#### RAPID REPORT

# Kinetics of Mg<sup>2+</sup> unblock of NMDA receptors: implications for spike-timing dependent synaptic plasticity

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> The time course of Mg<sup>2+</sup> block and unblock of NMDA receptors (NMDARs) determines the extent they are activated by depolarization. Here, we directly measure the rate of NMDAR channel opening in response to depolarizations at different times after brief (1 ms) and sustained (4.6 s) applications of glutamate to nucleated patches from neocortical pyramidal neurons. The kinetics of  $Mg^{2+}$  unblock were found to be non-instantaneous and complex, consisting of a prominent fast component (time constant  $\sim 100 \ \mu s$ ) and slower components (time constants 4 and  $\sim$  300 ms), the relative amplitudes of which depended on the timing of the depolarizing pulse. Fitting a kinetic model to these data indicated that  $Mg^{2+}$  not only blocks the NMDAR channel, but reduces both the open probability and affinity for glutamate, while enhancing desensitization. These effects slow the rate of NMDAR channel opening in response to depolarization in a time-dependent manner such that the slower components of  $Mg^{2+}$ unblock are enhanced during depolarizations at later times after glutamate application. One physiological consequence of this is that brief depolarizations occurring earlier in time after glutamate application are better able to open NMDAR channels. This finding has important implications for spike-timing-dependent synaptic plasticity (STDP), where the precise (millisecond) timing of action potentials relative to synaptic inputs determines the magnitude and sign of changes in synaptic strength. Indeed, we find that STDP timing curves of NMDAR channel activation elicited by realistic dendritic action potential waveforms are narrower than expected assuming instantaneous Mg<sup>2+</sup> unblock, indicating that slow Mg<sup>2+</sup> unblock of NMDAR channels makes the STDP timing window more precise.

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Excitatory synaptic transmission at vertebrate central synapses is mediated primarily by the neurotransmitter glutamate. The resulting postsynaptic current typically consists of a fast component mediated by AMPA receptors and a slow component medicated by NMDARs (Forsythe & Westbrook, 1988; Bekkers & Stevens, 1989). Current flow through NMDAR channels is largely blocked by external Mg<sup>2+</sup> ions at resting membrane potentials, but can be relieved by depolarization (Mayer *et al.* 1984; Nowak *et al.* 1984). The voltage-dependent block and unblock of NMDAR channels by Mg<sup>2+</sup> is thought to be extremely rapid (Jahr & Stevens, 1990*a*,*b*), and is usually assumed to be effectively instantaneous. A recent study, however, indicates there is a slow component to Mg<sup>2+</sup> unblock of NMDAR channels (Vargas-Caballero &

Robinson, 2003), which may have important physiological implications.

NMDARs receptors play a key role in the induction of many forms of synaptic plasticity (Bliss & Collingridge, 1993). As NMDARs are largely blocked by  $Mg^{2+}$  at resting membrane potentials, the kinetics of  $Mg^{2+}$  unblock of NMDAR channels will influence NMDAR activation during synaptic plasticity induction. This is likely to be particularly important during spike-timing dependent plasticity (STDP), where the coincidence of EPSPs and action potentials (APs) within a brief time window determines the magnitude and sign of changes in synaptic strength (Markram *et al.* 1997; Bi & Poo, 1998). In cortical pyramidal neurons APs are brief events which attenuate as they propagate back into the dendritic tree (Stuart *et al.* 1997). Hence, the ability of backpropagating APs to activate synaptic NMDARs, and so control calcium influx through the NMDAR channel, will be critically dependent on the time course of  $Mg^{2+}$  unblock. Here, we directly investigate the kinetics and time dependence of  $Mg^{2+}$  unblock of NMDARs during rapid applications of glutamate to nucleated patches from cortical layer 5 pyramidal neurons. In addition, we provide a kinetic model that can explain our findings.

