# Is Measurement of End-tidal CO<sub>2</sub> Through a Nasal Cannula Reliable?

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When using a nasal cannula to sample gases expired by a patient, air from the room may dilute the sample. For this reason, the accuracy of the partial pressure of endtidal carbon dioxide ( $E_TCO_2$ ) measurements is questionable. We experimentally examined the reliability of  $E_TCO_2$  measurements through a nasal cannula and found that they depended on both biological factors (tidal volume and respiratory rates) and mechanical factors (the diameter and the length of the cannula and the diameter of the prongs). These results suggest that the correct use of an appropriate sampling cannula will provide reliable  $E_TCO_2$  measurements without clinical problems.

**Key Words:** End-tidal CO<sub>2</sub>; Nasal cannula; Capnography.

**C**apnography is useful for respiratory monitoring during intravenous sedation.<sup>1-6</sup> However, because the air in a room may dilute the gases expired by a patient during sampling through a nasal cannula, a question arises regarding the accuracy of measurements of the partial pressure of end-tidal carbon dioxide ( $E_TCO_2$ ). It is necessary to have accurate values of  $E_TCO_2$  during intravenous sedation to detect respiratory depression, including apnea. In this study we experimentally examined this issue, including the reliability of various nasal cannulas for measuring  $E_TCO_2$ .

#### **METHODS**

### **Experimental Model**

Figure 1 shows the experimental model. We used a volume-limited ventilator (ARF-850E; Acoma Medical Industry, Tokyo, Japan) as a model lung. By connecting a  $CO_2$  cylinder to the ventilator, the rate of delivery of  $CO_2$  was constant. The experimental model also allowed us to preset the partial pressure of the  $CO_2$  eliminated at 40 mmHg. A face model, with a dead air space of 150 ml, was connected to the ventilator. Two types of nasal cannulas were examined (Figure 2). The type

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one cannula was handmade and used for carbon dioxide sampling and oxygen delivery. The cannula was 300 cm long and composed of two portions. The distal 80-cm portion, including the prongs, was 2.0 mm in diameter. The proximal 220-cm portion was only 1.7 mm in diameter. The distal portion had a removable part, which was 53 cm long that permitted us to change the length of the cannula (from 300 to 247 cm), the diameter of the cannula (from 2.0 to 1.5 mm), and the diameter of the prongs (from 2.0 to 1.0 mm). The type two cannula is commercially available (Model 4000; Salterlabs). This cannula was 240 cm long and 1.5 mm in diameter, but the prongs were only 1.0 mm in diameter.

#### **Experimental Protocol**

The  $E_TCO_2$  of the expired gas from the experimental model was sampled with an anesthetic gas monitor (Capnomac; Datex, Helsinki, Finland) using both types of nasal cannulas. The sampling rate was calibrated to 200 ml/min. The  $E_TCO_2$  was measured under the following seven different conditions: tidal volumes ( $V_T$ ) of 250, 380, and 500 ml with respiratory rates (RR) of 10 and 14/min, and a  $V_T$  of 250 ml with a RR of 20/min. With the type one cannula, the  $E_TCO_2$  was measured under three additional conditions: changing the diameter of the prongs from 2.0 to 1.0 mm, changing the diameter of the distal portion of the cannula from 2.0 to 1.5 mm, and changing the length of the cannula, the  $V_T$  was

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**Figure 1.** Experimental model: the  $CO_2$  was delivered at a constant flow rate from the cylinder. The partial pressure of the  $CO_2$  eliminated from the nares of the face model was preset to a constant 40 mmHg.

gradually increased from 380 to 500 ml at a constant RR of 14/min. This protocol was used to detect the  $V_T$  level at which the  $E_TCO_2$  approximated 40 mmHg, the preset partial pressure of the  $CO_2$  eliminated.

