BioMolecular Atlas Program (HuBMAP)<sup>126</sup>, the Human Tumor Atlas Network (HTAN)<sup>127</sup>, and the Kidney Precision Medicine Project (KPMP)<sup>128</sup>, represent recent efforts to provide a comprehensive atlas of human tissues using traditional histology methods, fluorescence microscopy, IMS, and other cellular and molecular characterization methods. Ultimately, multimodal imaging strategies are promising for broad biomedical and clinical applications, including disease prediction, diagnosis, guiding treatment, and improving patient care.

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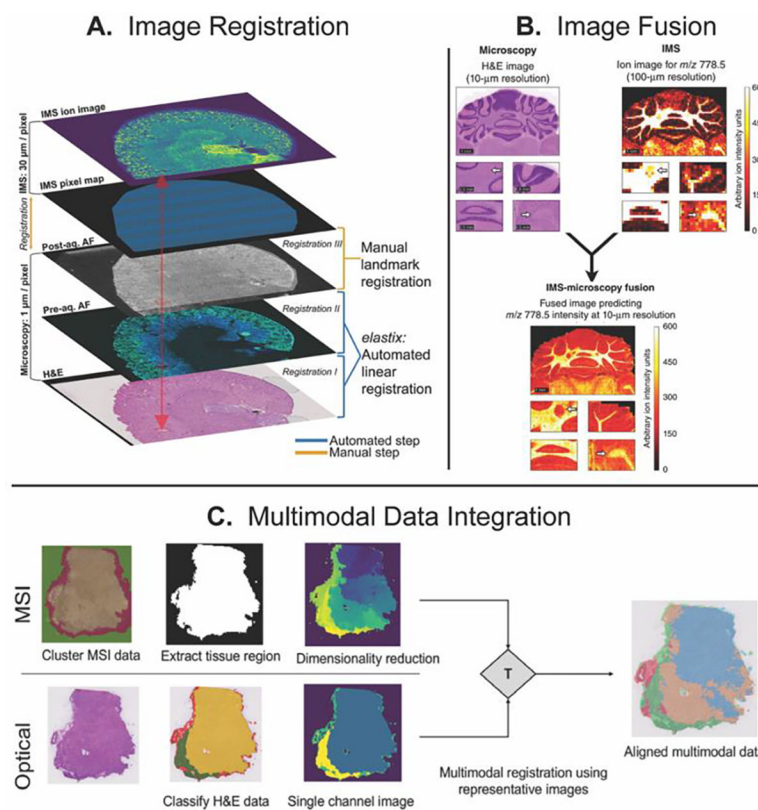
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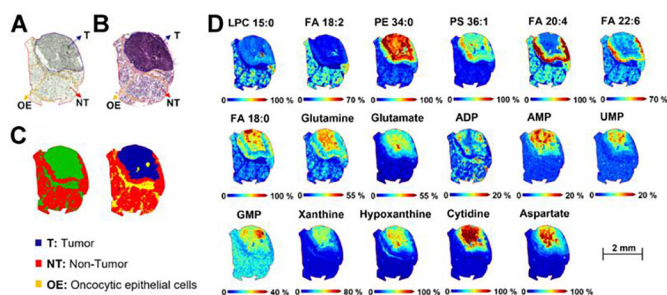
**HIGHLIGHTS**

- Imaging mass spectrometry can advance clinical and biomedical research by providing molecular context to tissue pathology.
- Instrumentation developments are improving molecular coverage, image quality, reproducibility, and throughput.
- Multimodal data integration and visualization enable novel data mining strategies and are essential for deriving biological insight.
- Recent studies showcase the value of MALDI and DESI IMS in clinical tissue interrogation.

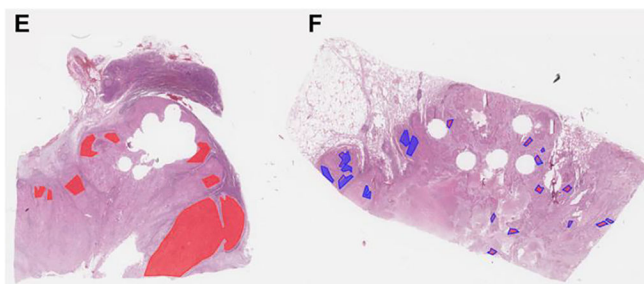


**Figure 1.** Multimodal image registration workflows by (A) Patterson et al., (B) data-driven image fusion by Van de Plas et al., and (C) Deep-learning image registration by Race et al. Figures adapted from Ref. [75], [76], and [77], with permission from the publishers.

