

Establishing a Reference Database for Select Clinical Measures in National Basketball Association Players

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Background: Musculoskeletal injuries are prevalent in the NBA and are associated with a significant number of games missed. There is a lack of reference data for clinical measures in NBA players, making it difficult for sports medicine professionals to set goals and develop programs.

Hypothesis: Values for clinical measures in NBA players will differ from those of the general population but will not differ between dominant (D) and nondominant (ND) limbs.

Study Design: Descriptive laboratory study.

Level of Evidence: Level 3.

Methods: Clinical measures were taken on 325 players invited to NBA training camp (2008-2022). Measures included range of motion for great toe extension, hip rotation, weightbearing ankle dorsiflexion, flexibility, arch height (AH) indices, and tibial varum.

Results: Clinical values for NBA players differ from reference norms of the general population. Results for NBA players include great toe extension (D, 40.4°; ND, 39.3°), 90/90 hamstring (D, 41.5°; ND, 40.9°), hip internal rotation (D, 29.0°; ND, 28.8°), hip external rotation (D, 29.7°; ND, 30.9°), total hip rotation (D, 60.2°; ND, 60.4°), Ely (D, 109.9°; ND, 108.8°), AH difference (D, 0.5 mm; ND, 0.5 mm), AH index (D, 0.310; ND, 0.307), arch stiffness (D, 0.024; ND, 0.024), arch rigidity (D, 0.924; ND, 0.925), tibial varum (D, 4.6°; ND, 4.5°), and weightbearing ankle dorsiflexion (D, 35.4°; ND, 35.6°). Descriptive statistics are presented; 2-tailed paired *t* tests show that, whereas most measures demonstrated differences between sides, the results were not statistically significant.

Conclusion: Clinical measures of NBA players differ from those reported for the general population and athletes of other sports although there were no statistically significant differences between D and ND limbs.

Clinical Relevance: Establishing a reference database may help clinicians develop more sensitive and more effective preseason and return-to-play screening processes, aiding the management of player orthopaedic care and reducing injury risk.

Keywords: basketball; clinical measures; compliance; NBA; ROM; stiffness

Over the last decade, there have been a significant number of games missed in the National Basketball Association (NBA) due to injury.^{28,43,63} It has been estimated that the direct cost of injuries in the NBA is US\$350 million in lost revenue each season.^{62,63} Many of these injuries

are musculoskeletal in nature^{28,43} and may be related to an inappropriate degree of stiffness and/or compliance in the lower extremities as they relate to tissue stress-strain dynamics.^{11,12} The concept of stiffness is based on Hooke's Law, which refers to a tissue's ability to resist deformation.^{11,12}

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Whereas lower extremity stiffness is considered to be a key factor in optimizing running, jumping, and hopping activities, too much stiffness has been associated with reduced joint motion, a decreased ability to absorb forces, and bony injury.^{4,15,17,72} On the other side of the continuum, too much compliance has been linked to an increased risk for soft tissue injury and muscle strain.^{11,12,71} Therefore, there appears to be an optimal level of muscle stiffness for athletes that allows them to maximize performance and minimize injury. However, the relationship between stiffness, compliance, and injury risk may not be linear.

Sports medicine professionals utilize a variety of assessments to help understand these factors to make informed decisions about an athlete's rehabilitation or sports performance program. However, there is a lack of reference data for clinical measures in professional basketball players, making it difficult for sports medicine professionals to set goals, develop programs, and make interventions. In contrast, normative data exists for certain clinical measures for other professional athletes. In Major League Baseball (MLB) players, it has been well established that the degree of shoulder external rotation (ER) range of motion (ROM) (140°) - a reflection of compliance - differs from textbook values that have been reported for the general population (90°).^{7,10,19,23,24,29,57,58} The relationship between ROM and injury risk has been described for the lower extremity as well.^{3,9,25,30,31,35,36,40,44,59,64} As such, sports medicine professionals understand that not only are the ROM goals for elite overhead athletes different, but their unique degree of compliance or stiffness is vital for these athletes to perform efficiently and effectively in their sport.

For jumping athletes, it has been noted that measures such as lower extremity flexibility, ROM, and arch height (AH) and rigidity indices reflect the stiffness-compliance continuum that influences performance and functional movement. If a reference database were established and these factors were better understood, more sensitive and effective preseason and return-to-play screening could be adopted.^{11,12,14,18,21,22,28}

The aim of this study is to retrospectively analyze preseason testing measures to establish reference values in professional NBA players.

