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Non-invasive brain stimulation enhances motor and cognitive performances during dual tasks in patients with Parkinson's disease: a systematic review and meta-analysis

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# **Abstract**

**Background** Parkinson's disease (PD) induces progressive deficits in motor and cognitive functions as well as impaired dual-task performance requiring both motor and cognitive functions. This systematic review and metaanalysis evaluated the effects of non-invasive brain stimulation (NIBS) on dual-task performance in patients with PD.

**Methods** 11 studies met the following inclusion criteria: (a) patients with PD, (b) NIBS intervention, (c) comparison with the sham stimulation group, (d) motor and cognitive performance outcomes during dual tasks, and (e) randomized controlled trials with parallel or crossover designs. Individual effect size (i.e., comparison) was quantified by comparing motor and cognitive performances changes during dual tasks between active NIBS and sham stimulation conditions. Thus, higher values of the overall effect size indicate more improvements in either motor or cognitive performances after NIBS. Moreover, moderator variable analyses determined whether NIBS effects on dual-task performances differed depending on targeted brain regions. Finally, meta-regression analyses determined whether NIBS effects on dual-task performances were associated with demographic characteristics.

**Results** The random-effects model meta-analysis revealed that NIBS significantly improved motor (73 comparisons from 11 studies) and cognitive (12 comparisons from four studies) performances during dual tasks in patients with PD. Specifically, anodal transcranial direct current stimulation protocols on the dorsolateral prefrontal cortex were effective. Moreover, greater improvements in motor performance during dual tasks significantly correlated with decreased age and increased proportion of females, respectively.

**Conclusion** This meta-analysis suggests that excitatory stimulation on the dorsolateral prefrontal cortex may be effective for improving dual-task performance in patients with PD.

**Keywords** Parkinson's disease, Dual task, Non-invasive brain stimulation, Transcranial direct current stimulation, Dorsolateral prefrontal cortex

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## **Introduction**

Parkinson's disease (PD), the second-most common neurodegenerative disorder, normally induces progressive deficits in motor and cognitive functions, as indicated by slower gait speed and impaired executive functions in patients with PD  $[1-5]$  $[1-5]$  $[1-5]$ . Moreover, patients with PD presented more impairments when performing dual tasks that simultaneously require motor and cognitive task goals than healthy older adults [[6–](#page-13-1)[8\]](#page-13-2). For example, patients with PD exhibited 18% reduction of step length from single-task walking to dual-task walking, whereas healthy older adults showed only 2% decrease in step length [[9](#page-13-3)]. Given that many activities of daily living frequently require dual tasks such as reading text messages on a smartphone while walking, patients with PD may be challenging for increasing independent life without specific rehabilitation protocols that effectively address dual-task impairments [[10](#page-13-4), [11](#page-13-5)].

Non-invasive brain stimulation (NIBS) techniques including transcranial direct current stimulation (tDCS) and transcranial magnetic stimulation (rTMS) have been explored as intervention protocols for improving dual-task performance due to their potential effects on modulating cortical excitability and facilitating neuroplasticity  $[12-15]$  $[12-15]$  $[12-15]$ . According to the central capacity sharing model [\[16\]](#page-13-8), cognitive resources may be divided when concurrently processing multiple stimuli due to a limited capacity. Thus, dual tasks such as using a smartphone while walking can lead to cognitive-motor interference presumably impairing the performance of either one or both tasks [[17](#page-13-9)]. Importantly, patients with PD typically showed impaired gait automaticity so that they may use more cognitive resources for successful locomotion while increasing cognitive-motor interference patterns [[18](#page-13-10), [19\]](#page-13-11). For example, although patients with PD revealed greater excitability in the dorsolateral prefrontal cortex (DLPFC) for executive functions, their gait patterns during dual tasks were slower and more variable than those of age-matched healthy older adults [[20\]](#page-13-12). These findings indicated that patients with PD may need more neural resources in the brain (e.g., DLPFC excitability) to compensate for their motor and executive deficits. Potentially, the primary motor cortex (M1) may be an additional key area to preserve motor functions during dual tasks because M1 excitability may advance the cortico-basal ganglia connections affected by striatal dopamine depletion [[21](#page-13-13)–[23](#page-13-14)]. Thus, NIBS protocols targeting these cortical regions may improve dual-task performance by attenuating cognitive-motor interferences. A systematic review and meta-analysis investigating tDCS effects on dual-task performances in older adults reported that anodal tDCS on the DLPFC significantly reduced dual-task cost of gait speed [\[24\]](#page-13-15). Taken together, quantifying potential overall effects of NIBS on dual-task performances in patients with PD may provide meaningful information on identifying optimal rehabilitation protocols contributing to increasing their independent life.

A recent systematic review study performed by Lin and colleagues [[25](#page-13-16)] revealed potential positive effects of NIBS protocols on gait speed and timed up and go (TUG) during dual tasks in patients with PD from three studies [\[14](#page-13-17), [26](#page-13-18), [27\]](#page-13-19). Although this study suggested a possibility of improvements in dual-task performances after NIBS protocols, these findings were still insufficient because of the limited number of included studies and no quantitative evidence by conducting data synthesis procedures. Thus, we investigated effects of NIBS on dual-task performances in patients with PD by conducting a systematic review and meta-analysis. Moreover, NIBS effects can vary with different targeted brain areas [\[28,](#page-13-20) [29](#page-13-21)]. Based on these findings, we addressed two leading questions: (1) Do NIBS techniques improve motor and cognitive performances during dual tasks in patients with PD? and (2) Do the effects of NIBS on motor and cognitive performances in patients with PD differ depending on the targeted brain regions?

## **Methods**

## **Literature search and study inclusion criteria**

We conducted the systematic review and meta-analysis consistent with Preferred Reporting Items for Systematic Reviews and Meta-analysis (PRISMA) guidelines [[30](#page-13-22)]. To formulate convincing eligibility criteria [[31\]](#page-13-23), we used Population, Intervention, Comparison, Outcomes, and Study design (PICOS) framework. Specifically, five inclusion criteria included: (1) Population: patients with PD; (2) Intervention: NIBS protocols; (3) Comparison: controls who received sham stimulation; (4) Outcome: motor and cognitive performance during dual tasks; and (5) Study design: studies that included randomized controlled trials (RCT) with either a parallel or crossover design. Moreover, we excluded case studies, animal studies, review articles, and studies that reported insufficient data for calculating effect sizes. Using two databases including PubMed and Web of Science, the literature search was performed from July 12, 2023, to August 14, 2023. For both search engines, we used the following keywords: (PD OR Parkinson's disease OR Parkinson) AND (NIBS OR noninvasive brain stimulation OR tDCS OR transcranial direct current stimulation OR tACS OR transcranial alternating current stimulation OR TMS OR transcranial magnetic stimulation OR rTMS OR repetitive transcranial magnetic stimulation OR tPCS OR

transcranial pulsed current stimulation OR tRNS OR transcranial random noise stimulation) AND (dualtask OR dual task OR concurrent OR walk OR gait OR locomotion OR cognition OR interference).

