

# Maxi K<sup>+</sup> Channels and Their Relationship to the Apical Membrane Conductance in *Necturus* Gallbladder Epithelium

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**ABSTRACT** Using the patch-clamp technique, we have identified large-conductance (maxi) K<sup>+</sup> channels in the apical membrane of *Necturus* gallbladder epithelium, and in dissociated gallbladder epithelial cells. These channels are more than tenfold selective for K<sup>+</sup> over Na<sup>+</sup>, and exhibit unitary conductance of ~200 pS in symmetric 100 mM KCl. They are activated by elevation of internal Ca<sup>2+</sup> levels and membrane depolarization. The properties of these channels could account for the previously observed voltage and Ca<sup>2+</sup> sensitivities of the macroscopic apical membrane conductance ( $G_a$ ).  $G_a$  was determined as a function of apical membrane voltage, using intracellular microelectrode techniques. Its value was 180  $\mu\text{S}/\text{cm}^2$  at the control membrane voltage of -68 mV, and increased steeply with membrane depolarization, reaching 650  $\mu\text{S}/\text{cm}^2$  at -25 mV. We have related maxi K<sup>+</sup> channel properties and  $G_a$  quantitatively, relying on the premise that at any apical membrane voltage  $G_a$  comprises a leakage conductance and a conductance due to maxi K<sup>+</sup> channels. Comparison between  $G_a$  and maxi K<sup>+</sup> channels reveals that the latter are present at a surface density of 0.09/ $\mu\text{m}^2$ , are open ~15% of the time under control conditions, and account for 17% of control  $G_a$ . Depolarizing the apical membrane voltage leads to a steep increase in channel steady-state open probability. When correlated with patch-clamp studies examining the Ca<sup>2+</sup> and voltage dependencies of single maxi K<sup>+</sup> channels, results from intracellular microelectrode experiments indicate that maxi K<sup>+</sup> channel activity in situ is higher than predicted from the measured apical membrane voltage and estimated bulk cytosolic Ca<sup>2+</sup> activity. Mechanisms that could account for this finding are proposed.

## INTRODUCTION

Large-conductance (maxi) K<sup>+</sup> channels have been characterized in numerous excitable and nonexcitable tissues (Latorre and Miller, 1983; Latorre, 1986; Blatz and Magleby, 1987). Ion permeation and gating behavior in maxi K<sup>+</sup> channels have been examined in depth, and recent studies have highlighted the complexity of these processes. Maxi K<sup>+</sup> channels are highly K<sup>+</sup> selective and exhibit large (>150 pS) unitary conductances; both of these properties figure into recent models of multi-ion con-

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duction in maxi K<sup>+</sup> channels (Eisenman et al., 1986; Neyton and Miller, 1988). Gating is governed primarily by membrane voltage and internal Ca<sup>2+</sup> activity. Transitions occur among a multiplicity of open and closed states, and among qualitatively different kinetic modes (McManus and Magleby, 1988).

In excitable cells, it is clear that maxi K<sup>+</sup> channels are well suited to repolarize the cell membrane voltage during the action potential, as they activate in response to membrane depolarization and/or to transient increases in intracellular Ca<sup>2+</sup> (Lang and Ritchie, 1987). The role of maxi K<sup>+</sup> channels in nonexcitable cells, including epithelial tissues, has been more difficult to ascertain. Large-conductance Ca<sup>2+</sup>-activated K<sup>+</sup> channels are present in the apical membrane of several epithelia (for reviews see Palmer, 1986; Greger and Gögelein, 1987; Wills and Zweifach, 1987), including amphibian gallbladder (Maruyama et al., 1986). In segments of the distal tubule, maxi K<sup>+</sup> channels may provide a pathway for K<sup>+</sup> secretion, though the mechanism(s) by which channels are activated remain in question (Hunter et al., 1986; Frindt and Palmer, 1987; Guggino et al., 1987). In *Necturus* choroid plexus, maxi K<sup>+</sup> channels in the ventricular membrane appear to play a role in the volume regulatory decrease elicited by hyposmotic swelling (Christensen, 1987). In these and other cases, maxi K<sup>+</sup> channel open probability under resting conditions appears to be small (< 0.1).

In this paper, we describe maxi K<sup>+</sup> channels that are present in the apical membrane of *Necturus* gallbladder, and in dissociated *Necturus* gallbladder epithelial cells. Our major goal is to assess the contribution of these channels to the resting apical membrane K<sup>+</sup> conductance ( $G_a$ ), and to the increase in  $G_a$  elicited by apical membrane depolarization (García-Díaz et al., 1983; Stoddard and Reuss, 1988b). We develop simple models to describe the steady-state gating and conduction properties of single maxi K<sup>+</sup> channels, and use these models as a basis to draw quantitative comparisons with the apical membrane conductance, assessed using intracellular microelectrode techniques.

Parts of this work have appeared in preliminary form (Segal and Reuss, 1988).

#### MATERIALS AND METHODS

Mudpuppies (*Necturus maculosus*) were purchased from Nasco Biologicals (Ft. Atkinson, WI) or Kon's Scientific (Germantown, WI) and kept in tap water at 5°C. The animals were anesthetized in tricaine methanesulfonate. All experiments were performed at room temperature.

##### *Patch-Clamp Experiments*

*Experimental preparations.* Patch-clamp studies were carried out on intact gallbladders and on dissociated gallbladder epithelial cells from *Necturus maculosus*. In experiments on the intact gallbladder, the tissue was excised and mounted as a flat sheet, apical side up, in a modified Ussing chamber, as previously described (Reuss and Finn, 1975a, b; Weinman and Reuss, 1982). In attempts to remove mucus, the apical surface of the tissue was exposed for 1 h to 1 mg/ml hyaluronidase (Sigma Type IV or V, dissolved in NaCl Ringer's solution), and then rinsed. Hyaluronidase treatment had no effects on the electrical properties of the tissue, assessed using microelectrode techniques.

To prepare suspensions of dissociated cells, gallbladders were removed, sliced open, drained of bile, and pinned apical side up in a Sylgard-coated Petri dish filled with NaCl

Ringer's. Sheets of epithelial cells were scraped from the tissue with a glass coverslip; in many cases, it was possible to remove the entire epithelial cell layer as a single sheet. Epithelial sheets were collected with a 200- $\mu$ l pipettor and transferred to a 15-ml centrifuge tube, where they were bathed for 7 min in 1 mg/ml hyaluronidase. Cells were then spun down; the cell-free supernatant was aspirated from the centrifuge tube, and dissociated cells were resuspended in NaCl Ringer's. Cells were transferred to an experimental chamber (described below) positioned on the stage of an inverted microscope (Diaphot; Nikon, Garden City, NY). Dissociated cell suspensions contained spherical cells that excluded the dye trypan blue, and broken cells that did not. Dye-excluding cells could be patched; these cells comprised 5–80% of the cells in any given experimental preparation.

**Solutions.** Tissues or dissociated cells were initially bathed in NaCl Ringer's solution containing (in millimolar): 97.5 NaCl, 2.5 KCl, 1 MgCl<sub>2</sub>, 1 CaCl<sub>2</sub>, 10 N-2-hydroxyethylpiperazine-*N'*-2-ethanesulfonic acid (HEPES)/NaOH, pH 7.4. The patch pipette was usually filled with KCl solution containing (in millimolar): 100 KCl, 1 MgCl<sub>2</sub>, 10 HEPES/KOH, pH 7.4. KCl and K gluconate solutions used in determining the ion selectivity of channels in excised patches contained (in millimolar): 100 KCl or K gluconate, 1 CaCl<sub>2</sub>, 10 HEPES/KOH, pH 7.4. In inside-out patch experiments measuring *I*-*V* relations for channels exposed to physiologic K<sup>+</sup> and Na<sup>+</sup> concentrations, the bath contained (in millimolar): 90 KCl, 10 NaCl, 1 CaCl<sub>2</sub>, 10 HEPES/KOH, pH 7.4; the pipette contained NaCl Ringer's. In studies examining the Ca<sup>2+</sup> sensitivity of channels in excised patches, the bathing solutions contained (in millimolar): 100 KCl, 10 HEPES/KOH, pH 7.4, 3 ethyleneglycol-bis( $\beta$ -aminoethylether)-*N,N'*-tetraacetic acid (EGTA), and sufficient CaCl<sub>2</sub> to achieve the desired free Ca<sup>2+</sup> concentration (range, 0.1–1  $\mu$ M), calculated using equilibrium constants from Martell and Smith (1974) and a H<sup>+</sup> activity coefficient of 0.78. In pilot studies, the Ca<sup>2+</sup> activity of these solutions was verified using a Ca<sup>2+</sup>-sensitive macroelectrode (World Precision Instruments, New Haven, CT), calibrated in the pCa range of 3–7 using commercial standards (World Precision Instruments) or the calibration solutions described by Tsien and Rink (1980).

**Patch-clamp techniques.** Patch pipettes were made from Corning 7052 capillary glass (1.5 mm o.d., 1.0 mm i.d.; Friedrich and Dimmock, Millville, NJ) or from hematocrit glass (blue-tip; Fisher Scientific), using a two-stage vertical puller (model PP-83; Narishige, Japan). Pipettes made from Corning 7052 glass were Sylgard-coated and fire-polished to a resistance of 7–10 M $\Omega$ . Pipettes made from hematocrit glass were Sylgard-coated and used without fire-polishing; useful pipettes had 7–10 M $\Omega$  resistances. Resistances were measured with NaCl Ringer's in the bath and 100 mM KCl solution in the pipette.

In studies on the intact epithelium, patch pipettes were lowered gently onto the apical surface of the tissue. Application of suction to the pipette interior generally resulted in the formation of an ~100-M $\Omega$  seal, and in <5% of the trials, formation of a tight (>1 G $\Omega$ ) electrical seal. Here, we report results obtained with gigaseals only. Membrane patches were excised by rapidly withdrawing the pipette.

Seals in the range 10–20 G $\Omega$  were routinely achieved on dissociated cells. In these experiments, patches were excised by gently tapping the microscope stage. Vesicle formation at the pipette tip usually accompanied patch excision; vesicles were disrupted by passing the pipette tip through the bath-air interface, or by applying slight positive pressure to the pipette interior. Once excised, membrane patches were transferred from the main compartment of the chamber (2–3 ml volume) to a 0.5-ml subcompartment, where they were superfused continuously at a rate of 3–5 ml/min.

Patch currents were amplified with a List EPC-7 patch clamp and recorded at wide bandwidth (DC to 20 kHz bandwidth) on video tape, using an Indec IR-2 Digital Instrumentation Recorder (Indec Systems Inc., Sunnyvale, CA). Stored records were low-pass filtered at 1–2 kHz with an eight-pole Bessel filter (model 902LPF; Frequency Devices, Inc., Haverhill, MA), and played onto a strip chart recorder (model 220; Gould Instruments, Cleveland, OH) for

analysis by hand, or digitized at 5–10 kHz for analysis by computer. In cell-attached patch experiments, pipette potentials ( $V_p$ ) are expressed with respect to the bath. In experiments on inside-out patches, holding potentials are expressed so as to correspond to the cell membrane voltage ( $V_m$ ), i.e., with respect to the pipette solution. In most experiments,  $V_m$  was limited to the range  $\pm 60$  mV, since seals tended to degrade at more extreme membrane voltages. Holding potentials were corrected for liquid junction potentials which arose at the bridge-bath interface during solution changes. Positive current is deemed to flow from the cellular to the extracellular side of the patches, and is depicted as upward deflections. In all experiments, the bath was grounded with an Ag-AgCl wire immersed in a Ringer's agar bridge.

