

1 HOCl-producing Electrochemical Bandage is Active in Murine Polymicrobial Wound Infection

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19 Methicillin-Resistant *Staphylococcus aureus*, anti-biofilm, *in vivo* wound infection

## 20 **Abstract**

21 Wound infections, exacerbated by the prevalence of antibiotic-resistant bacterial pathogens,  
22 necessitate innovative antimicrobial approaches. Polymicrobial infections, often involving  
23 *Pseudomonas aeruginosa* and methicillin-resistant *Staphylococcus aureus* (MRSA), present  
24 formidable challenges due to biofilm formation and antibiotic resistance. Hypochlorous acid  
25 (HOCl), a potent antimicrobial agent produced naturally by the immune system, holds promise  
26 as an alternative therapy. An electrochemical bandage (e-bandage) that generates HOCl *in situ*  
27 was evaluated for treatment of murine wound biofilm infections containing both MRSA and *P.*  
28 *aeruginosa* with “difficult-to-treat” resistance. Previously, the HOCl-producing e-bandage was  
29 shown to reduce wound biofilms containing *P. aeruginosa* alone. Compared to non-polarized e-  
30 bandage (no HOCl production) and Tegaderm only controls, the polarized e-bandages reduced  
31 bacterial loads in wounds infected with MRSA plus *P. aeruginosa* (MRSA: vs Tegaderm only –  
32 1.4 log<sub>10</sub> CFU/g, p = 0.0015, vs. non-polarized – 1.1 log<sub>10</sub> CFU/g, p = 0.026. *P. aeruginosa*: vs  
33 Tegaderm only – 1.6 log<sub>10</sub> CFU/g, p = 0.0015, vs non-polarized – 1.6 log<sub>10</sub> CFU/g, p = 0.0032),  
34 and MRSA alone (vs Tegaderm only – 1.3 log<sub>10</sub> CFU/g, p = 0.0048, vs. non-polarized – 1.1 log<sub>10</sub>  
35 CFU/g, p = 0.0048), without compromising wound healing or causing tissue toxicity. Addition of  
36 systemic antibiotics did not enhance the antimicrobial efficacy of e-bandages, highlighting their  
37 potential as standalone therapies. This study provides additional evidence for the HOCl-  
38 producing e-bandage as a novel antimicrobial strategy for managing wound infections, including  
39 in the context of antibiotic resistance and polymicrobial infections.

## 40 Introduction

41 The emergence of bacteria that are resistant to antibiotics demands the investigation of  
42 new antimicrobial strategies. This is particularly critical in the context of wound infections.  
43 Studies suggest that almost 90% of wound samples may carry microorganisms with resistance  
44 to at least one antibiotic, with about 30% exhibiting resistance to six or more antibiotics.<sup>1</sup>  
45 Among these, *Pseudomonas aeruginosa* is a Gram-negative pathogen that is intrinsically  
46 resistant to multiple antibiotics and prone to acquiring resistance,<sup>2</sup> and methicillin-resistant  
47 *Staphylococcus aureus* (MRSA), are frequently identified as wound infection culprits.<sup>3,4</sup>

48 The presence of biofilms, communities of microorganisms protected by a complex  
49 matrix of polysaccharides, proteins, DNA, and other substances called extracellular polymeric  
50 substance (EPS), further enhances resistance in pathogens like *P. aeruginosa* and MRSA.  
51 Biofilm-related infections can be challenging to treat with existing therapies, hindering wound  
52 healing and causing persistent inflammation.<sup>5,6</sup> In the United States, around 7 million patients  
53 suffer from chronic wounds annually, with approximately 60% of these wounds associated with  
54 microbial biofilms.<sup>7,8</sup> Given the recalcitrance of chronic wound infections, and the common  
55 involvement of multi drug-resistant *P. aeruginosa* and MRSA, it is essential to develop new  
56 antibiofilm strategies that do not contribute to further antibiotic resistance.

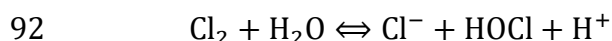
57 Hypochlorous acid (HOCl) is a reactive oxygen species (ROS), naturally produced by  
58 phagocytes, that has potent antimicrobial properties.<sup>9,10</sup> In past studies it has been shown that  
59 HOCl is broadly effective at killing both bacterial and fungal pathogens.<sup>11-13</sup> A barrier to clinical  
60 use has been the inability to continuously deliver microbicidal, non-toxic concentrations to the  
61 infection site. In past studies, we developed an electrochemical platform for the *in situ*  
62 generation of HOCl. This platform was active against both bacterial and fungal biofilms *in vitro*,

63 and against *P. aeruginosa in vivo* wound infections.<sup>11-15</sup> Here, it is shown that an HOCl-  
64 producing electrochemical bandage (e-bandage), controlled by a miniature ‘wearable’  
65 potentiostat, is effective in treating murine wound biofilm infections containing *P. aeruginosa*  
66 and MRSA together (and MRSA alone). The effectiveness of an HOCl-generating e-bandage  
67 was assessed on infections in mouse wounds. The assessment involved measuring the  
68 decrease in live bacteria within the wound, examining the progress of wound healing through  
69 the reduction of wound size, scoring of purulence reduction, analyzing tissue histopathology,  
70 and measuring levels of blood biochemistry markers and inflammatory cytokines. Additionally,  
71 the concentration of HOCl in the wound was measured, and scanning electron microscopy was  
72 conducted on excised wound biofilms to evaluate the treatment's impact on the biofilm matrix  
73 and the integrity and abundance of the bacterial cells. Lastly, HOCl producing e-bandage  
74 treatment was compared with systemic antibiotic treatment, and the ability of e-bandage  
75 treatment to potentiate concurrently administered systemic antibiotics evaluated.