# Methods

Wistar rats (2-4 weeks old) were anaesthetized by inhalation of isoflurane, decapitated, and sagittal brain slices  $(300 \,\mu\text{m})$  of somatosensory cortex were prepared according to guidelines approved by the Animal Ethics Committee of the Australian National University and the University of Freiburg. During recording, slices were superfused with oxygenated extracellular solution containing 125 mм NaCl, 3 mм KCl, 1.25 mм NaH<sub>2</sub>PO<sub>4</sub>, 25 mM NaHCO<sub>3</sub>, 25 mM glucose, 2 mM CaCl<sub>2</sub>, 1 mм MgCl<sub>2</sub> (pH 7.4 with 5% CO<sub>2</sub>). Nucleated patch experiments were performed at room temperature (~23°С) using pipettes filled with 137 mм CsCl, 4 mм MgCl<sub>2</sub>, 10 mM Hepes, 10 mM EGTA, 4 mM Na<sub>2</sub>ATP, 10 mм Na<sub>2</sub>-phophosphocreatine (pH 7.2 with CsOH) or in some cases with 80 mM CsCl, 80 mM CsF, 4 mM Na<sub>2</sub>ATP, 2 mм MgCl<sub>2</sub> (pH 7.2 with CsOH). Gigaseals  $(5-10 \text{ G}\Omega)$ were formed onto the soma of layer 5 pyramidal neurons with patch pipettes (resistance  $3-5 \text{ M}\Omega$ ) using a patchclamp amplifier (AxoPatch 200A; Axon Instruments). After obtaining the whole-cell configuration negative pressure was applied to the recording pipette and the nucleus with the surrounding cell membrane was pulled out of the slice to obtain a nucleated patch (Sather et al. 1992). The solution around nucleated patches was changed rapidly using a two-barrel application pipette attached to a piezo-electric device (Colquhoun et al. 1992). Nucleated patches were superfused with Hepes-buffered extracellular solution containing 125 mм NaCl, 10 mм Hepes, 3 mм KCl, 2 mm CaCl<sub>2</sub>, 1 mm MgCl<sub>2</sub>, 20  $\mu$ m DNQX, 10  $\mu$ m glycine, 200 μM CdCl<sub>2</sub>, 0.1 μM TTX (pH 7.4 with NaOH) and for the times indicated switched to the same solution containing 1 mM L-glutamate. Traces were recorded with and without glutamate application for subtraction of leak and capacitance currents and averaged. Open tip responses during brief (1 ms) and long (4.6 s) changes into and out of diluted (10%) Hepes-buffered extracellular solution were checked before each experiment (20-80% rise time  $\sim 200 \ \mu$ S). For the kinetic model (Fig. 2), and during pairing of glutamate applications with voltage commands obtained during dendritic recordings (Fig. 4), the timing of glutamate applications was corrected for the delay ( $\sim 2 \text{ ms}$ ) required for the glutamate solution to reach the patch following activation of the piezo-electric device. The holding potential during action potential waveforms (-66 mV, Fig. 4A) was corrected for the difference in junction potential between the potassium gluconate- and CsCl-based recording solutions (-9 mV). Glutamate-activated currents were hardware filtered at 5 kHz (8-pole Bessel; Axopatch 200A) and sampled at 50 kHz on a Macintosh computer. AxoGraph software (Axon Instruments) was used for both acquisition and analysis. Statistical significance was tested with the Students t test ( $\alpha = 0.05$ ) and pooled data shows mean  $\pm$  s.E.M. For display purposes current traces in the figures were digitally filtered at 1 kHz.