## **Data synthesis for meta-analysis**

Meta-analysis procedures were conducted using the Comprehensive Meta-Analysis software version 4.0 (Englewood, NJ, USA). Individual effect size (i.e., comparison) and overall effect size (i.e., effect size after data synthesis) were quantified by calculating standardized mean difference (SMD) with a 95% confidence interval (CI). We included multiple comparisons from one study when each comparison could be calculated based on different types of dual tasks, outcome variables, and NIBS protocols (e.g., targeted regions and timing). Higher SMD values indicate more improvements in dual-task performances after applying active NIBS protocols than those for sham stimulation condition. For RCT with a parallel design, individual effect sizes were calculated by comparing mean and standard deviation values of motor and cognitive performances between active and sham stimulation groups. For RCT with a crossover design, we calculated individual effect sizes using a paired analysis that applied the sample size and mean difference values with standard error  $[32-34]$  $[32-34]$  $[32-34]$ . To synthesize individual effect sizes, we used the random-effects model meta-analysis based on the traditional assumptions that inherent heterogeneity may exist among individual studies because of different experimental characteristics (e.g., participants, study protocols, and outcome measures). This approach may minimize the potential variability of effect sizes by reducing the influence of these methodological differences across individual studies [[35](#page-13-26)].

To estimate the heterogeneity levels across individual effect sizes, we used Higgins and Green's I-squared (*I* 2 ) indicating relationship between the distribution of true effects and observed effects [[36\]](#page-13-27). Typically, the  $25\%$ ,  $50\%$ , and  $75\%$  values of  $I^2$  denote low, moderate, and high heterogeneity levels, respectively [[37\]](#page-13-28). Moreover, the Egger's regression test was performed to determine whether significant levels of publication bias exist across individual effect sizes. A *P*-value for the intercept  $(\beta_0)$  of less than 0.05 indicates significant levels of publication bias [[38\]](#page-13-29).

### **Moderator variable analysis**

Additional moderator variable analyses were performed to specify effects of NIBS protocols on motor and cognitive performances during dual tasks in patients with PD. First, we investigated how NIBS influenced dual-task performances based on different types of motor functions (i.e., gait speed, cadence, double support time, stride time, stride length, step length, step width, stride time variability, stride length variability, TUG, time to return, and writing amplitude) and cognitive functions (i.e., number of correct generating words and counting). Second moderator analysis specified NIBS effects on dual-task performances according to different targeted brain areas (i.e., DLPFC, supplementary motor area; SMA, M1, and cerebellum). Finally, we conducted additional metaregression analyses to determine whether the effects of NIBS on motor and cognitive performances were associated with different demographic characteristics (i.e., mean age, proportion of the females, and duration since PD diagnosis).

## **Methodological quality assessment**

Using the Cochrane risk of bias assessment tool version 2 [[39](#page-13-30)], two researchers (H.L. and B.J.C.) independently evaluated potential methodological issues based on six specific domains: (1) randomization process (2), timing of identification or recruitment of participants (3), deviations from intended intervention (4), missing outcome data (5), measurement of the outcome, and  $(6)$  selection of the reported result  $[40]$  $[40]$  $[40]$ . Based on the criteria for algorithms in the Cochrane risk of bias assessment tool [[41](#page-13-32)], we judged the risk of bias for each domain by assigning one of three levels: (1) low risk of bias (2), some concern, and (3) high risk of bias. In the case of any discrepancy between the researchers, one leading researcher (N.K.) made a final decision.

## **Results**

### **Study identification procedure**

Initially, a systematic literature search identified 1,662 studies including 1,238 from the PubMed and 424 from the Web of Science, and then we removed 240 duplicated studies. The title and abstract of 1,422 studies were firstly screened, and 527 studies were excluded because of the following: (1) 404 review articles (2), 92 animal studies (3), 18 case studies, and (4) 13 studies that reported inaccessible contents. Full texts of the remaining 895 studies were carefully reviewed based on our inclusion and exclusion criteria, and 884 studies were further excluded: (1) 474 studies that did not focus on patients with PD (2), 62 studies that did not use NIBS intervention (3), 11 studies that did not involve sham stimulation group, and (4) 337 studies that did not estimate dual-task performances. Finally, 11 studies qualified for this meta-analysis [[14,](#page-13-17) [15](#page-13-7), [26](#page-13-18), [27,](#page-13-19) [42–](#page-13-33)[48\]](#page-13-34). Our study identification procedures are described in Fig. [1.](#page-3-0)

<span id="page-3-0"></span>



Fig. 1 PRISMA flowchart for the study identification procedure. PD=Parkinson's disease; NIBS=non-invasive brain stimulation; tDCS=transcranial direct current stimulation; rTMS=repetitive transcranial magnetic stimulation; RCT=randomized control trials

### **Demographic information on patients with PD**

From the 11 qualified studies, 284 patients with PD participated in experiments (a range of mean  $age = 50.1 - 72.8$  years and a range of mean duration after PD diagnosis = 3.5–9.3 years). Motor impairments in patients with PD at baseline was mild to moderate [[49](#page-13-35)[–51\]](#page-14-0): (1) a range of mean Hoehn and Yahr scale  $(H&Y) = 1.7-2.3$  and (2) a range of mean unified Parkinson's disease rating scale part III (UPDRS-III) = 15.8–47.7. Cognitive function of the participants was relatively normal  $[52, 53]$  $[52, 53]$  $[52, 53]$  $[52, 53]$ : (1) a range of mean mini-mental state examination (MMSE) = 25.5–29.7 and (2) Montreal cognitive assessment  $(MoCA) = 26.1-$ 28.0. The included studies reported that all patients with PD were on medication state. Table [1](#page-5-0) shows specific details on demographic information of patients with PD.

