

Analysis on the Propagation and Assembly of Metallic Nanoparticles through Subwavelength Apertures with Overlapping Electrical Double Layers

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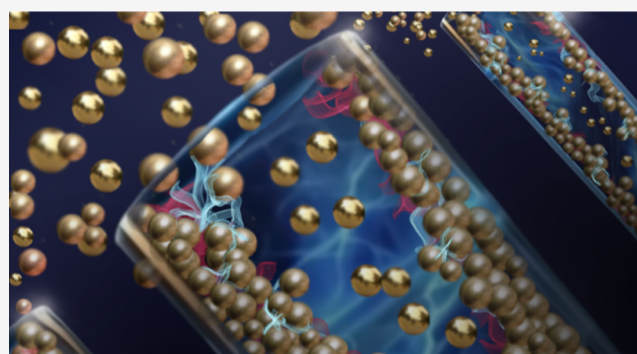
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ABSTRACT: Hybrid nanoplasmonic structures composed of subwavelength apertures in metallic films and nanoparticles have recently been demonstrated as ultrasensitive plasmonic sensors. This work investigates the electrokinetically driven propagation of the assembly mechanism of the metallic nanoparticles through nanoapertures. The Debye–Hückel approximation for a symmetric electrolyte solution with overlapping electrical double layers (EDLs) is used to obtain an analytical solution to the problem. The long-term silver nanoparticle concentration response is derived using the homogenization method and a multiscale analysis. The results indicate that uncharged nanoparticles will flow through the nanohole array if the nanochannel height is larger than the Debye length ($h_0 > \lambda_D$), while a trapping mechanism occurs, due to the overlapping of the EDL, when $h_0 \sim 3.8\lambda_D$. For charged nanoparticles, the response to the electric field occurs locally with the walls of the nanochannel, regardless of its height. For a critical value of the nanochannel length, the leading order of the concentration field becomes purely diffusive.



INTRODUCTION

Optofluidics, the emergent field arising from the synergistic combination of photonics and microfluidics, has enabled the development of ultracompact devices with applications in different fields, such as label-free sensing.¹ Ordered arrays subwavelength apertures, known as nanohole arrays (NHAs), have been demonstrated as nanoplasmonic sensors that can be fabricated with accurate periodicities and aperture shapes due to recent advances in nanofabrication techniques.² NHAs feature relatively long channels (in the order of 10^1 to 10^2 nm)^{3,4} with customizable pore sizes.^{5,6} These nanoapertures have been used for fluidic transport of considerably small volumes, and the enrichment of electrocharged analytes results in improved sensor response^{7–12} and controllable nano-injection across the nanostructured substrate. Unlike microfluidics, nanofluidics involve nanostructures where the solid boundaries are extremely close, and overlapping of electrical double layers (EDLs) is possible,¹³ which invalidates the use of Boltzmann distribution for ionic charge density.

Recent studies have presented analytical models for overlapped EDLs. Qu and Li¹⁴ derived a model to determine the electrical potential and ionic concentration distributions between two infinitely large flat plates, establishing corrected boundary conditions for these distributions. Golovnev and Trimper¹⁵ obtained an analytical solution for the Poisson–

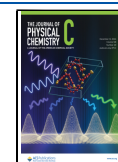
Nernst–Planck equation when Faradaic processes are discarded, revealing different ion concentration behaviors in both the short- and the long-time regimes. Zachariah et al.¹⁶ analyzed the repulsive forces that appear during the collapse of the EDLs using the DLVO theory, concluding that the hydration force is due to multiple layering of hydrate ions, which subsequently undergo transitions between different confined adsorbed ion states. Such a case occurs when a microchannel is connected to a nanochannel, and a micro–nano interface is formed, leading to charge transport and ion concentration polarization (ICP).¹⁷ ICP enables the enrichment of charged particles, such as biomarkers and ions, as well as rectification effects on ionic current.^{18,19} In this regard, Mani et al.²⁰ and Yaroshchuk and Bondarenko²¹ established transport analytical models considering the area average for ICP, with emphasis on the dominance of axial diffusion in determining the extent of diffuse layers at micro-to-nanochannel interfaces when the ion reservoir is large. In the

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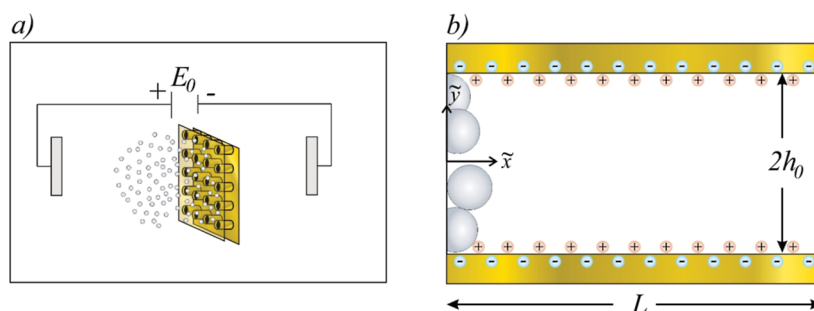


Figure 1. (a) Schematic representation of the microfluidic chip assembly connected to a DC source containing multiple silver nanoparticles and an NHA embedded in a gold film. (b) Close-up view of a nanohole from the NHA where silver nanoparticles respond to the induced electrical potential in the overlapped EDL.

context of sensing, the transport and placement of metallic nanoparticles within and around NHAs to construct hybrid nanoplasmonic structures with improved sensitivity have been demonstrated experimentally.^{11,22,23} However, the reported analytical work has focused on ionic concentration and does not address the transport scenarios with charged colloidal systems.

In this work, we investigate the role of the EDL overlapping on both charged and uncharged metallic nanoparticles in nanoconfinement using an analytical approach. The analysis is focused on the creation of hybrid nanostructures as surface-enhanced Raman scattering (SERS) substrates, as previously reported experimentally.¹¹ The investigation involves flow-through metallic nanoapertures that support surface plasmon resonance and metallic nanoparticles that naturally exhibit localized surface plasmon resonance, within a microfluidic environment under an applied electric field. We analyze the significance of the field distribution and the influence of the overlapping EDL on it, elucidating the critical impact of some parameters leading to novel perspectives on the physics of nanoparticle transport.

