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## Fluid Transport Phenomena in Ocular Epithelia

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### Abstract

This article discusses three largely unrecognized aspects related to fluid movement in ocular tissues; namely, a) the dynamic changes in water permeability observed in corneal and conjunctival epithelia under anisotonic conditions; b) the indications that the fluid transport rate exhibited by the ciliary epithelium is insufficient to explain aqueous humor production; and c) the evidence for fluid movement into and out of the lens during accommodation. We have studied each of these subjects in recent years and present an evaluation of our data within the context of the results of others who have also worked on electrolyte and fluid transport in ocular tissues. We propose that 1) the corneal and conjunctival epithelia, with apical aspects naturally exposed to variable tonicities, are capable of regulating their water permeabilities as part of the cell-volume regulatory process, 2) fluid may directly enter the anterior chamber of the eye across the anterior surface of the iris, thereby representing an additional entry pathway for aqueous humor production, and 3) changes in lens volume occur during accommodation, and such changes are best explained by a net influx and efflux of fluid.

### Keywords

unidirectional water fluxes; net water fluxes; electrolyte transport; corneal epithelium; conjunctival epithelium; ciliary body epithelium; crystalline lens

### Introduction

Most ocular tissues transport fluid. This property is widely recognized in the cases of the corneal endothelium and ciliary body epithelium, which are largely responsible for corneal deturgescence and aqueous humor formation respectively. When isolated under *in vitro* conditions, the epithelia of the cornea, conjunctiva and lens have also exhibited fluid transport activity. We recently provided an overview of the established transporters and channels likely to underpin such fluid transport in these latter tissues, and suggested possible functional roles for active fluid movement by these epithelia (Candia, 2004; Candia and Alvarez, 2005). More recently, Levin and Verkman (2006) presented a fundamentally similar overview, but emphasized the central roles of CFTR and aquaporins (AQPs) in the fluid transport effected by most ocular epithelia. As such, these authors implicitly espoused the commonly held view

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that the underlying linkage between fluid and electrolyte transport is via a transcellular local osmotic mechanism, a concept rigorously defended by Mathias and Wang (2005).

In contrast, Fischbarg and his associates have recently provided data on the corneal endothelium that are inconsistent with the transcellular local osmotic hypothesis, whereby AQPs are required to facilitate fluid transport, and instead they promote the idea that net fluid movement across this tissue occurs paracellularly driven by an electro-osmotic coupling to recirculating  $\text{Na}^+$  currents at the level of the intercellular tight-junctions (Fischbarg, 2003, 2006; Fischbarg *et al.*, 2006). Succinctly, their model rests upon various observations including the findings that fluid transport persists in the face of inhibited transcellular  $\text{HCO}_3^-$  and  $\text{Cl}^-$  secretion (Diecke *et al.*, 2007), and that *in vitro* measurements of net fluid transport across endothelial cells isolated from AQP1 null mice exhibited fluid transport rates largely similar to those obtained with cells isolated from control animals (Fischbarg *et al.*, 2006). In addition, Hill's group have provided reviews on the evidence for paracellular fluid transport (Shachar-Hill and Hill, 2002) and on work with AQP knockout mice (Hill *et al.*, 2004), while Larsen *et al.* (2007) have also analyzed the  $\text{Na}^+$  recirculation theory as it pertains to ion-coupled water transport in both low- and high resistance epithelia. Conversely, although Mathias and Wang (2005) do not question the possible validity of fluid transport models employing electro-osmosis, they deduced that local osmosis will also be present and sufficient to generate the nearly isotonic fluid that is transported. Their conclusions were based on theoretical models containing high transcellular water permeability provided by AQPs in both apical and basolateral membranes.

Fischbarg (2003,2006) does not dispute an important role for AQPs in transcellular water movement across tissues normally exposed to large transepithelial osmotic gradients (e.g., kidney collecting ducts), but questions their necessity as water conduits for the secretory or absorptive functions of "low-volume fluid transporting" epithelia, such as those in the eye. Instead, he suggests that AQPs may be involved in cell volume regulation given his group's recent findings of impaired regulatory volume decrease (RVD) in corneal endothelial cells from AQP knockout mice. They posit that the cytoplasmic aspects of the water channels may interact with other regulatory proteins (Fischbarg *et al.*, 2006), a hypothetical notion that has recently been buttressed by recent work on AQP5, which was demonstrated to co-localize with TRPV4 (the transient receptor potential vanilloid 4), a molecule thought to function as an osmosensor (Liedtke 2005a,2005b;Liu *et al.*, 2006). It was shown that AQP5 and TRPV4 concertedly controlled regulatory volume decrease in salivary gland cells (Liu *et al.*, 2006). Hill *et al.* (2004,2006) have also suggested a role for AQPs in osmosensing.

Interestingly, histological observations by Levin and Verkman (2006) of corneas from AQP-deficient mice have provided somewhat curious findings that perhaps may be related to changes in cell volume regulatory processes. For example, they report increased corneal stromal and epithelial thickness in mice lacking AQP5, the aquaporin expressed at the epithelial apical surface, but reduced corneal thickness in mice deficient in AQP1, the only AQP found in the endothelium. Presumably, AQP5 was needed to prevent *in vivo* swelling. This suggests a possible role of the epithelium in *in vivo* corneal deturgescence as reported by Klyce (1975, 1977). On the other hand, AQP1 deficiency did not lead to swelling *in vivo*. However, AQP1 was required in order to restore corneal thickness in corneas pre-exposed to hypotonic solutions, implying a role for AQP1 in the deturgescence of pre-swollen corneas (Levin and Verkman, 2006).

Moreover, it is also important to note that the *in vivo* corneal endothelium does not transport a net flow of fluid. This occurs because either 1) there is a recirculation - a flow in one direction in one pathway and the same flow in the opposite direction in another pathway (i.e., a level flow), or 2) the negative, imbibition pressure of the stroma is balanced by a force produced by

the transport mechanisms, and there is no net flow across either pathway (i.e., a static head). This question has not yet been resolved. Furthermore, net flows are always determined in swollen corneas, which is not the *in vivo* situation; or with isolated, or cultured, corneal endothelial cells which are isolated from the negative pressure of the stroma. Thus, one must question if Fischbarg's circulating  $\text{Na}^+$  currents cease, or do not exist *in vivo*, when there is no net flow across the corneal endothelium, or if the paracellular fluid transport proposed by Fischbarg's model is balanced by an equal and opposite transcellular movement of fluid towards the stroma.

Overall, the disparate observations noted above, as well as the conflicting views on the epithelial mechanisms for solute-solvent coupling in fluid transport, require further analysis and experimentation, and cannot be easily resolved at the present time. As such, the purpose of this article is to highlight other unsettled phenomena in ocular fluid transport physiology that have remained unrecognized and warrant further thought. We will focus on the effects of anisotonic conditions on the epithelial water permeability of the cornea and conjunctiva, the meager fluid transport activity of the isolated ciliary body epithelium, and the apparent fluid transport that accompanies shape changes of the lens under conditions mimicking the accommodative process.

