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### **Cardiopulmonary exercise testing criteria for advanced therapies in patients with heart failure**

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#### **Abstract**

Many cardiology associations endorse the role of the cardiopulmonary exercise test (CPET) to define the severity of impairment of functional capacity in individuals with heart failure with reduced ejection fraction (HFrEF) and when evaluating the need for advanced therapies for these patients. The focus of the CPET within the cardiology community has been on peak volume of oxygen uptake  $(VO<sub>2</sub>)$ . However, several CPET variables are associated with outcomes in individuals with and without chronic disease and can inform clinical decisions in individuals with HFrEF. In this manuscript, we will review the normal cardiopulmonary response to a graded exercise test and review current guideline recommendations relative to CPET in patients with HFrEF.

#### **Keywords**

Cardiology; Exercise testing; Oxygen uptake; Risk assessment

#### **Introduction**

Many cardiology associations endorse the role of the cardiopulmonary exercise test (CPET) to define the severity of impairment of functional capacity in individuals with heart failure with reduced ejection fraction (HFrEF) and when evaluating the need for advanced therapies in these patients [1–5]. Starting with the seminal study by Mancini et al. [6], the focus of the CPET within the cardiology community has been on peak volume of oxygen uptake (VO2). However, several CPET variables (e.g., ventilatory efficiency, oxygen pulse, and breathing reserve) are associated with outcomes in individuals with and without chronic disease and can inform clinical decisions in individuals with HFrEF. In this manuscript, we

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review the normal cardiopulmonary response to a graded exercise test and current guideline recommendations relative to CPET in patients with HFrEF.

#### **Overview of cardiopulmonary exercise testing**

During a CPET, expired gas from the patient is continuously measured by a metabolic cart while the patient exercises at increasing intensities (e.g., graded exercise test). The test is typically performed on a treadmill or leg (cycle) ergometer. An exercise protocol is selected to allow a patient to start at a very low exercise intensity and progresses until they reach their maximum tolerance or a clinical sign or symptom is noted indicating exercise should be stopped. An exercise protocol is typically selected with the goal exercise duration of about 10 min. There are several excellent resources that extensively cover exercise testing procedures, data collection, and averaging methodology available [7–9].

Nearly all metabolic carts approved for clinical use measure expired gas on a breathby-breath frequency. The data is then reported in intervals of 10–30 s. The primary measurements made by the metabolic cart are volume of expired gas, respiratory rate, and concentration of oxygen and carbon dioxide. From these measurements and data on the temperature, humidity, and barometric pressure of the laboratory, various CPET variables are derived including  $VO_2$ , volume of carbon dioxide output  $(VCO_2)$ , and minute ventilation  $(V<sub>E</sub>)$ . Calibration and maintenance of the metabolic cart per manufacture recommendations, along with appropriately trained staff, are critical to valid and repeatable CPET data [10]. With appropriately trained staff and quality assurance procedures [11], the coefficient of variation of various CPET variables among patients with HFrEF is 4–10% [12]. While there are no formal accreditation requirements for CPET laboratories, there are some minimal standards for software considerations, system maintenance, and quality control that are important [8, 9]. However, minimal standards for staff training are lacking. Additional noteworthy items are provided in Table 1.

#### **Cardiopulmonary exercise test response**

During acute exercise, skeletal muscle cells meet the energy demands of work through aerobic and anaerobic metabolic pathways. As the exercise workload increases during a CPET, additional muscle fibers are recruited. As a result,  $VO_2$ ,  $VCO_2$ , and  $V_E$  increase with increasing exercise intensity. An example of a normal individual during a CPET using the Bruce treadmill protocol is shown in Fig. 1. As shown in Fig. 1A, during early exercise,  $VO<sub>2</sub>$ and VCO<sub>2</sub> increase at a similar rate. As exercise intensity progresses, an increasing number of muscle cells augment the production of adenosine triphosphate (ATP) from aerobic metabolism through anaerobic glycolysis which results in increasing concentrations of blood lactate. The resultant metabolic acidosis is buffered by bicarbonate and can be observed in the increasing rate of  $VCO<sub>2</sub>$  output. The respiratory centers of the autonomic nervous system respond to increasing hydrogen ion concentration by increasing  $V_E$  [10]. This is shown in the near linear response of VCO<sub>2</sub> and V<sub>E</sub> (Fig. 1B). The slope of the change in V<sub>E</sub> relative to change in  $VCO_2$  is called the  $V_E/VCO_2$  slope (aka, ventilatory efficiency).

