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Unveiling tryptophan dynamics and functions across model organisms via quantitative imaging

Kui Wang^{1†}, Tian-lun Chen^{1†}, Xin-xin Zhang^{1,3†}, Jian-bin Cao^{4†}, Pengcheng Wang^{1,5}, Mingcang Wang⁴, Jiu-lin Du^{1,2,3*}, Yu Mu^{1,2*} and Rongkun Tao^{1*}

Abstract

Background Tryptophan is an essential amino acid involved in critical cellular processes in vertebrates, serving as a precursor for serotonin and kynurenine, which are key neuromodulators to infuence neural and immune functions. Systematic and quantitative measurement of tryptophan is vital to understanding these processes.

Results Here, we utilized a robust and highly responsive green ratiometric indicator for tryptophan (GRIT) to quantitatively measure tryptophan dynamics in bacteria, mitochondria of mammalian cell cultures, human serum, and intact zebrafsh. At the cellular scale, these quantitative analyses uncovered diferences in tryptophan dynamics across cell types and organelles. At the whole-organism scale, we revealed that infammation-induced tryptophan concentration increases in zebrafsh brain led to elevated serotonin and kynurenine levels, prolonged sleep duration, suggesting a novel metabolic connection between immune response and behavior. Moreover, GRIT's application in detecting reduced serum tryptophan levels in patients with infammation symptoms suggests its potential as a high-throughput diagnostic tool.

Conclusions In summary, this study introduces GRIT as a powerful method for studying tryptophan metabolism and its broader physiological implications, paving the way for new insights into the metabolic regulation of health and disease across multiple biological scales.

Keywords Tryptophan quantitative imaging, Bacteria, Mitochondria, Zebrafsh, Human serum

† Kui Wang, Tian-lun Chen, Xin-xin Zhang and Jian-bin Cao contributed equally to this paper.

*Correspondence: Jiu-lin Du forestdu@ion.ac.cn Yu Mu my@ion.ac.cn Rongkun Tao rktao@ion.ac.cn ¹ Institute of Neuroscience, State Key Laboratory of Neuroscience, Center for Excellence in Brain Science and Intelligence Technology, Chinese Academy of Sciences, 320 Yue-Yang Road, Shanghai 200031, China ² University of Chinese Academy of Sciences, 19A Yu-Quan Road, Beijing 100049, China ³ School of Life Science and Technology, ShanghaiTech University, 319

Yue-Yang Road, Shanghai 200031, China

4 Department of Anesthesiology, Taizhou Hospital of Zhejiang Province Afliated to Wenzhou Medical University, 150 Xi-Men Road, Zhejiang 317000, China

5 Department of Pediatric Cardiology, Xinhua Hospital, Shanghai Jiao Tong University School of Medicine, 1665 Kong-Jiang Road, Shanghai 200092, China

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Background

Tryptophan, an essential amino acid exclusively obtained from food, plays a crucial role in cellular protein synthesis and survival. Its absorption, transportation, and metabolic pathways within all vertebrates are highly conserved, leading to the production of various active molecules through pathways involving kynurenine, serotonin, and indole $[1-3]$ $[1-3]$ $[1-3]$. Thus, tryptophan metabolism serves as a pivotal metabolic regulator for processes such as immune responses, neural activities, and intestinal functions across vertebrates. Given the wide-ranging infuence of tryptophan metabolism, abnormalities in its regulation can trigger systemic efects, potentially exacerbating diseases like neurodegeneration, infections, and cancer [[4\]](#page-11-2). Notably, plasma tryptophan levels are closely linked to disease progression and prognosis [[5\]](#page-11-3), underscoring the need for precise, quantitative measurement of tryptophan dynamics across biological systems.

Traditional methods for measuring tryptophan, such as high-performance liquid chromatography (HPLC), fall short in revealing the minor metabolic diferences between cell types and subcellular compartments [[6,](#page-11-4) [7](#page-11-5)], and they lack the temporal resolution necessary to track rapid metabolic changes during cellular stress $[8]$ $[8]$. This limitation has hindered a comprehensive understanding of tryptophan's role in various physiological and pathological contexts.

In contrast, our recently developed green ratiometric indicator for tryptophan, GRIT [\[9](#page-11-7)], represents a significant advancement in the feld of metabolic measurement. GRIT surpasses existing FRET-based tryptophan indicators (FLIPW-CTYT) [\[10](#page-11-8)], ofering a substantially larger dynamic range (9.55 versus 0.3), a smaller molecular size (39.7 kDa versus 80.1 kDa), and an excitation ratio that is independent of photobleaching $[10, 11]$ $[10, 11]$ $[10, 11]$. These improvements make GRIT a highly efective tool for the quantitative measurement of tryptophan.

In this study, we demonstrate GRIT allows a new paradigm offering high spatiotemporal resolution, systematically quantifying dynamic changes in quantitatively mapping tryptophan dynamics in bacteria, mitochondria, zebrafsh, and human serum. Such advancements uncovered previously unrecognized diferences in tryptophan dynamics across cell types and organelles, and revealed that infammation-induced tryptophan redistribution in the zebrafsh brain is associated with increased serotonin and kynurenine levels, linking immune response to behavioral changes. Additionally, we found that reduced serum tryptophan levels in patients with infammation could serve as a potential biochemical marker for infammatory conditions.

The introduction of GRIT as a robust, versatile, and quantitative tool for studying tryptophan metabolism

marks a signifcant step forward in our ability to systematically measure and understand this critical amino acid's role in health and disease. This work opens new avenues for research into the metabolic regulation of immune responses, neural function, and disease progression, with broad implications for clinical diagnostics and therapeutic strategies.

