Cooperative Regulation of Myosin-Actin Interactions by a Continuous Flexible Chain I: Actin-Tropomyosin Systems

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ABSTRACT We present a model for cooperative myosin binding to the regulated actin filament, where tropomyosins are treated as a weakly-confined continuous flexible chain covering myosin binding sites. Thermal fluctuations in chain orientation are initially required for myosin binding, leaving kinked regions under which subsequent myosins may bind without further distortion of the chain. Statistical mechanics predicts the fraction of sites with bound myosin-S1 as a function of their affinities. Published S1 binding curves to regulated filaments with different tropomyosin isoforms are fitted by varying the binding constant, chain persistence length ν (in actin monomers), and chain kink energy A from a single bound S1. With skeletal tropomyosin, we find an S1 actin-binding constant of 2.2 \times 10⁷ M⁻¹, A = 1.6 k_BT and ν = 2.7. Similar persistence lengths are found with yeast tropomyosin. Larger values are found for tropomyosin-troponin in the presence of calcium ($\nu = 3.7$) and tropomyosins from smooth muscle and fibroblasts ($\nu = 4.5$). The relationship of these results to structural information and the rigid-unit model of McKillop and Geeves is discussed.

INTRODUCTION

The regulation of contractility in striated muscle by calcium is effected via tropomyosin on the actin filament (Ebashi, 1969). The tropomyosin molecule is a coiled-coil 42 nm in length, which covers seven monomers on one strand of the actin double helix. On each strand these units are disposed end-to-end to form what appears to be a continuous chain (Lorenz et al., 1995; Vibert et al., 1997). The steric blocking model of Haselgrove (1973) and Huxley (1973) proposes that myosin binding sites are blocked by tropomyosin troponin (TmTn) in the absence of calcium, and that tropomyosin moves to a position which allows myosin binding when calcium is bound to troponin-C. The two positions of tropomyosin may be viewed as two states of an allosteric system if transitions between them are rapid and in equilibrium (Lehrer and Geeves, 1998). The steric blocking model is broadly confirmed by a variety of experiments (Gordon et al., 2000), although the fact that myosin binds weakly in the absence of calcium suggests that a two-state model may be oversimplified.

The statistical-mechanical model of thin filament regulation proposed by Hill, Eisenberg, and Greene (Hill et al., 1980a) is based on these ideas. The key assumptions of their model are that 1), each tropomyosin molecule can be treated as a rigid unit moving between two discrete orientations which generate different actin affinities for myosin; 2), states of the same kind are favored by weak end-to-end interactions between adjacent tropomyosins; and 3), Tm-Tm interaction energies vary with the number of calcium ions bound to

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the nearest molecule of TnC. This model contains two mechanisms for cooperativity in myosin binding; a single bound myosin activates the six additional actin monomers covered by one tropomyosin, and this activation is partially transmitted to neighboring tropomyosins by end-to-end interactions. Cooperativity is observed in solution studies of the extent and kinetics of myosin binding (Greene and Eisenberg, 1980; Trybus and Taylor, 1980; McKillop and Geeves, 1991) and of actomyosin ATPase (Bremel et al., 1972; Lehrer and Morris, 1982). In vertebrate striated muscle, the high sensitivity of isometric force to changes in calcium level can also be explained in terms of calciumdependent Tm-Tm interactions (Hill, 1985).

Later cryo-EM studies show that there are actually three orientational states of tropomyosin (Vibert et al., 1997), designated by Lehman et al. (2000) as B (blocked), C (calcium-induced), and M (myosin-induced). A model with three regulatory states of the thin filament (blocked, closed, and open) was previously proposed by McKillop and Geeves (1993), based on solution studies of myosin-S1 binding to thin filaments. However, this model did not invoke end-to-end Tm interactions; the regulatory unit was originally identified as the structural repeat unit of one tropomyosin and seven actin monomers (A_7Tm) . The development of assay methods sensitive to the size of the regulatory unit showed that cooperativity could extend significantly beyond the structural unit size for both actin-Tm and actin-Tm-Tn filaments (Geeves and Lehrer, 1994, Lehrer et al., 1997, Maytum et al., 1999). For these systems, a model of independent regulatory units is structurally inappropriate. A version of the Hill-Eisenberg-Greene model with three regulatory states would provide a way out of these difficulties.

In fact, we wish to argue for a more radical revision of existing regulatory models, in which individual tropomyosin molecules have intrinsic flexibility and are coupled by strong

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end-to-end interactions to form a semiflexible chain. Evidence which points in this direction is as follows.

In solution, tropomyosin readily polymerizes end-to-end at ionic strengths below ~ 0.3 M, and the polymer is flexible with a persistence length of 50–200 nm (Howard, 2001). However, individual molecules of tropomyosin have a very low affinity for actin (Wegner, 1979), so that the binding of Tm filaments to actin can also be described as a polymerization process (Vilfan, 2001). This view is supported by the observation that minor modifications to either the N-terminus (loss of acetylation) or the C-terminus (loss of the terminal amino acid) of the Tm polypeptide chain does not greatly affect the stability of Tm but results in loss of polymerization and actin binding (Heald and HitchcockdeGregori, 1988; Maytum et al., 2001). Thus the head-to-tail interactions between tropomyosins along the actin filament are essential for actin affinity. High-resolution structural data (Brown et al., 2001, Whitby and Phillips, 2000) also suggest that tropomyosin is a semiflexible molecule (see also Stewart, 2001). Atomic modeling of tropomyosins on the actin surface suggests that Tm is bound by weak electrostatic interactions which are not highly stereospecific (Lorenz et al., 1995). Furthermore, both the Hill-Eisenberg-Greene and McKillop-Geeves models give an equilibrium constant of 0.2 for the transition between closed and open states of the actin-Tm filament, so that the Gibbs energy difference between these states is $1.6 \times$ thermal energy. The rate of transitions between these states is estimated at above 500 s^{-1} (Geeves and Lehrer, 1994), suggesting a low activation barrier between binding positions. If a single Tm molecule in a Tm chain were to move between the discrete binding sites on actin inferred from EM and x-ray scattering, a major reorganization of the Tm-Tm contacts would be required, yet these are the contacts which are essential for binding to actin.

Whatever the exact nature of Tm-Tm and Tm-actin interactions, there is now a body of evidence which suggests that tropomyosin molecules on actin form a loosely-confined quasi-continuous semiflexible chain which spans the whole actin filament. We propose a new model of thin-filament regulation along these lines. To make the problem mathematically tractable the tropomyosin chain is treated as elastically homogeneous. Similarly, the potential well which provides angular confinement is assumed to have a single minimum in the absence of myosin or troponin. As discussed in the last section, the second hypothesis is still open.

