

NIH Public Access

Author Manuscript

Brain Res. Author manuscript; available in PMC 2008 August 3.

Published in final edited form as: *Brain Page* 2007 August 3: 1161: 05

Brain Res. 2007 August 3; 1161: 95–105.

Attenuation of β -amyloid induced toxicity by sialic acidconjugated dendrimers: role of sialic acid attachment

Dhara A. Patel, James E. Henry^{*}, and Theresa A. Good

Department of Chemical and Biochemical Engineering, University of Maryland Baltimore County, Baltimore, MD 21250, USA.

Abstract

 β -amyloid (A β) is the primary protein component of senile plaques in Alzheimer's disease and is believed to be associated with neurotoxicity in the disease. We and others have shown that A β binds with relatively high affinity to clustered sialic acid residues on cell surfaces and that removal of cell surface sialic acids attenuate A β toxicity. We have also shown that sialic acid functionalized dendrimeric polymers can act as mimics of cell surface sialic acid clusters and attenuate A β induced neurotoxicity. In the current study, we prepared sialic acid conjugated dendrimers using a physiologically relevant attachment of the sialic acid to the dendrimeric termini, and evaluated the A β toxicity attenuation properties of the dendrimers. We compared performance of sialic acid conjugated dendrimeric polymers in which the sialic acid moeties were attached to dendrimeric termini via the anomeric hydroxyl group of the sialic acid group on the sialic acid, a non-physiological attachment. This work enhances our understanding of A β -cell surface binding and is a step towards the development of new classes of sequestering agents as therapeutics for the prevention of A β toxicity in AD.

Keywords

Alzheimer's disease; amyloid; dendrimer; sialic acid; toxicity

1. Introduction

Alzheimer's disease (AD) is the leading cause of neurodegeneration in the United States, affecting approximately 4.5 million Americans in 2003 (Hebert et al., 2003), with an annual cost of care for these individuals estimated at over \$100 billion (Ernst and Hay, 1994). The cost of care for patients also increases with progression of the disease (Zhu et al., 2006). One of the pathological hallmarks of AD is the formation of amyloid plaques in the cerebral cortex, the primary protein component of which is the 39–43 amino acid peptide β -amyloid (A β) (Selkoe, 1994). A β in a number of aggregated states including fibrils, protofibrils, and spherical oligomers, has been shown to be toxic to neurons and neuron-like cells in culture (Hartley et al., 1999;Seilheimer et al., 1997;Ward et al., 2000). It is believed that A β may play a major role in neurodegeneration associated with AD. To that end, agents which either sequester A β or interfere with A β interaction/binding to cells have been sought after as a means to reduce

Corresponding author: Theresa Good, Department of Chemical and Biochemical Engineering, University of Maryland Baltimore County (UMBC), 1000 Hilltop Circle, Baltimore, MD 21250, Fax: 410 455 1049, Ph.: 410 455 3403, Email: tgood@umbc.edu *Current address: Department of Chemical Engineering, Louisiana State University, Baton Rouge, LA.

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the pathological effects of A β (Drouet et al., 1999;Gelinas et al., 2004;Hertel et al., 1997;Hock et al., 2003;Matsuoka et al., 2003;Schenk et al., 2004).

A variety of evidence suggests that $A\beta$ binds to cells via an interaction with surface glycolipids or glycoproteins (Ariga and Yu, 1999; Ariga et al., 2001; Avdulov et al., 1997; Choo-Smith et al., 1997;Kakio et al., 2001;Matsuzaki and Horikiri, 1999;McLaurin and Chakrabartty, 1996;McLaurin et al., 1998;Wakabayashi et al., 2005;Wang et al., 2001;Yanagisawa et al., 1995). Moreover, the sialic acid moiety is necessary for such interactions (Williamson et al., 2006). The affinity of the A β interaction increases when the gangliosides or sialic acid molecules on the cell surface are clustered (Kakio et al., 2001;Kakio et al., 2004). Based on these data, we had previously prepared sialic acid conjugated dendrimeric polymers of various sizes that mimicked the clustered sialic acid structure of the cell surface, and that bound with specificity to A β (Patel et al., 2006). We have shown that by introducing sialic acid-conjugated dendrimers to an in vitro system of SH-SY5Y neuroblastoma and Aβ, Aβ-induced neurotoxicity was attenuated. In these constructs, sialic acid molecules were attached using EDC chemistry to the amine termini of the dendrimers via the carboxylic acid group of the sialic acid. This attachment is different than that found on cell surface gangliosides in which sialic acid moieties are attached to the rest of the gangliosides via the anomeric hydroxyl group. In the current work, we constructed sialic acid functionalized dendrimers of similar sizes as before, but with the physiologically relevant attachment. Furthermore, we tested the ability of these constructs to attenuate A β -induced neurotoxicity and compared their efficacy to do so with sialic acid-dendrimer complexes made using the non-physiological attachment chemistry. Fig. 1 illustrates the differences in structure of these two constructs. Sialic acid dendrimer complexes made using the physiological attachment attenuated A^β toxicity at lower concentrations than those made with the non-physiological attachment, although the binding affinity of the constructs for A β did not improve with physiological attachment of the sialic acid. These results could have implications for the design of new agents that bind pathogenic A β peptides for the treatment of neurodegenerative disease.

