

## Depolarization increases the apparent affinity of the Na<sup>+</sup>–K<sup>+</sup> pump to cytoplasmic Na<sup>+</sup> in isolated guinea-pig ventricular myocytes

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1. In order to investigate the possible effect of membrane potential on cytoplasmic Na<sup>+</sup> binding to the Na<sup>+</sup>–K<sup>+</sup> pump, we studied Na<sup>+</sup>–K<sup>+</sup> pump current–voltage relationships in single guinea-pig ventricular myocytes whole-cell voltage clamped with pipette solutions containing various concentrations of Na<sup>+</sup> ([Na<sup>+</sup>]<sub>pip</sub>) and either tetraethylammonium (TEA<sup>+</sup>) or *N*-methyl-D-glucamine (NMDG<sup>+</sup>) as the main cation. The experiments were conducted at 30 °C under conditions designed to abolish the known voltage dependence of other steps in the pump cycle, i.e. in Na<sup>+</sup>-free external media containing 20 mM Cs<sup>+</sup>.
2. Na<sup>+</sup>–K<sup>+</sup> pump current ( $I_p$ ) was absent in cells dialysed with Na<sup>+</sup>-free pipette solutions and was almost voltage independent at 50 mM Na<sup>+</sup><sub>pip</sub> (potential range: –100 to +40 mV). By contrast, the activation of  $I_p$  by 0.5–5 mM Na<sup>+</sup><sub>pip</sub> was clearly voltage sensitive and increased with depolarization, independently of the main intracellular cation species.
3. The apparent affinity of the Na<sup>+</sup>–K<sup>+</sup> pump for cytoplasmic Na<sup>+</sup> increased monotonically with depolarization. The [Na<sup>+</sup>]<sub>pip</sub> required for half-maximal  $I_p$  activation ( $K_{0.5}$  value) amounted to 5.6 mM at –100 mV and to 2.2 mM at +40 mV.
4. The results suggest that cytoplasmic Na<sup>+</sup> binding and/or a subsequent partial reaction in the pump cycle prior to Na<sup>+</sup> release is voltage dependent. From the voltage dependence of the  $K_{0.5}$  values the dielectric coefficient for intracellular Na<sup>+</sup> binding/translocation was calculated to be ~0.08. The voltage-dependent mechanism might add to the activation of the cardiac Na<sup>+</sup>–K<sup>+</sup> pump during cardiac excitation.

The Na<sup>+</sup>–K<sup>+</sup> pump of animal cells exchanges three intracellular Na<sup>+</sup> (Na<sub>i</sub><sup>+</sup>) for two extracellular K<sup>+</sup> (K<sub>o</sub><sup>+</sup>) per ATP molecule hydrolysed and is, therefore, electrogenic. It generates the steady-state pump current,  $I_p$ . Under physiological conditions  $I_p$  is an outward current exhibiting a characteristic voltage dependence. The current decreases at negative membrane potentials and displays a maximum (Lafaire & Schwarz, 1986) or remains nearly constant (Gadsby *et al.* 1985) at positive voltages. Na<sup>+</sup>-free external solution containing physiological [K<sup>+</sup>]<sub>o</sub> reduces or abolishes the voltage dependence of  $I_p$  at negative potentials (Gadsby & Nakao, 1989; Rakowski *et al.* 1989, 1991; Bielen *et al.* 1991). A negative slope of the  $I_p$ – $V$  relationship can be observed at low [K<sup>+</sup>]<sub>o</sub>, especially in Na<sup>+</sup>-free media (Bielen *et al.* 1991, 1993; Rakowski *et al.* 1991). These and other findings reveal voltage-dependent (re)binding of extracellular Na<sup>+</sup> and K<sup>+</sup> to the Na<sup>+</sup>–K<sup>+</sup> pump. The voltage dependence of cation binding is probably due to the existence of a ‘high-field, narrow access channel’ (cf. Läuger, 1991) at the bottom of which the interaction between external Na<sup>+</sup>, K<sup>+</sup> and their respective binding sites takes place (review: Rakowski *et al.* 1997*b*). Whether a similar access channel to the intracellular

cation binding sites of the pump exists is an unsettled question. Data from vesicles (Goldshlegger *et al.* 1987; Or *et al.* 1996) and membrane fragments containing Na<sup>+</sup>–K<sup>+</sup> pumps (Stürmer *et al.* 1991; Heyse *et al.* 1994; Wuddel & Apell, 1995) suggest a positive answer to this question, whereas whole-cell recordings from cardiac myocytes do not permit an unequivocal conclusion (Nakao & Gadsby, 1989; Kockskämper & Glitsch, 1997). Binding of internal Na<sup>+</sup> to the Na<sup>+</sup>–K<sup>+</sup> pump is a mechanism of physiological relevance since, under physiological conditions, the pump activity is predominantly regulated by changes in [Na<sup>+</sup>]<sub>i</sub>. The aim of the present work was to find out if the binding of intracellular Na<sup>+</sup> to the Na<sup>+</sup>–K<sup>+</sup> pump is voltage dependent. The experiments to be described were carried out on whole-cell voltage-clamped guinea-pig ventricular myocytes under conditions designed to exclude the troublesome effects of simultaneous, voltage-dependent binding of extracellular cations on the steady-state  $I_p$  measurements. The results suggest that cytoplasmic Na<sup>+</sup> binding and/or another step in the Na<sup>+</sup> translocation limb of the pump cycle prior to Na<sup>+</sup> release is voltage dependent.

