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## Coligand Effects on Solution Stability, Biodistribution and Metabolism of $^{99m}\text{Tc}$ -Labeled Cyclic RGDfK Tetramer

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### Abstract

In this study, we present the evaluation of two new ternary ligand  $^{99m}\text{Tc}$  complexes [ $^{99m}\text{Tc}(\text{HYNIC-tetramer})(\text{tricine})(\text{L})$ ] (L = ISONIC and PDA) as potential radiotracers for tumor imaging. The athymic nude mice bearing the MDA-MB-435 human breast cancer xenografts were used to evaluate their biodistribution and metabolic properties. The solution stability data showed that [ $^{99m}\text{Tc}(\text{HYNIC-tetramer})(\text{tricine})(\text{L})$ ] (L = ISONIC and PDA) had a significant (14% and 35%, respectively) at 6 h in the absence of excess ISONIC or PDA coligand. Biodistribution data clearly showed that [ $^{99m}\text{Tc}(\text{HYNIC-tetramer})(\text{tricine})(\text{PDA})$ ] has much lower uptake in most organs of interest than [ $^{99m}\text{Tc}(\text{HYNIC-tetramer})(\text{tricine})(\text{ISONIC})$ ] during the 2 h study period. Results from metabolism studies revealed that ~50% of [ $^{99m}\text{Tc}(\text{HYNIC-tetramer})(\text{tricine})(\text{ISONIC})$ ] remained intact in feces samples at 120 min p.i. Only 10% of [ $^{99m}\text{Tc}(\text{HYNIC-tetramer})(\text{tricine})(\text{PDA})$ ] remained intact in feces samples. The extent of metabolism correlates well with the radiotracer solution stability. The results from this and our previous studies clearly demonstrated that coligands (TPPTS, ISONIC and PDA) have a significant impact on tumor uptake, excretion kinetics and metabolism of the  $^{99m}\text{Tc}$ -labeled cyclic RGDfK tetramer. Among the three radiotracers evaluated in this tumor-bearing animal model, [ $^{99m}\text{Tc}(\text{HYNIC-tetramer})(\text{tricine})(\text{TPPTS})$ ] remains the best with respect to blood clearance, tumor uptake, target/background ratios.

### INTRODUCTION

Angiogenesis depends on vascular endothelial cell migration and invasion, is regulated by cell adhesion receptors [1-4]. Integrins are such a family of proteins that facilitate cellular adhesion to and migration on extracellular matrix proteins found in intercellular spaces and basement membranes, and regulate cellular entry and withdraw from the cell cycle [5-8]. Integrin  $\alpha_v\beta_3$  is a receptor for the extracellular matrix proteins with exposed arginine-glycine-aspartic (RGD) tripeptide sequence [6-10]. Integrin  $\alpha_v\beta_3$  is normally expressed at low levels on epithelial cells and mature endothelial cells; but it is highly expressed on the activated endothelial cells in neovasculature of tumors, including osteosarcomas, glioblastomas, melanomas, lung carcinomas, and breast cancer [5,11-18]. It has demonstrated that integrin  $\alpha_v\beta_3$  is overexpressed on both endothelial and tumor cells in human breast cancer xenografts [19]. It was also reported that the integrin  $\alpha_v\beta_3$  expression correlates well with tumor progression and invasiveness of melanoma, glioma, ovarian and breast cancers [8-18]. The highly restricted expression of integrin  $\alpha_v\beta_3$  during tumor growth, invasion and metastasis present an interesting molecular target for early detection of rapidly growing and metastatic tumors [19-23]. The nuclear medicine applications of radiolabeled integrin  $\alpha_v\beta_3$  antagonists for imaging tumors by single photon emission computed tomography (SPECT) or positron emission tomography (PET) has been reviewed extensively [23-26].

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We and others have been using multimeric cyclic RGD peptides to develop the integrin  $\alpha_v\beta_3$ -targeted radiotracers to image rapidly growing and metastatic tumors in several tumor-bearing animal models [27-39]. The RGD peptides serve as the targeting biomolecules to carry radionuclide (e.g.  $^{99m}\text{Tc}$ ,  $^{111}\text{In}$  and  $^{64}\text{Cu}$ ) to the integrin  $\alpha_v\beta_3$  overexpressed on both tumor cells and endothelial cells of tumor neovasculature. Recently, we reported the  $^{111}\text{In}$ - and  $^{64}\text{Cu}$ -labeled cyclic RGDfK tetramer as radiotracers for SPECT and PET imaging of integrin  $\alpha_v\beta_3$  expression in tumors [33,37]. Results from *in vitro* assays showed that the tetramer had higher integrin  $\alpha_v\beta_3$  binding affinity than the dimer. As a result,  $^{111}\text{In}(\text{DOTA-tetramer})$  and  $^{64}\text{Cu}(\text{DOTA-tetramer})$  (DOTA = 1,4,7,10-tetraazacyclododecane-1,4,7,10-tetraacetic acid) both have high tumor uptake with long tumor retention [33,37]. The tetramer,  $\text{E}\{\text{E}[\text{c}(\text{RGDfK})]_2\}_2$ , is a much better targeting biomolecule than the dimer,  $\text{E}[\text{c}(\text{RGDfK})]_2$ , with respect to the tumor uptake and T/B ratios of their radiotracers [28].

Previously, we reported the evaluation of [ $^{99m}\text{Tc}(\text{HYNIC-tetramer})(\text{tricine})(\text{TPPTS})$ ] (TPPTS = trisodium triphenylphosphine-3,3',3''-trisulfonate) as a new radiotracer for tumor imaging [30]. We found that [ $^{99m}\text{Tc}(\text{HYNIC-tetramer})(\text{tricine})(\text{TPPTS})$ ] had a high tumor uptake with long tumor retention ( $5.60\pm 0.87\%$  ID/g and  $7.30\pm 1.32\%$  ID/g at 5 and 120 min postinjection (p.i.), respectively). SPECT images displayed significant localization in tumor as early as 60 min p.i. The combination of high tumor uptake and fast renal excretion suggests that [ $^{99m}\text{Tc}(\text{HYNIC-tetramer})(\text{tricine})(\text{TPPTS})$ ] is a promising radiotracer for non-invasive imaging of integrin  $\alpha_v\beta_3$ -positive tumors. Since our previous studies have shown that the coligand has a significant impact on biological properties of [ $^{99m}\text{Tc}(\text{HYNIC-dimer})(\text{tricine})(\text{L})$ ] (L = TPPTS, ISONIC and PDA) [28], we decided to explore the impact of coligands on solution stability and biological properties of the  $^{99m}\text{Tc}$ -labeled cyclic RGDfK tetramer.