## Measurements of Water Fluxes and Water Permeability

We have applied two commonly used methods to measure water fluxes across various ocular epithelia: a) unidirectional/diffusional flow with tritiated water ( $^3\text{H}_2\text{O}$ ); and b) net water flow by volumetric/gravitational procedures.

With method "a", the diffusion permeability coefficient,  $P_{dw}$ , is expressed in cm/s and given by:

$$P_{dw} = J_{dw} / (A \cdot V_w \cdot C_w)$$

where,  $A$  is the area of the membrane ( $\text{cm}^2$ ),  $V_w$  is the partial volume of water ( $\text{cm}^3/\text{mol}$ ),  $C_w$  is the concentration of water ( $\text{mol}/\text{cm}^3$ ), and  $J_{dw}$  is the measured flux in  $\text{cm}^3/\text{s}$ .

In this case, a 2-compartment chamber is used. The tissue is mounted between compartments;  $^3\text{H}_2\text{O}$  is added to one side and samples are taken periodically from both sides to determine the diffusion of  $^3\text{H}_2\text{O}$ , which is proportional to  $J_{dw}$ . Details of the method and evaluations have been published (Candia and Zamudio, 1995; Candia *et al.*, 1997, 1998a, 1998b).

With method "b", the osmotic permeability coefficient,  $P_f$ , is expressed in cm/s and can be calculated from the following expression:

$$P_f = J_v / (A \cdot V_w \cdot \Delta C_s)$$

where,  $J_v$  is in  $\text{cm}^3/\text{s}$  and  $\Delta C_s$  is the difference in solute concentration ( $\text{mol}/\text{cm}^3$ ). For this approach, a two-compartment arrangement could also be used, along with a graduated capillary tube, or appropriate detection system, in order to directly measure  $J_v$  as a function of time. Examples of this approach were given by Maurice (1972) and by Fischbarg and his associates (Narula *et al.*, 1992; Yang *et al.*, 2000). This method is analogous to the gravimetric methods used earlier to quantify fluid movement across the urinary bladder (Parisi and Bourguet, 1983; Finkelstein, 1987), and we have recently presented our application of this approach on the ciliary epithelium (Candia *et al.*, 2005).

Unidirectional fluxes of water determined with  $^3\text{H}_2\text{O}$  (method "a") are usually large and similar in both directions. Thus, a small difference (the net volumetric flow, which is detected directly with method "b") is difficult to detect by method "a" and is usually not calculated as a difference

between two unidirectional fluxes. For example, in the case of the conjunctival epithelium, we demonstrated that such unidirectional water fluxes ( $J_{dw}$ ) across the tissue were statistically identical in either direction (Candia *et al.*, 2006), and have a magnitude  $\approx 60$ -fold larger than the reported values for the net flux ( $J_v$ ) of fluid secreted to the tear side by the isolated conjunctiva ( $\approx 4 - 6 \mu\text{l} \cdot \text{h}^{-1} \cdot \text{cm}^{-2}$ , data from Shiue *et al.*, 2000 and Li *et al.*, 2001 using their applications of method “b” (a volumetric approach). Because of this discrepancy in magnitude, it is unfeasible (if not impossible) to calculate  $J_v$  as the difference between the two, relatively large, unidirectional fluxes in the opposite directions. However, method “a” (a diffusional approach) is useful for determining the effects of agents or various experimental conditions on water permeability ( $P_{dw}$ ); because although labeled water will cross cell membranes via all available pathways - lipid bilayer, AQPs, and other channels, we have demonstrated that measurements of  $J_{dw}$ , which reflect  $P_{dw}$ , change equally in both directions when an experimental maneuver changes the water permeability of the epithelium (Candia *et al.*, 1997; 1998a; 1998b; 2006).

The discovery of the aquaporins (Preston and Agre, 1991; Preston *et al.*, 1992; King and Agre, 1996) led us to re-examine some of the phenomenological data of water fluxes that had remained unexplained, such as the apparent “rectification” phenomenon that existed in measurements of transepithelial water movement across the amphibian bladder (Candia, Mia and Yorio, 1997). Briefly, arginine vasopressin (AVP) elicits as much as a 40-fold increase in net water fluxes across the bladder when the mucosal-side osmolarity is diluted 10-fold. But an AVP induction of a net water flux is not obtained when the osmotic gradient is in the opposite direction (serosal-side hypotonic), implying a rectification phenomenon. However, this condition (i.e., serosal-side hypotony) elicits a reduction of unidirectional water fluxes in both directions indicating no rectification, but rather a simple decrease in permeability by the unilateral hypotonic conditions from the basal side. It is possible that the basolateral water permeability could have been down regulated, when these cells are swollen from their basolateral sides, due to either aquaporin closure or the removal of constitutive water channels from the membrane. Such reduction in water permeability, which was also observed in corneal and conjunctival epithelia (Candia *et al.*, 1998a, 1998b), may be part of a regulatory mechanism to help maintain cell volume. Consistent with this possibility, it was suggested that water permeability mediated by AQP4 might be regulated by a gating mechanism (Zelenina *et al.*, 2002).

Another observation that has received varied interpretations is the conflicting values obtained for  $P_f$  and  $P_{dw}$  in an individual tissue. Furthermore, whereas AVP increases  $P_f$  by 40 times, it only increases  $P_{dw}$  no more than 6 fold (Hays and Franki, 1970; Parisi and Bourguet, 1983). The accepted interpretation is that in bulk flow (where the radius of the pore is much larger than that of a water molecule, and laminar flow occurs) a difference between  $P_f$  and  $P_{dw}$  is predicted so that  $P_f/P_{dw} \gg 1$  for pores of large radius. This explanation also predicts that when a pore is only slightly larger than a water molecule, so that it restricts water translocation to a single file movement,  $P_f = P_{dw}$  (Finkelstein, 1987). Determinations of the most constricted pore region of the aquaporin structure indicate a diameter of 4 Å (Ren *et al.*, 2001), thereby sufficient to only allow for single-file water movement. Thus, an alternative interpretation must be found for the discrepancy in  $P_f$  and  $P_{dw}$  values. As noted above, we have suggested that the imposed osmotic gradient necessary for  $P_f$  measurements induces, in itself, cell volume changes that in turn modify membrane water permeability via an effect on aquaporins, or other water-transporting channels, i.e., possibly either gating or retrieval of the channels into submembrane endosomes. This phenomenon would not be elicited when measuring  $P_{dw}$  in the absence of an osmotic gradient, but detected as a change in  $P_{dw}$  in the presence of such gradient. Because it is now clear that the large-pore radius theory cannot be applied to the aquaporins, this reasoning may explain published discrepancies between  $P_f$  and  $P_{dw}$ .