## METHODS

### Isolation of ventricular myocytes

Ventricular myocytes were isolated essentially as described previously (Kockskämper *et al.* 1997). Briefly, adult female guinea-pigs (200–450 g) were killed by cervical dislocation. Following thoracotomy, hearts were cannulated via the aorta and quickly excised, then mounted on a Langendorff apparatus and perfused at 37 °C with oxygenated Ca<sup>2+</sup>-free solution containing (mM): sucrose, 204; NaCl, 35; KCl, 5.4; MgCl<sub>2</sub>, 1.0; EGTA, 2.0; Hepes, 10; pH 7.4 (adjusted with NaOH). After 2 min, perfusion was changed to a medium additionally containing collagenase B (0.4 mg ml<sup>-1</sup>, Boehringer Mannheim, Mannheim, Germany), protease (type XIV, 0.3 mg ml<sup>-1</sup>, Sigma, Deisenhofen, Germany), elastase (10 µl ml<sup>-1</sup>, Serva, Heidelberg, Germany), DNase (0.15 mg ml<sup>-1</sup>, Sigma), bovine serum albumin (BSA, 0.5 mg ml<sup>-1</sup>, Sigma), and 0.1 mM instead of 2.0 mM EGTA. Digested ventricles were cut into small pieces and transferred to nominally Ca<sup>2+</sup>-free, protease-free solution containing BSA and DNase. Finally, this solution was exchanged for cell culture medium (1.3 mM Ca<sup>2+</sup>; Hanks' medium 199, PAA, Linz, Austria) supplemented with 10<sup>5</sup> i.u.l<sup>-1</sup> penicillin and 100 mg l<sup>-1</sup> streptomycin (both from Sigma). Isolated cardiomyocytes were plated on culture dishes and kept in an incubator (37 °C, 3% CO<sub>2</sub>) until use on the same day.

### Experimental solutions

The extracellular (superfusion) solution was composed of (mM): *N*-methyl-D-glucamine (NMDG) 145; CsCl 20; BaCl<sub>2</sub> 4.0; MgCl<sub>2</sub> 1.0; CdCl<sub>2</sub> 0.2; Hepes 10; pH 7.4 (adjusted with HCl).

Two pipette solutions were used, one based on NMDG and the other based on tetraethylammonium (TEA<sup>+</sup>). The Na<sup>+</sup> concentration of the respective solution was varied by equimolar substitution for NMDG or TEA<sup>+</sup>. The composition of the NMDG-based solution was (mM): NMDG plus Na<sup>+</sup>, 160; aspartic acid, 120; HCl, 40; MgCl<sub>2</sub>, 3; EGTA, 6; Hepes, 10; MgATP, 10; pH 7.3 (adjusted with NMDG). TEA<sup>+</sup>-based solution contained (mM): TEA-Cl plus NaCl, 135; TEA-OH, 20; MgCl<sub>2</sub>, 3; EGTA, 6; Hepes, 16; MgATP, 10; pH 7.3 (adjusted with TEA-OH).

The solutions were designed in order to abolish voltage-dependent (re)binding of extracellular Na<sup>+</sup> and Cs<sup>+</sup> to the Na<sup>+</sup>-K<sup>+</sup> pump (cf. Rakowski *et al.* 1997b) and to suppress currents via ion channels and electrogenic transporters. Thus, the superfusate was Na<sup>+</sup>-free and contained a high concentration of Cs<sup>+</sup> (20 mM) saturating the external K<sup>+</sup>/Cs<sup>+</sup> binding sites of the cardiac Na<sup>+</sup>-K<sup>+</sup> pump (Bielen *et al.* 1993). We used Cs<sup>+</sup> rather than K<sup>+</sup> as the extracellular activator cation of the pump because it also blocks K<sup>+</sup> conductances. To avoid any possible competition between Na<sup>+</sup> and K<sup>+</sup>/Cs<sup>+</sup> at the internal cation binding sites, the pipette solutions were free of K<sup>+</sup> and Cs<sup>+</sup>. Furthermore, any putative voltage-dependent binding of the latter two cations to cytoplasmic binding sites of the Na<sup>+</sup>-K<sup>+</sup> pump (Hansen *et al.* 1997) is absent under these conditions. *I<sub>p</sub>*, the outward current generated by the Na<sup>+</sup>-K<sup>+</sup>-ATPase, was measured as the inward shift of the membrane current upon application of 0.1 mM ouabain, a specific inhibitor of this enzyme (cf. Fig. 1A). This ouabain concentration completely blocked the Na<sup>+</sup>-K<sup>+</sup> pump current under our experimental conditions since a tenfold higher concentration did not cause any further inward shift of the holding current (*n* = 2; data not shown). The NMDG-based solutions used resembled those previously described by Dobretsov & Stimers (1997), with slight modifications.

### Experimental procedure and electrical measurements

A culture dish containing isolated ventricular myocytes was placed on the stage of an inverted microscope (Diaphot-TMD, Nikon). The

cell under study was positioned in the laminar solution flow (0.4 ml min<sup>-1</sup>) of a multibarrelled, solenoid-operated pipette that allowed rapid exchange of the superfusate (~1 s). Experiments were conducted in the whole-cell mode of the patch clamp technique (Hamill *et al.* 1981). Ventricular myocytes were voltage clamped by means of an EPC-8 patch clamp amplifier (HEKA, Lambrecht, Germany) connected to a personal computer (386) via 12 bit AD- and DA-converters, respectively. Commercially available software (ISO2, MFK, Niedernhausen, Germany) was used for generation of the voltage protocols and current recording. Membrane currents were low pass filtered at 200 Hz and digitized at 1 kHz.

Patch pipettes were made from borosilicate glass capillaries (GC150TF-10, Clark Electromedical Instruments, Reading, UK). The resistance of the pipettes amounted to 2–4 MΩ when backfilled with the respective pipette solution. Potential differences between the pipette and superfusion solution were nulled immediately before patch formation. Membrane capacitance (*C<sub>m</sub>*) was estimated at a holding potential of 0 mV by a program routine applying ±10 mV voltage ramps or by integration of the capacitive current transient during a voltage step from 0 to -10 mV. Both estimates were almost identical. Mean *C<sub>m</sub>* of the guinea-pig ventricular myocytes used in this study was 103 ± 5 pF (*n* = 55).