In this article, the continuous-flexible-chain (CFC) model is applied to actin-tropomyosin systems in the absence of troponin. Mathematical developments appear in a selfcontained section (Theory), which can be omitted if desired. Here we show that the model can fit published experimental myosin binding curves in solution, using reasonable values of parameters such as chain stiffness and the distortion energy of the chain accompanying myosin binding. The results are in broad agreement with those obtained from the independent-rigid-unit model (McKillop and Geeves 1991, 1993). Chen et al. (2001) have shown that the same binding curves can also be fitted with the model of Hill, Eisenberg, and Greene (Hill et al., 1980a). Thus the CFC model should be tested against a much wider range of experiments. In the following article, the model is generalized to actin-Tm-Tn systems and regulation by calcium.

Definitions of model parameters and other symbols are collected in Table 1. Fortran programs for numerical predictions and data-fitting to the model are available at www.kcl.ac.uk/depsta/biomedical/randall/dasmith.html.

REGULATION BY A CONTINUOUS FLEXIBLE CHAIN

This section gives the basic assumptions of the proposed model, its mathematical formulation, and a qualitative description of how it regulates the energetics of myosin binding. Exact results quoted without proof are derived in a preliminary article (Smith, 2001). Kinetic aspects of myosin regulation will be considered elsewhere.

1. Tropomyosin units on the surface of F-actin are intrinsically flexible and linked to form a continuous semiflexible chain along the length of the actin filament (Fig. 1 A).

2. This chain is confined to a range of orientations on one strand of the actin double helix (here termed the closed state) by a weak electrostatic potential, arising from ionic or van der Waals interactions.

This model becomes mathematically tractable if we suppose that the chain is elastically homogeneous, with a finite bending stiffness κ_{Tm} per unit length, and the confining

Definitions of mathematical symbols appearing outside the Theory section. In this article, ln and log denote logarithms to base e and 10 respectively.

FIGURE 1 Schematics of orientational configurations of a continuous flexible tropomyosin chain on actin (A) , and a cross section of the actin filament (B) . A1, A chain configuration in the absence of myosin (upper diagram), with thermally excited angular fluctuations about $\phi = 0$, close to the groove between the inner and outer domains of G-actin depicted in B (see also Lehman et al., 2000). These fluctuations cover the myosin binding interface and collectively define a closed regulatory state. A2, The tropomyosin chain with a low density of myosins bound to actin, which push the chain beyond angle ϕ_+ toward the inner domain. A local open state is created by each myosininduced kink. A3, At higher myosin density, an extended open state is created. If the persistence length covers several actin sites, this can occur even when most sites are unoccupied.

potential is a quadratic function of chain orientation ϕ (in radians) from a preferred orientation which tracks one helical strand. A distorted chain configuration is specified by angular displacements $\phi(s)$ at each position s along a chain of length L. The energy of this configuration is

$$
E = \int_0^L \left(\frac{\kappa}{2}\phi''(s)^2 + \frac{\alpha}{2}\phi(s)^2\right)ds,\tag{1}
$$

where $\kappa = \kappa_{\text{Tm}} R^2$ and R the radius at which tropomyosin sits on the actin filament. Estimates of κ_{Tm} from the persistence length of tropomyosin in solution (Howard, 2001; Hvidt et al., 1983, Phillips and Chacko, 1996) and by scaling as $(radius)^4$ from actin measurements (Yanagida et al., 1984, Yasuda et al., 1996) suggest that $\kappa_{\text{Tm}} \sim 0.4{\text{--}}1.6 \times 10^{-27}$ N·m². With $R = 4-5$ nm (Vibert et al., 1997; Xu et al., 1999), $\kappa \sim 0.6{\text -}4.0 \times 10^{-44} \text{ N} \cdot \text{m}^4$. For estimation we use a value of 2.5×10^{-44} N·m⁴.

If the chain is forcibly pinned to angle ϕ_+ at one point, the rest of the chain adopts a minimum-energy configuration in which displacements away from the pinning point revert smoothly to zero over a characteristic distance called the persistence length. The persistence length is estimated by minimizing the energy of a smooth kink of half-width l , which is of the form $\kappa(\phi_+ / l^2)^2 l + \alpha \phi_+^2 l$ apart from numerical factors of order unity. This energy is minimized when $l = (3\kappa/\alpha)^{1/4}$. An exact calculation gives the kink energy A as

where

$$
A = 4\kappa \xi^3 \phi_+^2 \tag{2}
$$

$$
\xi = (\alpha/4\kappa)^{1/4} \tag{3}
$$

and $1/\xi$ is the persistence length. It will be shown later that myosin binding data can be fitted to the model if $\xi^{-1} = 16.5$ nm (three actin repeats). Hence, $\alpha = 1.34 \times 10^{-12}$ J/m. which implies that the energy required to displace a single 42-nm tropomyosin unit from its resting angle by 30° is

 \sim 8 × 10⁻²¹ J, or twice thermal energy k_BT (k_B = Boltzmann's constant; $T =$ absolute temperature).

3. In the absence of bound myosin, the chain makes thermal fluctuations about its preferred orientation. The standard angular deviation from thermal noise can be estimated by equating the energy of a kink of amplitude $\delta\varphi$ to k_BT . This argument is not rigorous because thermal noise excites fluctuations on a range of wavelengths above the persistence length, but gives the correct result,

$$
\delta \phi = (k_{\rm B} T / 8 \kappa \xi^3)^{1/2},\tag{4}
$$

apart from a numerical factor. The preceding estimates for κ and α give $\delta \varphi \sim 0.30$ radians (17°), which is physically reasonable. These fluctuations are intrinsic to the closed state.

4. In the absence of myosin, myosin-binding sites on the actin filament are covered by most thermally-driven configurations of the chain (Fig. 1), which define a closed state.

5. A myosin binding site is exposed only by a sufficiently large positive kink $\phi > \phi_+$ in chain angle. To achieve myosin binding rates comparable with unregulated actin (Trybus and Taylor 1980), ϕ_+ should not exceed two standard deviations from thermal noise, as above. Equivalently, the kink energy A should not exceed $2k_BT$. The binding site should span a range of angles from ϕ_+ to a larger negative angle (Fig. 1 B), to prevent exposure by negative deviations of the chain.

Fig. 1 A shows how this model leads to cooperative myosin binding. The first myosin to bind under thermal fluctuations of the Tm or Tm-Tn chain produces a positive kink of amplitude ϕ_+ and a half-width of one persistence length (a local open state). We define a persistence number as

$$
\nu = \frac{\text{persistent}}{\text{actin site spacing}} = \frac{1}{\xi c},\tag{5}
$$

so the first bound myosin exposes ν sites on either side, and the kink size (the number of actin sites exposed by the kink) is $2\nu + 1$.