It is also important to note that although the units of  $P_f$  and  $P_{dw}$  are identical (cm/sec), these parameters are actually different measurements.  $J_{dw}$  is directly proportional to the activity (concentration) of water, whereas  $J_v$  is proportional to the solute concentration, which decreases the activity of water as solute levels are increased. For a detailed analysis of these phenomena, see Katchalsky and Curran (1967), and Finkelstein (1987).

## Water Permeability Studies on Isolated Corneal and Conjunctival Epithelia

Our studies examined the water permeability characteristics of the epithelia of the frog cornea and rabbit conjunctiva isolated in Ussing-type chambers under short-circuited conditions (Candia *et al.* 1998a, 1998b). While the frog corneal epithelium is similar to the toad bladder in that its apical aspect had relatively lower water permeability than its basolateral surface (Candia *et al.*, 1998a), such sidedness is not a characteristic of the conjunctiva in that neither surface is rate limiting to transepithelial water movement (Candia *et al.*, 1998b). More importantly, it was found that a reduction in  $J_{dw}$  in response to basolateral hypotony was a trait common to both of these ocular tissues, as we initially observed with the amphibian bladder (Candia *et al.*, 1997). Furthermore, unidirectional water fluxes across both the frog corneal epithelium and the rabbit conjunctiva are also inhibited by unilateral hypertonic conditions (Candia *et al.*, 1998a; Candia *et al.*, 2006).

Typically, the unilateral introduction of anisotonic media produced  $\approx 20\text{-}30\%$  reductions in  $J_{dw}$  in both tissues, which were reversible upon restoring the control physiological osmolality. The corneas were more responsive to changes in bath tonicity from the stromal, or basolateral side of the preparations, than from the tear side. With the conjunctiva, the introductions of either hypo- or hypertonic solutions against the tear- or stromal-sides of the preparations were equally effective in reducing  $J_{dw}$ , with the exception that in order to obtain such reduction with increased tonicity from the stromal side (medium osmolality increased by adding sucrose), conditions inhibiting regulatory volume increase (RVI) mechanisms (e.g., pretreatment with amiloride and bumetanide, or  $\text{Na}^+$ -free Tyrode's solution) were also required. Putatively, when present in the stromal-side bath, sucrose may diffuse slowly through the relatively thick conjunctival stroma so that its concentration in the lateral spaces may rise in a manner sufficiently limited that intrinsic RVI mechanisms (e.g.,  $\text{Na}^+/\text{H}^+$  exchange, NKCC activity) could come into play and maintain cell volume. As such, the apparent down-regulation of membrane  $P_{dw}$  would not occur under conditions with an adequate RVI response, but would do so under conditions with which RVI mechanisms were inhibited. Thus, these experiments suggested that the reductions in epithelial membrane permeability occurred secondarily to changes in cell volume (Candia *et al.*, 2006); presumably the epithelial cell volume had to be perturbed markedly in order to elicit the decline in  $P_{dw}$ .

In both corneal and conjunctival epithelia, the transepithelial water fluxes ( $J_{dw}$ ) seem to be predominately transcellular because data were obtained that indicate independence between unidirectional water fluxes and the integrity of the paracellular pathway - 1) there is no correlation between control levels of  $J_{dw}$  and control transepithelial electrical resistance ( $R_t$ ) values, which inversely reflect paracellular conductances; and 2) mannitol fluxes, which solely traverse paracellular pathways, are increased by both hypertonic and hypotonic conditions that reduce  $J_{dw}$  comparably (Candia *et al.*, 1998b; 2006). Apparently, the unilateral anisotonic environment compromised the integrity of the tight junctions leading to the mannitol flux increase, thereby indicating that the concomitant reduction of  $J_{dw}$  occurred via an inhibition of a transcellular pathway.

Further evidence for a predominately transcellular route for  $J_{dw}$  was obtained using Arrhenius plots, which indicated that the tonicity-elicited water permeability reduction occurred at the level of "water transporting" channels (Candia *et al.*, 1998a; 2006). Moreover, in experiments

with the conjunctiva, transepithelial fluxes of n-butanol, a highly lipophilic compound, were measured under anisotonic conditions to test whether or not water movement across the lipid bilayer was affected due to any putative alteration of tissue geometry *in vitro* (Candia *et al.*, 2006). The unilateral anisotonic conditions did not affect the transconjunctival n-butanol fluxes (suggesting that the integrity of the lipid bilayer was not affected), but did increase the energy of activation ( $E_a$ ), implying that the tonicity shifts produced less water movement through water channels (Candia *et al.*, 1998a; 2006).

Data from the latter approach on the conjunctiva suggested that most of the transepithelial water diffusion ( $J_{dw}$ ) occurs via water-transporting channels presumably at both surfaces and perhaps, as well, through the communicating junctions within the multilayered epithelium. This is based upon the finding that the control  $E_a$  for water diffusion of 4.93 kcal/mole that was calculated with the conjunctiva, resides between the value of 2.7 kcal/mole reported for isolated endosomes containing the water channels of the anuran urinary bladder (Verkman, 1992), and a value of 10.2 kcal/mole obtained with native *Xenopus* oocytes (Zhang and Verkman, 1991), which naturally exhibit relatively low intrinsic water permeability. An approximate 30-40% increase in  $E_a$  was calculated with conjunctivae under anisotonic conditions (Candia *et al.*, 2006), implying a partial reduction in water movement via channel-mediated pathways; similar increases in  $E_a$  were obtained with the frog corneal epithelium under hypotonic conditions (Candia *et al.* 1998a).

However, we have not yet identified the specific channels that are “down-regulated” by non-physiological osmolalities. The possibility that AQPs could be involved in the observed reduction in  $J_{dw}$  evoked by the anisotonic conditions remains an open question. Both the corneal and conjunctival epithelia exhibit an identical AQP distribution with AQP5 residing in the apical domain and AQP3 in the basolateral membranes (Verkman, 2003; Oen *et al.*, 2006). Both of these AQPs have reported sensitivities to mercurial agents (Kuwahara *et al.*, 1997), but the use of compounds such as  $HgCl_2$  elicits a rapid loss of the transepithelial short-circuit current (a measure of net electrolyte transport across the tissue) and an elimination of  $R_t$  (to that of the solution resistance) suggesting that  $Hg^{2+}$  is injurious to the epithelium (Candia *et al.*, 1998a, see Fig. 1; Candia *et al.*, 2006). As such, the fact that subsequent tonicity changes do not evoke further reductions in  $J_{dw}$  in  $HgCl_2$ -pretreated conjunctivae (Candia *et al.*, 2006) does not in itself demonstrate a role for AQPs in the apparent down regulation in water permeability, given that the epithelium may no longer be biochemically viable, because  $Hg^{2+}$  (at levels 1-2 orders of magnitude lower than that used to block AQPs) reacts with numerous biological ligands and produces cytotoxic effects (Issa *et al.*, 2003; Kim and Sharma, 2004; Shih *et al.*, 2005). The putative future development of non-toxic AQP blockers would be important for determining a possible role for AQPs in the observed phenomena. Alternatively, should tonicity changes reduce the  $J_{dw}$ , and hence the calculated  $P_{dw}$ , of murine tissues, such reductions could be examined with aquaporin-deficient mice.