As an extension of our continuing interest in the  $^{99m}\text{Tc}$ -labeled cyclic RGD peptides as SPECT radiotracers for tumor imaging, we now present the synthesis and evaluation of two new ternary ligand  $^{99m}\text{Tc}$  complexes [ $^{99m}\text{Tc}(\text{HYNIC-tetramer})(\text{tricine})(\text{L})$ ] (L = ISONIC and PDA). The athymic nude mice bearing MDA-MB-435 human breast cancer xenografts were used to evaluate their biological properties. Results from these studies will allow us to compare their biodistribution characteristics (tumor uptake, T/B ratios, excretion kinetics and metabolic stability) with those of [ $^{99m}\text{Tc}(\text{HYNIC-tetramer})(\text{tricine})(\text{TPPTS})$ ] [30].

## EXPERIMENTAL SECTION

### Materials

Isonicotinic acid (ISONIC), 1,5-pyridinedicarboxylic acid (PDA), and tricine were purchased from *Sigma/Aldrich*. Pentapeptide c(RGDfK) was purchased from Peptides International, Inc. (Louisville, Kentucky). HYNIC-E{E[c(RGDfK)]<sub>2</sub>}<sub>2</sub> (HYNIC-tetramer) and [ $^{99m}\text{Tc}(\text{HYNIC-tetramer})(\text{tricine})(\text{TPPTS})$ ] were prepared according to procedures described in our previous report [30].  $\text{Na}^{99m}\text{TcO}_4$  was obtained from a commercial DuPont Pharma  $^{99}\text{Mo}/^{99m}\text{Tc}$  generator, N. Billerica, MA.

### Instruments and Methods

The radio-HPLC method used a LabAlliance HPLC system equipped with a  $\beta$ -ram IN-US detector and Zorbax Rx-C<sub>18</sub> column (4.6 mm  $\times$  250 mm, 300 Å pore size). The flow rate was 1 mL/min. The mobile phase was isocratic with 90% solvent A (25 mM ammonium acetate buffer, pH = 5.0) and 10% solvent B (acetonitrile) at 0 – 2 min, followed by a gradient mobile phase going from 10% solvent B at 2 min to 15% solvent B at 5 min and to 20% solvent B at 20 min. The ITLC method used Gelman Sciences silica-gel paper strips and a 1:1 mixture of acetone and saline as the eluent. Using this method, the radiotracer and  $\text{Na}^{99m}\text{TcO}_4$  migrate to the solvent front and the [ $^{99m}\text{Tc}$ ]colloid remains at the origin.

### **[<sup>99m</sup>Tc(HYNIC-tetramer)(tricine)(ISONIC)]**

To a clean vial were added 1.0 mL of solution containing 10 mg of ISONIC, 20 mg of tricine, 40 mg of mannitol, 38.5 mg of disodium succinate hexahydrate, and 12.7 mg of succinic acid, were added 0.2 mL of the HYNIC-tetramer solution (100 µg/mL in water), 0.3 mL of Na [<sup>99m</sup>TcO<sub>4</sub>] solution (110 – 220 MBq/mL), and 30 µL SnCl<sub>2</sub> solution (1 mg/mL in 1.0 N HCl). The vial was heated at 100 °C for 15 – 20 min in a lead-shielded water bath. After heating, the vial was placed back into the lead pig, and allowed to stand at room temperature for ~10 min. A sample of the resulting solution was analyzed by radio-HPLC and TLC. The percentage of [<sup>99m</sup>Tc]colloid was minimal (<1%). The RCP was >90%. The HPLC retention time was ~14.5 min.

### **[<sup>99m</sup>Tc(HYNIC-tetramer)(tricine)(PDA)]**

To a clean vial were added 1.0 mL of solution containing 15 mg of PDA, 20 mg of tricine, 40 mg of mannitol, 38.5 mg of disodium succinate hexahydrate, and 12.7 mg of succinic acid, were added 0.2 mL of the HYNIC-tetramer solution (100 µg/mL in water) 0.3 mL of Na [<sup>99m</sup>TcO<sub>4</sub>] solution (110 – 220 MBq/mL), and 25 – 30 µL SnCl<sub>2</sub> solution (1 mg/mL in 1.0 N HCl). The vial was sealed and heated at 100 °C for 15 min. After cooling to room temperature, a sample of the resulting solution was analyzed by radio-HPLC and TLC. The RCP was >90%. The HPLC retention time was ~14.0 min.

### **Doses Preparation**

For biodistribution studies, [<sup>99m</sup>Tc(HYNIC-tetramer)(tricine)(L)] (L = ISONIC and PDA) were prepared, and then were purified by radio-HPLC. Volatiles in the HPLC mobile phase were completely removed under the reduced pressure. Doses were prepared by dissolving the purified radiotracer in saline to give a concentration of ~0.37 MBq/mL. The resulting solution was filtered with a 0.20 µm Millex-LG filter to remove any particles before being injected into animals. Each tumor-bearing mouse was injected with 0.1 mL of the dose.

### **Solution Stability**

For solution stability in kit matrix, samples of the reaction mixture containing the radiotracer were analyzed by HPLC at 0, 2, 4, and 6 h post-labeling. For cysteine challenging experiment, the solution containing the radiotracer was mixed with an equal volume of a cysteine solution (1 mg/mL). Samples were analyzed by radio-HPLC at 0, 2, 4, and 6 h. For solution stability after HPLC purification, the radiotracer was separated from reaction mixture. Volatiles were removed under reduced pressure. The residue was dissolved in saline. Samples of the resulting solution were analyzed by HPLC at 0, 2, 4, and 6 h post-labeling.

### **Determination of Log P Values**

The radiotracer was prepared and purified by HPLC. Volatiles were removed completely under vacuum. The residue was dissolved in a mixture of equal volume (3 mL:3 mL) n-octanol and 25 mM phosphate buffer (pH = 7.4). After stirring vigorously for ~20 min, the mixture was centrifuged at a speed of 8,000 rpm for 5 min. Samples (in triplets) from both n-octanol and aqueous layers were counted in a gamma counter (Perkin Elmer Wizard – 1480). The partition coefficients were calculated. The log P value was measured three different times and reported as an average of three different measurements plus the standard deviation.

### **Animal Studies**

Biodistribution, imaging and metabolism studies were performed using athymic nude mice bearing MDA-MB-435 human breast cancer xenografts in compliance NIH animal experiment guidelines (*Principles of Laboratory Animal Care*, NIH Publication No. 86-23, revised 1985).

The animal protocols were approved by the Purdue University Animal Care and Use Committee (PACUC) for biodistribution and metabolism studies.

### Tumor-Bearing Mice

Female athymic nu/nu mice (4 – 5 weeks) were purchased from Harlan (Indianapolis, IN). The mice were implanted with  $5 \times 10^6$  cells of MDA-MB-435 estrogen receptor-negative human breast cancer cells into the mammary fat pad. Tumor cells were grown at 37 °C in Minimal Essential Medium (Alpha Modification) containing 3.7 g of sodium bicarbonate/L, 10% fetal bovine serum v/v, in a humidified atmosphere of 5% carbon dioxide. Four weeks after implantation, animals with tumors in the range of 0.3 – 0.5 g were used for biodistribution studies.

