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## Delivery of therapeutic agents and cells to pancreatic islets: Towards a new era in the treatment of diabetes

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### Abstract

Pancreatic islet cells, and in particular insulin-producing beta cells, are centrally involved in the pathogenesis of diabetes mellitus. These cells are of paramount importance for the endocrine control of glycemia and glucose metabolism. In Type 1 Diabetes, islet beta cells are lost due to an autoimmune attack. In Type 2 Diabetes, beta cells become dysfunctional and insufficient to counterbalance insulin resistance in peripheral tissues. Therapeutic agents have been developed to support the function of islet cells, as well as to inhibit deleterious immune responses and inflammation. Most of these agents have undesired effects due to systemic administration and off-target effects. Typically, only a small fraction of therapeutic agent reaches the desired niche in the pancreas. Because islets and their beta cells are scattered throughout the pancreas, access to the niche is limited. Targeted delivery to pancreatic islets could dramatically improve the therapeutic effect, lower the dose requirements, and lower the side effects of agents administered systemically. Targeted delivery is especially relevant for those therapeutics for which the manufacturing is difficult and costly, such as cells, exosomes, and microvesicles. Along with therapeutic agents, imaging reagents intended to quantify the beta cell mass could benefit from targeted delivery. Several methods have been developed to improve the delivery of agents to pancreatic islets. Intraarterial administration in the pancreatic artery is a promising surgical approach, but it has inherent risks. Targeted delivery strategies have been developed based on ligands for cell surface molecules specific to islet cells or inflamed vascular endothelial cells. Delivery methods range from nanocarriers and vectors to deliver pharmacological agents to viral and non-viral vectors for

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the delivery of genetic constructs. Several strategies demonstrated enhanced therapeutic effects in diabetes with lower amounts of therapeutic agents and lower off-target side effects. Microvesicles, exosomes, polymer-based vectors, and nanocarriers are gaining popularity for targeted delivery. Notably, liposomes, lipid-assisted nanocarriers, and cationic polymers can be bioengineered to be immune-evasive, and their advantages to transport cargos into target cells make them appealing for pancreatic islet-targeted delivery. Viral vectors have become prominent tools for targeted gene delivery. In this review, we discuss the latest strategies for targeted delivery of therapeutic agents and imaging reagents to pancreatic islet cells.

## Keywords

Targeted delivery; Pancreatic islet; Beta cells; Diabetes; Type 1 diabetes; Type 2 diabetes; T1D; T2D; Nanocarriers; Cell therapy; Exosomes; Microvesicles

## 1. Diabetes mellitus, pancreatic islets, and insulin-producing beta cells

In the USA, diabetes mellitus affects more than 9% of the population, is the seventh leading cause of death, and its incidence is increasing (Cowie et al., 2018). Diabetes mellitus manifests clinically with elevation of glucose concentration in the blood – a condition termed hyperglycemia. Chronic hyperglycemia and broad, rapid swings in glycemia cause devastating acute and chronic complications. This disease results from a lack, dysfunction, or insufficiency of pancreatic islet beta cells, the cells that release insulin to control glucose metabolism (Fig. 1) (Cowie et al., 2018). Patients with type 1 diabetes mellitus (T1D) and advanced type 2 diabetes (T2D) require life-long treatment with exogenous insulin to survive. Despite advances in treatment strategies, complications of diabetes mellitus, hypoglycemic unawareness, and severe hypoglycemic episodes still lead to high morbidity and mortality in advanced disease stages.

The various forms of diabetes mellitus, including T1D, T2D, and genetic forms, involve endocrine cells and primarily beta cells with a central role in the hormonal control of glucose metabolism. These endocrine cells reside in the pancreas, clustered in groups of cells that are termed pancreatic islets or islets of Langerhans and that constitute approximately 1–2% of the volume of the pancreas (Abdulreda and Berggren, 2021). The main constituents of pancreatic islets are insulin-secreting beta cells and glucagon-secreting alpha cells.

A rise in blood glucose levels, such as after the ingestion of a meal, stimulates islet beta cells to release the hormone insulin. Insulin has systemic effects, determining glucose utilization for energy and energy storage in various tissues, hence lowering blood glucose levels (Fig. 1).

In certain individuals, an autoimmune attack leads to a progressive loss of beta cells and thus loss of insulin release, resulting in T1D (Fig. 1) (Pugliese, 2014). In T1D patients, the autoimmune attack causes beta cell loss, and the residual beta cells become insufficient to adequately regulate body glycemia, leading to onset of life-threatening T1D (Eisenbarth, 2010). In other individuals, a combination of predisposing genetic factors, improper diet,

and sedentary lifestyle determine chronic increase in blood glucose (hyperglycemia), paralleled by the acquisition of resistance to the effect of insulin in peripheral tissues (insulin resistance). Insulin resistance and chronic hyperglycemia impart beta cell stress and determine dysfunction of beta cells, leading to Type 2 Diabetes (T2D) (Fig. 1) (Cowie et al., 2018). In certain individuals, genetic variants impair development and function of pancreatic islet cells and insulin-producing beta cells, leading to genetic forms of diabetes mellitus.

## 2. Current and emerging therapeutics for diabetes mellitus

The current therapeutic options for diabetes mellitus include insulin therapy, intended to substitute the function of beta cells, and pancreas or pancreatic islet transplantation, intended to replace beta cells (see BOX 1). These therapeutic options have limitations. Insulin therapy has the potential to cause life-threatening iatrogenic hypoglycemia (a dangerous decrease of blood glucose due to the drug); moreover, it provides suboptimal glycemic and metabolic control. Pancreas transplantation has substantial risks of morbidity and mortality. Both pancreas and pancreatic islet transplantation are limited by insufficient donor organ availability and the requirement of chronic immunosuppression - which is associated with side effects and health risks (see BOX 1).

Looking ahead, a multitude of therapeutic strategies are emerging (see BOX 2). Glucagon-like peptide 1 (GLP-1) Receptor agonists and Dipeptidyl peptidase-4 (DPP-4) inhibitors have been developed for the potentiation of beta cell function. Immunomodulatory agents such as low-dose anti-thymocyte globulin (ATG), low-dose interleukin-2 (IL-2), anti-CD3, and anti-tumor necrosis factor  $\alpha$  (TNF $\alpha$ ) antibodies are under intense investigation to inhibit T1D autoimmunity against beta cells. Cell therapies are under development for the replacement of beta cells and the inhibition of beta cell autoimmunity. Growth factors and small molecules are under investigation for their ability to stimulate beta cell replication and regeneration (see BOX 2). Notably, many of these emerging strategies aim at exerting effects on beta cells or in the pancreas environment. Hence, targeted delivery strategies for such agents could be highly beneficial.

## 3. Need for targeted delivery of therapeutic agents to pancreatic islets

An array of agents can stimulate beta cell function, modulate beta cell gene expression, or increase beta cell proliferation (see BOX 2). Other agents can inhibit autoimmunity and prevent beta cell loss (see BOX 2). One problem that most of these agents have in common is that systemic administration leads to a range of off-target, undesired side effects. Targeted delivery strategies could improve substantially the effect of therapeutic agents designed to yield effects on beta cells or in the pancreas environment. Delivery of such agents to the pancreatic islet environment could result in an amplified effect for the preservation or regeneration of functional beta cells, with minimal side effects. Innovative approaches, presented in the next paragraphs, are allowing the *in vivo* targeted delivery of agents to pancreatic islets, beta cells, or inflamed pancreatic islets.

#### 4. Surgical approach for targeted delivery: intra-arterial administration in the pancreatic arteries

The pancreas is perfused from arteries branching from the abdominal aorta. Although pancreatic islets constitute only 1–2% of the pancreatic mass, they are highly vascularized and receive 5–10% of the pancreatic blood flow (Brissova and Powers, 2008). (Brissova and Powers, 2008). The endothelium of pancreatic islets is fenestrated, a feature that facilitates exchanges of solutes (Brissova and Powers, 2008). The body and tail of the pancreas contain most of the islet cells (van Suylichem et al., 1987; Wittingen and Frey, 1974); these regions of the pancreas are perfused by the dorsal pancreatic artery and great pancreatic artery (Wu et al., 2011).

MSCs for diabetes therapy have been successfully infused through the pancreatic arterial system in an attempt to inhibit autoimmune processes and improve islet endocrine function (Cai et al., 2016). In a pilot randomized controlled trial, Cai and colleagues infused Umbilical Cord (UC)-derived MSC and BM-derived stem cells through the dorsal pancreatic artery or its substitute supplying the pancreatic body and tail (Cai et al., 2016). This treatment resulted in improved metabolic profiles in patients with T1D, with a doubling of endogenous C-peptide production, a marker of beta cell function, at 1 year (Cai et al., 2016).

This surgical approach enables a first passage of the therapeutic agent or imaging reagent through the pancreatic vascular bed. It requires a skilled surgeon and is facilitated by imaging (angiography). The surgical procedure requires deep sedation of the patient. Importantly, it bears risks connected with puncturing of the arteries and of the pancreas.

#### 5. Targeting cell surface molecules specific of islet cells

One key goal of targeted delivery strategies for diabetes mellitus is to facilitate accumulation of an agent of interest in pancreatic islet cells. Pancreatic islets contain a wide range of different cell types, characterized by specific expression of cell surface molecules (Dybala and Hara, 2019; RKPHodson, 2018; Cabrera et al., 2006). During pancreatic islet development, CD142+ pancreatic endoderm cells mature into CD200+ and CD318+ endocrine cells (Kelly et al., 2011). Cell-surface markers have been identified for all major cell types of the human pancreas: monoclonal antibodies, such as H1C0, H1C1 and DH1C2/3 clones, are especially useful because of their specificity for pancreatic islet endocrine cells (Dorrell et al., 2016).