### Drugs

Ouabain (Sigma), a specific inhibitor of the Na<sup>+</sup>-K<sup>+</sup> pump, was prepared as a 10 mM stock solution in 10% ethanol (v/v). Thus, at 0.1 mM ouabain, the concentration used in most experiments, the superfusate contained 0.1% ethanol which, by itself, had no effect on the membrane current under the present experimental conditions (*n* = 2; data not shown).

### Statistics

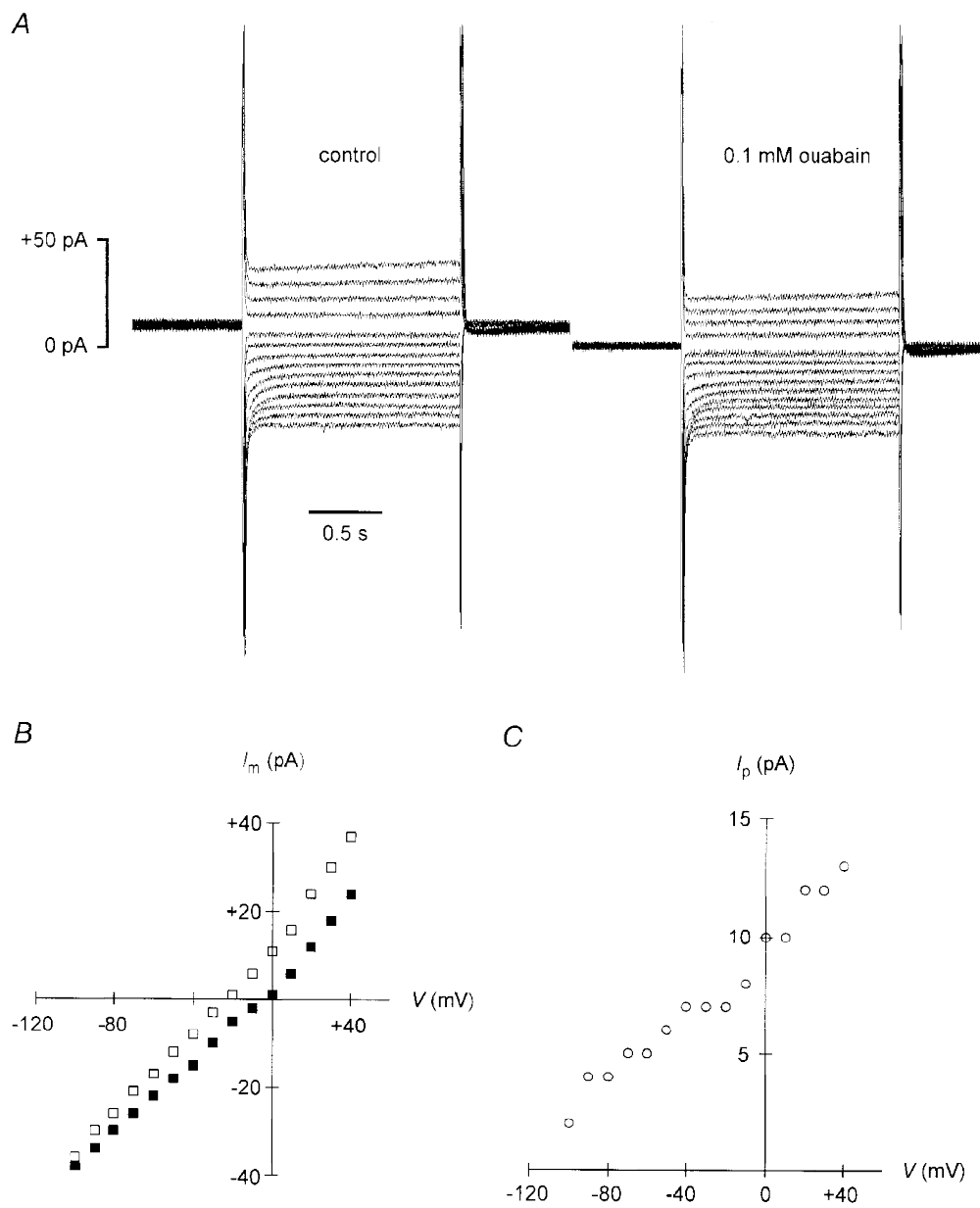
Data are presented as means ± s.e.m. and *n* indicates the number of cells studied. Error bars are shown only when exceeding the size of the symbol. Differences between data points were checked by Student's unpaired *t* test and considered significant if *P* < 0.05.

## RESULTS

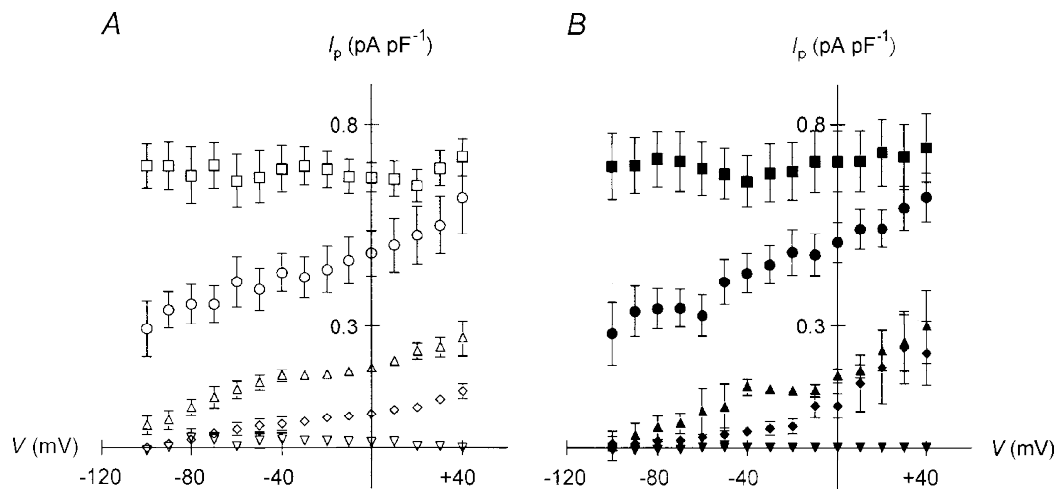
In order to investigate the possible effects of membrane voltage on cytoplasmic Na<sup>+</sup> binding to the Na<sup>+</sup>-K<sup>+</sup> pump, experimental conditions were designed to eliminate the voltage dependence of other partial reactions in the pump cycle (cf. Methods for details). Figure 1 illustrates the experimental protocol for the measurement of *I<sub>p</sub>* and the *I<sub>p</sub>*-*V* relationship. A ventricular myocyte was voltage clamped at 0 mV and internally perfused with a pipette solution containing 0.5 mM Na<sup>+</sup> and 159.5 mM NMDG<sup>+</sup>. When the holding current remained constant, the cell was subjected to 1.5 s voltage steps to potentials between +40 and -100 mV in 10 mV increments at a rate of 0.25 Hz (Fig. 1A, left panel). Afterwards, 0.1 mM ouabain was applied and the same voltage protocol was repeated in the presence of the drug (Fig. 1A, right panel). The steady-state membrane currents in the absence (□) and in the presence (■) of the cardiac glycoside are plotted as a function of clamp potential in Fig. 1B. The respective difference currents, i.e. the Na<sup>+</sup>-K<sup>+</sup> pump currents, are displayed in Fig. 1C. It is evident from these data that *I<sub>p</sub>* is voltage dependent: its amplitude is small at negative membrane