Single-channel open probabilities ( $P_o$ ) were estimated using segments of digitized data 10–60 s in duration, according to  $P_o = (1/N_c) \sum_i P_i$ , where  $i$  is a summation index from 0 to  $N_c$ ,  $P_i$  is the fraction of time during which  $i$  channels are open, and  $N_c$  is the total number of channels in the patch. This expression assumes that channels in multiple-channel patches gate identically and independently, that is, in a binomial fashion. In compiling our results, we did not use patches in which channels deviated from binomial behavior (<20% of the total). Channel openings were detected by an amplitude-threshold technique. In some cases, records were digitally filtered at 100 Hz before analysis.

A single set of voltage-step experiments was carried out to assess the time course of maxi  $K^+$  channel activation. These experiments were carried out using inside-out patches exposed to symmetrical 100 mM KCl solutions, with internal  $Ca^{2+}$  buffered to 500 nM. For each voltage step, 30–70 current traces were averaged to construct an ensemble current. Capacitive currents were digitally subtracted from the ensemble current, using steps during which no channels were activated.

#### *Microelectrode Experiments*

Details on electrical measurements of the transepithelial voltage ( $V_{ms}$ ), and the cell membrane voltages (apical,  $V_{mc}$ ; basolateral,  $V_{cb}$ ) have appeared previously (Reuss and Finn, 1975*a, b*). Gallbladders were mounted in a modified Ussing chamber and superfused symmetrically with Ringer's containing (in millimolar): 97.5 NaCl, 2.5 KCl, 1  $MgCl_2$ , 1  $CaCl_2$ , 10 HEPES/NaOH, pH 7.5. Cells were impaled with microelectrodes pulled from inner-fiber borosilicate glass (1 mm o.d., 0.5 mm i.d.; Glass Company of America, Millville, NJ) and filled with 1 M KCl; tip resistances ranged from 40 to 100 M $\Omega$ .

The goal of these microelectrode experiments was to estimate the apical and basolateral membrane conductances ( $G_a$  and  $G_b$ ) under control conditions and during perturbations of  $V_{mc}$  induced by transepithelial current clamps. To estimate  $G_a$  and  $G_b$  under control conditions, we carried out a series of two-electrode intraepithelial cable analysis experiments, in combination with measurements of transepithelial electrical resistance ( $R_t$ ) and the apparent ratio of cell membrane resistances  $R_a/R_b$  (Frömter, 1972; Reuss and Finn, 1975*a*). Cable experiments were performed as described previously (Reuss and Finn, 1975*a*; Stoddard and Reuss, 1988*a*). Hyperpolarizing current pulses 1 s in duration and 25 nA in amplitude were injected intracellularly through one electrode, and basolateral membrane voltage deflections in nearby cells were recorded as a function of distance [ $\Delta V_{cs}(x)$ ] with a second intracellular microelectrode. Estimates for  $R_t$  and  $R_a/R_b$  were obtained using mucosa-to-serosa current pulses 1 s in duration and 50  $\mu A/cm^2$  in amplitude; these current pulses hyperpolarized  $V_{mc}$  by < 5 mV, minimizing voltage-induced changes in  $G_a$ . Estimation of equivalent circuit parameters from two-microelectrode cable data was carried out as described previously (Frömter, 1972; Reuss and Finn, 1975*a*). Briefly, the tissue was treated as a two-dimensional cable. Experimentally determined  $\Delta V_{cs}(x)$  was used to estimate  $R_t$ , which equals  $R_a$  and  $R_b$  in parallel.  $R_t$ , coupled with measurements of  $R_t$ ,  $R_a/R_b$ , and the cell membrane voltages, permit-

ted calculation of the resistances,  $R_a$ ,  $R_b$ , and  $R_s$ , and the equivalent electromotive forces (EMFs)  $E_a$  and  $E_b$ .

In a separate set of studies,  $G_a$  was estimated as a function of  $V_{mc}$  using 1-s transepithelial current clamps in the range  $\pm 300 \mu\text{A}/\text{cm}^2$  (Stoddard and Reuss, 1988b). The ratio of cell membrane voltage deflections ( $\Delta V_{mc}/\Delta V_{cs}$ ) was measured 800 ms after the onset of each clamp, when the voltage deflections  $\Delta V_{mc}$  and  $\Delta V_{cs}$  had reached stable values. By this time, channels had reached steady-state gating (see Results), permitting comparisons between microelectrode measurements and results obtained from single-channel studies. Barring changes in  $R_a$  and  $R_b$  induced by the current clamp, the ratio of the voltage deflections  $\Delta V_{mc}/\Delta V_{cs}$  provides a reasonable estimate for  $R_a/R_b$  (Stoddard and Reuss, 1988a). Recent work has revealed that depolarizing  $V_{mc}$  decreases  $R_a$  (García-Díaz et al., 1983; Stoddard and Reuss, 1988b). In the Appendix, we refine the procedure for estimating  $R_a/R_b$  from  $\Delta V_{mc}/\Delta V_{cs}$  measurements, accounting for voltage-induced changes in  $G_a$  and  $E_a$ .

### *Statistics and Curve Fitting*

Experimental values are expressed as mean  $\pm$  standard error of measurement (SEM). Fitting programs used a grid-search algorithm for minimizing the sum of squared deviations (Bevington, 1969).

### MODELS

The basic expression relating the macroscopic apical membrane conductance  $G_a(V_{mc})$  to ion channels in the apical membrane is:

$$G_a(V_{mc}) = \sum_{i=0}^M N_a^i P_o^i(V_{mc}) g^i(V_{mc}) \quad (1)$$

where  $M$  is the number of distinct channel types in the apical membrane, and  $N_a^i$ ,  $P_o^i(V_{mc})$ , and  $g^i(V_{mc})$  are the surface density, the steady-state open probability, and the unitary conductance of channel type  $i$ , respectively. We take  $G_a$  to arise from only two channel types (see Results): background, voltage-independent, ohmic channels which can be lumped ( $G_a^0$ ), and voltage-activated maxi K<sup>+</sup> channels. Then, Eq. 1 becomes:

$$G_a(V_{mc}) = G_a^0 + N_a P_o(V_{mc}) g(V_{mc}) \quad (2)$$

where  $g(V_{mc})$ ,  $P_o(V_{mc})$ , and  $N_a$  now refer specifically to maxi K<sup>+</sup> channels. For data analysis, it is convenient to scale Eq. 2 by the basolateral membrane conductance ( $G_b$ ), which is taken to be voltage independent, so that:

$$\frac{G_a(V_{mc})}{G_b} = \frac{G_a^0}{G_b} + \frac{N_a}{G_b} P_o(V_{mc}) g(V_{mc}) \quad (3)$$

$G_a(V_{mc})$  and  $g(V_{mc})$  are measured experimentally, while  $G_a^0$ ,  $N_a$ , and  $P_o(V_{mc})$  are evaluated using Eqs. 2 and 3, as described below. The voltage dependence of  $G_a$  is ascribed solely to maxi K<sup>+</sup> channels on the basis of single-channel studies which indicated that these are the predominant voltage-activated K<sup>+</sup> channels in the apical membrane (see Results).

### Measuring $g(V_{mc})$

The current-voltage ( $I$ - $V$ ) relation for maxi  $K^+$  channels exposed to physiological  $K^+$  and  $Na^+$  concentrations was described using a simplified barrier rate model consistent with emerging views of multi-ion conduction in maxi  $K^+$  channels (see Neyton and Miller, 1988). The channel is modeled as a pore containing five barriers of equal width and four wells of equal depth. The channel has a high affinity for  $K^+$ , and resides solely in high-occupancy states. Transitions among occupancy states obey microscopic reversibility. Energy barriers to  $K^+$  movements within the pore are neglected. This model gives rise to an explicit expression for single-channel current containing three adjustable barrier rate constants. Single-channel slope conductance  $g(V_m)$  is given by the derivative of this expression with respect to voltage.

### $Ca^{2+}$ and Voltage Dependencies of Channel Gating

Expressions relating single-channel open probability to  $V_m$  and  $[Ca^{2+}]_i$  are developed empirically. For  $[Ca^{2+}]_i$  equal to 0.1, 0.3, and 1  $\mu M$ , the relationship between  $P_o$  and  $V_m$  is approximated by a Boltzmann relation:

$$P_o = \frac{P_o^{\max}}{1 + e^{[-n_z F(V - V^0)/RT]}} \quad (4)$$

where  $P_o^{\max}$  is maximum  $P_o$ ,  $n_z$  describes the voltage sensitivity of the gating reaction, and  $V^0$  is the membrane voltage at which  $P_o$  is half-maximal. The experimental results suggest that changing  $[Ca^{2+}]_i$  in the range 0.1–1  $\mu M$  shifts  $P_o(V_m)$  along the voltage axis, without changing the voltage dependence of the gating reaction (see also Latorre et al., 1982; Methfessel and Boheim, 1982; Singer and Walsh, 1987; Reinhart et al., 1989). This observation allows  $P_o(V_m)$  data to be fitted simultaneously, assigning one value of  $V^0$  to data obtained at a given  $[Ca^{2+}]_i$ , and one value of  $n_z$  to the combined data. Shifts of  $V^0$  are roughly constant for half-log unit changes in  $[Ca^{2+}]_i$ , so that  $V^0$  can be approximated by:

$$V^0 = a \log_{10}[Ca^{2+}]_i + b \quad (5)$$

where  $a$  and  $b$  are constants. Eq. 5 is used to estimate  $[Ca^{2+}]_i$  in the intact gallbladder, where  $[Ca^{2+}]_i$  is unknown, but  $V^0$  can be estimated.

### Measuring $G_a(V_{mc})$

Estimates of  $G_a$  and  $G_b$  at the resting apical membrane voltage are obtained from cable analysis experiments.  $G_a(V_{mc})$  is determined over a range of  $V_{mc}$  values using 1-s transepithelial current clamps, as described in Materials and Methods. Calculations of  $G_a$  account for changes in  $G_a$  and  $E_a$  elicited by transepithelial current clamps (see Appendix).

### Reconstructing $P_o(V_{mc})$ for Apical Membrane Channels

A three-step fitting procedure is used to estimate  $P_o(V_{mc})$  for apical membrane maxi  $K^+$  channels, as well as  $G_a^0$  and  $N_a$ . In step 1,  $G_a(V_{mc})/G_b$  data are used without correction for voltage-induced changes in  $G_a$  and  $E_a$ . These data are fitted to Eq. 3 with  $P_o(V_{mc})$  described by a Boltzmann relation. Estimates are obtained for  $G_a^0/G_b$ ,

$N_a/G_b$ ,  $n_z$ , and  $V^0$ . In step 2, best-fit parameters obtained in step 1 are substituted into Eq. 3 to generate a  $G_a(V_{mc})/G_b$  curve that is representative of the pooled experimental points. Points on this curve are corrected for voltage-induced changes in  $G_a$  and  $E_a$ , as outlined in the Appendix. In step 3, the corrected points are fitted as in step 1, yielding revised estimates for  $G_a^0$ ,  $N_a$ ,  $n_z$ , and  $V^0$ . The revised estimates for  $n_z$  and  $V^0$  define  $P_o(V_{mc})$  for apical membrane channels according to Eq. 4.