## 76 **Methods and Materials**

### 77 Electrochemical bandage

78 The e-bandage and wearable potentiostat have been previously described.<sup>15-17</sup> Briefly,  
79 the e-bandage comprises two carbon fabric electrodes (Panex 30 PW-06, Zoltek Companies  
80 Inc., St. Louis, MO) with surfaces measuring 1.77 cm<sup>2</sup> each for the working and counter  
81 electrodes, along with a silver/silver chloride (Ag/AgCl) wire serving as a quasi-reference  
82 electrode (QRE). A wearable potentiostat, powered by a 3-volt coin cell battery, maintains the  
83 operational potential of the working electrode at +1.5 V<sub>Ag/AgCl</sub>. Carbon fabric electrodes are  
84 separated by two layers of cotton fabric, with an additional layer placed over the counter  
85 electrode to aid in moisture retention. These layers are secured using silicone adhesive. The  
86 QRE is positioned between the cotton fabric layers separating the carbon electrodes. Titanium  
87 wires (TEMCo, Amazon.com, catalog #RW0524) with nylon sew-on caps (Dritz, Spartanburg,  
88 SC, item#85) connect to opposite ends of the e-bandage and link to the potentiostat. Under  
89 physiological conditions, polarization of the bandage leads to the generation of HOCl through  
90 these reactions:



93 At pH 7.4 and 25°C, the conditions under which e-bandage was employed, HOCl  
94 dissociates to ~57% HOCl and ~43% ClO<sup>-</sup>.<sup>18</sup>

### 95 Mice skin wound infection model

96 All animal experiments were approved by the Mayo Clinic Institutional Animal Care and  
97 Use Committee (A00003272-20). Full-thickness skin wounds were generated on Swiss

98 Webster mice (Charles River, Wilmington, MA). Animals were anesthetized by intraperitoneal  
99 injection of a mixture of ketamine (90 mg/kg) and xylazine (10 mg/kg). Subcutaneous  
100 buprenorphine ER-Lab (1 mg/kg) was administered for analgesia. Creation of mature wound  
101 biofilms was as previously reported.<sup>19,20</sup> The dorsal surface was shaved and disinfected, and a  
102 circular full-thickness skin wound created using a 5-mm biopsy punch (Acuderm Inc., Fort  
103 Lauderdale, FL). Wounds were then infected with 10  $\mu$ l of 10<sup>6</sup> colony-forming units (CFUs) of  
104 clinical isolates of MRSA IDRL-6169 and/or *P. aeruginosa* IDRL-11442 which has “difficult-to-  
105 treat” resistance, suspended in 0.9% sterile saline. MRSA IDRL-6169 is a methicillin and  
106 mupirocin-resistant isolate from a prosthetic hip. *P. aeruginosa* IDRL-11442 is a wound isolate  
107 resistant to piperacillin/tazobactam, cefepime, ceftazidime, meropenem, aztreonam,  
108 ciprofloxacin, and levofloxacin.<sup>21</sup> Bacterial suspensions were permitted to settle in wound beds  
109 for 5 minutes. Subsequently, wounds were covered with semi-occlusive transparent  
110 Tegaderm® (3M, St. Paul, MN) secured using the liquid adhesive Mastisol® (Eloquest Health  
111 care, Ferndale, MI). Images of the wounds were captured, and wound diameters documented  
112 every other day using a Silhouette wound imaging system (Aranz Medical Ltd, Christchurch,  
113 NZ). Purulence was assessed before and after treatment to evaluate immune response to  
114 biofilm infection and treatment. The purulence scoring system was based on previous work<sup>19</sup>  
115 using the following scale: 0 – no exudate in the wound-bed; 1 – slight turbid exudate at the  
116 wound site; 2 – mild amount of white exudate at the wound site; 3 – moderate amount of white  
117 exudate at the wound site; 4 – moderate amount of yellowish exudate at the wound site; 5 –  
118 large amount of turbid yellow exudate extending beyond the wound-bed.

119 e-Bandage treatment

120 Following the establishment of 48-hours infections in mouse wound beds, mice were  
121 anesthetized with isoflurane, Tegaderm was removed, and wearable potentiostats were  
122 sutured to the scruff of the neck. Sterile e-bandages were pre-hydrated in sterile 1X  
123 phosphate-buffered saline (1X PBS), and 200  $\mu$ L of sterile hydrogel (1.8% [w/v] xanthan gum  
124 in 1X PBS) were injected between the e-bandage layers. An additional 200  $\mu$ L of hydrogel was  
125 applied to the wound beds, and e-bandages sutured on top to maintain close contact of the  
126 entire working electrode with the dorsal surface during mouse activity. e-bandages were then  
127 connected to the potentiostats and an additional 200  $\mu$ L of hydrogel was placed on top, after  
128 which the entire e-bandage setups were covered with Tegaderm. Coin cell batteries (3V,  
129 Ecr1220 Energizer, St. Louis, MO) were inserted into the potentiostats to initiate e-bandage  
130 polarization (HOCl production). Treatment commenced for 48 hours with hydrogel refreshment  
131 and battery changes every 24 hours. Potentials of the working electrodes relative to the QREs  
132 were measured following treatment initiation, before and after each battery change, and prior  
133 to euthanasia to continuous operation.

134 Control groups included wounds administered only hydrogel and Tegaderm, and  
135 wounds treated with non-polarized e-bandages (i.e., no potentiostat or HOCl production).  
136 Additional animals from experimental and control groups underwent concurrent antibiotic  
137 dosing, with MRSA-infected mice treated with vancomycin and MRSA plus *P. aeruginosa*-  
138 infected mice treated with vancomycin and amikacin. Previously, the pharmacokinetic profiles  
139 of amikacin and vancomycin was established in Swiss Webster mice to determine a treatment  
140 dose of 15 mg/kg subcutaneous every 6 hours for amikacin and 150 mg/kg IP every 12 hours  
141 for vancomycin.<sup>20</sup> At least 7 mice were included in each experimental and control group.