Let $K_{S1} = K_{S1} [S1]$ be the first-order affinity of S1 to actin in the absence of chain distortion, proportional to free myosin-S1 concentration in solution. The first myosin to bind does so with affinity

$$
K = K_{\rm SI} \exp(-A/k_{\rm B}T) \tag{6}
$$

reduced by the probability of a kink fluctuation. Those that follow are presented with a predominantly unkinked filament, so that at low S1 concentration the fraction θ of occupied sites is $K/(K + 1)$. At higher concentrations, latebinding myosins see a significant fraction of sites exposed by kinked regions of the chain, and may bind to these sites at a higher affinity approaching K_{S1} , enlarging the kinks. As more myosins bind, all kinked regions eventually overlap and further bindings are not inhibited by the chain.

The cooperative transition between these regimes should occur when the bound fraction $\theta \approx (2\nu + 1)^{-1}$. If $\theta =$ $K/(K + 1)$, switching occurs when $K \approx (2\nu)^{-1}$. Hence the switching value of K_{S1} , here denoted by K_{*} , is estimated at $\exp(A/k_BT)/2\nu$. This formula exaggerates the dependence on A, because the binding curve lies between $K/(K + 1)$ and $K_{S1}/(K_{S1} + 1)$. A better estimate can be obtained from predicted binding curves.

The structure of the model is now specified. To make quantitative predictions, expressions for the free energy of the kinked chain are needed for at least two kinks of the same angle as a function of their separation. For two kinks of angle ϕ_+ at separation ξx , the energetic component of the distortion energy can be written in terms of the single-kink energy A as

$$
E^{(2)}(x) = A\Gamma_{\mathcal{S}}(x) \tag{7}
$$

(Smith, 2001). The function $\Gamma_{S}(x)$ tends to unity when $x \rightarrow$ 0 and to 2 for $x \gg 1$. When the kinks are merged, the pair energy is that of a single kink, but when widely separated the pair energy is the sum of the energies of each kink in isolation. The entropic contribution is expected to vary similarly with x , in which case A can be regarded as a free energy.

Please note the following corrections to the article (Smith, 2001) in which the interaction potentials were derived:

- Eq. 3.2: Replace $Z_{ab}(\Phi_1, \Phi_b)$ by $Z_{ab}(\Phi_a, \Phi_b)$ in both denominators.
- Eq. 4.7: The lower limit of the second sum should be i , not $i + 1$.

MYOSIN BINDING TO ACTIN-TROPOMYOSIN

This section develops the statistical mechanics of equilibrium myosin-S1 binding to actin regulated by a continuous flexible chain. The theoretical formalism can be used to predict the bound S1 fraction as a function of the free S1 concentration in solution, and other statistical measures of occupancy such as the correlation length between occupied sites. This model is applied to the actin-tropomyosin system in the absence of troponin. It should also be applicable to the actin-tropomyosin-troponin system at saturating levels of calcium, as troponin-I does not bind significantly to actin under these conditions.

Theory

The fraction of monomers with myosin bound can be calculated if the distortion energy of the kinked chain with an arbitrary number and position of bound myosins is known. Let $F^{(n)}(\mathbf{s}_n)$ be the free energy of the distorted chain covering N monomers on one strand of F-actin, with n myosins bound to monomers at positions $\mathbf{s}_n = (s_1, \ldots, s_n)$, listed in increasing order. The equilibrium probability of this configuration is a Boltzmann factor in the corresponding Gibbs energy, which is the sum of the above distortion energy and the Gibbs energy $-nk_BT \ln K_{S1}$ of myosin binding. Thus the probability of all configurations with n myosins bound is

$$
P_n = \frac{1}{Z_N} \sum_{[\mathbf{s}_n]} K_{S1}^n \exp(-\beta F^{(n)}(\mathbf{s}_n)) \tag{8}
$$

where $\beta = 1/k_B T$ and

$$
Z_N = \sum_{n=0}^{N} \sum_{[s_n]} K_{S1}^n \exp(-\beta F^{(n)}(\mathbf{s}_n))
$$
(9)

is the partition function for regulated binding; the inner sum is over all ordered arrangements of n sites out of N . Hence the mean number \bar{n} of occupied sites is given by

$$
\bar{n} = K_{\rm SI} \frac{d \ln Z_{\rm N}}{d K_{\rm SI}} \tag{10a}
$$

and the bound fraction is $\theta = \bar{n}/N$. Similarly, the mean square deviation in n is

$$
\overline{(\Delta n)^2} = \bar{n} + K_{\rm SI}^2 \frac{d^2 \ln Z_{\rm N}}{dK_{\rm SI}^2}.
$$
 (10b)

It is instructive to apply these formulae to a rigid chain covering N sites, as envisaged by Geeves and Halsall (1987) for protomeric tropomyosin with $N = 7$. If one bound myosin displaces the whole chain, $Z_N = 1 + [(1 + K_{S1})^N - 1]e^{-\beta A}$ where A is the displacement energy. The corresponding formula for the bound fraction θ is equivalent to that of Geeves and Halsall if $K_T = 1/(e^{\beta A} - 1)$, where K_T is the equilibrium constant between the closed and open states of their model. Nevertheless, the rigid-chain model considered here is different, because the totality of chain configurations in the absence of bound myosin defines a closed state, but a subset of these configurations with excitation energy $> A$ allow myosin binding. If $\beta A \ll 1$, nearly all configurations permit binding and the fraction of nonbinding configurations, which should be associated with the closed state of the Geeves-Halsall model, becomes small. Hence $K_T \gg 1$ as predicted above.

Apart from end effects, the distortion energy $F^{(n)}(\mathbf{s}_n)$ depends only on the spacings $x_{i,i+1} = \xi(s_{i+1} - s_i)$ between

bound myosins as a fraction of chain persistence length $1/\xi$. For $n = 2$, a closed analytic expression is available via Eq. 7. For convenience, each bound myosin is assumed to pin the chain to angle ϕ_+ at the point of contact. It can be argued that pinning is more realistic than the one-sided constraint ϕ > ϕ_{+} . Both types of constraint have similar consequences, but the former is easier to handle mathematically.