### **NIBS protocols for dual tasks**

For 11 qualified studies, nine studies applied tDCS and two studies used rTMS. For specific brain region of NIBS stimulation, tDCS protocols targeted: (1) DLPFC from five studies (2), M1 from three studies, and (3) three different targeted regions (i.e., DLPFC, M1, and cerebellum) from one study. Two studies that used rTMS protocols stimulated M1 and SMA, respectively. For the stimulation protocol type, nine tDCS studies applied anodal stimulation. For rTMS protocols, one study applied inhibitory stimulation  $(≤ 1 Hz)$ , whereas another study used both inhibitory and excitatory stimulation  $(> 5 Hz)$ . For the number of sessions, eight tDCS studies applied a single session and one study administered multiple sessions. Two rTMS studies applied multiple stimulation sessions. For the timing of NIBS protocols, seven tDCS studies used off-stimulation (i.e., tDCS before dual tasks) and two studies administered on-stimulation (i.e., tDCS during dual tasks) and off-stimulation, respectively. Two rTMS studies applied off-stimulation. Specifically, six out of the studies that used off-stimulation provided additional training while administering NIBS protocols: (1) writing figure-8 (2), physical therapy from one study (3), treadmill walking from one study (4), stationary bicycle and golf video game from one study, and (5) dual-task walking from two studies. In Table [2](#page-7-0), we describe the specific parameters of NIBS techniques.

## **Motor and cognitive performances during dual tasks**

Nine out of 11 included studies tested following motor performance during dual tasks: (1) gait (e.g., speed and cadence) from four studies (2), TUG from four studies, and (3) time to turn from one study. The remaining one study assessed both gait and TUG, and the other study evaluated writing amplitude. Moreover, three out of four studies estimated following cognitive performance during dual tasks: (1) the number of correct generating words from two studies and (2) the number of correct counting from one study. The remaining one study assessed both the number of correct generating words and counting. Table [3](#page-8-0) shows the specific motor and cognitive performances during dual tasks.

## **Methodological quality assessment results**

The Cochrane risk of bias assessment for the 11 qualified studies showed a relatively low risk of methodological biases across three domains: (1) timing of identification or recruitment of participants (2), missing outcome data, and (3) selection of the reported result. However, a relatively moderate risk of methodological biases was confirmed in following three domains: (1) randomization process (2), deviation from intended interventions, and (3) measurements of the outcome. Specifically, four studies failed to mention a specific randomization process and did not report information about the blinding of people who implemented the interventions or assessed performances. The methodological quality assessment for the included studies are described in Fig. [2.](#page-8-1)

## **Meta-analytic findings**

## *NIBS effects on motor performances during dual tasks in PD*

A random-effects model meta-analysis confirmed that NIBS significantly improved motor performances during dual tasks on 73 comparisons from 11 studies (Fig. [3\)](#page-9-0): *SMD* = 0.163; *SE* = 0.055; 95% CI = 0.056–0.271;  $Z = 2.975$ ;  $P = 0.003$ . Heterogeneity tests indicated that overall variability of individual effect sizes was relatively moderate  $(I^2=33.7\%)$ . Publication bias assessment indicated relatively symmetrical distribution of individual effect size (Egger's  $β_0 = -0.402$  with  $P=0.395$ ). These findings indicated that NIBS protocols may slightly improve motor performances during dual tasks with small heterogeneity.

Moreover, a moderator variables analysis showed that NIBS on the DLPFC significantly improved motor performances during dual tasks on 33 comparisons from six studies (Fig. [4](#page-10-0)): *SMD* = 0.298; *SE* = 0.069; 95% CI = 0.163–0.433; Z = 4.317; *P* < 0.001; *I* <sup>2</sup> = 35.5%; Egger's  $\beta_0 = 2.048$  with *P* = 0.003. Importantly, the six studies that reported overall positive effects used tDCS protocols. However, NIBS on the M1 failed to report significant effects on motor performances during dual tasks on 32 comparisons from five studies (Additional file 1): *SMD* = − 0.014; *SE* = 0.094; 95% CI =  $-0.199 - 0.171$ ; Z =  $-0.145$ ;  $P = 0.885$ ;  $I^2 = 27.8\%$ ; Egger's  $\beta_0 = -5.525$  with *P* < 0.001. These findings suggested that tDCS protocols targeted the DLPFC may

<span id="page-5-0"></span>

produce slight enhancements in motor performances during dual tasks with small heterogeneity.

## *NIBS effects on cognitive performances during dual tasks in PD*

A random-effects model meta-analysis found that NIBS significantly enhanced cognitive performances during dual tasks on 12 comparisons from four studies (Fig. [5\)](#page-10-1): *SMD* = 0.375; *SE* = 0.110; 95% CI = 0.161–0.590;  $Z = 3.427$ ;  $P = 0.001$ . Importantly, the four studies that reported overall positive effects used tDCS protocols. Heterogeneity tests showed that overall variability of individual effect sizes was relatively moderate  $(I^2 = 36.3\%)$ . Publication bias assessment showed a no significant publication bias across individual effect sizes (Egger's  $\beta_0$  = 2.047 with *P* = 0.070). These findings implied that tDCS protocols may moderately improve cognitive performances during dual tasks with small heterogeneity.

Moreover, moderator variables analysis reported that NIBS on the DLPFC significantly improved cognitive performances during dual tasks on eight comparisons from three studies (Fig. [6\)](#page-10-2): *SMD* = 0.283; *SE* = 0.099; 95% CI = 0.089–0.478; Z = 2.860; *P* = 0.004; *I <sup>2</sup>* = 20.9%; Egger's  $\beta_0 = -0.061$  with *P* = 0.985. Importantly, the three studies that reported overall positive effects used tDCS protocols. These findings showed tDCS protocols on the DLPFC may lead to small enhancements in cognitive performances during dual tasks with minimal heterogeneity.

## **Meta-regression analyses**

The random-effects meta-regression analyses revealed that greater improvements in motor performances during dual tasks after NIBS were significantly associated with decreased age (*Y* = 1.61 − 0.02*X*; *P* = 0.004; Fig. [7](#page-11-0)A) and increased proportion of females in total patients with PD (*Y* = 0.00 + 0.58*X*; *P* = 0.026; Fig. [7B](#page-11-0)), respectively. However, the amount of duration since PD diagnosis was not significantly associated with improvements in motor performances during dual tasks after NIBS (*Y* = 0.10 + 0.01*X*; *P* = 0.727). The metaregression analyses found no significant relationships between improvements in cognitive performances during dual tasks after NIBS and following demographic characteristics: (1) age (*Y* = − 9.13 + 0.14*X*; *P* = 0.052) (2), proportion of females in total patients with PD (*Y* = 0.80 − 1.77*X*; *P* = 0.075), and (3) duration since PD diagnosis (*Y* = 0.17 + 0.04*X*; *P* = 0.686).

