Detection of methylation of human $p16^{lnk4a}$ gene 5¢-CpG islands by electrochemical method coupled with linker-PCR

Peng Hou, Meiju Ji, Cunwang Ge, Jiayao Shen, Song Li, Nongyue He and Zuhong Lu*

Chien-Shiung Wu Laboratory, Department of Biological Science and Medical Engineering, Southeast University, Nanjing, 210096, China

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ABSTRACT

Aberrant DNA methylation of the CpG site is among the earliest and most frequent alterations in cancer. Detection of promoter hypermethylation of cancerrelated genes may be useful for cancer diagnosis or the detection of recurrence. p16, an inhibitor of the cyclin D-dependent protein kinases, is a classical tumor suppressor gene, and its inactivation is closely associated with carcinogenesis. p16 hypermethylation could be detected in each stage, which is consistent with the finding that aberrant methylation of p16 is a very early event in carcinogenesis. We have developed an electrochemical procedure for detecting DNA methylation of the human p16Ink4a gene. The procedure is based on the coupling of DNA electrochemical sensors with linker-PCRamplified DNA from human gastric tumor tissue and whole blood cells of healthy human. The synthesized oligonucleotide was immobilized on the modi fied gold electrode to fabricate a DNA biosensor. The hybridization reaction on the electrode surface was monitored by cyclic voltammogram (CV) and square wave voltammogram (SWV), using $[Co(phen)₃](ClO₄)₃$ as a redox indicator. Methylation status of human $p16^{ln k4a}$ gene was detected and the results were validated by bisulfite DNA sequencing. A good reproducibility was observed in several parallel experiments. The coupling of DNA electrochemical sensors with PCR allowed quick detection and have the potential of the quantitative evaluation of the methylation status of the human $p16^{lnk4a}$ gene.

INTRODUCTION

The methylation of DNA is an epigenetic modification that can play an important role in the control of gene expression in mammalian cells. The epigenetic event has been observed in GC-rich regions, called CpG islands, frequently located in the promoter and the first exon regions of genes. CpG island

hypermethylation is closely associated with transcriptional inactivation of the classic tumor suppressor genes, which is a common feature in human carcinomas (1). p16, an inhibitor of the cyclin D-dependent protein kinases, is a tumor suppressor gene, and its inactivation is closely associated with carcinogenesis. Hypermethylation on the CpG islands of the p16 gene has been proposed as an alternative mechanism for the loss of p16 expression. p16 hypermethylation could be detected in each stage, which is consistent with the finding that aberrant methylation of $p16$ is a very early event in carcinogenesis (2). Detection of aberrant promoter hypermethylation of cancerrelated gene may be useful for cancer diagnosis or the detection of recurrence (3,4). Several methods have been developed to evaluate the methylation status of genes, such as Southern blot (5) , bisulfite genomic DNA sequencing (6) , restriction enzyme-PCR (7), MSP (methylation-specific PCR) (8), methylation-sensitive single nucleotide primer extension $(MS-SNuPE)$ (9) , DNA microarray based on fluorescence or isotope labeling (10,11) and so on. They have offered useful and powerful tools in studying the phenomenon of DNA methylation. However, the present methods are still laborious, time-consuming, less sensitive and not rigid enough for the clinical applications. It is of great importance to establish sensitive and reliable methods for the methylation detection of earlier cancer diagnosis.

In recent years, there has been considerable interest in developing a DNA electrochemical biosensor for rapid applications in genetic analysis. DNA electrochemistry biosensor plays an enormous potential for the detection of the presence of genes or mutant genes associated with inherited human diseases, because electrochemical ones provide simple, rapid and low-cost point-of-care detection of specific nucleic acid sequences $(12-15)$. A DNA electrochemical biosensor generally is an electrode with an oligonucleotide immobilized on the surface. Recently, some reports have indicated that electrochemical techniques are well suited for measuring hybridization events (16–24). The electrochemical detections of DNA hybridization have been mainly oriented to the application of labeling or unlabeling target. A number of papers focused on the application of electroactive DNA intercalators such as daunomycin, $[Co(phen)_3] (ClO_4)_3$ and $Co(bpy)_3^{3+}$ intercalates in the double strand to detect DNA hybridization (16–21). However, most of the present research was demonstrated only by using

*To whom correspondence should be addressed. Tel: +86 25 3792245; Fax: +86 25 3619983; Email: zhlu@seu.edu.cn

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synthetic oligonucleotides as target gene. Only Marrazza et al. (17) have reported the experiments of DNA electrochemical biosensors for detection of PCR-amplified DNA products. We have not found any report to use the DNA electrochemical biosensor for methylation detection until now.