142 Total wound HOCl measurement

143           Following wound bed excision and homogenization, the remaining portion (900  $\mu$ L) of  
144 the wound homogenate, which was not used for quantifying bacterial load, was employed to  
145 determine the total wound HOCl content using free chlorine spectrophotometer test kits  
146 (TNT866; Hach Company, Ames, IA), following manufacturer's instructions. In brief,  
147 homogenized wound contents were mixed with 4.1 mL of 1X PBS and centrifuged at 5000 rcf  
148 for 15 minutes. Resulting supernatants were filtered through syringe filters (0.22  $\mu$ m pore size),  
149 and 4 mL of the filtrate added to free chlorine test tubes, allowing them to react for 1 minute  
150 before being measured at 515 nm using a Hach DR 1900 portable spectrophotometer (Hach  
151 Company). The free chlorine content was then converted to HOCl content using a specific  
152 equation, considering volume adjustment.

$$153 \quad \text{Concentration of HOCl [M]} = \frac{\text{Concentration of free chlorine } \left[ \frac{\text{mg}}{\text{L}} \right] \times \text{conversion factor } \left[ \frac{\text{g}}{\text{mg}} \right]}{\text{Molecular weight of chlorine } \left[ \frac{\text{g}}{\text{mol}} \right]}$$

154           The molecular weight of chlorine (70.906 g/mol) and a conversion factor of 0.001 g/mg  
155 were used. Complete conversion of HOCl from free chlorine was assumed.

#### 156 Wound biofilm quantification

157           Following the conclusion of treatment, Tegaderm and e-bandages were removed from  
158 wound beds, and wound tissue excised using a 10 mm biopsy punch tool (Acuderm Inc., Fort  
159 Lauderdale, FL). Skin tissue was weighed, homogenized (Omni International, Kennesaw, GA)  
160 in sterile PBS, vortexed for 20 seconds and sonicated for 5 minutes in a water bath.  
161 Subsequently, 100  $\mu$ L of the resulting homogenate underwent serial dilution (10-fold dilutions)  
162 in 0.9% saline, and colony-forming units (CFUs) were determined by spread-plating 100  $\mu$ L of  
163 each dilution onto tryptic soy agar with 5% sheep blood. Enumeration of mixed-species biofilm



164 CFU counts was conducted using eosin methylene blue and colistin nalidixic acid agar plates.  
165 After 24 hours of incubation at 37°C, colonies were counted, and the results were reported as  
166 log<sub>10</sub> CFU/g of tissue.

### 167 Histopathology

168 For each treatment and control group, a subset of animals (n=3) was utilized for wound  
169 histopathology evaluation. The wounds were excised using a 10 mm biopsy punch and  
170 preserved in 10% formalin. After fixing, the specimens were dyed with hematoxylin and eosin  
171 (H&E) stains. Subsequently, a board-certified clinical pathologist, who was not aware of the  
172 sample origins, examined the slides. The pathologist assessed the level of inflammation on a  
173 scale from 0 (none) to 3 (severe), and checked for the presence of abscesses, ulceration,  
174 tissue death, and neutrophil infiltration, marking them as either present (Yes) or absent (No).

### 175 Scanning Electron Microscopy

176 Following e-bandage treatment, the wound tissues from a subset of three animals from  
177 both the treatment and control groups were extracted with a 10 mm biopsy punch (Acuderm  
178 Inc., Fort Lauderdale, FL) and placed in sterile tubes containing a fixative solution composed of  
179 4% formaldehyde plus 1% glutaraldehyde in phosphate buffer. The samples were then rinsed  
180 in PBS and dehydrated through a series of ethanol washes (10%, 30%, 50%, 70%, 90%, 95%,  
181 and 100% - twice). Dehydrated samples underwent critical point drying in a vacuum sputter  
182 coater (Bio-Rad E5100) and were coated with gold/palladium (60/40%). Finally, samples were  
183 visualized using a Hitachi S4700 cold-field emission scanning electron microscope (Hitachi  
184 High Technologies America, Inc., Schaumburg, IL). Samples assigned non-descriptive  
185 numbers upon collection by study staff and were then randomized by an electron microscopy  
186 technologist before imaging. Images were blindly reviewed by 8 members of the Mayo Clinic

187 Infectious Diseases Research laboratory and scored on a scale of 1-3 for biofilm matrix  
188 integrity, bacterial cell integrity, and bacterial cell abundance.

### 189 Toxicity screen analysis and inflammatory panel screening

190 After euthanasia, blood was drawn via cardiac puncture and then centrifuged to separate the  
191 serum. The serum samples were then examined for various biochemical markers using a  
192 Piccolo® Xpress™ Chemistry Analyzer at the Mayo Clinic Central Clinical Laboratory. This  
193 analysis included measuring levels of glucose, amylase, blood urea nitrogen, alkaline  
194 phosphatase, alanine aminotransferase, aspartate aminotransferase, gamma  
195 glutamyltransferase, lactate dehydrogenase, C-reactive protein, total bilirubin, creatinine, uric  
196 acid, albumin, total protein, calcium, chloride, magnesium, potassium, sodium, and total  
197 carbon dioxide. Furthermore, the serum was analyzed with a MesoScale Discovery SQ 120 to  
198 determine the presence of inflammatory biomarkers, including IFN- $\gamma$ , IL-4, IL-5, IL-6, TNF- $\alpha$ ,  
199 and KC/GRO.

### 200 Statistical analysis

201 SEM scores from blind review were compared using ordinary two-way ANOVA with  
202 Tukey's multiple comparisons test, with a single pooled variance. This allowed for comparison  
203 of the pooled reviewer scores for all sample types while accounting for reviewer and sample  
204 variability within each treatment group. For all other parameters, initial analysis among the  
205 experimental groups was performed using the Kruskal-Wallis test. For further detailed  
206 comparisons between specific groups, the Wilcoxon rank sum test was applied. The choice of  
207 non-parametric tests was driven by the small size of the samples and the lack of evidence  
208 supporting the normal distribution of the data. All statistical tests were conducted as two-tailed,  
209 considering p-values under 0.05 as statistically significant. When dealing with comparisons

210 involving more than three groups, adjustments were made to account for the False Discovery  
211 Rate. The data analysis was conducted using SAS software (version 9.4, SAS Institute), while  
212 GraphPad Prism (version 10.1, GraphPad Software) was used for the creation of graphs.

## 213 **Results**

### 214 HOCl was produced by polarized e-bandages *in situ*

215 In previous studies, microelectrodes were used to demonstrate that e-bandages  
216 generate HOCl at the working electrode. HOCl was shown to penetrate biofilms, explant  
217 tissue, and wound beds in live mice.<sup>15,16,22</sup> In this study, free chlorine spectrophotometer test  
218 kits were used to quantify the total concentration of HOCl in wounds infected with MRSA  
219 alone, and with *P. aeruginosa*. In both infection scenarios, wounds from mice treated with  
220 polarized electric bandages exhibited elevated levels of HOCl compared to those treated with  
221 non-polarized electric bandages or Tegaderm alone (**Figure 1**).