### RESULTS

The measurements were repeated many times in this study and equivalent values were obtained for each ex-



**Figure 2.** Type one nasal cannula (handmade) showing the anterior portion (diameter 2.0 mm, length 80 cm), posterior portion (diameter 1.7 mm, length 220 cm), removable anterior portion (diameter 1.5 mm, length 53 cm), and the prongs (diameter 2.0 mm). Type two nasal cannula (Salterlabs model 4000) showing the prongs (diameter 1.0 mm) and the tube (diameter 1.5 mm, length 240 cm).

periment. Larger  $V_T$  resulted in more reliable  $E_TCO_2$ measurements (Figure 3) than did smaller  $V_T$ . The type two cannula for a  $V_T$  of 500 ml produced an accurate  $E_TCO_2$ , measurement; however, the type one cannula for a  $V_T$  of 250 ml showed far less  $E_TCO_2$  than the preset partial pressure of the  $CO_2$  eliminated. Lower RR



**Figure 3.** A larger tidal volume  $(V_T)$  resulted in a more reliable measurement of the partial pressure of the end-tidal carbon dioxide  $(E_T CO_2)$ 



**Figure 4.** A lower respiratory rate (RR) resulted in a more reliable measurement of the partial pressure of the end-tidal carbon dioxide ( $E_TCO_2$ ).

gave more reliable  $E_TCO_2$  measurements (Figure 4) than higher RR did. The type two cannula for RR of 10 and 14/min and a  $V_T$  of 500 ml gave accurate  $E_TCO_2$  values, but the type one cannula for the same conditions showed less  $E_TCO_2$  than the preset partial pressure of the  $CO_2$  eliminated. For the lowest  $V_T$  and the highest RR, the  $E_TCO_2$  measured using the type two cannula was 37 mmHg, and it was 28 mmHg when the type one cannula was used. The latter value is far less than the preset partial pressure of the  $CO_2$  eliminated (Figure 5a). This value was slightly improved by using the smaller diameter prongs (Figure 5b), by using the smaller diameter cannula (Figure 5c), or by using the shorter cannula (Figure 5d). When the  $V_T$  was gradually increased with a constant RR of 14/min using the type two cannula, the value for  $E_{\rm T} CO_2$  approximated 40 mmHg at 410 ml  $V_{\rm T}.$ 

#### DISCUSSION

The accuracy of the  $E_TCO_2$  measurements depends on several factors, including the  $V_T$  and the RR (biological factors) and the diameter and length of the cannula (mechanical factors). The capnogram shows a plateau when the alveolar gas is expired because, at that time, the gas in the dead air space no longer influences the capnogram. The maximum value at the end of the plateau is equal to the alveolar  $CO_2$  concentration. For the  $E_TCO_2$ to approximate the alveolar  $\mbox{\rm CO}_2$  concentration, there must be sufficient  $V_T$  to completely flush the dead air space. Badgwell et al reported that low  $V_T$  values resulted in low  $E_T CO_2$  values.<sup>7</sup> Kugimiya pointed out that in cases of anesthetized small children with low  $V_{T}$ , even 20 ml of dead air space results in low  $E_T CO_2$  values.<sup>8</sup> In spontaneously breathing patients, the dead air space is about twice as large as the dead air space in intubated patients. Therefore the patient's dead air space, especially during low  $V_T$ , may readily influence the values of  $E_TCO_2$  monitored using a nasal cannula. An increase in the RR causes parabolic distortion of the capnogram that is followed by a decrease in the value of  $E_T CO_2$ because the time is too short to eliminate the gases in the dead air space.9,10 These results suggest that inaccurately low  $E_TCO_2$  levels may be detected during low



**Figure 5.** Capnographs when the tidal volume was 250 ml and the ventilation rate was 20/min. (a) The difference in values of the partial pressure of the end-tidal carbon dioxide ( $E_TCO_2$ ) between type one and type two nasal cannulas. (b) The effect of reducing the diameter of the prongs of the type one nasal cannula from 2.0 to 1.0 mm. (c) The effect of reducing the diameter of the type one nasal cannula from 2.0 to 1.5 mm. (d) The effect of reducing the length of the type one nasal cannula from 300 to 247 cm.