potentials and increasingly larger upon depolarization. The monotonic increase of the  $I_p$ - $V$  curve argues for only one voltage-dependent partial reaction in the pump cycle under the chosen experimental conditions (cf. De Weer *et al.* 1988). Because effects of membrane potential on extracellular ion binding are very unlikely under these conditions, intracellular  $\text{Na}^+$  binding remains a possible candidate for the voltage-dependent step. Hence, we recorded  $I_p$ - $V$

relationships at various concentrations of  $\text{Na}^+$ <sub>pip</sub>. Figure 2A summarizes data obtained with NMDG-based pipette solution containing 50 mM ( $\square$ ), 5 mM ( $\circ$ ), 2 mM ( $\triangle$ ), 0.5 mM ( $\diamond$ ) or 0 mM ( $\nabla$ )  $\text{Na}^+$ <sub>pip</sub>, respectively ( $n = 4-8$ ).  $\text{Na}^+$ - $\text{K}^+$  pump current densities are plotted *versus* membrane potential. No pump current was observed at zero  $\text{Na}^+$ <sub>pip</sub>, demonstrating that the cells were reasonably well dialysed via the patch pipette. Increasing  $[\text{Na}^+]_{\text{pip}}$  resulted in



**Figure 1.** Voltage dependence of  $\text{Na}^+$ - $\text{K}^+$  pump current activated by 0.5 mM  $\text{Na}^+$ <sub>pip</sub>. *A*, whole-cell recording from a guinea-pig ventricular myocyte. The patch pipette contained 0.5 mM  $\text{Na}^+$  and 159.5 mM NMDG<sup>+</sup> as the main cation. Current traces in response to voltage steps from zero potential to potentials between -100 and +40 mV in 10 mV increments are displayed. Left panel: control in  $\text{Na}^+$ -free solution containing 20 mM  $\text{Cs}^+$ . Right panel: currents obtained following application of 0.1 mM ouabain. Note the inward shift of the current traces after inhibition of the  $\text{Na}^+$ - $\text{K}^+$  pump by ouabain. Cell capacitance: 111 pF. *B*, steady-state membrane current ( $I_m$ )-voltage relationships from the data shown in *A*.  $\square$ , control in drug-free medium;  $\blacksquare$ , currents measured under 0.1 mM ouabain. *C*, pump current ( $I_p$ )-voltage relationship. Data represent the differences between membrane currents recorded in the absence and in the presence of ouabain (shown in *B*). Note the steep positive slope of the  $I_p$ - $V$  curve.



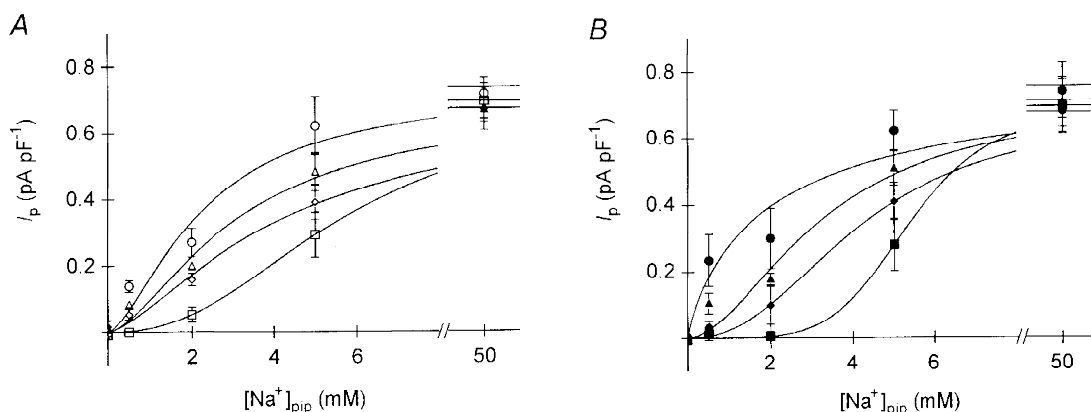
**Figure 2.**  $I_p$ - $V$  relationships at various  $[\text{Na}^+]_{\text{pip}}$