## Lipidomic and metabolomic profiling of salivary gland tumor tissues using MALDI IMS

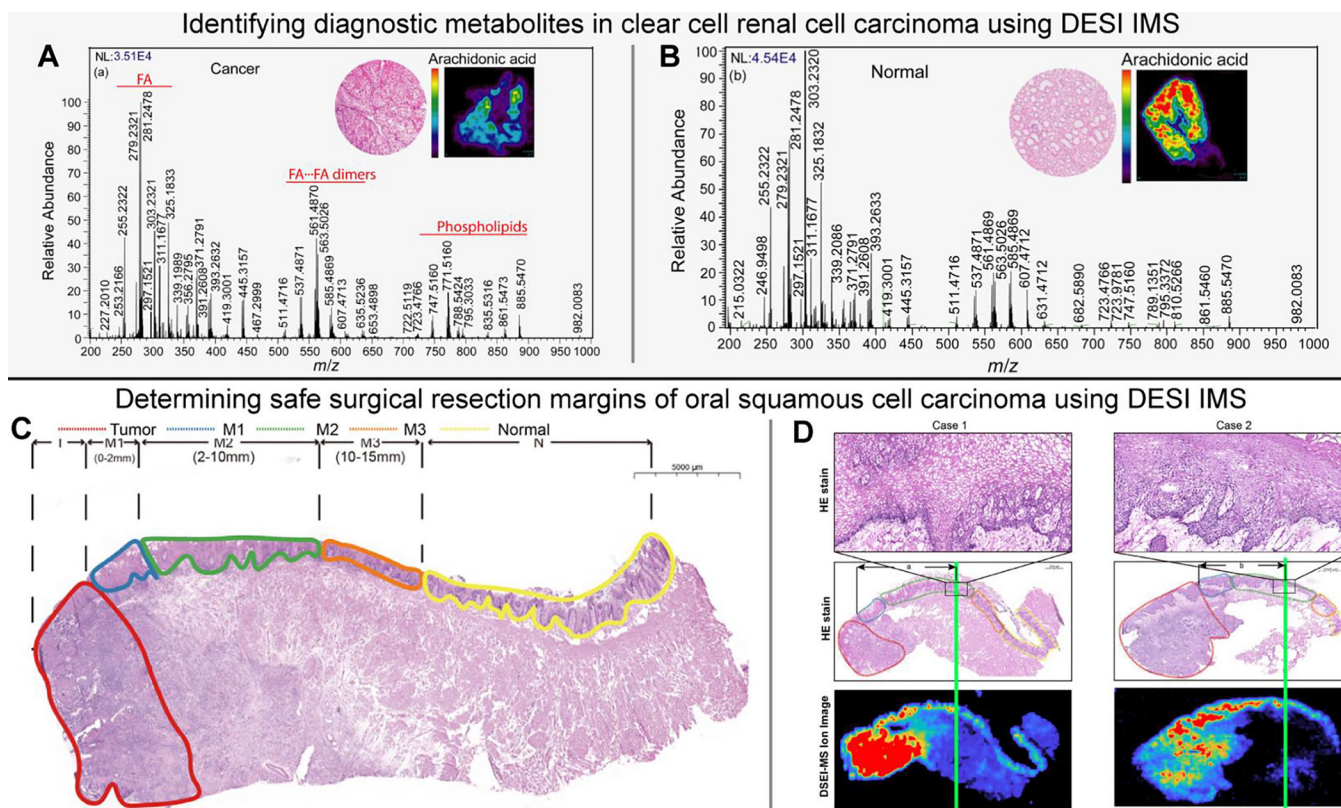


## Subtyping of non-small cell lung cancer using MALDI IMS

**Figure 2.**

Determining the metabolomic and lipidomic profiles of salivary tumor tissue (**A-D**) [reference: 103], and subtyping non-small cell lung cancer (**E-F**) [reference: 104] using MALDI IMS. Annotated optical image (**A**) and hematoxylin and eosin-stained parotid tissue (**B**), bisecting K-means segmentation map generated from the MALDI data (**C**). MALDI IMS images of relevant lipids and metabolites obtained in negative ionization mode, comparing the distribution between tumor and healthy regions of the tissue (**D**). Annotated (lines) stained sections of adenocarcinoma (**E**), squamous cell carcinoma (**F**), and heatmaps (filling) of the neural network classification. Heatmaps show the location of spectra in colors corresponding to their classification: adenocarcinoma –red and squamous cell carcinoma–blue. Figures adapted from Sommella et al. (2022) [reference: 103] and Janßen et al. (2022) [reference: 104] with permissions from the publisher.



**Figure 3.**

Identifying diagnostic metabolite signatures in clear cell renal cell carcinoma (A-B) [Reference 113] and determining safe surgical resection margins of oral squamous cell carcinoma (C-D) [Reference 114] using DESI IMS. Comparison between average mass spectra of normal (A) and ccRCC tissues (B) ( $m/z$ 200–1000), where the inset shows hematoxylin and eosin stains of each as well as ion images of arachidonic acid. Annotated hematoxylin and eosin-stained tissue with oral squamous cell carcinoma including T - Tumor (red), M1- positive margin (blue), M2 - close margin (green), M3 - negative margin (orange), N - normal (yellow) (C). Annotated stains and DESI IMS ion images depicting safe margin distance (green line) as the region where ion intensity decreases/disappears (D). Figures adapted from Vijayalakshmi et al. (2019) [Reference 113] and Yang et al. (2022) [Reference 114] with permissions from the publisher.