■ HYDRODYNAMIC FORMULATION

The system used in this study encompasses a microfluidic chip assembly with an embedded metallic NHA under the influence of a direct current (DC) electric field applied externally, as shown in Figure 1a. A Newtonian fluid is assumed to contain small ions (average size ~ 1 Å) and large silver nanoparticles (Ag NPs), flowing through an NHA. Both the ionic and Ag NP concentrations are initially uniform throughout the system. An electroosmotic flow (EF) emerges from an externally imposed electric field \vec{E} and the induced field in the EDL. The imposed external field yields the transference of electrons to particles, resulting in the acquisition of a net negative surface electric charge. Some particles may undergo polarization while retaining their electrical neutrality; in this manner, consideration of both charged and uncharged nanoparticles in the present analysis is warranted. Figure 1b depicts a cross-sectional view of a single nanohole within the NHA. Notably, silver nanoparticles exhibit a distinct Gaussian distribution concentration close to the nanohole's entrance, a phenomenon attributed to the localized enhancement of the electric field.⁸ The effect of the electric field gradient at the rim of the nanoholes on both the ions and the Ag NPs is of particular interest for producing hybrid nanostructures that enable SERS. This system, along with the assumption of NHA axis symmetry regarding electrokinetic phenomena, is the main domain for the analytical solution presented in this work. The nanohole is

modeled as an isothermal flat nanochannel of height h_0 and length L . A 2D Cartesian system of coordinates (\tilde{x}, \tilde{y}) is adopted at the nanochannel left inlet, where \cdot indicates that the variable has dimensional units. The extension of the model to cylindrical coordinates is trivial, as reported by Pennathur and Santiago.³

Governing Equations. The governing equations that serve as a starting point to investigate the EF in this study are the continuity equation

$$\nabla \cdot \tilde{\mathbf{u}} = 0 \quad (1)$$

and the Navier–Stokes equations

$$\rho_m \left[\frac{\partial \tilde{\mathbf{u}}}{\partial \tilde{t}} + (\tilde{\mathbf{u}} \cdot \nabla) \tilde{\mathbf{u}} \right] = -\nabla \tilde{P} + \nabla \cdot \tilde{\boldsymbol{\tau}} - \rho_e \nabla \tilde{\Phi} \quad (2)$$

where ρ_m is the fluid density, considered constant, $\tilde{\mathbf{u}} = (\tilde{u}, \tilde{v})$ is the velocity vector, \tilde{t} is the time, \tilde{P} is the pressure, ∇ is the Nabla operator defined as $\nabla \equiv (\partial/\partial \tilde{x}, \partial/\partial \tilde{y})$, and $\tilde{\boldsymbol{\tau}}$ is the stress tensor for a Newtonian fluid, given by

$$\tilde{\boldsymbol{\tau}} = \mu(\nabla \tilde{\mathbf{u}} + \nabla \tilde{\mathbf{u}}^T) \quad (3)$$

where μ is the dynamic viscosity of the fluid. The hydrodynamic boundary conditions related to the impermeability and no-slip condition at the walls are given by

$$\tilde{\mathbf{u}} \cdot \mathbf{n} = 0 \quad (4)$$

and

$$\tilde{\mathbf{u}} - (\tilde{\mathbf{u}} \cdot \mathbf{n}) \mathbf{n} = 0 \quad (5)$$

respectively. \mathbf{n} represents the unit vector normal to the microelectrode surface pointing toward the fluid. The pressure is \tilde{P}_0 at $\tilde{x} = 0, L$. The electrical body force in eq 2 consists of the electric charge density ρ_e and the total electrical potential $\tilde{\Phi}$, which is governed by Poisson's equation

$$\nabla^2 \tilde{\Phi} = -\frac{\rho_e}{\epsilon_m} \quad (6)$$

where ϵ_m denotes the dielectric permittivity of the medium. Here, $\tilde{\Phi}$ is split into the induced nonuniform equilibrium potential in the EDL, $\tilde{\psi}(\tilde{y})$, and the potential describing the external electric field $\gamma(\tilde{x}) = -\tilde{x}E_x$, where $E_x = \phi_0/L$ and ϕ_0 is the voltage provided by the generator. The boundary condition for $\tilde{\psi}$ at the walls is $\tilde{\psi} = \zeta$, where ζ is the zeta potential. The electrical charge density ρ_e is proportional to the local concentration difference between the cations and anions. For

a symmetric (z/z) electrolyte solution, the charge density can be defined as

$$\rho_e = ze(\tilde{n}_+ - \tilde{n}_-) \quad (7)$$

where z is the valence of the electrolyte, e represents the fundamental charge of an electron, and \tilde{n}_\pm represents the concentration of cations and anions, respectively. Transport of ions in a dilute solution is described by the Nernst–Planck equation²⁴

$$\frac{\partial \tilde{n}_\pm}{\partial \tilde{t}} = -\nabla \cdot \left(\mp \tilde{n}_\pm \frac{D_i z e}{k_B T} \nabla \tilde{\Phi} - D_i \nabla \tilde{n}_\pm - \tilde{\mathbf{u}} \tilde{n}_\pm \right) \quad (8)$$

where D_i is the diffusion coefficient of the ions, k_B is the Boltzmann constant, and T is the absolute temperature. Equation 8 is subject to the following boundary conditions¹⁴

$$\tilde{n}_+ = \tilde{n}_+^c \text{ and } \tilde{n}_- = \tilde{n}_-^c \text{ at } \tilde{y} = 0 \quad (9)$$

The concentration field \tilde{c} of the diffusing charged NPs is governed by the convective diffusion equation²⁵

$$\frac{\partial \tilde{c}}{\partial \tilde{t}} + \tilde{\mathbf{u}} \cdot \nabla \tilde{c} = D \nabla^2 \tilde{c} + \frac{Dze}{k_B T} \nabla \tilde{\Phi} \cdot \nabla \tilde{c} \quad (10)$$

where the molecular diffusion coefficient of nanoparticles, denoted as D , is determined through the Stokes–Einstein equation²⁶

$$D = \frac{k_B T}{6\pi\mu R_p} \quad (11)$$

where R_p is the hydrodynamic radius of the nanoparticles. In eq 10, the second right-hand term corresponds to an electromigration phenomenon, which consists of nanoparticle motion under the influence of Coulomb force. The Coulomb force appears between the gradient of the total electrical potential and the electrically charged NPs. Therefore, this term should only be considered for charged NPs. The boundary and initial conditions associated with eq 10 are

$$D \frac{\partial \tilde{c}}{\partial \tilde{y}} + \tilde{\beta} \tilde{c} = 0 \text{ at } \tilde{y} = \pm h_0 \quad (12)$$

$$\frac{\partial \tilde{c}}{\partial \tilde{x}} = 0 \text{ at } \tilde{x} = 0, L \quad (13)$$

$$\tilde{c} = C^* f(\tilde{x}) \text{ at } \tilde{t} = 0 \quad (14)$$

where $\tilde{\beta}$ is the rate of disappearance of NPs due to an irreversible first-order reaction between the solution and the walls,²⁷ C^* is the initial concentration of NPs, $f(\tilde{x}) = \exp[-(\tilde{x}/aL)^2]$, and a is a constant. In boundary conditions 12 we consider two cases: (i) the nonpenetration boundary for uncharged nanoparticles and (ii) the so-called perfect-sink model for charged nanoparticles. The nonpenetration boundary is obtained when $\tilde{\beta} = 0$, which specifies that there is no penetration of the particles at the boundary, ensuring that any change in concentration at the wall is solely due to diffusion and not advection.²⁸ The boundary acting as a perfect sink, which is used in theories of diffusion of charged particles,²⁹ is obtained when $\tilde{\beta} \gg h_0/D$. This model assumes that all particles arriving at the wall will be irreversibly adsorbed immediately and subsequently disappear from the system.³⁰