Results

Monitoring tryptophan dynamics in living bacteria

Bacteria possess a tight regulatory mechanism on tryptophan metabolism [[12\]](#page-11-10). We investigated tryptophan uptake into *Escherichia coli* cells by expressing the GRIT sensor in the cytoplasm (Fig. $1A$ $1A$, [B\)](#page-2-0). Exogenous tryptophan addition induced a strong and rapid fuorescence response in GRIT-positive bacteria, with a maximum ~ threefold increase (Fig. $1B-D$ $1B-D$), but not in GRITOL (GRIT control sensor)-expressing bacte-ria (Fig. [1B](#page-2-0)). GRIT could respond to $0.1-100 \mu M$ exogenous tryptophan in a dose-dependent manner (Fig. [1](#page-2-0)D, Additional fle 1: Fig. S1A) with an absorption rate of \sim 16.5 μ M/s (Additional file 1: Table S1). The Michaelis constant (K_m) of tryptophan uptake (~0.58 μ M) is similar to the reported biophysical properties of aroP (\sim 0.4 μ M) [[13\]](#page-11-11), a tryptophan transporter that is highly expressed in bacteria according to the transcriptome [[14\]](#page-11-12) (Additional file 1: Fig. S1B). The free concentrations of intracellular tryptophan in tryptophan deprivation and tryptophan exposure conditions were measured to be 10.6 ± 3.7 μM (similar to the reported level 12 μM [[15\]](#page-11-13)) and 192 ± 23.9 μ M, respectively (Additional file 1: Table S1). In addition, no signifcant fuorescence change was observed when 19 other tested amino acids were added in the absence or presence of tryptophan (Additional file 1: Fig. $S1C$). These results suggest that GRIT sensor can monitor the uptake and concentration changes of tryptophan in living bacteria in real-time and with high sensitivity (Fig. [1](#page-2-0)C–D, Additional file 1: Fig. S1A) and specifcity (Additional fle 1: Fig. S1C), thereby aiding in the study of the regulatory mechanisms of bacterial tryptophan metabolism.

Detection of mitochondrial tryptophan dynamics in mammalian cells

Mitochondria are semiautonomous subcellular organelles with their own genome and require tryptophan transport from the cytosol to synthesize mitochondrial proteins. However, due to the lack of specifc detection methods, reports on mitochondrial tryptophan metabolism have been sparse [[16\]](#page-11-14). We selectively targeted the GRIT sensor in the mitochondrial matrix (Fig. $2A$ $2A$, B and Additional fle 1: Note S1), resulting in a marked increase in fuorescence signals compared to the control cells (Additional

Fig. 1 Detection of tryptophan uptake in bacteria with GRIT sensor. **A** Schematic representation illustrating the fuorescence detection of tryptophan (Trp) dynamics with the GRIT or GRITOL sensor in *Escherichia coli* cells. **B** Fluorescence images of bacteria expressing GRIT and GRITOL upon the addition of 0.1 mM Trp. **C** Changes in the fuorescence of GRIT in response to various concentrations of Trp in *Escherichia coli*. **D** The dose–response curve of GRIT-positive bacteria treated with exogenous Trp. Data are from Fig. S1A. The curve was ftted using Eq. 1 provided in the ["Methods"](#page-7-0) section, with the binding constant being~0.33 μM. Scale bars, 1 μm. Data shown as mean±s.e.m., *n*=3 independent experiments in **C** and **D**. See also Additional fle 1: Fig. S1 and Table S1

file 1: Fig. S2A, B). This enhancement enables effective fuorescence measurement using both microplate readers and microscopy (Fig. [2](#page-3-0)A). Mito-GRIT showed an \sim 1.7fold fuorescence increases upon the addition of 0.5 mM tryptophan (Fig. [2](#page-3-0)B). The mitochondrial tryptophan concentration was determined to be 112.4 ± 10.0 μ M (Additional fle 1: Table S1), which was close to the HPLC measurements (108.0±10.3 μM, Additional fle 1: Table S1). However, the tryptophan uptake rate of mitochondria (~9.6 μ M/min) was only~18% of that in the cytoplasm (~52.6 μM/min) (Fig. [2C](#page-3-0), Additional file 1: Table S1). Upon tryptophan deprivation, the mitochondrial tryptophan level was relatively stable in the frst 20 min and decreased linearly at a rate of \sim 0.8 μM/min (Additional file 1: Fig. S2D, E and Table S2). This suggests that the mitochondrial tryptophan pool is predominantly regulated by cytosolic supply and the mitochondrial consumption, such as protein synthesis.

We have demonstrated that cytosolic tryptophan pool is fnely regulated by the supply of external amino acids, which can be classifed into three groups, class I (large and neutral amino acids, classic LAT1 substrate), class II (fve uncharged amino acids), and class III (six charged or nonpolar amino acids) [\[9](#page-11-7)]. To further understand the characteristics of mitochondrial tryptophan transportation, we detected mitochondrial tryptophan dynamics in response to all other 19 amino acids. The six amino acids from class III, which have no efect on cytosolic tryptophan fux, also did not afect mitochondrial tryptophan dynamics (Additional fle 1: Fig. S2C–D, F and Table S2). In contrast, the 13 amino acids from class I and class II, despite their varied effects on cytosolic tryptophan efflux, displayed similar impacts on mitochondrial tryptophan dynamics, both in the absence or presence of tryptophan (Additional fle 1: Fig. S2C–D, F and Table S2). Collectively, the biophysical properties of mitochondrial tryptophan metabolism suggest specifc and unidirectional mitochondrial tryptophan transporters, which are diferent from the bidirectional transportation of cell surface SLC7A5 (LAT1) [[9](#page-11-7)].