### Biodistribution Studies

Sixteen tumor-bearing mice (20 – 25 g) were anesthetized by IP injection of Ketamine (40 – 100 mg/kg) and Xylazine (2 – 5 mg/kg). Once the animal was in surgical plane of anesthesia, the radiotracer (~37 Bq) in saline was administered via tail vein. Four tumor-bearing mice were sacrificed by sodium pentobarbital overdose (150 – 200 mg/kg, IP) at 5, 30, 60 and 120 min p.i. Blood was withdrawn from heart through a syringe. Organs of interest (tumor, brain, eyes, heart, intestine, kidneys, liver, lungs, muscle and spleen) were excised, weighed, and counted on a gamma-counter (Perkin Elmer Wizard – 1480). The organ uptake was calculated as a percentage of the injected dose per gram of wet tissue (%ID/g).

### Metabolism

Each tumor-bearing mouse was administered with the radiotracer at a dose of ~3.7 MBq/mice. Urine samples were collected at 2 h p.i. by manual void, and were mixed with equal volume of acetonitrile. The mixture was centrifuged at 8,000 rpm. The supernatant was collected and filtered through a 0.20 micron Millex-LG syringe driven filter unit. The filtrate was analyzed by radio-HPLC. Feces samples were collected at ~120 min p.i. The sample was suspended in a mixture of 50% acetonitrile aqueous solution, and the mixture was vortexed for 5 – 10 min. After centrifuging at 8,000 rpm for 5 min, the supernatant was collected and passed through a 0.20 micron Millex-LG syringe driven filter unit. The filtrate was analyzed by radio-HPLC. Two tumor-bearing mice were used for the metabolism study of each radiotracer.

### Imaging Studies

Planar imaging studies on [ $^{99m}\text{Tc}$ (HYNIC-tetramer)(tricine)(ISONIC)] were performed using the athymic nude mice bearing MDA-MB-435 human breast cancer xenografts. Two tumor-bearing mice (20 – 25 g) were anesthetized by IP injection of Ketamine (40 – 100 mg/kg) and Xylazine (2 – 5 mg/kg). Once the animal was in surgical plane of anesthesia, the radiotracer (~3.7 MBq) in saline was administered via tail vein. Animals were monitored on the gamma camera (PhoGama large field-of-view Anger camera and NucLearMac computer system). Sequential anterior images were collected for 5 min at the specified time (5, 15, 30, 45, 60, 90 and 120 min) using the 256 × 256 image matrix while animals remained under anesthesia. Upon completion of the experiment, the tumor-bearing mice were sacrificed by sodium pentobarbital overdose (150 – 200 mg/kg).

### Data and Statistical Analysis

The biodistribution data and T/B ratios are reported as an average plus the standard variation based on the results from four animals for each time point. Comparison between two different radiotracers was also made using the one-way ANOVA test. The level of significance was set at  $p < 0.05$ .

## RESULTS

### Radiochemistry

Ternary ligand  $^{99m}\text{Tc}$  complexes [ $^{99m}\text{Tc}(\text{HYNIC-tetramer})(\text{tricine})(\text{L})$ ] (L = ISONIC and PDA) were prepared using tricine/ISONIC and tricine/PDA as coligands. Since stannous chloride was used as the reducing agent for the radiolabeling, a large excess of tricine ( $\geq 20$  mg/vial) is needed to prevent formation of [ $^{99m}\text{Tc}$ ]colloid. The radiochemical purity of [ $^{99m}\text{Tc}(\text{HYNIC-tetramer})(\text{tricine})(\text{L})$ ] (L = ISONIC and PDA) was  $>90\%$  with minimal amount ( $<0.5\%$ ) of [ $^{99m}\text{Tc}$ ]colloid. Their log P values in a mixture of n-octanol and 25 mM phosphate buffer (pH = 7.4) were  $-3.17 \pm 0.12$  and  $-3.10 \pm 0.15$ , respectively. Figure 2 shows the HPLC chromatograms of [ $^{99m}\text{Tc}(\text{HYNIC-tetramer})(\text{tricine})(\text{L})$ ] (L = ISONIC and PDA), and the comparison of their solution stability data with that of [ $^{99m}\text{Tc}(\text{HYNIC-tetramer})(\text{tricine})(\text{TPPTS})$ ] after purification. The HPLC retention times of [ $^{99m}\text{Tc}(\text{HYNIC-tetramer})(\text{tricine})(\text{L})$ ] (L = ISONIC and PDA) were almost identical (14.0 – 14.5 min). Both remained stable in the kit matrix for  $>12$  h. They had a significant decomposition (14% and 35%, respectively) at 6 h after HPLC-purification while [ $^{99m}\text{Tc}(\text{HYNIC-tetramer})(\text{tricine})(\text{TPPTS})$ ] remains stable for  $>6$  h after purification. Apparently, coligands have a significant impact on solution stability of the  $^{99m}\text{Tc}$ -labeled cyclic RGDfK tetramer.

The solution structure of [ $^{99m}\text{Tc}(\text{HYNIC-tetramer})(\text{tricine})(\text{L})$ ] (L = ISONIC and PDA) at the tracer level remains unknown. For the last decade, we have been using ternary ligand systems (HYNIC, tricine, water soluble phosphine or pyridine analog) for  $^{99m}\text{Tc}$ -labeling of small biomolecules, including chemotactic peptides [40] and  $\text{LTB}_4$  antagonists [41,42] for imaging infection/inflammation, integrin  $\alpha_v\beta_3$  antagonists for tumor imaging [27-30], and a GPIIb/IIIa antagonist for imaging thrombosis [43-46]. Regardless of the biomolecule, the Tc:HYNIC:L:tricine ratio in [ $^{99m}\text{Tc}(\text{HYNIC-biomolecule})(\text{tricine})(\text{L})$ ] always remains 1:1:1:1 as demonstrated via mixed ligand experiments at the tracer level [43,44], and has been further confirmed by the LC-MS data of [ $^{99m}\text{Tc}(\text{HYNIC-biomolecule})(\text{tricine})(\text{L})$ ] (L = TPPTS and ISONIC) at both macroscopic and tracer levels [47,48]. Based these results, it is reasonable to believe that ternary ligand complexes [ $^{99m}\text{Tc}(\text{HYNIC-tetramer})(\text{tricine})(\text{L})$ ] (L = ISONIC and PDA) contain one HYNIC-tetramer, one tricine, and one monodentate ISONIC or PDA. This conclusion is also supported by the coligand effect observed in this and our previous studies [28]. The HYNIC technology and its utility in the development of target-specific radiopharmaceuticals have been reviewed extensively [49-52].