## RESULTS

### *Patch-Clamp Experiments*

Maxi K<sup>+</sup> channels were identified in the apical membrane of the intact epithelium, and in dissociated epithelial cells. The low yield of patch-clamp studies on intact tissues precluded their use in detailed characterizations of apical maxi K<sup>+</sup> channels. Thus, the majority of our studies were carried out using dissociated cells, which were easily patched, and which exhibited maxi K<sup>+</sup> channels similar to those in the intact apical membrane, as demonstrated below.

*Maxi K<sup>+</sup> channels in the apical membrane of the intact epithelium.* Records from a cell-attached patch in the apical membrane of the intact epithelium are illustrated in Fig. 1. In this patch, obtained with the tissue bathed in NaCl Ringer's and with 100 mM KCl in the pipette solution, a single major channel type is evident, which activates when the membrane is depolarized. Single-channel current amplitude approaches zero as the membrane is depolarized, suggesting that the channels are primarily K<sup>+</sup> selective, inasmuch as the expected reversal potentials for K<sup>+</sup>, Na<sup>+</sup>, and Cl<sup>-</sup>, estimated from previously determined membrane voltages and intracellular ionic activities (see Reuss, 1989), occur at  $V_p = -60$  mV,  $V_p \gg 0$  mV, and  $V_p = -25$  mV, respectively.

Channel activity in a second patch excised from the apical membrane of the intact epithelium are shown in Fig. 2. Again, channel activity in the cell-attached configuration was low (Fig. 2 A). Excising the patch into a bathing solution containing 1 mM Ca<sup>2+</sup> activated three channels of similar conductance. *I-V* relations for these channels are shown in Fig. 2 C. In symmetrical KCl solutions, the single-channel *I-V* relationship was linear, with a slope conductance of 162 pS, and a reversal potential of 3 mV. Reducing K<sup>+</sup> in the bath to 5 mM shifted the reversal potential to  $V_m = 62$  mV, as expected for a K<sup>+</sup>-selective channel. Assuming that the channels are permeable to Na<sup>+</sup> and K<sup>+</sup> only, application of the Goldman-Hodgkin-Katz equation yields an estimated K<sup>+</sup>:Na<sup>+</sup> permeability ratio of 23:1.

The effects of applying 1 mM Ba<sup>2+</sup> to the internal face of a patch exposed to symmetrical KCl solutions and 1 mM internal Ca<sup>2+</sup> are illustrated in Fig. 3. In the absence of Ba<sup>2+</sup>, single-channel open probability ( $P_o$ ) was high and decreased slightly with depolarization; the latter effect may have been caused by a voltage-dependent low-affinity block by internal Ca<sup>2+</sup> (Vergara and Latorre, 1983). Internal Ba<sup>2+</sup> reduced single-channel  $P_o$  in a voltage-dependent manner, with more pronounced inhibition at positive membrane voltages.

These and other experiments on intact gallbladders ( $n = 5$ ) indicate that the predominant channel in the apical membrane is a large conductance K<sup>+</sup> channel, which is activated by membrane depolarization. Because of their large conductance, Ca<sup>2+</sup>

sensitivity, and voltage-dependent  $\text{Ba}^{2+}$  sensitivity, these channels classify among the maxi  $\text{K}^+$  channels first described in nerve and muscle preparations, and later reported to be present in numerous epithelial systems.

*Maxi  $\text{K}^+$  channels in dissociated cells.* Currents through a single maxi  $\text{K}^+$  channel

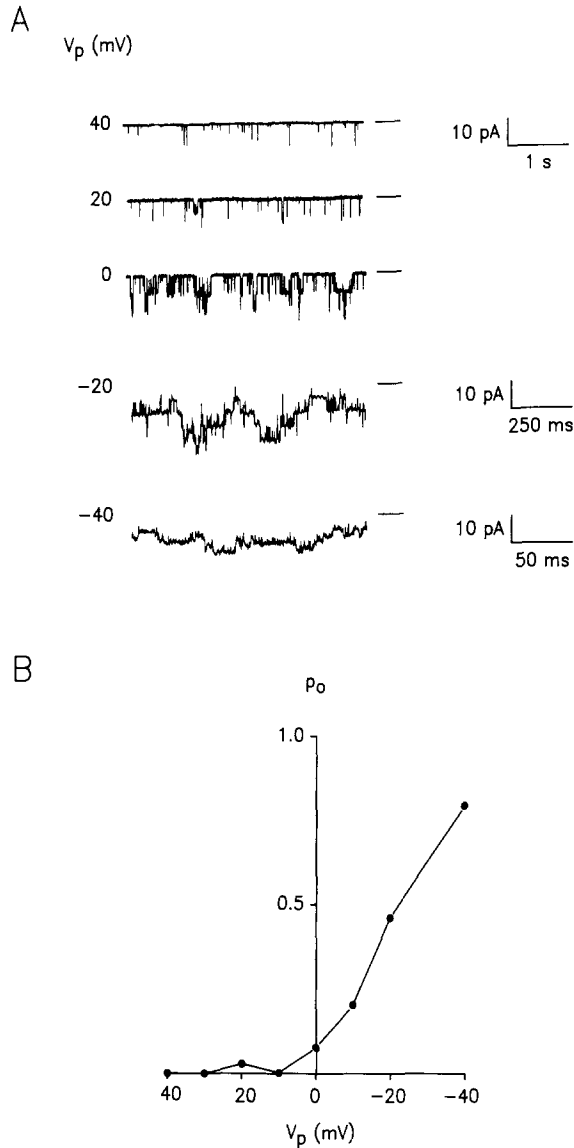


FIGURE 1. Single maxi  $\text{K}^+$  channels in the apical membrane of the intact epithelium. (A) Recordings from a cell-attached patch in the apical membrane of the intact epithelium. The tissue was bathed in NaCl Ringer's; the patch relative to the bath. Downward deflections correspond to channel openings; baselines are indicated to the right of the current records. (B) Open probability  $P_o$  vs.  $V_p$ .

excised from a dissociated cell are shown in Fig. 4. In symmetrical KCl solutions, the  $I$ - $V$  relation was linear, with a slope conductance of 199 pS, and a reversal potential of 0 mV. With 2.5 mM  $\text{K}^+$  in the bath, the  $I$ - $V$  relation rectified, and did not reverse in the membrane voltage range spanning  $-40$  to  $40$  mV, placing a lower limit of 6:1



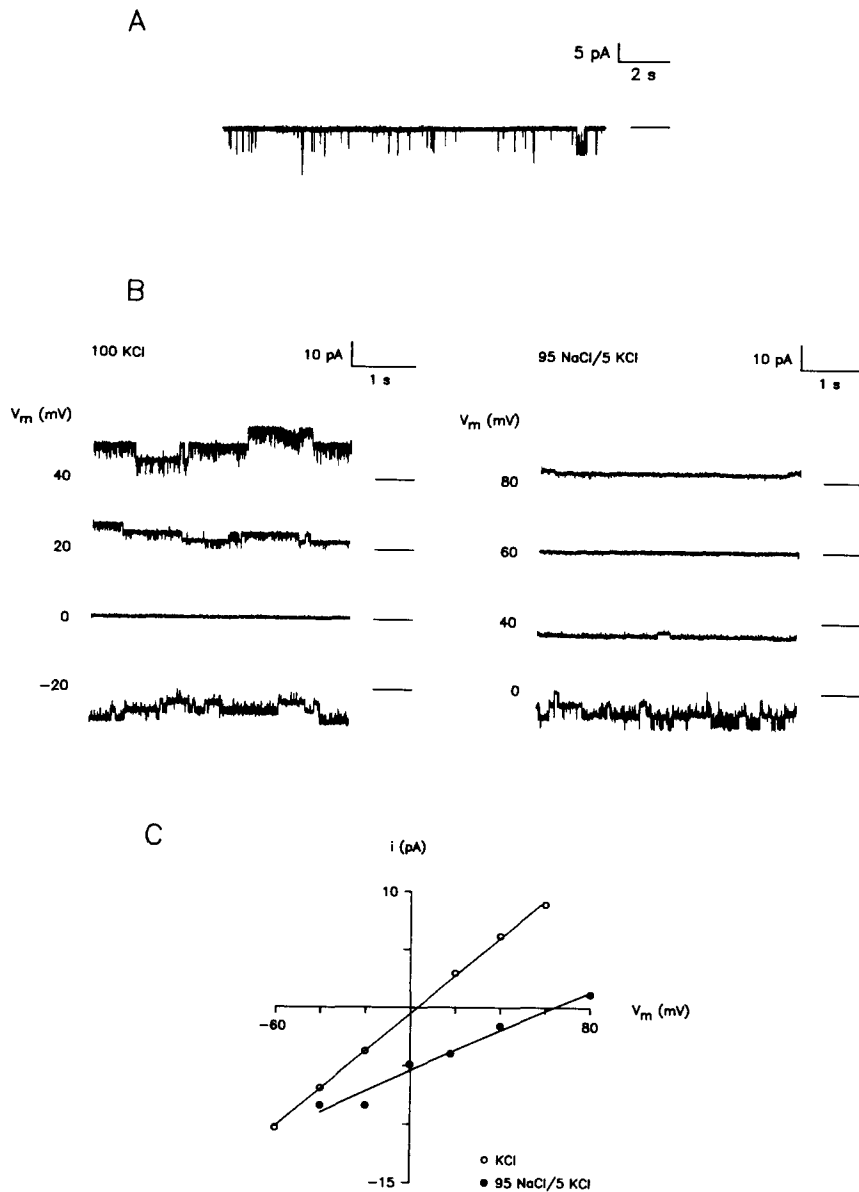


FIGURE 2. Ion selectivity and  $\text{Ca}^{2+}$ -dependent activation of apical membrane channels. (A) Channel activity in the cell-attached mode. The tissue was bathed in NaCl Ringer's; the patch pipette contained 100 mM KCl solution.  $V_p$  was held at 0 mV. (B) Channel activity in the inside-out configuration, with 100 mM KCl or 95 mM NaCl/5 mM KCl in the bath. Bath  $[\text{Ca}^{2+}]$  was 1 mM. (C) Single-channel  $I$ - $V$  relations in symmetrical KCl, or under  $\text{Na}^+:\text{K}^+$  biionic conditions. Channels were activated by excision into a bathing solution containing 1 mM  $\text{Ca}^{2+}$ . Reducing internal  $\text{K}^+$  from 100 to 5 mM shifted the channel reversal potential from 3 to 62 mV, as expected for a  $\text{K}^+$ -selective channel.

on the  $K^+ : Na^+$  permeability ratio. Replacing KCl in the bath with K gluconate had no effect on the  $I$ - $V$  relation, confirming the anion impermeability of this channel. The single-channel conductance in symmetrical 100 mM KCl solution was  $202 \pm 12$  pS ( $n = 7$ ).