Fig. 2 GRIT sensor reports mitochondrial tryptophan dynamics in cultured HeLa cells. **A** Schematic showing the fuorescence detection with mito-GRIT or mito-GRITOL sensor in HeLa cells. **B** Fluorescence responses of HeLa cells expressing GRIT (upper) and GRITOL (bottom) in mitochondria upon the addition of exogenous 0.5 mM Trp in HBSS bufer. The traces (**C**) and dose-dependence curve (**D**) of mitochondrial GRIT sensor in response to varying concentrations of added tryptophan. The gray trace in **C** represents the fuorescence response kinetics of cytosolic GRIT to indicated Trp concentration (64 μM) in HBSS bufer, suggesting a signifcantly faster tryptophan uptake into the cytosol compared to the mitochondria. The curve in **D** was ftted using Eq. 1 provided in the ["Methods](#page-7-0)" section, with the binding constant being~5.84 μM. Scale bars, 10 μm. Data shown as mean±s.e.m. *n*=3 independent experiments. See also Additional fle 1: Fig. S2 and Tables S1 and S2

Detection of serum tryptophan in patients with infammation syndrome

The clinical relevance of tryptophan metabolism lies in its association with various diseases and infammatory responses, particularly evident in the variations in serum levels $[5]$ $[5]$. Therefore, a rapid and efficient in vitro detection method could signifcantly advance diagnostic technologies. We demonstrated that purifed GRIT sensor could show large fuorescence ratio changes to tryptophan ranging from 20 μM to 1 mM (Additional fle 1: Fig. S3A). This broad detection range is line with the theoretical prediction of an established R package "SensorOver-lord" [[17\]](#page-11-15) (Additional file 1: Fig. S3B), which overlaps with the concentration fuctuations of tryptophan in most physiological and pathological conditions.

We collected serum samples from patients with infammatory symptoms characterized by following specifc clinical criteria [\[17\]](#page-11-15): hypersensitive C-reactive protein (hs-CRP) concentration > 50 mg/L, neutrophil ratio > 80%, and white cell count > $10,000/\mu L$ (Fig. [3A](#page-4-0)). We frst analyzed serum tryptophan levels using HPLC assay, followed by GRIT sensor detection of the remaining portion of the same sample (Fig. [3A](#page-4-0)). Despite the autofuorescence of blood may interfere with the fuorescence assays, our results showed that GRIT sensor possesses much higher fuorescence signal than the serum background (Additional fle 1: Fig. S3C–F). In addition, the quantifed tryptophan concentration was highly consistent between HPLC and GRIT sensor measurements (Fig. [3B](#page-4-0)), demonstrating the robustness of tryptophan measurement with purifed GRIT sensor in human serum samples. The serum tryptophan level in inflamed patients $(44.7 \pm 4.7 \mu M)$ decreased ~ 25% compared with that of control $(59.6 \pm 3.6 \mu M)$ (Additional file 1: Table S1). This reduction in serum tryptophan was consistently observed under various conditions, including diferent sexes, ages, and extents of infammation (Fig. [3C](#page-4-0)–F, Additional fle 1: Fig. S3G– I). These results validate the GRIT sensor as an alternative high-throughput in vitro diagnostic method and a decrease in serum tryptophan level could be a biochemical marker of infammation in patients.

Fig. 3 Decreased serum tryptophan concentration is a biochemical mark of infamed patients. **A** Schematic of the experimental procedures for the quantifcation of human serum tryptophan. **B** A comparative analysis of quantitative serum tryptophan level in identical samples measured by GRIT sensor assay or HPLC measurement (*n*=42). **C** Tryptophan concentrations of human serum samples in the control group (gray, *n*=12 in 20–65 subgroup, *n*=13 in the 66–100 subgroup) and infammation group (green, *n*=17 in 20–65 subgroup, *n*=35 in the 66–100 subgroup) based on age. Note that the total *n* number (42) in **B** is smaller than the *n* number (77) in **C**, due to the volume of some serum samples were not enough for GRIT sensor assay after HPLC (<0.3 mL). Relationships between tryptophan concentrations in human serum samples and concentrations of hypersensitive C-reactive protein **D**, neutrophil ratio **E**, and white cell number **F**. The dashed magenta line represents a linear ft of the data, with the shaded area indicating the ftting confdence interval. Two-tailed Student's unpaired *t*-test for **C**. See also Additional fle 1: Fig. S3 and Table S1

Detection of tryptophan metabolites and behaviors during infammation in animal model

In the central nervous system, tryptophan is catabolized into serotonin and kynurenine, both of which modulate neural activities and are related to sleep, depressive behaviors, and fatigue symptoms [[18,](#page-11-16) [19\]](#page-11-17). To further explore the pathological implications of the documented infammation-triggered tryptophan redistribution phenomenon [[9](#page-11-7)], we subsequently exposed zebrafsh to lipopolysaccharide (LPS). This resulted in a dose-dependent increase in sleep duration (Fig. [4](#page-5-0)A–C, Additional fle 1: Fig. S4A), consistent with the sustained elevation of tryptophan levels in the brain following LPS treatment (Additional fle 1: Fig. S4B, C). Next, we measured the concentrations of tryptophan, serotonin, and kynurenine in isolated zebrafsh brains. Infamed zebrafsh showed a slight but non-signifcant increase in total tryptophan, a signifcant over threefold increase in serotonin, and a 36% increase in the kynurenine, compared to control individuals (Fig. $4E$, [F\)](#page-5-0). The rises of tryptophan metabolites in

the brain may contribute to the increased sleep behaviors during infammation. Furthermore, inhibiting these metabolic pathways resulted in developmental deformities, leading to their demise (Additional fle 1: Fig. S4D, E), suggesting that disrupting tryptophan metabolism leads to severe pathological consequences.

