

Health Research Alliance

Member Organization Author Manuscript J Mol Cell Cardiol. Author manuscript; available in PMC 2024 April 15.

Published in final edited form as:

J Mol Cell Cardiol. 2020 February ; 139: 62–74. doi:10.1016/j.yjmcc.2020.01.005.

Age- and sex-dependent differences in extracellular matrix metabolism associate with cardiac functional and structural changes

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Abstract

Age-related remodeling of the heart causes structural and functional changes in the left ventricle (LV) that are associated with a high index of morbidities and mortality worldwide. Some cardiac pathologies in the elderly population vary between genders revealing that cardiac remodeling during aging may be sex-dependent. Herein, we analyzed the effects of cardiac aging in male and female C57Bl/6 mice in four age groups, 3, 6, 12, and 18 month old (n = 6-12 animals/sex/age), to elucidate which age-related characteristics of LV remodeling are sex-specific. We focused particularly in parameters associated with age-dependent remodeling of the LV extracellular matrix (ECM) that are involved in collagen metabolism. LV function and anatomical structure were assessed both by conventional echocardiography and speckle tracking echocardiography (STE). We then measured ECM proteins that directly affect LV contractility and remodeling. All data were analyzed across ages and between sexes and were directly linked to LV functional changes. Echocardiography confirmed an age-dependent decrease in chamber volumes and LV internal diameters, indicative of concentric remodeling. As in humans, animals displayed preserved ejection fraction with age. Notably, changes to chamber dimensions and volumes were temporally distinct between sexes. Complementary to the traditional echocardiography, STE revealed that circumferential strain rate declined in 18 month old females, compared to younger animals, but not in males, suggesting STE as an earlier indicator for changes in cardiac function between sexes. Age-dependent collagen deposition and expression in the endocardium did not differ between sexes; however, other factors involved in collagen metabolism were sex-specific. Specifically, while decorin, osteopontin, Cthrc1, and Ddr1 expression were age-dependent but sex-independent, periostin, lysyl oxidase, and Mrc2 displayed age-dependent and sex-specific differences. Moreover, our data also suggest that with age males and females have distinct TGFB signaling pathways. Overall, our results give evidence of sex-specific molecular changes during physiological cardiac remodeling that associate with age-dependent structural and functional

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Declaration of Competing Interest None.

dysfunction. These data highlight the importance of including sex-differences analysis when studying cardiac aging.

Keywords

Aging; Cardiac dysfunction; Strain analysis; Collagen metabolism; Sex differences

1. Introduction

Independent of conventional risk factors (e.g. hypertension, smoking, and diabetes), physiological remodeling of the heart during natural aging is a major component for the development of cardiovascular diseases (CVD) and heart failure (HF) [1–3]. In the United States, recent statistical data evaluating aging and CVD report that: 1) There is a 145% increase in the number of deaths caused by CVD in patients between 65 and 85 years of age; 2) Mortality on individuals > 85 years old represents 40% of all CVD-related deaths [4]; and 3) HF prevalence rises from 2% in the general population to > 10% among people > 70years of age [5,6]. This occurs not only because aging prolongs exposure to several other cardiovascular risks, but also due to intrinsic cardiac aging. Intrinsic cardiac aging is defined by the following factors: an increase in left ventricular (LV) hypertrophy, as well as in atrial fibrillation; a slowly progressive age-dependent degeneration and decline in diastolic function, which reduces cardiac functional reserve, predisposes the heart to stress, and contributes to increased cardiovascular mortality in the elderly [7,8]; and preserved systolic function during rest that declines with physical activity [9].

Aging causes structural deterioration of the cardiac tissues that associates with deregulation of the extracellular matrix (ECM). In particular, collagen deposition (fibrosis) is a hallmark of age-dependent LV remodeling [10]. Myocardial fibrosis results from excessive deposition and accumulation of collagen in the cardiac walls; this leads to a progressive increase of ventricular stiffness with the overall effect of reduced contractility [10]. Changes to the cardiac ECM composition directly affect cardiac structure and function. For example, cardiovascular aging not only includes an increase on collagen content but also the fragmentation and rupture of elastin fibers in the arterial walls [11]. This causes reduced arterial resilience that appears to be directly related to the pathogenesis of cardiac ECM also acts as a scaffold for cardiac cells, such as cardiomyocytes, to provide anatomical support and facilitate cell-cell and cell-matrix interactions. With age, the continuous increase of cardiac compliance, leads to hypertrophic changes in cardiomyocytes [13]. These structural modifications are irreversible and result in permanent changes in cardiac function.

Gender related differences in cardiac structure and function have been reported in several clinical studies [14–17]. Data suggest some CVDs are more prominent in men, while others are seen more frequently in women [15]. These observations emphasize the concept that intrinsic cardiac alterations are not only age-dependent, but also sex-dependent, and that as aging occurs sex differences can predispose the prognosis of some cardiac pathologies.

Rodent models of cardiac aging, particularly mouse models, are a valuable tool as their cardiac aging phenotypes closely recapitulate the phenotypes of human cardiac aging [18,19]. Moreover, unlike humans laboratory mice do not develop the traditional risk factors that affect cardiac function with age, meaning that functional changes are dependent on intrinsic aging. In addition, their brief lifespan provides the opportunity to utilize mice as aging models to study the molecular, cellular, and anatomical processes involved in the intrinsic cardiac aging process within a short time period [20]. Accordingly, murine models are highly useful to investigate the underlying mechanisms involved in age-dependent LV remodeling and the physiology of cardiac aging.