Nondimensional Mathematical Model. The governing equations together with their corresponding boundary conditions can be written in a nondimensional form by introducing the dimensionless variables $x = \tilde{x}/L$, $y = \tilde{y}/h_0$, $u = \tilde{u}/U_c$, $v = \tilde{v}/h_0 U_c$, $t = \tilde{t} D/L\lambda_D$, $p' = (\tilde{P} - \tilde{P}_0)h_0^2/U_c \mu L$, $\tau = \tilde{\tau} h_0/U_c \mu$, $\psi = \tilde{\psi}/\zeta$, $\Phi = \tilde{\Phi}/\phi_0$, $n_\pm = \tilde{n}_\pm/n_\infty$, and $c = \tilde{c}/C^*$. Here, $U_c = \epsilon_m \zeta^2/\mu L$ is the characteristic velocity,³¹ $t_c = L\lambda_D/D$ is the harmonic time,³² $\lambda_D = (\epsilon_m k_B T/2z^2 e^2 n_\infty)^{1/2}$ is the Debye length, and n_∞ is the ionic number in the concentration in the bulk solution. When defining the nondimensional pressure p' , we have introduced the useful definition $P = p' - (1/2)(d\psi/dy)^2$ introduced by Ajdari,³³ which serves to eliminate the electric terms in the momentum equation in the y direction. Therefore, the expanded nondimensional forms of the hydrodynamic, electric, and concentration governing eqs 1–3, 6–8, and 10 are as follows

$$\frac{\partial u}{\partial x} + \frac{\partial v}{\partial y} = 0 \quad (15)$$

$$\begin{aligned} Re\eta \left(\frac{1}{Pe} \frac{\partial u}{\partial t} + u \frac{\partial u}{\partial x} + v \frac{\partial u}{\partial y} \right) \\ = -\frac{\partial P}{\partial x} + \epsilon^2 k^2 \frac{\partial^2 u}{\partial x^2} + \frac{\partial^2 u}{\partial y^2} + \frac{1}{\alpha} \frac{d^2 \psi}{dy^2} \end{aligned} \quad (16)$$

$$\begin{aligned} Re\eta^3 \left(\frac{1}{Pe} \frac{\partial v}{\partial t} + u \frac{\partial v}{\partial x} + v \frac{\partial v}{\partial y} \right) \\ = -\frac{\partial P}{\partial y} + \epsilon^4 k^4 \frac{\partial^2 v}{\partial x^2} + \epsilon^2 k^2 \frac{\partial^2 v}{\partial y^2} \end{aligned} \quad (17)$$

$$\frac{d^2 \psi}{dy^2} = \frac{k^2}{2\delta} (n_+ - n_-) \quad (18)$$

$$\begin{aligned} -\epsilon D_T \frac{\partial n_\pm}{\partial t} = \frac{\partial}{\partial x} \left[\epsilon^2 \left(\pm \frac{\delta}{\alpha} n_\pm - \frac{\partial n_\pm}{\partial x} \right) - \epsilon D_T Pe (un_\pm) \right] \\ + \frac{\partial}{\partial y} \left[\frac{1}{k^2} \left(\pm \delta n_\pm \frac{d\psi}{dy} - \frac{\partial n_\pm}{\partial y} \right) - \epsilon D_T Pe (vn_\pm) \right] \end{aligned} \quad (19)$$

$$\begin{aligned} \epsilon k^2 \left[\frac{\partial c}{\partial t} + Pe \left(u \frac{\partial c}{\partial x} + v \frac{\partial c}{\partial y} \right) \right] \\ = \frac{\partial^2 c}{\partial y^2} + \frac{d\psi}{dy} \frac{\partial c}{\partial y} + \epsilon^2 k^2 \left(\frac{\partial^2 c}{\partial x^2} + \frac{1}{\alpha} \frac{\partial c}{\partial x} \right) \end{aligned} \quad (20)$$

In eqs 15–20, $\epsilon = \lambda_D/L$, $\eta = h_0/L$, $k = h_0/\lambda_D$, $\alpha = -\zeta/\phi_0$, $\delta = -\zeta ze/k_B T$, $D_T = D/D_i$, $Pe = U_c \lambda_D/D$ is the Péclet number, and $Re = \rho_m U_c h_0/\mu$ is the Reynolds numbers. The dimensionless boundary conditions of eqs 15–20 are

$$u = v = 0 \text{ at } y = \pm 1 \quad (21)$$

$$P = 0 \text{ at } x = 0, 1 \quad (22)$$

$$\psi = 1 \text{ at } y = \pm 1 \quad (23)$$

$$n_+ = \frac{\tilde{n}_+^c}{n_\infty} \text{ and } n_- = \frac{\tilde{n}_-^c}{n_\infty} \text{ at } y = 0 \quad (24)$$

$$\frac{\partial c}{\partial y} + \beta c = 0 \text{ at } y = \pm 1 \quad (25)$$

$$\frac{\partial c}{\partial x} = 0 \text{ at } x = 0, 1 \quad (26)$$

and

$$c = f(x) \text{ at } t = 0 \quad (27)$$

where

$$f(x) = \exp\left[-\left(\frac{x}{a}\right)^2\right] \quad (28)$$

and $\beta = \tilde{\beta}h_0/D$. In conditions 22, the induced potential gradient is zero at $x = 0, 1$ due to symmetry. In nanofluidic systems, typical values of the parameters ϵ , D_T , and Re are very small ($\lambda_D = 10$ nm, $L = 200$ nm, $D_i = 10^{-9}$ m²/s, $D = 8.5844 \times 10^{-12}$ m²/s, $U_c = 0.002$ m/s, $\epsilon = 0.05$, $D_T = 10^{-3}$, and $Re = 2.5 \times 10^{-4}$), while $\eta < 1$ ($\eta = 0.5$). Therefore, a simplified version of the nondimensional governing equations, as well as a regular perturbation technique,³⁴ can be used to solve the set of mentioned equations for small values of the parameter ϵ . Thus, a regular expansion is proposed for each dependent variable (say, X) in the following form