In summary, our results demonstrate that infammatory responses modulate tryptophan levels across tissues, with altered metabolic levels in the brain infuencing behavior. This indicates a metabolic link between the infammatory response and animal behavior.

Discussion

In this study, we have demonstrated the versatility of using GRIT biosensor for quantitatively measuring tryptophan levels across divers biological models, including bacteria, subcellular organelles, and human serum. The GRIT, a superior genetically encoded tool, supports multiple applications and long-term recordings of tryptophan.

Fig. 4 Detection of metabolite levels in zebrafsh larvae and zebrafsh sleep changes during infammation. **A** Schematic of the zebrafsh sleep behavior measurement during infammation. **B** Changes in the sleep time of zebrafsh in response to various concentrations of LPS (*n*=60 fshes from 5 to 7 independent experiments). LPS was added at 0 h with indicated concentrations. **C** The dose–response curve of mean sleep time at night of zebrafsh treated with diferent concentrations of LPS. The curve was ftted to a sigmoidal function. **D** Schematic of the experimental procedures for the quantifcation of zebrafsh brain tryptophan. The absolute levels (pg/mg) (**E**) and relative changes (**F**) of tryptophan, kynurenine, and serotonin in isolated zebrafsh brain with (*n*=7) or without LPS treatment (*n*=6). Data shown as mean±s.e.m. Two-tailed unpaired Student's *t*-test for **D**. See also Additional fle 1: Fig. S4

We have diagrammed tryptophan metabolism and functions in bacteria, HeLa cells, intact zebrafsh, and human serum for reference (Fig. [5\)](#page-6-0). Our fndings show that intracellular tryptophan levels of diferent cell types and animal models typically lie in the sub-millimolar range with distinct transportation properties (Additional fle 1: Table S1), which are in relevance to their specifc functions in respective cells. In *Escherichia coli*, tryptophan anabolism stands out as one of the most energyintensive metabolic pathways [[20\]](#page-11-18), which is activated exclusively under tryptophan deprivation conditions (lower than sub-micromolar), along with a signifcant increase in its half-proliferation time $[21]$ $[21]$. The high afnity and rapid response to tryptophan facilitate rapid growth to adapt variable environments [[21](#page-11-19)] and allow gut microbes to continually metabolize tryptophan into indole derivatives, infuencing host the enteric nervous systems [\[22,](#page-11-20) [23](#page-11-21)] (Fig. [5](#page-6-0)A).

In mammal system, reprogramming tryptophan metabolism has become attractive for tumor therapy, such as targeting LAT1 or indoleamine 2,3-dioxygenase (IDO) [\[5](#page-11-3), [24\]](#page-11-22). In contrast to the bidirectional and rapid turnover of the cytosolic tryptophan pool, mitochondrial tryptophan

transportation exhibits a slower rate and higher specifcity. The stringent regulation of mitochondrial tryptophan pool may beneft protein synthesis and quality control within mitochondria. Considering that the intense, ratiometric GRIT sensor is suitable for high-throughput screening, it offers an opportunity to identify the mitochondrial transporter [\[25](#page-11-23)], and an optical method and paradigm for studying the metabolism of subcellular organelles (Fig. [5](#page-6-0)B). Unlike the invasive method like HPLC, genetically encoded GRIT sensor can monitor the mitochondrial tryptophan dynamics in living cells, thus eliminating the need for sample preparation and inaccurate mitochondrial volume estimation for quantifcation $[26]$ $[26]$. This could potentially lead to accurate tryptophan concentration in situ.

Quantitative measurements by GRIT sensor in intact animal and human serum could reveal systemic tryptophan dynamics and its functions (Fig. [5](#page-6-0)C–D). Tryptophan metabolism regulates immune systems and neural behaviors through kynurenine and serotonin pathways [\[5](#page-11-3), [19,](#page-11-17) [27](#page-11-25)], making the redistribution of tryptophan crucial for balancing the physiological functions under pathological conditions [\[5](#page-11-3), [28](#page-11-26)]. Our measurements suggest that

Fig. 5 The proposed biophysical models of tryptophan dynamics in bacteria, mammalian cells, zebrafsh, and human serum. **A** Pathways contributing to tryptophan metabolism in bacteria. Bacteria absorb external tryptophan mainly by aroP and export excess tryptophan with yddG and yedA. Gut microbe could utilize tryptophan to synthesize indole compounds to regulate neuron activities. **B** Proposed model for the tryptophan metabolism in the mitochondria of mammalian cells. Tryptophan enters mitochondria as the speed of 10 μM/min. Mitochondrial tryptophan pool depends on the cytosolic infux and endogenous consumption. **C** Proposed model of tryptophan dynamics in zebrafsh larvae under LPS-induced infammation. During infammation, plasma tryptophan enters the brain and increases the levels of kynurenine and serotonin, leading to prolonged sleep time of zebrafsh larvae. **D** The serum tryptophan levels in infamed patients and control individuals. All the uptake rates or efflux rates are calculated at the Trp concentration around the Michaelis constant (*K_m*) of relative transporters

a flow of plasma tryptophan to the brain and the consequent increase of tryptophan metabolites (serotonin and kynurenine) during infammation resulted in prolonged sleep time in zebrafish (Fig. $5C$). These results align with the elevated serotonin concentration in the brain and fatigue and depression behaviors in LPS-treated mice [[29\]](#page-11-27) and patients with infammation symptoms, suggesting a potential metabolic link between immune response and animal behavior [\[1](#page-11-0)].

