

# Mammalian cell survival and processing in supercritical CO<sub>2</sub>

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We demonstrate that mammalian cells can survive for 5 min within high-pressure CO<sub>2</sub>. Cell survival was investigated by exposing a range of mammalian cell types to supercritical CO<sub>2</sub> (scCO<sub>2</sub>) (35°C, 74 bar; 1 bar = 100 kPa) for increasing exposure and depressurization times. The myoblastic C2C12 cell line, 3T3 fibroblasts, chondrocytes, and hepatocytes all displayed appreciable but varying metabolic activity with exposure times up to 1 min. With depressurization times of 4 min, cell population metabolic activity was ≥70% of the control population. Based on survival data, we developed a single-step scCO<sub>2</sub> technique for the rapid production of biodegradable poly(DL-lactic acid) scaffolds containing mammalian cells. By using optimum cell-survival conditions, scCO<sub>2</sub> was used to process poly(DL-lactic acid) containing a cell suspension, and, upon pressure release, a polymer sponge containing viable mammalian cells was formed. Cell functionality was demonstrated by retention of an osteogenic response to bone morphogenetic protein-2 in C2C12 cells. A gene microarray analysis showed no statistically significant changes in gene expression across 4,418 genes by a single-class *t* test. A significance analysis of microarrays revealed only eight genes that were down-regulated based on a  $\delta$  value of 1.0125 and a false detection rate of 0.

biodegradable polymer | bone | scaffolds

Standard methods of combining mammalian cells and synthetic polymers for biotechnological applications (1–3) must minimize disruption to the cell component from fluctuations in solvent composition, temperature, pressure, and shear forces (4, 5). However, processing synthetic polymers by conventional routes requires organic solvents, elevated temperatures or pressures, and sometimes mechanical agitation to produce the required 3D form (6, 7). For this reason, an inefficient two-step process is required to generate the prefabricated polymer structure, with the cell component seeded as a second step (8).

One method for generating macroporous, biodegradable scaffolds is by using high-pressure or supercritical CO<sub>2</sub> (scCO<sub>2</sub>) processing. This technique is solvent-free and has been used for the fabrication of tissue engineering and drug delivery devices because of a number of processing advantages (9, 10). When CO<sub>2</sub> is raised above the critical pressure and temperature (31.2°C, 73.8 bar; 1 bar = 100 kPa), it forms a phase with the characteristics of both a liquid and a gas with selective solvent power and high diffusivity (11). It is then able to penetrate into the amorphous regions of polymers, such as poly(DL-lactic acid) (P<sub>DL</sub>LA), liquefying them at near ambient temperatures. Release of the pressure results in the nucleation of gas bubbles within the polymer, which become permanent upon solidification, creating a reticulated porous structure (9).<sup>||</sup> As a result, scaffold fabrication is possible without introducing high temperatures or organic solvents. This fact has made it possible for sensitive biological molecules, such as protein drugs, to be incorporated into polymeric-controlled release matrices during fabrication (12, 13). This method has already been tailored and

used with bone morphogenetic protein-2 (BMP-2), stimulating the formation of bone tissue *in vivo* (14).

We hypothesized that a similar one-step scCO<sub>2</sub> processing technique might be used to produce biodegradable foams containing mammalian cells. The rapid plasticization and subsequent foaming of P<sub>DL</sub>LA by scCO<sub>2</sub> could limit the required survival time for mammalian cells within supercritical conditions to <5 min. However, the retention of cell viability and functionality after exposure to high-pressure CO<sub>2</sub> and rapid decompression could be problematic, because other supercritical fluid processes have been used for bacterial cell inactivation (15, 16).

A number of mechanisms have been proposed to explain high-pressure CO<sub>2</sub> sterilization, including cell membrane rupture caused by the increase in internal pressure combined with rapid pressure release (17, 18) and the extraction of lipids from the cell membrane (19). Equally, scCO<sub>2</sub> diffusion into the cell and the resultant changes in the cellular environment, such as a decrease in pH, could be lethal (17). As a result of this sterilizing power, subcritical CO<sub>2</sub> and scCO<sub>2</sub> has been used to inactivate bacterial cells and spores when injected into poly(lactic acid) for medical sterilization (17) and for sterilization of food stuffs (20). Even short exposure times (150 sec) to CO<sub>2</sub> at just above its critical point (38°C, 74 bar) are sufficient to inactivate both Gram-negative and Gram-positive bacteria (21).