In the last decades, conventional echocardiography has been routinely used in aging studies to analyze changes in cardiac structure and function both in humans and animal models [21]. More recently, strain analysis (also known as speckle tracking echocardiography, STE) emerged as a novel technique used for the assessment of LV global and segmental wall motion [22]. While strain determines how much the myocardium has deformed, strain rate indicates how fast the myocardium is deforming. This method identifies both regional and global systolic and diastolic LV function based on changes in the LV contractility [23]. STE is a recent, highly sensitive, and reproducible method that has been showed to be favorable for the examination of cardiac diseases and it is being used as a tool for the early detection of heart failure [24]. This non-invasive technique has also been used in the examination of myocardial function in translational research [25], and STE measurements further extend the quantitative parameters of conventional echocardiography.

In the present study, we had two main goals: 1) investigate sex-specific differences in cardiac ECM remodeling that occur in an age-dependent matter and 2) determine whether STE is a more sensitive tool, compared to conventional echocardiography, to identify earlier cardiac functional changes that are both sex- and age-dependent.

2. Materials and methods

2.1. Animals

Animal procedures were performed according to the "Guide for the Care and Use of Laboratory Animals" (NIH Notice Number: NOT-OD-12-020) and were approved by the Institutional Animal Care and Use Committee at the East Carolina University. Both male and female C57BL/6 mice (Charles River stock #027) were used in this study (n = 6-12/sex/age). Animals were bred in-house in the fully accredited animal facility at ECU managed by the Department of Comparative Medicine. Animals were housed at a controlled temperature (22 ± 2 °C) on a 12 h light/dark cycle, fed standard laboratory mice chow ad libitum, and had free access to tap water. Four age groups were analyzed: young (3–3.5 month old, m.o.), adult (6–6.5 m.o.), middle-aged (12–12.5 m.o.), and old (18–18.5 m.o.).

2.2. Conventional and speckle tracking echocardiography

Transthoracic echocardiography was performed using a Vevo 2100[™] system (VisualSonics) with a 30 MHz image transducer (MS400). Mice were anesthetized with 1–2% isoflurane in an oxygen mix and hair was removed from the chest. Mice were placed on a supine position

on a heated platform with embedded electrocardiogram (ECG) leads. The body temperature and heart rate were monitored throughout the imaging procedure. Core body temperature was maintained at 37 $^{\circ}$ C and all images were acquired at heart rates > 400 bpm to achieve physiologically relevant measurements. Measurements were taken from the LV parasternal long axis (B-mode) and short axis (M-mode) views. For conventional echocardiography, three images of the parasternal long axis B-Mode were used to delineate the LV trace in full diastole (see Fig. 1E) and its consecutive full systole to obtain the averaged measurements of heart rate (HR), end-diastolic volume (EDV), end-systolic volume (ESV), stroke volume (SV), ejection fraction (EF), and cardiac output (CO) using the VevoLab 1.7.1 software. The wall thickness (anterior, AW; posterior, PW) and internal diameter (ID) of the LV were measured using three consecutive cardiac cycles in short-axis M-Mode (see Fig. 1E) that were averaged to evaluate LVAW;d, LVAW;s, LVID;d, LVID;s, LVPW;d and LVPW;s by the same methods as we previously described [26–32]. Fractional shortening (FS) and EF were calculated using the Vevo Lab 1.7.1 software algorithms. For STE, tracing of the cardiac wall was performed using 2D grayscale echocardiographic films of parasternal long and short axis views with a frame rate above 200 frames per second. Image depth, width, and gain settings were optimized to improve image quality. Images in B-mode displaying clear visualization of the LV endocardial border of both axes were selected and 3 successive cardiac cycles were chosen to delineate the myocardium by tracing the endocardial margin with an adjusted epicardial border. The long axis view was used to determine the longitudinal and radial peaks, while the short axis provided the respective radial and circumferential peaks. Measurements of the peaks of strain, strain rate, displacement, and velocity were calculated using the algorithm from VevoStrain[™] (VisualSonics). The cardiac wall was separated in 6 distinct anatomical segments (anterior base, anterior middle, anterior apex, posterior apex, posterior middle, and posterior base) to determine regional strain parameters, and the average of these segments defined the global longitudinal, radial, and circumferential strain values. All echocardiographic readings/measurements were performed by one blinded individual to avoid technical variation and interpretation bias.

2.3. Collagen turnover

Collagen ELISA assays using plasma were performed using LSBio Mouse CTX/Collagen C-Terminal Telopeptide (Cat. # LS-F21349) and LSBio Mouse Procollagen I C-Terminal Propeptide (Cat. #LS-F14803). Samples from groups 6, 12, and 18 m.o. (n = 6 each) were diluted 1:10, and assays were performed per manufacturer's instructions.

2.4. Histological quantification of collagen, elastin, and myocyte cross-sectional area

Image acquisition was obtained with an Olympus BX51 Microscope (Olympus, Pennsylvania) and CellSens V1.7 software (Olympus, Pennsylvania). For each LV, one image was taken at 4×, and a minimum of five images were taken at 40×. The picro-sirius red (PSR, collagen) and Miller's elastin positive stain were then quantified utilizing Image-Pro Premier Offline 9.1 Software (Media Cybernetics, Maryland). The 40× images of each animal were quantified based on total collagen or elastin positive area (β m²) per field of view and averaged. Myocyte cross-sectional analysis was completed using the same images and software that were used for PSR collagen analysis and quantification. Only images that showed distinct cross-sections of cardiomyocytes were used, with a minimum of 10

myocytes measured per animal. The average cardiomyocyte cross-sectional area (βm^2) was calculated for each animal and compared among groups.