The partition function can be evaluated by the transfermatrix method if $F^{(n)}(\mathbf{s}_n)$ can be expressed in terms of localized interactions between the n bound myosins. For $n = 1$, $F^{(1)}(\mathbf{s}_1) \equiv A$ is the energy of a single kink. Chain energies expressing the interaction of localized pairs, triplets of bound myosins are defined as

$$
V^{(2)}(x_{12}) = F^{(2)}(s_1, s_2) - 2A,
$$

\n
$$
V^{(3)}(x_{12}, x_{23}) = F^{(3)}(s_1, s_2, s_3) - V^{(2)}(x_{12}) - V^{(2)}(x_{23}) - 3A
$$
\n(11)

and

$$
V^{(n)}(x_{12},...,x_{n-1,n}) = F^{(n)}(s_1,...,s_n) - nA
$$

-
$$
\sum_{k=2}^{n-1} \sum_{j=1}^{n+1-k} V^{(k)}(x_{j,j+1},...,x_{j+k-2,j+k-1})
$$

(12)

for a localized *n*-myosin interaction. By construction, these functions tend to zero when all spacings between bound myosins are increased beyond the persistence length. Using Eq. 7 for the distortion energy of two kinks gives the pairinteraction energy $V^{(2)}(x) = A(\Gamma_S(x) - 2)$, which varies from $-A$ at $x = 0$ to zero when $x \gg 1$ (Fig. 2). These definitions imply that the higher-order interactions approach zero when at least one spacing between adjacent myosins approaches zero or becomes much greater than the persistence length. They also vanish in the limit of large

FIGURE 2 The universal chain-induced interaction potential $V^{(2)}(x) =$ $A(\Gamma_{\mathcal{S}}(x) - 2)$ for a pair of bound myosins at separation x in units of the persistence length. Ticks on the x-axis denote binding sites on actin for a persistence length of five actin sites ($\nu = 5$). The interaction is attractive $(V^{(2)}(x) < 0)$ almost everywhere, because the energy of two isolated kinks has been subtracted. A closed analytic formula is available (Smith, 2001).

persistence lengths, when the kink from a single myosin spans many binding sites. Hence the distortion energy will be approximated by the sum of nearest-neighbor pair interactions, namely

$$
F^{(n)}(s_1,\ldots,s_n) \approx nA + \sum_{j=1}^{n-1} V^{(2)}(x_{j,j+1}). \tag{13}
$$

The accuracy of this approximation can be investigated numerically from recursion formulae for the n -body free energy function (Smith, 2001).

The transfer-matrix method for pair interactions

Under the pair approximation (Eq. 13), the partition function of Eq. 9 can be calculated by the transfer-matrix method if the range of interactions is limited and interactions over all pairs within that range are included correctly. To this end, the pair energy $V^{(2)}(x)$ is assumed to be zero for $x > 2$, which neglects an oscillating tail of order 10% (Fig. 2). The range of this truncated potential is r actin sites, where $r = 2\nu$.

The transfer-matrix method for Z_N proceeds by a recursion on the number of sites N. For this purpose, the following set of constrained N-site partition functions are sufficient. Let z_{N1} be the partition function with the leading site occupied by myosin. For $j = 2, \ldots, r$, let z_{Ni} be the partition function with the leading $j-1$ sites empty and the site behind occupied. We also need the partition function with the leading r sites empty; it is convenient to denote this quantity by $z_{N,r+1}$, although $z_{N,j}$ then has different meanings for $j =$ $r + 1$ and $j < r + 1$. As shown in Fig. 3, adding one more site gives

$$
z_{N+1,1} = \sum_{j=1}^{r} K_j z_{N,j} + K z_{N,r+1}
$$
 (14a)

$$
z_{N+1,j+1} = z_{N,j} \ (j = 1, \ldots, r-1) \tag{14b}
$$

$$
z_{N+1,r+1} = z_{N,r+1} + z_{N,r}, \qquad (14c)
$$

where $K_j \equiv K \exp(-\beta V^{(2)}(j/\nu))$ $(j = 1, ..., r)$ is myosin affinity under the chain but enhanced by a jth-nearestneighbor myosin. In vector-matrix form, $z_{N+1} = Tz_N$ where **T** is a transfer matrix of dimension $r + 1$. For $r = 7$,

$$
\mathbf{T} = \begin{pmatrix} K_1, & K_2, & K_3, & K_4, & K_5, & K_6, & K_7, & K \\ 1 & 0 & & & & & \mathbf{0} \\ & 1 & 0 & & & & & \\ & & 1 & 0 & & & & \\ & & & 1 & 0 & & & \\ & & & & 1 & 0 & & \\ & & & & & 1 & 1 \end{pmatrix}
$$
 (15)

For the interaction potential in Fig. 2 with $A > 0, K_1 > K_2$ \ldots $K_r > K$ so the transfer matrix has rank $r + 1$. Although this matrix is not symmetric, it has a simple form which facilitates the construction of eigenvalues and eigenvectors.

FIGURE 3 Diagrams illustrating iterative rules (Eq. 14) for components of the N-site myosin-only transfer matrix Z_N , with interaction range $r = 7$. The component $z_{N+1,1}$ in which the leading site is occupied by myosin (\bullet), can be expressed in terms of N -site components, z_{Ni} , in which the leading $j - 1$ sites are unoccupied (0) and the jth site is occupied ($j \le 7$) or unoccupied $(j = 8)$. In the bottom diagram, the leading myosin binds independently and requires a multiplicative factor K (Eq. 6). Interacting myosins within range r are linked, and require a factor $K_i =$ $Kexp(-\beta V^{(2)}(j/\nu))$ when separated by j sites. Similar diagrams apply for the $z_{N+1,j}$.

As shown below, a symmetric transfer matrix is not required to calculate the partition function.

Let λ_{α} be an eigenvalue of T, with right and left eigenvectors $\mathbf{u}^{(\alpha)}$ and $\mathbf{v}^{(\alpha)}$ respectively. All eigenvalues are assumed to be distinct, though not necessarily real. Hence the eigenvectors satisfy mutual orthogonality and completeness conditions, which in terms of the matrices $U =$ $({\bf u}^{(1)}, \dots, {\bf u}^{(r+1)}), \; {\bf V} = ({\bf v}^{(1)}, \dots, {\bf v}^{(r+1)})$ can be written as $\mathbf{V}^{\mathrm{T}}\mathbf{U} = \mathbf{I}$ and $\mathbf{U}\mathbf{V}^{\mathrm{T}} = \mathbf{I}$ respectively. I is the unit matrix and superscript T indicates the transposed matrix. Then

$$
\mathbf{T} = \mathbf{U}\mathbf{D}\mathbf{V}^{\mathrm{T}},\tag{16}
$$

where **D** is the diagonal matrix of eigenvalues $\lambda_1, \ldots, \lambda_{r+1}$.

These results determine the required partition function Z_N . The vector form of Eq. 14 has the solution $z_N = T^N z_0$ where z_0 is a constant vector. With Eq. 16, $z_N = UD^N V^T z_0$. The sum of the elements of this vector gives Z_N in the form

$$
Z_{\rm N} = \sum_{\alpha=1}^{\rm r+1} b_{\alpha} \lambda_{\alpha}^{\rm N} \underset{(\rm N \to \infty)}{\sim} b_{\rm m} \lambda_{\rm m}^{\rm N}, \qquad (17)
$$

where $\lambda_{\rm m}$ is the maximum eigenvalue and the b_{α} are determined by the eigenvectors. In the limit of large N , the Gibbs energy of the system is $-k_BT(N \ln \lambda_m+O(1))$ and extensive thermodynamic variables such as \bar{n} are determined by the maximum eigenvalue. The limiting form

$$
\theta = K \frac{d \ln \lambda_{\rm m}}{dK} \tag{18}
$$

of the bound fraction is independent of N.