2. Results

We have previously shown that artificial clusters of sialic acid that mimic cell surface sialic acid can act as decoy molecules for A β binding and attenuate A β induced neurotoxicity *in vitro* (Patel et al., 2006). The sialic acid moieties on those decoy molecules were attached to PAMAM dendrimers via the carboxylic acid group of the sialic acid (Fig. 1). Here, we prepared sialic acid conjugated dendrimers for use as A β binding decoy molecules in which the sialic acid moieties were attached to the dendrimers in a biologically relevant manner via the anomeric hydroxyl group of the sialic acid. We hypothesized that the biologically relevant attachment of sialic acid to dendrimers would improve the performance of the dendrimers in A β toxicity attenuation assays because the physiological attachment would lead to increased binding affinity of A β to dendrimers and decreased intrinsic toxicity of the sialic acid modified dendrimers.

Dendrimer Characterization

We used FTIR and NMR to confirm synthesis of the sialic acid conjugated dendrimers, shown in Figures 2 and 3, respectively. We used relative abundance of certain protons in the NMR spectra along with a colorimetric periodate-recorcinol assay to determine the percent of total end groups on the dendrimer that were sialic acid modified (Table 1). Using the physiological sialic acid attachment, a greater percent sialation was observed with the generation 4.0 dendrimer than the generation 3.0 dendrimer. Sialic acid conjugation was more efficient with the physiological attachment chemistry compared to the EDC chemistry used for the non-physiological attachment for the generation 4.0 dendrimer but not the generation 3.0 dendrimer.

Intrinsic toxicity of dendrimers

We examined the intrinsic toxicity of sialic acid dendrimers prepared using the physiological sialic acid attachment (Fig. 4). It is evident that for the same dendrimer concentrations, the generation 4.0 dendrimer-sialic acid complex is more toxic to the cells than the generation 3.0 conjugate. The LD_{50} values estimated from this data, along with the LD_{50} values of unconjugated dendrimers of the same size and those conjugated to sialic acid via the carboxylic acid group are compared in Table 2. Like the dendrimer sialic acid complexes conjugated via the carboxylic acid group, the newer constructs conjugated via the hydroxyl group had higher LD₅₀ values, or lower intrinsic toxicity compared to the same-sized unconjugated dendrimers. Also, for all the dendrimers, unconjugated and conjugated, the LD₅₀ values decreased with increase in generation number. For the generation 4.0 conjugate, physiological attachment of the sialic acid at the anomeric –OH resulted in a dendrimer conjugate that was less toxic than the conjugate prepared with the non-physiological attachment (at the -COOH). While sialic acid conjugation reduced the intrinsic toxicity of the generation 3.0 conjugates compared to the unmodified dendrimer, sialic acid attachment at the anomeric -OH did not significantly alter intrinsic toxicity of the generation 3.0 conjugate relative to the non-physiological attachment.

Sialic acid dendrimer – Aß binding

To test whether physiological attachment of sialic acid to dendrimers would lead to enhanced A β binding affinity to sialic acid dendrimer conjugates, we prepared equilibrium binding isotherms of radioiodinated A β to immobilized dendrimers. Representative binding isotherms for generation 4.0 are shown in Fig. 5. In Table 3, equilibrium dissociation constants for A β to sialic acid modified dendrimers are shown. There were no statistically significant differences in A β equilibrium dissociation constants for the generation 3.0 dendrimer using the different sialic acid conjugation chemistries, while physiological attachment of sialic acid led to a modest increase in dissociation constant compared to the non-physiological attachment (or a reduction in binding affinity) for the generation 4.0 dendrimer. This result indicates that by conjugating sialic acid moieties to dendrimeric termini for use as A β binding decoy molecules via the anomeric hydroxyl group instead of the carboxylic acid group does not improve its A β binding affinity. Nonetheless, the binding affinities of all the dendrimer-sialic acid conjugates were on order of 10^{-8} M.

In addition to examining the binding of $A\beta$ to sialic acid modified dendrimers, we also examined the binding of lysozyme, which is also known to form amyloid fibrils under some experimental conditions. It was found that like the sialic acid dendrimeric polymers prepared using the non-physiological attachment of sialic acid (Patel et al., 2006), the molecules prepared using a physiological attachment of sialic acid only bound lysozyme non-specifically (Fig. 5).