2.5. Protein quantification

LV proteins were extracted by Protein Extraction Reagent Type 4 (Sigma, C0356) with $1 \times$ Protease Inhibitors (Roche, #11836153001) as described previously [33]. Due to the large number of groups, samples were randomized for protein extraction to avoid experimentdependent bias and ensure reproducibility across groups. The Bradford assay was used for protein quantification with IgG serving as standards. Immunoblots against collagen 1, collagen 3, decorin, lysyl oxidase, periostin, osteopontin, Smad2/3, pSmad2/3, ERK1/2, pERK1/2, TGFβ1, TGFβRI, and TGFβRII were performed using the following antibodies and dilutions: Collagen I alpha 1 1:1000 (Novusbio, NBP2-29651), Collagen III alpha 1/COL3A1 1:1000 (Novusbio NBP2-15946), Decorin 1:2000 (R&D Systems, AF1060), Lysyl oxidase 1:2000 (LOX, Novusbio, NBP1-74065), Periostin1:6000 (R&D Systems, AF2955), Osteopontin 1:2000 (OPN, R&D Systems, AF808), Smad2/3 1:125 (R&D Systems, AF3797-SP), pSmad2/3 [p Ser465, p Ser467] 1:4000 (Novusbio, NBP2-44217), ERK1/2 1:5000 (Novusbio, NBP2-67378), pERK1/2 [Thr185, Tyr187] 1:1000 (Thermo, 44-680-G), TGFβ1 1:500 (Thermo, MA5-15065), TGFβR1 1:1000 (Thermo, MAB5871) and TGFβRII 1:500 (Thermo, AF532). Ten µg of total protein was loaded per well (n = 4/sex/age; groups 6, 12, and 18 m.o.) and visualized with Pierce reversible membrane protein stain kit to ensure equal loading and extraction reproducibility. Image acquisition was performed using a UVP ChemiDoc-It TS2 Imager. Densitometry was performed using UVP software and values were normalized to total loaded protein.

2.6. RNA extraction and cDNA amplification

RNA was obtained to determine whether age- and sex-dependent changes were present either at the transcription or translation level. Total RNA was extracted using TRIzol and the Pure Link RNA mini kit (Ambion, 12183018A) according to manufacturer's instructions. RNA was treated with ezDNAse (Invitrogen) and reverse-transcribed into cDNA using the High capacity RNA to cDNA kit (Applied Biosystems) according to the manufacturer's instructions.

2.7. Aging and extracellular matrix remodeling gene arrays

Custom gene arrays for aging pathways (24 genes,3 housekeeping genes, genomic DNA control, reverse transcription control, and positive control) and factors involved in extracellular matrix remodeling (84 genes, 5 housekeeping genes, and controls) were purchased (Qiagen) and performed using the QuantStudio Flex 6 (Applied Biosystems). Values were expressed as 2^{-Ct} .

2.8. Statistical analysis

Power analysis was used to determine group sizes (GraphPad StatMate 2) based on previous data from our lab and others. Data are reported as mean \pm SD, outliers were identified using the Grubbs method with an alpha set at 0.05 [34]. Outliers were included when it did not affect the final statistical result; when the outlier affected overall results this was noted

on the results section and the final statistical analysis was presented with and without the outlier. Comparisons between groups were performed using one-way ANOVA followed by the Student-Newman-Keuls post hoc test when the Bartlett's variation test passed or using the nonparametric Kruskal-Wallis test followed by Dunn post hoc test when the Bartlett's variation test did not pass. A p < .05 was considered significant (GraphPad InStat 3).

3. Results and discussion

3.1. C57BI/6 mice as a model of age-dependent cardiac dysfunction

A large body of evidence has firmly established the laboratory mouse as an excellent model of human aging [35–38]. As the mouse has a relatively short lifespan it allows for aging studies to proceed in a reasonable amount of time. Additionally, environmental factors that affect aging can be easily controlled [39]. In this study we used C57Bl/6 mice as a model of cardiac aging. All conventional echocardiography data was normalized according to the methods described by Hagdorn et al. [40] Shortly, one-dimensional measures (i.e. length) were indexed to body weight (BW)^{1/3}, and three-dimensional measures (i.e. volumes and mass) to BW. As in humans, we observed reduction in chamber volumes in the older animals (18 m.o.) compared to all other ages, seen as decreased end-diastolic (EDV) and end-systolic (ESV) volumes (Table 1). In accordance with these data, LV internal diameters in diastole and systole (LV IDd and LV IDs) were reduced in the old animals compared to the younger groups, suggestive of concentric remodeling. This was concomitant with preserved ejection fraction and, therefore, preserved systolic function in the adult, middle-age, and old animals. HF with preserved ejection fraction (HFpEF) is a hallmark of age-dependent cardiac dysfunction in humans [41,42]. Of note, while EF and fractional shortening (FS) did not decline after 6 months of age, young adults (3 m.o. group) displayed higher EF and FS compared to other ages. Several reports have shown that EF and stroke volume (SV) are higher in adolescence compared to adults; it was proposed that this was a result of increased growth hormones and physical activity in adolescents [42,43]. We also observed higher SV in the young adults compared to middle-age and old groups (p < .05).