The secular equation for the eigenvalues of T is the polynomial

$$
R(\lambda) \equiv \lambda^{r+1} + \sum_{j=1}^{r} a_j \lambda^j = 0
$$
 (19)

with coefficients $a_r = -(1 + K_1), a_j = K_{r-j} - K_{r+1-j}$ (j = $1, \ldots, r$ and $a_{\rm o} = K_{\rm r} - K$. Manipulations based on this polynomial allow the bound fraction to be written in the form

$$
\theta = \frac{\lambda_{\rm m}^{\rm r-1}(\lambda_{\rm m}-1)}{R'(\lambda_{\rm m})},\tag{20}
$$

which is used for numerical calculations.

Numerical predictions

Binding curves for θ as a function of the first-order binding constant K_{S1} have been computed from Eq. 20 using the pair interaction in Eq. 7. Three parameters are involved; the ratio βA of kink energy to thermal energy, the persistence number ν , and the range r of the truncated potential such that $r \geq 2\nu$.

Fig. 4 shows the predicted fraction of actin sites occupied by myosin as a function of its first-order affinity K_{S1} . At low affinity, myosin binding is inhibited by the need to create kinked regions of the chain. As K_{S1} rises through a characteristic switching value K_* , this inhibitory mecha-

FIGURE 4 The fraction θ of actin sites occupied by myosin-S1 as a function of first-order myosin affinity K_{S1} , as predicted by Eq. 20. Graphs A and B show binding curves for kink energies $A = 1.5k_BT$ and $3k_BT$ respectively; plots selected along the arrow from right to left are in increasing order of the persistence number ν . Graphs C and D show the above curves for $\nu = 1$ and 5 respectively, and $A = 1.5k_BT$, accompanied by the hyperbolic curves $K/(K + 1)$ and $K_{S1}/(K_{S1} + 1)$ for independent binding in the presence and absence of inhibition. The crossover effect is discussed in the main text.

nism is removed as the kinks overlap and the binding curve switches smoothly to a higher-level curve. As the persistence number ν is increased, less myosin is required to effect switching and the width of the switching range of K_{S1} values decreases. With a bigger kink energy, the initial inhibition is increased and more myosin is required to overcome it.

Fig. 4, C and D show that as $K_{S1} \rightarrow 0$ the bound fraction approaches the function $K/(1 + K)$ where K is affinity under the chain (Eq. 6). When $K_{S1} \gg 1$, binding is not inhibited, and the asymptotic form slightly exceeds $K_{S1}/(1+K_{S1})$ and therefore approaches unity more slowly. The overshoot is most pronounced for persistence lengths of the order of the actin site spacing ($\nu \approx 1$), and appears to be due to the neglect of triplet and higher-order interactions as defined by Eq. 11. This claim is substantiated by analyzing the behavior of the chain model for $\nu \leq 1$, when the range of myosin interaction is substantially limited to nearest neighbors (Fig. 2). In this case, the model is mathematically equivalent to a one-dimensional lattice gas with a one-particle energy $A - k_B T \ln K_{S1}$ and a nearest-neighbor pair energy $V^{(2)}(1/\nu) = -A_1$, for which an analytic solution exists (Baxter, 1982). The correct partition function per site is the maximum eigenvalue of the transfer matrix

$$
\mathbf{T} = \begin{pmatrix} K_1 & K \\ 1 & 1 \end{pmatrix}
$$

for $r = 1$ (see Eq. 15), from which the binding curve follows as before. This nearest-neighbor model also generates an overshoot effect but only when $\nu > 0.58$, for which $A_1 >$ A/2 (Fig. 2). This condition relates to the change in Gibbs energy, $A - k_B T \ln K_{S1} - 2A_1$, when myosin binds to a single vacant site between occupied sites—the overshoot that occurs when $\nu > 0.58$ is a consequence of lowering the chain energy by $2A_1 - A > 0$. However, when the chain energy is not approximated by a sum of pair interactions, it is clear that adding one more myosin always increases the distortion energy of the chain. Thus the overshoot effect is a consequence of the neglect of triplet and higher-order interactions.

The chain model also shows an opposing effect at small ν which is not an artifact of the pair approximation; with the interaction potential in Fig. 2, the chain is unable to open fully for a single actin site between two bound myosins. This effect changes the expected high-affinity binding law from $K_{S1}/(1 +$ $K_{\rm S1}$) to $K_1/(1 + K_1)$ where $K_1/K_{\rm S1} = \exp\{-\beta[A + V^{(2)}(1)$ $[v] \leq 1$. Taken together, these effects imply that the secondorder affinity K_{S1} cannot be correctly estimated from experimental binding curves by fitting the high concentration region to $K_{S1}/(1 + K_{S1})$. Rather, the whole curve should be fitted to Eq. 20 or its counterpart for the tropomyosin-troponin system. The reliability of the pair approximation can then be assessed by the degree of overshoot.

It is desirable to have a general method for characterizing cooperative binding curves, without invoking a specific model. The value of K_{S1} at the point of inflection in the

binding curve can be interpreted as a switching affinity K_{*} . However, the slope of the curve at this point reflects the degree of binding as well as the tightness of the switch and is therefore not a unique measure of cooperativity. One approach is to construct a Hill plot (Hill, 1913), which is based on the approximate binding fraction $x^n/(1 + x^n)$ where $x \propto K_{\text{S1}}$ in this context. Hill plots for the binding curves of Fig. 4 are shown in Fig. 5. Each plot has a characteristic sigmoidal shape, so that the slope is not constant but varies with K_{S1} . In fact $n \approx 1$ at low and high values of K_{S1} , reflecting first-order binding kinetics with or without inhibition, whereas larger values are found in the switching region $K_{S1} \sim K_{*}$. The customary definition of the Hill coefficient, as the slope at half activation (zero ordinate), underestimates the maximum slope if $K_* \, < 1$, and in this article the Hill coefficient is defined as the maximum slope of the Hill plot. Even so, the Hill coefficients from Fig. 5, A and B generally underestimate the persistence number ν , which is the basic measure of cooperativity in the present model, and a different kind of data analysis is required.

A general method for quantifying the degree of cooperativity in an autocooperative binding curve is presented in the Appendix. Cooperative binding curves which switch from one affinity to another as a function of enzyme concentration x can be characterized by deriving an associated switching function $F(x)$. The point of inflection of this function determines the switching concentration x_* and the corresponding affinity K_{\ast} . The slope S_{\ast} at this point is a useful index of cooperativity if $1/\tilde{K}_{S1}$ is used as the unit of concentration. The relationship between the switching parameters K_*, S_* and the parameters A, ν of the continuousflexible-chain model are tabulated in this Appendix. In particular, the empirical relation $\nu \approx S_*$ (Eq. A4) is usually accurate to within 10%. The same method also extracts the apparent second-order affinity at high concentrations, which falls below K_{S1} at small persistence numbers as expected.