Recently, four distinct subtypes of pancreatic islet beta cell have been described, known as Beta 1–4: they have different kinetics of insulin release, and they are distinguished by specific surface marker expression of ST8S1A1 and CD9 (Dorrell et al., 2016). The majority of proinsulin + beta cells appear to be CD9+ (Kelly et al., 2011). These recent observations may open the path to strategies aimed at targeting specific beta cell subtypes, such as to affect specifically mature and functional or immature and dormant beta cells.

The GLP-1 receptor (GLP-1R) represents a major target on the surface of islet beta cells. The GLP-1R receives the signal of GLP-1, an incretin peptide hormone released by small

intestinal cells in response to nutrient ingestion, and released also by a subtype of islet alpha cells (Campbell et al., 2020). GLP-1 binds to GLP-1R on the surface of islet beta cells, potentiating glucose-induced insulin secretion, upregulating insulin biosynthesis, and inhibiting apoptosis of beta cells. GLP-1R has been targeted to deliver therapeutic agents and imaging agents to islet cells *in vivo*, predominantly via conjugation of the GLP-1R ligand exendin-4 to moieties of interest in nanoparticles (Wang et al., 2014). One limitation of GLP-1R targeting is that this molecule is broadly expressed in cells of the gastrointestinal tract, hence the selectivity for islet cells is limited.

Vesicular monoamine transporter 2 (VMAT-2) is a cell-surface molecule responsible for the release of dopamine and serotonin. VMAT-2 is found on both beta cells and neuroendocrine cells (Sheehy et al., 2019). VMAT-2 is highly expressed in pancreatic islet cells (Anlauf et al., 2003). Notably, VMAT-2 has a high specificity for islet beta cell targeting: VMAT-2 was found to be expressed in insulin-producing beta cells but not in glucagon-, somatostatin-, or pancreatic polypeptide-producing cells (Anlauf et al., 2003). VMAT-2 is present in cell types that store and release monoamines (Anlauf et al., 2003). VMAT2 gene expression may differ in subsets of beta cells (Harris et al., 2008).

The Prostaglandin D2 receptor 2, also called GPR44, is localized into the cell surface, binds Prostaglandin D2, and appears to be almost exclusively restricted to human beta cells (Hellstrom-Lindahl et al., 2016; Lindskog et al., 2012). Zinc transporter 8 (ZnT8) is a zinc transporter related to the beta cell function of insulin secretion. Frequent insulin secretion exposes ZnT8 to the cell surface (Merriman et al., 2018). Ligands and targeting moieties that bind the above cell surface molecules appear to have good specificity for beta cells, and have been utilized for the targeted delivery of agents to beta cells (see Fig. 2, Fig. 3, Table 1). The field of targeted delivery utilizing islet cell-specific and beta cell-specific cell surface marker appears to be largely unexplored; further analyses are warranted.

## 6. Targeting cell surface molecules of inflamed endothelial cells and inflamed pancreatic islets

Because of their function in endocrine hormone release, pancreatic islets are highly vascularized and thus rich of vascular endothelial cells. When pancreatic islets become inflamed, such as during development of T1D and around the time of disease onset (peri-onset period), islet vascular endothelial cells increase expression of adhesion molecules on the luminal surface and recruit immune cells (Figs. 2 and 4). Endothelial cells respond to inflammatory cytokines by overexpressing the adhesion molecules intercellular adhesion molecule 1 (ICAM-1, CD54), E-selectin (CD62E), P-selectin, L-selectins and vascular cell adhesion molecule VCAM-1. These molecules render inflamed endothelial cells “sticky”: they become docking sites for circulating immune cells, endothelial progenitor cells (EPC), and MSC (Linn et al., 1994; Martin et al., 1996; Morgan et al., 2014; Pugliese, 2016; Pezhman et al., 2021; Chen et al., 2020; Phillips et al., 2008; Koh et al., 2000).

To adhere to inflamed endothelia and initiate extravasation, immune cells present the corresponding ligands, e.g.: Lymphocyte function-associated antigen 1 (LFA-1) for ICAM-1 (Wu et al., 2019), very late antigen-4 (VLA-4) for VCAM-1, and the carbohydrate Sialyl

Lewis<sup>X</sup> for E- and L-selectins (Abdi et al., 2015). These binding partnerships have been utilized for the development of targeted delivery systems. The LFA-1:ICAM-1 binding appears of great interest. ICAM-1, a type I transmembrane protein expressed by endothelial cells, is a critical regulator of immune responses: when overexpressed, it facilitates the trans-endothelial migration of T-cell to sites of inflammation. The major binding partner for ICAM-1 is Leukocyte function antigen-1 (LFA-1, CD11a/CD18), a T-cell integrin (Staunton et al., 1990) that enables T cell adhesion to the inflamed endothelium. The LFA-1 alpha subunit I-domain (LFA-1-Id) contains a binding site for ICAM-1 (Lee et al., 1995; Edwards et al., 1995), and could be thus be utilized for targeted delivery. The very late antigen-4 (VLA-4), expressed by multiple immune cells, is the main ligand for VCAM-1 (Gorelik et al., 2012). Multiple studies have employed the VLA-4:VCAM-1 targeting to deliver MSCs to endothelial cells (Majumdar et al., 2003; Ruster et al., 2006; Liu et al., 2018).

Selectins, transmembrane glycoproteins, are adhesion molecules central to the docking and trafficking of immune cells and platelets: E-selectin is found on endothelial cells, L-selectin is found mainly on leukocytes, and P-Selectin is found mainly on platelets and endothelial cells (Bevilacqua and Nelson, 1993). E-selectin is an inducible cell-adhesion molecule that helps localize circulating cells to the inflamed vascular endothelium (Leeuwenberg et al., 1992). Inflammation causes E-selectin to become upregulated on endothelium (Oh et al., 2007; Dedrick et al., 2003). E-selectin binds the P-selectin glycoprotein (CD162), CD44, and Hematopoietic Cell E- and L-selectin ligand (HCELL, a sialofucosylated form of CD44). These are expressed in circulating cells (Lasky, 1992), stem cells, progenitor cells, endothelial progenitor cells (EPC), and hematopoietic cells (Sackstein, 2010). CD162 helps platelet-monocyte complexes and monocytes tether to inflamed endothelium (da Costa Martins et al., 2007). HCELL enables docking of circulating cells to inflamed endothelial cells expressing E-selectin. EPCs express both E-selectin, as well as the E-selectin ligand (Oh et al., 2007). The existing physiological and pathological mechanism that enables the docking of immune cells to inflamed endothelium can thus be utilized to deliver therapeutic cells to target sites.

In Type 1 Diabetes, an islet-specific activation of the endothelium appears to precede overt diabetes and subsequent systemic changes in the endothelium. This is evident in the NOD mouse of T1D. Notably, in this mouse model, ICAM-1 deficiency or blockage of the ICAM-1 and LFA-1 interaction can prevent diabetes (Martin et al., 2001; Yagi et al., 1995). In the presence of a functional ICAM-1 gene, a hyperexpression of ICAM-1 occurs in the islet endothelium of NOD mice, in parallel with insulinitis, shortly before and around the time of onset of diabetes (Linn et al., 1994; Martin et al., 1996) and before systemic endothelial activation resulting from hyperglycemia. A similar sequence of events could occur in patients with T1D, as suggested by the observation of inflammatory changes specifically in the islet endothelium appearing in patients with elevated risk of T1D and around the time of initial disease manifestation (Morgan et al., 2014; Pugliese, 2016). Hence, it could be appropriate to target the inflamed islet endothelium in the peri-onset period of T1D. In Type 2 Diabetes, there seems to be more overlap in the timing of inflammatory changes in the endothelium of islets and of the rest of the body (Pezhman et al., 2021), hence this type of targeting could have limited specificity.



During the development of targeted delivery strategies for the inflamed endothelium, the nature of the disease and the stage of disease progression need to be carefully considered to ensure specificity of the targeting and to avoid off-target side effects. Long term hyperglycemia, metabolic syndrome, and entirely unrelated conditions (e.g., trauma) can determine inflammatory changes systemically or determine endothelial activation in specific tissues of the body, and these in turn would affect the distribution of ligands engineered to bind inflamed endothelia.

Strategies for the targeted delivery of *cells* to regions with inflamed endothelia are detailed in section ‘Targeted delivery of therapeutic cells and exosomes’.

## 7. Nanocarrier-based delivery to islet cells

Nano-sized carriers have been developed to enable targeted delivery of therapeutic agents to pancreatic islets, for the treatment of diabetes mellitus (Fig. 3).

Gosh and colleagues engineered nanoparticles by utilizing a peptide that binds preferentially to islet microvasculature (CHVLWSTRKC), connected to a PLGA-b-PEG-COOH block copolymer, and incorporating the anti-inflammatory agent genistein in the nascent nanoparticles. With this strategy, the team observed that the engineered nanoparticles enabled a 3-fold stronger binding to pancreatic islet endothelial cells, and this binding led to a 200-fold increase in the immunosuppressive effect of genistein (Ghosh et al., 2012).

In other studies, iron oxide nanoparticles have been utilized to deliver the microRNA miR-216a, a potent modulator of beta cell proliferation: the treatment of diabetic mice with miR-216a mimics, conjugated with iron oxide nanoparticles, led to potentiation of beta cell proliferation and beta cell function (Wang et al., 2020; Luo et al., 2020).