In the simplest sense, the ability to increase  $VO<sub>2</sub>$  to meet the metabolic oxygen demand is dependent on the capacity to transport and utilize oxygen. This is described in the Fick equation that is rearranged to solve for  $VO<sub>2</sub>$  (see Fig. 2, Eqs. 1a and 1b). In this equation, the transport and utilization of oxygen are conditional on cardiac output and the arterial-mixed venous oxygen content difference, respectively. Increases in cardiac output are dependent on increases in heart rate and stroke volume [10]. And increases in arterial-mixed venous oxygen content difference are dependent on the diffusing capacity of the lungs and skeletal muscle, oxygen capacity of arterial blood, distribution of blood to the lungs and skeletal muscle, oxidative capacity of skeletal muscle, and oxyhemoglobin dissociation [10]. Factors that hinder the transportation and utilization of oxygen will limit the individual's ability to increase  $VO<sub>2</sub>$  and result in exercise intolerance.

The response of factors represented in the Fick equation and their collective effect on exercise capacity in healthy individuals and those with systolic dysfunction is shown in Fig. 2. As shown in Fig. 2, increases in peak  $VO<sub>2</sub>$  are seen in healthy individuals after an aerobic exercise training program due to the ability to increase both stroke volume and the extraction of oxygen by skeletal muscle. Normal aging results in reductions in peak stroke volume and heart rate. Patients with systolic dysfunction have a peak  $VO<sub>2</sub>$  that is as much as 70% below age-matched norms largely due to a reduced ability to increase stroke volume and heart rate, and a reduced capacity to metabolize oxygen by skeletal muscle. In addition to low peak stroke volume, chronotropic incompetence, and skeletal muscle abnormalities, additional limiters include endothelial dysfunction, pulmonary hypertension, right ventricular dysfunction, and anemia [10]. Because of the multiple factors that contribute to exercise intolerance in patients with HFrEF, resting ejection fraction is not an accurate predictor of peak  $VO<sub>2</sub>$  (Fig. 3).

A submaximal exercise test would result in an underestimated exercise capacity. Therefore, the goal of a CPET should be a sign/symptom-limited effort by the patient. The respiratory exchange ratio (RER;  $VCO_2/VO_2$ ) provides an estimate of the degree of cardiometabolic stress. As a measure of whole-body gas exchange, RER is affected by ventilatory patterns and the composition of metabolites being consumed which changes during a CPET. During steady-state conditions (e.g., rest), RER is equivalent to the respiratory quotient, which is the analogous measure at the cellular level. RER is typically 0.85–0.95 at rest but can be > 1 if the patient is overbreathing or when oscillatory ventilation is present. During early exercise, RER will remain steady at  $0.75-0.90$  (or decline to  $< 0.90$  if  $> 1$  at rest) and then gradually increase up to values as high as  $\sim$  1.3. Various peak RER criteria have been used to define a maximal cardiometabolic stress [13]. The International Society for Heart Lung Transplantation (ISHLT) defines a submaximal stress at RER = 1.05 [1, 13].

During exercise, normal individuals typically have ample pulmonary reserve despite reaching their peak  $VO<sub>2</sub>$  [14]. In other words, in individuals without high levels of aerobic training, the lungs typically do not impose a limitation on exercise capacity [15]. If a patient is limited from a pulmonary standpoint, they usually have one of the following limitations: a mechanical ventilatory limitation, a diffusion abnormality, or a gas exchange abnormality.

A mechanical ventilatory limitation is typically identified based on an individual's ventilatory reserve (aka, breathing reserve) at peak exercise. Ventilatory reserve is the percent difference between an individual's peak  $V<sub>E</sub>$  and their maximal ventilatory capacity. Maximal ventilatory capacity during exercise is estimated by measuring the maximal voluntary ventilation (MVV) or estimating MVV from the forced expiratory volume in 1 s (FEV<sub>1</sub>) [9, 10]. The latter is defined as estimated MVV = FEV<sub>1</sub>  $\times$  *k*, where *k* is a value of 35 to 40 [9, 10, 16, 17] which is a hypothetical maximal respiratory rate.