FIGURE 5 Hill plots corresponding to Fig. 4 for the bound myosin fraction θ against myosin affinity K_{S1} . The Hill coefficient $n_{\rm H}$, defined as the maximum slope of the Hill plot, is generally less than the persistence number ν ($n_{\rm H}$ = 1.1 and 1.9 for ν = 1 and 5, respectively, in A) but also increases with kink energy A (n_H = 2.6 and 3.8 for ν = 1 and 5 in B). The persistence number is better estimated from the binding curves by the method described in the Appendix. The plots are indexed as described under Fig. 4.

When \vec{A} is zero, myosin affinity for actin is not inhibited by the chain, and the bound fraction is equal to $K_{S1}/(1 +$ K_{S1}). This result is duplicated numerically as $A \rightarrow 0$. However, the calculation is technically invalid when $A =$ 0 because the transfer matrix then has rank r , the top row being K times the sum of the remaining rows.

The model predicts that the extent of myosin binding depends on free myosin concentration [S1] and second-order affinity K_{S1} only through their product $K_{S1} = K_{S1} [S1]$ (the first-order affinity). For specific proteins, the second-order affinity is fixed and titrations are performed against [S1], but the theory applies equally to the binding of different myosins at the same concentration. For this reason, model curves are plotted against K_{S1} . The second-order affinity refers to binding at high concentrations, in the absence of inhibition.

EXPERIMENTAL BINDING CURVES

Myosin binding data for various regulated actin systems have been fitted by the CFC model. As this data has already been fitted by the rigid-regulatory-unit model of McKillop and Geeves (1991), it is convenient to discuss the fits in relation to the parameters of this model, namely K_T (equilibrium constant between closed and open states) and n_U (number of actin sites per unit). Numerically, K_T tracks the Boltzmann factor $exp(-\beta A)$ of the chain model, although the latter quantity is usually larger. If the regulatory unit is equivalent to a single chain kink in the CFC model, then $n_U = 2\nu + 1$. In fact, this condition is not observed and the comparison highlights an essential difference between the models.

Skeletal tropomyosin

Fig. 6 A shows myosin-S1 binding curves of Maytum et al. (1999) against free S1 concentration to actin-Tm and actin-Tm-Tn filaments, and fitted curves generated from Eq. 20. The fitting process was well-conditioned and gave unique optimum values of the three adjustable parameters K_{S1} , A and ν , summarized in Table 2. Myosin kink energy A is typically 1.6 k_BT , so exp($-\beta A$) = 0.22 compared with K_T = 0.15. Both curves are fitted by similar values of the secondorder affinity K_{S1} in the absence of chain distortion. The persistence length is increased by adding troponin if calcium is present at 0.1 mM or more. The corresponding kink sizes, namely 6.5 and 8.4 for A-Tm and A-Tm-Tn+Ca respectively, should be compared with unit sizes of 7 and 11 from the rigid-unit model.

The fits show that the persistence length of the tropomyosin chain is increased by troponin, but not to the extent indicated by the McKillop-Geeves model. This may be due to the dynamic nature of chain kinks in the CFC model. Kink size $2\nu + 1$ and unit size n_U should be equal only at low myosin concentrations where bound myosins are well separated and their associated kinks do not overlap. At higher concentrations, myosin kinks begin to overlap and the

FIGURE 6 Experimental myosin binding curves versus free S1 concentration for regulated actin systems and curves of best-fit to the CFC model. (A) from skeletal muscle (Maytum et al., 1999) and (B) from nonskeletal actin-tropomyosin filaments as listed (Maytum et al., 2001). Fitting procedures and values of fitted parameters are given in Table 2. For filaments from smooth muscle, the data falls below the fitted curve at the highest concentrations used.

correlation length of the multipally kinked chain increases with the density of kinks. Thus the apparent unit size may correspond to a concentration-averaged correlation length. The dynamic nature of chain kinks implies that the discrepancy between these measures is bigger in systems with a high persistence length, as observed.

Other actin systems

Myosin binding data of Maytum et al. (2001) for actintropomyosin from smooth muscle and nonmuscle cells, which contain no troponin, are also fitted by the chain model. These systems use structurally different tropomyosins, which may be shorter than skeletal tropomyosin. A key assumption of the present model, that these molecules interact to form a continuous semiflexible chain, can be tested by using A-Tm constructs with a common actin structure and tropomyosins of different lengths.

Fitting parameters and goodness-of-fit for myosin binding curves of Maytum et al. (*1999, [†]2001) for various actin-tropomyosin systems, fitted to Eq. 20. Least-squares fitting was performed with the Levenberg-Marquardt method. Fits were made to raw data as shown and to data filtered by averaging both coordinates over a centered running window of 50 points. Fitted parameter values were not significantly affected by filtering, but listed values of χ^2/N (chisquared per data point) are for filtered data, relative to a standard deviation of 0.02 for raw data points. Bracketed values of the kink size were obtained by weighted fitting in favor of the lowest S1 concentrations, which did not change the fitted values of K_{S1} and A. Where bracketed values are not given, weighted and unweighted fits gave the same results. Values of K_{S1} have not been corrected for the overshoot effect described in the main text.

Fitted binding curves for tropomyosins from smooth muscle, fibroblasts, and two kinds of yeast tropomyosin are shown in Fig. 6 B; the fitted parameters are also in Table 2. In contrast to skeletal tropomyosin, we find kink sizes significantly greater than the length of the tropomyosin molecule in all four systems, and especially for smooth-Tm and fibroblast-Tm where the kink size is almost twice the monomer length. Thus, actin-tropomyosin systems exist where the tropomyosins behave as a continuous semiflexible chain.

In these systems also, the kink size obtained from the CFC model generally tracks the unit size obtained from the rigidunit model (Table 2; see also Maytum et al., 2001). There is also a general correlation between values of $exp(-\beta A)$ from myosin kink energy A and the closed-to-open equilibrium constant K_T of the rigid-unit model; both quantities are two to three times bigger for yeast-Tm relative to skeletal-Tm, although the kink sizes (and unit sizes) are similar. In the CFC model, the reduced value of A for yeast-Tm can be produced by a 25% drop in kink angle ϕ_+ , say by 5–7°. As the myosin binding interface is the same in both systems, this shift implies that the resting position ($\phi = 0$ in Fig. 1 B) of the chain in yeast actin has shifted slightly toward the inner domain. Cryo-EM studies (Lehman et al., 2000) suggest that there is no shift in resting orientation. However, Table 2 predicts a similar small shift toward the inner domain for smooth-muscle Tm, whereas Lehman et al. (2000) report a large shift toward the outer domain. This discrepancy may have a structural explanation, but the available binding data for smooth-Tm was less well fitted (see text under Table 2), and for this system the value of A may be unreliable.