Other studies have utilized low molecular weight and biodegradable polymers, to facilitate gene delivery. The application of low molecular weight and biodegradable polymers is advantageous for multiple reasons: these polymers are easy to manufacture; they have low immunogenicity; their chemical composition and their *in vivo* degradation can be tightly controlled, which can reduce cytotoxicity (Chen et al., 2020). Gene delivery with polymers targeting the islet microvasculature has provided protection of beta cells from autoimmune destruction. The targeted delivery of nucleic acids through a variety of polymers enabled the maintenance of sequence integrity and the halting of diabetes mellitus progression in animal models. Microspheres were engineered to deliver antisense RNAs for CD80, CD86 and CD40, intended to silence the expression of these costimulatory molecules on dendritic cells in the NOD mouse model of autoimmune diabetes; this treatment enabled prevention and reversal of autoimmune diabetes (Phillips et al., 2008). Recently, the codelivery of guide RNAs for CD80, CD86, and CD40, an autoimmune diabetes relevant peptide (2.5mi), and CRISPR-Cas9 through cationic lipid assisted poly (ethylene glycol)-b-poly(lactide--co-glycolide) (PEG-PLGA) nanoparticles (CLAN) has prevented islet cell autoimmunity by restoring immune tolerance and induced long-term protection of islet beta cells (Luo et al., 2020).

Immune regulatory pathways may be harnessed to prevent autoimmune insulinitis: regulatory T-cells (T regs) produce the molecules interleukin-10 (IL-10) and interleukin-4 (IL-4) to modulate immune functions. In the NOD mouse model, the biodegradable polymer polyaminobutyl glycolic acid (PAGA) was used to deliver a plasmid encoding IL-10 and concurrently protect it from DNase-I degradation (Koh et al., 2000; Kim, 2011). This treatment enabled prevention of the onset of autoimmune diabetes in a majority of recipient NOD mice (Koh et al., 2000; Kim, 2011). A water soluble lipopolymer (WSLP) nanocarrier was engineered to deliver a plasmid encoding for IL-4 with rat insulin promoter [WSLP-(pRIP-IL4)]. The WSLP-pRIP-IL4 enabled pancreas beta-cell specific and glucose responsive expression of IL-4. This system demonstrated no systemic side effects along with high protection of plasmid DNA from DNase I, and was proposed for use for the prevention of autoimmune diabetes (Lee et al., 2001a). Treatment with combined delivery of IL-4 and IL-10 gene plasmid DNA using PAGA in NOD mice resulted in prevention of autoimmune diabetes; in treated animals, 75% of islets remained intact compared to only less than 3% in control animals (Ko et al., 2001).

Glutamic acid decarboxylase (GAD) is a major autoantigen in T1D. Silencing of the expression of GAD by antisense DNA in NOD mice enabled protection of islet beta-cells from autoimmunity and inhibition of progression of diabetes. The delivery of antisense expression plasmid, complexed with polymeric gene carrier of PEG-grafted poly(lysine) (PEG-g-PLL), to GAD-producing cells determined repression of GAD autoantigen expression specifically in pancreatic beta cells (Lee et al., 2001b). This system demonstrated that repression of GAD expression using AS-GAD/PEG-g-PLL may not have any effect on normal expression of GAD in other organs nor have any side effects on normal function of the pancreas.

Yamada et al. targeted pancreatic beta cells via a nanocarrier system composed of sphingomyelin, phosphatidyl choline, and cholesterol, to deliver nucleic acids. To increase insulin secretion, the team knocked down the expression of miR-375 with an antisense RNA in MIN6 pancreatic beta-like cells. This knockdown led to increased insulin secretion via enhanced expression of Pdk1 and Mtpn (Yamada et al., 2014).

Interactions between Fas (CD95) and its ligand (FasL) activate multiple signaling pathways leading to the T cell-mediated beta cell apoptosis. Suppression of Fas (CD95) expression in beta cells by a complex of Fas silencing small interfering RNA (siRNA) has been studied by Kim's group (Jeong et al., 2010). The application of siRNA in clinical settings is challenging due to its highly negative charged backbone, that results in a low intracellular uptake by a negatively charged plasma membrane and a fast degradation by extracellular enzymes. Jeong and colleagues developed an islet cell targeting polymeric gene carrier by conjugating anti-GAD Fab' fragment to PEI via a PEG linker (PEI--PEG-Fab'). This carrier enabled an increase in the specificity of transfection to beta cells, that was dependent on the binding of the beta cell specific GAD (Jeong et al., 2005). The application of a cationic polymer-based nanocarrier of polyethylenimine (PEI) in the delivery of Fas siRNA lead to benefits in the NOD mouse model of diabetes (Jeong et al., 2010). Another pathway that has been successfully harnessed is that of the activating receptor natural killer group 2 member D (NKG2D), which is involved in the progression of T1D, and its ligand retinoic



acid early inducible gene-1 (RAE-1). The RAE-1 ligand is present in prediabetic islets of NOD mice, and autoreactive CD8<sup>+</sup> T cells infiltrating the pancreas express the receptor NKG2D. Kim and colleagues engineered a delivery system with plasmid coding for the islet microvasculature, via targeting the EphA2 and EphA4 receptors. This system was intended to deliver the soluble ligand to NKG2D (sRAE-1y) and protect beta cells from autoimmune destruction. In that study, the bioreducible cationic polymer poly(cystamine bisacrylamide–diamino hexane) (p(CBA-DAH)), poly(ethylene glycol) (PEG), and the targeting peptide to the EphA2 and EphA4 receptors were used to deliver the sRAE-1y in the pancreas of NOD mice. This resulted in a significant improvement in the degree of insulinitis and lower infiltration of CD8<sup>+</sup> T-cells in the treated NOD mice (Blevins et al., 2012; Joo et al., 2012).

Nanocarriers have also been developed to improve islet vascularization and increase insulin production. To improve vascularization, Shimoda and colleagues developed a method based on ultrasound triggered delivery (ultrasound-targeted microbubble destruction) for plasmid gene delivery of vascular endothelial growth factor (VEGF)-A to islet cells. This method was applied in a model of islet transplantation, leading to increased vessel density and improved function of transplanted islets (Shimoda et al., 2010). To increase insulin production and decrease glycemia, Chen et al. engineered phospholipid shell bubbles to deliver plasmids encoding genes for human insulin and hexokinase I to pancreatic beta cells (Chen et al., 2006). Nanoparticles have emerged as a promising vehicle to improve islet cell transplant outcomes. Following islet cell transplantation, islet cell viability could be protected by liposomes containing calcein to increase fibronectin production and decrease apoptosis (Atchison et al., 2010).

Even though nanocarriers offer several potential advantages through targeted delivery of therapeutic agents, the application of nanoparticles can determine side effects and toxicity; the nanoparticles might aggregate or agglomerate *in vivo*, which could result in unforeseen side effects (Patra et al., 2018). Unfortunately, there is limited information regarding the toxicity of newly designed nanocarriers. Further research on the safety and efficacy of nanocarriers is warranted.

## 8. Targeted delivery for gene editing

Gene editing with tools such as CRISPR-Cas9 is opening exciting avenues for therapy of genetic forms of diabetes. Genetic variants involved in pancreatic islet cell and beta cell development can cause diabetes. Diabetes-causing variants can occur in the gene Wolfram syndrome 1 (WFS1). With CRISPR-Cas9, one such genetic variant has been successfully corrected via gene editing (Maxwell et al., 2020). Targeted delivery of all gene editing tools in a single vector, such as a non-integrating lentiviral vector, encoding guide RNA and donor DNA, could allow for delivery of the CRISPR-Cas9 components to islet cells (Uchida et al., 2021). CRISPR-Cas9 delivery can be further optimized by transient endonuclease function and gene correction in the target tissue (Uchida et al., 2021).

Gene transfer using recombinant adeno-associated viral (AAV) vectors has delivered clinical successes, but islets are notoriously difficult to target. A chimeric AAV capsid has been generated to facilitate AAV-based transduction to human islet cells and human embryonic

stem cell-derived beta cells (Pekrun et al., 2019). While this field of investigation is in its infancy, its potential for therapy appears remarkable.

## 9. Targeted delivery of therapeutic cells and exosomes

MSCs have immunomodulatory, anti-inflammatory, and pro-regenerative properties. MSCs have yielded remarkable therapeutic benefits in early-phase trials for the treatment of T1D, T2D, and in the context of islet transplantation (see BOX 2) (Huang et al., 2010). In a majority of applications, MSCs are delivered via systemic intravascular administration. When administered intravenously, most cells become trapped in organs such as the liver, lung, spleen, and kidneys - that function as filters for MSCs. Only a small fraction of cells reaches the target tissues. Local MSC administration in the region of the pancreas has challenges, including difficult accessibility and risk of damaging the pancreas via surgical tools. For applications in diabetes mellitus, especially in the context of T1D, one option could be to deliver MSC specifically to inflamed endothelia in pancreatic islets. For such goal, ICAM-1, VCAM-1, E- and L-selectins are candidate targets. At sites of inflammation, vascular endothelial cells hyperexpress ICAM-1, VCAM-1, E-, P- and L-selectins on the luminal surface, determining recruitment of immune cells (Fig. 2). As stated before, to adhere to inflamed endothelia and initiate extravasation, immune cells present the corresponding ligands: LFA-1 for ICAM-1 (Wu et al., 2019), VLA-4 for VCAM-1 (Dedrick et al., 2003; Gorelik et al., 2012), Sialyl Lewis<sup>X</sup> for E- and L-selectins (Abdi et al., 2015).