### 222 Wound bacterial loads were reduced by polarized e-bandage treatment

223 To assess the efficacy of HOCl-generating e-bandage therapy in reducing bacterial  
224 biofilm burden *in vivo*, endpoint wound colony-forming units (CFUs) were quantified after 48  
225 hours of treatment. Treatment of MRSA wound biofilms with polarized e-bandages reduced  
226 bacterial loads compared to non-polarized e-bandages ( $p = 0.0048$ ) or Tegaderm alone ( $p =$   
227  $0.0048$ , **Figure 2a**). Treatment of wound biofilms infected with both MRSA and *P. aeruginosa*  
228 by polarized e-bandages reduced bacterial loads of both species compared to non-polarized e-  
229 bandages (MRSA:  $p = 0.026$ ; *P. aeruginosa*:  $p = 0.0032$ ) or Tegaderm alone (MRSA:  $p =$   
230  $0.003$ ; *P. aeruginosa*:  $p = 0.0015$ ; **Figure 2b**).

231 Three wounds from each treatment group for both MRSA alone and MRSA plus *P.*  
232 *aeruginosa* infected mice were blindly scored for biofilm matrix integrity, bacterial cell integrity,  
233 and bacterial cell abundance. Bacterial cell abundance was significantly lower after polarized  
234 e-bandage treatment for both MRSA and MRSA plus *P. aeruginosa*-infected wounds in

235 comparison to Tegaderm only and non-polarized control groups (**Figure 3**), in agreement with  
236 reduced bacterial loads.

237 To test if e-bandage treatment of established wound biofilms exhibited potential synergy  
238 with antibiotics against established wound biofilms, additional mice from all groups for both  
239 MRSA and MRSA plus *P. aeruginosa* infections were administered concurrent systemic  
240 vancomycin (for MRSA alone), or vancomycin and amikacin (for MRSA plus *P. aeruginosa*) for  
241 the duration of e-bandage treatment. Antibiotic treatment did not result in lower end-point  
242 bacterial loads for wounds treated with polarized e-bandages for either the single or dual-  
243 species infection groups. For MRSA alone, vancomycin reduced bacterial loads in only the  
244 non-polarized group (**Figure 2a**). For MRSA plus *P. aeruginosa*, MRSA load was not reduced  
245 in any group, however *P. aeruginosa* was reduced in both the Tegaderm only and non-  
246 polarized groups (**Figure 2b**).

#### 247 Wound healing was not hampered by polarized e-bandage treatment

248 To determine if HOCl-producing e-bandage treatment, with and without concurrent  
249 systemic antibiotics, affected wound closure over 48 hours of treatment, total wound area was  
250 measured before and after application. No significant differences in overall wound closure  
251 percentage were observed between any group for either MRSA alone, or MRSA plus *P.*  
252 *aeruginosa* infections (**Figure 4**). Interestingly, wound closure was less complete in the non-  
253 polarized group for MRSA plus *P. aeruginosa*-infected wounds when antibiotics were used.  
254 This effect (though not significant) was also observed with the Tegaderm only and polarized  
255 groups for the dual-infection wounds, but with MRSA alone.

#### 256 Treatment of infected wounds with polarized e-bandages resulted in reduced purulence

257 The impact of e-bandage and/or antibiotic therapy on wound bed purulence was  
258 evaluated by scoring purulence before and after treatment (**Figure 5**). The use of polarized e-  
259 bandages resulted in a marked reduction in purulence compared to the Tegaderm-only control  
260 group in wounds infected with both MRSA and MRSA combined with *P. aeruginosa*. There  
261 was no significant improvement in purulence reduction between polarized and non-polarized e-  
262 bandage groups for either the mono or dual species infection, although the non-polarized  
263 group exhibited significantly less purulence than the polarized group in the dual-species  
264 infections (and to a lesser, insignificant amount in the MRSA only infections). Concurrent  
265 antibiotics did not improve purulence reduction in any treatment group in either the mono- or  
266 dual-species infected wounds.

#### 267 Polarized e-bandage treatment produced no observable tissue toxicity

268 To ascertain whether e-bandage therapy led to increased tissue toxicity compared to  
269 infection alone, samples were evaluated by a clinical pathologist blinded to the treatment. No  
270 notable variances were observed in overall inflammation, necrosis levels, abscess formation,  
271 ulceration, or neutrophilic inflammation across all treatment groups for both MRSA and MRSA  
272 plus *P. aeruginosa* infections.

#### 273 Assessment of inflammation and blood biomarkers for indication of animal health

274 Blood biochemical biomarker assessment and measurement of inflammatory cytokines  
275 was performed on a subset (n=3) of animals from each group to examine the immune  
276 response and general health of infected animals compared uninfected control animals at the  
277 time of euthanasia. As expected, all infected animals exhibited an elevated proinflammatory  
278 response compared to uninfected controls for both infection types (**Figure 6**). In particular, the  
279 proinflammatory cytokines INF- $\gamma$  and IL-6 were elevated approximately 4 to 16-fold and 2 to 9-

280 fold respectively, indicating a strong, macrophage-driven immune response in all infected  
281 groups. Between infected groups, only KC/GRO showed significant elevation in animals  
282 treated with polarized vs non-polarized e-bandages. Notably, IL-6 was also most elevated in  
283 the polarized group for both infection types, albeit not to the level of statistical significance. For  
284 blood biochemical analysis, mean analyte levels were within normal healthy range for all  
285 groups, with no significant difference between animals treated with polarized or non-polarized  
286 e-bandages for both infection types (data not shown).