Attenuation of toxicity of A_β by dendrimer-SA complexes

We analyzed the ability of the sialic acid functionalized dendrimers with the physiologically relevant sialic acid attachment to attenuate toxicity of 50 μ M aggregated A β when added to differentiated SH-SY5Y neuroblastoma cells (Fig. 6). Typical cell viability after 24 hour treatment with 50 μ M A β as prepared in our laboratory was between 60 and 75 %. Fig. 6 also shows the data for unconjugated dendrimer and the older dendrimer-sialic acid complexes prepared via the non-physiological attachment chemistry for comparison. It can be seen that for the generation 3.0 conjugate with the –OH linkage, the protective effect of the dendrimer complex, and then started to decrease. Compared to the generation 3.0 conjugate with the –OH linkage maximally protected cells from A β toxicity at a lower concentration. But, the concentration of the –OH conjugate at which viability of cells decreased was also lower than concentration of the –COOH conjugate. This

is corroborated by the lower LD_{50} value of the physiological (-OH) conjugate, compared to the non-physiological (-COOH) conjugate (Table 2). The same phenomenon was observed for the generation 4.0 molecules.

To quantify this behavior of increase in viability due the protective effect of sialic acid dendrimeric polymers from A β , the data in Fig. 6 was fit to Eq. 1 and the constants obtained for the newer conjugates with the –OH linkage were compared to those obtained for the older conjugated with the –COOH linkage. Table 4 displays the A β toxicity attenuation or inhibition constants, K_i, obtained for each dendrimer. It can be seen that for the new dendrimer-sialic acid complexes generation 3.0 and 4.0 linked via the anomeric hydroxyl group, the A β toxicity attenuation constant K_i decreased, compared to the older dendrimer sialic acid complexes conjugated dendrimers prepared using a physiological sialic acid attachment were only slightly less toxic than dendrimers prepared with a non-physiological attachment of sialic acid, and had no significant improvement in binding affinity compared to the dendrimer prepared with a non-physiological attachment of sialic acid, these dendrimers attenuated the toxic effects of A β at significantly lower (a factor of 3 or more) concentrations of dendrimer.

3. Discussion

We originally hypothesized that we could generate cell surface mimicking compounds by conjugating sialic acid to PAMAM dendrimers, and that the efficacy of these compounds in attenuating A β toxicity would be related to sialic acid valency, physiological attachment of the sialic acid, and intrinsic toxicity of the sialic acid dendrimer conjugate. In this work we compare data obtained from dendrimers in which sialic acids were conjugated at the anomeric –OH (physiological attachment) and at the carboxylic acid (non-physiological attachment).

We had hoped that the chemistry used in this work that produced a physiological sialic acid attachment to the dendrimers would result in increased sialation of dendrimers compared to EDC chemistry used in previous work (Patel et al., 2006), and thus reduce the instrinsic toxicity of the polymers. Others have shown that toxicity of these dendrimeric compounds is a function of both size or molecular weight of the molecule, and the charge on their termini (Choksakulnimitr et al., 1995;Fischer et al., 2003;Reuter et al., 1999;Wittmar et al., 2005). As seen in Table 1, only for the generation 4.0 dendrimer did we increase sialic acid conjugation relative to the dendrimers prepared with the non-physiological attachment of sialic acid. As seen in Table 2, the intrinsic toxicity of the newer sialic acid conjugated dendrimer generation 4.0 that was conjugated via the anomeric –OH group was slightly less cytotoxic than its counterpart conjugated via the –COOH group. This is not surprising given that the surface charge of the generation 4.0 molecule had been greatly reduced by the higher degree of sialic acid modification. With the same reasoning, it is apparent for generation 3.0 that the lower degree of modification achieved with the physiological (anomeric -OH) conjugation compared to the non-physiological (-COOH) attachment resulted in lesser dendrimer charge reduction and thus a more toxic construct.

We have previously shown that increasing the number of sialic acid moieties on a dendrimer resulted in a higher A β binding affinity and greater A β toxicity attenuation ability (Patel et al., 2006). This concept of improving a desired property in a molecule by multivalency has been nicely reviewed by Huskens (Huskens, 2006) and demonstrated by various groups in different biological systems (Kumar et al., 2006;Lees et al., 1994;Polizzotti and Kiick, 2006;Prieto et al., 2006;Woller and Cloninger, 2002). But this enhancement in A β binding with greater sialic acid valency was at the cost of increasing toxicity due to the larger size of dendrimers used to cluster more sialic acid. We had hoped that with a sialic acid attachment that was more biologically relevant, we would increase sialic acid conjugation efficiency, and thus increase

valency without increasing size of dendrimer and the dendrimer intrinsic toxicity. We were only partially successful in increasing the sialic acid conjugation of the dendrimers (generation 4.0 only, Table 1). The increased conjugation efficiency of the generation 4.0 dendrimers with the physiological sialic acid attachment, and associated increased sialic acid valency, was associated with an increased ability to attenuate $A\beta$ (Fig. 6, Table 4).