Myosin binding data of Tobacman and Butters (2000) for mutant tropomyosins with internal deletions suggests that myosin kink energy has been raised, perhaps because of a shift in the resting orientation of the chain toward the outer domain of actin. Their binding curves for mutant and wild-type tropomyosins should be compared with

those in Fig. 4, B and A respectively, with the same value of ν . Fitting the CFC model to their data should reveal whether the persistence length is also altered by these mutations.

In general, the fitted binding curves overshoot the curve $K_{S1}/(1 + K_{S1})$ expected in the absence of inhibition, by 1.5– 3% at $K_{S1} = 4$. We have argued that this effect is an artifact of the model, produced by the neglect of chain-induced interactions between bound myosins not reducible to pair interactions. Hence the best-fit value of the second-order affinity K_{S1} should be corrected upwards so that the hyperbola $K_{S1}/(1 + K_{S1})$ does not lie below the measured binding curve; this procedure gives affinity corrections of the order of 10% for the data presented here. It is desirable to predict myosin binding curves from the chain model without invoking the pair approximation. The inclusion of triplet interactions complicates the transfer-matrix approach considerably and a different methodology may be required; this task should be addressed in the future.

In conclusion, the CFC model is able to generate similar results to the rigid-unit model for the binding of S1 to regulated actin systems. In addition, the optimum values of fitted parameters appear to be consistent with thin-filament structure within the assumption of a continuous semiflexible tropomyosin chain.

DISCUSSION

Any discussion of the merits and predictive power of models of thin-filament regulation inevitably reverts to the structural assumptions underlying each model. The structural motivation for the CFC model is given in the Introduction and under Fig. 1. As the key assumption of this model (that tropomyosins act as a continuous semiflexible chain which fluctuates about a single resting position in the absence of myosin and troponin) runs counter to all previous regulatory

models, a closer look at the evidence is desirable before returning to the models themselves.

The structural basis of regulatory models

The steric blocking model of Haselgrove and Huxley supposed that individual tropomyosin molecules switched between two discrete orientational states on actin, and did not determine whether these regulatory units switched independently or not. Two discrete orientations are observed but under different conditions: the closed state is observed in the absence of myosin and the open state in the presence of enough bound myosin to force all tropomyosins open. This observation does not imply that each unit has two possible resting orientations in the absence of myosin, as assumed by all previous models except the alternative model of Hill et al. (1980b). The observation of a third orientation, in the Tm-Tn-Ca system only (Vibert et al., 1997), appears to confirm the model of McKillop and Geeves (1993) in which three orientational states of tropomyosin are always present, with myosin and calcium (through troponin-I) acting as allosteric effectors by changing the balance of equilibrium between them (Lehrer and Geeves, 1998). More recent cryo-EM studies of various actin-tropomyosin systems with no troponin reveal only a single resting orientation; however, this orientation may vary significantly with troponin and actin isoforms (Lehman et al., 2000). Studies of filaments sparsely decorated with myosin show a gradual shift in tropomyosin position toward the closed state on moving away from the border of a myosin-decorated area, as far as 100 nm (Vibert et al., 1997). The spatial persistence of this effect is larger than the persistence lengths estimated in this article, perhaps because of hidden myosins. Similar effects are found in x-ray diffraction studies of the thin filament in vertebrate muscle stretched to zero overlap (Poole et al., 1995, 1996). The corresponding effect on moving away from a bound troponin-I has been reported by Lehman et al. (2001). Thus there is reasonable evidence for a single resting orientation of tropomyosin on actin, but with the capacity to depart from that orientation by $10-20^\circ$ in either direction in the presence of bound myosin or troponin-I. On the other hand, a double orientational potential well, with minima separated by an energy barrier of order k_BT , cannot be ruled out.

Evidence for semiflexible rather than rigid tropomyosins, and for the end-to-end interactions required to make a chain, is given in the Introduction. In fact, the observed flexibility of polymeric Tm in solution implies a bending stiffness at the lower end of values quoted in this article. It is possible that tropomyosin is stiffened by electrostatic interactions with actin, in addition to the postulated confining potential in Eq. 1. If end-to-end interactions are interpreted as an elastic link, the resulting chain will appear homogeneous if the bending stiffness of the link is similar to that between tropomyosin residues. With troponin present, this may be achieved by end-to-end interactions via troponin-T, which also links the

other components of troponin to tropomyosin and is required for activation (Greaser and Gergely, 1971). The validity of the CFC model for tropomyosin-only systems is less clear, but is supported by comparing estimated kink sizes in systems with tropomyosins of different length, as discussed in the previous section.

Weakly-bound actomyosin states (Chalovich et al., 1991) have not been incorporated in the chain model. This was done for simplicity, and because these states are not populated at the low myosin concentrations used for titrations. Nevertheless, a weakly-bound actin-myosin-products state may be an intermediate in the ATP-hydrolyzing actin-myosin cycle, and one can ask how it would be affected by tropomyosin in the present model. Atomic reconstructions of the actin-myosin interface suggest that weak-binding regions lie at negative angles in Fig. 1 B, not substantially covered by tropomyosin in its thermal fluctuations $\sim \phi = 0$, whereas the strongbinding interface requires additional contacts over a wider range of angles of both sign (Holmes, 1995; Hodgkinson et al., 1997), requiring myosin to skew as well as tilt axially in the force-generating transition (Corrie et al., 1999). Thus, only strongly-bound myosin states are inhibited by tropomyosin in the closed state of the CFC model, as assumed by McKillop and Geeves for the closed state of the rigid-unit model. In the presence of a more strongly-bound final state, as expected for nucleotide-free myosin and myosin-ADP (Geeves, 1991), the weakly-bound state will not be populated significantly and its omission should not be significant.

The quadratic angular confining potential used in Eq. 1 is necessary for mathematical developments and is intended only as a parody of orientational confinement of tropomyosin by electrostatic interactions, which also provide radial confinement. Hence the CFC model does not address tropomyosin binding data, in particular the observation that the binding of vertebrate tropomyosin to actin is increased fourfold by one bound myosin-S1, or 4^7 -fold when all seven sites are occupied (Tobacman and Butters, 2000). This suggests that when myosin binds to regulated actin, it captures the tropomyosin chain at a point of contact after displacing it to the open position (Fig. 1), leaving it pinned to actin rather than free to make larger displacements; in fact this assumption was made in developing the model. The related observation that myosin-S1 binds four times more strongly to actin-tropomyosin than unregulated actin implies only that the second-order myosin affinity K_{S1} of the model is not transferable to unregulated actin. An operational definition may not be available, since K_{S1} was defined in the absence of chain distortion and the chain must distort to allow myosin binding at low density.

Outlook

The form of the myosin binding curve against myosin concentration does not provide a complete test of the CFC model, and can generally be fitted by all current models.