## **Discussion**

This meta-analysis investigated effects of NIBS techniques including tDCS and rTMS on motor and cognitive performances during dual tasks in patients with PD. The findings revealed that NIBS protocols significantly enhanced motor and cognitive performances during dual tasks. Specifically, these improvements were observed when tDCS stimulated the DLPFC regions. Moreover, the meta-regression analyses revealed that greater improvements in motor performances during dual tasks after NIBS protocols were significantly associated with decreased age and increased proportion of females in patients with PD, respectively.

The meta-analytic findings demonstrated that tDCS protocols increasing DLPFC excitability improved motor performances during dual tasks in patients with PD. Successful walking in well-functioning people is typically based on the automaticity allowing the motor system to quickly and efficiently coordinate movements with minimal cognitive involvement [[54\]](#page-14-3). However, individuals with impaired automaticity such as older adults and patients with stroke may require more cognitive resources (e.g., executive control involving conscious processing of information for organizing, managing, and controlling movements) for executing gait performances [\[55,](#page-14-4) [56](#page-14-5)]. Several studies reported impaired automaticity during gait performances in patients with PD due to dopamine depletion in the posterior putamen, a sensorimotor region of the striatum that potentially acquires, stores, and facilitates automated motor skills [[18,](#page-13-10) [57](#page-14-6)–[59\]](#page-14-7). However, patients with PD who exhibited greater DLPFC excitability showed no significant impairments in normal gait performances as compared with those for age-matched controls [[20](#page-13-12)]. Given that the DLPFC is important for executive functions [[60\]](#page-14-8), these findings indicated that patients with PD may be dependent on executive control processing during normal locomotion to compensate for their impaired automaticity  $[61-63]$  $[61-63]$ . Importantly, dual tasks such as walking with subtraction or generating words normally increase cognitive workload [[64\]](#page-14-11). Perhaps, dual tasks for patients with PD may attenuate executive resources being applied to compensate for impaired automaticity consequently interfering with gait performances [[20](#page-13-12)]. A recent meta-analysis demonstrated that anodal tDCS on the DLPFC reduced dual-task cost on gait speed in older adults, suggesting that increasing DLPFC excitability may improve executive control associated with gait [[24](#page-13-15)]. Taken together, brain stimulation for facilitating DLPFC excitability may contribute to locomotion improvements during dual tasks in patients with PD by maintaining neural resource levels for executive control processing on gait.

In addition to improved motor performance, applying tDCS protocols targeting the DLPFC facilitated cognitive improvements during dual tasks in patients



<span id="page-7-0"></span>

Study	<b>Motor Performance</b>	<b>Cognitive Performance</b>	<b>Dual Task</b>
Broeder 2023	DTC-writing amplitude	<b>NA</b>	Writing figure-8 patterns while counting low and high tones
<b>Bueno 2023</b>	Speed, Cadence, Step length, Step width	<b>NA</b>	Walking while counting backwards by three
Chung 2020	<b>TUG</b>	<b>NA</b>	TUG test while counting backwards by three
Criminger 2018	<b>TUG</b>	<b>NA</b>	TUG test while carrying a full cup of water TUG test while counting backwards by three
Lench 2021	Time to turn	<b>NA</b>	TUG test while counting backwards by seven
Mishra 2021	Speed, DTC-speed	Number of correct generated words, DTC-number of cor- rect generated words	Walking while generating words starting from a given alphabet
Mishra 2022	TUG, DTC-TUG	words	Number of correct generated TUG test while generating words starting from a given alphabet
Putzolu 2018	DTC-speed, DTC-step length, DTC- double support time, DTC-stance time	<b>NA</b>	Walking while counting backwards by seven
Schabrun 2016	Speed, Cadence, Stride length, Double support time, TUG	Number of correct generated words, Number of correct backward counts	Walking while counting backwards by three Walking while generating words starting from a particular letter Walking while conversation TUG test while counting backwards by three TUG test while generating words starting from a particular letter
Swank 2016	TUG, DTC-TUG	Number of correct backward counts, DTC-number of cor- rect backward counts	TUG test while carrying a full cup of water TUG test while counting backwards by three
<b>Wong 2022</b>	Speed, Cadence, Stride length, Stride time, Stride length vari- ability, Stride time variability, DTC-speed	<b>NA</b>	Walking while counting backwards by three

<span id="page-8-0"></span>**Table 3** Specific motor and cognitive performances during dual tasks