In the normal ventilatory response during a CPET, initial increases in  $V<sub>E</sub>$  are due to increases in tidal volume. Tidal volume continues to increase through about 60–70% of exercise capacity, and additional increases in  $V<sub>E</sub>$  are due to increases in respiratory rate (see Fig. 1C). At maximal effort,  $V_E$  typically reaches 70 to 85% MVV ( $-15$ % breathing reserve) in healthy individuals [9, 10]. If a patient's  $V_E$  at peak exercise is > 85% MVV (< 15% breathing reserve), they do not have adequate pulmonary reserve to continue to exercise and are mechanical ventilatory limited [18, 19].

Not all patients with a mechanical ventilatory limitation will have a breathing reserve < 15% during CPET; there may be more subtle abnormalities. A healthy individual should be able to augment tidal volume during exercise to 2–3 times their resting value [18–20]. In addition, they should be able to achieve a maximal tidal volume that is approximately 50–60% of their resting vital capacity [21]. Finally, the normal response for respiratory rate does not typically exceed 50 breaths.min−1 even at peak exercise [10]. Rapid, shallow breathing is an inefficient means to exchange gas, and a high respiratory rate (with a likely corresponding limitation in tidal volume) can also be an example of a mechanical ventilatory limitation.

A mechanical ventilatory limitation can also be defined by dynamic hyperinflation. When patients begin to exercise, they will have a corresponding increase in their tidal volume and respiratory rates secondary to increases in ventilatory demand. If expiratory time during exercise is insufficient to return to baseline end-expiratory lung volume, patients will begin to trap gas. This process is referred to as dynamic hyperinflation [22]. As exercise continues, dynamic hyperinflation can lead to mechanical inefficiency and reduction in tidal volume and prevent necessary augmentation of  $V_E$  [22]. This process will ultimately accelerate a ventilatory limitation [22]. Dynamic hyperinflation is shown in Fig. 4. Note the decreasing tidal volume despite increasing workload. While it is feasible patients with HFrEF can develop air trapping and dynamic hyperinflation during an exercise test, it is typically the result of other comorbid conditions, especially reactive airway disease, asthma, or chronic obstructive pulmonary disease.

Oxygen desaturation during exercise can be a clue to underlying pulmonary disease; however, it is rare to have a corresponding reduction in peak  $VO<sub>2</sub>$  unless a patient has significant arterial hypoxemia [23]. As such, exercise capacity is typically not exclusively limited by a diffusion abnormality unless a patient has a significant arterial desaturation < 89% [24]. Using pulse oximetry, a technically significant drop in oxygen saturation during exercise is  $5\%$  from rest and should be confirmed with arterial blood gases [9].

Ventilatory efficiency and respiration are governed by the ventilatory demand equation (aka, modified alveolar equation; see Eq. 1) [9, 10, 25]. As shown in the rearranged version of this equation,  $V_E/VCO_2$  is directly related to ventilatory dead space  $(V_D/V_T)$  and inversely related to Pa<sub>CO2</sub> [9, 10]. An elevated  $V_E/VCO_2$  indicates an increased ventilatory requirement to eliminate a given amount of  $CO<sub>2</sub>$  due to inefficient gas exchange [9, 10] or a hyperventilatory response to exercise secondary to extrapulmonary mechanisms [25]. Many disease processes can lead to pathological elevations in  $V_E/VCO_2$ . This includes interstitial lung disease [26], chronic obstructive pulmonary disease [27, 28], pulmonary hypertension [29], congestive heart failure [30], and neuromuscular diseases [31]. However, differentiating pulmonary diseases causing gas exchange abnormalities from underlying cardiovascular processes by exclusively using the  $V_{E}/VCO_{2}$  requires arterial blood gases. During a CPET,  $V_F/VCO_2$  gradually declines with increasing exercise intensity until 60– 80% of exercise capacity after which it begins to increase due to compensatory increases in  $V_E$  (see Fig. 1D). The nadir of  $V_E/VCO_2$  is the best estimate of increases in dead space ventilation [32]. In the absence of a hyperventilatory response to exercise (with a corresponding decrease in PaCO<sub>2</sub>), a  $V_E/VCO_2$  nadir that is greater than normal for age suggests an increase in dead space ventilation [10, 32]. In healthy individuals,  $V_{E}/VCO_{2}$ increases with age and is higher in women (see Fig. 5) [32]. Based on data from Sun et al. [32], a  $V_F/VCO_2$  nadir 25 is above the upper limit of normal for men and women across all age groups and might serve as a convenient "rule of thumb."

$$
V_E = [863 \times VCO_2]/[Pa_{CO2} \times (1-V_D/V_T)]
$$
  
Rearranged, V<sub>E</sub>/VCO<sub>2</sub>=863/[Pa<sub>CO2</sub> × (1-V<sub>D</sub>/V<sub>T</sub>)] (1)

where  $VCO_2$  is the volume of carbon dioxide to be exhaled,  $Pa_{CO2}$  is the partial pressure of  $CO_2$  in arterial blood,  $V_D$  is the physiologic dead space, and  $V_T$  is the tidal volume.