METHODS

This study was approved by the university Institutional Review Board (IRB). The participants include 325 NBA players from 3 teams who were invited to NBA training camp or were on the roster for the 2008-2022 seasons (age, 25.5 ± 3.9 years; height, 2.00 ± .079 m; weight, 99.89 ± 12.38 kg; body mass index [BMI], 24.66 ± 1.89 kg/m²). In this study, 74.2% of the players were Black, 17.8% were White, 2.1% of the players were Latino of any race, and 5.9% of the players were classified as either multiracial or "other" races. Clinical measures were taken as part of the team's typical clinical care and assessment program by a single examiner who is a board-certified clinical specialist in orthopaedic physical therapy with >20 years of experience. All

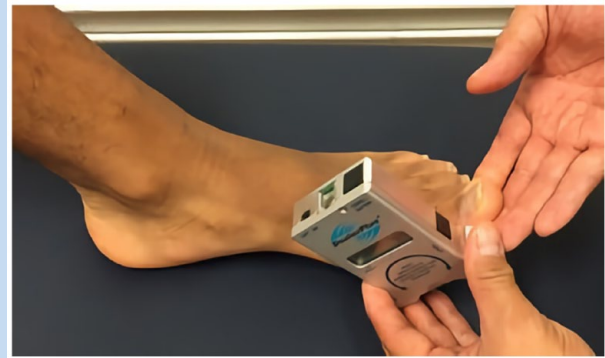


Figure 1. Great toe extension measured with the subject supine and knee flexed to 90° with the foot flat.

research initiatives were retrospective in nature. Data were excluded for players who were injured, rehabilitating an injury, or not cleared by their team medical staffs to participate in preseason assessments. Great toe extension was measured with the subject supine and the test side knee flexed to 90° with the foot flat (Figure 1). Maintaining contact with the plantar surface of the foot on the table, the great toe was extended passively at the metatarsophalangeal joint to the first tissue stop, and ROM was measured with a digital inclinometer.^{33,39} The arch height index (AHI) measurement system (AHIMS) protocol was utilized to assess the arch in sitting and standing positions (Figure 2).^{8,16,55,65,68,71,73,74} Measurements were made in a seated position with the subject's hips and knees flexed to 90°. Using the AHIMS protocol, foot length, truncated position, and AH were recorded. These measures were repeated with the subject standing with maximum pronation. Subsequently, AHI, AH difference, stiffness, and rigidity values were calculated. Weightbearing ankle dorsiflexion was measured with the player facing the wall with the test leg forward and the contralateral limb in-line behind the subject with the heel raised (Figure 3).^{5,27,40,56,70} The test foot was placed 5 inches from the wall on a taped line so that the heel and the second digit were aligned. The player was then instructed to flex the knee and bring the center of the patella as close to the wall as they could without raising the heel. The degree of ankle dorsiflexion was measured with a digital inclinometer. Hamstring (HS) length was measured with the 90/90 test (Figure 4).^{33,39} The athlete was positioned supine with the contralateral limb extended with neutral rotation. The test leg was flexed to 90° at the hip and knee. The knee was then extended until the first tissue stop and the ROM was measured with a digital inclinometer. Hip ROM was measured with the subject prone and the contralateral limb in a neutral position (Figure 5).^{1,33,39} The test leg was flexed at the knee to 90° and moved into internal rotation (IR) and ER for 3 repetitions. The hip was then moved into IR until the first tissue stop without the pelvis raising and ROM was measured with a digital inclinometer. The hip was returned to neutral and then into ER until the first tissue stop and measured with a digital inclinometer. Tibial varum



Figure 2. AHI measures were taken to classify arch type and to calculate arch rigidity and stiffness. AHI, arch height index.



Figure 3. Weightbearing ankle dorsiflexion was measured with tibial advancement without raising of the heel.

was measured with the athlete standing, feet together, with a digital inclinometer aligned with a line made at the bisection of the distal third of the lower leg (Figure 6).^{1,33}

Data Analysis

Data were retrospectively pooled, analyzed, and correlated using JMP (<https://www.jmp.com>). Descriptive summary statistics were calculated for all outcome measures, enabling the establishment of the reference values. Inferential statistics were also calculated and *t* distribution values are presented to