In vitro diagnostics plays a pivotal role in disease detection, monitoring, and personalized medicine, ultimately contributing to better patient outcomes and overall public health $[30, 31]$ $[30, 31]$ $[30, 31]$ $[30, 31]$ $[30, 31]$. The simple, fast, and accurate GRIT probe allows high throughput quantifcation of tryptophan concentrations in a patient's serum, which marks a signifcant advancement in the clinical applications of fluorescent probes (Fig. [5D](#page-6-0)). The reductions in serum tryptophan levels during infammatory responses exhibit

remarkable consistency between zebrafsh and human patients. Interestingly, a similar redistribution of tryptophan has been observed in glioblastoma [\[32](#page-11-30)]. Moreover, our results suggest a correlation between patients' ages and serum tryptophan levels (Fig. [3](#page-4-0)C, Additional fle 1: Fig. S3H, I), but not with gender, implying a potential role of tryptophan in aging, which are consistent with a previous report that tryptophan supplement could extend worm lifespan via mitochondria NAD de novo synthesis $[33]$ $[33]$. These results underscore the highly conserved nature of tryptophan metabolism and circulation among vertebrates, emphasizing the relevance of our observations across diferent species. Considering infammation is a hallmark of various diseases, such as cancer, aging, obesity, and cardiovascular disease, the systemic and quantitative measurement of tryptophan dynamics on zebrafish offers new insights into the metabolic regulation mechanisms of these diseases [[4](#page-11-2), [5,](#page-11-3) [34](#page-12-1)].

Limitations of study

The GRIT sensor can detect intracellular tryptophan dynamics in a wide range of scenarios, including tryptophan deprivation conditions (\sim 5 μ M) [[35\]](#page-12-2). However, when the direct detection of low extracellular tryptophan is desirable to evaluate microenvironments, such as in tumor tissues, new versions of GRIT sensors with tight afnities should be designed.

Sensors with diferent emission spectra could further broaden the applications. A red fuorescent control sensor can be developed as a reference channel to enable cell-by-cell corrections in situ [\[36\]](#page-12-3). In addition, far-red versions of the tryptophan sensors could be developed to overcome the low penetration depth of visible light in deep tissue imaging of non-transparent organisms.

Conclusions

Overall, the systemic quantifcation of tryptophan metabolism using the GRIT sensor represents a major advancement in our understanding of this essential amino acid. By enabling precise measurements across diferent biological contexts, GRIT has the potential to signifcantly impact both basic research and clinical practice, offering new insights into the metabolic regulation of health and disease. Quantitative imaging paradigms in model animals also establish a foundation for future studies aimed at uncovering the broader implications of amino acid metabolism in human diseases.

Methods

Cell cultures

HeLa and HEK293T cell lines, obtained from the Cell Bank of the Chinese Academy of Science, were confirmed to be free of mycoplasma contamination. These cell lines were cultured in high glucose DMEM (BBI), supplemented with 10% FBS (ExCell Bio) and 1% penicil $lin-$ streptomycin (10,000 U/mL). The cells were maintained at 37 °C in a humidifed atmosphere composed of 95% air and 5% $CO₂$.

Zebrafsh

Colonies of zebrafsh (*Danio rerio*), specifcally the Nacre strain ($mitfa^{w2/w2}$), were maintained following standard procedures. The experimental protocols involving zebrafsh were approved by the Chinese Academy of Sciences (Approval no. NA-046–2019). The zebrafish were kept under a light–dark cycle of 14 h light to 10 h dark, and the water temperature was consistently maintained at 28 °C.

Human plasma samples

All the population studied were from patients of Taizhou Hospital of Zhejiang Province afliated to Wenzhou Medical University. The experiments were performed according to the medical ethics rules (no. K20211202).

Technical details for GRIT and GRITOL indicators

GRIT sensor was engineered via inserting circularly permuted superfolder YFP (cpSFYFP) into TrpR followed by several cycles of iterative sensor design and optimization [[8\]](#page-11-6). As a single fuorophore dual channel sensor, GRIT sensor exhibits two excitation peaks near 420 nm and 500 nm and one emission peak near 515 nm. In practical experiments, we measure the fuorescence ratio ($R_{485/420}$ or $R_{488/405}$) of the sensor at similar wavelengths (microplate reader: Ex1 420/10, Ex2 485/20, Em 528/20; confocal microscope: Ex1 405 nm, Ex2 488 nm, Em 500–550 nm) to measure tryptophan concentration. In tryptophan quantifcation experiments, it is necessary to conduct parallel control experiments with tryptophaninsensitive control sensor GRITOL to correct for the effects of other environmental factors, such as pH. The correction is achieved by dividing the fuorescence ratios of GRIT and GRITOL from parallel experiments, resulting in the normalized $R_{488/405}$ or $R_{485/420}$.

Plasmid construction

For mitochondrial expression, the mitochondrial signal peptide from CoxVIII (cytochrome c oxidase subunit VIII) was duplicated and fused at the N-terminus of tryptophan biosensors [\[8\]](#page-11-6). To make lentiviral vectors, genes of mito-GRIT and mito-GRITOL were subcloned into pLVX-IRES-Puro backbone by NheI and PmeI.