Recorded NMDAR currents were fitted using a 10-state Markov model of the NMDAR, five states with Mg<sup>2+</sup> bound and five unbound states (Fig. 2A). Reaction rates between the states were adjusted until the best fit to the data was obtained. Modelling and fitting were performed using AxoGraph 4.9 (Axon Instruments), which employs a simplex algorithm to minimize the sum of squared errors between simulated traces and data. The model incorporated several simplifications and constraints to keep the number of free parameters manageable. Only a single glutamate binding step was included as binding is effectively instantaneous at 1 mm. The binding rate was constrained to  $10 \,\mu \text{M}^{-1} \text{ s}^{-1}$  based on previous estimates (Clements & Westbrook, 1991). As the NMDAR channel opening rate is low (Rosenmund et al. 1995), and has negligible influence on the kinetic properties of the receptor, this was arbitrarily constrained to 10 s<sup>-1</sup>. The data contain no information about the Mg<sup>2+</sup> binding rate, and this was constrained to  $0.05 \,\mu \text{M}^{-1} \text{ s}^{-1}$  for Mg<sup>2+</sup> binding to the open state at +40 mV based on previous estimates (Ascher et al. 1988; Jahr & Stevens, 1990a,b). Mg<sup>2+</sup> binding to the other four states was arbitrarily constrained to be 1000 times slower. The voltage dependence of the Mg<sup>2+</sup> binding and unbinding rates is determined by the  $Mg^{2+}$  ion valency (2) and the position of the  $Mg^{2+}$ binding site 80% of the way from the extracellular side through the membrane field (Jahr & Stevens, 1990a). Mg<sup>2+</sup> concentration was set to 1 mm. As the time course of desensitization during long pulses was double exponential, two desensitized states were required. The model contains four reaction cycles, so four of the rates were constrained by cyclic reversibility. The fitting process started by fitting data recorded at +40 mV with a five-state model that excluded Mg<sup>2+</sup> bound states. The optimum rates obtained were then constrained in the subsequent fit of the full 10-state

model to the data incorporating voltage steps from -60 to +40 mV (Fig. 2*B*). The microscopic  $K_d$  for glutamate binding was calculated as unbinding rate/binding rate, open probability was calculated as opening rate/(opening

rate + closing rate), and percentage desensitization was calculated as desensitization rate/(desensitization rate + re-sensitization rate). Changes in microscopic  $K_d$  are unlikely to be due to changes in glycine affinity as the





A, superimposed NMDAR currents during 1 ms applications of 1 mM glutamate in the presence of 1 mM Mg<sup>2+</sup> at holding potentials of -60 and +40 mV (black), and during a step from -60 to +40 mV starting 10 ms after glutamate application (grey). The timing of glutamate application and the voltage step from -60 to +40 mV are indicated at the bottom. *B*, same as in *A* but during a long (4.6 s) application of glutamate. *C*, same as *A* and *B* during a 1 s voltage step from -60 to +40 mV starting 3.5 s after a long (4.6 s) application of 1 mM glutamate (grey). Inset shows same voltage step applied to a different patch in solution without external Mg<sup>2+</sup>. *D*, NMDAR current at +40 mV divided by that during steps from -60 to +40 mV starting 10 ms ('early step'; data from *B*) or 3.5 s ('late step'; data from C) after long (4.6 s) applications of 1 mM glutamate. Black traces show multiexponential fits. *E*, pooled data (n = 5) of the time constant (columns) and relative amplitude ( $\textcircled{\bullet}$ ) of multiexponential fits to Mg<sup>2+</sup> unblock during steps from -60 to +40 mV starting 10 ms ('early step'; dark grey) and 3.5 s ('late step'; light grey) after long applications of glutamate. Steps at 10 ms were fitted with a double exponential, whereas a triple exponential was required to fit steps at 3.5 s.

concentration of glycine used in our experiments (10  $\mu$ M) is approximately 100 times the apparent  $K_d$  (Johnson & Ascher, 1992).

Simultaneous somatic and dendritic recordings were made from the soma and apical dendrite of layer 5 pyramidal neurons as previously described (Stuart *et al.* 1997) using current-clamp amplifiers (Dagan), hardware filtered at 10 kHz and sampled at 50 kHz on a Macintosh computer. Recordings were made at 35°C using pipettes filled with 135 mM potassium gluconate, 7 mM NaCl, 10 mM Hepes, 2 mM MgCl<sub>2</sub>, 2 mM Na<sub>2</sub>ATP (pH 7.2 with KOH). EPSPs were evoked by extracellular stimulation with a patch pipette filled with external solution placed approximately 20  $\mu$ m from the dendritic recording site, and APs were evoked by brief (2 ms) somatic current injections (3 nA).