**Figure 6.** The smaller the cross-sectional area of the prongs of nasal cannula, the less likely the values of the partial pressure of the end-tidal carbon dioxide will be reduced by the surrounding air.

 $V_T$  and high RR, such as sedation with intravenous midazolam.<sup>11,12</sup>

The smaller diameter prongs, the shorter cannula, and the smaller diameter cannula resulted in improved measurement of  $E_T CO_2$ . The turbulence generated by the expired gases may essentially close the prongs of the cannula (Figure 6) and thus prevent the aspiration of surrounding air into the cannula. We therefore speculated that even longer prongs into the nose might improve reliability of the measurements as long as it did not cause the patient discomfort. Moreover, the capnometer with side-stream sampling, a low sampling rate, and a large diameter cannula result in a lower  $E_T CO_2$  value, because expired gases are diluted with inspired gases in the cannula.<sup>13</sup> It is clear that the  $E_T CO_2$  value was influenced by the volume of the cannula. When the type two cannula, which has a smaller volume than the type one cannula, was used in the present study, the  $E_TCO_2$  value was 37 mmHg. This value is clinically acceptable, even at a  $V_{T}$ of 250 ml and a RR of 20/min. However, thoughtless extension of the cannula should be avoided.

In conclusion, the accuracy of the measurement of the  $E_TCO_2$  through a nasal cannula depends on the patient's  $V_T$  and RR. However, if an appropriate nasal cannula is used then there should be no clinical problems and end-tidal  $CO_2$  measurements should be reliable in these situations.

#### REFERENCES

1. Ibarra E, Lees DE: Mass spectrometer monitoring of patients with regional anesthesia. Anesthesiology 1985;63: 572–573.

2. Anderson JA: Respiratory monitoring for anesthesia and sedation. Anesth Prog 1987;34:228–231.

3. Ackerman WE, Phero JC, Reaume D: End-tidal carbon dioxide and respiratory rate measurement during conscious sedation through a nasal cannula. Anesth Prog 1990;37:199–200.

4. Hunter JA: A cost-free, simple method for monitoring end-tidal carbon dioxide through nasal cannula. Anesth Prog 1990;37:301–303.

5. Derrick SJ, Waters H, Kang SW, Cwalina TF, Simmons W: Evaluation of a nasal/oral discriminate sampling system for capnographic respiratory monitoring. J Am Assoc Nurse Anesthetist 1993;61:509–520.

6. Kaneko Y: Clinical perspectives on capnography during sedation and general anesthesia in dentistry. Anesth Prog 1995;42:126–130.

7. Badgwell JM, McLeod ME, Lerman J, Creighton RE: End-tidal  $PCO_2$  measurements sampled at the distal and proximal ends of the endotracheal tube in infants and children. Anesth Analg 1987;66:959–964.

8. Kugimiya T: The difference of the  $CO_2$  values sampled at the patient side and the machine side of HME. J Jpn Clin Monit 1993;3:515–519.

9. Badgwell JM, Kleinman SE, Heavner JE: Respiratory frequency and artifact affect the capnographic baseline in infants. Anesth Analg 1993;77:708–712.

10. Sha M, Koishi K, Ohmura A, Miyaji T, Shimazu T: The influence of expiratory time on the arterial to end-tidal carbon dioxide tension differences. J Jpn Soc Clin Anesth 1993;13: 54–59.

11. Kaneko Y, Kobayashi M, Tanabe K, et al: Cardiorespiratory effects of midazolam for intravenous sedation in dentistry. J Jpn Dent Soc Anesthesiol 1985;13:600–606.

12. Forster A, Morel D, Bachmann M, Gemperle M: Respiratory depressant effects of different doses of midazolam and lack of reversal with naloxone. Anesth Analg 1983;62: 920–924.

13. Schena J, Thompson J, Crone RK: Mechanical influences on the capnogram. Crit Care Med 1984;12:672–674.