$\text{Na}^+$ - $\text{K}^+$  pump currents normalized to cell capacitance are plotted *versus* membrane potential. *A*,  $I_p$ - $V$  relationships at 0 mM ( $\nabla$ ), 0.5 mM ( $\diamond$ ), 2 mM ( $\Delta$ ), 5 mM ( $\circ$ ), and 50 mM ( $\square$ )  $\text{Na}^+$  pip in cells dialysed with NMDG<sup>+</sup>-containing pipette solution ( $n = 4-8$ ). *B*, corresponding  $I_p$ - $V$  curves for myocytes containing TEA<sup>+</sup> as the main cation ( $n = 4-7$ ). Symbols have the same meaning as in *A*. Note the absence of  $I_p$  in  $\text{Na}^+$ -free pipette solutions and the voltage dependence of  $I_p$  at low ( $\leq 5$  mM)  $\text{Na}^+$  pip. In contrast,  $I_p$  activated by 50 mM  $\text{Na}^+$  pip is voltage insensitive.

progressively larger pump currents. At low ( $\leq 5$  mM)  $[\text{Na}^+]_{\text{pip}}$   $I_p$  was voltage dependent: the pump currents were small at negative membrane potentials and increased with depolarization. The relative  $I_p$  activation was clearly stronger at more positive potentials. The voltage dependence of  $I_p$  was almost entirely abolished at 50 mM  $\text{Na}^+$  pip, a concentration saturating the internal  $\text{Na}^+$  binding sites of the cardiac  $\text{Na}^+$ - $\text{K}^+$  pump (Nakao & Gadsby, 1989). Analogous experiments with TEA<sup>+</sup>-based pipette solution produced very similar results, as shown in Fig. 2*B*

( $n = 4-7$ ; symbols have the same meaning as in Fig. 2*A*). Again, there was no  $\text{Na}^+$ - $\text{K}^+$  pump current in the absence of  $\text{Na}^+$  pip. Increasing  $[\text{Na}^+]_{\text{pip}}$  evoked increasingly larger pump currents.  $I_p$  was voltage dependent at 0.5–5 mM  $\text{Na}^+$  pip and voltage independent at 50 mM  $\text{Na}^+$  pip. Once more, the relative activation of  $I_p$  by low  $[\text{Na}^+]_{\text{pip}}$  became stronger with depolarization.

Figure 3*A* displays the activation of  $I_p$  by various  $[\text{Na}^+]_{\text{pip}}$  at +40 mV ( $\circ$ ), 0 mV ( $\Delta$ ), -50 mV ( $\diamond$ ), and -100 mV ( $\square$ )



**Figure 3.** Activation of  $I_p$  by  $[\text{Na}^+]_{\text{pip}}$  at various membrane potentials

$I_p$  activation as a function of  $[\text{Na}^+]_{\text{pip}}$  in cardiomyocytes dialysed with NMDG<sup>+</sup>-containing (*A*) or TEA<sup>+</sup>-containing (*B*) pipette solutions. Activation was measured at +40 mV (circles), 0 mV (triangles), -50 mV (diamonds), and -100 mV (squares) ( $n = 4-8$ ). The curves fitted to the data points obey the Hill equation (eqn (1)) with the following parameters (for *A* and *B*): +40 mV:  $K_{0.5} = 2.3$  and 2.1 mM  $\text{Na}^+$  pip,  $I_{p(\text{max})} = 0.75$  and 0.81 pA pF<sup>-1</sup>,  $n_H = 1.5$  and 0.8; 0 mV:  $K_{0.5} = 3.1$  and 3.3 mM  $\text{Na}^+$  pip,  $I_{p(\text{max})} = 0.68$  and 0.72 pA pF<sup>-1</sup>,  $n_H = 1.6$  and 1.8; -50 mV:  $K_{0.5} = 4.3$  and 4.2 mM  $\text{Na}^+$  pip,  $I_{p(\text{max})} = 0.70$  and 0.68 pA pF<sup>-1</sup>,  $n_H = 1.4$  and 2.3; -100 mV:  $K_{0.5} = 5.8$  and 5.4 mM  $\text{Na}^+$  pip,  $I_{p(\text{max})} = 0.70$  and 0.70 pA pF<sup>-1</sup>,  $n_H = 2.3$  and 5.2.  $r^2 = 0.984-1.000$ . Note that  $K_{0.5}$  values increase with hyperpolarization, whereas  $I_{p(\text{max})}$  remains constant.

(*n* = 4–8). The patch pipette solution contained NMDG<sup>+</sup> as the main cation. As can be seen from the figure the *I<sub>p</sub>* density increased with increasing [Na<sup>+</sup>]<sub>pip</sub>. At a distinct [Na<sup>+</sup>]<sub>pip</sub> depolarization caused a stronger activation of *I<sub>p</sub>*, except at 50 mM Na<sup>+</sup><sub>pip</sub>. The curves fitted to the data obeyed the Hill equation:

$$I_p = I_{p(max)}[Na^+]_{pip}^{n_H} / ([Na^+]_{pip}^{n_H} + K_{0.5}^{n_H}), \quad (1)$$

where *I<sub>p(max)</sub>* denotes the maximal pump current density, *K<sub>0.5</sub>* represents the [Na<sup>+</sup>]<sub>pip</sub> required for half-maximal *I<sub>p</sub>* activation (*K<sub>0.5</sub>* value), and *n<sub>H</sub>* is the Hill coefficient. *I<sub>p(max)</sub>* fluctuated between 0.68 and 0.75 pA pF<sup>-1</sup>. *n<sub>H</sub>* varied between 1.4 and 2.3 and increased with hyperpolarization. The *K<sub>0.5</sub>* value amounted to 5.8 mM Na<sup>+</sup><sub>pip</sub> at -100 mV and decreased to 2.3 mM Na<sup>+</sup><sub>pip</sub> at +40 mV. Thus, the apparent affinity of the cardiac Na<sup>+</sup>-K<sup>+</sup> pump to Na<sup>+</sup><sub>pip</sub> increases with depolarization. Figure 3*B* shows corresponding data from cells internally perfused with a solution containing TEA<sup>+</sup> as the major cation (*n* = 4–7, symbols have the same meaning as in Fig. 3*A*). Again, the *I<sub>p</sub>* density increased with larger [Na<sup>+</sup>]<sub>pip</sub> and the *I<sub>p</sub>* activation at a distinct [Na<sup>+</sup>]<sub>pip</sub> became stronger with depolarization. *I<sub>p(max)</sub>* varied between 0.68 and 0.81 pA pF<sup>-1</sup>. The Hill coefficient amounted to 0.8 at +40 mV and increased with hyperpolarization to 5.2 at -100 mV. The *K<sub>0.5</sub>* value decreased with depolarization from 5.4 mM Na<sup>+</sup><sub>pip</sub> at -100 mV to 2.1 mM Na<sup>+</sup><sub>pip</sub> at +40 mV. As in cells dialysed with NMDG<sup>+</sup>, the apparent affinity of the pump towards intracellular Na<sup>+</sup> decreased with hyperpolarization, whereas the Hill coefficient increased. The latter finding confirms earlier observations by Goldshlegger *et al.* (1987) and Or *et al.* (1996) on proteoliposomes containing Na<sup>+</sup>-K<sup>+</sup>-ATPase suggesting that the binding sites of the pump for cytosolic Na<sup>+</sup> are differently affected by the membrane potential. However, it