## 287 Discussion

288 Development of alternative antimicrobial strategies is imperative in the face of rising  
289 antibiotic-resistant bacterial pathogens, particularly in the context of polymicrobial wound  
290 infections. In this study, efficacy of a previously developed HOCl-producing e-bandage for  
291 treatment of wound biofilm infections with antibiotic resistant clinical isolates of MRSA and *P.*  
292 *aeruginosa* was investigated. In a previous study efficacy of HOCl-producing e-bandages  
293 against wounds infected with *P. aeruginosa* alone was demonstrated.<sup>15</sup> Polymicrobial  
294 infections, particularly with antibiotic resistant strains, pose additional challenges to wound  
295 infection healing. MRSA and *P. aeruginosa* are two of the most commonly isolated wound  
296 pathogens, and are often found together,<sup>4,23</sup> with worse outcomes compared to mono-species  
297 infections.<sup>24-26</sup>

298 Results confirm the ability of polarized e-bandages to produce HOCl *in situ*, leading to  
299 elevated levels of HOCl in wound beds compared to non-polarized e-bandages or Tegaderm  
300 alone. Production of HOCl was associated with a significant reduction in bacterial biofilm  
301 burden *in vivo*, as demonstrated by lower bacterial loads in wounds infected with MRSA alone  
302 or co-infected with MRSA and *P. aeruginosa* following treatment with polarized e-bandages.  
303 Further, blind review of SEM images of the wound beds taken from all groups revealed lower  
304 bacterial abundance in the animals treated with polarized e-bandages. No significant effect on  
305 the biofilm matrix was observed, indicating that the treatment is likely directly biocidal to  
306 biofilm-dwelling pathogens, as opposed to acting as an anti-EPS or pro-dispersal agent.

307 While polarized e-bandage treatment alone effectively reduced bacterial loads, addition  
308 of systemic antibiotics did not result in any additional microbicidal activity for either the MRSA  
309 infected or MRSA plus *P. aeruginosa* infected wounds, indicating that the antibacterial efficacy



310 of e-bandages is independent of systemic antibiotic administration. This highlights the potential  
311 of e-bandages as a standalone antimicrobial strategy for wound infections, particularly in the  
312 context of antibiotic-resistant pathogens.

313 All infected groups showed an elevated, macrophage-driven immune response  
314 compared to uninfected controls. Between infected groups, animals treated with polarized e-  
315 bandages showed significantly elevated levels of KC/GRO when infected with MRSA alone,  
316 and insignificantly elevated levels of IL-6 when infected with both MRSA alone and in  
317 combination with *P. aeruginosa*. This indicates that inflammation in the polarized group may be  
318 more pronounced.

319 No adverse effects on wound healing or tissue toxicity associated with polarized e-  
320 bandage treatment was observed. Assessment of wound closure, purulence, histopathology,  
321 and blood biomarkers revealed no significant differences between non-polarized and polarized  
322 groups, indicating the safety and biocompatibility of e-bandage therapy in this context.  
323 Previous results with e-bandages that produce an alternative reactive oxygen species,  
324 hydrogen peroxide (H<sub>2</sub>O<sub>2</sub>), found that wound healing was not only unimpeded but  
325 augmented,<sup>20</sup> however, antimicrobial efficacy of electrochemically generated H<sub>2</sub>O<sub>2</sub> was less  
326 than HOCl against a broad spectrum of microorganisms.<sup>12,22,27-30</sup> Therefore, a programmable  
327 e-bandage that can produce both HOCl and H<sub>2</sub>O<sub>2</sub> for optimal biocide and wound healing  
328 augmentation respectively should be explored.

329 In conclusion, these findings support promising efficacy of polarized HOCl-producing e-  
330 bandages in treating wound biofilm infections containing MRSA and *P. aeruginosa*. The ability  
331 of e-bandages to locally generate HOCl offers a novel and effective antimicrobial strategy that  
332 may address the challenges associated with antibiotic resistance in wound management,

333 particularly in the context of polymicrobial infections. Further clinical studies are warranted to  
334 validate these findings and assess clinical application of e-bandage therapy for treatment of  
335 wound infections.

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344 Netflix and CARB-X. In addition, R.P. has a patent on *Bordetella pertussis/parapertussis* PCR  
345 issued, a patent on a device/method for sonication with royalties paid by Samsung to Mayo  
346 Clinic, and a patent on an anti-biofilm substance issued. R.P. receives honoraria from Up-to-  
347 Date and the Infectious Diseases Board Review Course. H.B. holds a patent  
348 (US20180207301A1), “Electrochemical reduction or prevention of infections,” which refers to  
349 the electrochemical scaffold upon which the current design of e-bandage is based.