Cell culture, transfections, and establishment of stable cell lines

To generate lentiviral particles, HEK293T cells were transfected with lentiviral plasmids, including two packaging vectors (pMD2.G and psPAX2), using Hieff Trans (YEASEN). Lentivirus-containing supernatants were collected at 48 and 72 h post transfection and subsequently applied to HeLa cells cultured in 6-well tissue culture plates supplemented with 8 μg/mL polybrene. Stable HeLa cell lines were established by cultivating the cells with 1 μg/mL puromycin for 1 week, followed by sorting using MoFlo Astrios EQ (Beckman Coulter) with a 488 nm laser line. The resulting stable HeLa cells were used for subsequent fuorescence measurement experiments.

Fluorescence measurement of living cells with microplate reader

For bacterial experiment, fuorescent bacteria cells were centrifugated at 4000 rpm for 2 min, followed by washing three times with modifed PBS bufer containing 10 mM HEPES, pH 7.3. The optical density (OD_{600}) of bacterial suspensions was diluted to \sim 0.01, followed by a 30-min

pre-starvation before measurements. Three points were detected as the steady state, followed by addition of different concentrations of tryptophan and a 10-min continuous reading on the BioTek SynergyNeo Multi-Mode microplate reader. The fluorescence ratios $(R_{485/420})$ of GRIT and GRITOL were divided to ft with titration curve for calibration.

For mammalian cell experiments, the HeLa cell lines stably expressing GRIT sensors were trypsinized, resuspended, and plated in a black 96-well fat-bottom plate at a density of 26,000 cells per well, allowing them to cultivate for 10–12 h. Before the fuorescence measurements, the DMEM media was removed, and cells were washed twice with freshly prepared HEPES bufer. Various amino acids were then introduced into the detection bufer, each at specifed absolute concentrations. To correct the fuorescence values of GRIT sensors, the signals from HeLa cell samples were background-subtracted.

Fluorescence microscopy

For bacterial imaging, fuorescent bacteria cells were collected and diluted to the $OD_{600} \sim 0.2$ with modified PBS bufer with or without 0.1 mM tryptophan. Bacteria solution (10 μ L) was added on the 0.17 mm coverslips (Nunc), then the coverslip was put upside down on a glass slide for imaging.

For cell culture imaging, cultured HeLa cells expressing Mito-GRIT and Mito-GRITOL were transferred to an 8-well glass-bottomed dish (Cellvis) where the culture medium was replaced with HEPES bufer with or without 0.5 mM tryptophan prior to experimentation. Utilizing an inverted confocal Olympus FV3000 automatic microscope with a UPlanSApo $40 \times$ Sil objective (N.A. 1.25), dual-excitation ratio imaging was performed.

For in vivo imaging, zebrafsh larvae were paralyzed and immobilized dorsal side up in 1.5% low-melting agarose on a glass-bottom dish under a stereoscopic microscope. The larvae were immersed in egg water for 20 min, followed by imaging on an Olympus FV3000 upright confocal microscope with a XLUMPlanFL N 20X waterimmersion objective (N.A. 1.0).

The GRIT sensor was excited using 405-nm and 488nm lasers, capturing emission fgures between 500 and 550 nm with a photomultiplier tube (PMT) in a 1024×1024 format and 12-bit depth. For subsequent data analysis, a semiautomatic analysis was carried out using the FIQA code implemented in ImageJ Fiji. This analysis involved several crucial steps, including background subtraction to eliminate unwanted noise, skin removal for enhanced clarity, generation of ratiometric pseudocolored images to visualize variations, and batch measurement of fuorescence intensities.

In vitro transcription and mRNA purifcation

The mRNA preparation involved the utilization of a T7 mMESSAGE mMACHINE kit (Invitrogen). We amplifed the cDNAs corresponding to GRIT, GRITOL, or Tol2 and performed in vitro transcription following the manufacturer's guidelines. To obtain purifed mRNA, a 2-h incubation in lithium chloride at−20 °C was performed, followed by dilution with DEPC-treated nuclease-free water. This approach facilitated the generation of high-quality mRNA samples for further experimental applications.

Zebrafsh sleep and locomotion analysis

Sleep analysis was performed based on tracking results of individual larval zebrafsh. Zebrafsh larvae were raised with a light $(14 h)$ and dark $(10 h)$ cycle. The daytime starts at 9 am and the night-time starts at 11 pm. When experiments started, individual larvae were transferred into wells of a 96-well plate, which was placed inside Zebrabox (Viewpoint Life Sciences, Lyon, France). Their locomotor activity was recorded using the quantization mode in a video-tracking system (Viewpoint Life Sciences). Parameters for detecting diferent movement patterns were determined empirically: detection thresholds, 15; burst, 29; freeze, 3; and bin size, 60 s. PBS or diferent doses of LPS were added into the bath at 9 am on the second morning and maintained throughout the experiment.

Human plasma sample preparation

Venous blood samples of patients were collected in tubes early in the morning, after an overnight fast for a standard blood test, which are divided into control group and infammation group based on the blood test with clinical criteria [[37](#page-12-4)]. For control group: (1) the number of white cells is between 4000 and $9000/\mu L$; (2) the concentration of hypersensitive C-reactive protein (hs-CRP) is less than 20 mg/L; and (3) the neutrophil ratio is between 50 and 70%. For infammation group: (1) the number of white cells is over $10,000/\mu L$; (2) the concentration of hs-CRP is more than 50 mg/L; and (3) the neutrophil ratio is over 80%. The studied population consisted of 77 adult subjects, which were randomly selected independent of gender and age. Selected plasma samples were centrifuged at 3500 rpm for 2 min and kept at 4 °C until analysis.