It is also possible that changes in the activity of ionic channels that are known to exhibit relatively high water permeabilities could underlie the reductions in water fluxes evoked by osmolality perturbations. CFTR might be a candidate in this regard given that its reported water permeability is in the order of that seen with AQP3 (Pohl, 2004). In addition, some classes of  $K^+$  channels also appear to have equally high water permeabilities as the aquaporins (Pohl, 2004, see Fig. 4). Ionic channels (possibly carrying water) typically close under hypertonic conditions and contribute towards RVI mechanisms; thus, such closure might explain the reduction in  $J_{dw}$  with elevated osmolality. However, the opposite would be expected with hypotonic solutions, with which ionic channels open as part of the RVD response. Hence, the reduction in  $J_{dw}$  under anisotonic conditions may not necessarily involve the same channels when tissues are exposed to hypo- and hypertonic media. However, it should also be pointed out that the expression levels of AQPs in membranes appear to be in the order of 1,000 AQP

monomers per square micrometer, which is generally greater than the density of ion channels, or  $\approx 1$  channel/ $\mu\text{m}^2$  (Verkman and Mitra, 2000), thereby suggesting that AQPs may make a larger contribution than ion channels to the membrane water permeability phenomena described herein.

In our experiments, the tonicity changes were introduced unilaterally on either the tear or stromal sides of the preparations in separate experiments. We initially adopted this protocol with the amphibian bladder to re-examine the “rectification” phenomenon discussed above, and kept it with the ocular tissues to determine the relative responsiveness of the corneal and conjunctival epithelia to unilateral changes in bath tonicity. With these latter tissues, one would expect the osmolality of the stromal-side milieu to remain fairly constant *in vivo*. However, the apical aspects of these epithelia are naturally exposed to varied osmolalities including virtually pure water, or strongly hyposmotic solutions, as well as elevated tonicities in the cases of individuals with lacrimal gland deficiencies (Farris *et al.*, 1986). As such, the demonstrated reduction of water permeability upon the imposition of anisotonic conditions in the tear-side bath seems relevant to the physiology of the epithelia lining the ocular surface; and as noted above, the conjunctiva is more sensitive to tear-side tonicity changes than is the corneal epithelium.

A second observation consistent with the finding that the corneal apical surface is rate limiting to transepithelial water movement was obtained by the use of the polyene antibiotic, amphotericin B, which has also been used as an artificial water channel in lipid bilayers (Holz and Finkelstein, 1970). Its addition to the tear-side bath of the frog cornea increased  $J_{dw}$  by 20% (Candia *et al.*, 1998a), but such addition to the rabbit conjunctiva does not elicit marked effects (Candia *et al.*, 1998a), indicating that the conjunctival water permeability of the apical surface cannot be increased above that of the control levels, likely due to the presence of AQP5, which we have recently identified in this domain (Oen *et al.*, 2006).

Upon initially finding that the imposition of stromal-side hypotonicity rapidly reduced  $J_{dw}$  across the epithelia of the bladder, cornea and conjunctiva, we proposed that the water permeability of the basolateral membrane could have been down regulated when these cells began to swell from their serosal sides, due to either AQP closure or the removal of constitutive water channels from the membrane (Candia *et al.*, 1997, 1998a, and 1998b). As such, the reduction of basolateral water permeability would have the beneficial effect of slowing the inflow of water, thereby abetting solute-based RVD mechanisms, and contribute towards cell-volume maintenance. This idea has to be reconciled with more recent reports suggesting possible roles for AQPs in both RVD and osmosensing (Fischbarg *et al.*, 2006; Hill *et al.* 2004,2006;Liu *et al.*, 2006). Clearly, a unifying explanation for these phenomena is a contemporary question.

In the case of tear-side hypertonic conditions with the conjunctiva, the decline in  $J_{dw}$  was gradual with the largest changes measured between 45 and 60 min after the application of the tonicity increase (Candia *et al.*, 2006). Unequivocally, water must enter the epithelium for RVI mechanisms to restore cell volume and a reduction in water permeability would not be advantageous. It is tempting to speculate that in this case water-transporting channels closed after RVI mechanisms had reverted cell volume closer to that of the control state. If so, it is not immediately apparent as to why the epithelium would putatively express lower water permeability after cell volume had recovered, presumably to, or close to, its control value. However, it should be noted that the new steady-state was attained with the cellular compartment hypertonic and that by itself may be a factor affecting water permeability.

Nevertheless it is clear from our data that the water permeability of epithelia is dynamic and mutable under anisotonic conditions. To illustrate a possible functional role for this property

we provide the following examples to show how we would expect an epithelial cell layer to react to tonicity changes from either side bathing solution. Our models use the hypothetical situation that the water permeability of the basolateral membrane is ten times larger than that of the apical aspect, a feature that might exist in the corneal epithelium. Permeability (P) and net water flow ( $J_v$ ) are given in arbitrary units for illustrative purposes.

Figure 1, top cell, shows the system at equilibrium. Assuming no ionic transport mechanisms and minimal pressure gradients, there is no net water flow ( $J_v$ ) across either the apical or basolateral membrane because the osmolality is the same in the three compartments. Notice, however, that the permeability of the basolateral membrane is ten times larger than that of the apical. This includes the intrinsic permeability of the basolateral membrane and a possible larger surface area. If the diffusional water flow ( $J_{dw}$ ) could be measured separately across each membrane, it is expected that it would be much larger across the basolateral membrane.

The center cell shows what happens before volume regulatory mechanisms are activated (or if they are inexistent) when the apical-side bath osmolality is reduced to 100. The cell will swell; the cell compartment osmolality will be reduced to a value intermediary between the osmolalities of the two bathing solutions until the gradient across each membrane times its permeability gives equal fluxes ( $172.7 \times 1 = 17.3 \times 10$ ). Such equality of fluxes is required for a steady state of the transepithelial flux and cellular osmolyte concentration. The cell needs to increase its volume about 6% to reduce its concentration from 290 to 272.7. If regulatory volume decrease mechanisms exist, solute extrusion would occur with concomitant volume reduction maintaining the cellular osmolality at 272.7. It is clear that steady-state osmolality of the cell, 272.7, is proportionally closer to the bath in contact with the membrane of the larger permeability. It is calculated by:

$$\text{cell osmolality} = \frac{290 + 100 (P_a/P_b)}{(P_a/P_b) + 1}$$

By a similar reasoning, it is easy to calculate the steady state cell osmolality (300) and net water flow towards the apical solution (100) when the apical side is made hypertonic (400). Initially the cell reaches this osmolality by shrinking about 3.4% (Figure 1, bottom cell). Such putative changes in volume would be minimal and would not severely affect cellular mechanisms. Furthermore, this explanation illustrates the tolerance that epithelia, such as that of the cornea, exhibit against extreme osmolality changes on the apical side.