Contrarily to systolic function, a decline in diastolic function is a key characteristic of cardiac aging [44,45]. While active relaxation is reduced due to age-associated decreases in sarcoplasmic reticulum calcium uptake [46,47], passive stiffness can significantly contribute to the impaired diastolic function [48,49]. As mentioned above, we observed an age-dependent reduction in volumes and dimensions, representative of decreased relaxation and increased concentric remodeling. Overall, our results demonstrate that C57Bl/6 mice are an excellent tool to study age-dependent cardiac remodeling and dysfunction as the model mimics human aging.

3.2. Sex-dependent differences in concentric remodeling and hypertrophy

The age-dependent differences observed in SV were driven only by males. While middleage and old males displayed reduced SV (p < .05) compared to young adults, females did not present SV differences with age (Fig. 1A). As expected, age-dependent decrease to chamber volumes were mostly observed in males (EDV: p < .05 18 m.o. versus 3 m.o.; ESV: p < .05 18 m.o. versus all other ages), while females displayed reduced ESV and EDV only

at 18 months compared to 12 m.o. animals. These results are suggestive of earlier concentric remodeling in males (Fig. 1B and C). Similarly, while old males presented reduced LV IDd and LV IDs compared to all other groups, old females only showed changes when compared to the middle-aged (12 m.o.) group. Other labs have reported the reproductive senescent phase of female mice to occur between 9 and 12 m.o [50–52]. It is possible that the drastic cardiac changes we are observing in 18 m.o. females, compared to 12 m.o., are a result of established reproductive senescence. Measurements of posterior (LVPW) and anterior (LVAW) wall thicknesses were sex-independent. Overall, these data indicate that LV remodeling occurs at a later stage in females compared to males and/or the remodeling rate is slower in females. To further analyze sex-related differences in LV function with age, we plotted EDV and ESV values stratified by sex to visualize the volume regulation graph, as proposed recently by Kerkhof and coworkers as a means of analyzing LV pump function, independent of afterload variations [53]. The regression lines for males and females did not differ significantly between sexes, although males presented higher linearity fit ($R^2 = 0.82$ in males versus 0.53 in females, Fig. 2). Importantly, data plotted was age-matched and both females and males presented significant EDV and ESV relationship in an age-dependent manner (p < .0001 for both sexes).

Detailed studies that report sex-differences in physiological cardiac aging in animal models are rather scarce. We compared our data to that of others and found both similarities [25,54], as well as critical differences, mainly due to the strain and age of the animals when the echocardiography was acquired. For example, Koch et al. analyzed cardiac function in both male and female FVB/N mice from 3 to 16 months of age [55]. On their study they observed both reduced systolic and diastolic function in males but not in females. This difference could be a result of the animal strain used, as well as the age of the animals; particularly, since for females we mostly observed cardiac changes only between the 12 m.o. and 18 m.o. groups. Several manuscripts on age-related changes in cardiac function report decreasing diastolic and systolic function beginning as early as 12 m.o. of age; however, those reports did not track gender differences [56–59]. When we combined all data, independent of sex, EDV, ESV, IDd, and IDs were all significantly reduced in the old mice (18 m.o.) compared to all other groups, suggestive of cardiac remodeling and hypertrophy. Indeed, the cross-section areas of cardiomyocytes were significantly higher at 18 m.o. compared to all other ages (Fig. 3), and this was independent of sex. Age-related cardiomyocyte loss can increase the mechanical burden on the surviving cardiomyocytes and lead to compensatory hypertrophy [60]. Morphometric analysis in humans suggest that the volume of LV cardiomyocytes increases with age and that this is more pronounced in men than in women [61,62]. Nonetheless, whether age-dependent cardiomyocyte loss and hypertrophy occur at different rates and through different mechanisms in male and female hearts has not been established, and additional studies are necessary to answer this question. In our mouse model, we did not observe a histological difference in cardiomyocyte hypertrophy between males and females. This raised the question whether males and females displayed differences in age-dependent ECM secretion and remodeling that could explain the age-dependent reduced chamber volumes.

3.3. Left ventricular loss of contractility

Two-dimensional STE enabled us to assess myocardial strain, i.e. deformation resulting from changes in length. Strain analysis is a derivative of Doppler imaging and has been reported to be a more direct measurement of intrinsic myocardial contractility than global values such as EF or FS [23,63]. While a positive strain value indicates elongation of tissue, a negative strain value indicates shortening of tissue. Longitudinal strain (long axis) analysis revealed higher strain rate (rate of strain change over time) at 6 and 12 m.o., compared to the young 3 m.o. group and this change was only observed in females (Fig. 4A). These data were similar to what we observed with conventional echocardiography (see Table 1). We also measured radial strain, both in the long and short axes. Both global radial strain and strain rate displayed an age-dependent increase trend, but this did not reach significant values. Finally, analysis of circumferential strain (short axis) revealed the 18 m.o. group displayed increased velocity and reduced strain rate compared to all other ages (Fig. 4B), giving evidence of increased strain deformation in the older animals. For both of these datasets, one outlier was identified and removed in the 6 month group [including outlier p < p.05 6 \times 18 and 12 \times 18; excluding outlier p < .05 3 \times 18, 6 \times 18, and 12 \times 18]. Increased circumferential strain displacement was also observed in the 18 m.o. group compared to 12 m.o. Interestingly, all circumferential changes were driven by females, while males did not display any age-dependent significant changes. This suggests STE allows for earlier detection of age-dependent and sex-specific cardiac changes. Several studies support STE measurements as a more sensitive and informative technique regarding cardiac contractility [25,64]. Shah and colleagues showed that impaired longitudinal strain could represent a novel imaging biomarker to identify patients with heart failure and preserved EF, since STE allowed for identification of impaired systolic function even when EF seemed normal [65]. In our study, STE confirmed what we observed with conventional echocardiography and further allowed to identify age-dependent strain changes in females.