The aims of the present work are to develop a new and label-free method for detecting DNA methylation. We describe an electrochemical method to detect DNA methylation, using DNA fragments amplified by linker-PCR. The procedure involves the use of an electroactive indicator, [Co $(\text{phen})_3$](ClO₄)₃, which can intercalate the double strand DNA (25) . We selected a segment of the 5 \prime untranslated region and the first exon of the $p16^{lnk4a}$ gene, as the investigated target, which includes the recognition site of BstUI restriction endonuclease. Genomic DNA is restricted with MseI from human gastric tumor tissue and whole blood cells of healthy human, and the cleaved ends of DNA are ligated to unphosphorylated linkers as universal PCR primers. Then the ligated DNA is digested with methylation-sensitive endonucleases BstUI. The digested products are amplified by PCR as targets. An oligonucleotide was synthesized and purified to completely match with the target DNA fragments. The oligonucleotide was immobilized on the modified gold electrode to fabricate a DNA biosensor. The DNA biosensor is hybridized with the target solution to determine methylation status of p16 gene according to peak current. We have successfully used the above electrochemical method to detect the methylated CpG islands of $p16$ gene from human gastric tumor tissue, and the results showed that the electrochemical monitoring of the DNA hybridization at the transducer surface would be reliable, low cost and the analysis would be rapid.

MATERIALS AND METHODS

2-Aminoethanethiol (AET), 1-ethyl-3 (3-dimethyl-aminopropyl)-carbodiimide (EDC) and N-hydroxysulfosuccinimide (NHS) were purchased from Sigma Chemicals. $[Co(phen)_3]$ $(CIO₄)$ ₃ was prepared according to the literature (26). Other chemicals were of analytical reagent grade.

Pretreatment and modification of the electrodes

The electrodes were pretreated and modified according to Ge et al. (26) . Gold electrodes were polished firstly with w5 abrasive paper and subsequently with chamois followed by rinsing with water and sonification in ethanol and water for 2 min each, respectively. The extent of electrode pretreatment was evaluated by a cyclic voltammogram (CV) measurement in 1 mM K_3Fe (CN)₆ solution containing 0.1 M KCl. The peak-to-peak separation should be <70 mV at a scan rate of 100 mV/s.

Before chemisorptions, the electrodes were treated with 'piranha solution' $(H_2SO_4/30\% H_2O_2, 7:3$ in v/v) for 5 min at room temperature and subsequently rinsed thoroughly with twice distilled water and, finally, ultrasonically cleaned with ethanol and twice distilled water for 3 min, respectively. The pretreated electrodes were immersed in 1 mM AET ethanol solution for 16 h resulting in the AET deposition on the electrodes. After that, the electrodes were thoroughly washed with ethanol and distilled water. The electrode was kept in distilled water till use and denoted as AET/Au.

Figure 1. A schematic outline of the procedure for the preparation of the DNA targets. M, B and B^m represent MseI, unmethylated and methylated BstUI recognition sites, respectively. Genomic DNA comes from whole blood cells of healthy human (normal) and gastric tumor tissue (tumor).

DNA self-assembly on the modified gold electrodes

The phosphorylated oligonucleotide was synthesized and purified by Shenyou Inc. (Shanghai, China). The oligonucleotide sequence was 5'-ACGGCCGGGCCCGGGGT-3'. A gold electrode modified with AET (denoted as AET/Au) was immersed in a 5 mM EDC and 8 mM NHS in PB buffer (pH 7.0) for 15 min containing DNA probes. The DNA modified electrode (denoted as DNA/AET/Au) was then soaked for 5 min in 0.1% SDS and distilled water, respectively, to remove any non-specially absorbed DNA.