When MSC are stimulated with interleukin-1beta (IL-1B), they increase their expression of LFA-1 and adhere more efficiently to inflamed Human Umbilical Vein Endothelial Cells (HUVEC) through LFA-1/ICAM-1 interaction (Wu et al., 2019). Although pretreatment of MSCs with factors such as IL-1B may increase MSC migration and adhesion to the site of inflammation, this method generates a harsh microenvironment and modifies the function of MSCs - which may limit such application (Guo et al., 2018; Lin et al., 2015). An alternative strategy to enhance MSCs applications is the targeting of cell surface markers of the inflamed endothelium via engineered nanocarriers (Cuesta-Gomez et al., 2021).

Nanocarriers consisting of functionalized dendrimers may increase the adhesion of cells to inflamed endothelia (Fig. 4). Liu et al. engineered nanocarriers to enable targeted delivery of MSCs to sites with inflamed endothelium. The team generated nanocarriers by combining acetylated, fifth generation, polyamido amine (PAMAM) dendrimers with soluble E-selectin (sE-sel) as the targeting moiety (Liu et al., 2016). MSCs coated with this dendrimer sE-sel complex can be captured at the microcirculatory bed of the inflamed target site. The coated MSCs underwent extravasation and efficiently migrated into the target inflamed tissue (Liu et al., 2016). Coating with nanocarriers could thus potentiate the localized immunomodulatory, pro-angiogenic, and pro-regenerative effects of MSCs (Liu et al., 2016).

It is important to note that dendrimers present positively charged groups that can lead to toxicity *in vivo*. Acetylation is a highly effective strategy to abate such toxicity (Mishra et al., 2019).

To increase delivery of MSC to inflamed islets, Abdi et al. engineered MSC via exofucosylation with the enzyme fucosyltransferase, to generate the carbohydrate Sialyl Lewis<sup>X</sup> (Abdi et al., 2015). This enzymatic modification of the MSC cell surface led to the generation of the Sialyl Lewis<sup>X</sup> on CD44, yielding HCELL. The modified HCELL<sup>+</sup> MSC, exhibited a three-fold increase in islet infiltration. Administration of HCELL<sup>+</sup> MSCs resulted in durable reversal of hyperglycemia in NOD mice, whereas only transient reversal was observed following administration of HCELL<sup>-</sup> MSCs (Abdi et al., 2015).

MSCs appear to have great potential as a therapeutic agent for T1D and T2D. However, it is important to consider the limitations and potential side effects arising from MSC-based cell therapy. Several factors can affect the MSCs application as a therapeutic agent such as the method of culture, cell heterogeneity, cell dose. MSC are living cells, hence standardizing products made with MSC is difficult. After transplantation in the allogenic setting, the cells will have numerous interactions with cells and tissue of the recipients: the effect of these interactions may vary greatly in different recipients. MSCs are considered hypoimmunogenic, but they can elicit an immune response in the recipient, potentially leading to sensitization and rejection (Avivar-Valderas et al., 2019). The long-term effects of MSC therapy still need to be explored in depth via long term follow-up in recipients (Kassem, 2004). The specific culture methods affect MSC phenotype, differentiation, and immunomodulatory effect (Yang et al., 2018). Long term culture can also increase the probability of malignant transformation. There is controversy on MSCs' pro-tumor and anti-tumor effects: reports suggest that MSC treatment could increase tumor progression via secretion of proangiogenic factors (Pan et al., 2014). The potential negative effects of MSC-based cell therapy have been discussed in other reviews in detail (Musial-Wysocka et al., 2019)(Li et al., 2021b).

Exosomes, small bilayer vesicles derived from eukaryotic cells, present a promising delivery platform (Barile and Vassalli, 2017). Exosomes exhibit low toxicity, structural stability, and cargo loading ability at a nanoscale (Fu et al., 2020). As natural carriers of functional proteins and regulatory nucleic acids, exosomes have emerged as a novel therapeutic tool to deliver RNA and DNA for the treatment of T1D (Pang et al., 2020). Human bone marrow mesenchymal stem cells (hBM-MS) and their exosomes have been reported to promote islet function and inhibit immune rejection (Wen et al., 2016). Mahato and colleagues found that hBM-MS-derived exosomes delivered a plasmid encoding anti-miR-375 and shFas to downregulate miR-375 and Fas to improve islet function in NOD mice (Wen et al., 2016). MSC-derived exosomes are emerging as a viable therapeutic strategy for diabetes, and could improve islet cell transplantation outcomes (Keshtkar et al., 2020). Exosomes derived from UC-MS) led to improvements in viability, survival, and function of islets transplanted in hypoxic conditions (Nie et al., 2018). Beta cell-derived exosomes play a central role in preserving islet architecture and vascularization (Sun et al., 2019). Jia et al. reported that beta cell-derived exosomes promote islet cell angiogenesis leading to improved glucose tolerance and increased insulin production in STZ-induced diabetic mice (Sun et al., 2019). Although the matter of islet cell targeting was not investigated in depth, it is possible that beta cell-derived exosomes could bind natural targets preferentially in the islet environment.

Although exosomes appear promising as agents for beta cells- and diabetes-targeted therapies, caution should be exercised with these agents. Future research in extracellular vesicles merits that different isolation procedures are unified, gender and age matching are considered, and other metabolic conditions are carefully analyzed in the selection of donors. Exosomes have a risk of biological contamination and can transport infectious agents. Moreover, they can affect target and non-target cells in a variety of ways. Caution should be exercised to ensure that exosomes or other extracellular vesicles (EV) are not derived from cancer cells. EV's derived from cancer cells have been shown to transfer miRNAs and oncoproteins which may result in oncogenic effects (Andre et al., 2002; Valadi et al., 2007). Exosomes derived from human Umbilical Cord MSC were shown to promote growth of lung adenocarcinoma cells via transmission of miR-410 - which suppresses the expression of PTEN, a tumor suppressor gene (Dong et al., 2018). Exosomes derived from human Bone Marrow MSC increase VEGF and CXCR4 expression in a dose-dependent manner, leading to tumor growth and angiogenesis *in vivo* (Zhu et al., 2012). Further investigation of MSC-derived and islet-cell derived exosomes are of great interest for the delivery of agents to islet cells and for the advancement of therapies for diabetes.

In summary, MSC and exosomes are emerging as therapeutic agents for diabetes mellitus. Coating of MSC with functionalized nanocarriers has enabled targeted delivery to inflamed endothelia. Enzymatic modification of glycoproteins in the MSC cell surface has been successfully applied for the same goal. Exosomes may be amenable to similar modifications. Based on the cell derivation, exosomes could deliver cargos of interest and could bind preferentially to target islet or vascular cells. A substantial amount of work will be required to address the open issues related to these biological agents, that range from limited knowledge of the mechanism of effect, to difficult standardization, to unknown long-term safety. Nevertheless, these agents appear as excellent candidates for islet-targeted strategies for diabetes mellitus.

## 10. Imaging of beta cells *in vivo* with ligands and nanoparticles

Beside the need for targeted delivery of therapeutic agents to pancreatic islets, there is a need for the targeted delivery of imaging reagents. The latter would enable the development of noninvasive imaging methods to quantify the beta cell mass. Such methods could be extremely useful for monitoring the progression of diabetes mellitus and the response to treatments. The pancreatic beta cell mass is severely depleted in T1D as well as T2D. Concerning T1D, it is believed that beta cell loss occurs long before diabetes diagnosis, as suggested by tests using indirect parameters (Velikyan and Eriksson, 2020). To determine beta cell function, blood glucose, HbA1c, insulin, and C-peptide levels are analyzed in blood plasma. However, none of these directly measures beta cell mass.

Two possible targets for the non-invasive imaging of pancreatic beta cell mass are GLP-1R and ZnT8. As previously discussed, GLP-1R is abundantly expressed on the surface of pancreatic beta cell, and it can be targeted with the GLP-1 mimetic Exendin-4. ZnT8 is also expressed in beta cells, mainly in insulin granules. ZnT8 becomes exposed in the surface of beta cells at the time of insulin release. ZnT8 expression seems to be confined to pancreatic islet beta cells. Antibodies have been generated to target ZnT8 on the cell

surface. One antibody, Ab31, targeting loop 2 of ZnT8, appears to be useful for imaging beta cell mass (Eriksson et al., 2018). Ab31 was radiolabeled with iodine-125 ([<sup>125</sup>I] Ab31) and compared with Exendin-4, radiolabeled with the same iodine-125 ([<sup>125</sup>I] Exendin-4). *In vivo*, [<sup>125</sup>I]Exendin-4 showed superior targeting ability when compared to [<sup>125</sup>I]Ab31, possibly because GLP-1R is constitutively present onto the cell surface, whereas ZnT8 is most frequently residing in its intracellular location in beta cells. GLP-1R was thus found to be a promising target for human beta cell imaging. In studies in the NOD mouse model of autoimmune diabetes, probes engineered with Exendin-4 conjugated with magnetic oxide-based nanoparticle (MN-exendin-4) demonstrated decrease binding in diabetic mice, correctly indicating beta cell loss (Wang et al., 2014). Future studies focused on affinity, ligand miniaturization, and radionuclide selection will be required to improve beta cell imaging (Eriksson et al., 2018).