is likewise possible to fit the data in Fig. 3*A* or *B* by assuming a common *I<sub>p(max)</sub>* value and Hill coefficient for each series of experiments, although the fit is less good.

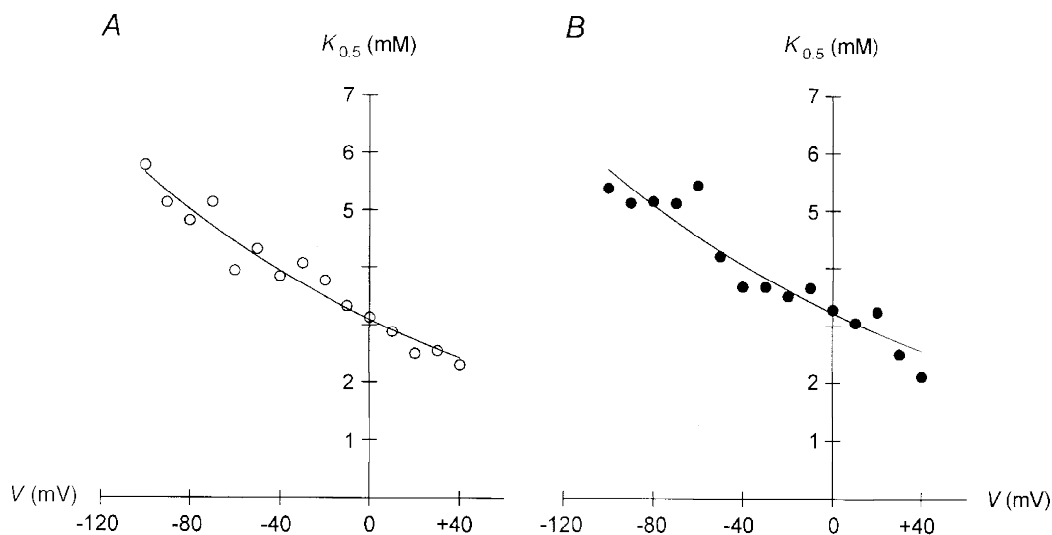
Figure 4 depicts the voltage dependence of the *K<sub>0.5</sub>* values for *I<sub>p</sub>* activation by internal Na<sup>+</sup> for myocytes containing either NMDG<sup>+</sup> (*A*) or TEA<sup>+</sup> (*B*) as the main cation. Under both conditions the *K<sub>0.5</sub>* values declined by a factor of ~2.5 with depolarization from -100 to +40 mV. Correspondingly, the apparent Na<sup>+</sup> affinity of the Na<sup>+</sup>-K<sup>+</sup> pump increased by the same factor within this range of membrane potentials. The data in Fig. 4*A* and *B* are fitted by the Boltzmann function (cf. Apell, 1989):

$$K_{0.5}(V) = K_{0.5}(V=0)\exp(-\alpha FV/RT), \quad (2)$$

where *K<sub>0.5</sub>(V)* is the *K<sub>0.5</sub>* value at the membrane potential *V* and *K<sub>0.5</sub>(V=0)* the *K<sub>0.5</sub>* value at zero potential. *F*, *R* and *T* have their usual meanings. *α* is a steepness factor and represents the fraction of an elementary charge moving through the membrane dielectric during binding/translocation of intracellular Na<sup>+</sup> ions. *α* amounted to 0.16 in myocytes internally perfused with NMDG<sup>+</sup>-containing pipette solution (Fig. 4*A*) and to 0.15 in cells dialysed with TEA<sup>+</sup>-containing medium (Fig. 4*B*). According to Sagar & Rakowski (1994) *α* is related to *δ*, the dielectric coefficient, by:

$$\alpha = n_H \delta, \quad (3)$$

where *n<sub>H</sub>* is the Hill coefficient. The dielectric coefficient indicates the mean fraction of membrane potential dissipated between the inner side of the sarcolemma and the Na<sup>+</sup> binding sites of the Na<sup>+</sup>-K<sup>+</sup> pump within the membrane. In order to calculate *δ* a mean Hill coefficient for Na<sup>+</sup> binding of 1.7 (the mean value for cells containing NMDG<sup>+</sup>) or 2.1 (the mean value for myocytes containing



**Figure 4.** *K<sub>0.5</sub>* values for *I<sub>p</sub>* activation by Na<sup>+</sup><sub>pip</sub> are voltage dependent  
*K<sub>0.5</sub>* values for activation of *I<sub>p</sub>* by Na<sup>+</sup><sub>pip</sub> in cells containing either NMDG<sup>+</sup> (*A*) or TEA<sup>+</sup> (*B*) are plotted *versus* membrane potential. In both cases *K<sub>0.5</sub>* values decrease monotonically with depolarization. The fitted curves obey a Boltzmann equation (eqn (2)) with *α* values of 0.16 for NMDG<sup>+</sup> (*A*) and 0.15 for TEA<sup>+</sup> (*B*). *r*<sup>2</sup> = 0.948 (*A*) and 0.895 (*B*).