3.4. Sex-specific regulation of cardiac collagen pathway and metabolism

To determine changes in myocardial matrix composition that could explain the changes observed in cardiac contractility, chamber volumes, and concentric remodeling, we first assessed total levels of LV elastin and collagen both by histological analysis and by protein expression. No significant changes were observed in elastin levels independent of sex or age. Nonetheless, a trend for an age-dependent decrease in elastin was observed, which would be expected and match the age-dependent loss of contractility. We quantified the area of interstitial collagen in the LV using PSR staining. The histological analysis showed that old, 18 m.o., mice displayed significant interstitial myocardial fibrosis compared to younger mice (Fig. 5A). This increase in fibrosis is a sign of myocardial stiffness that leads to impaired relaxation and, therefore, diastolic dysfunction. This was confirmed by immunoblot quantification of collagen type 1 (Fig. 5B, n = 4/sex/age). Age-dependent fibrosis did not differ between sexes. We also quantified collagen type 3 to assess levels of turnover, but no differences were observed independent of age or sex (Fig. 5B). Finally, we assessed levels of collagen turnover in plasma. For homeostasis, a healthy heart needs to maintain a balance between collagen synthesis and degradation (i.e. collagen turnover). Myocardial fibrosis, including age-dependent fibrosis, can result from an imbalance between the dynamics of collagen metabolism that leads to increased synthesis (deposition) of

collagen I and III with reduced or unchanged collagen degradation. As a marker of collagen synthesis, we quantified the circulatory levels of the procollagen I C-terminal propeptide (PICP); additionally, the collagen I C-Terminal telopeptide (CITP) was measured as a marker of collagen degradation [66]. Plasma levels of PICP were similar among ages; however, we observed reduced collagen degradation at 12 and 18 m.o. visualized by reduced levels of CITP (Fig. 5C). These data are in accordance with the observed interstitial collagen deposition and protein expression in these age groups. The onset of age-dependent cardiac stiffness is likely a result of increased cardiac ECM remodeling, in particular, a shift in the collagen turnover pathway towards decreased degradation resulting in an overall increase in collagen levels. To further test this hypothesis, we investigated changes in the canonic transforming growth factor (TGF)- β pathway. TGF β 1 expression in males was not different with age; however, females presented enhanced TGF β 1 expression (p < .05, Fig. 6A). We then looked at TGF β receptor (TGF β R) levels; as observed with the ligand, TGF β R1 was increased only in females and this increase was age dependent (Fig. 6B). No differences were noted on TGFBR2 for either sex. Smad2/3 was again increased in an age-dependent manner only in females (Fig. 6C) and pSmad2/3 was increased in both males and females in the 18 m.o. animals. The ratio pSmad/Smad was not different with age in the females but was increased in both 12 and 18 m.o. males (p < .05 versus 6 m.o.). Since we did not observe an increase in either TGF β 1 and TGF β R1 in males with age, we did not expect to see increased pSmad2/3 However several labs have reported that the linker region of nuclear localized Smads can undergo phosphorylation by extracellular signal regulated kinase (Erk) and c-Jun N-terminal kinase (JNK) [67–70]. This suggests that even though both male and females display age-dependent cardiac fibrosis the underlying pathways may be distinct.

Using immunoblotting, we further looked at proteoglycans and proteins known to be involved in collagen deposition and maturation that could participate in sex-specific fibrosis (Fig. 7). Decorin, a small leucine-rich proteoglycan, has been implicated in the regulation of fibrillogenesis [71]. Similar to the observations from collagen type 1, decorin levels increased in both sexes at 18 m.o. (p < .05 versus all other ages). Decorin has previously been reported to directly affect collagen structure, particularly, decorin deficiency results in mice with fragile skin, abnormal tendons, and fundamental alterations in collagen fibers [72].

Lysyl oxidase (LOX), necessary for collagen fibril crosslinking, and periostin, a matricellular protein, showed sex-dependent data. Specifically, an age-dependent increase in LOX was only present in females and periostin was increased in males only (p < .05 at 18 m.o. versus all other ages). An increase in LOX in old mice supports the observed reduction in cardiac contractility since higher levels of collagen crosslinking imply increased LV stiffness. Reports have shown periostin to associate with levels of fibrosis in failing hearts [73]. In addition, excessive periostin expression in old rat hearts (24 m.o.) has been shown to contribute to cardiomyocyte senescence [74], implicating periostin in age-dependent cardiac fibrosis and dysfunction.