Another cell surface molecule with high specificity for beta cells is VMAT-2. A selective ligand for VMAT-2, dihydrotetabenazine (DTBZ), has been utilized to build radiotracers such as [<sup>18</sup>F]-DTBZ and [<sup>11</sup>C]-DTBZ for imaging via positron emission tomography (PET). PET imaging for [<sup>11</sup>C]-DTBZ was tested for the measurement of beta cell mass in patients with long-standing T1D (Goland et al., 2009). The results suggested that [<sup>11</sup>C]-DTBZ PET could allow quantification of VMAT2 binding in the human pancreas, but the beta cell mass appeared to be overestimated. For this approach to be successful, current limitations with PET imaging need to be overcome (Alavi and Werner, 2018), and measurement of non-displaceable tracer uptake need to be refined to enable quantification of the specific binding to beta cells (Naganawa et al., 2018).

Other strategies under investigation have utilized perfluorocarbon nanoparticles carrying Rhodamine to non-invasively track transplanted human islets through MRI imaging (Barnett et al., 2011). Among the possible MRI contrast probes, iron oxide nanoparticles have important advantages and are commonly used in the clinical setting (Wang et al., 2014).

These observations represent important steps towards a reliable imaging of beta cell mass, but further refinements are needed.

## 11. Conclusion

Diabetes affects more than 9% of the population and is the seventh leading cause of death. Current therapeutic strategies have substantial limitations and do not correct the root causes of the disease at the level of pancreatic islets. Emerging therapeutic strategies for the treatment of diabetes are increasingly centered around pancreatic islet cells, islet beta cells, and their microenvironment. In the context of T1D, remarkable results were obtained with novel agents that counteract beta cell autoimmunity, such as Teplizumab (anti-CD3), Golimumab (anti-TNF $\alpha$ ), ATG (anti-Thymocyte Globulin), and Mesenchymal Stem Cells (MSC). In the context of T2D, GLP-1 mimetics for the potentiation of beta cell function have radically improved the treatment paradigm. Targeting these therapeutic agents specifically to pancreatic islets appears of great importance, because it could maximize therapeutic benefits while avoiding off-target side effects. The targeted delivery of agents to pancreatic islets could result in preservation or regeneration of functional beta cells with

minimal side effects. A multitude of targeted delivery strategies have harnessed ligands for cell surface molecules specific to islet cells and have shown great promise to improve therapeutic outcomes. Among the many islet cell surface molecules chosen as targets, GLP-1R has been utilized frequently, but VMAT-2, GPR44 and ZnT8 appear to have excellent specificity for islet beta cells and should thus be investigated in depth. Engineered nanoparticles and nanocarriers are emerging as viable options to enable targeted delivery of therapeutic agents and cells to inflamed islet endothelia. Targeting inflamed endothelia appears as an intriguing strategy, especially in the context of T1D, but the window of applicability could be limited to the peri-onset period - when such inflammation occurs specifically in islets. MSCs and their exosomes have yielded remarkable benefits in animal models of diabetes, ranging from prevention to correction of disease. Modification of MSCs or of their exosomes to deliver them to inflamed islet endothelia appears as a very promising strategy. Further investigations of nanocarrier-targeted delivery of therapeutic agents in animal models are required to determine homing, therapeutic effects, and toxicity.

Along with the need for islet-targeted therapeutic strategies, there is an urgent need of imaging methods to quantify the mass of insulin producing beta cells – which is severely depleted in Type 1 Diabetes mellitus and partially depleted or dysfunctional in Type 2 Diabetes. The targeted delivery of imaging reagents to islet beta cells, via ligands for cell surface molecules such as GLP-1R and VMAT2, could enable beta cell mass quantification and the development of improved therapeutic protocols.

Studies focused on safety and efficacy of targeted delivery to the islet environment are warranted, to enable translation of the most promising interventions to clinical trials, and ultimately to effective therapies for diabetes.

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## Glossary

<b>T1D</b>	Type 1 Diabetes
<b>T2D</b>	Type 2 Diabetes
<b>MSC</b>	Mesenchymal Stem Cells
<b>UC-MSC</b>	Umbilical Cord-derived Mesenchymal Stem Cells
<b>BM-MSC</b>	Bone Marrow-derived Mesenchymal Stem Cells



<b>GLP-1R</b>	Glucagon-like peptide 1 Receptor
<b>ICAM-1</b>	Intercellular Adhesion Molecule 1
<b>VCAM-1</b>	Vascular Cell Adhesion Molecule 1
<b>VMAT-2</b>	Vesicular Monoamine Transporter 2
<b>GPR44</b>	G protein coupled receptor 44 (Prostaglandin D2 receptor 2)
<b>ZnT8</b>	Zinc transporter 8
<b>LFA-1</b>	Lymphocyte function-associated antigen 1
<b>VLA-4</b>	Very Late Antigen-4
<b>HCELL</b>	Hematopoietic Cell E- and L-selectin ligand
<b>DTBZ</b>	dihydrotrabenazine
<b>PET</b>	Positron Emission Tomography
<b>MRI</b>	Magnetic Resonance Imaging

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**BOX 1****Current therapeutic options for diabetes mellitus, and their limitations****Agents intended to substitute the function of beta cells: insulin therapy (relevant to: T1D, advanced T2D, certain genetic forms, and other rare forms of diabetes mellitus)**

Insulin is the hormone secreted by beta cells in response to increased glucose concentration. Insulin is a century-old pharmacological agent, the go-to agent utilized to substitute the function of beta cells when they are lost (in T1D) or severely dysfunctional and insufficient (in advanced T2D and certain genetic forms of diabetes). A large fraction of patients with advanced diabetes mellitus requires insulin treatment to control glucose metabolism and survive (Cowie et al., 2018). However, this treatment brings risks of life-threatening iatrogenic hypoglycemia and provides suboptimal metabolic control.

Current therapeutic approaches for T1D include daily insulin injections to maintain blood glucose control (Sutton et al., 2014; Reinhart and Panning, 2002; Sands et al., 2015). Exogenous insulin therapy is not a cure for T1D, it is life-long, and after decades of chronic treatment, it can become inadequate.

**Replacement of beta cells: transplantation of pancreas and pancreatic islets (relevant to: T1D, advanced T2D, and other forms of diabetes mellitus)**

The transplantation of pancreas or isolated pancreatic islets from deceased donors have been performed for decades to control blood glucose and prevent long-term complications of diabetes. The transplantation option is intended for patients with severe forms of diabetes (predominantly 'brittle', unstable T1D), forms that are difficult to manage with current pharmacological treatments. Even though whole organ pancreas transplantation is a major surgical procedure, with substantial risks of morbidity and mortality, it has become a common therapeutic intervention for patients with advanced T1D. Pancreas transplantation led to over 80% insulin independence in recipients one year after transplantation (Ferrer-Fabrega and Fernandez-Cruz, 2020; Ichii and Ricordi, 2009; Shapiro et al., 2003). Besides the application in brittle T1D, pancreas transplantation is also offered increasingly to patients who have advanced forms of T2D (10% of pancreas transplants in the U.S.), or who have lost pancreatic endocrine and exocrine function due to trauma, surgery, or chronic pancreatitis. The transplantation of adult pancreatic islets represents a safer alternative to whole pancreas transplantation (Ricordi et al., 2016; Lablanche et al., 2018; Ricordi and Japour, 2019). A successful phase 3 clinical trial of adult islet transplantation built the groundwork for islet cell replacement therapies (Ricordi et al., 2016; Hering et al., 2016).

Pancreas and islet cell transplantation are limited by insufficient donor organ availability and by the requirement of chronic immunosuppression to prevent rejection - a treatment associated with well-described side effects and health risks (Nathan and Group, 2014; Dominguez-Bendala and Ricordi, 2012; Dominguez-Bendala et al., 2012; Mineo et al., 2009; Mehrabi et al., 2014; Ryan et al., 2005).

**BOX 2****Emerging therapeutic strategies for diabetes mellitus****Pharmacological agents for the potentiation of beta cells: (relevant to: T2D, increasing interest in T1D)**

Glucagon-like peptide-1 (GLP-1) receptor agonist and related treatments show great promise for the potentiation of beta cell function, both in T2D and T1D. GLP-1 is a hormone released by intestinal cells upon meal ingestion and digestion. Pancreatic beta cells present the GLP-1 receptor on their cell surface. When GLP-1 binds to the GLP-1 receptor on beta cells, insulin secretion is promoted in a glucose-dependent manner. GLP-1 is then rapidly degraded by enzymes such as dipeptidyl peptidase-4 (DPP-4). GLP-1 receptor agonists include molecules such as exenatide, liraglutide, and semaglutide, which activate signaling through the GLP-1 receptor and are more stable than the naturally occurring GLP-1 (Hinnen, 2017; Kielgast et al., 2009). An effect similar to GLP-1 agonists is exerted by DPP-4 inhibitors - molecules that inhibit the breakdown of GLP-1 and thus enable increased signaling through the receptor (Kodera et al., 2014; Gurgel Penaforte-Saboia et al., 2021). While the results of GLP-1 related therapies are robust in the context of T2D (Hinnen, 2017), the results are still far from optimal in T1D. Notably, besides the potentiation of insulin secretion and insulin biosynthesis, GLP-1 agonists can stimulate beta cell proliferation and inhibit beta cell apoptosis (Hinnen, 2017). The off-target effects and side effects of these treatments, primarily gastrointestinal, are connected to the widespread expression of the GLP-1 receptor in intestinal tissues (Tuttle et al., 2018). GLP-1 receptor agonists have been used extensively in T2D and show great promise as future therapies in other forms of diabetes mellitus.