We had believed that physiological attachment of sialic acid relative to the non-physiological attachment of sialic acid to dendrimers would lead to greater A β binding to the dendrimers as some investigators have suggested that sialic binding proteins in general (Attrill et al., 2006) and Aß in particular (Williamson et al., 2006) bind to the carboxylic acid on sialic acid via a positively charged amino acid residue. The same electrostatic interactions have been noted for sialic acids that are associated with gangliosides and the peptides that bind to those sialic acids (Ariga and Yu, 1999; Valdes-Gonzalez et al., 2001; Williamson et al., 2006). This electrostatic interaction would not occur with sialic acid modified dendrimeric polymers prepared with the -COOH attachment, but could occur in polymers prepared with the -OH sialic acid attachment. As seen in Fig. 5 and Table 3, while $A\beta$ bound to dendrimers specifically and with an affinity at least an order of magnitude higher than what others have measured for A β binding to gangliosides (Ariga et al., 2001; Choo-Smith et al., 1997), there was no improvement in measured binding affinities of AB towards dendrimers with physiological sialic acid attachment compared to the non-physiological attachment. The lower dissociation constant or improved affinity seen with the sialic acid modified dendrimers compared to gangliosides may be due to the clustering of sialic acids on the dendrimeric polymers, or the combined effects of the electrostatic interaction of A β with the dendrimer backbone and the interaction of A β with the surface sialic acids on the dendrimer.

While there was no significant improvement in the ability of the same polymers to bind $A\beta$, there was a small improvement in ability of sialic acid polymers to attenuate AB toxicity when the sialic acid was attached to the polymer using a physiologically relevant chemistry as compared to the less relevant chemistry. There are several possible explanations for this apparent anomaly. We have assumed that the sialic acid conjugated dendrimers attenuated A β toxicity because of their ability to compete with the cell surface for A β binding. However, we have not examined A β binding and A β toxicity at the same concentration ranges. Low concentrations of A β were needed to get sensitive estimates of binding affinity, while higher concentrations of A β were needed in order to get reproducible estimates of A β toxicity. Thus, different physical phenomena could be occurring at the different concentration regimes. In particular, the aggregation properties of AB may change dramatically at the different concentrations. An alternate mechanism of action of sialic acid conjugated dendrimers than the one we propose (i.e. competitive binding of $A\beta$) is that the positively charged dendrimer associates with the negatively charged cell surface, thus preventing transport of the A β to the cell surface. If this alternate mechanism were responsible for the observed AB toxicity attenuation, we would expect to see toxicity attenuation regardless of the degree of sialic acid modification of the dendrimer and chemistry with which the sialic acid was attached. Based on our results, we can not discriminate between the two potential mechanisms of action of the sialic acid conjugated polymers.

We expected improved binding of $A\beta$ to sialic acid dendrimers with the use of the physiological attachment of sialic acid, however, this improved binding affinity was not observed. We may have maintained the negative charge on the sialic acid that others suggest in important for $A\beta$ binding by attaching the sialic acid to a dendrimer at the anomeric –OH. However, it is possible that we obscured any attractive electrostatic interactions of $A\beta$ to sialic acid by attaching the sialic acid to a polycationic dendrimer. Moreover, it is possible that crowding sialic acid to a spatial arrangement that suboptimal for $A\beta$ binding (Ariga et al., 2001). It is also possible that if the deprotecting or demethylation step in the chemistry was

Brain Res. Author manuscript; available in PMC 2008 August 3.

not complete, the negative charges of the sialic acid were not recovered, leading to a lower affinity for A β . Thus, we believe that with the use of a less highly charged polymer backbone and longer spacer between the charged polymer and the sialic acid, we may have seen greater A β binding affinity and greater toxicity attenuation properties of sialic acid polymers that employed a physiological attachment chemistry than seen in this work.

It is not clear from our data if monomeric, oligomer or more aggregated (fibril or protofibril) forms of $A\beta$ bind to the sialic acid modified dendrimers. Work by Matsuzaki and coworkers indicate that fresh, not aggregated $A\beta$ binds to cell surface gangliosides (Wakabayashi et al., 2005). On the contrary, work by others suggest that aggregated species bind gangliosides and that the oligomerization or fibrillization is independent of $A\beta$ binding to gangliosides (Inaba et al., 2005;Williamson et al., 2006). In toxicity experiments reported here, $A\beta$ was prepared such that there was always a mixture of both small and large $A\beta$ oligomers.

There has been some controversy over the years as to the size of the toxic A β oligomer (Dahlgren et al., 2002;Kayed et al., 2003;Wang et al., 2002;Ward et al., 2000), confounded somewhat by the probability that A β aggregates when associated with cell membranes during the course of a toxicity experiment (Inaba et al., 2005). We can not address what form of A β binds to GM1 rich regions of cells and/or eventually leads to toxicity, nor can we address what population of A β species bind to sialic acid modified dendrimers prepared in experiments reported here.