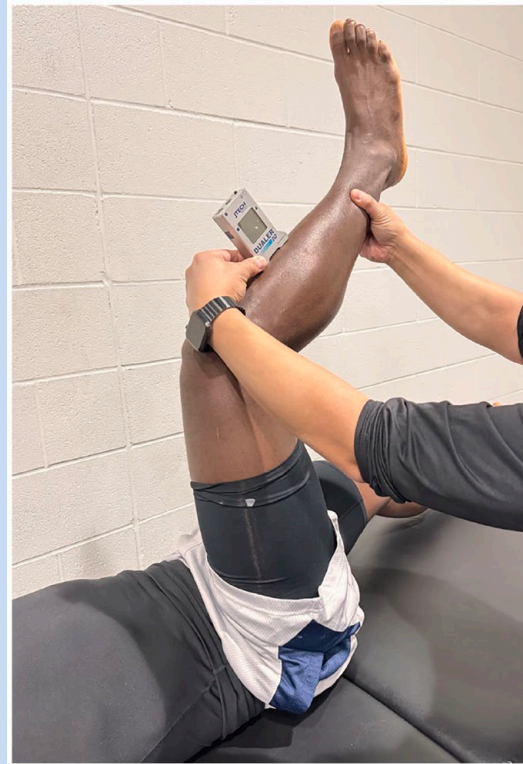


Figure 4. HS flexibility via the 90/90 HS test. HS, hamstring.

demonstrate any significant differences between the dominant (D) and nondominant (ND) side.

RESULTS

The results for all NBA players include great toe extension (D, 40.4°; ND, 39.3°), 90/90 HS (D, 41.5°; ND, 40.9°), hip IR (D, 29.0°; ND, 28.8°), hip ER (D, 29.7°; ND, 30.9°), total hip rotation (D, 60.2°; ND, 60.4°), Ely (D, 109.9°; ND, 108.8°), AH difference (D, 0.5 mm; ND, 0.5 mm), AHI (D, 0.310; ND, 0.307), arch stiffness (D, 0.024; ND, 0.024), arch rigidity (D, 0.924; ND, 0.925), tibial varum (D, 4.6°; ND, 4.5°), and weightbearing ankle dorsiflexion (D, 35.4°; ND, 35.6°). Descriptive statistics for D and ND limbs are tabulated in Table 1.

Two-tailed paired *t* tests were run comparing the D and ND clinical measures. Whereas the majority of these measures demonstrated differences between sides, the results were not statistically significant (Table 1).

DISCUSSION

Many decisions in sports medicine and performance practice are based on clinical values, despite the fact that athletes from different sports have anatomic and physiological characteristics that lead to associated variance in their measures. Establishing a reference database of select clinical measures in specific athletic



Figure 5. The hip was measured for IR, ER, and total rotation ROM. ER, external rotation; IR, internal rotation; ROM, range of motion.



Figure 6. Tibial varum.

populations may be important in distinguishing the interpretation between normal variance, being advantageous to performance, or pathological versus subgroup variance. The absence of reference clinical data can lead to challenges in understanding how the interpretation of measures associated with preparticipation screening relates to risk stratification, the creation of injury prevention programs, and setting appropriate rehabilitation or performance goals.^{49,50,53,54,61} Of specific interest are measures that have been identified as risk factors in athletes and clinical patterns that have been identified by experienced practitioners.^{15,24,46,64,70}

Lower extremity mobility and flexibility in basketball athletes influences performance and risk of lower quarter injury. These factors may be related to a less-than-optimal degree of stiffness and/or compliance. Stiffness has been described as the resistance of a structure to deform in response to an applied force.^{15,37,52} Athletic performance in tasks associated with sports, such as hopping, jumping, running, and change of direction, have been shown to be influenced by global stiffness characteristics of the lower extremity. Compliance is viewed as the inverse of stiffness and is found on the other end of the structural deformity continuum. A compliant tissue is more easily deformed under load.¹³

Overall, the current study suggests that professional basketball players have less range of motion, decreased flexibility, and

increased stiffness compared with the general population (Table 2). An athlete who demonstrates greater stiffness characteristics should be able to store more elastic energy when contacting the ground during the yielding phase of jumping and, thus, generate a higher level of concentric force output when pushing off. It is logical that professional basketball players present with different structural characteristics than the general population.