### Biodistribution Characteristics

[ $^{99m}\text{Tc}(\text{HYNIC-tetramer})(\text{tricine})(\text{L})$ ] (L = ISONIC and PDA) were purified by HPLC for biodistribution studies to remove the “unlabeled” HYNIC-tetramer. HPLC purification is needed to study their intrinsic capability to localize in tumor. Biodistribution data for [ $^{99m}\text{Tc}(\text{HYNIC-tetramer})(\text{tricine})(\text{L})$ ] (L = ISONIC, and PDA) are summarized in Tables 1 and 2. The organ uptake is expressed %ID/g. Each data point represents an average of biodistribution data in four tumor-bearing mice.

Figure 3 illustrates the direct comparison of organ uptake and excretion kinetics of [ $^{99m}\text{Tc}(\text{HYNIC-tetramer})(\text{tricine})(\text{L})$ ] (L = TPPTS, ISONIC, and PDA) in tumor, blood, kidneys, liver, lungs and muscle. The biodistribution data for [ $^{99m}\text{Tc}(\text{HYNIC-tetramer})(\text{tricine})(\text{TPPTS})$ ] are obtained in the same tumor-bearing animal model from our previous study [30]. In general, [ $^{99m}\text{Tc}(\text{HYNIC-tetramer})(\text{tricine})(\text{PDA})$ ] had lower uptake in most organs of interest. Both radiotracers had a rapid clearance via renal and hepatobiliary routes. Their blood clearance curves were similar even though [ $^{99m}\text{Tc}(\text{HYNIC-tetramer})(\text{tricine})(\text{ISONIC})$ ] had a higher initial blood activity ( $7.40 \pm 0.41$  %ID/g). [ $^{99m}\text{Tc}(\text{HYNIC-tetramer})(\text{tricine})(\text{ISONIC})$ ] had the tumor uptake comparable to that of [ $^{99m}\text{Tc}(\text{HYNIC-tetramer})(\text{tricine})(\text{TPPTS})$ ] at 5 –

60 min p.i. The initial kidney uptake of [ $^{99m}\text{Tc}(\text{HYNIC-tetramer})(\text{tricine})(\text{ISONIC})$ ] ( $53.81 \pm 17.33$  %ID/g at 5 min p.i.) was much higher than that of [ $^{99m}\text{Tc}(\text{HYNIC-tetramer})(\text{tricine})(\text{TPPTS})$ ] ( $33.05 \pm 5.75$  %ID/g) [30], but this difference disappeared between 30 and 120 min p.i. A similar trend was also observed for [ $^{99m}\text{Tc}(\text{HYNIC-tetramer})(\text{tricine})(\text{ISONIC})$ ] in liver and lungs (Figure 3).

Figure 4 shows T/B ratios of [ $^{99m}\text{Tc}(\text{HYNIC-tetramer})(\text{tricine})(\text{L})$ ] (L = TPPTS, ISONIC and PDA). The T/B ratios of [ $^{99m}\text{Tc}(\text{HYNIC-tetramer})(\text{tricine})(\text{TPPTS})$ ] are obtained from our previous study [30]. Even though [ $^{99m}\text{Tc}(\text{HYNIC-tetramer})(\text{tricine})(\text{ISONIC})$ ] had a higher tumor uptake than [ $^{99m}\text{Tc}(\text{HYNIC-tetramer})(\text{tricine})(\text{PDA})$ ], their T/B ratios were well within experimental error, likely due to the high uptake of [ $^{99m}\text{Tc}(\text{HYNIC-tetramer})(\text{tricine})(\text{ISONIC})$ ] in non-tumor organs (Figure 3). Among the three radiotracers evaluated in this specific tumor-bearing animal model, [ $^{99m}\text{Tc}(\text{HYNIC-tetramer})(\text{tricine})(\text{TPPTS})$ ] has the best tumor/liver, tumor/lung and tumor/muscle ratios (Figure 4).

### Metabolism

We performed metabolism studies on [ $^{99m}\text{Tc}(\text{HYNIC-tetramer})(\text{tricine})(\text{L})$ ] (L = ISONIC and PDA) using the tumor-bearing mice. Figure 5 shows representative radio-HPLC chromatograms of [ $^{99m}\text{Tc}(\text{HYNIC-tetramer})(\text{tricine})(\text{L})$ ] (L = ISONIC and PDA) in the kit matrix before injection, urine and feces at 120 min p.i. About 35% metabolite(s) from [ $^{99m}\text{Tc}(\text{HYNIC-tetramer})(\text{tricine})(\text{ISONIC})$ ] was detected in the urine sample and more than 50% metabolism was observed in the feces samples at 120 min p.i. (Figure 5). For [ $^{99m}\text{Tc}(\text{HYNIC-tetramer})(\text{tricine})(\text{PDA})$ ], however, about 40% remained intact in urine samples and only ~10% of it remained intact in feces samples at 120 min p.i. Apparently, both radiotracers underwent extensive metabolism, and the extent of metabolism seems to correlate well with their solution stability after HPLC purification.

### Planar Imaging

Figure 6 illustrates planar images of the tumor-bearing mouse administered with ~3.7 MBq of [ $^{99m}\text{Tc}(\text{HYNIC-tetramer})(\text{tricine})(\text{ISONIC})$ ] at 30 and 120 min p.i. The breast tumor is clearly visualized as early as 30 min p.i. The activity level in the abdominal region was low at 120 min p.i., which agreed well with the ex vivo biodistribution data at the same time point (Figure 3). However, the image quality is not as good as that in the tumor-bearing mouse administered with [ $^{99m}\text{Tc}(\text{HYNIC-tetramer})(\text{tricine})(\text{TPPTS})$ ] [30].

## DISCUSSION

The *in vivo* biodistribution patterns of a radiotracer is determined by several factors, including binding affinity of the targeting biomolecule (cyclic RGDfK tetramer versus dimer), metal chelate and coligands, molecular weight and charge, and lipophilicity [26]. In this study, we found that coligands have a significant impact on solution stability, biodistribution and metabolic characteristics of the  $^{99m}\text{Tc}$ -labeled cyclic RGDfK tetramer. When ISONIC and PDA are used as coligands, their  $^{99m}\text{Tc}$  complexes, [ $^{99m}\text{Tc}(\text{HYNIC-tetramer})(\text{tricine})(\text{ISONIC})$ ] and [ $^{99m}\text{Tc}(\text{HYNIC-tetramer})(\text{tricine})(\text{PDA})$ ], show 14% and 35% decomposition, respectively, at 6 h after HPLC purification (Figure 2). When TPPTS is used as the coligand, [ $^{99m}\text{Tc}(\text{HYNIC-tetramer})(\text{tricine})(\text{TPPTS})$ ] remains stable for >6 h. We believe that the coligand effect on solution stability of the  $^{99m}\text{Tc}$ -labeled RGDfK tetramer is most likely caused by lower electron-donating capability of pyridine-N in ISONIC and PDA as compared to that of TPPTS.