In recent years there has been great interest and progress made in the development of molecular level strategies to target the formation, deposition, and cellular interaction of A β associated with neurotoxicity seen in Alzheimer's disease (Blumberg, 1988;Etcheberrigaray et al., 2004, Blanchard et al., 2004; Ghanta et al., 1996, Gelinas et al., 2004; Hock et al., 2003; Mandavilli, 2006; Mount and Downton, 2006; Schenk et al., 2004). There is increasing evidence that molecules that sequester A β show mitigation in A β induced neurotoxicity (Drouet et al., 1999). Moreover, there is evidence that agents which sequester A β in the plasma may actually be effective at reducing A β levels in the cortex and may have the potential of reducing cognitive decline associated with disease (Bard et al., 2000;Bergamaschini et al., 2004; DeMattos et al., 2001; Matsuoka et al., 2003). In the current and previous works, we have demonstrated that sialic acid functionalized dendrimers that mimic cell surface sialic acid clusters can bind Aβ and attenuate Aβ induced neurotoxicity in vitro (Patel et al., 2006). In the current work, we demonstrated that attachment of sialic acid to dendrimeric termini via the anomeric hydroxyl group as opposed to the carboxylic acid group modestly enhances their ability to mitigate A β induced neurotoxicity. These findings add to our understanding of the A sialic acid interaction and encourage further investigation into the development of sialic acid modified materials for use in prevention of AB toxicity.

4. Experimental Procedures

Materials

A β (1–40) was purchased from Biosource International (Camarillo, CA). Human neuroblastoma SH-SY5Y cells were purchased from ATCC (Manassas, VA). Cell dissociation buffer and cell culture reagents were purchased from Gibco-Invitrogen (Grand Island, NY). Propidium iodide (PI) was purchased from Molecular Probes (Eugene, OR). Human recombinant nerve growth factor – β (NGF- β), sialic acid (N-Acetylneuraminic acid, NANA) and polyamidoamine (PAMAM) dendrimer polymers generation 3.0 and 4.0 were purchased from Sigma-Aldrich (St. Louis, MO)., Iodo-Beads, G-5 desalting columns, Bolton-Hunter reagent (Sulfo-SHPP) and AminoLink Coupling Gel were purchased from Pierce Biotechnology (Rockford, IL). ¹²⁵I was purchased from Amersham Biosciences (Piscataway, NJ). Ultrafiltration membranes were purchased from Millipore (Billerica, MA). All other chemicals were purchased from Sigma-Aldrich.

Peptide preparation

 $A\beta(1-40)$ stock solutions were prepared by dissolving the lyophilized peptide in anhydrous dimethyl sulfoxide (DMSO) to make 10 mg/ml stock solutions. After incubating for 30–45 minutes to 1h at 25°C, stock solutions of A β were diluted directly to their final concentrations in sterile cell culture medium and rotated at 25°C for 24 h prior to addition to cells. This method of peptide preparation yielded A β fibril and other aggregated species containing samples that were consistently toxic to cells in culture at concentrations between 20 and 100 μ M (Lee et al., 2005;Lee et al., 2006;Patel et al., 2006;Rymer and Good, 2001).

Cell culture

Human neuroblastoma SH-SY5Y cells were cultured in a humidified 5% CO₂/air incubator at 37°C in Minimum Essential Media (MEM), supplemented with 10% (vol/vol) fetal bovine serum, 2.2mg/ml NaHCO₃, 100 U/ml penicillin, 100 µg/ml streptomycin and 2.5 µg/ml amphotericin B (fungizone). SH-SY5Y cells were NGF differentiated prior to use in toxicity experiments by addition of 20 ng/ml NGF to cells for 5–7 days in 96 well plates.

Synthesis and purification of sialic acid-conjugated dendrimeric polymers

The procedure was adapted from work done by Woller et al. (Woller and Cloninger, 2002;Woller et al., 2003).

Acetylation of sialic acid (compound 1)

The acetyl protection was performed by first dissolving 250 mg of NANA in 10 ml of pyridine. To this solution was added 537 mg (497 μ L) of acetic anhydride and 37 mg of 4- (dimethylamino)pyridine (DMAP). The solution was reacted at room temperature for 3 hours. After 3 hours, a 1 ml solution of hydrazine acetate in dimethyl formamide (DMF) was added to the pyridine solution. The mixture was reacted at 55°C for 15 min. 1 ml trichloroacetonitrile and 45.3 μ l of 1,8- diazabicyclo[5.4.0]undec-7-ene (DBU) were then added, and the system was reacted at 0°C for 1.5 hours. The final solution was stored at -80°C until used.

Production of 2-(2-isothiocyanatoethoxy ethanol) (compound 2)

A solution containing 700 μ l of 2-(2-aminoethoxy)ethanol and 2 ml of triethylamine in 10 ml of chloroform was added slowly over the course of an hour to a stirred solution containing 540 μ l of thiophosgene in 40 ml of chloroform. The solvent was removed *in vacuo*. The resulting residue was dissolved in 10 ml of deionized water. A two-step extraction was performed using two 10 ml volumes of dichloromethane. The organic phases from the extraction were combined and washed twice with deionized water (2 × 10 ml). The organic layer was then dried over magnesium sulfate and filtered. The solvent was removed *in vacuo*. The resulting yellowish oil was stored at -80° C until used.