$$X = X_0 + \epsilon X_1 + O(\epsilon^2) \quad (29)$$

where $X = u, v, P, \psi$. Substituting the expansion eq 29 into the nondimensional governing eqs 15–19, and collecting terms of $O(1)$, we obtain the following problems

$$\frac{\partial u_0}{\partial x} + \frac{\partial v_0}{\partial y} = 0 \quad (30)$$

$$\frac{\partial^2 u_0}{\partial y^2} = \frac{\partial P_0}{\partial x} - \frac{1}{\alpha} \frac{d^2 \psi_0}{dy^2} \quad (31)$$

$$\frac{\partial P_0}{\partial y} = 0 \quad (32)$$

$$\frac{d^2 \psi_0}{dy^2} = \frac{k^2}{2\delta} (n_{0,+} - n_{0,-}) \quad (33)$$

$$\frac{1}{n_{0,\pm}} \frac{dn_{0,\pm}}{dy} = \pm \delta \frac{d\psi_0}{dy} \quad (34)$$

From eq 32, $P_0 = P_0(x)$ should be determined as a part of the hydrodynamics problem together with u_0 and v_0 . The solution of Nernst–Planck eq 34 is given by¹⁴

$$n_{0,+} = \exp\left[\delta\left(\psi_0 - \frac{\psi_c}{\zeta}\right)\right] \quad (35)$$

and

$$n_{0,-} = \exp\left[-\delta\left(\psi_0 - \frac{\psi_c}{\zeta}\right)\right] \quad (36)$$

where ψ_c is the unknown electrical potential at the center of the nanochannel. In eqs 35 and 36 it is assumed that the concentrations of cations and anions at the center are the same ($n_{0,+} = n_{0,-} = 1$ at $y = 0$). Further applying the Debye–Hückel approximation yields

$$n_{0,+} = 1 + \delta\left(\psi_0 - \frac{\psi_c}{\zeta}\right) \quad (37)$$

and

$$n_{0,-} = 1 - \delta\left(\psi_0 - \frac{\psi_c}{\zeta}\right) \quad (38)$$

Substituting eqs 37 and 38 in 33 returns

$$\frac{d^2 \psi_0}{dy^2} = k^2\left(\psi_0 - \frac{\psi_c}{\zeta}\right) \quad (39)$$

The $O(1)$ solution of Poisson eq 39, considering the boundary conditions [eq 23], is given by

$$\psi_0 = \frac{\psi_c}{\zeta} + \left(1 - \frac{\psi_c}{\zeta}\right) \frac{\cosh(ky)}{\cosh(k)} \quad (40)$$

To recover the Boltzmann equation ($\psi = 0$ at $y = 0$ and $k \gg 1$), we have assumed that $\psi_c = \zeta/k$, obtaining the following simplification

$$\psi_0 = \frac{1}{k} + \left(\frac{k-1}{k}\right) \frac{\cosh(ky)}{\cosh(k)} \quad (41)$$

The general hydrodynamic solution of eq 31 is obtained by substituting eq 41 in the momentum equation and integrating the result twice with respect to y ; considering eq 21 as the boundary condition, we obtain that the velocity profile in the lowest order is given as

$$u_0 = \frac{dP_0}{dx}(y^2 - 1) + \frac{1}{\alpha}(1 - \psi_0) \quad (42)$$

In the above equation, the pressure gradient is unknown and can be obtained using the continuity equation, eq 30. The suggested procedure is to substitute eqs 42 into 30, obtaining a solution for v_0 and P_0 . However, one should find that the leading order for the variables v_0 and P_0 is zero. Therefore, the above physically means that there are no induced pressure terms in this order and that the velocity field is hydrodynamically developed. Therefore, substituting eqs 41 in 42 yields

$$u_0 = \frac{1}{\alpha} \left[1 - \left(\frac{k-1}{k}\right) \frac{\cosh(ky)}{\cosh(k)} - \frac{1}{k} \right] \quad (43)$$

The next step is to assess the $O(\epsilon)$ solutions for ψ_1 , u_1 , v_1 , and P_1 . In this order, the ion concentration does not get affected by convection, thus making the $O(\epsilon)$ Poisson equation to yield $\psi_1 = 0$, leading to $u_1 = v_1 = P_1 = 0$ due to its role as the primary force in the momentum equations.

Homogenization Method. To obtain an analytical solution for the concentration field of Ag NPs, the homogenization method³⁵ is proposed to derive an expression that allows us to solve the convective diffusion equation. Thus, three distinct time scales are involved in the analysis of Ag NPs, which are as follows: the harmonic time,³² $t_0 \sim L\lambda_D/D$, the transverse diffusion time, $t_1 \sim 4h_0^2/D$, and the longitudinal diffusion time, $t_2 \sim L^2/D$.

From typical values of the previous times ($L = 200$ nm, $h_0 = 100$ nm, $t_0 = 2 \times 10^{-4}$ s, and $t_1 = t_2 = 4 \times 10^{-3}$ s), the following two time scales can be introduced

$$t_0 = t, \quad t_1 = t_2 = \epsilon t \quad (44)$$

and using eq 29 to expand for the dimensionless concentration

$$c = c_0 + \epsilon c_1 + \epsilon^2 c_2 + O(\epsilon^2) \quad (45)$$

where $c_j = c_j(x, y, t_0, t_2)$ and $j = 0, 1, 2$. The original time derivate becomes, according to the chain rule

$$\frac{\partial}{\partial t} \rightarrow \frac{\partial}{\partial t_0} + \epsilon \frac{\partial}{\partial t_2} \quad (46)$$

Substituting eqs 45 and 46 in 20 yields

$$\begin{aligned} \epsilon k^2 \left[\left(\frac{\partial}{\partial t_0} + \epsilon \frac{\partial}{\partial t_2} \right) (c_0 + \epsilon c_1) + Pe u_0 \frac{\partial (c_0 + \epsilon c_1)}{\partial x} \right] \\ = \epsilon^2 k^2 \frac{\partial^2 c_0}{\partial x^2} + \frac{\partial^2 (c_0 + \epsilon c_1 + \epsilon^2 c_2)}{\partial y^2} + \frac{\epsilon^2 k^2}{\alpha} \frac{\partial c_0}{\partial x} \\ + \frac{d\psi_0}{dy} \frac{\partial (c_0 + \epsilon c_1 + \epsilon^2 c_2)}{\partial y} \end{aligned} \quad (47)$$