Preparation of targets and hybridization

Whole blood cells of healthy human and gastric tumor tissue obtained from GuLou hospital (Nanjing, China). Genomic DNA was extracted from whole blood cells and gastric tumor tissue by standard methods using proteinase K digestion and phenol/chloroform extraction. The DNA derived from the blood cells of healthy human was divided into two parts. One aliquot was treated by methylase Sss I (SM) as a positive control with the conditions recommended by the supplier (New England Biolabs, Beverly, MA). Another was not treated by methylase Sss I (SM) as negative control. The positive control generated in this way had 100% methylated cytosine in the test CpG sites, whereas the negative control had all unmethylated cytosine residues in the test CpG sites.

The preparation process of targets is illustrated in Figure 1. Approximately $2 \mu g$ DNA was restricted to completion with 20 U of MseI following the conditions recommended by the supplier (New England Biolabs, Beverly, MA). This enzyme

Primer set	Sense primer $(5' \rightarrow 3')$	Antisense primer $(5' \rightarrow 3')$	Size (bp)	Temperature	Genomic position
$p16-M$	TTATTAGAGGGTGGGGCGGATCGC	CCACCTAAATCGACCTCCGACCG	234	60	$+167$
$p16-U$	TTATTAGAGGGTGGGGTGGATTGT	CCACCTAAATCAACCTCCAACCA	234		$+167$

Table 1. PCR primers used for methylation-specific PCR

Sequence differences between methylation/modified and unmethylated/modified are underlined. Primers were placed near the transcriptional start site. Genomic position is the location of the 5' nucleotide of the sense primer in relation to the major transcriptional start site (GenBank accession no. X94154).

restricts bulk DNA into small fragments. As its recognition site (TTAA) rarely occurs in GC-rich regions, most CpG islands remain intact after the restriction. The digests were purified with QIAquick column (Qiagen) and mixed with 0.5 nmol of unphosphorylated linkers H-24 and H-12 in a DNA ligase buffer (New England Biolabs). The linker sequences were H-24, 5'-AGG CAA CTG TGC TAT CCG AGG GAT, and H-12, 5'-TAA TCC CTC GGA (27). Oligonucleotides were annealed by cooling the mixture gradually from 55°C to room temperature over 1 h and then ligated to the cleaved ends of the DNA fragments by incubation overnight with 400 U of T4 DNA ligase (New England Biolabs) at 16°C.

The ligated DNA was digested with the methylationsensitive endonucleoase BstUI following the conditions recommended by the supplier (New England Biolabs). PCR reactions were performed in a $100 \mu l$ volume, containing 0.4 μ M H-24 primer, 4 U Taq DNA polymerase, 5% DMSO and 200 μ M dNTP in a buffer provided by the supplier. The tubes were incubated for 3 min at 72° C to fill in 5^{\prime}-protruding ends of the ligated DNA and subjected to 20 cycles of amplification consisting of 1 min at 97 $\mathrm{^{\circ}C}$ and 3 min at 72 $\mathrm{^{\circ}C}$ in a PTC-225 thermocycler (MJ Research, Watertown, MA). The final extension was lengthened to 10 min.

The PCR products were suspended in unihybridization solution [1:4 dilution (v/v), Telechem]. The electrode hybridization was conducted in a moist hybridization chamber under a cover slip at 42°C for 2 h. After hybridization, the electrode was rinsed and washed at room temperature with $2\times$ SSC -0.1% SDS and $0.1 \times$ SSC -0.1% SDS, respectively, for a total of 15 min, and dried under the flow of argon. The electrodes were denoted as positive control hybrid-DNA/ AET/Au, negative control hybrid-DNA/AET/Au and sample hybrid-DNA/AET/Au, respectively.

Electrochemical measurement

CV and square wave voltammogram (SWV) experiments were performed on a CHI 660A workstation (American CH instrument). The electrochemical cell consisted of a threeelectrode system with gold or modified gold electrode (0.5 mm in diameter) as the working electrode, a saturated calomel electrode (SCE) and a platinum wire as the reference and the counter electrode, respectively. The experimental temperature was controlled at 25 ± 1 °C.