## Results

NMDAR currents were evoked in nucleated patches from neocortical layer 5 pyramidal neurons by brief (1 ms) glutamate pulses to mimic the synaptic release of glutamate (Clements et al. 1992; Colquhoun et al. 1992). Currents recorded at a holding potential of +40 mV to prevent  $Mg^{2+}$  block had an average amplitude of  $189 \pm 29$  pA, a rise time constant of  $2.0 \pm 0.2$  ms and decayed in a double exponential manner with time constants of  $32 \pm 1.5$  ms (amplitude:  $51 \pm 1.6\%$ ) and  $176 \pm 17.2$  ms (amplitude:  $49 \pm 1.6\%$ ; n = 12). In the presence of physiological concentrations of external Mg<sup>2+</sup> (1 mm) NMDAR currents were largely blocked at -60 mV (Fig. 1A). Stepping the holding potential from -60 to +40 mV starting 10 ms after onset of glutamate application resulted in a reversal of the inward current at -60 mV towards the outward current obtained during application of glutamate at +40 mV (Fig. 1A). However, the NMDAR current did not instantaneously reach that observed during glutamate application at +40 mV, but showed a slow component (Fig. 1A). Similar results were observed when glutamate was applied throughout the duration of depolarizing voltage steps from -60 to +40 mV (Fig. 1*B*). In Mg<sup>2+</sup>free solutions the current reversed instantaneously during depolarizations from -60 to +40 mV (time constant of  $0.07 \pm 0.01$  ms, n = 5), indicating that the slow time course of current reversal was due to slow unblock by Mg<sup>2+</sup> (see Fig. 1*C*, inset). The ratio of the current evoked at +40 mVand that evoked by stepping from -60 to +40 mV starting 10 ms after onset of glutamate application was used to assess the rate of  $Mg^{2+}$  unblock (Fig. 1D; 'early step'). After brief (1 ms) glutamate applications this current ratio was best fitted with two exponentials with average time constants of  $0.13 \pm 0.02$  ms and  $3.1 \pm 0.7$  ms and relative amplitudes of  $68 \pm 3\%$  and  $32 \pm 3\%$ , respectively (n=7). A similar time course of Mg<sup>2+</sup> unblock was observed when glutamate was applied throughout the duration of these depolarizations (Fig. 1*E* and 0.13  $\pm 0.01$  ms and  $4.6 \pm 0.5$  ms with relative amplitudes of  $77 \pm 3\%$  and  $23 \pm 3\%$ , respectively; n = 5).

To investigate the dependence of this slow  $Mg^{2+}$  unblock on the timing of the depolarization we also applied





A, reaction scheme shows two molecules of glutamate (A) binding to the NMDA receptor (R), opening of the channel (O), and transition to fast and slow desensitization states (D<sub>f</sub> and D<sub>s</sub>). Mg<sup>2+</sup> binds to all five states, although binding is much more rapid to the open state (thick lines) than to the other states (dashed lines). *B*, recorded and simulated NMDAR current during 4.6 s applications of 1 mm glutamate in the presence of 1 mm Mg<sup>2+</sup> at holding potentials of -60 and +40 mV (black), and during a step from -60 to +40 mV starting 10 ms (see inset with expanded time scale) or 3.5 s after the glutamate application (grey). Fitted transients (smooth curves) generated by the model shown in *A* are superimposed on the data.

Table 1. Optimum reaction rates for the Markov model of the NMDAR. Average results from 5 patch	ates for the Markov model of the NWDAR. Average results from 5 patch
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Transition	Forward Rate		Reverse Rate	
	Mg <sup>2+</sup> not bound	Mg <sup>2+</sup> bound	Mg <sup>2+</sup> not bound	Mg <sup>2+</sup> bound
Glutamate binding ( $\mu$ M <sup>-1</sup> s <sup>-1</sup> )	10 (fixed)	10 (fixed)	$5.6\pm1.0$	$17.1\pm2.5$
Channel opening (s <sup>-1</sup> )	10 (fixed)	10 (fixed)	$273\pm12$	$548 \pm 60$
Fast desensitisation $(s^{-1})$	$2.2\pm0.2$	$2.1\pm0.3$	$1.6\pm0.1$	$\textbf{0.87} \pm \textbf{0.14}$
Slow desensitisation $(s^{-1})$	$\textbf{0.43} \pm \textbf{0.09}$	$\textbf{0.26} \pm \textbf{0.07}$	$\textbf{0.50} \pm \textbf{0.13}$	$\textbf{0.42}\pm\textbf{0.30}$
Mg $^{2+}$ binding ( $\mu$ M $^{-1}$ s $^{-1}$ )*	0.05 (fixed)		12 800 $\pm$	2 200