It is important to note that  $V_F/VCO_2$  (aka,  $V_F/VCO_2$  ratio) can be calculated at any time point during a CPET with the nadir being the best representation of increased dead space ventilation. However, in the HFrEF literature, the slope of the change in  $V_E$  versus change in VCO<sub>2</sub> (V<sub>E</sub>/VCO<sub>2</sub> slope) during exercise is reported more often than V<sub>E</sub>/VCO<sub>2</sub>. Although the  $V_F/VCO_2$  slope is calculated using linear regression from the start of exercise up to anaerobic threshold (e.g., the onset of exercise-induced metabolic acidosis) or to the end of exercise, the relationship between change in  $V_E$  and change in  $VCO_2$  is hyperbolic and the nadir of  $V_F/VCO_2$  is similar to the  $V_F/VCO_2$  slope (see Fig. 1B, D).

Over the past 30 years, there have been many studies that support a strong and independent relationship between various CPET variables and outcomes in patients with HFrEF. Among these, the study by Brawner et al. [33] is one of the few to assess the prognostic value of a majority of proposed CPET variables in a side-by-side comparison. Among patients with HFrEF ( $n = 1201$ ), they evaluated the relationship of 36 CPET variables to risk for a composite outcome of all-cause mortality, left ventricular assist device implantation, or cardiac transplantation [33]. After adjustment for age, sex, ejection fraction, and betaadrenergic blockade, all but 5 variables were related to the composite outcome [33]. The

rank order of the variables that were significantly associated with the composite outcome is shown in Table 2.

The Metabolic Exercise Test Data Combined with Cardiac and Kidney Indexes (MECKI) is a prospective, multisite study (13 sites in Italy) to develop a model to predict cardiovascular death or heart transplant that incorporates CPET data along with other clinical data (e.g., renal function, ejection fraction) in patients with HFrEF ( $n = 2716$ ) [34]. From a list of 19 CPET variables that were considered in a stepwise selection method, percent-predicted maximum peak  $VO<sub>2</sub>$  and  $V<sub>E</sub>/VCO<sub>2</sub>$  slope were the only CPET variables retained in the final model along with hemoglobin, serum sodium, left ventricular ejection fraction, and glomerular filtration rate [34]. Among the many studies of HFrEF and prognosis, peak VO<sub>2</sub> (in mL.kg<sup>-1</sup>.min<sup>-1</sup> or % predicted) and V<sub>E</sub>/VCO<sub>2</sub> slope are consistently the strongest prognostic variables. An oscillatory response of ventilation (e.g., exercise oscillatory ventilation) is also frequently reported as a strong predictor.

#### **Overview of guideline statements on CPET**

Professional associations from the USA and Europe advocate the role of CPET to define advanced HF and to guide listing for advanced therapies in patients with HF [1–3, 5]. CPET recommendations from relevant guideline statements are shown in Table 3. The most detailed recommendations are from the ISHLT [1, 13] in which they provide advice for several patient characteristics (see Table 4). Criteria for peak  $VO<sub>2</sub>$  from the ISHLT is conditional on the presence of beta-adrenergic blockade which is based on the mortality benefit of beta-adrenergic blockade with no change in peak  $VO<sub>2</sub>$  [13].

The ISHLT recommends using a percent of predicted maximum  $\rm VO_2 < 50\%$  in addition to peak VO<sub>2</sub> < 12 (or 14) mL·kg<sup>-1</sup>·min<sup>-1</sup> in patients < 50 years and women (Table 4) [1, 13]. Several equations to predict normal maximum  $VO<sub>2</sub>$  have been published that are based on sex, age, height, and/or weight [35]. While the ISHLT does not recommend which VO2 prediction equation should be used, it is important to note that there are clinically meaningful differences in the identification of patients with predicted  $\text{VO}_2$  < 50% based on the equation used [35]. Observations by the authors suggest that the most frequently used equations in studies of CPET in patients with HF are those from Wasserman and Hansen [10]. Other authors have also recommended using the equations by Wasserman and Hansen [36]. It is also important to note that the Wasserman-Hansen equations solve for a predicted normal maximum VO<sub>2</sub> in L·min<sup>-1</sup>. A patient who is obese may have a peak VO<sub>2</sub> in L·min<sup>-1</sup> that is near normal, but a low peak  $VO_2$  when indexed to their body mass (i.e.,  $mL·kg<sup>-1</sup>·min<sup>-1</sup>$ ).