Coligands also have a significant impact on biodistribution and excretion kinetics of the  $^{99m}\text{Tc}$ -labeled cyclic RGDfK tetramer. For example, [ $^{99m}\text{Tc}(\text{HYNIC-tetramer})(\text{tricine})$ ]

(PDA)] has much lower uptake than [ $^{99m}\text{Tc}(\text{HYNIC-tetramer})(\text{tricine})(\text{ISONIC})$ ] in most organs of interest while the uptake of [ $^{99m}\text{Tc}(\text{HYNIC-tetramer})(\text{tricine})(\text{ISONIC})$ ] is similar to that of [ $^{99m}\text{Tc}(\text{HYNIC-tetramer})(\text{tricine})(\text{TPPTS})$ ] at 5 – 60 min p.i. Since all three radiotracers share the same cyclic RGDfK tetramer, the difference in their biodistribution characteristics is most likely related to their difference in solution stability.

In our previous study, we found that 85% of [ $^{99m}\text{Tc}(\text{HYNIC-tetramer})(\text{tricine})(\text{TPPTS})$ ] remains intact in the feces sample at 120 min p.i. [30]. In this study, >50% of [ $^{99m}\text{Tc}(\text{HYNIC-tetramer})(\text{tricine})(\text{ISONIC})$ ] exists as its metabolized form in feces samples at 120 min p.i. while only ~10% of [ $^{99m}\text{Tc}(\text{HYNIC-tetramer})(\text{tricine})(\text{PDA})$ ] remains intact in feces samples at 120 min p.i. The solution and metabolic stabilities of [ $^{99m}\text{Tc}(\text{HYNIC-tetramer})(\text{tricine})(\text{ISONIC})$ ] are between those of [ $^{99m}\text{Tc}(\text{HYNIC-tetramer})(\text{tricine})(\text{TPPTS})$ ] and [ $^{99m}\text{Tc}(\text{HYNIC-tetramer})(\text{tricine})(\text{PDA})$ ]. This correlates well with the order of electron-donating capability: TPPTS > ISONIC > PDA. The coligand effect has been reported for the  $^{99m}\text{Tc}$ -labeled chemotactic peptides [53,54], glycoprotein IIB/IIIa receptor antagonist [46], somatostatin analogs [55,56], interleukin-8 [57], and cholecystokinin (CCK8) peptides [58].

It is important to note that the coligand effect depends largely on the targeting biomolecule. For the  $^{99m}\text{Tc}$ -labeled HYNIC-IL-8 conjugate, the use of TPPTS results in the reduced receptor binding affinity, low abscess uptake, and high liver uptake [57]. Nicotinic acid and ISONIC are the best coligands for  $^{99m}\text{Tc}$ -labeled HYNIC-IL-8 and CCK8 peptides [58]. For the  $^{99m}\text{Tc}$ -labeled cyclic RGDfK dimer, changing coligand had a minimal effect on their tumor-targeting capability [28]. For the  $^{99m}\text{Tc}$ -labeled cyclic RGDfK tetramer, TPPTS has the advantage over ISONIC and PDA due to the high solution stability, high tumor uptake, high tumor/liver and tumor/lung ratios of [ $^{99m}\text{Tc}(\text{HYNIC-tetramer})(\text{tricine})(\text{TPPTS})$ ] [30].

## CONCLUSION

In conclusion, we evaluated the impact of coligands on solution stability, biodistribution and metabolic characteristics of the  $^{99m}\text{Tc}$ -labeled cyclic RGDfK tetramer using athymic nude mice bearing MDA-MB-435 breast cancer xenografts. On the basis of this and our previous studies, we believe that TPPTS is a better coligand than ISONIC or PDA due to high solution stability and favorable biological characteristics of [ $^{99m}\text{Tc}(\text{HYNIC-tetramer})(\text{tricine})(\text{TPPTS})$ ]. However, the choice of coligand for the  $^{99m}\text{Tc}$ -labeling of other HYNIC-conjugated biomolecules should be confirmed according to their biodistribution characteristics.

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## ABBREVIATIONS

### HYNIC-tetramer

[2-[[[5-[carbonyl]-2-pyridinyl]hydrazono]methyl]benzenesulfonic acid]-Glu {Glu[cyclo(Lys-Arg-Gly-Asp-D-Phe)]-cyclo(Lys-Arg-Gly-Asp-D-Phe)}- {Glu [cyclo(Lys-Arg-Gly-Asp-D-Phe)]-cyclo(Lys-Arg-Gly-Asp-D-Phe)}

### TPPTS

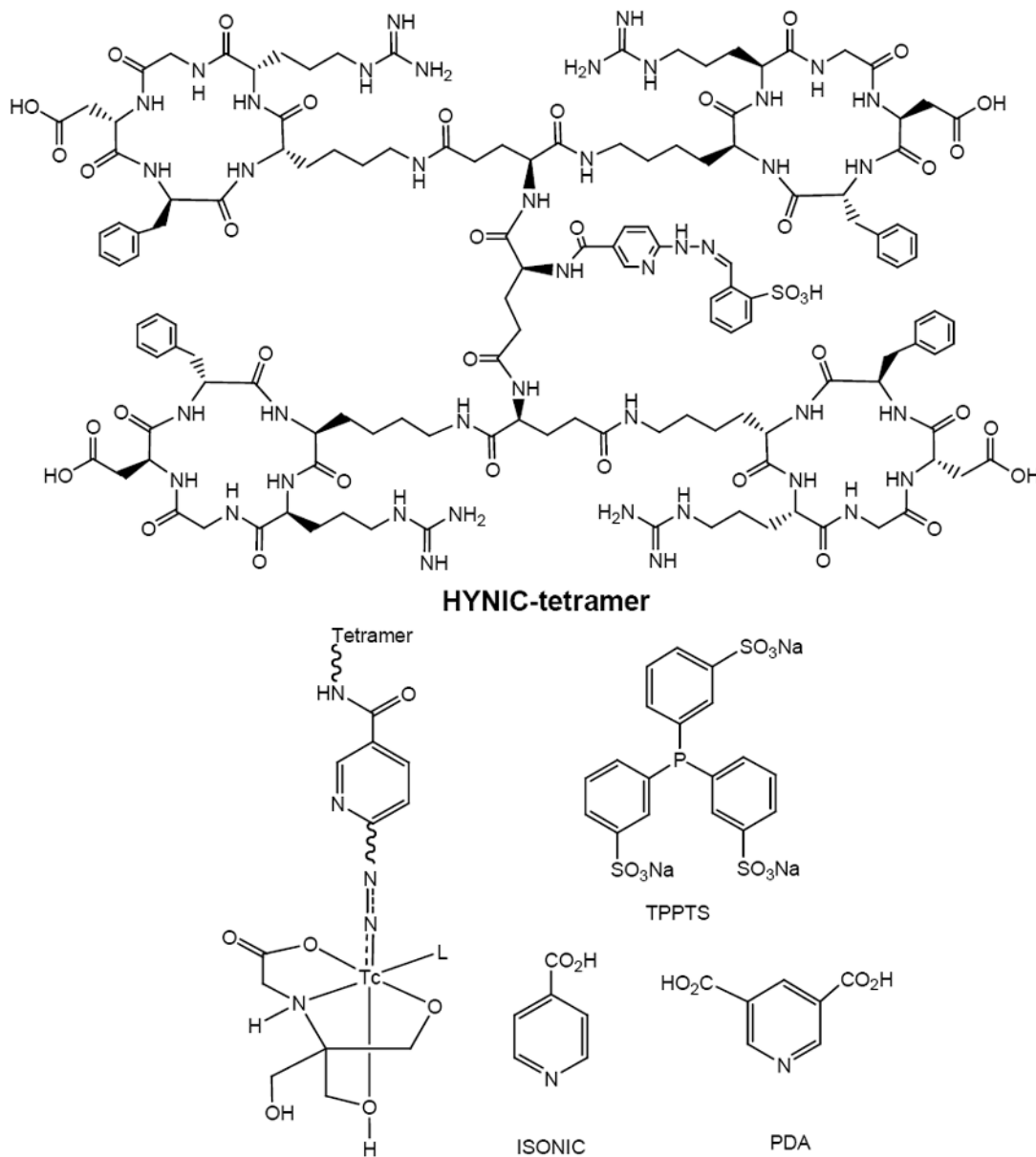
trisodium triphenylphosphine-3,3',3''-trisulfonate