Quantifying measurement accuracy using sensor overlord

To evaluate the quantitative capability of the GRIT sensor for measuring tryptophan concentration, we utilized the "SensorOverlord" R package to model the GRIT sensor and predict its accuracy. Based on our previous research [[9\]](#page-11-7), we calculated the midpoint potential (pK_d) to be 3.37,

derived from a dissociation constant (K_d) of 430 μ M, a critical parameter indicative of the sensor's affinity. Using our fuorescence spectral data and two excitation peaks, we determined the values of R_{min} , R_{max} , and delta2 to be 0.52, 7.73, and 0.25, respectively. For microscopy error, we determined it to be 0.02, based on our experimental fndings demonstrating that 95% of observed ratios had a relative error of no more than 2% [\[16](#page-11-14)]. Additionally, we set an error threshold 0.05–0.2 to represent the detection range of tryptophan concentrations by GRIT as previously described.

Principle and equations for quantitative measurement of tryptophan in vitro and in vivo

The fundamental assumption of quantitative measurement with the ratiometric biosensor GRIT is that the properties of the purifed sensor could be used as a reference to measure tryptophan levels in cells and in vivo [[38\]](#page-12-5).

 (1) The binding affinity of the GRIT sensor follows the Hill equation [[39\]](#page-12-6):

$$
[Trp] = K_d [(R - R_{min})/(R_{max} - R)]^{1/n}
$$
 (1)

where K_d is the apparent dissociation constant, which is equal to the tryptophan concentration when half of the sensor is bound, and n is the Hill coefficient. R represents the excitation fuorescence ratio of the biosensor (F_{485}/F_{420}) . R_{min} and R_{max} correspond to the 0% and 100% fraction bound, respectively.

 (2) The GRIT sensor is purified from the bacterial expression system, so we can calibrate tryptophan levels in bacteria by ftting the excitation fuorescence ratios of cells with the in vitro titration curve. Intracellular pH could change the excitation ratio of the GRIT sensor and mislead the calibration of tryptophan concentration; thus, the GRTIOL sensor should be used as a control in the parallel experiment for correction.

(3) It has been proven that the K_d values of biosensors in vitro and in cells are often comparable $[40]$. Thus, we could measure the R_{min} and R_{max} of the GRIT sensor in situ to calibrate the tryptophan concentration in HeLa cell cultures. LAT1 is highly expressed in HeLa cells and can import and export tryptophan upon the addition of tryptophan and histidine, respectively. Therefore, we could approximate the maximal and minimal fuorescence ratios of the GRIT sensor in living cells by those treatments, and the dynamic range of the GRIT sensor in cells (9.6-fold) is comparable with that of purifed protein $(12.9\text{-}fold)$. The control experiment with the GRITOL sensor should also be performed in parallel experiments. With the two points R_{min} and R_{max} , we can calculate the sensor occupancy using the equation below:

$$
\theta = (R - R_{min}) / (R_{max} - R_{min}) \tag{2}
$$

where θ is defined as the sensor occupancy, obtained by dividing the fuorescence ratio of bound GRIT to the fluorescence ratio of total GRIT. The sensor occupancy *θ* could be converted to tryptophan concentration by ftting with the in vitro titration curve.

$$
\theta = [\text{Trp}]^{n} / [(K_{d})^{n} + [\text{Trp}]^{n}]
$$
\n(3)

(4) To calculate the biophysical properties of tryptophan metabolism, we measured the parameters of K_m and tryptophan concentration change rate. K_m is defined as the concentration of substrate that is transported at half the maximal velocity (V_{max}) of transport. We calculated K_m with the Michaelis–Menten equation.

$$
V = V_{\text{max}}[\text{Trp}]/(K_m + [\text{Trp}])
$$
\n(4)

where *V* is defned as the change in the excitation ratio of the intracellular GRIT sensor per min and can be calculated with the equation below.

$$
V = (R_{t1} - R_{t0})/\Delta t \tag{5}
$$

The tryptophan concentration change rate is defined as the changes in intracellular tryptophan concentrations per min, including the tryptophan uptake rate, tryptophan export rate, and endogenous tryptophan consumption rate. These rates can be calculated with the equation below:

$$
Vt = (\left[Trp\right]_{t1} - \left[Trp\right]_{t0})/\Delta t \tag{6}
$$

where the [Trp] concentrations are calculated with Eq. 3 using the sensor occupancy at a specifc timepoint (t_0 and t_1), and Δt is the interval between t_0 and t_1 .

(5) For the quantitative measurement of tryptophan in zebrafsh, the ratiometric GRIT sensor provides builtin self-calibration for signal correction, which is not afected by sensor expression levels. We isolated primary zebrafsh cells expressing the GRIT sensor from zebrafsh larvae. We measured the R_{min} and R_{max} of the GRIT sensor by adding tryptophan and histidine because they also express the LAT1 transporter $[41]$ $[41]$ $[41]$. The dynamic range of the GRIT sensor in primary zebrafsh cells (7.5-fold) is comparable to that of HeLa cells (9.6-fold). Because we used the same imaging conditions and confocal microscopy, the R_{min} and R_{max} of primary cells in vitro can be used to calculate the mean GRIT sensor occupancy in tissue with Eq. 2.

The tryptophan concentrations in a given tissue were calibrated by normalizing the GRIT signals by the mean GRITOL signal from massive cells. Thus, the corrected mean GRIT sensor occupancy is independent of the minor heterogeneity among tissue cells (such as pH) and

represents the mean tryptophan concentration in this tissue with Eq. 3. This GRITOL-based calibration is applicable at the tissue level but not at the single-cell level.

Quantitative measurement of tryptophan with GRIT sensor in vitro and in vivo

Accurate and quantitative assessments of tryptophan levels in cells and serum samples are achievable through the calculation of normalized sensor fuorescence ratios and comparing these ratios with those obtained from purifed GRIT protein in vitro, as described previously [\[9](#page-11-7)].