The effects of 1 mM internal  $Ba^{2+}$  on a maximally activated  $K^+$  channel from a dissociated cell are summarized in Fig. 5. In the absence of  $Ba^{2+}$ , single-channel  $P_o$  was near 1 at all membrane voltages; there was no evidence of a decrease in  $P_o$  at positive membrane voltages. Internal  $Ba^{2+}$  reduced channel open probability in a voltage-dependent manner, with half-maximal inhibition at  $V_m = -19$  mV, com-

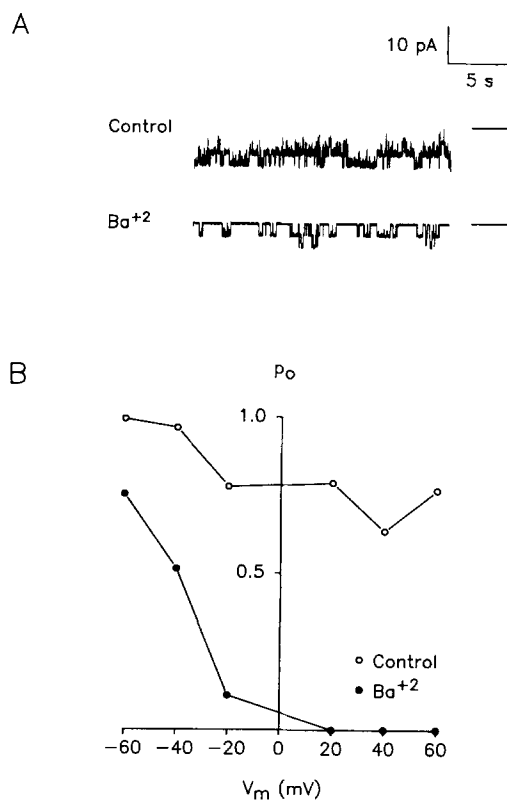


FIGURE 3.  $Ba^{2+}$  blockage of maxi  $K^+$  channels from the apical membrane of the intact epithelium. (A) Channel activity in an inside-out patch is shown before and after addition of 1 mM  $Ba^{2+}$  to the bath. Records were obtained in symmetrical 100 mM KCl solutions, with  $[Ca^{2+}]_i = 1$  mM, and  $V_m = -20$  mV. (B) Single-channel  $P_o$  measured as a function of membrane voltage. High  $P_o$  values determined in the absence of  $Ba^{2+}$  are due to the high  $[Ca^{2+}]_i$ . The effects of  $Ba^{2+}$  are voltage dependent, becoming clearest at  $V_m > 0$ , where no channel openings are observed.

pared with  $V_m = -40$  mV for maxi  $K^+$  channels excised from the apical membrane of the intact tissue.

The ion selectivity, unitary conductance, and  $Ba^{2+}$  sensitivity of maxi  $K^+$  channels in the apical membrane of the intact epithelium and in dissociated cells suggest that these channels are similar, and validate the use of dissociated cells in studies in apical channels. Additional evidence for the apical membrane origin of maxi  $K^+$  channels in dissociated cells rests on similarities between their  $Ca^{2+}$  and voltage sensitivities, examined below, and those of macroscopic  $G_a$ . Patterns of sensitivity to  $K^+$  channel blockers provide another important basis for correlating maxi  $K^+$  channels

and  $G_a(V_{mc})$ . Indeed, maxi K<sup>+</sup> channels and  $G_a(V_{mc})$  exhibit similar patterns of sensitivity to Ba<sup>2+</sup>, TEA<sup>+</sup>, and quinine, and we will address this issue in a later report.

*Single-channel I-V relations at physiologic K<sup>+</sup> and Na<sup>+</sup> concentrations.* As a first step in relating single-channel and microelectrode data, *I-V* relations were collected for maxi K<sup>+</sup> channels exposed to solutions containing monovalent cations at physiologic concentrations (Fig. 6 A). The average *I-V* relation ( $n = 3$ ) is shown in Fig. 6 B.

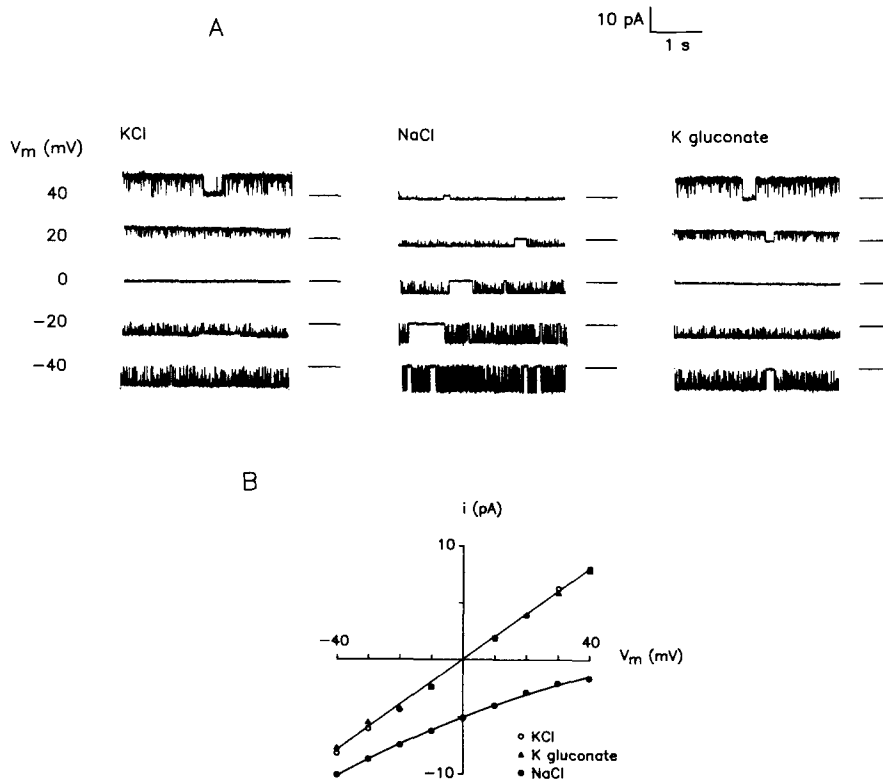


FIGURE 4. Ion selectivity of maxi K<sup>+</sup> channels from dissociated cells. *I-V* relations were obtained for a maxi K<sup>+</sup> channel in an inside-out patch. The patch pipette contained 100 mM KCl solution. (A) Channel activity observed with 100 mM KCl, 97.5 mM NaCl/2.5 mM KCl, or 100 mM K gluconate in the bath. Baselines are indicated to the right of the current records. (B) *I-V* relations determined under these three sets of ionic conditions. Reducing the internal [K<sup>+</sup>] from 100 to 2.5 mM shifted the reversal potential from 0 to >60 mV, while replacing KCl with K gluconate had no effect on the *I-V* relation.

As expected, the curve rectifies; current reversal is not observed in the experimental  $V_m$  range. In some systems, currents through maxi K<sup>+</sup> channels bathed in physiological gradients diminish as the membrane voltage is depolarized, reflecting internal Na<sup>+</sup> block (Marty, 1983). We did not observe diminution of the currents for  $V_m < 30$  mV.

Overlying the *I-V* relation in Fig. 6 B is the fitted curve given by a simple barrier

model of the channel pore (Fig. 6 C). Single-channel slope conductance  $g(V_m)$ , calculated as the derivative of the fitted  $I$ - $V$  relation, is shown in Fig. 6 D.

*Ca<sup>2+</sup> and voltage dependencies of channel gating.* Studies assessing the Ca<sup>2+</sup> and voltage-dependencies of maxi K<sup>+</sup> channel steady-state  $P_o$  were carried out using inside-out patches from dissociated cells (Fig. 7). Channels were activated by membrane depolarization and by elevation of internal Ca<sup>2+</sup> concentration. Channels exhibited wide quantitative variability in their Ca<sup>2+</sup> and voltage sensitivities, as reflected by the large SEMs in Fig. 7. Variability in the Ca<sup>2+</sup> and voltage sensitivities of maxi K<sup>+</sup> channels within experimental preparations has been noted previously

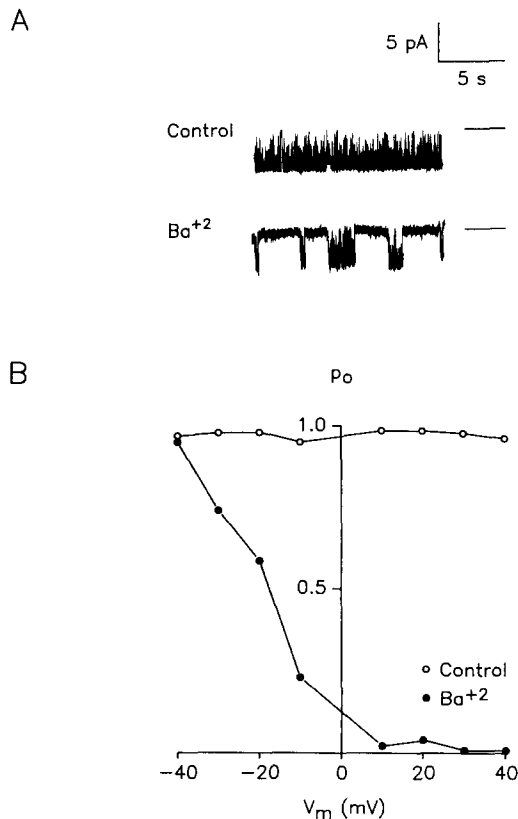


FIGURE 5. Ba<sup>2+</sup> sensitivity of maxi K<sup>+</sup> channels from dissociated cells. An inside-out patch was bathed symmetrically in 100 mM KCl, with [Ca<sup>2+</sup>]<sub>i</sub> = 1 mM, sufficient for maximal activation of the channels. Ba<sup>2+</sup> was added to the bath to a final concentration of 1 mM. (A) Channel activity at -20 mV, before and after addition of 1 mM Ba<sup>2+</sup>. (B) Single-channel  $P_o$  as a function of  $V_m$ , before and after Ba<sup>2+</sup> addition. Ba<sup>2+</sup> block was voltage dependent, increasing  $e$ -fold/15 mV in the range of -40 to 10 mV. Half-maximal block occurred at -19 mV, compared with -40 mV for maxi K<sup>+</sup> channels from the intact apical membrane.

(Moczydlowski and Latorre, 1983; Singer and Walsh, 1987). At  $V_m = 0$  mV, single-channel  $P_o$  was half-maximal at roughly 400 nM Ca<sup>2+</sup>, which is low in comparison to the half-maximal activation concentrations reported for excitable cells (Latorre, 1986; Blatz and Magleby, 1987) and some epithelia (Christensen and Zeuthen, 1987; Merot et al., 1989), typically 1–10  $\mu$ M, but similar to those for channels in other epithelia (Kolb et al., 1986; Maruyama et al., 1986; Sheppard et al., 1988).