Osteopontin (OPN), a phosphorylated glycoprotein that exists as an immobilized matrix protein and as a cytokine [75], was also overexpressed in both sexes at 18 m.o. compared to younger ages. OPN is secreted by several cell types including fibroblasts and macrophages

[76,77]. OPN is involved in a variety of biological processes, such as chemotaxis, adhesion support, cell survival, and wound repair [78]. In the healthy myocardium, OPN levels are negligible, but it is robustly expressed under pathological conditions [79]. Moreover, OPN cardiac expression is associated with consecutive development of extensive fibrosis, LV stiffness, and systolic dysfunction [80,81]. Our results are in accordance with this notion, both collagen type 1 (fibrosis) and OPN displayed an age-dependent increase in the LV, particularly at 18 m.o. This coincided with reduced LV chamber volumes.

Using gene array analysis, we assessed expression of 84 extracellular matrix proteins and adhesion molecules that may be involved in LV structural changes. In accordance with what we observed by collagen quantification, the collagen triple helix repeat-containing protein 1 (Cthrc1), a negative regulator of collagen deposition, was robustly decreased both at 12 and 18 m.o. in both sexes (Fig. 8). The discoidin domain receptor 1 (Ddr1) displayed an age-dependent decrease both in females and males. Ddr1 is a cell surface tyrosine kinase receptor for fibrillar collagen and regulates cell attachment to the extracellular matrix (ECM) and remodeling of the ECM by up-regulation of matrix metalloproteinases (MMPs) [82–84]. The C-type mannose receptor 2 (Mrc2), which deficiency leads to fibrosis as a result of reduced collagen uptake, was also reduced at 18 m.o. compared to younger groups; however, this reduction was driven by females. Overall, our results point to an age-dependent dysregulation of collagen metabolism that, with time, leads to cardiac fibrosis.

3.5. Cardiac homeostasis with age

Genes involved in cardiac homeostasis, such as the atrial natriuretic peptide A (Nppa), the receptor atrial natriuretic peptide receptor 1 (Npr1), and ubiquitin B (Ubb), were all reduced with age, particularly at 18 m.o. (Fig. 9). Of these, only Npr1 changes were driven by females, whereas Nppa and Ubb expression were sex independent. The cardiac hormone natriuretic peptide A (ANP), and its receptor Npr1, play a key role in cardiovascular homeostasis through regulation of natriuresis, diuresis, and vasodilation [85]. ANP is also anti-hypertrophic in the heart, which is independent of its systemic blood pressure-lowering effect. Studies using Nppa and Npr1 knockout mice, demonstrated that while dietary or pharmacological treatments lowered blood pressure, they did not prevent cardiac hypertrophy [86,87]. Additionally, cardiac-specific Npr1 knockout mice display normal blood pressure but exhibit marked cardiac hypertrophy [88]. When we plotted these markers of cardiac homeostasis against cardiomyocyte cross-sectional area (paired values), even though regression lines slopes were not different between sexes, females homeostasis significantly associated with myocyte area (p < .05 for all markers). Taken together, our results strongly suggest a link between age-dependent loss of cardiac homeostasis in females and cardiac hypertrophy.

4. Study limitations and perspectives

The use of a mouse aging model comes with inherent limitations. First, we recognize that older mice don't develop the same age-related cardiovascular pathologies (ex. atherosclerosis) as elderly humans that associate with differences in cardiac function. While this limits clinical significance, it has the advantage of allowing us to isolate only

age-specific changes. Second, we used 18 m.o. C57Bl/6 as the eldest group in our study, which is on the lower range for animals typically termed as old. Aging studies commonly refer to C57Bl mice > 17–32 m.o. as being "old"; however, some studies will term animals > 24 m.o. as senescent [89–92]. Nonetheless, it is feasible to surmise that the structural and functional changes observed at the investigated ages will be maintained with increasing age.

5. Conclusions

The purpose of this study was two-fold, first determine whether STE analysis could provide further insight in age-dependent and sex-dependent loss of cardiac contractility and function; and second, evaluate whether cardiac ECM remodeling with age evokes structural changes that differ between females and males.

Changes in conventional echocardiographic systolic indices, such as EF and FS, commonly manifest late in progressive cardiac disease and may not be sensitive enough to reveal subtle changes in the LV structure and global function. Thus, in this study we investigated whether functional changes in age-dependent cardiac remodeling could be earlier detected by STE analysis. Here the goal was to provide further insight into age- and sex-dependent loss of cardiac contractility and function. We found that both conventional echocardiography and STE provided evidence of age-related loss of contractility with preserved systolic function. However, STE allowed for the detection of sex-specific cardiac changes at an earlier life stage compared to traditional echocardiographic methods. By conventional echocardiography, most significant changes observed in LV chamber dimensions in females occurred between 12 and 18 months of age (e.g. EDV, ESV, IDd, IDs; Table 1). While males displayed a progressive decline with the 18 m.o. group showing reduced dimensions compared to all other ages. It is possible that the drastic cardiac changes we are observing in 18 m.o. females, compared to 12 m.o., are a result of established reproductive senescence. Noteworthy, measurements of STE indicated that female mice, but not males, present a significant deterioration in all circumferential strain modes in the 18 m.o. group compared to both the 6 and 12 m.o. animals.