TEA<sup>+</sup>) was used. Thus,  $\delta$  values amounted to 0.09 and 0.07 for NMDG<sup>+</sup>- and TEA<sup>+</sup>-containing cells, respectively.

## DISCUSSION

The main finding of the present study is that the apparent affinity of the cardiac Na<sup>+</sup>-K<sup>+</sup> pump towards intracellular Na<sup>+</sup> is voltage dependent. The observation is in agreement with a preliminary report by Kockskämper & Glitsch (1997) suggesting voltage-dependent binding of cytoplasmic Na<sup>+</sup> to the Na<sup>+</sup>-K<sup>+</sup> pump of cultured guinea-pig atrial myocytes. It is, however, in contrast to the conclusion drawn by Nakao & Gadsby (1989) that in Na<sup>+</sup>-free external media Na<sub>i</sub><sup>+</sup> binding to the Na<sup>+</sup>-K<sup>+</sup> pump of guinea-pig ventricular myocytes is independent of membrane potential. The discrepancy between their findings and ours might be caused by the different composition of the pipette solutions used. While Nakao & Gadsby (1989) employed Cs<sup>+</sup>-containing internal solutions, ours were devoid of any Cs<sup>+</sup> (and K<sup>+</sup>). Cs<sup>+</sup> is known to act as a K<sup>+</sup> congener. Both intracellular Cs<sup>+</sup> and K<sup>+</sup> change the kinetics of the cardiac Na<sup>+</sup>-K<sup>+</sup> pump, for instance by reducing maximal  $I_p$  (Kinard & Stimers, 1992) and by decreasing the apparent affinity to cytoplasmic Na<sup>+</sup> (Hilgemann *et al.* 1991; this work, see below). It is conceivable, therefore, that the apparent lack of voltage effects on intracellular Na<sup>+</sup> binding to the pump reported by Nakao & Gadsby (1989) may be due to the use of (varying concentrations of) cytoplasmic Cs<sup>+</sup>. Furthermore, in our opinion, the experimental data presented in their Fig. 7A and C do not exclude a weak voltage dependence of Na<sub>i</sub><sup>+</sup> binding at low [Na<sup>+</sup>]<sub>pip</sub>. Using giant membrane patches from guinea-pig ventricular myocytes and experimental conditions not directly comparable to ours (Na<sup>+</sup>-containing external media; pump currents obtained as difference currents in the presence or absence, respectively, of internal Na<sup>+</sup> or ATP), Hilgemann (1994) noted that cytoplasmic Na<sup>+</sup> binding to the pump is not strongly electrogenic. As to cell-free Na<sup>+</sup>-K<sup>+</sup>-ATPase systems, several earlier reports suggest that binding of Na<sup>+</sup> to the (internal) Na<sup>+</sup>-binding sites of the enzyme might depend on voltage (Goldshlegger *et al.* 1987; Stürmer *et al.* 1991; Heyse *et al.* 1994; Or *et al.* 1996; for further references, see Rakowski *et al.* 1997b). Most recently Pintschovius *et al.* (1999) demonstrated, by direct electrical measurements, electrogenic Na<sup>+</sup> binding on the cytoplasmic side of solid-supported membrane fragments containing pig kidney Na<sup>+</sup>-K<sup>+</sup>-ATPase.

The solutions used in the experiments described above were designed to avoid possible interference resulting from competition of K<sup>+</sup>/Cs<sup>+</sup> with Na<sup>+</sup> for internal cation binding sites of the Na<sup>+</sup>-K<sup>+</sup> pump. In addition, they guaranteed that the known voltage dependence of two steps in the pump cycle did not affect the measurements. These steps are rebinding of extracellular Na<sup>+</sup>, which affects Na<sup>+</sup> release by the pump to the exterior, and binding of extracellular K<sup>+</sup> (for further details see Rakowski *et al.* 1997a,b). In order to prevent voltage-sensitive Na<sup>+</sup> release/rebinding the

experiments were carried out in Na<sup>+</sup>-free superfusion media. In addition, the media contained 20 mM Cs<sup>+</sup> to saturate the external Cs<sup>+</sup>/K<sup>+</sup>-binding sites of the Na<sup>+</sup>-K<sup>+</sup> pump ( $K_{0.5}$  value for Cs<sub>o</sub><sup>+</sup> in Na<sup>+</sup>-free media at 0 mV  $\approx$  1.5 mM; cf. Bielen *et al.* 1993). Using these solutions  $I_p$ - $V$  curves at low [Na<sup>+</sup>]<sub>pip</sub> increased monotonically with depolarization, indicative of a single voltage-dependent step in the pump cycle (De Weer *et al.* 1988). Saturation of internal Na<sup>+</sup> binding sites at 50 mM Na<sub>pip</sub><sup>+</sup> abolished the voltage dependence of this partial reaction, suggesting that it is located in the Na<sup>+</sup> translocation limb. Furthermore, the partial reaction is supposed to occur prior to Na<sup>+</sup> release to the exterior which is voltage independent under our experimental conditions. We observed a decrease of the  $K_{0.5}$  value for  $I_p$  activation by intracellular Na<sup>+</sup> upon depolarization in the entire potential range studied, irrespective of the main internal cation used, NMDG<sup>+</sup> or TEA<sup>+</sup>. The  $K_{0.5}$  value dropped by a factor of  $\sim 2.5$  for a 140 mV depolarization. According to Läger (1991), the voltage dependence of the apparent affinity of the Na<sup>+</sup>-K<sup>+</sup> pump to cytoplasmic Na<sup>+</sup> may indicate the existence of a high-field, narrow access channel (ion well) connecting the cytosol with the pump's Na<sup>+</sup>-binding sites buried in the membrane. Thus, hyperpolarization of the sarcolemma would reduce the local [Na<sup>+</sup>] at the sites, whereas depolarization would increase local [Na<sup>+</sup>]. The calculated dielectric coefficients of 0.07–0.09 are similar to the values reported from membrane fragments and proteoliposomes containing Na<sup>+</sup>-K<sup>+</sup>-ATPase (Goldshlegger *et al.* 1987; Wuddel & Apell, 1995; Or *et al.* 1996) but lower than the corresponding numbers for Na<sub>o</sub><sup>+</sup> rebinding and K<sub>o</sub><sup>+</sup> binding to the pump (see Sagar & Rakowski, 1994). This agrees with the hypothesis that the putative ion well for internal Na<sup>+</sup> binding is shallower than those for external Na<sup>+</sup> and K<sup>+</sup> binding. However, as emphasized by Gadsby and colleagues (Gadsby *et al.* 1992; Rakowski *et al.* 1997b), voltage dependence of the apparent affinity of a transporter to a transported ion species does not prove the existence of a high-field, narrow access channel; it can also be explained by the voltage dependence of any other partial reaction in the transport cycle. Still, it seems possible to localize the voltage-dependent step observed in the present study to the Na<sup>+</sup> translocation limb of the pump cycle since there is strong evidence that the partial reactions in the K<sup>+</sup> limb subsequent to K<sub>o</sub><sup>+</sup> binding are most probably voltage independent (Goldshlegger *et al.* 1987; Bahinski *et al.* 1988; Peluffo & Berlin, 1997; see also Rakowski *et al.* 1997a). Furthermore, earlier studies on cell-free Na<sup>+</sup>-K<sup>+</sup>-ATPase systems have also shown that occlusion of internal Na<sup>+</sup> is potential independent (Apell *et al.* 1987; Borlinghaus *et al.* 1987), whereas the change from the E1 conformation to the E2 conformation of the pump is weakly voltage sensitive (Wuddel & Apell, 1995). Thus our data do not allow us to differentiate between internal Na<sup>+</sup> binding to the pump and the E1  $\rightarrow$  E2 conformational change as the reaction underlying the apparent voltage dependence of cytoplasmic Na<sup>+</sup> binding to the pump. They demonstrate, however, that