Therefore, we had four main objectives: (i) to process mammalian cells in scCO<sub>2</sub> and high-pressure N<sub>2</sub> to determine the effects of pressure, exposure time, and processing medium on cell survival; (ii) to investigate the effects of scCO<sub>2</sub> on important aspects of gene expression; (iii) to measure cell functionality by quantifying the ability of a scCO<sub>2</sub>-treated cell line to differentiate in response to growth factors; and (iv) to show cell viability, functionality, and location after combining cells and P<sub>DL</sub>LA into a single construct.

## Results

**Cell Survival After scCO<sub>2</sub> Processing.** The metabolic activity of cell populations after a 10-sec exposure at maximum pressure and 40-sec depressurization, in comparison with untreated controls, was >80% for all cell types (>90% for C2C12 cell line) (Fig. 1A). Cell survival remained at 50% or greater for all cell types at a 1-min exposure to maximum pressure and a 40-sec depressur-

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Abbreviations: AP, alkaline phosphatase; BMP-2, bone morphogenetic protein-2; LDH, lactate dehydrogenase;  $\mu$ CT, microcomputed tomography; P<sub>DL</sub>LA, poly(DL-lactic acid); *p*-NPP, *p*-nitrophenyl phosphate; scCO<sub>2</sub>, supercritical CO<sub>2</sub>; SEM, scanning electron microscopy.

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analysis of four samples that were independently exposed to scCO<sub>2</sub> confirmed that very few changes in gene expression were induced by the high-pressure CO<sub>2</sub> environment and rapid pressure fluctuations. Of eight genes that were significantly down-regulated, survivin, clast4 protein, and glutathione *S*-transferase could play a role in a biochemical response from the cell to the extreme changes in environment. Survivin is a component of the chromosomal passenger complex that acts as an inhibitor of apoptosis (24). Down-regulation of survivin is the only marker of an apoptotic response we have recorded.

Combining the polymer phase and the cells within scCO<sub>2</sub>, with a 30-sec exposure time to a maximum pressure of 74 bar and a depressurization time of 40 sec, generated macroporous scaffolds with cells distributed throughout the 3D matrix. Mixing of the cell and polymer components was achieved by combining a fine powder of the polymer and concentrated suspension of the cells. The cells within the scaffold were found to be viable, and C2C12 cells retained the ability to respond to BMP-2. Therefore, a composite structure of biodegradable polymer and mammalian cells could be formed through a process that was completed within 5 min to generate a viable, evenly distributed cell population that was able to differentiate within a porous scaffold.

### Conclusion

This study demonstrates that mammalian cells in suspension are able to survive exposure to scCO<sub>2</sub> for sufficient time periods to plasticize and foam P<sub>D</sub>LA. After exposure to scCO<sub>2</sub> and rapid depressurization, cells demonstrated high-population metabolic activity and retention of important aspects of functionality. However, although some cell death did occur, the rate of cell death was higher in CO<sub>2</sub> than in N<sub>2</sub>, and there is evidence of some mechanical disruption of the cell population. The effects of scCO<sub>2</sub> on relative gene expression were minimal in the C2C12 cell line, with small down-regulations of survivin, clast4 protein, and glutathione *S*-transferase providing some evidence of subtle changes at the mRNA level that do not lead to significant apoptosis. Overall, it can be concluded that scCO<sub>2</sub> can be used to process cells into polymer composite structures.

### Materials and Methods

**Equipment and Chemicals.** Food-grade CO<sub>2</sub> was supplied by Cryo-Service (Worcester, United Kingdom), N<sub>2</sub> was provided by BOC Industrial (Surrey, United Kingdom), and P<sub>D</sub>LA (Mw 52,000) was supplied by Purac (Birmingham, United Kingdom). The process was controlled by using a Bronkhorst (Cambridge, United Kingdom) High-Tec BV series flowmeter as a backpressure regulator. The recombinant human BMP-2 was kindly manufactured and supplied by Walter Sebald (Biozentrum der Universität Würzburg, Am Hubland, Würzburg, Germany).