\*Binding to the open state at +40 mV. The forward rate of  $Mg^{2+}$  binding to the other 4 states was arbitrarily constrained to be 1,000 times slower. Reverse rates were constrained by cyclic reversibility during fitting to data from individual patches.

Table 2. Effect of Mg<sup>2+</sup> binding on NMDAR properties

Property	Mg <sup>2+</sup> not bound	Mg <sup>2+</sup> bound
$K_d$ for glutamate ( $\mu$ M)	$\textbf{0.56} \pm \textbf{0.10}$	$\textbf{1.71} \pm \textbf{0.25}$
Open Probability (%)	$\textbf{3.6} \pm \textbf{0.2}$	$\textbf{1.9}\pm\textbf{0.2}$
Fast Desensitisation (%)	$58\pm2$	$71\pm3$

voltage steps from -60 to +40 mV starting 3.5 s after the onset of long (4.6 s) glutamate applications, at a time when the NMDAR current was approximately at steady state (Fig. 1C). The resultant current showed significantly slower Mg<sup>2+</sup> unblock compared to voltage steps evoked 10 ms after glutamate application (compare C with B in Fig. 1). The ratio between the current evoked at +40 mV and that evoked by stepping from -60 to +40 mV starting 3.5 s after onset of glutamate application was best fitted with three exponentials, with a fast time constant of  $0.15 \pm 0.04$  ms of amplitude  $46 \pm 3\%$ , and two slower time constants of  $4.0 \pm 0.4$  ms and  $322 \pm 78$  ms with amplitudes of  $22 \pm 4\%$  and  $32 \pm 6\%$ , respectively (Fig. 1D and E; 'late step'; n = 5). Interestingly, the main difference in the kinetics during early (10 ms) and late (3.5 s) voltage steps from -60 to +40 mV was a reduction in the amplitude of the fastest time constant and the appearance of a third, very slow time constant, with little change in the amplitude or kinetics of the intermediate time constant (Fig. 1*E*). Stepping back to -60 mV at the end of pulses to +40 mV blocked the channel (Fig. 1*C*). The time course of Mg<sup>2+</sup> block was rapid and could be fitted with a single exponential with a time constant of  $0.09 \pm 0.003$  ms (n = 5). Together, these results indicate that Mg<sup>2+</sup> unblock of NMDARs has a slow component, the magnitude and time course of which is dependent on the timing of depolarizations after the onset of glutamate applications.

A 10-state kinetic model of the NMDAR (Fig. 2*A*) was used to fit current transients generated by voltage steps from -60 to +40 mV applied at short (10 ms) and long (3.5 s) intervals after the onset of glutamate pulses. The fitted model accurately reproduced the slow recovery from  $Mg^{2+}$  block during steps from -60 to +40 mV at both early and late times (Fig. 2*B*). The optimized reaction rates were consistent from patch to patch (n = 5), and are summarized in Table 1. The rates were used to determine the effect of  $Mg^{2+}$  binding on NMDAR channel properties, and indicated that when  $Mg^{2+}$  is bound, it reduces the channel's affinity for glutamate ( $K_d$ ) and open probability, but increases the rate of desensitization (Table 2).