The best-fit parameters obtained when  $P_o$  vs.  $V_m$  curves in Fig. 7 were fitted individually to Boltzmann expressions are summarized in Table I (fit I). As expected,

elevating internal  $\text{Ca}^{2+}$  shifted  $V^0$  in the negative direction. Further, as internal  $\text{Ca}^{2+}$  was increased,  $n_z$  decreased, suggesting that the channel-gating mechanism becomes less voltage dependent at higher  $[\text{Ca}^{2+}]_i$ . We tested the alternative possibility that the voltage dependence of the gating reaction is in fact independent of  $[\text{Ca}^{2+}]_i$ , as

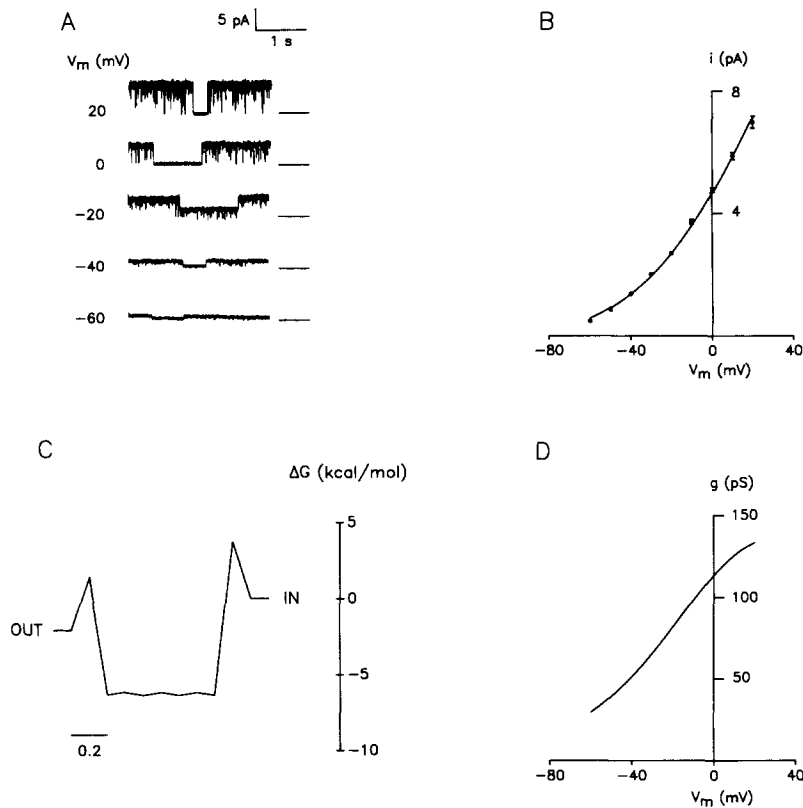


FIGURE 6. Conduction across maxi K<sup>+</sup> channels exposed to physiologic Na<sup>+</sup> and K<sup>+</sup> gradients. Inside-out patches were bathed in solutions containing physiological concentrations of monovalent cations (see Materials and Methods for solution compositions). (A) Channel activity. Baselines appear to the right of the current records. (B) Average *I-V* relation ( $n = 3$ ). The solid line depicts the best fit to the simple barrier model. (C) Barrier model for K<sup>+</sup> permeation, described in Models. The model is shown for the case of 0 mV applied voltage; the difference in the internal and external solution free energy levels reflects the K<sup>+</sup> concentration gradient across the membrane. (D) Single-channel slope conductance  $g(V_m)$ , given by the derivative of the fitted *I-V* relation with respect to voltage.

first proposed by Latorre et al. (1982). The  $P_o$  data shown in Fig. 7 were fitted simultaneously to the Boltzmann equation, assigning one value of  $n_z$  to the combined sets of points, and one value of  $V^0$  for each set of points (fit II). The curves resulting from this fit overlaid the data in Fig. 7.  $V^0$  was linearly dependent on

$\log_{10}[\text{Ca}^{2+}]_i$  (see Eq. 5), according to

$$V^0 = -94 \log_{10}[\text{Ca}^{2+}]_i - 36 \quad (6)$$

with  $[\text{Ca}^{2+}]_i$  given in micromolar.

If Eq. 5 holds, then the Boltzmann relation can be rewritten in the form:

$$P_o = \frac{P_o^{\max}}{1 + K[\text{Ca}^{2+}]_i^{-N} e^{(-n_e FV/RT)}} \quad (7)$$

where  $K = \exp(bn_e F/RT)$ , and  $N = an_e F/2.303 RT$ . Precise reaction schemes that

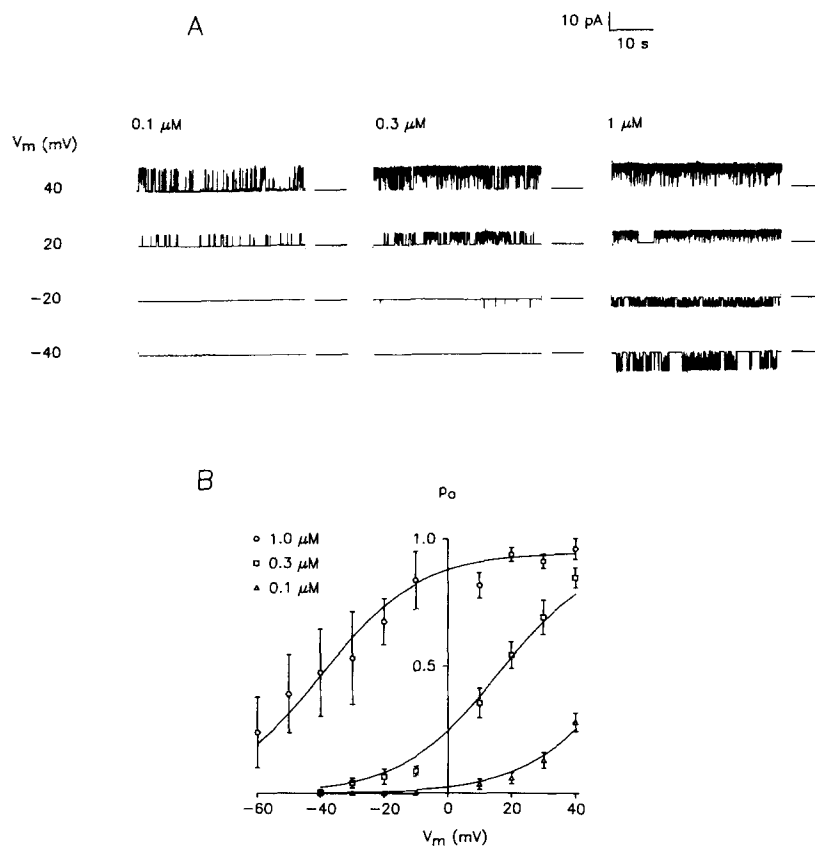


FIGURE 7.  $\text{Ca}^{2+}$  and voltage dependence of maxi  $\text{K}^+$  channel  $P_o$ . Inside-out patches from dissociated cells were exposed symmetrically to 100 mM KCl, with internal  $\text{Ca}^{2+}$  buffered to 0.1, 0.3, or 1  $\mu\text{M}$ . (A) Maxi  $\text{K}^+$  channel in a single inside-out patch is shown over ranges of  $[\text{Ca}^{2+}]_i$  and membrane voltage. (B)  $\text{Ca}^{2+}$  and voltage dependence of  $P_o$ , summarized from five experiments; each point represents the mean value determined from at least four of the experiments. Curves overlying the data represent the results of fits to Boltzmann relations (see Table I and text for details), with  $n = 1.6$  for the three sets of data, and  $V^0 = 56, 16,$  and  $-39$  for 0.1, 0.3, and 1  $\mu\text{M}$   $\text{Ca}^{2+}$ , respectively.  $P_o$ , single-channel open probability;  $n$ , number of gating charges;  $V^0$ , membrane voltage at which  $P_o$  is half-maximal.

can give rise to an expression of this form have been described previously (Methfessel and Boheim, 1982). In an attempt to incorporate the effects of internal  $\text{Ca}^{2+}$  and  $V_m$  into a single expression for  $P_o$ , data in Fig. 7 were fitted simultaneously to Eq. 7, with the results shown in Table I (fit III). This model predicted a shallower voltage dependence for  $P_o$  than did fit II; curves resulting from this fit (not shown) failed to describe the steep regions of  $P_o(V_m)$  for  $[\text{Ca}^{2+}]_i$  equal to 0.1 and 0.3  $\mu\text{M}$ . It is possible that Eq. 7 can in fact represent the data, and that use of  $V^0$  in fit II "loosens" the equation, allowing for small deviations in the specified values of  $[\text{Ca}^{2+}]_i$ . Regardless, for the purpose of relating single-channel data to microelectrode data, we settled on the results of fit II, which provide a reasonable description of the data with a minimum number of adjustable parameters.

*Time scale of channel activation.* The single-channel functions  $P_o(V_{mc})$  and  $g(V_{mc})$  represent the steady-state determinations. To relate these functions to the macro-

TABLE I  
Single-Channel Open Probability Described Using Boltzmann Relations

Fit	$[\text{Ca}^{2+}]_i$	$P_o^{\text{max}}$	$n$	$V^0$
	$\mu\text{M}$			$mV$
I	0.1	0.96	2.2	50
	0.3	0.96	2.0	17
	1	0.96	1.4	-37
II	0.1	0.95	1.6	56
	0.3	0.95	1.6	16
	1	0.95	1.6	-39
III	$P_o^{\text{max}}$	$n$	$K$	$N$
	0.96	1.5	0.11	2.6

Single-channel  $P_o$  was measured as a function of  $V_m$ , at 0.1, 0.3, and 1  $\mu\text{M}$   $\text{Ca}^{2+}$  (see text and Fig. 10). Values represent best-fit Boltzmann parameters. Fit I: sets of  $P_o(V_m)$  data were fitted individually to the Boltzmann equation. Fit II: sets of  $P_o(V_m)$  data were fitted simultaneously to Boltzmann relations, assigning one value of  $V^0$  to each set of data, and one value of  $n$  to the combined sets of data. Fit III: data were fitted simultaneously to Eq. 8 (see text).  $P_o^{\text{max}}$ , maximum  $P_o$ ;  $n$ , number of gating charges;  $V^0$ , membrane voltage at which  $P_o = P_o^{\text{max}}/2$ ;  $K$ , effective voltage- and  $\text{Ca}^{2+}$ -dependent equilibrium constant;  $N$ ,  $\text{Ca}^{2+}$  Hill coefficient.

scopic  $G_a$ , it is necessary to establish that microelectrode experiments also assess steady-state channel activity. Changes in apical membrane conductance elicited by transepithelial current clamps reach stable values within 200 ms (Stoddard and Reuss, 1988b), suggesting that channel activation is complete within this time frame. To further verify that gallbladder maxi  $\text{K}^+$  channels reach steady-state gating within 800 ms, voltage-step experiments were carried out using inside-out patches exposed to symmetrical 100 mM KCl and 500 nM internal  $\text{Ca}^{2+}$ . In the experiment summarized in Fig. 8, stepping  $V_m$  from -40 to 20 or 40 mV activated up to five channels in the patch. The ensemble currents assembled from the individual steps reveal that for steps to 20 mV, the shift from  $P_o = 0$  to the new steady-state  $P_o$  of 0.30 is essentially complete at 800 ms. The same is true for steps to 40 mV, where  $P_o$  increases to 0.65. The rapid establishment of gating steady state validates the use of 800-ms time

points in comparisons between microelectrode measurements and steady-state single-channel data. Steps from  $-40$  mV to  $V_m$  in the range of 10 to 40 mV did not reveal secondary channel inactivation processes, which have been observed with maxi  $K^+$  channels from cultured rat muscle (Pallotta, 1985).