The American Academy of Orthopaedic Surgeons¹ reports a mean hip internal and external ROM of 45°, but athletes from various sports have been shown to have hip IR values between 26° and 36° and ER values ranging from 39° to 44°.^{3,35,36,44,64} The current study found the mean degree of hip IR and ER for NBA players to be about 29° and 30°, respectively. It has been reported that decreased ROM is a risk factor for groin pain if the combined hip rotation ROM is <85°.⁶⁴ Cam morphology and dysfunction such as femoral acetabular impingement has been linked with limitations in hip ROM.^{36,44} It has been reported that male athletes participating in specific high-level impact sports such as basketball are at increased risk of physeal abnormalities of the anterosuperior head-neck junction, and are 1.9 to 8.0 times more likely to develop a cam deformity than male controls.⁴⁷ However, the exact relationship between hip structure and pain is unclear.³¹ In fact, increased stiffness at the hip joint may be an advantage in sport performance, and athletes have been identified as having mean rotational and

Table 1. Descriptive statistics for D and ND limbs

All	N	D	SD	ND	SD	t Value	df	Significance	Mean Difference	95% CI of the Difference	
										Lower	Upper
Great toe extension	326	40.380	8.9	39.26	8.3	1.7	650.0	0.1	1.1	-0.2	2.4
90/90	325	41.498	9.8	40.93	9.5	0.7	648.0	0.5	0.6	-0.9	2.1
Hip IR	326	28.969	9.4	28.76	9.9	0.3	650.0	0.8	0.2	-1.3	1.7
HIP ER	326	29.690	8.9	30.87	8.8	1.7	650.0	0.1	-1.2	-2.5	0.2
Total hip rotation ROM	326	60.230	12.2	60.42	12.6	0.2	650.0	0.8	-0.2	-2.1	1.7
Ely's test	208	109.856	16.3	108.82	14.8	0.7	414.0	0.5	1.0	-2.0	4.0
Arch height difference	314	0.475	0.2	0.472	0.2	0.2	626.0	0.8	0.0	0.0	0.0
AHI	314	0.310	0.0	0.307	0.0	1.5	626.0	0.1	0.0	0.0	0.0
Arch stiffness	314	0.024	0.0	0.024	0.0	0.6	626.0	0.5	0.0	0.0	0.0
Arch rigidity	315	0.924	0.1	0.925	0.1	0.1	628.0	0.9	0.0	0.0	0.0
Tibial varum	320	4.578	3.0	4.52	3.1	0.2	638.0	0.8	0.1	-0.4	0.5
Weightbearing ankle dorsiflexion	317	35.378	5.3	35.58	5.7	0.5	632.0	0.6	-0.2	-1.1	0.7

AHI, arch height index; D, dominant; ER, external rotation; IR, internal rotation; ND, nondominant; ROM, range of motion.

Table 2. Basketball players have less range of motion, decreased flexibility, and increased stiffness compared with the general population

All	D	ND	General Population	Sources
Great toe extension	40.38°	39.261°	50°-65°	Kendall, ³³ Magee ³⁹
90/90	41.49°	40.938°	20°-30°	Kendall, ³³ Magee ³⁹
Hip IR	28.96°	28.76°	45°	American Academy of Orthopaedic Surgeons, ¹ Kendall, ³³ Magee ³⁹
HIP ER	29.69°	30.87°	45°	
Total hip rotation ROM	60.23°	60.42°	90°	
Ely test	109.85°	108.82°	120°-125°	Kendell, ³³ Magee ³⁹
Arch height difference	0.475	0.472	NA	
AHI	0.310	0.307	0.326-0.350	Bjelopetrovich and Barrios, ⁸ Butler et al, ¹⁶ Pohl et al, ⁵⁵ Tipnis et al, ⁶⁵ Weimar and Shroyer, ⁶⁶ Williams et al, ⁷¹ Zhao et al, ⁷³ Zifchock et al ⁷⁴
Arch stiffness	0.024	0.024	0.031	Tipnis et al, ⁶⁵ Zhao et al, ⁷³
Arch rigidity	0.924	0.925	0.903-0.913	Tipnis et al, ⁶⁵ Zhao et al, ⁷³
Tibial varum	4.57°	4.525°	4°-6°	American Academy of Orthopaedic Surgeons, ¹ Kendall, ³³ Magee ³⁹
Weightbearing ankle dorsiflexion	35.37°	35.58°	50°-56.3°	Dill et al, ²⁷ Rabin et al ⁵⁶

AHI, arch height index; D, dominant; ER, external rotation; IR, internal rotation; ND, nondominant; ROM, range of motion.

^aLower value represents greater degree of compliance.

^bLower value is more stiff.