Figure 2, shows the consequences of reducing the osmolality of the basolateral side to 100 mOsM. The cellular compartment would only reach its predicted steady-state osmolality upon swelling 148%, or about 2.5 times its original volume. Red cells burst under these conditions, but intact epithelial layers do not. The rapidity of the swelling precludes prevention by regulatory volume decrease mechanisms that are likely present. However, as indicated by our results, epithelial cells do not burst in response to osmolalities approaching this example. We can explain this phenomenon by introducing a regulatory mechanism that, as the cell reaches a larger volume set point, the permeability of the basolateral side is reduced, let's say to 0.5 from 10 (Figure 2, bottom cell). In this situation, only a 27% increase in volume would be necessary to reach a steady state before volume regulatory decrease mechanisms are activated to reduce cell volume in the presence of the osmotic gradient.

In short, we posit that changes in water permeability in response to osmotic challenge may represent an unrecognized epithelial property that contributes towards cell-volume regulation, but the identities of the channels involved, and the signaling transduction pathways, remain to be elucidated.



## Fluid and Electrolyte Transport Studies on Isolated Ciliary Body Epithelia

Few studies have attempted to measure net fluid fluxes ( $J_v$ ) across isolated ciliary body preparations applying method “b” (a volumetric approach) described above. Cole (1966) and Burstein *et al.* (1984) described elaborate mounting protocols for such measurements, but neither reported fluid transport rates comparable to the generally accepted rate of *in vivo* aqueous formation (i.e.,  $\approx 3\text{--}4\ \mu\text{l}/\text{min}$  in rabbits; Murray and Bartels, 1993). We also designed our own approach to quantify  $J_v$  across ciliary epithelia (CE) from rabbit, bovine and porcine preparations and obtained rates of fluid transport  $\approx 60$ -fold less than the rate of aqueous formation (Candia *et al.*, 2005, 2007).

However, it is important to point out that it is difficult to accurately compare *in vitro* fluid transport by isolated CE preparations and *in vivo* rates of aqueous humor formation. Firstly, not all of the ciliary processes and pars plana are exposed to the bathing medium *in vitro*, and the actual surface area of the processes in the divided chambers that are used is an estimate (Candia *et al.*, 2005, 2007). Secondly, it may reasonably be supposed that the transport activity of the isolated CE *in vitro* is unlikely to be identical with that in the intact animal due to the absence of blood supply, a condition under which a partial collapse of the processes may occur, and/or hormones or other paracrine agents that stimulate active electrolyte transport may be lacking. Nevertheless, the detected fluid movement in the blood-to-aqueous direction that we and Burstein *et al.* (1984) observed solely reflects the secretory activity of the isolated CE (albeit possibly compromised) since these *in vitro* arrangements precluded contributions from ultrafiltration, as well as externally applied osmotic or pressure gradients.

Although the transport activity of the CE *in vitro* may not be as great as in the intact animal, it is clear that the tissue is not physically damaged by its mounting within divided chambers (Candia *et al.*, 2005). Transepithelial osmotic gradients produced by unilaterally adding 90 mM and 200 mM sucrose to the isolated bovine and rabbit preparations, respectively, were applied in order to calculate the osmotic permeability ( $P_f$ ) of these epithelia. Both specimens exhibited  $P_f$  values of  $\approx 10^{-3}\ \text{cm}/\text{sec}$  (Candia *et al.*, 2005), a reasonable value for an epithelium, and one that is similar to that of the unstimulated toad bladder, which expresses an increased  $P_f$  upon treatment with anti-diuretic hormone (Hayes and Leaf, 1962). We do not yet know whether or not the imposition of the transepithelial osmotic gradient with sucrose also affected  $P_{dw}$  as seen with the cornea and conjunctiva as described in the previous section of this article. Yet if there had been structural damage to the CE cells during the isolation and mounting of the ciliary body in the divided chambers, the imposition of the transepithelial osmotic gradient could have resulted in a larger fluid displacement from one hemichamber to the other, and a non-physiological osmotic permeability ( $P_f$ ) would have been calculated. Of course, extensive damage to the tissue would not necessarily result in large transmural fluid displacements if the reflection coefficient of the cells to sucrose had decreased and the solute permeated the tissue. With an intact epithelium, the imposed sucrose gradient necessary to calculate  $P_f$  can only dissipate slowly via the paracellular pathway, the integrity of which was corroborated by the measurements of mannitol fluxes (Candia *et al.*, 2005).

More importantly, approaches for measuring  $J_v$  *in vitro* could prove relevant for future work controlling of the secretory activity of the CE; the possibility of reduced transport activity *in vitro* is not withstanding in this regard. A putative lack of an effect by an agent capable of reducing aqueous humor formation *in vivo* on the *in vitro* fluid transport rate would be an indication that *in vivo* there are other important components involved in the production of aqueous humor.

It is well established that the driving forces for fluid production across the ciliary epithelium are the osmotic gradient (created by ionic transport mechanisms) and a possible hydrostatic

pressure difference. The relative contribution of these forces to the production of aqueous humor is still an open question, and a contribution from both appears likely (Beneyto *et al.*, 1995; Bill, 1973; Macri, 1982; Macri and Cevario, 1978). The fact that a pseudo-facility can be measured indicates that a change in intraocular pressure not only influences the efflux, but also the influx of aqueous humor. During tonometry, when an external pressure is applied to the eye, an increased outflow, as well as a decreased inflow, is observed. Thus, there is a pressure-dependent component in the aqueous humor inflow.

The importance of the osmotic force developed by active ionic transport became apparent from the initial work of Cole (1969, 1977). Following this, several investigators were able to isolate the ciliary body epithelia of toad, shark, rabbit, and bovine with which active transport mechanisms for  $\text{Cl}^-$ ,  $\text{Na}^+$  and  $\text{HCO}_3^-$  were described (To *et al.*, 2002). Complementing this work, other investigators have used the isolated tissue to look for transporters with intracellular electrodes (Chu and Green, 1990; Wiederholt and Zadunaisky, 1986), fluorescent probes (Butler *et al.*, 1994; Wolosin *et al.*, 1991), electron probe (Bowler *et al.*, 1996; Macknight *et al.*, 2000), and patch clamp techniques (Chen and Sears, 1997; Chen *et al.*, 1998; Edelman *et al.*, 1995; Wang *et al.*, 2000), or have used cultured CE cells to look for channels using microelectrodes (Helbig *et al.*, 1989c) or patch-clamping (Chen *et al.*, 1994; CoCa-Prados *et al.*, 1995, 1996; Yantorno *et al.*, 1992), and for transporters using radioisotopes (Helbig *et al.*, 1988, 1989a, 1989b), or fluorescent techniques (Tao *et al.*, 1998; Hou *et al.*, 1998, 2000). As a result of this wealth of information, several models have been proposed to explain aqueous humor production by the ciliary epithelium (Civan, 1997; Civan and Macknight, 2004; Jacob and Civan, 1996). Although the potential ions responsible for creating the necessary osmotic gradient have been identified, a quantitative accounting of the rate of ionic transport necessary for a fluid production of about 2-4  $\mu\text{l}/\text{min}$  is still elusive. Indeed, it was calculated (Chu and Candia, 1987; Krupin *et al.*, 1984) that the measured rate of ionic transport in the isolated rabbit ciliary epithelium could only account for about 15% of the observed fluid production *in vivo*. Moreover, there are no publications reporting a measured rate of active transport that can justify the *in vivo* rate of fluid transport. But as noted above, the *in vitro* transport rates may not represent the rates *in vivo*. Yet, it still appears likely that aqueous humor production is a concerted contribution by both active and passive processes, with the strongest indication for the latter coming from the pressure-dependent component of aqueous humor inflow as evidenced by the existence of pseudo-facility.