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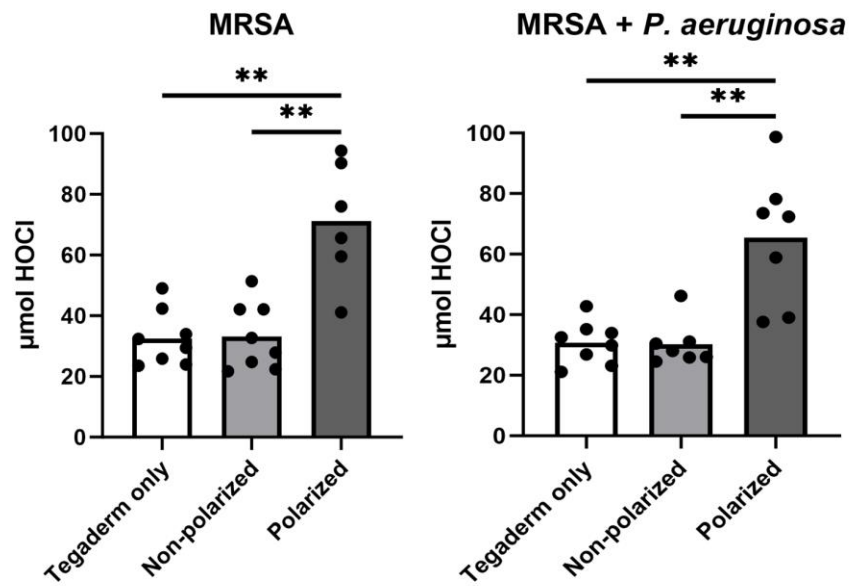
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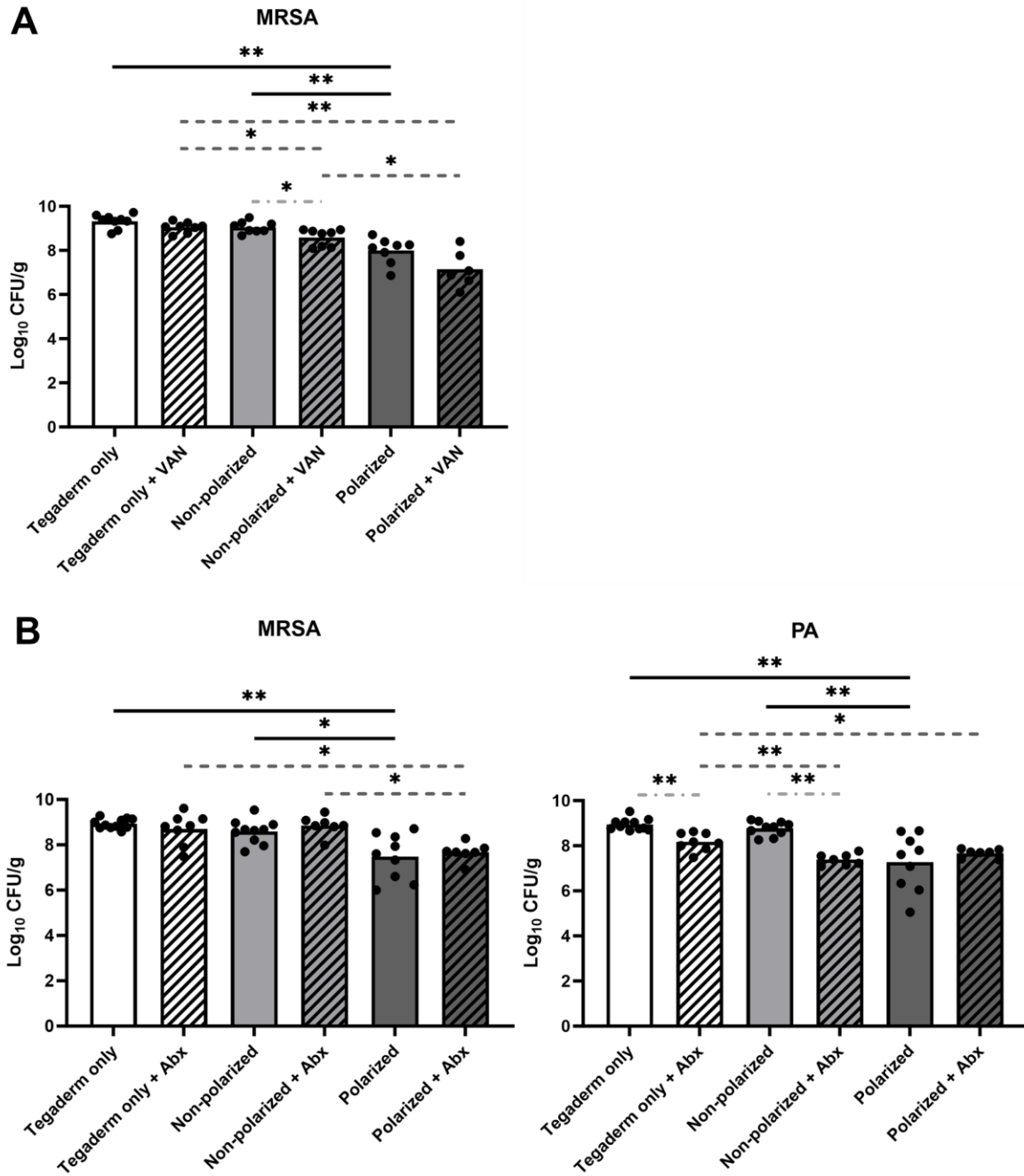
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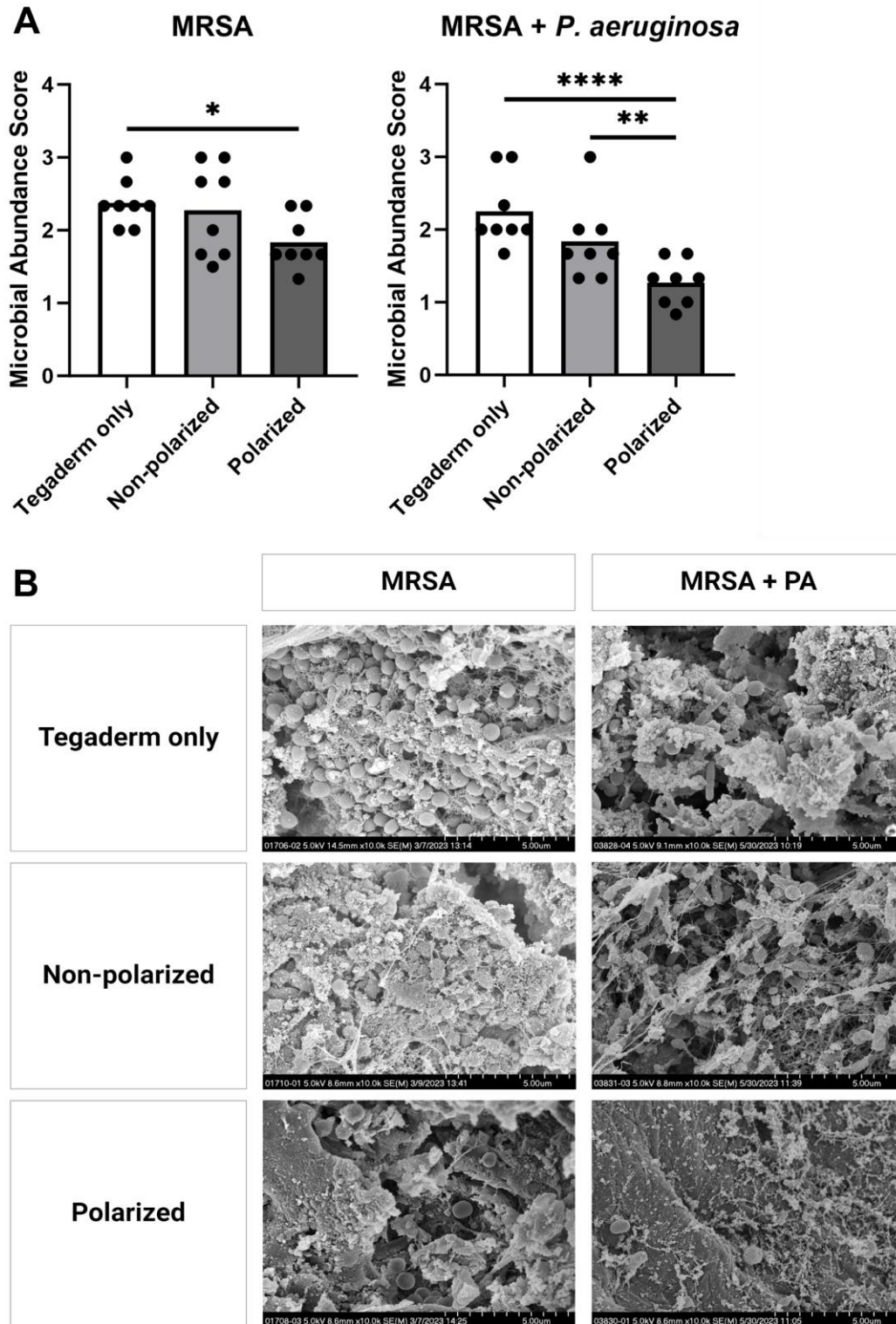
**Figure 1. Polarized e-bandage treatment resulted in increased total wound HOCl content.** 48-hour wound bed biofilms containing MRSA or MRSA plus *P. aeruginosa* (PA) were treated for 48 hours with either polarized (HOCl-producing) or non-polarized e-bandages and compared to Tegaderm only controls. Statistical analysis was performed using the Wilcoxon rank sum test with correction for false discovery rate. Individual data points with the means (bars) are shown.  $N \geq 7$ .  $**p \leq 0.01$ .