At order $O(1)$, the governing equation is given by

$$\frac{\partial^2 c_0}{\partial y^2} + \frac{d\psi_0}{dy} \frac{\partial c_0}{\partial y} = 0 \quad (48)$$

To obtain a solution for eq 48, we consider two cases: uncharged nanoparticles, which neglect the electromigration term (second left-hand term) in eq 48, and charged nanoparticles. In addition, both cases must satisfy the following boundary condition due to the symmetry of the nanochannel

$$\frac{\partial c_0}{\partial y} = 0 \text{ at } y = 0 \quad (49)$$

In both cases, the solution at $O(1)$ is $c_0 = C_x(x, t_0, t_2)$. The procedure that determines the function C_x is given in the lines below. Taking the $O(\epsilon)$ from eq 47 yields the governing equation for c_1

$$k^2 \left(\frac{\partial C_x}{\partial t_0} + Pe u_0 \frac{\partial C_x}{\partial x} \right) = \frac{\partial^2 c_1}{\partial y^2} + \frac{d\psi_0}{dy} \frac{\partial c_1}{\partial y} \quad (50)$$

The next step is to take the cross-sectional average of eq 50, defined as $\bar{f} = \frac{1}{2} \int_{-1}^1 f dy$ for any function f , where \cdot will indicate the averaged function. In this context, the first right-hand term in eq 50 becomes zero as a consequence of its symmetry with respect to the y -axis, which is known from the inflection point at $y = 0$ [eq 49]. Similarly, the second right-hand term becomes zero due to the product of two odd functions. Thus, the cross-sectional average of eq 50 is

$$\frac{\partial C_x}{\partial t_0} + Pe \bar{u}_0 \frac{\partial C_x}{\partial x} = 0 \quad (51)$$

where

$$\bar{u}_0 = \frac{1}{2} \int_{y=-1}^{y=1} u_0 dy = \frac{1}{\alpha} \left[1 - \left(\frac{k-1}{k^2} \right) \tanh(k) - \frac{1}{k} \right] \quad (52)$$

Substituting eqs 51 into 50 yields

$$\frac{\partial^2 c_1}{\partial y^2} + \frac{d\psi_0}{dy} \frac{\partial c_1}{\partial y} = k^2 Pe (u_0 - \bar{u}_0) \frac{\partial C_x}{\partial x} \quad (53)$$

Considering the linearity of eq 53, the solution c_1 can be expressed as

$$c_1 = k^2 Pe \frac{\partial C_x}{\partial x} B(y) \quad (54)$$

and its substitution in eq 53 leads to a second-order ordinary differential equation for $B(y)$ as follows

$$\frac{d^2 B}{dy^2} + \frac{d\psi_0}{dy} \frac{dB}{dy} = u_0 - \bar{u}_0 \quad (55)$$

where

$$u_0 - \bar{u}_0 = \frac{k-1}{\alpha k \cosh(k)} \left[\frac{\sinh(k)}{k} - \cosh(ky) \right] \quad (56)$$

First, eq 55 is solved for uncharged nanoparticles using boundary condition 25 considering $\beta = 0$ as follows

$$\frac{dB}{dy} = 0 \text{ at } y = \pm 1 \quad (57)$$

Solving eq 55 for uncharged NPs, neglecting the electromigration term (second left-hand term) in eq 55, yields

$$B = \frac{k-1}{\alpha k^3 \cosh(k)} \left[\frac{y^2}{2} k \sinh(k) - \cosh(ky) \right] \quad (58)$$

For charged nanoparticles ($\beta \gg 1$), eq 55 was solved using the fourth-order Runge–Kutta method with the aid of the shooting approach together with the following boundary condition [eq 25]

$$B = 0 \text{ at } y = \pm 1 \quad (59)$$

The $O(\epsilon^2)$ from eq 47 is given by

$$\begin{aligned} k^2 \left(\frac{\partial c_1}{\partial t_0} + \frac{\partial C_x}{\partial t_2} + Pe u_0 \frac{\partial c_1}{\partial x} \right) \\ = k^2 \left(\frac{\partial^2 C_x}{\partial x^2} + \frac{1}{\alpha} \frac{\partial C_x}{\partial x} \right) + \frac{\partial^2 c_2}{\partial y^2} + \frac{d\psi_0}{dy} \frac{\partial c_2}{\partial y} \end{aligned} \quad (60)$$

Substituting eqs 51 and 54 in 60 returns

$$\begin{aligned} k^2 \left\{ \frac{\partial C_x}{\partial t_2} - \frac{\partial^2 C_x}{\partial x^2} [1 - k^2 Pe^2 (u_0 - \bar{u}_0)] - \frac{1}{\alpha} \frac{\partial C_x}{\partial x} \right\} \\ = \frac{\partial^2 c_2}{\partial y^2} + \frac{d\psi_0}{dy} \frac{\partial c_2}{\partial y} \end{aligned} \quad (61)$$

Taking the cross-sectional average of eq 61, the following governing equation is obtained

$$\frac{\partial C_x}{\partial t_2} = \mathcal{D} \frac{\partial^2 C_x}{\partial x^2} + \frac{1}{\alpha} \frac{\partial C_x}{\partial x} \quad (62)$$

where

$$\mathcal{D} = 1 - \frac{k^2 Pe^2}{2} \int_{y=-1}^{y=1} B(u_0 - \bar{u}_0) dy \quad (63)$$

For uncharged nanoparticles, \mathcal{D} was calculated by substituting eqs 56 and 58 in 63, obtaining the following equation