Attachment of compound 2 to dendrimer (compound 3)

 $60 \mu l$ (2.89 µmoles) of the generation 3.0 dendrimer or 107 µl (0.75 µmoles) solution of generation 4.0 polyamidoamine (PAMAM) (0.57 µmol of dendrimer) was evaporated under reduced pressure. The resulting residue was dissolved in 5 ml of dimethyl sulfoxide (DMSO). A 1.5-fold molar excess of compound 2 was added to the DMSO mixture (this excess is based on the number of terminal amines available on the dendrimer and not the amount of dendrimer). The solution was reacted at room temperature for 8 hours. The solvent was removed *in vacuo*.

Attachment of sialic acid (compound 4)

The residue of compound 3 was dissolved in 20 ml of dichloromethane with 80 mg of 4Å molecular sieves under nitrogen. To the solution, equimolar quantities of (to dendrimeric terminii) of compound 1 and 200 μ L boron trifluoride-diethyl etherate was added slowly. The solution was reacted at room temperature for 7 hours. Sodium bicarbonate (100 mg) was added to the solution, and the solution was filtered over celite 545 filter agent. The solvent was removed *in vacuo*. The resulting compound was stored at -80° C until used.

Deprotection of sialic acid

Compound 4 was dissolved in 20 ml of a methanol/deionized water mixture (1:1). Methanolic base (1 M, 180 μ l or till pH reached 9.5) was added, and the solution was mixed overnight until all solid was dissolved. The solution was neutralized with Amberlite IR-120 and filtered using a glass filter. The solvent was removed *in vacuo*. The resulting residue was dissolved in deionized water, and purified using 10 kDa centrifuge filter units. The resulting solution was stored at 4°C until used.

Verification and quantification of extent of sialic acid conjugation

Verification of the presence of sialic acid on dendrimers was done by FT-IR spectroscopy using a System 2000 FTIR (Perkin Elmar, Norwalk, CT). The FTIR spectra of the unconjugated and conjugated dendrimers with both attachments are shown in Fig. 2. It is apparent by the presence of certain characteristic structures (thiourea, carboxylic acids, and alicyclic alcohols) and the loss of other peaks (amine structure) that the chemistry was successful. Moreover, the spectra for the sialic acid conjugated dendrimers with the anomeric hydroxyl group attachment shows the carboxylic acid group peak at 1730 cm⁻¹ that the older constructs do not show, suggesting that there are indeed, unmodified –COOH groups on the newer constructs.

Conjugation to sialic acid was also confirmed by the Periodate-Recorcinol assay that estimates the amount of sialic acid in the sample (Bhavanandan and Sheykhnazari, 1993). Samples were diluted in 0.1 N sulfuric acid and containing 0.2% sodium dodecyl sulphate. Hydrolysis of the sialic acid moieties was carried out at 80°C for 1h. After samples were allowed to equilibrate to room temperature, 40 μ l of the samples were mixed with 10 μ l periodic acid solution (0.032 M), shaken for 5 min and kept on ice for 35 min. Then, 100 μ l of recorcinol solution (0.6 g in 100ml 6 N HCl containing 25 µmol copper sulphate) was added. The samples were then covered and kept at 80°C for 1h. After adding 100 µl of tert-butyl alcohol to the samples, their absorbances were read at 650 nm as an estimate of amount of sialic acid present. The percentage sialation found in the generation 3.0 and 4.0 dendrimer sialic acid complexes were found to be 51 ± 3 and 56 ± 9 respectively. The thiol group present on the linker may have interfered in the assay. Thus, for confident estimates of percentages of sialic acid labeling, proton NMR was utilized. The solvent in the dendrimer solutions were evaporated using the Savant Speed Vac Plus concentrator (Cambridge Scientific Products, Cambridge, MA). The material was then dissolved in d₆-dimethyl sulphoxide to a concentration of roughly 5 mg/ml for 4 h prior to NMR scanning using the Joel ECX400 NMR system. 1024 scans were taken for each sample. Fig. 3 shows the NMR spectra of the generation 4.0 dendrimer sialic acid complex. The peaks at 7.09 ppm represent the protons neighboring the thiol group (NHCSNH) on linkers attached to dendrimeric termini but not to sialic acid. The peak at 7.6 ppm represents the protons neighboring the thiol group (NHCSNH) on linkers attached to both, dendrimeric termini and sialic acid. The peaks from 7.9–8.4 ppm represent the internal amides of the dendrimers. Table 1 shows the percentage sialation of the sialic acid functionalized dendrimers with the two different attachments for the different generations of dendrimers used. The low degree of sialic acid labeling for generation 3.0 may be attributed to the possible inhomogeneity of the dendrimer. The structural defects may have precluded a higher percentage labeling.

PI toxicity assay

Cell toxicity was measured as previously described (Patel et al., 2006). NGF-diiferenciated SH-SY5Y cells were stained with PI, a nucleic acid dye that stains cells with permeable membranes. In all experiments, $A\beta$ was added to cells approximately 30 minutes prior to the addition of dendrimer-sialic acid conjugates. 24 hours after addition of A β or other agent, cells were prepared for viability measurement as before using the FACSArray Bioanalyzer (Becton-Dickonson, Bedford, MA). Gating was done so as to obtain percentages of the total cell population that were viable. Normalized viability values were obtained by dividing the percentage of viable cells in the sample by that in the control samples with no $A\beta$ or other agent.