**Isolation and Culture of Primary Cells.** Fibrochondrocytes were isolated from the ovine knee joint meniscus by using a method adapted from Collier and Ghosh (25). Tissue was diced into 2-mm<sup>3</sup> cubes, and pronase E (VWR International, Leicestershire, United Kingdom) and type II collagenase (Lorne Laboratories, Reading, United Kingdom) were used to enzymatically digest the cells from the tissue. Cells were cultured in DMEM supplemented with 10% FCS, 2% nonessential amino acids, and 2% L-glutamine containing penicillin (100 units/ml), streptomycin (100 μg/ml), and amphotericin B (250 ng/ml) (Sigma). Hepatocytes were isolated from healthy rat liver by using a method modified from Seglen (26). Complete medium for hepatocytes contained Williams medium E (Invitrogen) supplemented with 10% FCS and 20 mM L-glutamine and containing penicillin (100 units/ml), streptomycin (100 μg/ml), and amphotericin B (250 ng/ml) (Sigma).

**Secondary Cell Line Culture.** The murine 3T3 and C2C12 cell lines were cultured in DMEM supplemented with 10% FCS, 2% nonessential amino acids, and 2% L-glutamine and containing penicillin (100 units/ml), streptomycin (100 μg/ml), and amphotericin B (250 ng/ml) (Sigma). C2C12 cells were passaged before attaining 70% confluence to avoid spontaneous differentiation to muscle (myoids).

**Processing Cells in scCO<sub>2</sub> and High-Pressure N<sub>2</sub>.** Cells were suspended in 200 μl of complete medium and placed into custom-made poly(tetrafluoroethylene) eight-well tissue culture chambers at 2 × 10<sup>5</sup> cells per well. Cells were processed inside a 60-ml stainless steel pressure vessel at an operating pressure of 74 bar at 35°C. Cells were processed at maximum pressure from 10 sec to 3 min with an additional 80 sec required to pressurize and depressurize the vessel by using sensitive backpressure regulation. This procedure was then repeated with N<sub>2</sub> in place of CO<sub>2</sub> by using C2C12 cells and exactly the same processing conditions to show any specific effects that CO<sub>2</sub> may have on cell survival. After processing, the cells were resuspended in 1 ml of complete DMEM and incubated for 24 h in a 48-well tissue culture plate (Falcon) before further analysis. To test the effects of a less rapid pressure release, 3T3 fibroblasts were subject to increasing depressurization times of up to 7 min after being held at maximum pressure for 1 min.

**Metabolic Activity of scCO<sub>2</sub> and High-Pressure N<sub>2</sub>-Processed Cells.** To measure metabolic activity, medium was aspirated and replaced by 1-ml solution of 10% AlamarBlue solution (vol/vol; Serotech) in phenol red-free Hank's buffered saline solution (Sigma). The cells were incubated for 90 min before 200 μl of solution from each well was transferred to a 96-well plate (Falcon). Fluorescence readings were then obtained at an emission wavelength of λ590 nm by using λ560 nm excitation.

**LDH Assay for Damage to Cell Membrane.** C2C12 cells were exposed to scCO<sub>2</sub> in DMEM (without phenol red and FCS) for increasing exposure times (as in survival experiments), and the cytosolic LDH released was measured to indicate the extent of damage to the cell membrane. Cells were removed by centrifugation for 2 min (1,000 rpm; 3K15; SciQuip, Freehold, NJ), and 100 μl of the DMEM supernatant was assayed for release of LDH by using an equal volume of the LDH substrate/dye reaction mixture in a 96-well plate (Roche). Absorbance readings were detected at λ490 nm.