**Pharmacological agents for the protection of beta cells from autoimmunity: (relevant to: T1D)**

T1D has an autoimmune basis and is characterized by progressive destruction of insulin-producing beta cells (Eisenbarth, 2004). Development of immunomodulatory therapies able to control islet autoimmunity and preserve insulin secretion from the residual beta cell mass at the time of diagnosis is of critical importance (Orlando et al., 2014). Even a partial level of insulin secretion affords protection from chronic complications (Steffes et al., 2003), hypoglycemia and diabetic ketoacidosis (Ludvigsson, 2013), which could all lead to death (Realsen et al., 2012; Castellanos et al., 2020; Weinstock et al., 2013).

In patients with new onset of T1D, treatment with Teplizumab, a humanized anti-CD3 monoclonal antibody, rendered CD8<sup>+</sup> T cells exhausted and inactive; remarkably, this correlated with significantly higher beta cell function (C-peptide) at follow-up, an average of 7 years after diagnosis (Perdigoto et al., 2019).

In a different trial in new onset T1D, treatment with low-dose ATG led to a reduction in CD4 T cells: this translated into a slowing of the decline of beta cell function and yielded improvements in metabolic parameters (HbA1c) (Haller et al., 2018). Other immunomodulatory strategies under development aim at inhibiting autoimmunity via

stimulation of Regulatory T cells via low dose IL-2 (Dwyer et al., 2016; Rosenzweig et al., 2020). Additional studies are aimed at inhibiting proinflammatory cytokines such as TNF $\alpha$ . TNF $\alpha$  plays a role in the development and progression of autoimmune T1D and is directly toxic to beta cells. In a trial in new onset T1D, Golimumab (a human monoclonal antibody for TNF $\alpha$ ) showed remarkable success, yielding improved endogenous insulin production and lowering exogenous insulin use than placebo (Quattrin et al., 2020). Most of these agents present risks for adverse events related to off-target effects connected with systemic administration. Although no drug has been approved as a disease-modifying therapy for T1D, the inhibition of autoimmunity against beta cells appears attainable.

#### **Cell therapy for the protection of beta cells from autoimmunity: (relevant to: T1D)**

Mesenchymal Stem Cells, also called Mesenchymal Stromal Cells (MSCs), are immunomodulatory cells under investigation for the treatment of T1D. MSCs have yielded promising results in clinical trials for autoimmune diseases, inflammatory disorders, and COVID-19 (Dominguez-Bendala et al., 2012; Lanzoni et al., 2020). MSCs can be safely administered intravenously (Dominguez-Bendala and Ricordi, 2012; Dominguez-Bendala et al., 2012; Bassi et al., 2012; Fotino et al., 2010). Results from a clinical study in Sweden showed that a single infusion of autologous Bone Marrow-derived MSCs (BM-MSC) ( $2.1\text{--}3.6 \times 10^6/\text{kg}$ ) preserved insulin secretion in patients with new onset T1D (Carlsson et al., 2015). In adult patients with established T1D, a single infusion of Umbilical Cord-derived MSCs (UC-MSC) and autologous BM-derived mononuclear cells (BM-MNCs) led to a range of improvements: improved beta cell function, improved glycemia, and lower insulin requirements at 1 year, compared to baseline and control group (Cai et al., 2016). Hu et al. reported that in patients with new onset T1D, UC-MSC treatment was associated with improvements in glycemic control and beta cell function compared to patients in the control group and compared to pre-UC-MSC infusion values (Hu et al., 2013). Lu et al. reported that UC-MSC treatment was associated with an increase in C-peptide levels in 40.7% of recipients at 1 year (Lu et al., 2021). MSCs represent a promising approach for the treatment of patients with T1D (Hu et al., 2013), with evidence of safety (Li et al., 2021a). Although these results appear very intriguing, controversies still exist in relation to the beneficial effects and risks of MSC (Musial-Wysocka et al., 2019). The mechanisms of action of MSCs is multifaceted and largely obscure. The transplantation of MSCs as live cells leads to a broad range of interactions, which are difficult to explore and that may translate into patient-specific effects and side effects (Avivar-Valderas et al., 2019). Standardization of MSC cell products is very challenging (Kassem, 2004). MSC therapy was not found to be associated with serious side effects, but the safety of MSCs, including their contribution to tumorigenesis in the long term, remains a matter of investigation (Musial-Wysocka et al., 2019).

#### **Cell therapy for the replacement of beta cells (relevant to: T1D, advanced T2D, chronic pancreatitis, and other forms)**

Patients with T1D could benefit greatly from islet cell replacement, and patients with T2D could benefit from islet cell supplementation. Pluripotent stem cells represent



an exciting source to generate new islet cells and beta cells for replacement. After pioneering work (D'Amour et al., 2006; Kroon et al., 2008; Pagliuca et al., 2014), remarkable progress has been made by employing human pluripotent stem cells (hPSC) to generate islet specific cells for clinical applications (D'Amour et al., 2006). As a source of islet cells, hPSC could solve cell availability issues related to adult islet transplantation and could enable substantially broader application of islet cell replacement (Augsornworawat et al., 2020; Lanzoni and Ricordi, 2021; Agulnick et al., 2015). Recent work has reported scalable differentiation of stem cells (Millman et al., 2016) into beta-like cells that are glucose-responsive and express markers of mature beta cells (Zhu and Chen, 2015).

The first clinical trials using human beta cells from pluripotent stem cells are ongoing ([ClinicalTrials.gov](https://clinicaltrials.gov) NCT number: [NCT02239354](#), [NCT02939118](#), [NCT03162926](#), [NCT03163511](#), [NCT04678557](#)) (Pullen, 2018). Transplantation of allogeneic cells requires immunosuppression or some form of immunomodulation. It would be ideal to transition from current immunosuppressive strategies to safer immunomodulation methods, to improve clinical outcomes (Mai et al., 2007). Beta cell replacement from pluripotent stem cells appears attainable, but it will probably require important refinements, such as localized or targeted immunomodulation.

**Agents to stimulate beta cell replication and regeneration: (relevant to: T1D, advanced T2D, chronic pancreatitis, and other forms)**

It is desirable to stimulate replication and regeneration of beta cells. GLP-1 agonists can stimulate beta cell proliferation and inhibit beta cell apoptosis (Hinnen, 2017). Exendin-4, a GLP-1 agonist, stimulates human beta cell proliferation, but this appears to occur almost exclusively in juvenile, and not in adult, islet beta cells (Dai et al., 2017).

Human pancreatic beta cells can proliferate after treatment with small molecules such as harmine analogs (Wang et al., 2015; Dominguez-Bendala et al., 2016). Hepatocyte-derived secretory SerpinB1 and its mimetic GW311616A also enhance beta cell proliferation (El Ouaamari et al., 2016). Gamma aminobutyric acid (GABA) was found to promote beta cell replication in grafted human islets (Purwana et al., 2014). Although the stimulation of beta cell replication is highly desirable, it may be an uphill battle in patients with advanced T1D, who present a near-complete beta cell loss.

**miRNAs - agents affecting islet cell gene expression: (relevant to: T1D, T2D, and other forms)**

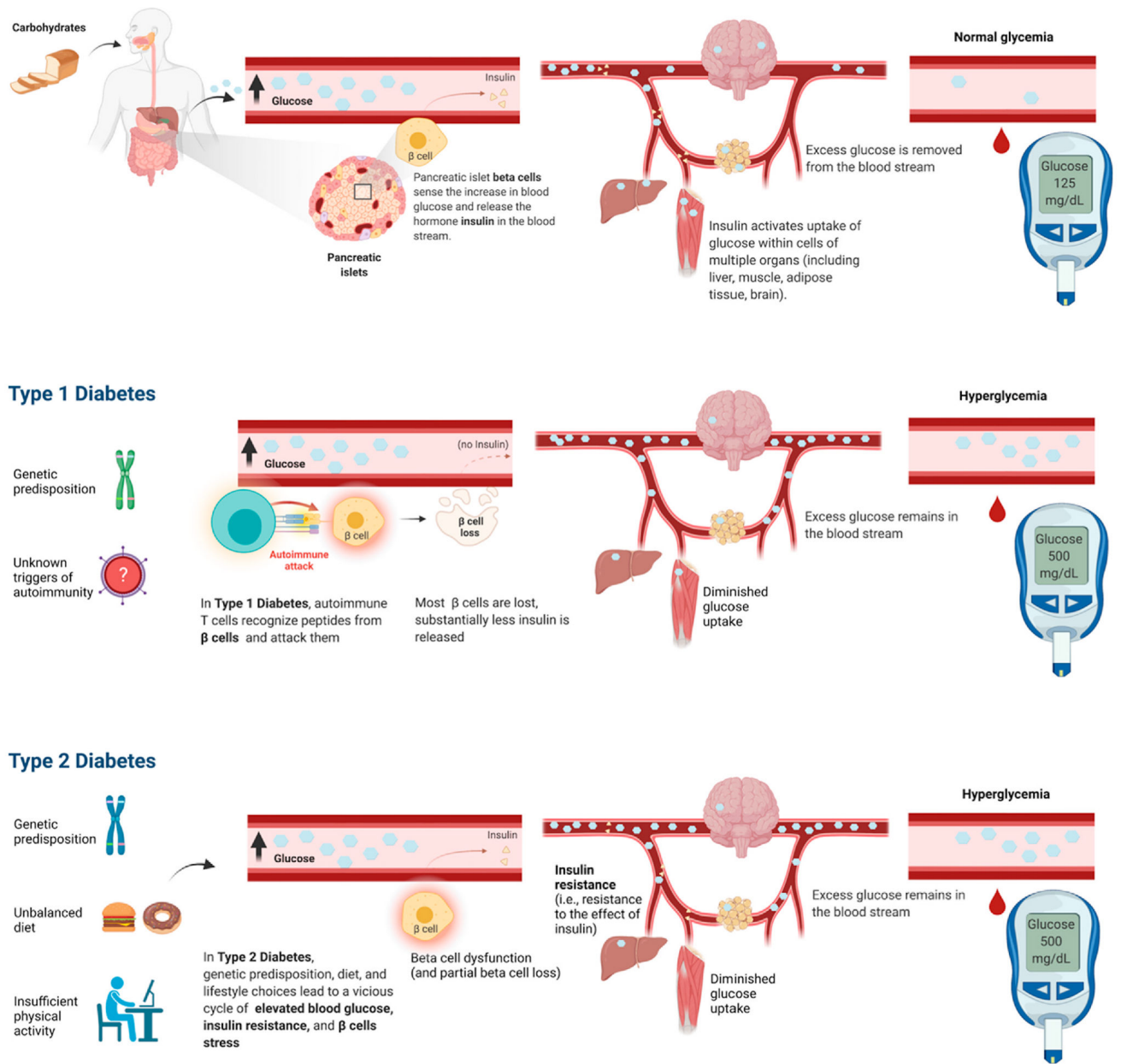
MicroRNAs (miRNAs) are key regulators of gene expression; miRNAs have been harnessed as therapeutics to impart genes expression changes in islet and vascular cells (He et al., 2017; Zampetaki et al., 2010). A number of miRNAs affect beta cell proliferation and insulin secretion, as reviewed in (Eliasson and Regazzi, 2020). In T2D, miRNA sets can determine a failure in beta cell compensation in response to insulin resistance, and are associated with beta cell dysfunction (Eliasson and Regazzi, 2020). Mir-216, as an example, is a potent modulator of beta cell proliferation: it decreases PTEN expression, which in turn activates beta cell proliferation pathways