Bisulfite analysis

Bisulfite processing of DNA was performed in principle as described by Frommer et al. (6) and the modifications introduced by Clark et al. (28) . Briefly, 1 µg of genomic DNA was digested by EcoRI and denatured in 0.35 M NaOH at 37° C for 20 min. The bisulfite reaction was carried out in 3.2 M sodium bisulfite and 0.5 mM hydroquinone (Sigma Chemical Co., USA) at 55° C for 16–24 h. DNA was recovered by a desalting column (DNA Clean-Up System, Promega Inc., USA) and desulphonated in 0.2 M NaOH at 37°C for 15 min, neutralized by ammonium acetate, alcohol precipitated, dried and then dissolved in 30μ of deionized water. After bisulfite processing, the all unmethylated cytosine residues converted to uracil, whereas the methylated ones remained unchanged.

The 5'-CpG island regions of the $p16^{Ink4a}$ gene were amplified with primers for methylated and unmethylated DNA, respectively. The primer pairs are described in Table 1. The PCR reaction was performed in buffer containing 10 mM Tris±HCl (pH 9.0), 50 mM KCl, 0.1% Triton X-100, 5% DMSO, 1.75 mM $MgCl₂$, 0.2 mM of each dNTP and 1 µl bisulfite-treated DNA. The amplification was carried out for 35 cycles (30 s at 95°C, 30 s at the annealing temperature listed in Table 1 and 30 s at 72° C), followed by a final 4 min extension at 72° C. The PCR products were gel purified and sequenced using an automated sequence analyzer (ABI377A, Applied Biosystem Inc.).

RESULTS AND DISCUSSION

Detection of methylation status of $p16^{Ink4a}$ gene with cyclic voltammogram

In the presence of water-soluble carbodiimide regent, the 5[']terminal phosphate of oligonucleotide probe formed a phosphoramidate bond with the primary amino group of aminoethanethiol monolayer on the gold electrode surface (29). These electrodes were reacted with positive control, negative control and sample in the hybridization buffer, respectively. The recognition of differently hybridized electrodes was justified by CV using $0.12 \text{ mM } [Co(phen)_3](ClO_4)_3$ as a redox indicator that was added in the Tris-HCl buffer solution. Figure 2a and b shows the CV measurement at the scan rate of 50 mV/S and anodic peak currents versus root of the scan rate of CV $v^{1/2}$ respectively for negative hybrid-DNA/ AET/Au (curve 1), sample hybrid-DNA/AET/Au (curve 2) and positive hybrid-DNA/AET/Au (curve 3) in Tris-HCl buffer (pH 7.1) containing $0.12 \text{ mM } [Co(phen)_3] (ClO_4)_3.$ Comprehensively, the following results were observed: (i) the peak current intensity reflected the methylation status of the $p16^{Ink4a}$ gene. Figure 2a shows that the redox peak currents of $Co(phen)₃³⁺$ species at the positive hybrid-DNA/AET/Au (curve 3) electrode (7.56 \pm 0.21) were much larger than those at sample hybrid-DNA/AET/Au (curve 2) (5.62 \pm 0.24) and negative hybrid-DNA/AET/Au (curve 1) (3.80 ± 0.31) . Because the peak current intensity of negative hybrid-DNA/ AET/Au (curve 1) was the smallest among three electrodes, a

Figure 2. CV at the scan rate of 50 mV/S (a) and anodic peak currents versus root of the scan rate of CV $v^{1/2}$ (b) for negative DNA/AET/Au (1), sample DNA/AET/Au (2) and positive DNA/AET/Au (3) in pH 7.1 Tris-HCl buffer containing 0.12 mM [Co(phen)₃](ClO₄)₃.