**ELISA for Apoptosis Detection.** C2C12 cells were exposed to increasing scCO<sub>2</sub> exposure times (as in previous experiments) before subsequent culture for 3 h more in fresh medium (so as to observe apoptosis rather than cell mechanical damage). The cells were then assayed for histone-associated DNA fragments indicative of apoptosis through the Cell Death Detection ELISAPLUS (Roche), which was used per the manufacturer's instructions. Briefly, cells from each processing cycle were lysed by using the provided buffer and centrifuged (200 × *g* for 10 min), and 20 μl of the lysate supernatant was added to a streptavidin-coated ELISA plate. Eighty microliters of the immunoreagent (containing the enzyme-linked antibody) was added to each well, and the plate was incubated at room temperature (for 2 h). The solution was then removed from each well and replaced with 100 μl of a 2,2'-azino-di-(3-ethyl)benzthiazoline-6-sulfonic acid (ABTS) solution before a 20-min incubation to allow the color to develop in the sample wells. Absorbance was detected at λ490 nm.

**Preparation of RNA and Hybridization.** After processing for 1 min at 74 bar and 35°C, murine C2C12 cells were cultured for 3 h more in complete medium. Cells were then rinsed in PBS and homogenized in an RNeasy lysis buffer containing 2-mercaptoethanol

(10  $\mu\text{l/ml}$ ). Total RNA content of the cell homogenate was assessed by using the RNeasy kit (Qiagen, Hilden, Germany) according to the manufacturer's instructions. Slides were Oci-Chip 30K set A arrays, and indirectly labeled probes were generated from 5  $\mu\text{g}$  of total sample RNA with Ambion (Austin, TX) MessageAmp II amplification (per the manufacturer's protocols). The probes were labeled with Alexa 555 or 647 *N*-hydroxysuccinimide ester dyes (Invitrogen), and 0.5  $\mu\text{g}$  ( $\approx 40$  pM of dye label) of each was used for each channel of two-color hybridizations. Hybridizations were performed for 16 h on a TEcan HTS 4800 hybridization station with moderate agitation by using the Ocumum recommended solutions and temperatures.

**Microarray Analysis.** Arrays were scanned with a GenePix 4000B laser scanner, and primary data was obtained by using GENEPIX PRO 6.0 software (Axon Instruments, Union City, CA). Filtering of array data and normalization by using the LOWESS algorithm were performed within the University of Nottingham microarray database (a version of BASE Version 1.2.16; Lund University, Lund, Sweden). Further analysis was performed on this data set by using MULTIEXPERIMENT VIEWER (MEV) software (Institute for Genomic Research, Rockville, MD) and the statistical analysis of microarrays algorithm.

**Osteogenic Differentiation of  $\text{scCO}_2$ -Processed C2C12 Cells.** To assess cell function we studied the differentiation of C2C12 cells, which are shown to have multipotential nature dependent on the cell environment (23, 27, 28). The osteoblast lineage can be induced in the C2C12 cell line by BMP-2 (27), an indicator of which is AP activity (22, 23). Before osteogenic culture of C2C12 cells, they were processed the same way as above but then added into six-well plates (Falcon) cultured to 80% confluency (1–2 days) before the addition of 500 ng/ml recombinant human BMP-2 in 2% FCS-supplemented DMEM medium (29). For cells processed into porous scaffolds, the same culture technique was used. After supercritical processing, the cell-loaded scaffolds were cut into four pieces and cultured for 24 h in complete DMEM before the addition of 500 ng/ml recombinant human BMP-2.

**AP Activity.** As a measure of the osteogenic status of C2C12 cells, a red color substrate was precipitated on the cells by the action of cellular AP activity. The substrate system was comprised of Naphthol AS-MX buffer solution (Sigma) containing 1 mg/ml fast violet B salt, as described by Oreffo *et al.* (30). For measurement of AP activity, a *p*-NPP substrate system was used. Cell cultures were fixed in 75% ethanol for 10 min and homogenized in 600  $\mu\text{l}$  of distilled water containing 0.001% Tween detergent after three cycles of freeze-thawing. Values were compared against known *p*-NPP standards and matched to DNA content to compensate for changes in cell number. This step was repeated in triplicate over four experiments for osteogenically prompted C2C12 cells.