For the quantifcation of serum tryptophan concentrations with GRIT sensor, serum sample was equally mixed with 1 μM GRIT or GRITOL sensor in 100 mM HEPES bufer, 100 mM KCl (pH 7.3), followed by routine fuorescence measurement similar to protein titration experiments.

For quantifcation bacterial tryptophan, we measured the excitation fuorescence ratios of cells expressing the GRIT sensor with or without 40 μ M tryptophan as the intracellular tryptophan levels in tryptophan-fed cells and tryptophan-starved cells, respectively. To account for the pH efect, the excitation ratios of cells expressing GRIT were corrected by those of cells expressing GRI-TOL measured in parallel and ftted with an in vitro protein titration curve at pH 7.3.

For in situ live-cell calibration, the unbound and saturated states of the mito-GRIT sensor in HeLa cells could be approximated by treatment with 5 mM histidine and 0.5 mM tryptophan in modified HEPES buffer (pH 7.4). The detection conditions were similar to those in live-cell fluorescence measurements. The mitochondrial tryptophan levels were estimated by ftting with purifed protein titration curves at pH 8.0.

Tryptophan quantifcation with high‑performance liquid chromatography

HPLC method was used to accurately quantify intracellular tryptophan levels in HeLa cells. We extracted the intracellular metabolites using 80% pre-cold methanol, evaporated the supernatant, and dissolved the samples in 100 µL of 90% acetonitrile to remove proteins before LC/MS quantification. The quantification process was carried out using a UHPLC system (1290 series; Agilent Technologies, USA) coupled with a quadruple time-offight mass spectrometer (TripleTOF 6600, AB SCIEX, USA). The results were analyzed using the Agilent Mass-Hunter Qualitative Analysis Navigator (B.08) software.

Mitochondria were extracted by a mitochondria isolation kit (Beyotime) and protein concentration was quantifed with a BCA kit (Mxbioscience LLC), followed by LC/MS measurement. The protein amount was converted to mitochondria volume as reported [\[8](#page-11-6)].

The plasma tryptophan level was quantified with precolumn derivatization and reverse phase ultra-performance liquid chromatography (RP-HPLC) [[42](#page-12-9)]. In brief, protein was precipitated by acetonitrile treatment in serum samples and centrifuged at 13,000 rpm for 20 min. Derivatization of the supernatant was carried out at 55 °C for 10 min, followed by separation and quantitative analysis by external standard method with RP-HPLC.

Statistical analysis

Data are presented as the mean±s.e.m. from at least three experiments. All statistical analyses and graphical representations were performed using R and Python. The fgures were compiled and fnalized using Adobe Illustrator 2020.

The normality of the data was tested using the Kolmogorov–Smirnov test. For comparisons between two groups, the two-tailed unpaired Student's *t*-test was employed for data with a normal distribution in the majority of results, while the Mann–Whitney test was used for data with a non-normal distribution. The specifc sample size (*n* numbers) and *P* values of each fgure in the zebrafsh and human serum sample experiments are listed in the corresponding fgures or legends.

Abbreviations

Supplementary Information

The online version contains supplementary material available at [https://doi.](https://doi.org/10.1186/s12915-024-02058-x) [org/10.1186/s12915-024-02058-x.](https://doi.org/10.1186/s12915-024-02058-x)

Additional fle 1: Figures S1-S4, Tables S1-S2 and Note S1. Figure S1 [[14\]](#page-11-12). Detection of tryptophan uptake in living bacteria. Figure S2. Detection of tryptophan dynamics in mitochondria of HeLa cells. Figure S3. Detection of tryptophan levels in the serum samples from infamed individuals. Figure S4. Zebrafsh sleep changes during infammation, detection of metabolites levels in zebrafsh larvae, and the death rate post tryptophan metabolism related inhibitors treatment. Table S1 [\[9,](#page-11-7) [10](#page-11-8), [15](#page-11-13), [26,](#page-11-24) [43](#page-12-10)]. Quantifcations of tryptophan level in bacteria, mammalian cells, zebrafsh, and human serum. Table S2. The effect of 19 amino acids on the tryptophan dynamics in mitochondria of HeLa cells. Note S1. The amino acid sequence information of Mito-GRIT and Mito-GRITOL sensor.

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Authors' contributions

 R. T. and Y. M. conceived the project. R. T., K. W., T. C., J. C., X. Z., and W. P. performed experiments. R. T., Y. M., K. W., T. C., and X. Z. analyzed data and made fgures. C. J. and W. M. provided the human serum samples. R. T., Y. M., and J. D. wrote the draft and revised the manuscript. All authors read and approved of the fnal manuscript.

Authors' Twitter handles

Twitter handles: @vivianstats (Wei Vivian Li).

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Data availability

All data generated or analyzed during this study are included in this published article and its supplementary information fles. The cytoplasmic version of the GRIT or GRITOL sensor sequences used for bacterial expression can be found in our previously published article [\[9](#page-11-7)]. The Mito-GRIT and Mito-GRITOL sensor amino acid sequences are listed in Additional fle 1: Note S1. All constructs are available upon requests.

Declarations

Ethics approval and consent to participate

The experimental protocols involving zebrafsh were approved by the Chinese Academy of Sciences (Approval no. NA-046–2019). All the population studied were from patients of Taizhou Hospital of Zhejiang Province afliated to Wenzhou Medical University. The experiments were performed according to the medical ethics rules (no. K20211202).

Consent for publication

Not applicable.

Competing interests

The authors declare no competing fnancial interests.

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