Despite the intensive effort noted above, a satisfying electrolyte transport model consistent with all the available experimental data does not exist. This situation may be due in part to the complexity of the CE and the variations in transport elements among the species studied. In the rabbit tissue, for example, the negative polarity of the aqueous side of the epithelium may be due to a blood-to-aqueous net transport of  $\text{HCO}_3^-$ , since removal of  $\text{HCO}_3^-$  from both bathing solutions reverses the electrical potential difference (PD) (Krupin *et al.*, 1984; Pesin and Candia, 1982; Sears *et al.*, 1991), whereas in the bovine tissue, a  $\text{Cl}^-$  transport from blood-to-aqueous seems to be responsible for the same PD orientation (To *et al.*, 1998a, 1998b; Do and To, 2000). Moreover, with the isolated rabbit ciliary epithelium, Kishida *et al.* (1982) and Crook *et al.* (2000) also described a net  $\text{Cl}^-$  transport as a component of the short-circuit current ( $I_{\text{SC}}$ ) across the tissue, although in the latter study there was a large discrepancy between the net  $\text{Cl}^-$  flux and the  $I_{\text{SC}}$ .

It is widely known that the composition of the aqueous humor of different species varies, particularly with regard to the  $\text{Cl}^-$  and  $\text{HCO}_3^-$  concentrations. In humans, for example,  $\text{Cl}^-$  concentration is higher and  $\text{HCO}_3^-$  concentration is lower in the posterior chamber than their concentrations in the plasma, whereas in the rabbit the reverse is true (Cole, 1970, 1984; Davson *et al.*, 1952; Kinsey, 1953; Gerometta *et al.*, 2005). Most of the transport work with the isolated rabbit ciliary epithelium has yielded results consistent with the *in vivo* higher-than-plasma

concentration of  $\text{HCO}_3^-$  in the aqueous (Krupin *et al.*, 1984; Sears *et al.*, 1991; Carre *et al.*, 1992; McLaughlin *et al.*, 1998). Even in the work of Crook *et al.* (2000), bumetanide inhibited only 43% of the  $I_{SC}$ , the remainder of which may be a net  $\text{HCO}_3^-$  flux. Evidence indicative of a net  $\text{HCO}_3^-$  flux across the rabbit CE was provided by Wolosin and coworkers, who demonstrated an asymmetry in the expression of  $\text{HCO}_3^-$  transporters in the non-pigmented and pigmented epithelia (Wolosin *et al.*, 1991, 1993; Butler *et al.* 1994). The latter exhibited the alkali-loading  $\text{Na}^+$ -dependent  $\text{Cl}^-/\text{HCO}_3^-$  exchanger, while the dominant bicarbonate transporters of the former resulted in  $\text{HCO}_3^-$  efflux. This expression of bicarbonate transporters would favor a net bicarbonate transport from blood-to-aqueous. In the isolated bovine ciliary body, in contrast, previous findings show a net  $\text{Cl}^-$  transport towards the aqueous (To *et al.*, 1998, 2001; Do and To, 2000), which is consistent with a higher-than-plasma concentration of  $\text{Cl}^-$  in the aqueous humor, as found in humans.

In collaboration with Chi-ho To, whom we lent our closed system for measuring transepithelial radiolabeled  $\text{CO}_2$  and bicarbonate fluxes (Candia, 1996), we published an explanation of the effects of the carbonic anhydrase inhibitor, acetazolamide, on the bovine ciliary epithelium (To *et al.*, 2001). In this study, we empirically ruled out the existence of a net bicarbonate transport across the bovine CE and instead showed that the inhibitory effects of acetazolamide on the  $I_{SC}$  across the CE resulted from an inhibition of a net  $\text{Cl}^-$  flux in the stromal-to-aqueous direction that was  $\text{HCO}_3^-$  dependent. We developed a vectorial model to explain the fact that the net  $\text{Cl}^-$  flux was 2-3 fold larger than the  $I_{SC}$  due to the secretion of  $\text{Na}^+$  and  $\text{K}^+$  into the aqueous that partially subtracts from the  $\text{Cl}^-$  flux. Our results (To *et al.*, 2001) suggested how carbonic anhydrase inhibitors could reduce intraocular pressure in the absence of net  $\text{HCO}_3^-$  transport as a driving force for fluid secretion; i.e., by reducing cellular  $\text{H}^+$  and  $\text{HCO}_3^-$  (generated from metabolic  $\text{CO}_2$  production), which are exchanged with  $\text{Na}^+$  and  $\text{Cl}^-$  via  $\text{Na}^+/\text{H}^+$  and  $\text{Cl}^-/\text{HCO}_3^-$  exchangers, thereby reducing the net  $\text{Cl}^-$  transport.

The net fluid flow ( $J_v$ ) is bicarbonate dependent in the rabbit CE and  $\text{Cl}^-$  dependent in the bovine CE (Candia, *et al.*, 2005), consistent with the ionic transport mechanisms summarized above. Moreover, we would expect  $J_v$  across the bovine preparation to also exhibit a bicarbonate dependency, given the  $\text{HCO}_3^-$ -dependent  $\text{Cl}^-$  fluxes that we described with this tissue (To *et al.*, 2001). However, this  $\text{HCO}_3^-$  condition was not tested on the bovine CE  $J_v$  measurements, but was done with porcine preparations, with which bumetanide inhibited  $J_v$  by  $\approx 40\%$ , while the removal of  $\text{CO}_2/\text{HCO}_3^-$  reduced  $J_v$  by  $\approx 50\%$  (Candia *et al.*, 2007), seemingly consistent with a bicarbonate-dependent  $\text{Cl}^-$  flux mechanism.