FIGURE 7 Derivative of the switching function $F(K_{+})$ of the Appendix, computed for the chain model with $A = 1.5 k_B T$. The abscissa is defined as $K_{+} = \tilde{K}_{+}$ [S1] where the apparent second-order affinity \tilde{K}_{+} is determined numerically as described in the Appendix. For each value of the persistence number ν , the inset table gives the coordinates K_{*,S^*} of the maximum, which characterize the cooperative binding curve, and K_+ . When $\nu > 2$, S* is very close to ν . The values of K_{+} are within 2% of those predicted by the expression exp $\{-\beta[A + V^{(2)}(1/\nu)]\}.$

Better tests are posed by 1), the calcium dependence of myosin binding, which requires an explanation of its high cooperativity and asymmetry as observed in the muscle fiber; and 2), the calcium dependence of calcium binding to TnC, which is more cooperative when the troponin complex is bound to tropomyosin on actin and more cooperative again with bound myosin present. These tests are addressed in the accompanying article.

The available models can be ranked in order of complexity, both conceptual and numerical (more complex models generally contain more parameters). The McKillop-Geeves model, despite its use of three regulatory states, is perhaps the simplest as it divides the tropomyosin assembly into independent rigid units, using four parameters in general

and three parameters for A-Tm and A-Tm-Tn+Ca systems; in its current form this model does not make predictions as a function of calcium level. The model of Hill, Eisenberg, and Greene (1980a) has only two regulatory states, equivalent to the closed and open states of the preceding model, and identifies the tropomyosin molecule as the rigid regulatory unit, but invokes state-dependent and calciumdependent interactions between units, requiring 17 parameters in all. This model has been applied to a variety of experiments. Motivated by the modulation of actin-myosin affinity by tropomyosin, the recent model of Tobacman and Butters (2000) adds complexity by postulating a cooperative conformational change in the actin filament. This fourparameter model also fits myosin binding curves for different filament systems.

What level of complexity in a mechano-kinetic model is desirable? One way of answering the question is by reference to molecular structure. In this sense, a model with independent regulatory units is inadequate when the unit size does not match the tropomyosin molecule. The CFC model is able to deal with filament systems with shortened tropomyosins and show that the regulatory unit can be dynamically determined and unrelated to the length of the tropomyosin molecule. The Hill-Eisenberg-Greene models apparently require calcium-dependent end-to-end tropomyosin interactions which cannot easily be interpreted in terms of known interactions between calcium, TnC and TnT. Devising mechanokinetic models which encapsulate key features of the wealth of structural information on these proteins will continue to be a major challenge.

On the other hand, the CFC and Tobacman-Butters models have not been tested against a sufficient variety of experiments. The CFC model needs to be developed further to explore kinetic aspects of thin filament regulation, which has been treated empirically by Razumova et al. (2000). The time courses of myosin binding and tropomyosin movements in A-Tm-Tn have been interpreted in terms of a regulatory

FIGURE 8 Contour maps for the switching variables $K_*(A,\nu)$, $S_*(A,\nu)$ of the Appendix, computed for the chain model as functions of its parameters A and ν .

unit of 10–12 monomers moving between discrete orientations (Geeves and Lehrer, 1994), but a similar kink size in the CFC model might not be necessary.

APPENDIX: A SWITCHING FUNCTION FOR AN AUTO-COOPERATIVE BINDING CURVE

Suppose an enzyme M binds auto-cooperatively to a substrate, so that M binds with low affinity at a low concentration of M and binds with high affinity at high concentration. We seek to characterize this transition by a switching function $F(x)$ which ranges from zero at low x to unity at high x, where $x = [M]$. The essential parameters of this function are the switching concentration x^* at which $F(x)$ has a point of inflection, and the slope S^* at this point. x_* is an inverse measure of the sensitivity of the transition to enzyme concentration. S^* measures intrinsic cooperativity, and $1/S^*$ is the range of concentrations over which switching occurs. In the context of this article, the motivation for constructing a switching function is to estimate the parameters of the chain model from a given binding curve without fitting to the model.

An auto-cooperative binding curve, which switches from a weak binding form with affinity \tilde{K}_{-} at small x to a strong binding form with affinity \tilde{K}_{+} at large x , can be described by the function

$$
\theta(x) = (1 - F(x)) \frac{\tilde{K}_{-x}}{1 + \tilde{K}_{-x}} + F(x) \frac{\tilde{K}_{+x}}{1 + \tilde{K}_{+x}}, \quad (A1)
$$

where $F(x)$ is a function which switches smoothly from zero for $x \ll x^*$ to unity for $x \gg x^*$. The binding curves predicted by our model are of this form. The switching function for a given binding curve can be calculated by the following procedure. An empirical partition function is first constructed numerically from the integral form

$$
\lambda(x) = \exp\left(\int_0^x \frac{\vartheta(x')}{x'} dx'\right) \tag{A2}
$$

of Eq. 18, where $\lambda(0) = 1$. The expected forms of $\lambda(x)$ at low and high concentrations are straight lines of slopes K_{\pm} , which can be extracted graphically once asymptotic straight-line behavior has been established. The point of maximum slope locates the switching concentration x^* . The maximum slope S^* of $F(x)$ is a useful measure of cooperativity if defined with respect to a dimensionless unit of concentration, such as first-order affinity. For this purpose, $F(x)$ should be plotted against the first-order affinity $K_{+} = \tilde{K}_{+}x$ and S_{*} defined as the maximum value of dF/dK_{+} .

The switching function has been calculated for modeled and experimental myosin-S1 binding curves. We describe results for the model curves of Fig. 4 A. For this purpose, it is convenient to set $x = K_{S1}$ rather than [S1], which is equivalent to setting $K_{S1} = 1$. Figure 7 shows the resulting plots of dF/dK_{+} and values of the switching parameters K_{*} , S_{*} . Their relation with the parameters A, ν of the chain model is shown graphically in Fig. 8, which enables the latter to be determined numerically. The empirical relations

$$
K_*(A,\nu) \approx \frac{4\beta A}{3\beta A + 8\nu}, \quad S_*(A,\nu) \approx \nu
$$
 (A3)

are generally accurate to 10%, though the second equation is unreliable when $\beta A > 2$.

Values of K_{\pm} determined by this procedure were in good agreement with those predicted from the expressions $K = \exp(-\beta A)$ and $K_+ =$ $exp{-\beta[A+V^{(2)}(1/\nu)]}$. The latter is generally close to unity except when $\nu \approx 1$ and/or $\beta A > 2$, when the chain is unable to open fully for actin sites next to an occupied site. Thus K_{+} is only a lower estimate for the fundamental second-order myosin affinity K_{S1} , although the difference is usually small if $\nu > 2$.

Biophysical Journal 84(5) 3155–3167

A Fortran program for generating the switching function and values of K_{\pm} , K_{\ast} , S_{\ast} from an experimental binding curve is listed on the website mentioned at the end of the Introduction.

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