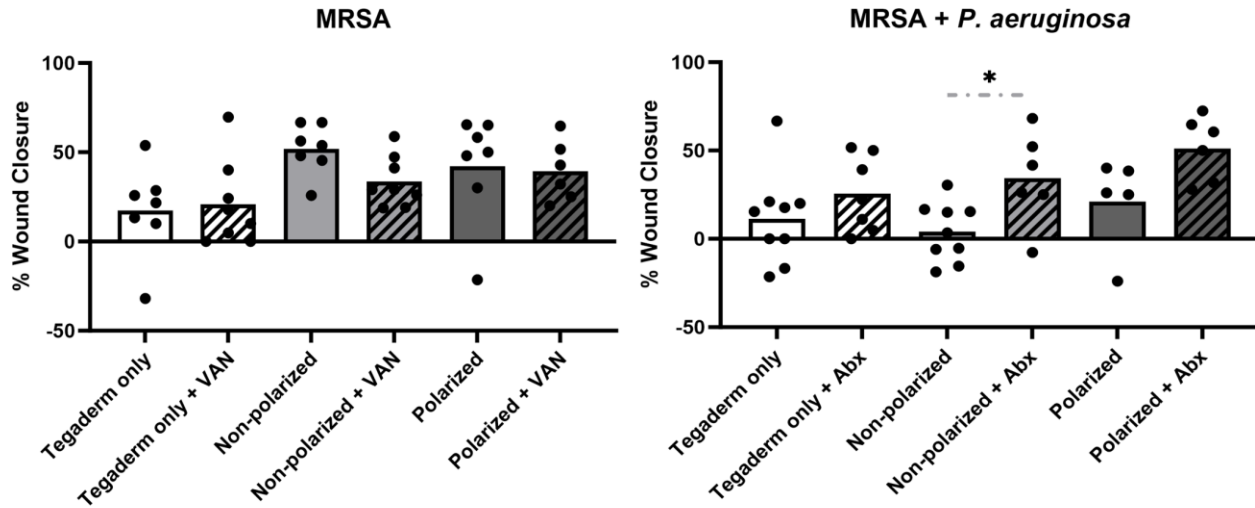
**Figure 2. Polarized e-bandage treatment reduces endpoint bacterial loads.** 48-hour wound bed biofilms containing MRSA (A) or MRSA plus *P. aeruginosa* (PA; B) were treated for 48 hours with either polarized (HOCl-producing) or non-polarized e-bandages, with or without systemic antibiotics (MRSA alone, vancomycin – VAN; MRSA plus *P. aeruginosa* –

vancomycin plus amikacin - Abx) and compared to Tegaderm only controls, with and without antibiotics. Statistical analysis was performed using the Wilcoxon rank sum test with correction for false discovery rate. Individual data points with the means (bars) are shown. Solid black significance bars show differences between non-antibiotic-treated groups; Dashed dark grey significance bars show differences between antibiotic-treated groups; light grey dashed and dotted significance bars show differences between antibiotic and non-antibiotic-treated groups with the same e-bandage treatment type).  $N \geq 7$ . \* $p \leq 0.05$ , \*\* $p \leq 0.01$ .