### ISONIC

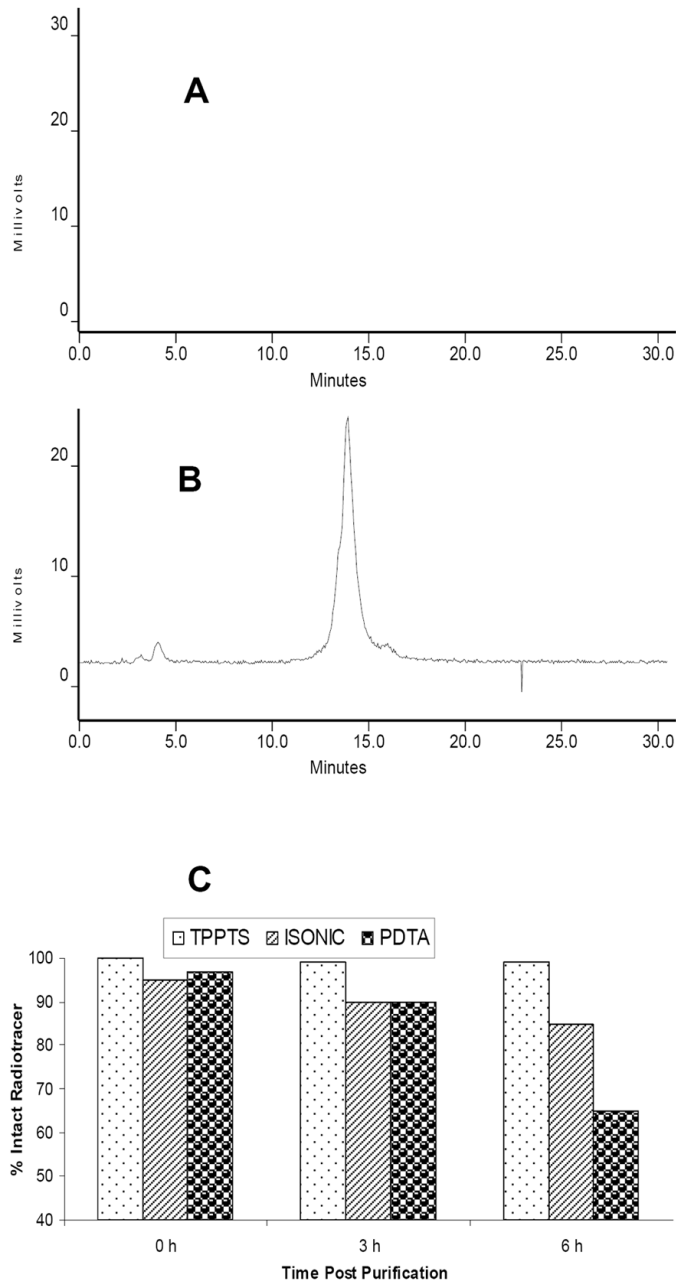
isonicotinic acid

### PDA

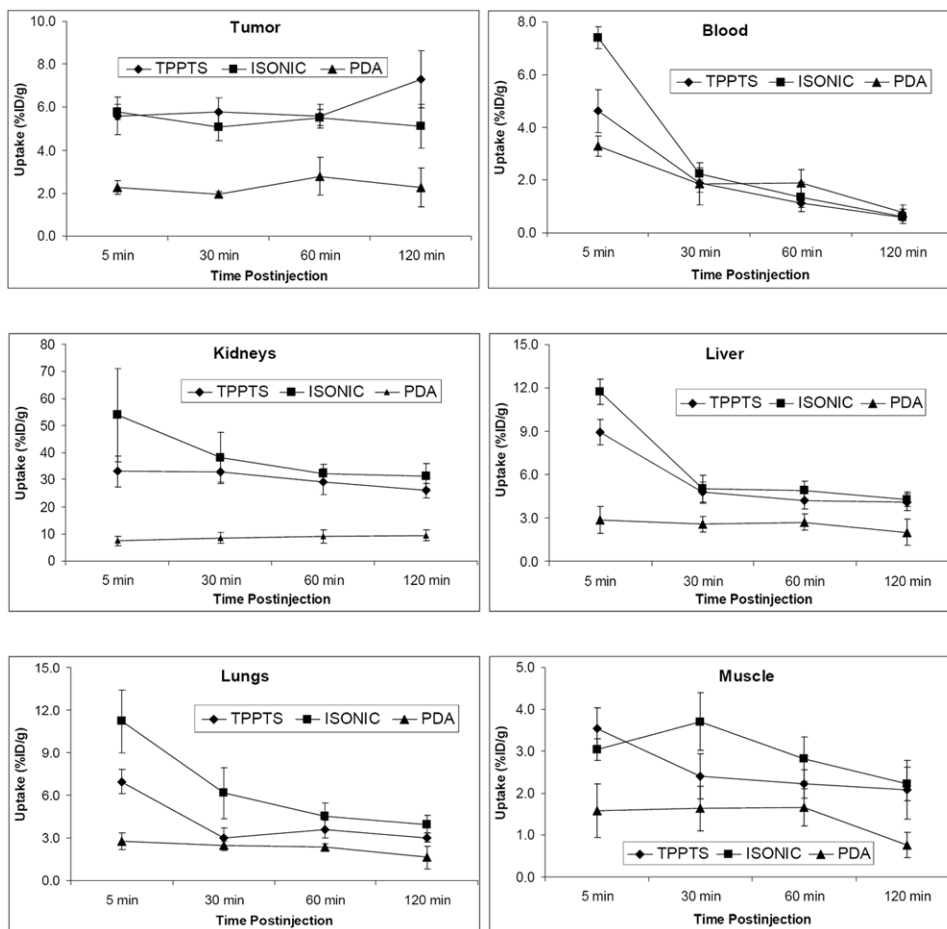
2,5-pyridinedicarboxylic acid



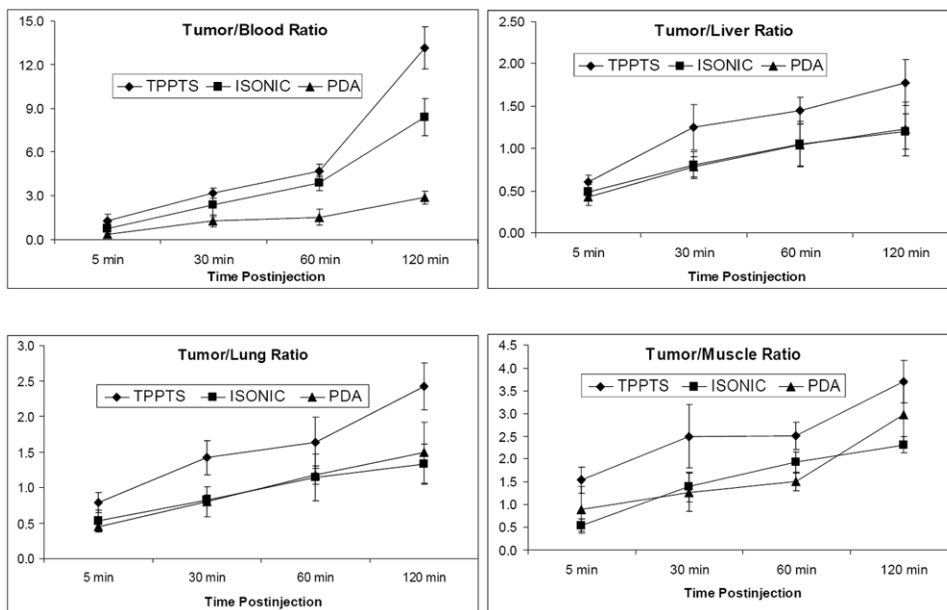
**Figure 1.** Structures of HYNIC-tetramer and its ternary ligand complexes [ $^{99\text{m}}\text{Tc}(\text{HYNIC-tetramer})(\text{tricine})(\text{L})$ ] (L = TPPTS, ISONIC and PDA).



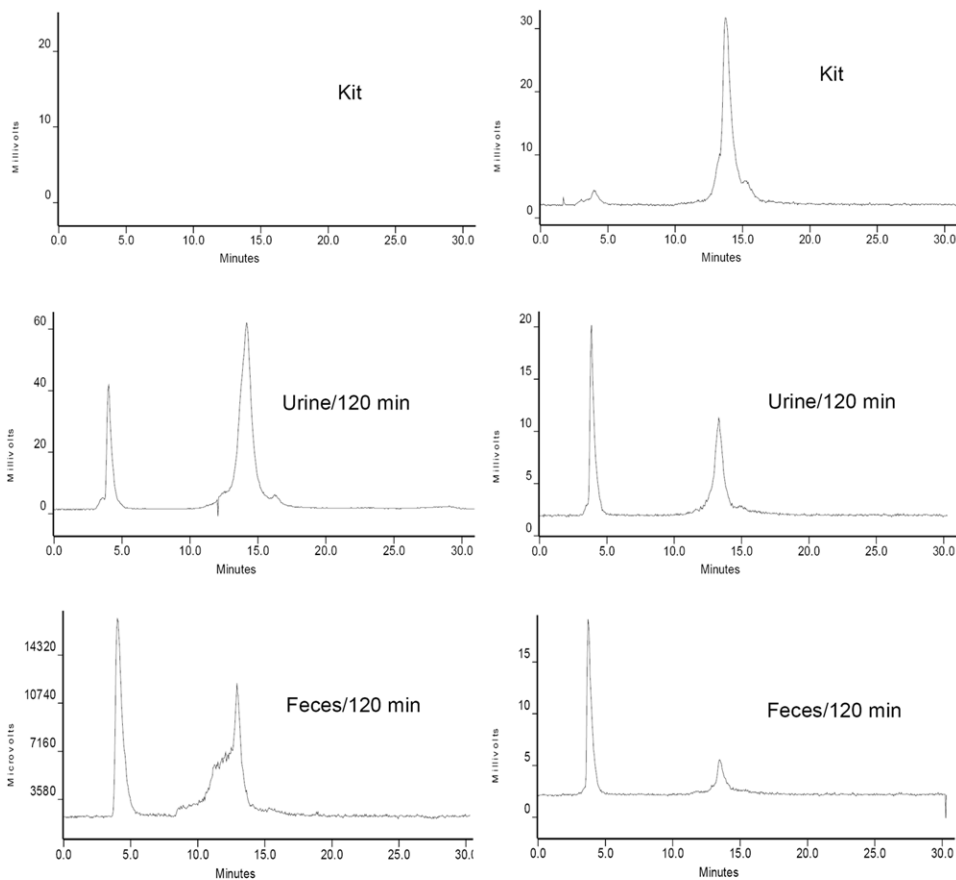
**Figure 2.** Typical radio-HPLC chromatograms of  $[^{99m}\text{Tc}(\text{HYNIC-tetramer})(\text{tricine})(\text{ISONIC})]$  (A) and  $[^{99m}\text{Tc}(\text{HYNIC-tetramer})(\text{tricine})(\text{PDA})]$  (B) in the kit matrix, and their solution stability data after HPLC purification (C). The solution stability data for  $[^{99m}\text{Tc}(\text{HYNIC-tetramer})(\text{tricine})(\text{TPPTS})]$  were obtained from our previous study [30].