Estimation of LD₅₀ values and toxicity inhibition parameters

 LD_{50} values, defined here as concentrations of dendrimer-sialic acid conjugate that led to a 50% reduction in cell viability, were obtained by linear interpolation of viability as a function of concentration data about the region of 50% viability. The uncertainty of the concentration of dendrimer was estimated by determining the 95% confidence interval of concentration from the viability curves, and using that to determine a coefficient of variation of the measurement.

We estimated toxicity inhibition constants for sialic acid dendrimers by fitting Equation (1) to viability using a non-linear least squares regression method (KaleidaGraph 3.6, Synergy Software, Reading, PA) (Patel et al., 2006).

$$V = V_0 + \frac{D_{SA}}{D_{SA} + K_i} * (V_{\max} - V_0) - \frac{D_{SA}}{k_t}$$
(1)

V is the normalized viability of the cell sample treated with 50 μ M A β and dendrimer-sialic acid conjugate. V_o is the normalized viability of the cell sample treated with 50 μ M A β and zero dendrimer-sialic acid conjugate. V_{max} is the maximum normalized viability attainable if treatment with sialic acid modified dendrimer totally protected cells from A β . V_{max} approaches a theoretical limit of 100%. K_i and k_t are empirical constants associated with sialic acid binding to A β (and inhibition of its toxicity by sequestering A β), and with the intrinsic toxicity of the dendrimer conjugates, respectively.

Radiochemical Binding assay

Binding of A β to sialic acid conjugated dendrimers was determined as previously done using radiochemical techniques. A β (1–40) was radioiodinated via a modified Bolton Hunter method to preferentially label at the N terminus of the peptide. Labeling at other primary amines was inhibited by maintaining the pH below the pKa of those residues. 100 nmol of sulfo-SHPP was iodinated with 200 µCi of ¹²⁵I using the IodoBead catalyst for 15 minutes at pH 8.0 borate buffer in a volume of 140 μ L. After removal of the catalyst, 2 nmol (100 μ L) of freshly prepared β -amyloid(1–40) (in water) was added and allowed to react to the iodinated sulfo-SHPP for 3 hours at 4°C. The resulting condensation product was separated from free ¹²⁵I using a G-5 desalting column, employing phosphate buffer as the eluent. By precipitation of the peptide with 20 wt% trichloroacetic acid in the presence of 1 mg/ml bovine serum albumin, the precipitatable activity was determined to be 80%. Peptide concentration was determined from the activity of the ¹²⁵I-labeled A β by assuming that the peptide was recovered from the desalting column using one column volume of the eluting buffer and that the peptide concentration was proportional to the precipitatable activity of the fraction. No attempt was made to remove unlabeled peptide from labeled peptide. Relative aggregation state of the peptide was assessed using native polyacrylamide gel electrophoresis, counting activity of sliced sections of gel to determine relative abundance of different molecular weight species.

The iodinated peptide was approximately 60% monomer or dimer, with the balance being large (above 100 kDa) aggregate.

Lysozyme was iodinated directly without using sulfo-SHPP. Two Iodobeads were added to 100 μ L PBS, to which 100 μ Ci ¹²⁵I (10 μ l) were added. 390 μ L of 1mg/ml of lysozyme was incubated in the presence of ¹²⁵I and Iodobeads for 10 minutes. Iodinated protein was separated from free ¹²⁵I using G-5 desalting columns. Iodinated protein concentration was determined from UV absorbance at 280 nm. The dendrimer-sialic acid complexes were immobilized to AminoLink agarose coupling gels that were activated to form aldehyde functional groups reactive with primary amines. These gels were used in radiochemical binding assays within 10 days of preparation.

Binding assays were carried out by incubating ¹²⁵I-labeled protein of different concentrations (nanomolar level) with 10 μ L of the immobilized dendrimer-sialic acid complexes (~10 μ M end concentration) of different generations at room temperature for 2 h. Tween-20 was also added at a final concentration of 0.1 % to block nonspecific binding. Thereafter, free A β was removed from that bound to the immobilized gel by centrifugation at 12,000 g for 5 minutes. The activities of both bound and unbound A β were counted separately using a Wallac MicroBeta TriLux microplate liquid scintillation counter (Perkin Elmer, Wellesley, MA). Equilibrium binding isotherms for binding to immobilized dendrimers or sialic acid conjugated dendrimers were corrected for binding of protein to unmodified agarose gel. Binding constants were determined from these resultant equilibrium binding isotherms by fitting a langmuir isotherm (Equation 2) to the data using a non-linear least squares regression algorithm in KaleidaGraph.

$$C_{abs} = \frac{C_t * C_{ab}}{K_{A\beta} + C_{ab}}$$
(2)

where C_{abs} is the amount of bound A β to the dendrimer-gel, C_{ab} is the concentration of free A β , C_t is the total A β binding sites on the surface of the gel, and $K_{A\beta}$ is the equilibrium dissociation constant (M).