positive threshold could be established (30); therefore, methylation could be determined. The ratios of positive control/negative control and sample/negative control were calculated respectively and averaged for three parallel experiments. The positive control/negative control (P/N) and sample/negative control (S/N) were 1.989 and 1.479, respectively (Fig. 4). These data indicated that the CV could be used to detect methylation status of $p16^{Ink4a}$ gene. (ii) The peak potential differences ($\Delta E_p = E_{pa} - E_{pc}$) and the peak shape $|E_{\text{pc}} - E_{\text{p/2}}|$ were found to be between 60 and 70 mV, independent of potential sweep rate ($10 \le v \le 100$ mV/s), where ΔE_p , E_{pa} , E_{pc} and $E_{p/2}$ represent the interspike interval, anodic spike potential, cathodic spike potential and half peak potential, respectively. These indicated that the reduction of $[Co(phen)₃]$ ³⁺ at the surface of the electrode is a one electron transfer reversible process. A linear correlation between the oxidation peak current and the square root of the scan rate $v^{1/2}$ was observed (Fig. 2b), as expected for a diffusion controlled electrochemical process. All electrodes are $R \ge 0.99$ and

Table 2. Diffusion coefficients for different hybridized electrodes for positive hybrid-DNA/AET/Au (P), sample hybrid-DNA/AET/Au (S), and negative hybrid-DNA/AET/Au (N) derived from CV

$i_p/v^{1/2}$ $(10^{-7}A \cdot S^{1/2}/V^{1/2})$ 29.7 34.5 $\Delta(i_p/v^{1/2})$ 0.8 0.7 1.1 0.9988 0.9981 R		N	S	p
ΔD_0 (10 ⁻⁶ cm ² /S) 0.7 0.5	D_0 (10 ⁻⁶ cm ² /S)	10.1	13.5	47.7 0.9996 25.9 1.2

Figure 3. SWV for positive hybrid-DNA/AET/Au (1), sample hybrid-DNA/ AET/Au (2) and negative hybrid-DNA/AET/Au (3) with an amplitude of 25 mV, a pulse frequency of 30 Hz and step potential of 4 mV, in pH 7.1 Tris-HCl buffer containing $0.12 \text{ mM } [\text{Co(phen)}_3](\text{ClO}_4)_3$.

 $P \le 0.001$, respectively (Fig. 2b). On the other hand, at the positive hybrid-DNA/AET/Au and sample hybrid-DNA/AET/ Au, the oxidation peak currents increase rapidly with the $v^{1/2}$, which is consistent with the behavior of adsorption of the electroactive species that occurred at the surface of the electrode. According to the relationship of peak current i_p with the scan rate $v(25)$: $i_p = 2.69 \times 10^5 \cdot n^{3/2} \cdot C_0 \cdot D_0^{1/2} \cdot V^{1/2} \cdot A$, where n, C_0, D_0 and A represent the number of electrons in redox reaction, concentration of electroactive species, diffusion coefficient and the area of electrode, respectively. The microscopic areas of 0.029 (\pm 0.004) cm² were determined by the integration of the cathode peak during the redox reaction of superficial gold in 1.0 M H₂SO₄ (26). For $n = 1$, the diffusion coefficients for differently hybridized electrodes with the measuring error were calculated from the slope of i_p versus $v^{1/2}$ (Fig. 2) and shown in Table 2.

From Table 2, the diffusion coefficient (D_0) for positive hybrid-DNA/AET/Au is as high as $(25.9 \pm 1.2) \times 10^{-6}$ cm²/S, which is apparently higher than for sample hybrid-DNA/AET/ Au $[(13.5 \pm 0.7) \times 10^{-6} \text{ cm}^2/\text{S}]$ and negative hybrid-DNA/ AET/Au $[(10.1 \pm 0.5) \times 10^{-6} \text{ cm}^2/\text{S})]$. This result showed a

Figure 4. The plot of current intensity ratios of CV and SWV for differently hybridized electrodes. P/N, positive hybrid-DNA/AET/Au/negative hybrid-DNA/AET/Au; S/N, sample hybrid-DNA/AET/Au/negative hybrid-DNA/ AET/Au.

reasonable agreement with the common conception that the Co (phen) 3^{3+} had the ability of strong interaction with dsDNA (31). Therefore, the CV could be used to detect methylation status of the $p16^{Ink4a}$ gene.