#### Microelectrode Experiments

Previous studies in this and other laboratories have revealed that the cable properties of *Necturus* gallbladder epithelium depend on the composition of bathing Ring-

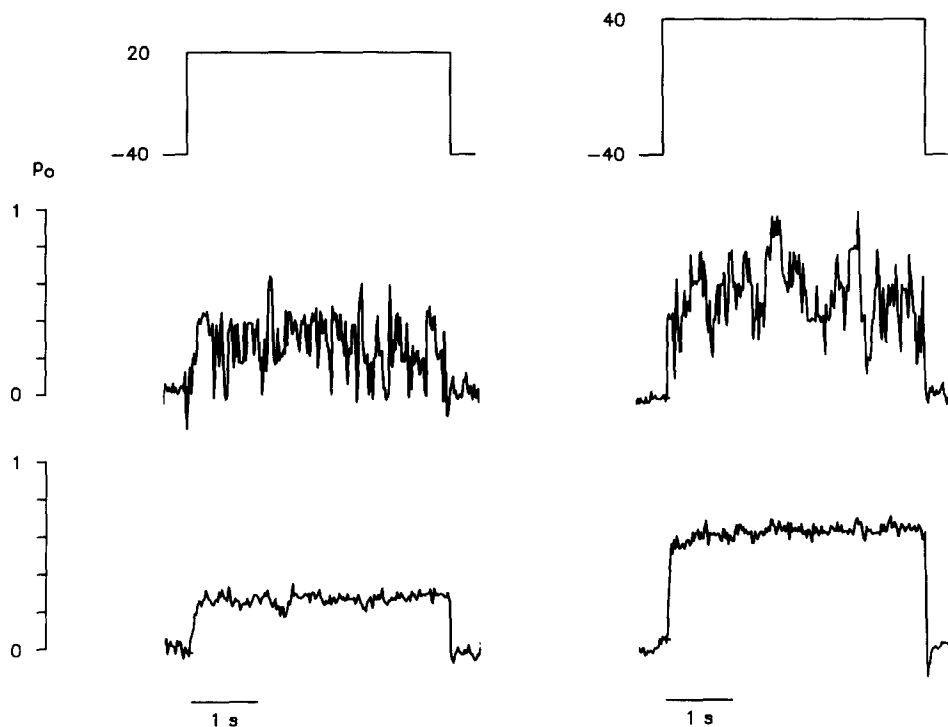


FIGURE 8. Time course of maxi  $K^+$  channel activation. Channels in an inside-out patch exposed symmetrically to 100 mM KCl, with  $[Ca^{2+}]_i = 500$  nM, were subjected to depolarizing steps from  $-40$  mV to 20 or 40 mV. Depolarizing steps caused activation of up to five channels. (Top traces) Holding voltage. (Middle traces) Channel activity elicited by single voltage steps to 20 or 40 mV. (Bottom traces) Ensemble currents assembled from multiple steps ( $n = 50$  for steps to 20 mV;  $n = 30$  for steps to 40 mV).  $P_o$ , single-channel open probability. The ensemble currents indicate that channel activation is essentially complete within 800 ms after the voltage step.

er's solution and on the measurement techniques (see Stoddard and Reuss, 1988a). To allow comparisons between single-channel and microelectrode data, we measured the cable properties of four tissues bathed in 10 mM HEPES-buffered Ringer's. The results of these experiments are summarized in Table II. The apical and basolateral membrane conductances were 180 and 350  $\mu S/cm^2$ , respectively.

To assess the voltage dependence of the macroscopic apical membrane conductance, we carried out a series of current-clamp experiments, summarized in Fig. 9 A.



TABLE II  
Equivalent Circuit Parameters for Gallbladders Bathed in 10 mM HEPES Ringer's

Resistances				
$R_a/R_b$	$R_t$	$R_s$	$R_b$	$R_i$
	$\Omega\text{-cm}^2$	$\Omega\text{-cm}^2$	$\Omega\text{-cm}^2$	$\Omega\text{-cm}^2$
$2.0 \pm 0.4$	$105 \pm 18$	5,500	2,800	106
Voltages and EMFs				
$V_{ms}$	$V_{mc}$	$V_{cs}$	$E_a$	$E_b$
	$mV$			
$0 \pm 1$	$-68 \pm 2$	$-68 \pm 2$	-68	-68

Values are mean  $\pm$  SEM of four experiments. Values without SEM were determined from the steady-state equivalent circuit model (see Reuss and Finn, 1975a).  $R_a$ , apical membrane resistance;  $R_b$ , basolateral membrane resistance;  $R_t$ , transepithelial resistance;  $R_s$ , paracellular resistance;  $V_{ms}$ , transepithelial voltage;  $V_{mc}$ , apical membrane voltage;  $V_{cs}$ , basolateral membrane voltage;  $E_a$ , apical membrane equivalent EMF;  $E_b$ , basolateral membrane equivalent EMF.  $\Delta V_{cs}(x)$  was measured as described in Materials and Methods. The pooled experimental points were fitted to a zero-order Bessel function (see Reuss and Finn, 1975a for details), yielding a space constant  $\lambda$  of 297  $\mu\text{m}$ , and an  $A_0$  value of 16.9 mV; these values for  $\lambda$  and  $A_0$  lead to an estimate of 1,900  $\Omega\text{-cm}^2$  for  $R_s$  (the resistance of  $R_a$  and  $R_b$  in parallel).

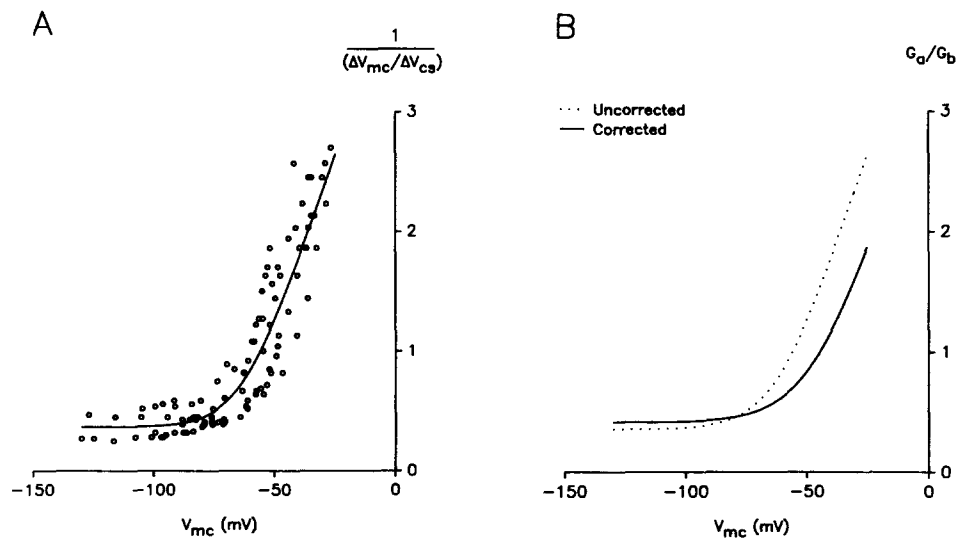


FIGURE 9. Voltage dependence of  $G_a/G_b$ . (A)  $1/(\Delta V_{mc}/\Delta V_{cs})$  vs.  $V_{mc}$  data were pooled for six current-clamp experiments. The solid line represents the best fit to Eq. 3 (see Table II). (B)  $G_a/G_b$  corrected for voltage-induced changes in  $G_a$  and  $E_a$ . (Dotted line) Fitted curve describing uncorrected  $G_a/G_b$  curve, transposed from A. (Solid line) Fitted curve describing corrected  $G_a/G_b$  curve, with  $G_a^0/G_b = 0.43$ ,  $N_a^0/G_b = 2.5 \times 10^{-4} \mu\text{m}^{-2}/(\mu\text{S}/\text{cm}^2)$ ,  $n = 1.6$  and  $V^0 = -46$  mV.

It is evident that as  $V_{mc}$  is depolarized, the apparent ratio of cell membrane conductances rises considerably, as previously observed (García-Díaz et al., 1983; Stoddard and Reuss, 1988*b*). The increase in apparent  $G_a/G_b$  is due to changes in  $G_a$ , i.e., to activation of conductive pathways in the apical membrane (García-Díaz et al., 1983; Stoddard and Reuss, 1988*b*). In light of the present work, maxi  $K^+$  channels are likely to account for this increase in conductance.

#### Correlation of Single-Channel and Microelectrode Data

Single maxi  $K^+$  channels and macroscopic  $G_a$  are related by Eqs. 2 and 3. In the first step of the three-step process for fitting  $G_a(V_{mc})/G_b$  (see Models), uncorrected  $G_a/G_b$  data were fitted to Eq. 3, with  $P_o(V_{mc})$  given by a Boltzmann relation. The resulting best-fit parameters are shown in Table III; the best-fit curve is shown in Fig. 9 A. This curve provides a reasonable description of the pooled data, but deviates from

TABLE III  
Reconstruction of the Apical Membrane Conductance  $G_a(V_{mc})$

Uncorrected $G_a/G_b$ data						
	$G_a^0/G_b$	$G_a^0$	$N_a/G_b$	$N_a$	$n$	$V^0$
		$\mu S/cm^2$	$\mu m^{-2}/(\mu S/cm^2)$	$1/\mu m^2$		$mV$
	0.37	130	$3.4 \times 10^{-4}$	0.12	2.1	-60
Corrected $G_a/G_b$ data						
Fixed $n$	0.42	150	$2.6 \times 10^{-4}$	0.09	1.6	-45
Varying $n$	0.43	150	$2.5 \times 10^{-4}$	0.09	1.8	-46

Values represent best-fit parameters obtained from fitting  $G_a/G_b$  data to Eq. 3. Uncorrected data were estimated from  $1/(\Delta V_{mc}/\Delta V_{cs})$ , as described in Materials and Methods. Corrected  $G_a/G_b$  data were obtained as described in the Appendix. Fixed  $n$ :  $n$  is fixed at 1.6, the value determined in single-channel studies. Varying  $n$ :  $n$  is adjustable.  $G_a$ , apical membrane conductance;  $G_b$ , basolateral membrane conductance;  $G_a^0$ , baseline apical membrane conductance;  $N_a$ , apical membrane maxi  $K^+$  channel surface density;  $n$  and  $V^0$  are defined in the legend to Table I. Estimates for  $G_a^0$  and  $N_a$  were obtained by multiplying  $G_a^0/G_b$  and  $N_a/G_b$  by  $350 \mu S/cm^2$ , the value of  $G_b$  determined in cable analysis experiments.

the true  $G_a(V_{mc})/G_b$  relation, inasmuch as estimation of  $G_a/G_b$  from  $1/(\Delta V_{mc}/\Delta V_{cs})$  neglects the voltage dependence of  $G_a$  and  $E_a$  (see Appendix). In the second step at the fitting process, the  $G_a/G_b$  relation was corrected for voltage-induced changes in  $G_a$  and  $E_a$ . As shown in Fig. 9 B, uncorrected  $G_a/G_b$  values deviate from corrected  $G_a/G_b$  values as the magnitude of  $\Delta V_{mc}$  increases, underestimating  $G_a/G_b$  by 9% at  $V_{mc} = -100$  mV, and overestimating  $G_a/G_b$  by 43% at  $V_{mc} = -25$  mV.

Although the region of overlap between single-channel and microelectrode data is restricted to the voltage range of  $-25$  to  $-60$  mV, we chose, in the third step of the fitting procedure, to fit the entire range of  $G_a(V_{mc})$ , with the results shown in Table III. When the fit was confined to the region of overlap, the best-fit parameters differed by less than 10% from those showed in Table III.

The results of the fit indicate that the leakage conductance of  $G_a^0$  is roughly  $150 \mu S/cm^2$ , or 83% of the control apical membrane conductance of  $180 \mu S/cm^2$ . The

remaining portion of control  $G_a$  can be accounted for by maxi K<sup>+</sup> channels, which are present at a surface density of  $0.09/\mu\text{m}^2$ , and which have a  $P_o$  of 0.15 and a slope conductance of  $\sim 23$  pS at control  $V_{mc}$ . Depolarizing  $V_{mc}$  increases macroscopic  $G_a$  as a result of both channel rectification and channel activation, inasmuch as channels at resting  $V_{mc}$  operate at the foot of the activation curve (see Fig. 10). The membrane voltage at which  $P_o$  is half-maximal ( $V^0$ ) is  $-45$  mV. If the Ca<sup>2+</sup> and voltage dependencies of channel gating are assumed to be similar in situ and in excised patches, as appears to be the case in other cells (Pallotta et al., 1987), then Eq. 6 yields an estimate of  $1.2 \mu\text{M}$  for free [Ca<sup>2+</sup>] near the channel regulatory site. That is, channel activity is higher than predicted from the bulk cytosolic Ca<sup>2+</sup> activity of 100–200 nM, measured using intracellular microelectrode techniques (Palant and Kurtz, 1986). Possible mechanisms accounting for the apparent enhancement of apical membrane maxi K<sup>+</sup> channel activity are considered in the Discussion.