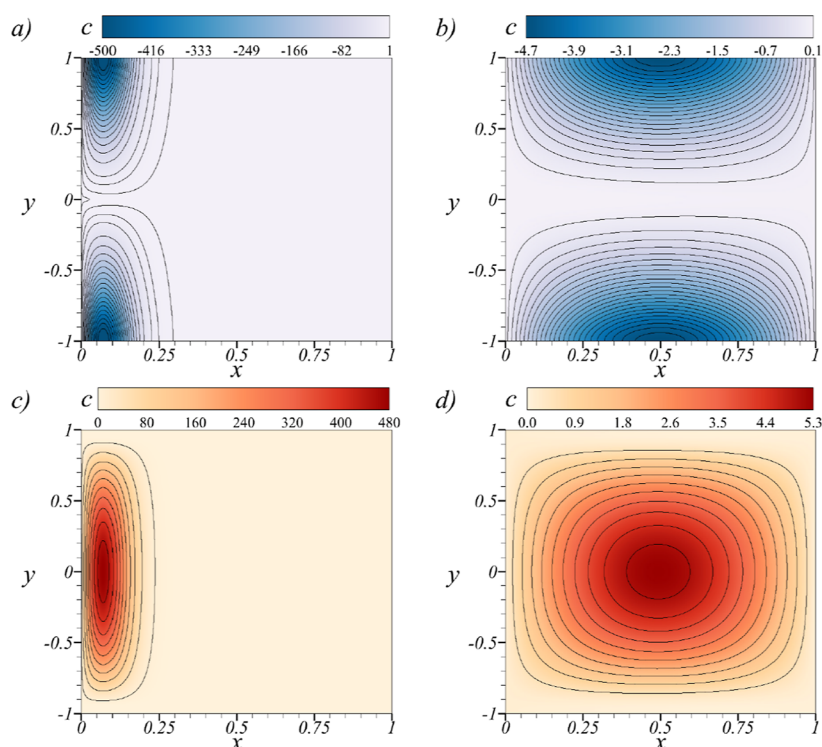


Figure 2. Nondimensional concentration field c for uncharged nanoparticles at $k = 10$, evaluated at the nondimensional time (a) $t = 0$ and (b) $t = 10^{-5}$. Nondimensional concentration field c for charged nanoparticles at $k = 10$ and (c) $t = 0$ and (d) $t = 10^{-5}$.

$$\mathcal{D} = 1 - \left[\frac{Pe(k-1)}{ak \cosh(k)} \right]^2 \left[\frac{1}{2} + \frac{\sinh(2k)}{4k} + \frac{\sinh(k) \cosh(k)}{k} - \sinh(k)^2 \left(\frac{1}{3} + \frac{2}{k^2} \right) \right] \quad (64)$$

For charged nanoparticles, \mathcal{D} was calculated by using numerical methods. Finally, eq 51 is added to 62, where the artifact of two times is no longer needed and can be removed³⁵

$$\frac{\partial C_x}{\partial t} = -\mathcal{A} \frac{\partial C_x}{\partial x} + \mathcal{D} \frac{\partial^2 C_x}{\partial x^2} \quad (65)$$

where

$$\mathcal{A} = Pe \bar{u}_0 - \frac{1}{\alpha} \quad (66)$$

The second right-hand term in eq 66 is part of electromigration and should only be considered for charged nanoparticles. First, we propose a solution for C_x that eliminates the convective term in eq 65, i.e., the first right-hand term, as follows

$$C_x = \exp \left[\frac{\mathcal{A}}{2\mathcal{D}} \left(x - \frac{\mathcal{A}t}{2} \right) \right] w(x, t) \quad (67)$$

Substituting eqs 67 into 65 yields

$$\frac{\partial w}{\partial t} = \mathcal{D} \frac{\partial^2 w}{\partial x^2} \quad (68)$$

The initial and boundary conditions of eq 68 are taken from eqs 26–28 as follows

$$\frac{\partial w}{\partial x} = 0 \text{ at } x = 0, 1 \quad (69)$$

and

$$C_x = f(x) \text{ at } t = 0 \quad (70)$$

The general solution for the leading order, using the Fourier method for eqs 68 and substituting 67, is

$$C_x = \frac{a\sqrt{\pi}}{2} + \sum_{n=1}^{\infty} \left[a\sqrt{\pi} \exp \left(-\frac{n^2 \pi^2 a^2}{4} \right) \exp \left[\frac{\mathcal{A}}{2\mathcal{D}} \left(x - \frac{\mathcal{A}t}{2} \right) \right] \exp[-\mathcal{D}n^2 \pi^2 t] \left[\cos(n\pi x) - \frac{\mathcal{A}}{2n\pi \mathcal{D}} \sin(n\pi x) \right] \right] \quad (71)$$

RESULTS AND DISCUSSION

In the **Nondimensional Mathematical Model** and **Homogenization Method** sections, the nondimensional potential in the EDL, velocity vector, and concentration field of silver nanoparticles, subjected to the electromigration effect, were calculated. To estimate the values of dimensionless parameters involved in the analysis, we consider values of physical and geometrical parameters that have been reported in previous work:¹¹ $h_0 = 100$ nm, $L = 200$ nm, $R_p = 25$ nm, $T = 293$ K, $\epsilon_m = 7.8 \times 10^{-10}$ C/V m, $\rho_m = 997$ kg/m³, $\mu = 1 \times 10^{-3}$ kg/ms, $\phi_0 = 3$ V, $\zeta = -25.4 \times 10^{-3}$ V, $z = 1$, $n_{\infty} = 6.022 \times 10^{23}$ m⁻³, $\lambda_D = 10$ nm, $U_c = 2.5 \times 10^{-3}$ m/s, $D = 8.58 \times 10^{-12}$ m²/s, and $D_i = 1.65 \times 10^{-9}$ m²/s. With the previous physical domain, the dimensionless parameters for the calculations assume the following values: $\epsilon = 0.05$, $k = 10$, $\eta = 0.5$, $\alpha = 8.4 \times 10^{-3}$, $\delta = 1$, $Re = 2.5 \times 10^{-4}$, $Pe = 2.93$, and $\bar{u}_0 = 95.68$. For the analytical process, we consider uncharged and charged Ag NPs, obtaining $\mathcal{A} \sim 2 \times 10^2$ and $\mathcal{D} \sim 1.8 \times 10^4$ at $k = 10$.

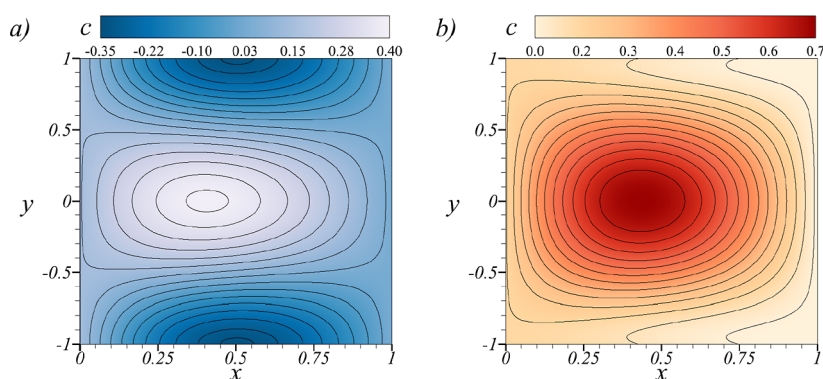


Figure 3. Nondimensional concentration field c at the nondimensional time $t = 10^{-4}$ and $k = 2.5$ for (a) uncharged nanoparticles and (b) charged nanoparticles.