Table I.

Overview of IMS Platforms Commonly Employed for Tissue Interrogation

	Ion Source	Matrix	Sample Preparation Time	Source Vacuum Requirements	Spatial Resolution	Molecular Class	Applications
<b>MALDI</b>	Laser	Yes	1 hour	Intermediate-High Vacuum	<1 µm possible, <sup>13</sup> 10–50 µm standard <sup>14,15</sup>	Drugs, metabolites, lipids, proteins	Molecular Profiling, Biomarker Discovery, Disease Classification
<b>DESI</b>	ESI	No	0 min	Ambient	10 µm possible (nanoDESI), 50–200 µm standard <sup>16,17</sup>	Drugs, metabolites, lipids, proteins	Margin Evaluation, Disease Classification, Biomarker Discovery
<b>SIMS</b>	Ion beam	No	0 min	High Vacuum	30 nm possible (nanoSIMS), 70–100 nm standard <sup>18,19</sup>	Elements, drugs, metabolites, lipids	Tissue characterization and biomarker discovery, single-cell imaging
<b>LAESI</b>	Laser/ESI	Yes	30 min	Ambient	20 µm possible, 200–400 µm standard <sup>3,20</sup>	Drugs, metabolites, lipids, proteins	Molecular profiling, biomarker discovery
<b>LESA</b>	Micro/nanoESI	No	0 min	Ambient	~100 µm possible (microLESA), >200 µm standard <sup>21,22</sup>	Metabolites, peptides, proteins	Molecular profiling, biomarker discovery
<b>MALDESI</b>	Laser/ESI	Yes	1 hour	Intermediate-High Vacuum	50 µm possible, 100–200 µm standard <sup>23,24</sup>	Drugs, metabolites, lipids, proteins	Molecular profiling, biomarker discovery
<b>LA-ICP</b>	Laser	No	0 min	Ambient; Vacuum	2.5 µm possible, 30 µm standard <sup>25</sup>	Elements	Elemental composition of biological samples

MALDI - Matrix-Assisted Laser Desorption/Ionization; DESI - Desorption Electrospray Ionization; SIMS - Secondary Ionization Mass Spectrometry; LAESI - Laser Ablation Electrospray Ionization; LESAs - Liquid Extraction Surface Analysis; MALDESI - Matrix-Assisted Laser Desorption/Ionization Electrospray Ionization; LA-ICP - Laser Ablation Inductively Coupled Plasma