We then focused on ECM components that could induce cardiac structural changes involved in reduced contractility, such as fibrillar collagen. We did not observe sex-differences in age-dependent deposition of cardiac collagen, a hallmark of cardiac physiological aging. Nonetheless, when we investigated other molecules involved in collagen metabolism, such as decorin, LOX, periostin, OPN, Cthrc1, Mrc2, and Ddr1, changes with age were sexspecific for periostin, LOX and Mrc2. While changes in periostin were present only in males, females presented age-dependent changes both in LOX and Mrc2. An increase in LOX affects collagen arrangement and crosslinking resulting in reduced contractility triggering concentric remodeling, which can associate with the robust differences observed in the functional parameters in the old females. Additionally, when we looked at the TGF β canonic pathway, we also observed the highest age-dependent increases in females. Notably, our results provide evidence that 1) structural proteins such as periostin and LOX (essential for collagen maturation and crosslinking) are both age-dependent and sex-specific and 2) physiological fibrosis in males and females may have distinct fibrotic pathways. These data highlight the notion that physiological LV remodeling is more complex and involve more

processes beyond collagen deposition; several factors participate in collagen metabolism – from expression, to deposition, alignment, and maturation – and these are age- and sex-specific.

In summary, STE allows for early detection of functional changes and LV remodeling with age is distinct between sexes. In particular, male mice appear to present progressive changes in cardiac structure and function, while females present drastic structural changes between 12 and 18 m.o.

Acknowledgments

We acknowledge the technical contribution of Kylie R. Kennedy and Valentine Okafor. We acknowledge funding support from the East Carolina University (US) and the American Heart Association (US) [grant number 18AIREA33960311 and 19PRE34450066].

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M-Mode short-axis

Fig. 1.

Sex-dependent cardiac dysfunction. A) Age-dependent stroke volume (SV) changes were observed only in males. B) Males show a trend for earlier concentric remodeling in old animals showing reduced end-diastolic volume (EDV) compared to young adults. C) and D) Old females displayed reduced ESV and internal diameter at diastole (IDd) compared only to middle-age while old males presented reduced ESV and IDd versus all other ages. E) Diagram depicting probe position during long-axis acquisition (left panel), the probe was rotated 90 degrees to acquire short-axis images; middle-panel displays representative image of a B-mode long-axis with LV trace; and right panel shows a representative image of M-Mode short axis with measurements of wall thicknesses and LV diameter. *p < .05 versus 3 m.o., ^p < .05 versus 6 m.o., #p < .05 versus 12 m.o., &p < .05 versus all other age groups, n = 6 - 12/age.

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Fig. 3.

Cardiomyoctye cross-sectional area. Old mice presented cardiomyocyte hypertrophy compared to all younger groups. Black circles are representative traces of cross-sections in cardiomyocytes. & p < .05 versus all other groups. n = 6/sex/age.



Fig. 4.

STE measurements. A) Longitudinal strain analysis (long-axis). B) Circumferential strain analysis (short-axis). Left panels: Both sexes; Middle-panels: Females; Right panels: Males; *p < .05 versus 3 m.o., $^p < .05$ versus 6 m.o., #p < .05 versus 12 m.o., & p < .05 versus all other age groups, n = 12-18/group (males and females).

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Fig. 5.

Interstitial collagen deposition increases with age in a sex-independent manner. A) Histological quantification of interstitial collagen deposition quantified by picro sirius red staining. B) Collagen type I and III protein expression measured by immunoblot. C) Plasma levels of PICP (collagen synthesis) and CITP (collagen degradation). n = 6/sex/age. (For interpretation of the references to colour in this figure legend, the reader is referred to the web version of this article.)

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Fig. 6.

The TGF β pathway was mostly affected in females, with increased signaling in the old mice compared to younger ages. $^{n}p < .05$ versus 6 m.o., #p < .05 versus 12 m.o., n = 4/group.

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Fig. 7.

ECM related proteins and proteoglycans with age. Decorin and osteopontin levels are increased at 18 m.o compared to younger groups and this is not dependent on sex. Lysyl oxidase was only observed at higher levels in old females, while periostin was augmented in old males. Quantification by densitometry was normalized to total protein (loaded protein) for each lane; n = 4-6/group. & p < .05 versus all groups.

Both sexes







Fig. 8.

Negative regulators of collagen deposition, such as collagen triple helix repeat-containing protein 1 (Cthrc1), discoidin domain receptor 1 (Ddr1), and C-type mannose receptor-2 (Mrc2) were all reduced with age. However, Mrc2 changes were driven by females only, n = 8/group. $^{\text{p}} < .05$ versus 6 m.o.; #p < .05 versus 12 m.o.

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Fig. 9.

Cardiac homeostasis is lost with age and in females this correlates with cardiomyocyte hypertrophy. Left panel: natriuretic peptide A; middle-panel: atrial natriuretic peptide receptor 1; and right panel: ubiquitin B. $^{p} < .05$ versus 6 m.o., #p < .05 versus 12 m.o. n = 8/group (4 males and 4 females).

Table 1

Echocardiographic (conventional) parameters normalized to BW or $BW^{1/3}$. Values are mean \pm standard deviation.