The ISHLT recommends using a  $V_F/VCO_2$  slope > 35 when the peak VO<sub>2</sub> < 12 (or 14) mL·kg−1·min−1 but the peak RER < 1.05, suggesting a submaximal cardiometabolic stress (Table 4) [1, 13]. While there are many studies to support using  $V_E/VCO_2$  slope to risk stratify patients with HF, it is unclear if the risk associated with a  $V_E/VCO_2$  slope > 35 is similar to a peak VO<sub>2</sub> < 12 (or 14) mL·kg<sup>-1</sup>·min<sup>-1</sup>. It is also unknown if a V<sub>E</sub>/VCO<sub>2</sub> slope > 35 represents a similar risk in patients with and without beta-adrenergic blockade, between men and women, and across age groups.

To address some of this knowledge gap, Ehrman et al. [36] reported the 1- and 3-year survival rates free from all-cause death, left ventricular assist device implant, or cardiac transplant among 1085 patients with HFrEF (33% women; 79% on beta-adrenergic blockade). As shown in Fig. 6, the % predicted  $VO_2$  and  $V_E/VCO_2$  slope associated with an event-free survival that exceeded the 1-year cardiac transplant survival rate were similar to the thresholds recommended by the ISHLT, but peak VO<sub>2</sub> (in mL·kg<sup>-1</sup>·min<sup>-1</sup>) was higher. In addition, the survival rate between men and women over a median of 5.7 years was not significantly different for predicted  $\rm VO_2 < 50\%$  but was significantly different for peak  $\rm VO_2$  $< 12 \text{ mL} \cdot \text{kg}^{-1} \text{min}^{-1}$  and V<sub>E</sub>/VCO<sub>2</sub> slope 36 [37]. More work is needed to refine the CPET criteria recommended by the ISHLT.

Finally, the ISHLT recommends calculating the lean body mass-adjusted peak  $VO<sub>2</sub>$  in patients who are obese (Table 4) [1, 13]. However, determining lean body mass requires additional equipment and expertise that is likely not available in most CPET laboratories or cardiology clinics.

#### **Conclusions**

In this manuscript, we reviewed the normal cardiopulmonary response to a graded exercise test and current guideline recommendations relative to CPET in patients with HFrEF. We just touched the surface of the data available from a CPET. For more in-depth reading, we suggest the 2003 review by the American Thoracic Society [9] or the text by Sietsema et al. [10]. CPET provides unique information on the physiological response to exercise, is useful in patients with HFrEF to determine the degree to which cardiac pathology limits their exercise capacity, and it provides valuable prognostic information.

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#### **Availability of data and materials**

Not applicable. The article type is a review.

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#### **Fig. 1.**

Exercise response of an apparently healthy individual who performed the Bruce treadmill protocol to maximum capacity. HR, heart rate; RR, respiratory rate; TV, tidal volume;  $VCO<sub>2</sub>$ , volume of carbon dioxide output;  $V<sub>E</sub>$ , minute ventilation;  $VO<sub>2</sub>$ , volume of oxygen uptake



#### **Fig. 2.**

Factors contributing to the ability to transport and utilize oxygen in apparently healthy individuals and those with systolic dysfunction.  $C(a-v)O_2$ , arterial-mixed venous oxygen content difference; HR, heart rate; SV, stroke volume; VO<sub>2</sub>, volume of oxygen uptake. Upward arrow (↑), increase; downward arrow (↓), decrease; left right arrow (↔), no-tominimal change

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Scatter plot of resting left ventricular ejection fraction and peak oxygen uptake  $(VO<sub>2</sub>)$  in patients with heart failure with reduced ejection fraction tested at Henry Ford Hospital

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#### **Fig. 4.**

Example of dynamic hyperinflation during exercise as demonstrated by the decreasing tidal volume (TV) despite increasing work

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#### **Fig. 5.**

Nadir of  $V_E/VCO_2$  in men and women. Bars represent the mean, and the error bars are the upper limit of normal (i.e.,  $1.96 \times$  standard deviation). Horizontal dashed line represents "rule of thumb" upper limit of normal for men and women. Data adapted from Sun et al. [32]