Supplementary Material

Refer to Web version on PubMed Central for supplementary material.

Acknowledgements

We would like thank Dr. Mary Cloninger for her guidance with the chemistry. The study was supported by grants from the NIH (NS050346, AG025586).

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Figure 1.

Two different attachments of the sialic acid moiety on the dendrimers: (a) non-physiological attachment of sialic acid to dendrimeric termini via carboxylic acid and (b) physiological attachment of sialic acid to dendrimeric termini via anomeric hydroxyl group.



Figure 2.

FTIR of conjugated and unconjugated PAMAM dendrimer generation 3.0. The dashed line represents the unconjugated dendrimer. The dotted line represents the sialic acid conjugated dendrimer attached to dendrimeric termini via the carboxylic acid group. The solid line represents sialic acid conjugated dendrimer attached via the anomeric hydroxyl group of the sialic acid. The –COOH peak can be seen at 1730 cm⁻¹ indicating linkage of sialic acid via the hydroxyl group and not the carboxylic acid group.



Figure 3.

Proton NMR spectra of dendrimer sialic acid complex 4.0. Peaks ranging from 8.6 to 7.9 ppm represent the protons on the internal amides of the dendrimer. Peaks at 7.0., 7.6 and 9.6 represent the two protons in the linker (linked to the dendrimer termini but not to sialic acid), two linker protons (linked to dendrimer termini and sialic acid) and two linker protons (linker to dendrimer termini and sialic acid).



Figure 4.

Intrinsic toxicity of sialic acid conjugated dendrimers 3.0 (open squares) and 4.0 (closed triangles) conjugated via the anomeric hydroxyl group.



Figure 5.

Representative equilibrium binding isotherms of A β (filled circles) and lysozyme (open circles) to dendrimer-sialic acid conjugate 4.0 with –OH linkage. The dashed line represents the fit of Eq. (2) to the data for A β binding.



Figure 6.

Normalized viability upon treatment with unconjugated dendrimer (open triangles), sialic acid conjugated dendrimers attached via carboxylic acid group (open circles), and sialic acid conjugated dendrimers attached via hydroxyl group (closed circles). (A) Generation 3.0 dendrimers. (B) Generation 4.0 dendrimers. The dashed line represents the model fit of Eq. (1) to sialic acid conjugated dendrimers attached via carboxylic acid group and the solid line represents the model fit to the data for the sialic acid conjugated dendrimer attached via the hydroxyl group. Viability data upon treatment with sialic acid conjugated dendrimers attached via carboxylic acid group adapted from Patel et al., 2006, with permission from Elsevier.

Percentage conjugation of dendrimeric termini with sialic acid determined by proton NMR

	Percentage sialation		
Generation	-COOH attachment	-OH attachment [*]	
3.0 4.0	41.4 21.8	22.5 61.2	

Percentages dendrimeric termini that were conjugated to the linker (not linked to sialic acid) and to linker (linked to a lactone derivative of sialic acid) were calculated to be 1.4 and 1.2 for dendrimer sialic acid complex 3.0, and 1.32 and 1.35 for generation 4.0 respectively.

LD₅₀ values for unconjugated and sialic acid conjugated dendrimers. LD₅₀ of sialic acid conjugated dendrimer conjugated at –COOH reprinted from Patel et al., 2006, with permission from Elsevier.

	LD ₅₀ (μM dendrimer)			
Generation	Unconjugated	Conjugated via -COOH group	Conjugated via anomeric –OH group	
3.0 4.0	$\begin{array}{c} 10\pm7\\ 1.7\pm0.2 \end{array}$	42 ± 14 3.5 ± 1.2	$\begin{array}{c} 26.8 \pm 9.6 \\ 16.4 \pm 1.6 \end{array}$	

Equilibrium dissociation constants for $A\beta$ to different generations with sialic acid modification. Equilibrium constant for dendrimer conjugated via –COOH reprinted from Patel et al., 2006, with permission from Elsevier.

	K _{Aβ} (μM	
Generation	-COOH attachment	-OH attachment
3.0 4.0	$\begin{array}{c} 0.02 \pm 0.01 \\ 0.009 \pm 0.005 \end{array}$	$\begin{array}{c} 0.02 \pm 0.01 \\ 0.05 \pm 0.03 \end{array}$

Model constants for different generations of sialic acid-conjugated dendrimers. Constants for dendrimer conjugated via –COOH reprinted from Patel et al., 2006 with permission from Elsevier.

	Кі (µ)		
Generation	-COOH attachment	-OH attachment	
3.0 4.0	$\begin{array}{c} 0.3 \pm 0.005 \\ 0.07 \pm 0.002 \end{array}$	$\begin{array}{c} 0.1 \pm 0.081 \\ 0.024 \pm 0.019 \end{array}$	

Brain Res. Author manuscript; available in PMC 2008 August 3.