Abbreviation. TUG=timed up and go; DTC=dual-task cost

<span id="page-8-1"></span>

**Fig. 2** Methodological quality assessment using Cochrane risk-of-bias tool

<span id="page-9-0"></span>

<b>Study Name</b>	<b>Outcome Measure (secondary task)</b>	<b>NIBS</b> (additional training)	<b>Targeted Brain Area</b>	<b>SMD</b>	LL	<b>UL</b>	P-value	SMD and 95% CI
	Schabrun 2016 Stride length (Counting)	tDCS (dual-task walking)	off: L-M1 (+)	$-1.250$	$-2.321$	$-0.179$	0.022	
	Schabrun 2016 Double support (Counting)	tDCS (dual-task walking)	off: L-M1 (+)	$-1.167$	$-2.227$	$-0.107$	0.031	Ð
	Schabrun 2016 Speed (Counting)	tDCS (dual-task walking)	off: L-M1 (+)	$-0.933$	$-1.965$	0.099	0.076	п
	Schabrun 2016 Double support (Generating words)	tDCS (dual-task walking)	off: L-M1 (+)	$-0.784$	$-1.801$	0.233	0 1 3 1	€
	Schabrun 2016 Stride length (Generating words)	tDCS (dual-task walking)	off: L-M1 (+)	$-0.728$	$-1.739$	0.284	0.159	г
<b>Wong 2022</b>	Stride time variability (Counting)	tDCS only	off: Cerebellum (+)	$-0.698$	$-1.650$	0.253	0.150	ο
	Schabrun 2016 Speed (Generating words)	tDCS (dual-task walking)	off: L-M1 (+)	$-0.692$	$-1.701$	0.317	0.179	⊓
<b>Wong 2022</b>	Stride length variability (Counting)	tDCS only	off: Cerebellum (+)	$-0.688$	$-1.639$	0.263	0.156	о
	Schabrun 2016 Cadence (Generating words)	tDCS (dual-task walking)	off: L-M1 (+)	$-0.668$	$-1.675$	0.339	0.193	o
	Schabrun 2016 Cadence (Counting)	tDCS (dual-task walking)	off: L-M1 (+)	$-0.533$	$-1.531$	0.464	0.294	o
Putzolu 2018	Non-FOG; DTC-step length (Counting)	tDCS only	off: L-DLPFC (+)	$-0.418$	$-1.304$	0.468	0.355	Ð
	Schabrun 2016 Speed (Conversation)	tDCS (dual-task walking)	off: L-M1 (+)	$-0.398$	$-1.388$	0.592	0.431	o
Putzolu 2018	Non-FOG; DTC-speed (Counting)	tDCS only	off: L-DLPFC (+)	$-0.373$	$-1.257$	0.511	0.408	Ð
<b>Wong 2022</b>	DTC-speed (Counting)	tDCS only	off: L-M1 (+)	$-0.280$	$-1.209$	0.648	0.554	Ð
<b>Wong 2022</b>	DTC-speed (Counting)	tDCS only	off: Cerebellum (+)	$-0.265$	$-1.193$	0.663	0.576	г
	Schabrun 2016 Stride length (Conversation)	tDCS (dual-task walking)	off: L-M1 (+)	$-0.243$	$-1.226$	0.741	0.629	г
	Schabrun 2016 TUG (Generating words)	tDCS (dual-task walking)	off: L-M1 (+)	$-0.190$	$-1.172$	0.792	0.704	г
	Criminger 2018 TUG (Counting)	tDCS (golf video game)	off: L-DLPFC (+), R-DLPFC (-)	$-0.188$	$-0.683$	0.306	0.455	⋒
	Schabrun 2016 TUG (Counting)	tDCS (dual-task walking)	off: L-M1 (+)	$-0.187$	$-1.169$	0.795	0.709	■
	Schabrun 2016 Cadence (Conversation)	tDCS (dual-task walking)	off: L-M1 (+)	$-0.176$	$-1.158$	0.805	0.725	г
	Schabrun 2016 Double support (Conversation)	tDCS (dual-task walking)	off: L-M1 (+)	$-0.167$	$-1,148$	0.815	0.739	г
<b>Lench 2021</b>	Time to turn (Counting)	rTMS (dual-task walking)	off: SMA (+)	$-0.160$	$-1.056$	0.736	0.726	∊
	Criminger 2018 TUG (Counting)	tDCS only	off: L-DLPFC (+), R-DLPFC (-)	$-0.063$	$-0.553$	0.428	0.802	- 89
Putzolu 2018	Non-FOG; DTC-double support time (Counting)	tDCS only	off: L-DLPFC (+)	$-0.047$	$-0.924$	0.829	0.916	
<b>Wong 2022</b>	Stride time (Counting)	tDCS only	off: Cerebellum (+)	$-0.033$	$-0.957$	0.891	0.944	
<b>Bueno 2023</b>	Step width (Counting)	tDCS (physical therapy)	off: $M1_{CZ}$ (+)	0.000	$-0.785$	0.785	1.000	
<b>Bueno 2023</b>	Cadence (Counting)	tDCS (physical therapy)	off: $M1_{c2} (+)$	0.032	$-0.752$	0.817	0.936	
	Criminger 2018 TUG (Counting)	tDCS (stationary bike)	off: L-DLPFC (+), R-DLPFC (-)	0.040	$-0.451$	0.530	0.874	
		tDCS (stationary bike)	off: L-DLPFC (+), R-DLPFC (-)	0.068	$-0.422$	0.559	0.785	
	Criminger 2018 TUG (Carrying a full cup of water)			0.080	$-0.359$	0.519	0.720	
Mishra 2022	DTC-TUG (Generating words)	tDCS only	on: L-DLPFC (+)					
<b>Bueno 2023</b>	Cadence (Counting)	tDCS (physical therapy)	off: M1 <sub>C3-C2-C4</sub> (+)	0.087	$-0.698$	0.872	0.828	
Mishra 2022	TUG (Generating words)	tDCS only	off: L-DLPFC (+)	0.094	$-0.346$	0.533 0.533	0.676 0.674	
Mishra 2022	TUG (Generating words)	tDCS only	on: $L-DLPFC (+)$	0.094	$-0.345$ $-0.383$	0.600	0.666	
	Criminger 2018 TUG (Carrying a full cup of water)	tDCS only	off: L-DLPFC (+), R-DLPFC (-)	0.108				
Swank 2016	DTC-TUG (Carrying a full cup of water)	tDCS only	off: L-DLPFC (+), R-DLPFC (-)	0.120	$-0.502$	0.742	0.705	
<b>Wong 2022</b>	Cadence (Counting)	tDCS only	off: $L-M1$ $(+)$	0.120	$-0.805$	1.045	0.799	
<b>Wong 2022</b>	Stride length variability (Counting)	tDCS only	off: L-M1 (+)	0.125	$-0.800$	1.050	0.791	
Chung 2020	<b>TUG</b> (Counting)	rTMS (treadmill walking)	1Hz: M1 (+)	0.129	$-0.555$	0.812	0.712	
Bueno 2023	Speed (Counting)	tDCS (physical therapy)	off: $M1_{CZ}(+)$	0.146	$-0.640$	0.932	0.716	
<b>Wong 2022</b>	Stride length variability (Counting)	tDCS only	off: L-DLPFC (+)	0.147	$-0.778$	1.073	0.755	
	Criminger 2018 TUG (Carrying a full cup of water)	tDCS (golf video game)	off: L-DLPFC (+), R-DLPFC (-)	0.186	$-0.308$	0.680	0.461	Æ
Mishra 2021	Speed (Generating words)	tDCS only	off: L-DLPFC (+)	0.207	$-0.236$	0.649	0.361	▬
Mishra 2022	DTC-TUG (Generating words)	tDCS only	off: L-DLPFC (+)	0.239	$-0.206$	0.683	0.292	▖
Putzolu 2018	Non-FOG; DTC-stance time (Counting)	tDCS only	off: L-DLPFC (+)	0.254	$-0.627$	1.134	0.572	
<b>Wong 2022</b>	Cadence (Counting)	tDCS only	off: Cerebellum (+)	0.254	$-0.673$	1.182	0.591	{
<b>Wong 2022</b>	Stride time (Counting)	tDCS only	off: $L-M1 (+)$	0.268	$-0.660$	1.196	0.571	▬
Mishra 2021	Speed (Generating words)	tDCS only	on: L-DLPFC (+)	0.285	$-0.162$	0.732	0.211	Ð
<b>Swank 2016</b>	TUG (Carrying a full cup of water)	tDCS only	off: L-DLPFC (+), R-DLPFC (-)	0.286	$-0.347$	0.918	0.376	⋒
<b>Wong 2022</b>	Stride time variability (Counting)	tDCS only	off: L-M1 (+)	0.292	$-0.637$	1.220	0.538	⋒
<b>Wong 2022</b>	DTC-speed (Counting)	tDCS only	off: L-DLPFC (+)	0.303	$-0.626$	1.233	0.522	
<b>Wong 2022</b>	Stride length (Counting)	tDCS only	off: L-M1 (+)	0.307	$-0.622$	1.236	0.517	Ð
Bueno 2023	Step width (Counting)	tDCS (physical therapy)	off: $M1_{C3.CZ.C4}$ (+)	0.333	$-0.457$	1.123	0.408	п
<b>Wong 2022</b>	Stride length (Counting)	tDCS only	off: Cerebellum (+)	0.336	$-0.595$	1.266	0.479	o
Mishra 2021	DTC-speed (Generating words)	tDCS only	off: L-DLPFC (+)	0.352	$-0.100$	0.804	0.127	o
<b>Wong 2022</b>	Speed (Counting)	tDCS only	off: L-M1 (+)	0.356	$-0.575$	1.287	0.454	▬
Chung 2020	TUG (Counting)	rTMS (treadmill walking)	25Hz: M1 (+)	0.394	$-0.296$	1.083	0.263	г
Mishra 2021	DTC-speed (Generating words)	tDCS only	on: L-DLPFC (+)	0.414	$-0.042$	0.871	0.075	€
Broeder 2023	DTC-writing amplitude (Counting low and high tones) tDCS (writing figure-8 patterns) off: L-M1 (+)			0.448	$-0.187$	1.084	0.167	
<b>Wong 2022</b>	Stride time variability (Counting)	tDCS only	off: L-DLPFC (+)	0.483	$-0.454$	1.420	0.312	
		tDCS only	off: L-DLPFC (+)	0.549	$-0.392$	1.490	0.253	■
<b>Wong 2022</b>	Stride length (Counting)			0.580	$-0.090$	1.250	0.090	
Swank 2016	TUG (Counting)	tDCS only	off: L-DLPFC (+), R-DLPFC (-)			1407	0 140	г
<b>Bueno 2023</b> Swank 2016	Step length (Counting) DTC-TUG (Counting)	tDCS (physical therapy) tDCS only	off: $M1_{CZ}$ (+) off: L-DLPFC (+), R-DLPFC (-)	0.604 0.693	$-0.198$ 0.003	1.383	0.049	п ▬
<b>Wong 2022</b>	Speed (Counting)	tDCS only	off: Cerebellum (+)	0.703	$-0.249$	1.655	0.148	π
<b>Wong 2022</b>	Speed (Counting)	tDCS only	off: L-DLPFC (+)	0.761	$-0.195$	1.718	0.119	п
<b>Wong 2022</b>	Cadence (Counting)	tDCS only	off: L-DLPFC (+)	0.773	$-0.185$	1.730	0.114	г
<b>Bueno 2023</b>	Speed (Counting)	tDCS (physical therapy)	off: M1 <sub>C3-CZ-C4</sub> (+)	0.828	0.010	1.645	0.047	Ð
<b>Wong 2022</b>	Stride time (Counting)	tDCS only	off: L-DLPFC (+)	1.075	0.087	2.064	0.033	€
Bueno 2023	Step length (Counting)	tDCS (physical therapy)	off: M1 <sub>C3-CZ-C4</sub> (+)	1.167	0.318	2.016	0.007	۰
Putzolu 2018	FOG; DTC-stance time (Counting)	tDCS only	off: L-DLPFC (+)	1.272	0.439	2.106	0.003	o
Putzolu 2018	FOG; DTC-step length (Counting)	tDCS only	off: L-DLPFC (+)	1.359	0.499	2.218	0.002	€
Putzolu 2018	FOG; DTC-double support time (Counting)	tDCS only	off: L-DLPFC (+)	1.512	0.605	2419	0.001	€
Putzolu 2018	FOG; DTC-speed (Counting)	tDCS only	off: L-DLPFC (+)	1.727	0.749	2.705	< 0.001	
			<b>Motor Performance Overall</b>	0.163	0.056	0.271	0.003	