A prediction of this model was that the response to a brief pulse of glutamate in the presence of Mg<sup>2+</sup> will decay more rapidly at negative potentials. This would be expected primarily due to the reduced affinity for glutamate when Mg<sup>2+</sup> is bound, but enhanced desensitization will also contribute. This prediction was confirmed experimentally. NMDAR current decay kinetics during brief (1 ms) glutamate applications in the presence of Mg<sup>2+</sup> were clearly voltage dependent, with NMDAR currents decaying faster at negative holding potentials where Mg<sup>2+</sup> block is greatest (Fig. 3A). This effect was due to the presence of Mg<sup>2+</sup> as the decay of NMDAR currents was largely voltage independent in  $Mg^{2+}$ -free solutions (Fig. 3A). A second prediction of the model was that in the presence of Mg<sup>2+</sup> more desensitization should be observed at negative holding potentials. Consistent with this, during long (4.6 s) applications of glutamate the steady-state current measured at +40 mV was  $33 \pm 2\%$  of the peak current, whereas at -60 mV it was only  $22 \pm 6\%$  (n = 5, P < 0.05). Since glutamate binding is saturated in these experiments, this difference is presumably due to the ability of  $Mg^{2+}$  to enhanced NMDAR desensitization.

The time dependence of slow  $Mg^{2+}$  unblock described here is likely to have important physiological consequences for STDP, as brief depolarizations that occur later in time after release of glutamate would be expected to evoke smaller NMDAR currents than predicted assuming instantaneous  $Mg^{2+}$  unblock. Indeed, the integral of NMDAR currents evoked by brief (10 ms) depolarizations to +40 mV at different times after brief (1 ms) glutamate applications was dependent on their millisecond timing, with the relative magnitude of NMDAR currents (compared to the response at +40 mV) smaller during depolarizations later in time after glutamate application (Fig. 3*B*). Depolarizations evoked 10 ms after glutamate application reached  $82 \pm 1\%$  of the maximum NMDAR current at +40 mV, whereas those evoked 100 ms after glutamate application reached only  $47 \pm 2\%$  of the maximum current (Fig. 3*B*; n = 6).

These findings suggest that the time dependence of slow  $Mg^{2+}$  unblock will influence the time window for NMDAR activation during STDP induction. To test this, we recorded the dendritic membrane potential during pairing of backpropagating APs with EPSPs at different times. Figure 4*A* (top) shows two examples at time intervals of 10 and 50 ms. We applied these voltage waveforms to patches together with brief (1 ms) glutamate applications

timed to occur at the onset of the dendritic EPSP. Examples of recorded NMDAR currents are shown in Fig. 4A (middle, black). The predicted NMDAR current assuming instantaneous Mg<sup>2+</sup> unblock was calculated from the steady-state I-V curve for each patch (Fig. 4A, middle, grey). Recorded (black) and predicted (grey) NMDAR conductance were calculated by dividing recorded and predicted NMDAR currents by the voltage driving force (Fig. 4A, bottom). NMDAR activation, defined as the area around the peak in conductance for each EPSP-AP time interval, was calculated for recorded (black) and predicted (grey) NMDAR conductance (Fig. 4B). The timing curve for NMDAR activation observed experimentally (Fig. 4B, black) was significantly narrower (half-duration 43 ms) than that predicted assuming instantaneous Mg<sup>2+</sup> unblock of NMDAR channels (half-duration 60 ms; Fig. 4B, grey).





A, normalized (at peak), superimposed NMDAR currents during 1 ms applications of 1 mM glutamate at the indicated holding potentials in the presence of 1 mM Mg<sup>2+</sup> (top) and in Mg<sup>2+</sup>-free solution (middle). Bottom, average duration at half-amplitude of NMDAR currents evoked by 1 ms applications of 1 mM glutamate normalized to that at +40 mV and plotted against the holding potential in solutions with ( $\bullet$ ) and without (O) Mg<sup>2+</sup> (n = 6). *B*, top, superimposed NMDAR currents during 1 ms applications of 1 mM glutamate at +40 mV, and during 10 ms voltage steps from -60 to +40 mV occurring 10, 50, 100 or 200 ms after onset of glutamate application. Bottom, ratio of the current integral during 10 ms voltage steps (as in *B*) relative to the integral (over the same time) of the response obtained at a holding potential of +40 mV (n = 6).