Besides, the nondimensional concentration field is governed by the following equation

$$c = C_x(x, t) + \epsilon k^2 P e \frac{\partial C_x}{\partial x} B(y) + O(\epsilon^2) \quad (72)$$

In Figure 2c, the nondimensional concentration field [eq 72] is shown for both charged and uncharged Ag NPs at $k = 10$. The selected times are determined using the time-dependent diffusive component in eq 71 to counteract the condition $D \gg 1$. As t increases beyond these selected values, the nondimensional concentration field converges to a constant value, i.e., $c = a\sqrt{\pi}/2$. The first noticeable effect in Figure 2a is the propagation of NPs from their initial concentration at $t = 0$, which occurs rapidly throughout the entire system. This phenomenon is primarily attributed to diffusion, and notably, it conserves the original distribution of NPs but elongates along the system. The concentration distribution at $x = 0.2$ at this initial time is exclusively influenced by the initial boundary condition [eq 70]. Figure 2b shows the concentration field for uncharged nanoparticles at $t = 10^{-5}$, where a distinctive negative concentration is observed at the walls of the nanochannel. This negative concentration indicates a deficit of nanoparticles close to the walls. On the other hand, positive concentration values at the entrance, middle, and exit of the nanochannel indicate that uncharged nanoparticles, initially located near the entrance, are driven toward the center of the channel, flow through it, and are eventually expelled at the opposite end. Figure 2d shows that the concentration field for charged nanoparticles is presented at $t = 10^{-5}$. In this case, a concentration value of $c = 0$ indicates the occurrence of the reaction of NPs with the walls, as can be appreciated from eqs 13 and 59. This outcome suggests that most charged NPs react primarily at the entrance and exit regions of the nanochannel, while the excess of NPs that cannot react at the walls is concentrated at the central region. Furthermore, the coefficient \mathcal{A} , as defined in eq 66, may become zero for charged nanoparticles implying that, under certain nanochannel dimensions, no convective transport can take place for the leading order of the concentration field. An analytical expression for the critical nanochannel length, denoted as L_{crit} is derived by eq 66, yielding $L_{\text{crit}} = 12\pi R_p \lambda_D^3 n_\infty f(k)$, where $f(k) = a\bar{u}_0$ [eq 52]. For instance, at $k = 10$, this results in $L_{\text{crit}} = 474$ nm. However, it is noteworthy to mention that for the current ratio $\mathcal{A}/D \ll 1$, no significant changes in the concentration fields are discernible even at the critical length L_{crit} . To improve the concentration field with

convection, it is necessary to increase the \mathcal{A}/D ratio. Our analysis, using eqs 64–66, reveals that this can only be achieved by increasing the parameter α and/or decreasing $k = h_0/\lambda_D$. The parameter $\alpha = -\zeta/\phi_0$ can be increased by subjecting the system to an external heat flux,³⁶ or by reducing the applied voltage from the generator. Caution must be exercised when decreasing ϕ_0 since this would cause a quadratic reduction in the dielectrophoretic force and thus is not recommended. Considering the reduction of h_0 , a lower limit of $k = 2.5$ is deduced. This requirement ensures that the height of the nanochannel allows the passage of at least one nanoparticle through it, i.e., $h_0 = R_p = 25$ nm.

In Figure 3, the nondimensional concentration field at $k = 2.5$ is shown. In Figure 3a, a pronounced trapping mechanism for uncharged nanoparticles is evident, whereby a significant quantity of Ag NPs becomes trapped near the center of the nanochannel. This change in behavior is governed by the variable $B(y)$, which, in return, is a consequence of the overlap within the EDL. This phenomenon can be elucidated by considering the representation of eqs 58 with 39 and 42, as follows

$$B = \frac{1}{\alpha k^2} \left(\frac{y^2}{2} \frac{d\psi_0}{dy} \Big|_{y=1} - \psi_0 + \frac{1}{k} \right) \quad (73)$$

The trapping mechanism is observed to manifest when $\tanh(k) < 0.999$ which is obtained when $k = 3.8$. In Figure 3b, the concentration field for charged Ag NPs is depicted, where it is observed that these nanoparticles undergo electrical reactions predominantly at the exit of the nanochannel while filling the nanohole in a counter-flow manner. For the specified value of $k = 2.5$, the critical length is calculated to be $L_{\text{crit}} = 212$ nm.

CONCLUSIONS

Propagation of uncharged and charged nanoparticles due to an EF and electromigration in a nanochannel with overlapping EDLs has been studied by deriving an analytical expression for the ionic distribution, hydrodynamic forces, and Ag NP concentration. From the current analysis, the following major points are obtained: (i) for charged nanoparticles, colloidal transport convection is countered by electromigration, where a critical length of the nanochannel will produce a pure diffusion process for the leading concentration field solution; (ii) for uncharged nanoparticles, a trapping mechanism can be achieved due to overlapping of the EDL at $k = 3.8$; and (iii)

in addition to modifying the nanochannel dimension, the propagation of colloids can be achieved by increasing the surface potential ζ through an external heat source. This last finding requires that the energy equation be coupled with the governing equations. Further studies on the propagation of colloids in nanoconfinement would be required to investigate, experimentally, the nanoaperture dimension and the variation in zeta potential. The latter could be achieved by using an external heat source³⁶ or by modifying the ionic concentration of the solvent,¹⁴ as both approaches invalidate the Debye–Hückel approximation.