Fig. 3 NIBS effects on motor performances during dual tasks. NIBS=non-invasive brain stimulation; tDCS=transcranial direct current stimulation; rTMS=repetitive transcranial magnetic stimulation; DLPFC=dorsolateral prefrontal cortex; M1=primary motor cortex; SMA=supplementary motor area; L=left; R=right; DTC=dual-task cost; FOG=freezing of gait; TUG=timed up and go

with PD. These findings indicate that increasing DLPFC excitability may enhance dual-task performance including both motor and cognitive tasks. Beneficial effects of NIBS protocols that targeted the DLPFC on dual-task performances appeared in healthy young adults and patients with stroke [[65](#page-14-12), [66\]](#page-14-13). DLPFC regions are typically associated with executive functions including shifting and inhibitory control [[67](#page-14-14), [68\]](#page-14-15). Furthermore, executive functions may be related to the ability to successfully perform dual tasks [[69\]](#page-14-16). For example, better shifting may decrease task-switch costs and inhibitory control may suppress inappropriate responses consequently contributing to efficient allocation of attention during dual tasks [[70\]](#page-14-17). Importantly, patients with PD often showed impaired executive functions because deficits in the striatal dopamine interfere with normal transmission of information through the frontostriatal circuits leading to dorsolateral frontal-lobe dysfunction [\[71,](#page-14-18) [72](#page-14-19)]. Thus, excitatory stimulation on the DLPFC may improve executive functions of patients with PD by increasing dopamine levels [[73–](#page-14-20)[77](#page-14-21)] via the meso-cortico-limbic pathway and local effects on the nigrostriatal pathway [\[78–](#page-14-22)[80\]](#page-14-23). In fact, patients with PD revealed lower functional connectivity patterns across cortico-subcortical areas including DLPFC, caudate, and motor networks [[81](#page-14-24),