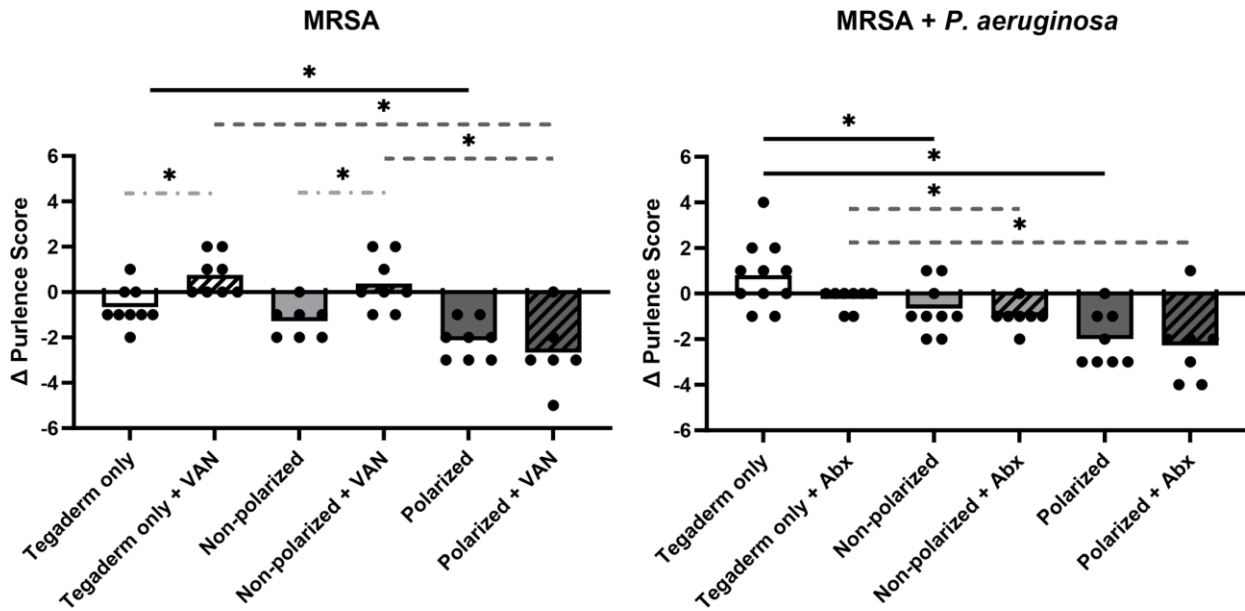


**Figure 3. Polarized e-bandage treatment reduces bacterial abundance observed in scanning electron microscopy (SEM) images. SEM images of 48-hour wound biofilms**

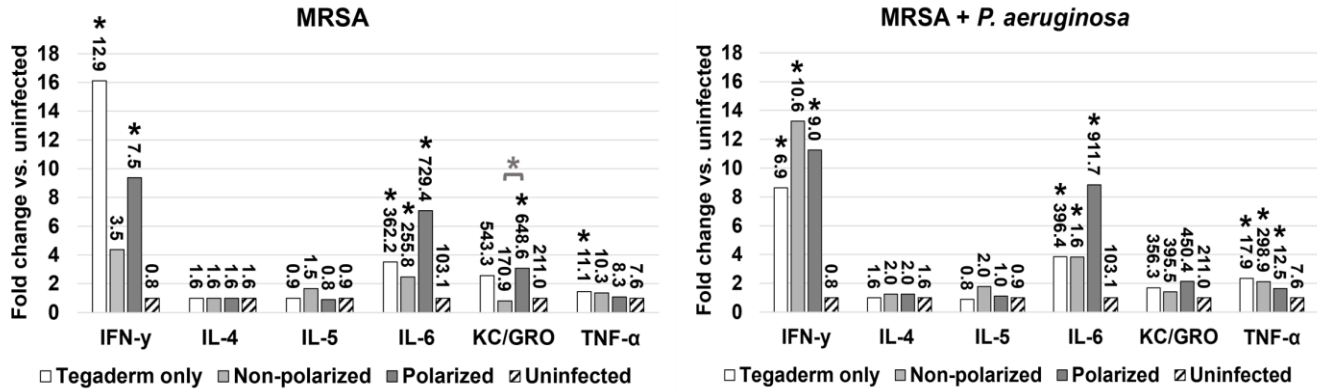
containing MRSA or MRSA plus *P. aeruginosa* treated for 48 hours with polarized or non-polarized e-bandages, or Tegaderm only, were blindly reviewed and scored for bacterial abundance (A). Individual data points with the means (bars) are shown. Representative images are shown in (B) at 10,000 x magnification. Statistical significance was determined via two-way ANOVA with Tukey's multiple comparisons test, with a single pooled variance. N = 3 samples per treatment type; 3-4 images per sample informed scoring. \*p ≤ 0.05, \*\*p ≤ 0.01. \*\*\*p ≤ 0.0001.



**Figure 4. Polarized e-bandage treatment did not hinder wound closure.** 48-hour wound bed biofilms containing MRSA (A) or MRSA plus *P. aeruginosa* (PA; B) were treated for 48 hours with either polarized (HOCl-producing) or non-polarized e-bandages, with or without systemic antibiotics (MRSA alone, vancomycin – VAN; MRSA plus *P. aeruginosa* – vancomycin plus amikacin - Abx) and compared to Tegaderm only controls, with and without antibiotics. Wound area was measured before and after treatment. Individual data points with means (bars) are shown. Statistical analysis was performed using the Wilcoxon rank sum test with correction for false discovery rate.  $N \geq 7$ .  $*p \leq 0.05$ .



**Figure 5. e-Bandage treatment resulted in reduced wound purulence.** 48-hour wound bed biofilms containing MRSA or MRSA plus *P. aeruginosa* (PA) were treated for 48 hours with either polarized (HOCl-producing) or non-polarized e-bandages, with or without systemic antibiotics (MRSA alone, vancomycin – VAN; MRSA plus *P. aeruginosa* – vancomycin plus amikacin - Abx) and compared to Tegaderm only controls, with and without antibiotics. Wound purulence was scored before and after treatment. Statistical analysis was performed using the Wilcoxon rank sum test with correction for false discovery rate. Individual data points with means (bars) are shown. Solid black significance bars show differences between non-antibiotic-treated groups; Dashed dark grey significance bars show differences between antibiotic-treated groups; light grey dashed and dotted significance bars show differences between antibiotic and non-antibiotic-treated groups with the same e-bandage treatment type). N ≥ 7. \*p ≤ 0.05.



**Figure 6. Inflammatory response in infected groups compared to uninfected controls.**

48-hour wound bed biofilms containing MRSA or MRSA plus *P. aeruginosa* (PA) were treated for 48 hours with either polarized (HOCl-producing) or non-polarized e-bandages, with or without systemic antibiotics (MRSA alone, vancomycin – VAN; MRSA plus *P. aeruginosa* – vancomycin plus amikacin - Abx) and compared to Tegaderm only controls, with and without antibiotics. Following treatment, plasma collected and analyzed for levels of IFN- $\gamma$ , IL-4, IL-5, IL-6, TNF- $\alpha$ , and KC/GRO. Fold change in comparison to uninfected controls is graphed, with analyte levels (in pg/ml) displayed as data labels. Statistical analysis was performed using the Wilcoxon rank sum test with correction for false discovery rate. Asterisks without bars represent significance compared to uninfected controls. Asterisks with bars represent significance between groups for the same analyte. N = 3. \*p  $\leq$  0.05.