Yet, more importantly, the relative contributions of secretion by the CE and ultrafiltration to aqueous humor formation have still not been determined. As mentioned above, the large discrepancy between the *in vitro* measures of  $J_v$  and the rates of aqueous humor formation does not by necessity demonstrate a large role for ultrafiltration in the *in vivo* production of aqueous humor; nor do the volumetric approaches with the CE provide any estimate of the relative proportions between secretion by the CE and ultrafiltration. An alternative, interesting arrangement for characterizing the mechanisms underlying aqueous humor formation involves the use of an *in vitro* perfused bovine eye (Shahidullah *et al.*, 2003). With this methodology, a perfusion pressure is applied, and 40% of aqueous humor formation was ouabain insensitive (Shahidullah *et al.*, 2003), suggesting that this may represent a proportion of the formation due to passive ultrafiltration. However, Shahidullah *et al.* (2003) point out that their resultant estimation of 40% ultrafiltration in aqueous humor formation may be an overestimation, because the inhibition of active transport processes with ouabain should have led to a reduction in the intraocular pressure, which would have favored more passive ultrafiltration of aqueous humor. Such passive ultrafiltration is commonly envisaged to occur via the paracellular pathways between the cells of the CE.

But there is still another possible pathway that would allow for the ouabain-insensitive fluid flow. Freddo (2001) has detailed an impressive overview of extensive studies done by his group and colleagues showing that the entry pathway for protein into the aqueous is limited to the anterior surface of the iris, i.e., proteins directly enter the anterior chamber near the angle and are not found in the posterior chamber. This direct entry pathway to the anterior chamber strongly implies that fluid can also passively enter via this route.

Current interpretations of aqueous humor dynamics indicate that all fluid entering the anterior chamber comes from the posterior chamber via the pupil. Thus, the solute composition of fluid in the anterior chamber should be equal to that in the posterior chamber. This equality will not hold for any solute with a higher concentration in the posterior chamber than plasma (due to active transport by the CE) if there is a dilution in the anterior chamber by plasma, or if such solutes are transported back to the posterior chamber across the iris epithelium.

One could also posit *a priori* that the solute content of fluid directly entering the anterior chamber across the anterior aspect of the iris would resemble that of the plasma. As such, compounds such as ascorbate that are actively transported by the CE into the aqueous, so that the aqueous levels are about  $\approx 25$  to 50-fold higher than plasma (Kinsey, 1953; To *et al.*, 2002; Table 1), would result in an ascorbate concentration gradient from the posterior chamber to the front of the iris, where the ascorbate levels would be diluted with ascorbate-deficient fluid directly entering the anterior chamber. Consistent with this possibility, measurements by Kinsey (1953) of the respective ascorbate concentrations in posterior and anterior aqueous samples from rabbits showed levels of 1.30 and 0.96 mM; i.e., a 35% higher concentration in the posterior chamber. We recently confirmed these findings by Kinsey in rabbit and our unpublished results are shown in Table 1.

A caveat can be taken that ascorbate consumption by the lens and/or other ocular tissues, such as the cornea, could account for the difference in the concentrations. However, Kinsey (1953) also found a higher concentration of  $\text{HCO}_3^-$  in the posterior aqueous (34.1 mM) than in the anterior (27.7 mM), a measurement consistent with the net  $\text{HCO}_3^-$  transport expected to exist across the CE of the rabbit, which has plasma  $\text{HCO}_3^-$  levels of 24 mM. Although Kinsey (1953) recognized that a gain of water across the blood-aqueous barrier of the anterior chamber could account for the lower concentrations of ascorbate and bicarbonate in the anterior aqueous, he felt it more likely that these anions left the anterior chamber by diffusion via iris vessels given the favorable gradient of the aqueous-to-plasma concentrations. We prefer the former possibility because of the demonstration of Freddo (2001) for the direct entry of plasma proteins into the anterior chamber across the anterior aspect of the iris.

A higher  $\text{K}^+$  concentration in the posterior chamber than the anterior chamber might be predicted given our models for a putative net  $\text{K}^+$  flux across the bovine CE (To *et al.*, 2001). In fact, Kinsey (1953) had also provided preliminary data showing higher  $\text{K}^+$  levels in the posterior chamber than the anterior chamber of rabbit. His potassium measurements were relative, and exact concentrations were not obtained. We recently examined this question and measured a 27% higher concentration of  $\text{K}^+$  in the bovine posterior aqueous than in the anterior chamber using  $\text{K}^+$ -selective electrodes (Figure 3). Thus in general, the composition of the posterior aqueous differs from that of the anterior in those electrolytes actively transported by the CE from the plasma (so that the posterior aqueous levels are higher than plasma), with the lower levels of the anterior chamber possibly reflecting a dilution from fluid leaving the iris. As such, another undefined component of “aqueous humor production” might exist.

One should also note that the methods used to measure the rate of so called “aqueous humor production” do not actually measure the production of aqueous humor into the posterior chamber, but instead measure the exit of aqueous humor from the anterior chamber (Lee and

Brubaker, 1982; Topper *et al.*, 1984; Vogh *et al.*, 1989), which may include a contributing flow of fluid from the iris into the anterior chamber.

Finally, it should be noted that an aqueous humor outflow of 3  $\mu\text{l}/\text{min}$  (as found in rabbit) carries 0.41  $\mu\text{mole}$  of  $\text{Na}^+$ , 0.31  $\mu\text{mole}$  of  $\text{Cl}^-$ , 0.02  $\mu\text{mole}$  of  $\text{K}^+$ , 0.09  $\mu\text{mole}$  of  $\text{HCO}_3^-$ , and 0.003  $\mu\text{mole}$  of ascorbate (Figure 4) that must be replenished by transport into the posterior chamber if all aqueous humor is produced into that compartment. However, as alluded to above, there are no publications reporting a measured rate of active transport that can account for these levels of electrolytes to cross the CE each min. We have extensive experience measuring  $\text{Na}^+$  and  $\text{Cl}^-$  fluxes across isolated CE preparations from rabbit and never obtained a net  $\text{Na}^+$  or  $\text{Cl}^-$  flux across this tissue (Pesin and Candia, 1982; Chu and Candia, 1987). Thus, we are suspicious of the net  $\text{Cl}^-$  flux data of Kishida *et al.* (1982) and Crook *et al.* (2000) in rabbit, and find the data in the latter erroneous, given that the reported net  $\text{Cl}^-$  flux was orders of magnitude greater than the simultaneously measured short-circuit current. Alternatively, if one considers the rate of active transport of  $\text{Cl}^-$  reported for the cat (Holland and Gipson, 1970), the net  $\text{Cl}^-$  flux of 2.89  $\mu\text{mole}/\text{cm}^2/\text{hr}$  represents 0.289  $\mu\text{mole}/\text{min}$  across the CE if one assumes a total surface area in cat of 6  $\text{cm}^2$  as reported for rabbit (Silverman *et al.* 2001). Thus, this  $\text{Cl}^-$  transport rate seems about right. However, no evidence of a net  $\text{Na}^+$  flux of 0.41  $\mu\text{mole}/\text{min}$  has been reported across the CE in any species. Moreover, because in live rabbits the aqueous levels of  $\text{Cl}^-$  in the aqueous are not higher than plasma (Gerometta *et al.*, 2005), and we found no evidence for active transport of  $\text{Cl}^-$  across the rabbit CE, we suggest that a major role of the rabbit ciliary epithelium appears to be the active transport of bicarbonate and ascorbate into the posterior chamber (Kinsey, 1953; and Figure 4). As such, we also propose that a direct flow of fluid from the iris to the anterior chamber is a real possibility.