<span id="page-10-0"></span>

<b>Study Name</b>	<b>Outcome Measure (secondary task)</b>	NIBS (additional training)	Targeted Brain Area	SMD	ᄔ	UL	P-value	SMD and 95% CI
Putzolu 2018	Non-FOG; DTC-step length (Counting)	tDCS only	off: L-DLPFC (+)	$-0.418$	$-1.304$	0.468	0.355	
Putzolu 2018	Non-FOG; DTC-speed (Counting)	tDCS only	off: L-DLPFC (+)	$-0.373$	$-1.257$	0.511	0.408	
	Criminger 2018 TUG (Counting)	tDCS (golf video game)	off: L-DLPFC (+), R-DLPFC (-)	$-0.188$	$-0.683$	0.306	0.455	
	Criminger 2018 TUG (Counting)	tDCS only	off: L-DLPFC (+), R-DLPFC (-)	$-0.063$	$-0.553$	0.428	0.802	
Putzolu 2018	Non-FOG; DTC-double support time (Counting) tDCS only		off: L-DLPFC (+)	$-0.047$	$-0.924$	0.829	0.916	
	Criminger 2018 TUG (Counting)	tDCS (stationary bike)	off: L-DLPFC (+), R-DLPFC (-)	0.040	$-0.451$	0.530	0.874	
	Criminger 2018 TUG (Carrying a full cup of water)	tDCS (stationary bike)	off: L-DLPFC (+), R-DLPFC (-)	0.068	$-0.422$	0.559	0.785	
Mishra 2022	DTC-TUG (Generating words)	tDCS only	on: L-DLPFC (+)	0.080	$-0.359$	0.519	0.720	
Mishra 2022	TUG (Generating words)	tDCS only	off: L-DLPFC (+)	0.094	$-0.346$	0.533	0.676	
Mishra 2022	TUG (Generating words)	tDCS only	on: L-DLPFC (+)	0.094	$-0.345$	0.533	0.674	
	Criminger 2018 TUG (Carrying a full cup of water)	tDCS only	off: L-DLPFC (+), R-DLPFC (-)	0.108	$-0.383$	0.600	0.666	
Swank 2016	DTC-TUG (Carrying a full cup of water)	tDCS only	off: L-DLPFC (+), R-DLPFC (-)	0.120	$-0.502$	0.742	0.705	
<b>Wong 2022</b>	Stride length variability (Counting)	tDCS only	off: L-DLPFC (+)	0.147	$-0.778$	1.073	0.755	
	Criminger 2018 TUG (Carrying a full cup of water)	tDCS (golf video game)	off: L-DLPFC (+), R-DLPFC (-)	0.186	$-0.308$	0.680	0.461	
Mishra 2021	Speed (Generating words)	tDCS only	off: L-DLPFC (+)	0.207	$-0.236$	0.649	0.361	
Mishra 2022	DTC-TUG (Generating words)	tDCS only	off: L-DLPFC (+)	0.239	$-0.206$	0.683	0.292	
Putzolu 2018	Non-FOG; DTC-stance time (Counting)	tDCS only	off: L-DLPFC (+)	0.254	$-0.627$	1.134	0.572	
Mishra 2021	Speed (Generating words)	tDCS only	on: L-DLPFC (+)	0.285	$-0.162$	0.732	0.211	
Swank 2016	TUG (Carrying a full cup of water)	tDCS only	off: L-DLPFC (+), R-DLPFC (-)	0.286	$-0.347$	0.918	0.376	
<b>Wong 2022</b>	DTC-speed (Counting)	tDCS only	off: L-DLPFC (+)	0.303	$-0.626$	1.233	0.522	
Mishra 2021	DTC-speed (Generating words)	tDCS only	off: L-DLPFC (+)	0.352	$-0.100$	0.804	0.127	
Mishra 2021	DTC-speed (Generating words)	tDCS only	on: L-DLPFC (+)	0.414	$-0.042$	0.871	0.075	
<b>Wong 2022</b>	Stride time variability (Counting)	tDCS only	off: L-DLPFC (+)	0.483	$-0.454$	1.420	0.312	
<b>Wong 2022</b>	Stride length (Counting)	tDCS only	off: L-DLPFC (+)	0.549	$-0.392$	1.490	0.253	
Swank 2016	<b>TUG</b> (Counting)	tDCS only	off: L-DLPFC (+), R-DLPFC (-)	0.580	$-0.090$	1.250	0.090	
<b>Swank 2016</b>	DTC-TUG (Counting)	tDCS only	off: L-DLPFC (+), R-DLPFC (-)	0.693	0.003	1.383	0.049	
<b>Wong 2022</b>	Speed (Counting)	tDCS only	off: L-DLPFC (+)	0.761	$-0.195$	1.718	0.119	
<b>Wong 2022</b>	Cadence (Counting)	tDCS only	off: L-DLPFC (+)	0.773	$-0.185$	1.730	0.114	
<b>Wong 2022</b>	Stride time (Counting)	tDCS only	off: L-DLPFC (+)	1.075	0.087	2.064	0.033	
Putzolu 2018	FOG; DTC-stance time (Counting)	tDCS only	off: L-DLPFC (+)	1.272	0.439	2.106	0.003	
Putzolu 2018	FOG; DTC-step length (Counting)	tDCS only	off: L-DLPFC (+)	1.359	0.499	2.218	0.002	
Putzolu 2018	FOG; DTC-double support time (Counting)	tDCS only	off: L-DLPFC (+)	1.512	0.605	2.419	0.001	
Putzolu 2018	FOG; DTC-speed (Counting)	tDCS only	off: L-DLPFC (+)	1.727	0.749	2.705	0.001	
			<b>Dorsolateral Prefrontal Cortex</b>	0.298	0.163	0.433	< 0.001	

Fig. 4 NIBS effects on motor performances during dual tasks based on stimulation site. NIBS=non-invasive brain stimulation; tDCS=transcranial direct current stimulation; DLPFC=dorsolateral prefrontal cortex; L=left; R=right; DTC=dual-task cost; FOG=freezing of gait; TUG=timed up and go