the membrane potential affects a partial reaction prior to  $\text{Na}^+$  release in the  $\text{Na}^+-\text{K}^+$  pump cycle.

There are two other points worth noting. First, the maximal  $I_p$  densities (at zero potential) measured in the present study under conditions maximally activating  $I_p$  are somewhat lower ( $\sim 0.75 \text{ pA pF}^{-1}$ ) than those reported earlier for cardiac cells ( $\geq 1 \text{ pA pF}^{-1}$ ; Gadsby *et al.* 1985; Glitsch *et al.* 1989). A possible reason is that the latter investigators used  $\text{K}^+$  or  $\text{Rb}^+$  as an equipotent external activator of the  $\text{Na}^+-\text{K}^+$  pump whereas in the experiments described above the myocytes were superfused with  $\text{Cs}^+$ -containing media. Hermans (1997, pp. 19–20) demonstrated that the maximal  $I_p$  density of guinea-pig ventricular cells declines with a decrease in the apparent affinity of the external activator cation species. Since  $\text{Cs}_o^+$  is a weaker activator than  $\text{K}_o^+$  or  $\text{Rb}_o^+$  our data are clearly in line with her observation. Second, our  $K_{0.5}$  values for  $I_p$  activation by internal  $\text{Na}^+$  are lower by a factor of 2–3 than previous estimates (e.g. Nakao & Gadsby, 1989). A possible explanation for this finding is that we used  $\text{K}^+/\text{Cs}^+$ -free pipette solutions. In contrast, most earlier investigations were conducted in the presence of intracellular  $\text{K}^+/\text{Cs}^+$ . Since intracellular  $\text{K}^+/\text{Cs}^+$  not only inhibits the forward running  $\text{Na}^+-\text{K}^+$  pump (Kinard & Stimers, 1992), but also appears to compete with  $\text{Na}^+$  for cytoplasmic binding sites (Hilgemann *et al.* 1991; Hermans, 1997, p. 121), the apparent affinity of the pump for intracellular  $\text{Na}^+$  is expected to increase in the absence of intracellular  $\text{K}^+/\text{Cs}^+$ . Our results thus underline the importance of an appropriate (ionic) composition of intra- and extracellular solutions, especially with respect to the transported cations, if one aims to investigate a distinct step in the pump cycle. In this regard it is important that the main intracellular cations used in this study, NMDG<sup>+</sup> and TEA<sup>+</sup>, do not markedly interact with the  $\text{Na}^+-\text{K}^+$  pump at cytoplasmic sites. There is evidence that TEA<sup>+</sup> weakly reduces extracellular  $\text{K}^+$  binding to the pump by inhibiting  $\text{K}^+$  entry into the access channel. However, intracellular TEA<sup>+</sup> only marginally inhibits  $I_p$  (Eckstein-Ludwig *et al.* 1998). Clearly, because of the rather large ionic diameters of both NMDG<sup>+</sup> and TEA<sup>+</sup> compared with  $\text{Na}^+$ ,  $\text{K}^+$  or  $\text{Cs}^+$ , competition between these groups of cations for binding to cytoplasmic sites of the pump appears unlikely. Furthermore, since the results presented above are almost identical for NMDG<sup>+</sup>- and TEA<sup>+</sup>-containing myocytes, both cation species, although quite different in structure, would have to exert identical effects on the  $\text{Na}^+-\text{K}^+$  pump. Thus, it seems reasonable to assume that intracellular NMDG<sup>+</sup> and TEA<sup>+</sup> do not substantially affect the pump and, consequently, are much better  $\text{K}^+$  substitutes than  $\text{Cs}^+$  for our purposes.

In conclusion, we have presented, for the first time in animal cells, conclusive evidence that cytoplasmic  $\text{Na}^+$  binding to the  $\text{Na}^+-\text{K}^+$  pump and/or a subsequent partial reaction prior to  $\text{Na}^+$  release is voltage dependent. This mechanism may be of physiological relevance for the clearance of  $\text{Na}^+$  loads during cardiac excitation.

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