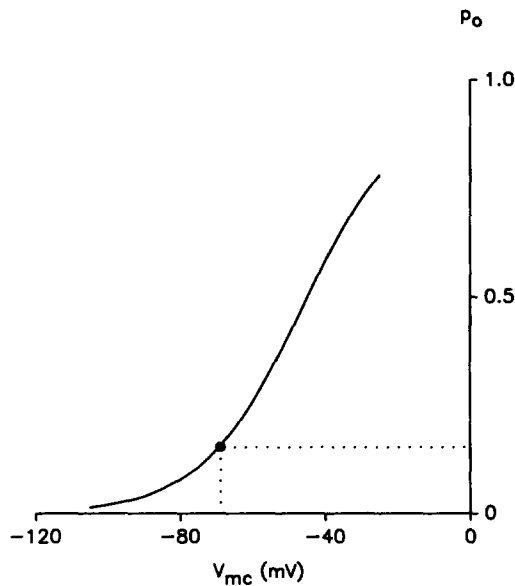


FIGURE 10. Reconstructed  $P_o(V_{mc})$  curve for apical membrane maxi K<sup>+</sup> channels. The curve is given by a Boltzmann relation (Eq. 4), with  $P_o^{\text{max}} = 0.94$ ,  $n_z = 1.9$  and  $V^0 = -46$  mV. Dotted lines denote control  $V_{mc}$  and  $P_o$  values of  $-68$  mV and 0.12, respectively. This is the shape that  $P_o(V_{mc})$  must take to account for the voltage dependence of the apical membrane conductance.

## DISCUSSION

### *Maxi K<sup>+</sup> Channels in Gallbladder Epithelium*

The apical membrane of *Necturus* gallbladder epithelium is predominantly K<sup>+</sup> conductive, and displays a small Na<sup>+</sup> conductance (Reuss and Finn, 1975*a, b*). Ordinarily, the apical membrane is the dominant resistance to transepithelial current flow, accounting for 60–90% of the transcellular resistance, although apical membrane resistance can be lowered by numerous factors, including membrane depolarization (García-Díaz et al., 1983; Stoddard and Reuss, 1988*b*), elevation of intracellular Ca<sup>2+</sup> (Bello-Reuss et al., 1981; García-Díaz et al., 1983) or cAMP levels (Petersen and Reuss, 1983), and extracellular alkalization (Reuss et al., 1981). The

apical membrane  $K^+$  conductance in guinea pig gallbladder is also  $Ca^{2+}$  and voltage sensitive (Gunter-Smith, 1988).

In this paper, we describe single channels whose properties would explain the depolarization-induced,  $Ca^{2+}$ -activated apical membrane  $K^+$  conductance in *Necturus* gallbladder. In cell-attached patches, these channels open infrequently at the resting apical membrane voltage, and activate with membrane depolarization. In excised, inside-out patches from the apical membrane of the intact epithelium, these channels are more than 20-fold selective for  $K^+$  over  $Na^+$ , display a large unitary conductance ( $>150$  pS) in symmetrical KCl solutions, and are blocked in a voltage-dependent manner by 1 mM internal  $Ba^{2+}$ . Similar large conductance  $K^+$  channels are observed in patches excised from dissociated gallbladder cells. Like apical membrane  $K^+$  channels, maxi  $K^+$  channels from dissociated cells are more than 10-fold selective  $K^+$  over  $Na^+$  and are blocked in a voltage-dependent manner by internal  $Ba^{2+}$  ions. In addition, they are activated by membrane depolarization and by elevation of internal  $Ca^{2+}$  levels.

#### *Origin of Gallbladder Maxi $K^+$ Channels*

The ion selectivity, unitary conductance, and  $Ca^{2+}$  and  $Ba^{2+}$  sensitivities of maxi  $K^+$  channels from dissociated cells suggest that these channels are similar to those in the intact apical membrane. Three additional items of evidence further support the notion that maxi  $K^+$  channels are of apical membrane origin. First, the  $Ca^{2+}$  and voltage sensitivities of these channels parallel those of the macroscopic apical membrane conductance, i.e., both activate with membrane depolarization and elevation of intracellular  $Ca^{2+}$  levels. Second, these channels and the voltage-dependent component of the macroscopic conductance exhibit similar patterns of sensitivity to the  $K^+$  channel blockers  $Ba^{2+}$  and  $TEA^+$  (Segal and Reuss, in press). Third, recent studies on dissociated cells isolated from cAMP-stimulated gallbladders reveal small-conductance (10 pS)  $Cl^-$  channels which colocalize with maxi  $K^+$  channels (Segal and Reuss, 1989). Since cAMP activates an apical membrane  $Cl^-$  conductance (Petersen and Reuss, 1983), it is likely that patches containing single  $Cl^-$  channels originate in the apical membrane. The notion that the apical membrane domain remains accessible in the plasma membrane of dissociated cells is supported by morphological studies on dissociated rat small intestinal epithelial cells (Ziomek et al., 1980; Bjorkman et al., 1986). In these systems, apical membrane markers such as microvilli or enzyme activities redistribute uniformly around the cell within minutes after dissociation.

Taken together, these pieces of evidence suggests that channels originating in the apical membrane remain accessible in dissociated cells. Although these arguments are indirect and do not strictly exclude the possibility that the channels under study are basolateral, the lack of voltage dependence of the basolateral membrane argues against the presence of maxi  $K^+$  channels in this membrane (García-Díaz et al., 1983; Stoddard and Reuss, 1988b). Basolateral membrane maxi  $K^+$  channels, considered hypothetically, do not have serious implications for our model, for the following reasons: first, the voltage and  $Ca^{2+}$  sensitivities of the channels are not expressed in situ (i.e.,  $G_b$  is constant), and second, these channels, if studied in excised patches, are similar to apical membrane channels in the intact epithelium.

Definitive localization of maxi K<sup>+</sup> channels will require further patch-clamp studies on the intact epithelium, and morphological studies, which will be made possible when probes for maxi K<sup>+</sup> channels become available.

Apical membrane maxi K<sup>+</sup> channels in *Necturus* gallbladder are similar to those observed in numerous leaky NaCl-absorbing epithelia, including *Triturus* gallbladder (Maruyama et al., 1986), *Necturus* proximal tubule (Kawahara et al., 1987), and primary cultures of rabbit proximal tubule cells (Merot et al., 1989). Basolateral membrane K<sup>+</sup> channels from leaky epithelia exhibit markedly different properties. The basolateral membrane of *Necturus* proximal tubule contains at least two types of K<sup>+</sup> channels, which have unitary conductances of <50 pS, and which are inactivated by membrane depolarization (Sackin and Palmer, 1987; Kawahara et al., 1987). The basolateral membrane of rabbit proximal tubule contains a K<sup>+</sup> channel that shows sharp inward rectification in symmetrical high K<sup>+</sup>, and that is weakly activated by membrane depolarization (Parent et al., 1988). Basolateral maxi K<sup>+</sup> channels have been identified in studies on dissociated enterocytes from rat and *Necturus* small intestine (Morris et al., 1986; Sheppard et al., 1988). Consistent with this observation, the small intestine mounted in vitro responds to apical membrane depolarization with an increase in basolateral membrane K<sup>+</sup> conductance, rather than an increase in apical membrane K<sup>+</sup> conductance (Grasset et al., 1983).

#### *Relating Single Maxi K<sup>+</sup> Channels to the Apical Membrane Conductance*

The common properties shared by the voltage-dependent component of the macroscopic apical membrane K<sup>+</sup> conductance and single maxi K<sup>+</sup> channels suggest a link between the two. To account for the macroscopic conductance in quantitative terms, we have used simple models to describe steady-state conduction and gating properties of maxi K<sup>+</sup> channels. Our analysis is based on the assumption that conduction and gating are distinct processes that can be studied separately, each under optimal experimental conditions. For instance, in studies examining conduction at physiological Na<sup>+</sup> and K<sup>+</sup> concentrations, channels were activated with high Ca<sup>2+</sup>, in order to obtain well-resolved transitions between open and closed states, and accurate estimates of the single-channel current amplitude. Analogously, in studies examining channel gating, patches were bathed in symmetrical K<sup>+</sup>, rather than physiological K<sup>+</sup> and Na<sup>+</sup> concentrations, to enhance the channel signal-to-noise ratio in the physiological V<sub>m</sub> range.

Steady-state conduction through channels exposed to physiological K<sup>+</sup> and Na<sup>+</sup> concentrations was described using a simplified barrier model, which borrows from multi-site models developed to describe conduction through maxi K<sup>+</sup> and other K<sup>+</sup> channels (Hodgkin and Keynes, 1955; Hille and Schwarz, 1978; Neyton and Miller, 1988). The Ca<sup>2+</sup> and voltage dependencies of channel gating were analyzed empirically using Boltzmann relations. Kinetic analyses provide another means of describing P<sub>o</sub>(Ca<sup>2+</sup>, V<sub>mc</sub>) (see Moczydlowski and Latorre, 1983), but such analyses are complex for maxi K<sup>+</sup> channels (McManus and Magleby, 1988), and beyond the scope of this paper. The expressions linking single-channel conductance and gating to macroscopic apical membrane conductance (Eqs. 2 and 3) give rise to estimates for the surface density and voltage-dependent P<sub>o</sub> of apical membrane maxi K<sup>+</sup> channels.

Single-channel  $P_o$  at the resting apical membrane voltage is roughly 0.15, and increases steeply with membrane depolarization to a value of 0.78 at  $V_{mc} = -25$  mV. A reexamination of two cell-attached patch experiments reveals the same pattern. Assuming that  $V_{mc}$  equals  $-70$  mV in cell-attached patch experiments, the  $P_o$  values in one experiment, shown in Fig. 1, increased from 0.08 at  $V_{mc} = -70$  mV to 0.79 at  $V_{mc} = -30$  mV; in the second experiment (not shown),  $P_o$  increased from 0.01 to 0.84. In these experiments,  $P_o$  at resting  $V_{mc}$  was less than the value of 0.15 estimated from intracellular microelectrode experiments. Inasmuch as the number of cell-attached patch-clamp experiments is small, the significance of this difference is unclear. Regardless, the best-fit parameters describing  $G_a(V_{mc})$  and results of cell-attached patch studies support the same conclusion, namely, that  $P_o$  is low at control  $V_{mc}$ , and that the steep increase in apical membrane conductance accompanying even small depolarizations (see Fig. 10) arises from both channel activation and outward rectification of the single-channel  $I$ - $V$  relation. The  $P_o(V_{mc})$  curves steepen at more negative membrane voltages than those predicted on the basis of inside-out patch studies (Fig. 7), if the intracellular free  $Ca^{2+}$  concentration is taken to be 100–200 nM (see Palant and Kurtz, 1986). Previous studies on rabbit cortical collecting tubule (Hunter et al., 1986) and *Necturus* choroid plexus (Christensen and Zeuthen, 1987) have noted that apical (or ventricular) membrane maxi  $K^+$  channel activity is higher than predicted from bulk cytosolic  $Ca^{2+}$  levels.