<span id="page-10-1"></span>

<b>Study Name</b>	Outcome Measure (secondary task) NIBS (additional training)		<b>Targeted Brain Area</b>	<b>SMD</b>	<b>LL</b>	<b>UL</b>	P-value	SMD and 95% CI
<b>Swank 2016</b>	Counting (TUG)	tDCS only	off: L-DLPFC (+), R-DLPFC (-)		$-0.130 -0.753 0.492$		0.682	
Mishra 2021	DTC-generating words (Gait)	tDCS only	off: $L-DLPFC (+)$		$-0.094$ $-0.533$ $0.346$		0.676	
Mishra 2021	DTC-generating words (Gait)	tDCS only	on: $L-DLPFC (+)$		0.138 -0.302 0.578		0.539	
	Schabrun 2016 Generating words (Gait)	tDCS (dual-task walking)	off: L-M1 (+)		0.205 -0.777 1.188		0.682	
Mishra 2021	Generating words (Gait)	tDCS only	on: $L$ -DLPFC $(+)$		0.277 -0.170 0.723		0.224	
Mishra 2021	Generating words (Gait)	tDCS only	off: $L-DLPFC (+)$		0.437 -0.021 0.896		0.062	
<b>Swank 2016</b>	DTC-counting (TUG)	tDCS only	off: L-DLPFC (+), R-DLPFC (-)		0.439 -0.210 1.088		0.185	
Mishra 2022	Generating words (TUG)	tDCS only	on: $L-DLPFC (+)$		0.525 0.057 0.992		0.028	
Mishra 2022	Generating words (TUG)	tDCS only	off: $L-DLPFC (+)$		0.650 0.168 1.133		0.008	
	Schabrun 2016 Counting (Gait)	tDCS (dual-task walking)	off: L-M1 (+)		0.880 -0.147 1.906		0.093	
	Schabrun 2016 Counting (TUG)	tDCS (dual-task walking)	off: L-M1 (+)		1.354 0.267 2.440		0.015	
	Schabrun 2016 Generating words (TUG)	tDCS (dual-task walking)	off: L-M1 (+)	1.386	0.294 2.477		0.013	
			Cognitive Performance Overall 0.375 0.161 0.590 0.001					

Fig. 5 NIBS effects on cognitive performances during dual tasks. NIBS=non-invasive brain stimulation; tDCS=transcranial direct current stimulation; DLPFC=dorsolateral prefrontal cortex; M1=primary motor cortex; L=left; R=right; DTC=dual-task cost; TUG=timed up and go

<span id="page-10-2"></span>

**Fig. 6** NIBS effects on cognitive performances during dual tasks based on stimulation site

NIBS=non-invasive brain stimulation; tDCS=transcranial direct current stimulation; DLPFC=dorsolateral prefrontal cortex; L=left; R=right; DTC=dualtask cost; TUG=timed up and go

[82\]](#page-14-25), whereas NIBS protocols upregulating DLPFC patterns increased functional connectivity across these areas [[83](#page-14-26), [84\]](#page-14-27). Taken together, given that patients with PD typically revealed both gait impairments as well as mild cognitive deficits [[85,](#page-14-28) [86\]](#page-14-29), applying NIBS for increasing DLPFC excitability may facilitate improvements in dual-task performances contributing to independent daily living.

Meta-regression analyses revealed that effects of NIBS on motor performances during dual tasks increased with lower age and greater proportion of females for patients with PD. Previous pharmacological studies argued that neuroplasticity facilitated by NIBS protocols may be related to the glutamatergic system [[87](#page-14-30)–[91](#page-14-31)]. Glutamate is the primary excitatory neurotransmitter allowing influx of  $Ca^{2+}$  associated with neuroplasticity via increased sensitivity of the synapse  $[92-94]$  $[92-94]$  $[92-94]$  $[92-94]$  $[92-94]$ . Given that aging normally decreases glutamatergic receptors and glutamate concentration in brain areas such as the frontal, parietal, and

<span id="page-11-0"></span>



**Fig. 7** NIBS effects on motor performances during dual tasks versus age (**A**) and female ratio (**B**). SMD=standardized mean difference

temporal cortical regions [\[95](#page-15-0), [96](#page-15-1)], positive effects of NIBS may be greater for younger patients with PD because of better brain neuroplasticity [\[97](#page-15-2)–[100\]](#page-15-3). Moreover, estrogen may protect dopaminergic neurons that presumably induce relatively lower symptom severity in women with PD than men  $[101-104]$  $[101-104]$  $[101-104]$ . Given that patients with PD who had lower symptom severity showed more neuroplasticity patterns facilitated by brain stimulation  $[105]$  $[105]$  $[105]$ , women with PD may receive greater therapeutic effects of NIBS protocols due to the neuroprotective effects of estrogen.

Although the current meta-analysis revealed potential effects of NIBS on dual-task performance in patients with PD, these findings should be cautiously interpreted. First, significant positive effects on both motor and cognitive performances during dual tasks were only observed in tDCS studies that targeting the DLPFC, and we found no rTMS studies. Given that potential neurophysiological changes may differ between tDCS and rTMS protocols [[106](#page-15-7), [107](#page-15-8)], our findings are still limited to tDCS effects. Thus, additional studies should determine whether rTMS protocols on the DLPFC improve dual-task performances in patients with PD. Importantly, improved cognitive performances during dual tasks after NIBS protocol are still tentative because of prior suggestion that at least five studies may be required for increasing validity of data synthesis [\[108\]](#page-15-9). Given that small number of studies may influence reliability of the results, more studies are necessary to determine positive effects of NIBS on cognitive function during dual tasks. In addition, seven out of 10 total studies focused on transient effects of NIBS by providing a single session of stimulation. Given that multiple sessions of NIBS protocols may result in cumulative effects [[109](#page-15-10), [110\]](#page-15-11), additional studies should investigate long-term effects of NIBS on dual-task performances in patients with PD by administering more sessions of stimulation. Finally, neurophysiological mechanisms underlying NIBS effects on dual-task performance in patients with PD are still inconclusive. Future studies using neuroimaging techniques should investigate how brain activation patterns are changed during and after different NIBS protocols for improving dual-task performance in patients with PD.

## **Conclusion**

This systematic review and meta-analysis found positive effects of NIBS on dual-task performances in patients with PD. Specifically, applying tDCS on the DLPFC effectively improved motor and cognitive performances during dual tasks. Furthermore, the metaregression analysis identified a significant relationship between greater improvements in motor performance during dual tasks after NIBS and younger age as well as a higher proportion of females in patients with PD. These findings suggest that NIBS protocols increasing DLPFC excitability may be a viable option for improving dual-task performance in patients with PD.

## **Abbreviations**



#### **Supplementary Information**

The online version contains supplementary material available at [https://doi.or](https://doi.org/10.1186/s12984-024-01505-8) [g/10.1186/s12984-024-01505-8](https://doi.org/10.1186/s12984-024-01505-8).

Supplementary Material 1

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#### **Author contributions**

Conceptualization: H.L.; Systematic review and meta-analysis: H.L.; Writing original draft: H.L. and B.J.C.; Writing—review and editing: N.K.; Supervision: N.K. All authors have read and agreed to the published version of the manuscript.

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#### **Data availability**

No datasets were generated or analysed during the current study.

## **Declarations**

#### **Ethics approval and consent to participate**

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**Consent for publication** Not applicable.

# **Competing interests**

The authors declare no competing interests.

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