**DNA Assay.** DNA content was estimated by using Hoechst 33258 dye binding, as modified from a method described in ref. 31. In brief, cell cultures were fixed in 75% ethanol and homogenized in 600  $\mu\text{l}$  of distilled water containing 0.001% Tween detergent. Cell homogenate (50  $\mu\text{l}$ ) was added to a 96-well plate (Falcon), and 100  $\mu\text{l}$  of 2  $\mu\text{g/ml}$  Hoechst 33258 was added. Fluorescence was detected at an emission wavelength of 460 nm by using 360

nm excitation and compared with a series of DNA standards from 0 to 20  $\mu\text{g/ml}$ .

**Fabrication of Cell-Loaded  $\text{P}_{\text{DL}}\text{LA}$  Scaffolds by Using  $\text{scCO}_2$ .** One hundred milligrams of  $\text{P}_{\text{DL}}\text{LA}$  was mixed with  $2 \times 10^5$  of either osmium tetroxide-stained 3T3 fibroblasts for distribution analysis or with live C2C12 cells suspended in 200  $\mu\text{l}$  DMEM. Cells and  $\text{P}_{\text{DL}}\text{LA}$  were mixed together to produce a polymer/cell slurry within the well of a 1-cm-diameter cylindrical poly(tetrafluoroethylene) mould before processing. Polymer and cells were foamed into a scaffold by exposure to  $\text{scCO}_2$  (35°C, 74 bar) for 30 sec, with an additional 80 sec required to pressurize and depressurize the vessel. After processing, scaffolds were either kept for  $\mu\text{CT}$  analysis or cut into four equal pieces and incubated for 24 h in 2 ml of DMEM culture medium in a six-well plate (Falcon) for SEM, viability, and functionality assessment.

**$\mu\text{CT}$  Imaging of Cells Within Scaffolds.** C2C12 cells were fixed with 10% formal saline and then with 1% osmium tetroxide before being processed into  $\text{P}_{\text{DL}}\text{LA}$  scaffolds as previously described. The construct was imaged by using a high-resolution  $\mu\text{CT}$  system ( $\mu\text{CT}$  40; Scanco Medical, Bassersdorf, Switzerland). The scanner was set to a voltage of 55 kVp, a current of 145 mA. Samples were scanned at 8- $\mu\text{m}$  voxel (3D-pixel) resolution with an integration time of 120 ms to produce 3D reconstructed images. The cell-loaded scaffolds were thresholded at 60 (arbitrary) to view the porous scaffold and then at 190 to view the osmium-stained cells contained within.

**Metabolic Activity of Cell-Loaded  $\text{scCO}_2$ -Processed Scaffolds.** Both cell viability and location were assessed with the use of LIVE/DEAD stain (Molecular Probes). The cells and polymers were incubated in 10 ml of complete DMEM containing 20  $\mu\text{l}$  of ethidium homodimer-1 (to highlight the dead cells red) and 5  $\mu\text{l}$  of calcein acetoxymethyl ester (to highlight the live cells green) for 1 h. The cells were then rinsed (four times) in PBS for 1 h before being observed by using fluorescence microscopy (DM IRB; Leica, Deerfield, IL).

**Scaffold Histology.**  $\text{P}_{\text{DL}}\text{LA}$  scaffolds containing cells were prepared for histology by fixing in 70% methanol for 30 min, drying overnight, and subsequent infiltration with 65°C Paraplast wax (Sigma). Ten-micrometer sections were cut by using a microtome and observed by using a fluorescence microscope for either propidium iodide-stained nuclei to identify cell location or for LIVE/DEAD-stained cells to show cell activity within the scaffolds.

**SEM.** Cell-seeded (3T3 fibroblast) scaffolds were fixed in 8% glutaraldehyde for 24 h and prepared for SEM analysis by dehydration and further fixation with 1% osmium tetroxide. The scaffolds were then gold-coated by using a Balzers Union SCD030 sputter coater before being scanned at 20 kV with a Philips (Eindhoven, the Netherlands) 505 scanning electron microscope.

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