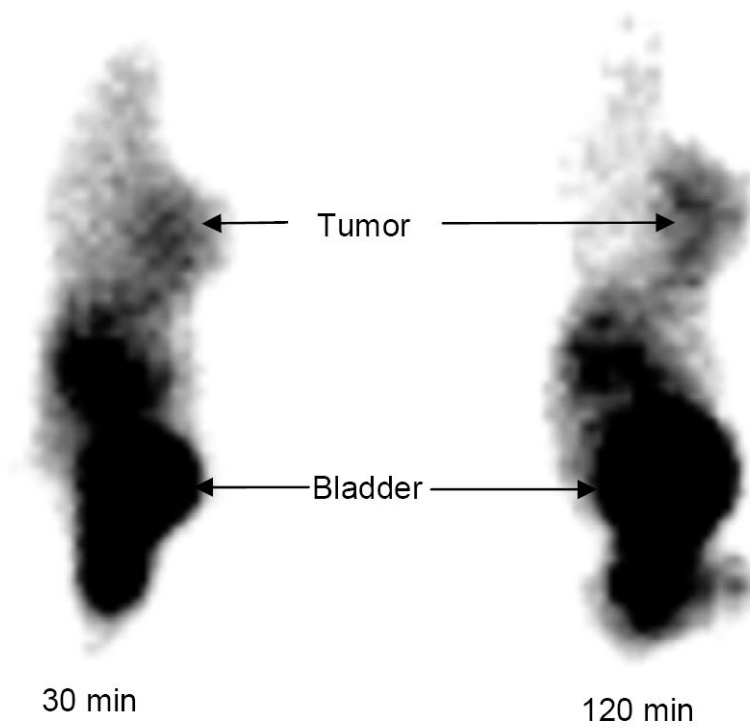
**Figure 3.** Coligand effect on tumor uptake and excretion kinetics of ternary ligand complexes [ $^{99m}\text{Tc}$ (HYNIC-tetramer)(tricine)(L)] (L = TPPTS, ISONIC, and PDA) in blood, kidneys, liver, lungs, and muscle with respect to their in athymic nude mice bearing MDA-MB-435 human breast cancer xenografts. Biodistribution data for [ $^{99m}\text{Tc}$ (HYNIC-tetramer)(tricine)(TPPTS)] are obtained from our previous studies in the same tumor-bearing animal model [30].



**Figure 4.** Coligand effect on T/B ratios of [ $^{99m}\text{Tc}(\text{HYNIC-tetramer})(\text{tricine})(\text{L})$ ] (L = TPPTS, ISONIC, and PDA) in athymic nude mice bearing MDA-MB-435 human breast cancer xenografts. T/B ratios for [ $^{99m}\text{Tc}(\text{HYNIC-tetramer})(\text{tricine})(\text{TPPTS})$ ] are obtained from previous studies in the same tumor-bearing animal model [30].



**Figure 5.** Radio-HPLC chromatograms of  $[^{99m}\text{Tc}(\text{HYNIC-dimer})(\text{tricine})(\text{ISONIC})]$  (left) and  $[^{99m}\text{Tc}(\text{HYNIC-tetramer})(\text{tricine})(\text{PDA})]$  (right) in the kit matrix before injection, in the urine and feces at 120 min postinjection. Each tumor-bearing mouse was administered with ~ 3.7 MBq of radiotracer. Two tumor-bearing mice were used for each radiotracer.



**Figure 6.** Representative static planar images of the tumor-bearing nude mice administered with ~3.7 MBq of [ $^{99m}\text{Tc}$ (HYNIC-dimer)(tricine)(ISONIC)] at 15 and 120 min p.i. Arrows indicate presence of tumor and bladder.



**Table 1**

Biodistribution data of [ $^{99m}\text{Tc}(\text{HYNIC-tetramer})(\text{tricine})(\text{ISONIC})$ ] in athymic nude mice bearing MDA-MB-435 human breast cancer xenografts. The organ uptake is expressed %ID/g. Each data point represents an average of biodistribution data in four animals

Organ	5 min	30 min	60 min	120 min
Blood	7.40±0.41	2.23±0.23	1.35±0.55	0.61±0.27
Brain	4.44±8.03	0.75±0.41	0.47±0.06	0.33±0.03
Eyes	14.52±4.45	6.51±3.51	3.58±0.73	2.82±0.29
Heart	8.02±0.91	3.06±0.69	2.66±0.81	2.33±0.41
Intestine	16.58±6.07	7.98±2.62	8.09±3.27	7.58±2.33
Kidneys	53.81±17.33	38.28±9.08	32.20±3.46	31.23±4.60
Liver	11.73±0.87	5.03±0.93	4.93±0.63	4.28±0.51
Lungs	11.23±2.21	6.15±1.79	4.53±0.93	3.97±0.64
Muscle	3.50±0.26	3.71±0.69	2.82±0.53	2.22±0.39
Tumor	5.77±0.35	5.07±0.63	5.51±0.37	5.12±1.02
Tumor/Blood	0.78±0.37	2.36±0.32	3.87±0.51	8.40±1.26
Tumor/Liver	0.49±0.09	0.86±0.16	1.05±0.27	1.20±0.21
Tumor/Lung	0.53±0.07	0.82±0.21	1.14±0.13	1.33±0.43
Tumor/Muscle	0.53±0.46	1.39±0.33	1.93±0.23	2.31±0.18

**Table 2**

Biodistribution data of [ $^{99m}\text{Tc}(\text{HYNIC-tetramer})(\text{tricine})(\text{PDA})$ ] in athymic nude mice bearing MDA-MB-435 human breast cancer xenografts. The organ uptake is expressed %ID/g. Each data point represents an average of biodistribution data in four animals

Organ	5 min	30 min	60 min	120 min
Blood	3.28 ± 0.37	1.85 ± 0.79	1.89 ± 0.51	0.78 ± 0.28
Brain	0.16 ± 0.04	0.15 ± 0.03	0.14 ± 0.04	0.12 ± 0.05
Eyes	1.12 ± 0.41	1.16 ± 0.36	0.85 ± 0.07	0.94 ± 0.19
Heart	1.95 ± 0.57	1.53 ± 0.10	1.23 ± 0.21	0.99 ± 0.40
Intestine	2.57 ± 2.22	2.93 ± 0.21	3.41 ± 0.72	2.77 ± 1.28
Kidney	7.39 ± 1.75	8.52 ± 1.94	8.88 ± 2.44	9.43 ± 1.90
Liver	2.86 ± 0.95	2.55 ± 0.52	2.69 ± 0.55	1.99 ± 0.90
Lungs	2.78 ± 0.60	2.45 ± 0.33	2.34 ± 0.26	1.62 ± 0.78
Muscle	1.58 ± 0.64	1.64 ± 0.53	1.67 ± 0.44	0.77 ± 0.30
Spleen	1.39 ± 0.55	1.40 ± 0.23	1.43 ± 0.32	1.35 ± 0.58
Tumor	2.20 ± 0.32	1.94 ± 0.12	2.79 ± 0.88	2.27 ± 0.89
Tumor/Blood	0.37 ± 0.13	1.26 ± 0.72	1.52 ± 0.54	2.88 ± 0.45
Tumor/Liver	0.43 ± 0.10	0.78 ± 0.12	1.04 ± 0.25	1.23 ± 0.32
Tumor/Lung	0.45 ± 0.15	0.80 ± 0.07	1.18 ± 0.33	1.49 ± 0.28
Tumor/Muscle	0.90 ± 0.49	1.27 ± 0.42	1.51 ± 0.20	2.97 ± 0.69