**Figure 4. NMDAR activation during STDP induction protocols** *A*, top, dendritic voltage (650  $\mu$ m from the soma) during pairing of an EPSP with a backpropagating AP 10 or 50 ms after EPSP onset. Middle, recorded (black) and predicted (grey, assuming instantaneous Mg<sup>2+</sup> unblock) NMDAR current during EPSP–AP pairing. Bottom, recorded (black) and predicted (grey) NMDAR conductance. *B*, NMDAR activation during EPSP–AP pairing at different time intervals for recorded (black) and predicted (grey) NMDAR currents. Currents were normalized in each patch to the response during 1 ms applications of 1 mM glutamate at +40 mV and the area around the conductance peak (3 ms before to 10 ms after) was used to quantify NMDAR activation.

### Discussion

Here, we report a slow component to  $Mg^{2+}$  unblock of NMDA receptors which has implications for STDP. The kinetics of this slow unblock were dependent on the timing of depolarizations after glutamate application, and were slower during depolarizations at later times. A kinetic model indicated that this occurs due to the ability of  $Mg^{2+}$  binding to enhance NMDAR desensitization, while decreasing affinity and open channel probability. Together, these effects act to sharpen the time window during which brief depolarizations, such as backpropagating APs, can activate NMDAR channels.

#### Comparison with earlier studies

The original studies investigating the kinetics of  $Mg^{2+}$ block of NMDARs analysed the dependence of short interruptions in single channel openings on  $Mg^{2+}$ concentration and membrane potential (Ascher *et al.* 1988; Jahr & Stevens, 1990*a,b*). These studies estimated that the kinetics of  $Mg^{2+}$  block and unblock were fast, with time constants between 80 and 190  $\mu$ s (Ascher *et al.* 1988; Jahr & Stevens, 1990*a,b*). We find here (see also Spruston *et al.* 1995; Vargas-Caballero & Robinson, 2003) that while the time course of  $Mg^{2+}$  block is very fast (~100  $\mu$ s), the time course of  $Mg^{2+}$  unblock of NMDARs is complex with a fast component (~150  $\mu$ s) similar to that found in the earlier single channel studies, as well as additional slower components ranging from a few to hundreds of milliseconds depending on the state of the NMDAR channel.

Other studies have reported that  $Mg^{2+}$  can be trapped in the NMDAR channel pore, and have proposed a symmetric trapping block model to account for the action of Mg<sup>2+</sup> on NMDAR channels (Sobolevsky & Yelshansky, 2000). Our model (Fig. 2B) also required  $Mg^{2+}$  binding to open, as well as closed and desensitized states, but is not strictly a 'trapping' model because Mg<sup>2+</sup> can unbind when the channel is closed (although at very low rates). Allowing Mg<sup>2+</sup> to bind and unbind from closed states was considered more realistic than a model where this was not the case, but was not essential to obtain adequate fits to the data (J. Clements, unpublished). Another important difference between our model and that of Sobolevsky & Yelshansky (2000) is that it is asymmetric, with transitions between Mg<sup>2+</sup>-bound states being different from equivalent transitions between Mg<sup>2+</sup>-free states. This asymmetry was essential for adequate fits to the data.

An important conclusion from our study is that Mg<sup>2+</sup> binding enhances NMDAR desensitization, while

decreasing affinity and open channel probability. This differs from recent data suggesting that Mg<sup>2+</sup> binding does not affect channel gating, desensitization or agonist dissociation based on the similarity of the IC50 for  $Mg^{2+}$  block and the  $K_d$  for  $Mg^{2+}$  binding determined from single channel data (Qian et al. 2002). Using the average reaction rates in Table 1, the IC<sub>50</sub> and  $K_{\rm d}$  for Mg<sup>2+</sup> block at -60 mV in our kinetic model were  $40 \,\mu\text{M}$  and  $19 \,\mu\text{M}$ , respectively. To detect such a relatively small difference would require an exceptionally accurate dose-response experiment, combined with very high quality single channel recordings from the same preparation. In addition, this previous study examined steady-state Mg<sup>2+</sup> block where effects of Mg<sup>2+</sup> binding on desensitization would not be apparent. Consistent with an effect of Mg<sup>2+</sup> binding on channel gating the extent of desensitization measured by the ratio of the peak to steadystate current during long glutamate pulses, as well as the rate of deactivation during brief glutamate applications, were greater at negative membrane potentials. Finally, these observations are in agreement with the original findings of Nowak et al. (1984), who reported that single channel burst duration and frequency are decreased at negative holding potentials where Mg<sup>2+</sup> binding is greatest.