Ages	Females				Males				Both sexes			
	3 m.o.	6 m.o.	12 m.o.	18 m.o.	3 m.o.	6 m.o.	12 m.o.	18 m.o.	3 m.o.	6 m.o.	12 m.o.	18 m.o.
Body weight (g)	20 ± 2	28 ± 3	32 ± 5 *	45 ± 10 *	26 ± 4	32 ± 6	$48 \pm 7^{* \star \star}$	$39 \pm 8^{*\#}$	23 ± 4	30 ± 5 *	$39 \pm 10^{*1}$	42 ± 9 *^
LV Mass wet weight (mg)	83 ± 19	97 ± 7.0	$115\pm22^{*}$	103 ± 13	91 ± 9	113 ± 17	123 ± 24	110 ± 17	87 ± 15	$105\pm15^{\ast}$	$118\pm23^{*}$	107 ± 15 *
Heart Rate (BPM)	411 ± 20	419 ± 33	419 ± 27	448 ± 42	407 ± 9	421 ± 22	436 ± 23	471 ± 91	409 ± 15	420 ± 27	426 ± 26	460 ± 71
EDV (µl)/ BW	1.6 ± 0.5	1.8 ± 0.3	2.0 ± 0.5	$1.1\pm0.3^{\Lambda\#}$	2.0 ± 0.4	1.6 ± 0.3	1.4 ± 0.4	$1.1\pm0.5^{*}$	1.8 ± 0.5	1.7 ± 0.3	1.7 ± 0.6	1.1 ± 0.4 &
ESV (μl)/ BW	0.6 ± 0.2	0.9 ± 0.2	0.9 ± 0.4	$0.5\pm0.1^{\#}$	0.8 ± 0.1	0.7 ± 0.2	0.7 ± 0.3	0.4 ± 0.2 &	0.7 ± 0.2	0.8 ± 0.2	0.8 ± 0.3	0.4 ± 0.2 &
SV (µL)/BW	1.0 ± 0.4	0.9 ± 0.1	1.0 ± 0.4	0.7 ± 0.2	1.1 ± 0.2	0.8 ± 0.2	$0.7\pm0.2^{*}$	$0.7\pm0.3{}^{*}$	1.1 ± 0.3	0.9 ± 0.1	$0.8\pm0.3~^{*}$	0.7 ± 0.3
EF (%, normalized volumes)	64 ± 5.0	49 ± 5.0	52 ± 15	59 ± 10.0	59 ± 3.0	53 ± 6.0	52 ± 6.0	$66\pm 8.0^{\prime\#}$	61 ± 5.0	$51\pm 6.0^{*}$	52 ± 12.0	$62 \pm 9^{\Lambda \#}$
LVAWd/BW ^{1/3}	0.3 ± 0.0	0.3 ± 0.0	0.3 ± 0.0	0.3 ± 0.1	0.3 ± 0.0	0.3 ± 0.1	0.3 ± 0.0	0.3 ± 0.1	0.3 ± 0.0	0.3 ± 0.0	0.3 ± 0.0	0.3 ± 0.1
LVAWs/BW ^{1/3}	0.3 ± 0.0	0.3 ± 0.0	0.3 ± 0.1	0.4 ± 0.1	0.4 ± 0.0	0.3 ± 0.1	0.3 ± 0.0	0.4 ± 0.1	0.3 ± 0.0	0.3 ± 0.1	0.3 ± 0.1	0.4 ± 0.1
LVIDd (mm)/BW ^{1/3}	1.3 ± 0.2	1.3 ± 0.1	1.3 ± 0.1	$1.1\pm0.1^{\#}$	1.3 ± 0.2	1.2 ± 0.1	1.2 ± 0.1	0.9 ± 0.2	1.3 ± 0.2	1.2 ± 0.1	1.3 ± 0.1	1.0 ± 0.2 &
LVIDs (mm)/BW ^{1/3}	0.8 ± 0.1	1.0 ± 0.1	0.9 ± 0.1	$0.7\pm0.1^{\Lambda\#}$	0.9 ± 0.1	0.8 ± 0.2	0.9 ± 0.1	0.5 ± 0.2 &	0.8 ± 0.1	0.9 ± 0.2	0.9 ± 0.1	0.6 ± 0.2 &
LVPWd (mm)/BW ^{1/3}	0.3 ± 0.0	0.2 ± 0.0	0.3 ± 0.0	0.3 ± 0.0	0.2 ± 0.0	0.3 ± 0.0	0.3 ± 0.0	0.3 ± 0.1	0.3 ± 0.0	0.2 ± 0.0	0.3 ± 0.0	0.3 ± 0.1
LVPWs (mm)/BW ^{1/3}	0.4 ± 0.1	0.4 ± 0.1	0.4 ± 0.1	0.4 ± 0.1	0.4 ± 0.1	0.4 ± 0.1	0.3 ± 0.1	0.4 ± 0.1	0.4 ± 0.1	0.4 ± 0.1	0.3 ± 0.1	$0.4\pm0.1^{\#}$
FS (%, normalized dimensions)	41 ± 4.0	25 ± 5.0 *	$30\pm8.0^{\ast}$	36 ± 9.0	35 ± 7.0	33 ± 10.0	26 ± 6.0	$43\pm13.0^{\#}$	38 ± 6.0	29 ± 9.0	$28\pm8.0^{\ast}$	$40\pm12.0^{\prime\#}$
Cardiac output (mL/min)/BW	0.4 ± 0.1	0.4 ± 0.0	0.4 ± 0.2	0.3 ± 0.1	0.5 ± 0.1	0.4 ± 0.1	0.3 ± 0.1	$2.9 \pm 1.4 $	0.4 ± 0.1	0.4 ± 0.1	0.4 ± 0.1	1.7 ± 1.7 &
* p<.05 versus 3 m.o.,												

J Mol Cell Cardiol. Author manuscript; available in PMC 2024 April 15.

 $^{\prime\prime} p < .05$ versus 6 m.o.,

p < .05 versus 12 m.o.,

& p < .05 versus all other age groups.