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REFERENCES

- (1) Wang, J.; Maier, S. A.; Tittel, A. Trends in Nanophotonics-Enabled Optofluidic Biosensors. *Adv. Opt. Mater.* **2022**, *10*, 2102366.
- (2) Escobedo, C. On-chip nanohole array based sensing: a review. *Lab Chip* **2013**, *13*, 2445–2463.
- (3) Pennathur, S.; Santiago, J. G. Electrokinetic Transport in Nanochannels. 1. Theory. *Anal. Chem.* **2005**, *77*, 6772–6781.
- (4) Pennathur, S.; Santiago, J. G. Electrokinetic transport in nanochannels. 2. Experiments. *Anal. Chem.* **2005**, *77*, 6782–6789.
- (5) Striemer, C. C.; Gaborski, T. R.; McGrath, J. L.; Fauchet, P. M. Charge- and size-based separation of macromolecules using ultrathin silicon membranes. *Nature* **2007**, *445*, 749–753.
- (6) Mukaibo, H.; Wang, T.; Perez-Gonzalez, V.; Getpreecharsawas, J.; Wurzer, J.; Lapizco-Encinas, B.; McGrath, J. L. Ultrathin nanoporous membranes for insulator-based dielectrophoresis. *Nanotechnology* **2018**, *29*, 235704.
- (7) Eftekhari, F.; Escobedo, C.; Ferreira, J.; Duan, X.; Giroto, E. M.; Brolo, A. G.; Gordon, R.; Sinton, D. Nanoholes as nanochannels: Flow-through plasmonic sensing. *Anal. Chem.* **2009**, *81*, 4308–4311.
- (8) Escobedo, C.; Brolo, A. G.; Gordon, R.; Sinton, D. Optofluidic Concentration: Plasmonic Nanostructure as Concentrator and Sensor. *Nano Lett.* **2012**, *12*, 1592–1596.
- (9) Ertsgaard, C. T.; McKoskey, R. M.; Rich, I. S.; Lindquist, N. C. Dynamic placement of plasmonic hotspots for super-resolution surface-enhanced Raman scattering. *ACS Nano* **2014**, *8*, 10941–10946.
- (10) Larson, S.; Luong, H.; Song, C.; Zhao, Y. Dipole Radiation-Induced Extraordinary Optical Transmission for Silver Nanorod-Covered Silver Nanohole Arrays. *J. Phys. Chem. C* **2019**, *123*, 5634–5641.
- (11) Bdour, Y.; Beaton, G.; Gomez-Cruz, J.; Cabezuelo, O.; Stamplecoskie, K.; Escobedo, C. Hybrid plasmonic metasurface as enhanced Raman hot-spots for pesticide detection at ultralow concentrations. *Chem. Commun.* **2023**, *59*, 8536–8539.
- (12) Khosravi, B.; Gordon, R. Accessible Double Nanohole Raman Tweezer Analysis of Single Nanoparticles. *J. Phys. Chem. C* **2024**, *128*, 15048–15053.
- (13) De Leebeeck, A.; Sinton, D. Ionic dispersion in nanofluidics. *Electrophoresis* **2006**, *27*, 4999–5008.
- (14) Qu, W.; Li, D. A model for overlapped EDL Fields. *J. Colloid Interface Sci.* **2000**, *224*, 397–407.
- (15) Golovnev, A.; Trimper, S. Analytical solution of the Poisson-Nernst-Planck equations in the linear regime at an applied dc-voltage. *J. Chem. Phys.* **2011**, *134*, 154902.
- (16) Zachariah, Z.; Espinosa-Marzal, R. M.; Spencer, N. D.; Heuberger, M. P. Stepwise collapse of highly overlapping electrical double layers. *Phys. Chem. Chem. Phys.* **2016**, *18*, 24417–24427.
- (17) Yeh, L.-H.; Zhang, M.; Qian, S.; Hsu, J.-P.; Tseng, S. Ion concentration polarization in Polyelectrolyte-modified nanopores. *J. Phys. Chem. C* **2012**, *116*, 8672–8677.
- (18) Lapizco-Encinas, B. H. Microscale electrokinetic assessments of proteins employing insulating structures. *Curr. Opin. Chem. Eng.* **2020**, *29*, 9–16.
- (19) Wu, Z.-Q.; Li, Z.-Q.; Ding, X.-L.; Hu, Y.-L.; Xia, X.-H. Influence of Asymmetric Geometry on the Ion Transport of tandem nanochannels. *J. Phys. Chem. C* **2021**, *125*, 24622–24629.
- (20) Mani, A.; Zangle, T. A.; Santiago, J. G. On the propagation of concentration polarization from microchannel-nanochannel interfaces Part I. Analytical model and characteristic analysis. *Langmuir* **2009**, *25*, 3898–3908.
- (21) Yaroshchuk, A.; Bondarenko, M. P. Current-Induced concentration polarization of nanoporous media: Role of electro-osmosis. *Small* **2018**, *14*, 1703723.
- (22) Chen, L.; Hu, C.; Dong, Y.; Li, Y.; Shi, Q.; Liu, G.; Long, R.; Xiong, Y. Tunable Layered Gold Nanochips for High Sensitivity and Uniformity in SERS. *J. Phys. Chem. C* **2023**, *127*, 8167–8174.
- (23) Sakamoto, M.; Saitow, K. Large-Area Plasmon Mapping via an Optical Technique: Silver Nanohole Array and Nano-Sawtooth Structures. *J. Phys. Chem. C* **2023**, *127*, 13105–13111.
- (24) Hille, B. *Ionic Channels of Excitable Membranes*; Sinauer Associates Inc., 1992.
- (25) Probstein, R. F. *Physicochemical Hydrodynamics*; Wiley-Interscience, 2005.
- (26) Philipse, A. P. *Brownian Motion. Elements of Colloid Dynamics*; Springer, 2018.
- (27) Vacik, J. *Electrophoresis a Survey of Techniques and Applications*; Elsevier, 1979.

(28) Elimelech, M.; Gregory, J.; Jia, X.; Williams, R. A. *Particle Deposition and Aggregation. Measurement, Modelling and Simulation*; Butterworth-Heinemann, 1995.

(29) Leonard, G.; Mitchner, M.; Self, S. A. Particle transport in electrostatic precipitators. *Atmos. Environ.* **1980**, *14*, 1289–1299.

(30) Adamczyk, Z. Particle deposition from flowing suspensions. *Colloids Surf.* **1989**, *39*, 1–37.

(31) Miloh, T.; Boymelgreen, A. Travelling wave diplophoresis of ideally polarizable nanoparticles with overlapping electric double layers in cylindrical pores. *Phys. Fluids* **2014**, *26*, 072101.

(32) Bazant, M. Z.; Thornton, K.; Ajdari, A. Diffuse-charge dynamics in electrochemical systems. *Phys. Rev. E: Stat., Nonlinear, Soft Matter Phys.* **2004**, *70*, 021506.

(33) Ajdari, A. Electro-osmosis on Inhomogeneously charged surfaces. *Phys. Rev. Lett.* **1995**, *75*, 755–758.

(34) Bender, C. M.; Orzag, S. A. *Advanced Mathematical Methods for Scientists and Engineers I: Asymptotic Methods and Perturbation Theory*; Springer Science and Business, 2013.

(35) Mei, C. C.; Vernescu, B. *Homogenization Methods for Multiscale Mechanics*; World Scientific Publishing Co., 2010.

(36) Vargas, C.; Bautista, O.; Méndez, F. Effect of temperature-dependent properties on electroosmotic mobility at arbitrary zeta potentials. *Appl. Math. Model.* **2019**, *68*, 616–628.