#### *Accounting for Apical Membrane Maxi $K^+$ Channel Activity*

There are several possible explanations for the higher-than-expected activity of apical membrane maxi  $K^+$  channels. First, the regulation of channels in excised patches may differ from regulation in situ, e.g., by loss of a channel-activating factor. Besides membrane voltage and intracellular  $Ca^{2+}$  levels, pH (Cook et al., 1984; Christensen and Zeuthen, 1987), and  $Mg^{2+}$  (Golowasch et al., 1986), and membrane surface charge (Moczydlowski et al., 1985) can regulate maxi  $K^+$  channel activity. A second possibility is that maxi  $K^+$  channel activity in situ is heightened by elevated  $Ca^{2+}$  levels in the immediate vicinity of the apical membrane. If the  $Ca^{2+}$ - and voltage-dependent mechanisms governing channel behavior in the intact epithelium and in cell-excised patches are similar, as has been demonstrated for maxi  $K^+$  channels from other tissues (Pallotta et al., 1987), then it follows from our estimate of  $V^0$  ( $-45$  mV) that free  $Ca^{2+}$  levels near the channel regulatory sites are 1–2  $\mu$ M. Steady-state elevations in internal  $Ca^{2+}$  near the apical membrane surface would require a constitutive  $Ca^{2+}$  influx, e.g., through  $Ca^{2+}$ -permeable channels, bile-acid anion-mediated pathways (Montrose et al., 1988), or sites of membrane damage, and means of rapidly buffering incoming  $Ca^{2+}$  ions. A final possibility is that maxi  $K^+$  channels are not the only  $K^+$  channels that underlie the voltage-dependent component of  $G_a$ . To play a role in the voltage activation of  $G_a$ , a second channel type would need to satisfy the following requirements: (a) marked outward rectification of the single-channel  $I$ - $V$  relation, and/or activation with membrane depolarization; (b) susceptibility to block by external TEA<sup>+</sup> and Ba<sup>2+</sup>; and (c) undetectability in patch-clamp experiments, by virtue of a small unitary conductance, low frequency of transitions between open and closed states, or tendency to run down in cell-excised patches.

*Significance of  $G_a^0$  and  $N_a$* 

Two additional parameters emerge from reconstruction of  $G_a(V_{mc})$ , namely the leakage conductance  $G_a^0$  and the apical membrane maxi K<sup>+</sup> channel surface density  $N_a$ . Given the estimate of 150  $\mu\text{S}/\text{cm}^2$  for  $G_a^0$  and the total  $G_a$  of 180  $\mu\text{S}/\text{cm}^2$  at control  $V_{mc}$ , it follows that the effective equilibrium potential of channels underlying  $G_a^0$  must be -64 mV, to account for the control apical membrane equivalent EMF of -68 mV. That is, the leakage conductance is predominantly K<sup>+</sup> selective, and probably harbors the small Na<sup>+</sup> permeability of the apical membrane (Reuss and Finn, 1975a, b). We have yet to identify the channels that underlie  $G_a^0$ . Difficulties in their identification would be expected if they have small unitary conductance and rarely close, like apical membrane K<sup>+</sup> channels recently described in rat renal cortical collecting tubule (Frindt and Palmer, 1989).

Estimates for the surface density of apical (or ventricular) membrane maxi K<sup>+</sup> channels are 0.06/ $\mu\text{m}^2$  in MDCK cells (Bolívar and Cerejido, 1987), 0.24/ $\mu\text{m}^2$  in *Triturus* gallbladder (Maruyama et al., 1986), and 0.4–0.9/ $\mu\text{m}^2$  in *Necturus* choroid plexus (Christensen and Zeuthen, 1987). Our estimate of 0.09  $\mu\text{m}^2$ , appears to fall within this range, and slightly outside the range (0.1–1.9/ $\mu\text{m}^2$ ) estimated for apical membrane K<sup>+</sup> channels in *Necturus* gallbladder on the basis of fluctuation analysis techniques (Gögelein and van Driessche, 1981). Importantly, our estimates are referred to  $\mu\text{m}^2$  of stretched epithelium, rather than the true surface area of the apical membrane, which contains microvilli. It is also possible to estimate  $N_a$  based on the number of channels in membrane patches, and the patch surface area. Patches from the apical membrane of the intact epithelium contained  $2.6 \pm 0.7$  channels/patch ( $n = 5$ ). To match  $N_a$  determined from macroscopic  $G_a$ , patch areas corresponding to 30  $\mu\text{m}^2$  of stretched epithelium would be required. Total patch areas of 25  $\mu\text{m}^2$  are in the upper range of those determined for chromaffin cells and neuroblastoma (Sakmann and Neher, 1983); thus, it would appear that 0.1/ $\mu\text{m}^2$  is the lower limit on  $N_a$  estimated from the number of channels per patch. Without capacitance measurements in our studies, the true surface area of patches excised from the folded apical membrane remains unknown.

*Function of Maxi K<sup>+</sup> Channels in Gallbladder Equilibrium*

The channels described here classify among the Ca<sup>2+</sup>-activated maxi K<sup>+</sup> channels first observed in nerve and muscle preparations, and later identified in the apical membrane of numerous epithelia. In *Necturus* gallbladder, maxi K<sup>+</sup> channels are unlikely to contribute substantially to the baseline K<sup>+</sup> permeability of the apical membrane, though their expected contribution (17%) exceeds that estimated for maxi K<sup>+</sup> channels in other epithelia (Frindt and Palmer, 1987). In light of their steep voltage and Ca<sup>2+</sup> sensitivities, it is more likely that maxi K<sup>+</sup> channels are important in cellular responses to physiological perturbations. These channels are equipped to repolarize the cell membrane voltage in response to agents which depolarize the apical membrane, and to promote KCl loss in response to cell swelling.

Maxi K<sup>+</sup> channels may also provide a pathway for transcellular K<sup>+</sup> secretion, which has been demonstrated in *Necturus* gallbladder (Reuss, 1981), and which is favored by the electrochemical gradient for K<sup>+</sup> movement across the apical mem-

brane. The sensitivities of the channels to membrane voltage and  $\text{Ca}^{2+}$  suggest that transcellular  $\text{K}^+$  secretion may be a highly regulated process. This is probably of secondary importance in leaky  $\text{NaCl}$ -absorbing epithelia like the gallbladder, in which transcellular  $\text{K}^+$  secretion is matched by paracellular absorption (Reuss, 1981), but may be crucial in  $\text{K}^+$ -secreting tight epithelia, like the mammalian cortical collecting tubule (see Hunter et al., 1984, 1986; Frindt and Palmer, 1987). The exact role(s) of these channels in the regulation of fluid absorption across gallbladder epithelium will require further examination.

#### APPENDIX

Intracellular microelectrode studies on epithelial tissues commonly use transepithelial current pulses as a means of estimating the ratio of apical to basolateral membrane resistances ( $R_a/R_b$ ). Current applied across the epithelium distributes between transcellular and paracellular pathways; the transcellular current ( $i_c$ ) gives rise to voltage deflections  $\Delta V_{mc}$  and  $\Delta V_{cs}$  across the apical and basolateral membranes, respectively. The ratio of the cell membrane resistances is estimated by:

$$\frac{R_a}{R_b} = \frac{\Delta V_{mc}/i_c}{\Delta V_{cs}/i_c} = \frac{\Delta V_{mc}}{\Delta V_{cs}} \quad (\text{A1})$$

In light of the voltage dependence of  $R_a$ , we have reexamined the accuracy of  $\Delta V_{mc}/\Delta V_{cs}$  as an estimator of  $R_a/R_b$ .

In the absence of an applied transepithelial current, the apical and basolateral membrane voltages  $V_{mc}$  and  $V_{cs}$  can be expressed as follows:

$$V_{mc} = E_a - \frac{(E_a + E_b) R_a}{R_a + R_b + R_s} \quad (\text{A2})$$

$$V_{cs} = E_b - \frac{(E_a + E_b) R_b}{R_a + R_b + R_s} \quad (\text{A3})$$

where  $E_a$  and  $E_b$  are the equivalent EMFs of the apical and basolateral membranes (Reuss and Finn, 1975a). For convenience,  $E_a$  and  $V_{mc}$  are referred to the cell interior, while  $E_b$  and  $V_{cs}$  are referred to the serosal solution. Cable experiments reveal that for tissues bathed in 10 mM HEPES-buffered Ringer's,  $E_a = E_b$  (see Table II), so Eqs. A2 and A3 simplify to:

$$V_{mc} = E_a \quad (\text{A4})$$

$$V_{cs} = E_b \quad (\text{A5})$$

Transepithelial serosa-to-mucosa current clamps depolarize  $V_{mc}$  and hyperpolarize  $V_{cs}$ . Depolarization of  $V_{mc}$  activates maxi  $\text{K}^+$  channels, reducing  $R_a$  to a new value  $R'_a$ . As the relative  $\text{K}^+$  conductance of the apical membrane increases,  $E_a$  shifts to a value  $E'_a$ , closer to  $E_K$ . Mucosa-to-serosa current clamps have the opposite effects. During a current clamp, the membrane voltages stabilize at values given by:

$$V'_{mc} = E'_a + \left[ \frac{i_c R_s - (E'_a + E_b)}{R'_a + R_b + R_s} \right] R'_a \quad (\text{A6})$$

$$V'_{cs} = E_b + \left[ \frac{i_b R_s - (E'_a + E_b)}{R'_a + R_b + R_s} \right] R_b \quad (\text{A7})$$

where  $i_c$  is the transepithelial current density, deemed positive for mucosa-to-serosa current



clamps.  $\Delta V_{mc}$  and  $\Delta V_{cs}$  are obtained by subtracting Eq. A4 from A6, and Eq. A5 from A7. Dividing  $\Delta V_{mc}$  by  $\Delta V_{cs}$ :

$$\frac{\Delta V_{mc}}{\Delta V_{cs}} = \frac{(E'_a - E_a) + \left[ \frac{i_1 R_s - (E'_a + E_b)}{R'_a + R_b + R_s} \right] R'_a}{\left[ \frac{i_1 R_s - (E'_a + E_b)}{R'_a + R_b + R_s} \right] R_b} \quad (\text{A8})$$

If  $R_a$  and  $E_a$  are unchanged by the current clamp, then Eq. A8 reduces to  $R_a/R_b$ . However, if  $R_a$  and  $E_a$  do change, then  $R'_a$  and  $E'_a$  emerge as unknowns, and a second equation relating  $R'_a$  and  $E'_a$  is required to calculate these two quantities. Recalling that the apical membrane consists to two functionally different channel types—maxi  $K^+$  channels and voltage-independent baseline channels—it follows that the apical membrane EMF at any membrane voltage is given by:

$$E'_a = \left( 1 - \frac{R'_a}{R_a^0} \right) E_K + \frac{R'_a}{R_a^0} E_a^0 \quad (\text{A9})$$

where  $R'_a = 1/G'_a = 1/(G_a^0 + G_a^K)$ , and  $R_a^0$  and  $E_a^0$  are the total resistance and the equilibrium potential of the leakage pathway. For the control case:

$$E_a = \left( 1 - \frac{R_a}{R_a^0} \right) E_K + \frac{R_a}{R_a^0} E_a^0 \quad (\text{A10})$$

Combining Eqs. A9 and A10 yields:

$$R'_a = R_a \frac{(E'_a - E_K)}{(E_a - E_K)} \quad (\text{A11})$$

Given an experimentally determined value of  $\Delta V_{mc}/\Delta V_{cs}$ , and the control parameters  $R_a$  and  $E_a$  from cable analysis experiments, Eqs. A8 and A11 can be used to solve for  $R'_a$  (thus  $G'_a$ ) and  $E'_a$ .

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