^cHigher value is more stiff.

combined motion <85°. ^{3,36,44} Hockey players have demonstrated a mean total hip rotational ROM of 70°, ⁴⁴ and soccer players have shown a mean of 75°. ³⁶ The mean degree of total hip rotation ROM in our study was 60°. This may suggest that professional basketball players have a stiffer hip joint, which may be advantageous with regard to their ability to pivot quickly and change direction during basketball play or, alternatively, this motion loss could be an acquired characteristic similar to the loss of IR of the throwing shoulder in baseball pitchers. ¹⁰

The 90/90 test has been described as a measure of HS flexibility with the general population presenting with a mean popliteal angle of 20°. ^{33,39} The NBA players in the current study demonstrated less flexibility, with a mean of 41.5° and 40.9° on D and ND limbs, respectively. Similarly, the Ely test is commonly used as a measure of rectus femoris flexibility with a positive sign being the inability to bring the heel of the test leg to the ipsilateral buttock. ^{33,39} The mean value of knee flexion in the current study during Ely tests was about 109°, with the inability

to meet the criteria for the test as noted. These measures are in alignment with the overall presentation of elite NBA players such that their lower extremity musculature appears to be less compliant and more stiff compared with the general population. It is well recognized that HS and quadriceps work synergistically to dynamically stabilize the knee joint during athletic activities, especially acceleration and deceleration. ^{25,27,42,65}

Tibial varum values in the general population have been reported at between 4° and 6°. ^{1,33,39} The athletes in this study demonstrated a mean of 4.5° bilaterally. An optimal degree of tibial varum may be important to elite basketball players because there may be an increased risk for injury at each extreme. A low degree of tibial varum is associated with genu valgus and can lead to excessive frontal plane motion at the knee, which is commonly associated with patellofemoral dysfunction and medial collateral ligament or anterior cruciate ligament (ACL) injuries. ⁶⁶ Likewise, an extreme degree of tibial varum is associated with a decreased ability to absorb ground reaction forces and has been linked to stress fractures, lateral

ankle sprains, and degenerative joint disease.⁶ The current study also demonstrated that the vast majority (>97%) of NBA players assessed presented with genu varus.

Dominant limb weightbearing ankle dorsiflexion in the general population has been shown to mean 50° with an ND side mean as high as 56.3°. ^{27,56} Limitations in ankle motion have been associated with injury risk such as ACL rupture, patellofemoral pain syndrome, or ankle sprains. ^{9,30,51}

In female volleyball athletes, <45° ankle motion had a strong correlation with patellar tendinopathy.⁴⁰ However, the optimal degree of stiffness does appear to vary for athletes of different sports.⁵ The current study found that professional basketball players have a mean 35.4° on the D limb and 35.6° on the ND side. Increased stiffness in the gastroc-soleus complex can be considered an advantage for jumping athletes because this tissue modulus offers a higher level of elastic energy and spring required to propel off the ground. ^{11-12,15,37,72}

Foot type may be associated with both performance and injury risk. A change in foot type may occur as an adaptation to physical demands. A large and planus foot may be associated with the athletic population.⁷³ Foot type may be predictive of function during athletic tasks such as running.² The AHIMS has been utilized to classify foot type and describe arch rigidity and stiffness. ^{8,16,55,65,68,71,73,74} The mean AHI measures in this study were 0.310 (D) and 0.307 (ND). These values are much lower than what has been reported in the general population (0.338-0.343) and suggest that the mean NBA player foot type is pes planus. ^{55,68,74} The mean arch rigidity index (ARI) values and arch stiffness (AS) values for our subjects were found to be 0.925 (ARI) and 0.024 (AS), respectively, suggesting that the typical NBA player has an arch that is more stiff and rigid compared with the general population. ^{16,65,74} A predominant foot type for performance by way of improved force production may come at the expense of other physical attributes such as balance, and may predispose players to certain pathologies due to its unbalanced position on the stiffness-compliance spectrum. ¹⁶

The kinetic chain relationship of stiffness and compliance throughout the lower extremity should be considered when reviewing clinical measures. Athletes may develop functional adaptations or biomechanically self-select toward a specific sport. We hypothesize that a stiff and planus foot with limited weightbearing ankle dorsiflexion may provide an athlete a stiffer spring to generate force and create a competitive advantage. Similarly, reduced mobility in the hips may be a driver of multiplanar force generation. The joint measures have been shown to influence movement at a fundamental and functional level.²⁰ Specifically, local mobility limitations at the ankle and hip have been shown to be associated with changes in multijoint movements such as squatting and lunging. ^{20,21,32,34,38} Further, morphological and mobility limitations may impact balance and multiplanar single leg control. ⁴⁸ The multifactorial relationship of various clinical measures on the movement system may be combined to assess the risk or association with future injury.⁴² Further analysis in different athletic populations may determine whether the relationships between various

clinical measures have direct implications on specific sporting populations as they relate to performance, injury risk, and return to performance after injury.