(Wang et al., 2020). Further developments are needed for enhancement of proliferation and regeneration of beta cells in the pancreas via miRNA manipulation.

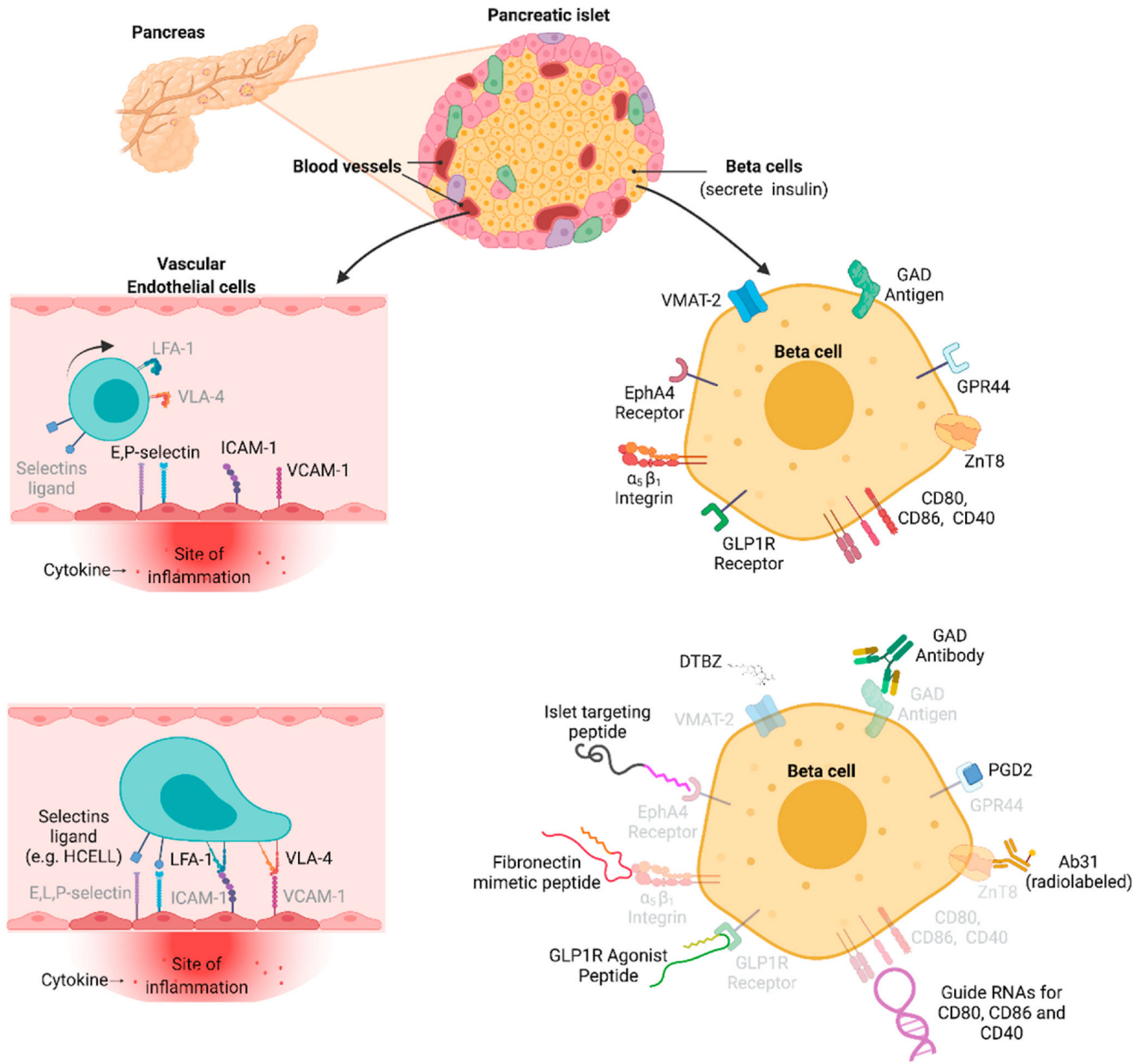
**Agents for other systemic effects - not directly related to islets or beta cells (relevant to: T1D, T2D, and other forms)**

Inhibitors of sodium-glucose cotransporter (SGLT1 and SGLT2) can yield robust improvements in glycemic control for patients with T1D and T2D. SGLT1 inhibitors reduce glucose absorption in the small intestine, whereas SGLT2 inhibitors decrease glucose reabsorption in the kidney. The combination of SGLT1 and SGLT2 inhibitors as an adjunct to insulin therapy appears promising (Sands et al., 2015).

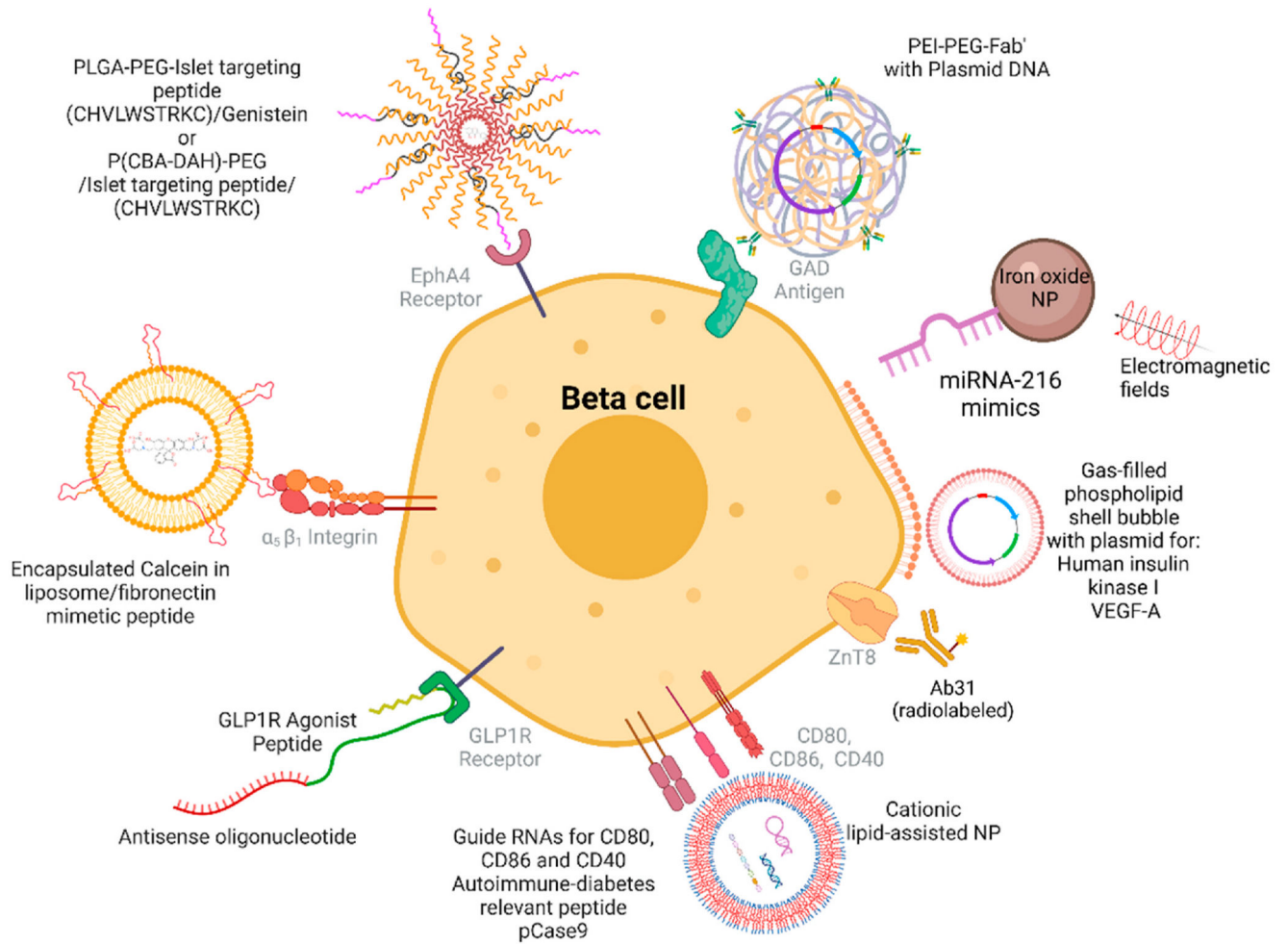
Metformin (Petrie et al., 2017) is an agent broadly utilized in the early stages of T2D. Metformin leads to improved insulin receptor function, increased glucose uptake and utilization, decreased hepatic glucose release, and decreased intestinal absorption of glucose. Hepatic and intestinal absorption is facilitated by Organic cation transporter 1 (OCT1) on the basolateral membrane of enterocytes and hepatocytes (Gong et al., 2012; Foretz et al., 2014). Plasma membrane monoamine transporter (PMAT) expressed on the luminal side of enterocytes has been reported to facilitate metformin intestinal absorption, and the agent subsequently determines a glucose lowering effect by inhibition of gluconeogenesis in the liver (Foretz et al., 2014; Natali and Ferrannini, 2006). Metformin enhances hepatic insulin function by altering lipid homeostasis and inhibiting acetyl Coa carboxylase phosphorylation via AMP- activated protein kinase (AMPK) (Fullerton et al., 2013).