#### **Fig. 6.**

Logistic regression scatterplots for a 1- and 3-year composite outcome for each cardiopulmonary exercise test variable. The probability of survival free from death, left ventricular assist device implant, or cardiac transplant is depicted using logistic regression for the composite outcome at 1 and 3 years for peak  $VO_2$ , percent-predicted peak  $VO_2$ , and  $V_E/VCO_2$  slope. Each individual's predicted survival probability is plotted, and a line of best fit is drawn for both men (blue dots) and women (green dots). Perspective horizontal dashed lines are placed on the graphs to depict the 1- (84%) and 3-year (78%) North

American cardiac transplant survival rate.  $V_E/VCO_2$  slope, slope of minute ventilation relative to carbon dioxide exhaled; VO<sub>2</sub>, peak oxygen uptake. Figure from Ehrman et al. [37]. Reprinted with permission from Elsevier

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Additional noteworthy items when considering a cardiopulmonary exercise test (CPET) Additional noteworthy items when considering a cardiopulmonary exercise test (CPET)

• Peak VO<sub>2</sub> is  $\sim$  10% higher when a test is performed on a treadmill compared to an upright leg (cycle) ergometer • Peak VO<sub>2</sub> is  $\sim$  10% higher when a test is performed on a treadmill compared to an upright leg (cycle) ergometer

A CPET *cannot* be performed on patients who require supplemental oxygen without additional equipment that might not be available in your local laboratory • A CPET cannot be performed on patients who require supplemental oxygen without additional equipment that might not be available in your local laboratory

• A CPET requires a sign/symptom-limited maximal effort by the patient • A CPET requires a sign/symptom-limited maximal effort by the patient

· It is critical that CPET staff are trained in the normal and anticipated pathologic response of CPET variables • It is critical that CPET staff are trained in the normal and anticipated pathologic response of CPET variables

· On some metabolic carts, the respiratory exchange ratio (RER) is labelled the respiratory quotient (RQ) • On some metabolic carts, the respiratory exchange ratio (RER) is labelled the respiratory quotient (RQ) • Performing a CPET with invasive monitoring of arterial/pulmonary pressures along with blood gases provides measured oxygen uptake for the calculation of the Fick-derived cardiac output • Performing a CPET with invasive monitoring of arterial/pulmonary pressures along with blood gases provides measured oxygen uptake for the calculation of the Fick-derived cardiac output

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### **Table 2**

a to a composite outcome of death, left ventricular assist device Relative ranking of cardiopulmonary exercise test variables based on and their association<sup>a</sup> to a composite outcome of death, left ventricular assist device Relative ranking of cardiopulmonary exercise test variables based on and their association implant, or heart transplant in patients with heart failure with reduced ejection fraction implant, or heart transplant in patients with heart failure with reduced ejection fraction



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Based on a Cox regression analysis adjusted for age, sex, ejection fraction, and beta-adrenergic blockade therapy Based on a Cox regression analysis adjusted for age, sex, ejection fraction, and beta-adrenergic blockade therapy

 $b$  circulatory power = peak VO<sub>2</sub> (mL-kg<sup>-1</sup>-min<sup>-1</sup>) × peak systolic blood pressure  $^0$ Circulatory power = peak VO2 (mL·kg<sup>-1</sup>·min<sup>-1</sup>) × peak systolic blood pressure

 $\mathbf{c}_{\text{Ventilatory power = peak systolic blood pressure/VEVOCO2 slope}}$  Ventilatory power = peak systolic blood pressure/V E/VCO2 slope

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# **Table 3**

Recommendations relevant to cardiopulmonary exercise testing from guideline statements on patients with heart failure (HF) Recommendations relevant to cardiopulmonary exercise testing from guideline statements on patients with heart failure (HF)



LVAD left ventricular assist device, VCO2 volume of carbon dioxide exhaled, VO2 volume of oxygen uptake, VEminute ventilation, ISHLT International Society for Heart Lung Transplantation VE minute ventilation, ISHLT International Society for Heart Lung Transplantation LVAD left ventricular assist device, VCO2 volume of carbon dioxide exhaled, VO2 volume of oxygen uptake,

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# **Table 4**

Listing criteria for heart transplantation based on cardiopulmonary exercise test data from the International Society for Heart Lung Transplantation Listing criteria for heart transplantation based on cardiopulmonary exercise test data from the International Society for Heart Lung Transplantation