Detection of methylation status of $p16^{Ink4a}$ gene with square wave voltammogram

SWV is a sensitive method in electrochemical measurement. The different hybridized electrodes were also characterized with the square wave voltammetry with an amplitude of 25 mV, a pulse frequency of 30 Hz and step potential of 4 mV using 0.12 mM $[Co(phen)_3]$ $ClO₄$) 3 as a redox indicator that was added in the Tris-HCl buffer solution. Figure 3 illustrates that the cathode peak current of of $Co(phen)₃³⁺$ species at the positive hybrid-DNA/AET/Au (curve 3) (12.22 \pm 0.32) was much larger than at the sample hybrid-DNA/AET/Au (curve 2) (9.02 \pm 0.22) and the negative hybrid-DNA/AET/Au (curve 1) (4.76 \pm 0.24). The peak current intensity of negative hybrid-DNA/AET/Au (curve 1) was the smallest among three electrodes, which can be taken as a baseline of the hybridization signal. Therefore, the signal of the methylated samples could be compared with both negative and positive ones. We have calculated the positive control/negative control and sample/negative control and averaged from three parallel experiments. The ratios of P/N and S/N were 2.567 and 1.895, respectively (Fig. 4). The results show that SWV is suited to detect methylation status of CpG sites. The ratios of peak current (P/N and S/N) for SWV were larger than those for CV. It means that SWV and CV are sensitive in detecting

Figure 5. (a) MSP of $p16$ gene. After treatment with bisulfate, amplification of DNA from gastric tumor tissue (A) and whole blood cells of healthy human (B) using unmethylated primer; amplification of DNA from gastric tumor tissue (C) and whole blood cells of healthy human (D) using methylated primer. Marker (M): from top to bottom, the bands are 2000, 1000, 750, 500, 250 and 100 bp, respectively. (b) Sequencing result of the PCR product with an ABI377A. The box indicates that the CpG sites in BstUI recognition sequence are methylated.

methylation status of CpG sites. Moreover, the technology will have potential in the quantitative measurement for methylation samples.

Methylation-specific PCR for methylation detection of p16 gene

MSP, which can rapidly assess the methylation status of virtually any group of CpG sites within a CpG island, independent of the use of methylation-sensitive restriction enzymes. This assay entails initial modification of DNA by sodium bisulfite, converting all unmethylated, but not methylated, cytosines to uracil, and subsequent amplification with primers specific for methylated versus unmethylated DNA (8). Primer pairs were designed to discriminate between methylated and unmethylated alleles following bisulfite treatment. To accomplish this, primer sequences were chosen for regions containing frequent cytosines, and CpG pairs near the 3¢-end of the primers (to provide maximal discrimination in the PCR between methylated and unmethylated DNA) (8). After bisulfite treatment, the amplification products were both detected with unmethylated primers (p16-U) in the genomic DNA from whole blood cells of healthy human and gastric tumor tissue. However, the amplification product was only obtained with methylated primers $(p16-M)$ in the genomic DNA from the gastric tumor tissue (Fig. 5a). The results indicate that methylation was only detected in the gastric tumor tissue for $p16^{lnk4a}$ gene, which further confirmed the conclusion of CV and SWV. The results of MSP were validated by bisulfite DNA sequencing. Figure 5b illustrates that methylation was detected in the recognition site of BstUI (CGCG) for the gastric tumor tissue.

CONCLUSION

In this paper, we have described an electrochemical method to detect DNA methylation, using label-free DNA fragments amplified by linker-PCR. The results presented here confirm that the electrochemical methods have been successfully used to detect methylated CpG sites within the 5'-CpG islands of the $p16^{Ink4a}$ gene. A great advantage of the electrochemical monitoring of the DNA hybridization at the transducer surface has proved to be: (i) faster measurements, ≤ 10 s; (ii) eliminating the need for gel, radioisotopes and blotting methods; (iii) coupled with PCR and high sensitivity; (iv) label-free target; (v) low-cost point-of-care and reliable detection results; and (vi) potential in quantitative measurments. The possibility of detection methylation opens realistic prospects for a number of important genetic analyses.

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