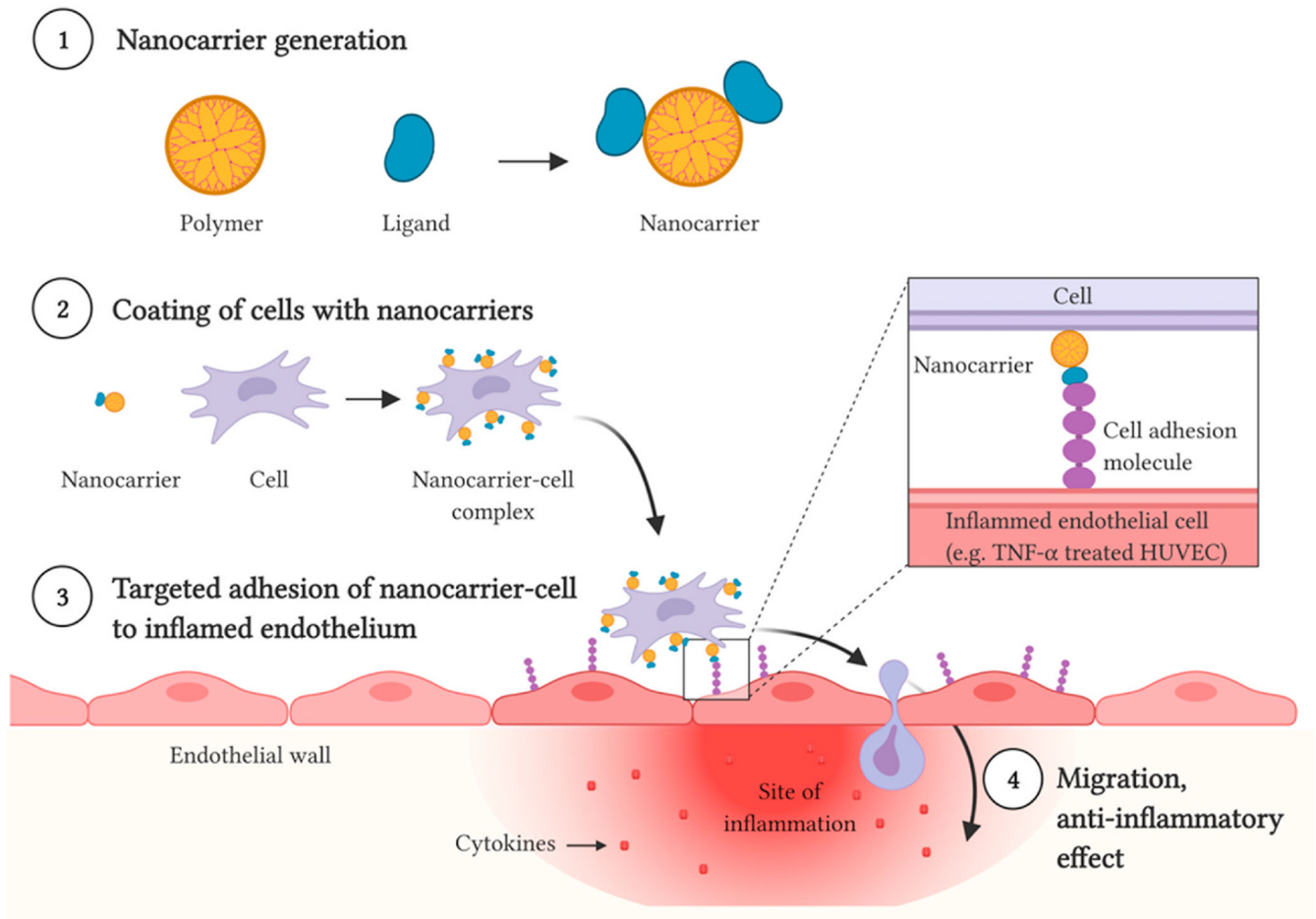
**Fig. 1.** Beta cells control glucose homeostasis via insulin secretion. These cells are centrally involved in Type 1 Diabetes (T1D) and Type 2 Diabetes (T2D).



**Fig. 2.** Cell surface molecules and ligands for targeting inflamed vascular endothelial cells and pancreatic islet beta cells.



**Fig. 3.** Targeting moieties, nanocarrier structures, and cargos for targeted delivery to beta cells.



**Fig. 4.** Targeted delivery of cells to inflamed endothelium.



Table 1

Cargos, Vehicles, and Targeting moieties for islet-targeted therapeutic agents.

Purpose	Cargo	Vehicle	Targeting Moiety/Target/Strategy	Outcome	Reference
Targeted delivery of an immunosuppressant drug to islet cells	Genistein	PLGA/PEG-COOH	Islet Targeting Peptide (Cyclic) (CHVLWSTRKC)/EphA4 Receptor	200x increased immunosuppressant effect	Ghosh et al. (2012)
Islet beta cells proliferation/Decreased expression of phosphatase and tensin homolog (PTEN)	miR-216 mimics/inhibitors	Iron Oxide Nanoparticles	miR-216 mimics/inhibitors	Decreased PTEN expression and increased beta cell proliferation	Wang et al. (2020)
Prevention of autoimmunity to islet components	Autoimmune diabetes relevant peptide/CRISPR-Cas9 plasmid	PLGA/PEG-COOH	Three separate guide RNAs for CD80, CD86 and CD40/CD80, CD86 and CD40	Prevention of autoimmunity to islet components and inhibition of T1D development	Luo et al. (2020)
Delivery of antisense oligonucleotides (ASO) to beta cells for knocking down islet amyloid polypeptide	Antisense oligonucleotides (ASO)	Glucagon Like Peptide 1 Receptor (GLPIR) agonist peptide ligands	GLPIR agonist peptide ligands/GLPI Receptor	Successful knocking down of islet amyloid polypeptide	Kneer et al. (2021)
Polymeric gene delivery system to deliver a plasmid coding for soluble RAE-1 $\gamma$ to the pancreatic islet microvasculature	Soluble Retinoic acid early inducible gene-1 (RAE-1) Plasmid	Poly(cystamine bisacrylamide-diamino hexane) (p(CBA-DAH)/poly(ethylene glycol) (PEG)	CHVLWSTRC Peptide/EphA2 and EphA4 receptors	Protection of beta cells from autoimmune destruction and prevention of type 1 diabetes.	Blevins et al. (2012) Joo et al. (2012)
<sup>19</sup> F MRI imaging of the transplanted human islets	Rhodamine	Perfluoroethylbromide (PFOB) nanoparticles		Non-invasive multimodal cell tracking of human pancreatic islets	Barnett et al. (2011)
Increasing fibronectin production to decrease apoptosis and therefore increase viability of transplanted islets	Calcein	Liposomes	Fibronectin mimetic peptide/ $\alpha_5\beta_1$ integrin expressed on pig islets	Targeted liposomes containing calcein was delivered and they showed improved cell binding and internalized	Atchison et al. (2010)
Increasing hexokinase protease I expression, increasing insulin levels in blood and decreasing circulating glucose levels	Plasmids encoding for the genes for Human Insulin and Hexokinase I	Gas-filled Phospholipid Shell Bubbles	Insulin 1 Promoter/beta-cells/ Ultrasound triggered delivery	Efficient gene delivery to pancreatic islets with the detection of transgene-encoded proteins for up to 3 weeks after transfection	Chen et al. (2006)
Increasing vascular endothelial growth factor A (VEGF-A) expression in transplanted islets to increase vessel density and graft function	Plasmid encoding for the gene for VEGF-A	Gas-filled Phospholipid Shell Bubbles	Ultrasound triggered delivery	Efficient gene delivery of VEGF-A to pancreatic islets was successful, increased vessel density, and improved graft function	Shimoda et al. (2010)
Increasing transfection efficiency and gene delivery to islet cells	Plasmid encoding for the gene for luciferase enzyme	PEI-PEG-Anti GAD Fab polymeric gene carrier	Antibody against glutamic acid decarboxylase/glutamic acid decarboxylase antigen	10-fold transfection efficiency to beta islet cells	Jeong et al. (2005)