Our analyses did not demonstrate any statistically significant differences between D and ND side. This finding is of note because side-to-side ROM differences have been documented in other sports. Asymmetrical glenohumeral ROM in professional baseball pitchers is well established, ^{7,10,19,23,24,29,57,58} whereas American college football players show no lower extremity ROM differences in D versus ND limb or across positions.²⁵ Male field hockey players were found to have no clinically relevant differences in hip ROM between D or ND leg or different playing positions.³ In elite soccer academy players, higher ROM values were found in D versus ND hip ROM, whereas playing position yielded no differences. Interestingly, in professional soccer players, leg dominance did not yield side-to-side ROM differences. ⁴⁴

Although there may be a perception that basketball players prefer to jump and pivot off 1 leg, our findings suggest that this preference does not impact D versus ND side-to-side ROM values but may be better explained by positional demands and body type. In today's NBA, certain positions demand more frequent sprints at full speed, more frequent and abrupt changes of direction, and more repetitive jumping and intense deceleration, all of which can impact body stresses and subsequent ROM. Our results suggest that leg dominance may not need to be accounted for when examining injury risk. We would suggest that positional demands and subsequent movement strategies specific to those demands account for ROM differences between professional basketball players.

In elite sport, overdiagnosis is always a risk given the ready access to diagnostic capabilities via imaging, movement assessments, and a seemingly endless choice of technologies promising to reduce injuries.²⁶ These data, often not clinically meaningful or fully understood, should lead clinicians to be cautious that it does not lend itself to overdiagnosis of the athlete. Overdiagnosis occurs when an abnormality is diagnosed correctly (ie, limited dorsiflexion) but the abnormality or diagnosis is irrelevant. ^{45,67}

Our hope is that proper understanding of these reference values, combined with an athlete's history and physical exam, will better inform clinicians as they develop an evidence-based plan of care. Incorrectly labeling an athlete as high risk is unfair to the athlete and may lead clinicians down an incorrect and inefficient plan of care. This reference database decreases instances of overdiagnosis and frees clinicians up from unnecessary treatment strategies. ⁴¹

LIMITATIONS

In line with clinical practice patterns, we used a digital inclinometer to measure ROM without any stabilization equipment (ie, belts). Additional stabilization would improve the validity and/or reliability of these measurements. Although all measures were taken by a single examiner, due to time

constraints we did not determine intrarater reliability measures. The findings of this study are also specific to NBA players and should be applied accordingly. The measures are not generalizable to other populations including women, or high school or collegiate players, etc. Unfortunately, we were unable to identify a database that contained these measures of persons from the general population that were of a similar height, weight, and body composition as the NBA players in this study. A limitation of this investigation is that the reference database was the more heterogeneous “general population.” In addition, although we attempted to represent a wide spectrum of NBA players from 3 teams over many seasons, it is likely that selection bias occurred regarding the type of player each team prefers (athletic vs strong vs long, etc).

CONCLUSION

The findings of this study support the hypothesis that NBA players present with clinical measures that are different from textbook values reported for the general population and athletes of other sports. Establishing a reference database for elite basketball players is relevant clinically and regarding performance because values that most accurately represent the physical characteristics of the player can give insight into their anatomic, biomechanical, and physiological make-up.

Lower extremity injury in elite basketball players is a significant problem for athletes, coaches, medical and performance staff members, and their teams.²⁸ The identification of modifiable risk factors is essential for injury prevention and management of player health.⁶⁰ Establishing a reference database for elite basketball players may play an important role in the management of the player's orthopaedic care and in reducing subsequent risk. By understanding these reference values, clinicians can better assess risk (or lack thereof) and mitigate unnecessary anxiety for both the athlete and clinician on clinical findings that may be abnormal for a normal population but are very well the norm in elite basketball players.

Requisite mobility norms for professional basketball players are not well quantified, nor is the effect, or lack thereof, of limb dominance on these reference values. Understanding these values, in addition to the impact of sport-specific joint kinematics and strength, may play a role in identifying athletes that carry higher susceptibility to acute or chronic orthopedic conditions.⁶⁹ This information may lead the clinician to a more detailed and efficient plan of care.

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