Consistent with the recent findings of Vargas-Caballero & Robinson (2003), we observed that the slow component of Mg<sup>2+</sup> unblock accounts for approximately 50% of the amplitude of NMDAR current during depolarizations from -60 to +40 mV under steady-state conditions (Fig. 1*E*, 'late step'). In our hands, slow unblock at these times was better fitted with two exponentials with time constants of approximately 4 and 300 ms rather than one with a time constant of approximately 20 ms. Importantly, we found that the kinetics of slow unblock were faster during depolarizations at earlier times after the onset of glutamate application, with the slow component of Mg<sup>2+</sup> unblock of NMDARs being best fitted with a single exponential of approximately 4 ms and an amplitude of approximately 25% during depolarizations 10 ms after the onset of glutamate application (Fig. 1E, 'early step').

#### Mechanism underlying slow unblock

We hypothesize that the slow component to  $Mg^{2+}$  unblock described here arises because at negative potentials NMDAR channels go into  $Mg^{2+}$ -bound closed and desensitized states, and only slowly re-sensitize and become available to reopen following a step from negative to positive potentials. As the number of NMDAR channels in  $Mg^{2+}$ -bound closed and desensitized states increases with time after the onset of glutamate application, the magnitude and kinetics of  $Mg^{2+}$  unblock depend critically on the millisecond timing of depolarizations, with depolarizations occurring early in time after glutamate application leading to larger NMDAR currents due to reduced slow  $Mg^{2+}$  unblock (Fig. 3*B*).

## **Functional implications**

There are a number of potentially important functional implications of our findings. Firstly, we show that enhanced desensitization by Mg<sup>2+</sup> results in the decay of NMDAR currents being voltage dependent, and faster at negative holding potentials where Mg<sup>2+</sup> block is greatest (Fig. 3A). This finding is consistent with earlier observations in motoneurons and hippocampal granule cells where the kinetics of NMDAR EPSCs were also found to be voltage-dependent and faster at more negative holding potentials (Konnerth et al. 1990; Keller et al. 1991). One consequence of this voltage dependence is that synaptic NMDAR currents are prolonged at depolarized membrane potentials, which could enhance NMDARdependent calcium influx and synaptic plasticity when presynaptic synaptic activity is paired with postsynaptic depolarization.

Secondly, we show that the magnitude of NMDAR current generated by brief voltage steps or dendritic AP waveforms is dependent on their millisecond timing relative to the onset of glutamate applications (Figs 3B and 4B). This is because  $Mg^{2+}$  binding enhances desensitization and reduces glutamate affinity, reducing the relative current flow through NMDARs during brief depolarizations occurring later in time after glutamate application. As the timing of APs relative to EPSP onset plays an important role in determining both the sign and the magnitude of changes in synaptic strength during STDP (Bi & Poo, 1998; Markram et al. 1997), the time dependence of slow Mg<sup>2+</sup> unblock observed here would be expected to sharpen the time window for STDP induction, increasing the ability of the NMDAR channel to function as a coincidence detector.

Finally, slow  $Mg^{2+}$  unblock will favour NMDAR activation, and associated calcium influx, during slow dendritic depolarizations, as occurs during dendritic calcium spikes associated with burst firing (Stuart *et al.* 1997) or synaptic stimulation (Schiller *et al.* 1997), increasing the importance of local dendritic regenerative activity near the site of synaptic input for the induction of synaptic plasticity (Golding *et al.* 2002).

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