### Fluid Transport by the Crystalline Lens during Accommodation

The lens is an asymmetrical organ system with localized transport properties. Early work on lens asymmetry emphasized the influence of the lens epithelium in conferring to the lens its asymmetrical electrophysiological properties (Candia *et al.*, 1970; Candia, Bentley and Mills, 1971; Candia, 1973; Duncan, Juett and Croghan, 1977). When isolated in a double chamber that separated the anterior from the posterior lens surfaces, an anteriorly directed, positive electrical potential developed, as a result of an electrogenic  $\text{Na}^+/\text{K}^+$  pump located in the surface, basolateral membrane of the epithelium (Duncan *et al.*, 1980), along with parallel basolateral  $\text{K}^+$  conductance(s) (Alvarez, Wolosin and Candia, 1991). Logically, it was assumed that the activity of this monolayer was relatively uniform, and that a positive current emanated from the anterior pole to the equator. However, Patterson and coworkers (Robinson and Patterson, 1982; Patterson, 1988; Wind, Walsh and Patterson, 1988a, 1988b) using the vibrating probe, showed in frog and rat lenses a non-homogenous distribution of currents around the lens surface.

Initially, the findings of Patterson's group were not widely received, and no other laboratory attempted to reproduce their results. Nevertheless, based on Patterson's model, in which ionic currents exited around the equator and re-entered the lens at the poles, Mathias, Rae and Baldo (1997) developed a theoretical model for electrolyte and fluid circulation inside the lens. This latter model also included information obtained from impedance analysis and structural studies.

Subsequently, Candia and Zamudio (2002) designed a novel Ussing-type chamber that enabled the short-circuiting approach to be used to characterize the regional distribution of  $\text{Na}^+$  and  $\text{K}^+$  currents around the surface of the rabbit lens. A non-uniform current distribution was found in the epithelium from the anterior pole to the equator due to the absence of the  $\text{Na}^+/\text{K}^+$  pump-generated current at the anterior polar region, where passive inflow of  $\text{Na}^+$  occurred, and the dominance of  $\text{K}^+$  conductances plus the pump current at the equatorial surface, as well as, an

area just anterior to it. As such, this work represented the first independent confirmation of the findings of Patterson and coworkers, as well as provided the identification of an additional asymmetrical aspect in the lens, namely the absence of  $\text{Na}^+\text{-K}^+$  pump-generated current at the anterior-most surface. Consistent with this characteristic, Gao *et al.* (2000) estimated that the pump-current density at the frog lens equator was 20-fold larger than that at the anterior pole.

Our interest in electrolyte and fluid transport in ocular epithelial led us to apply method “b” (a volumetric approach described above) to measure  $J_v$  across distinct regions of the isolated bovine lens (Candia, 2004) in order to determine if data consistent with the model of Mathias *et al.* (1997) for an internal fluid circulation within the lens could be acquired. Measurements largely in accord with the Mathias model were indeed obtained under control steady-state conditions with inward fluid movement detected across the anterior face and fluid efflux across the equatorial and posterior surfaces (Candia, 2004). The posterior fluid efflux was not predicted, and suggests that the electrolyte transport mechanisms at the posterior aspect of the bovine lens may differ from that of other more widely studied lens species (e.g., frog, rat and rabbit).

Yet the high water permeability exhibited by the bovine lens suggested to us that fluid might readily enter and exit the lens when its shape is changed. This had also been suggested by earlier studies (Cotlier *et al.*, 1968) demonstrating that lenses swell or shrink when exposed to anisotonic solutions, an indication of high capsular and fibril water permeability. We thus decided to examine the possibility that fluid movement, to and from the lens, accompanies the shape changes that occur during the accommodation process. However, for these studies, we have not applied either a volumetric or diffusional approach to directly measure water movement, but instead calculated changes in lens volume under conditions mimicking accommodation.

Accommodation is the ability of the normal eye to focus on the retina the image of objects situated within a range of distances. This change in refractive power is accomplished in lower vertebrates by an anterior-posterior movement of the crystalline lens (Gillum, 1976), and in higher primates, including man, by changes in lens curvature with minimal displacement within the eye (Garner and Yap, 1997; Glasser and Kaufman, 1999). Both the mechanisms of accommodation and its decrease with age (presbyopia) have been the subject of numerous studies (Atchison, 1995; Croft *et al.*, 2001; Glasser *et al.*, 2001). The lens is suspended inside the eye by the attachment to the capsule (around the equatorial region) of the zonulae, which are in turn attached on their opposite end to the ciliary body. The accepted theory, although there are those who dispute it (Schachar *et al.*, 1996), is that when the ciliary muscle is relaxed and flattened against the sclera, the zonulae are under tension and thus pulling eccentrically on the lens equator. This action forces the lens to adopt a more flattened shape with a larger equatorial diameter and a shorter anterior-to-posterior length. Such change in shape of the human lens has been actually recorded *in vivo* with high resolution MRI (Strenk *et al.*, 1999, 2004). When the subject is focusing on infinite, the ciliary muscle is relaxed, but the zonulae and the lens capsule are under tension deforming the pliable lens content. When the subject focuses on a short distance, the ciliary muscle contracts, its distance to the lens decreases, the zonulae relax and the lens as a whole adopts a more rounded shape, which is its normal tendency. The failures of any of these components (ciliary muscle, less pliable lens content, shortened distance from the ciliary muscle to the equator) have been accepted as contributing factors for presbyopia (Atchison, 1995; Croft *et al.*, 2001; Garner and Yap, 1997; Glasser and Kaufman, 1999; Glasser *et al.*, 2001).

However, it was not the purpose of our work to study the mechanisms of accommodation and this introduction does not attempt to cover this subject exhaustively. We merely propose the possible existence of a fluid flow between the lens and the intraocular fluids during

accommodation. This possibility has not been considered (except by Reiff (1995)) in the many publications on accommodation. The fundament of this assertion is based on physical laws governing the relation between surface and volume of a body changing shape. To introduce this concept, two extreme situations are described below.

First, let's assume a sphere with a given volume and a surface area which cannot change. It can be deformed or folded, but it cannot be stretched or retracted. The sphere is a body that contains a given volume with minimum surface. An example could be a soccer ball with a leather (un-stretchable) surface. When inflated it assumes a spherical shape, and this shape does not change despite being kicked around for 90 minutes. The only way to flatten it, is to let some air out (thus, reducing volume at constant surface area).

The other extreme will be an impermeable rubber balloon. We can deform its shape by pressing (or other means) without changing its volume because its surface stretches. What is the situation with the lens capsule and its contents? The capsule is rather stiff and more than 100 times stiffer than the lens content due to its collagen composition (Krag and Andreassen, 2003, see Table 2). Nevertheless, it is possible that the lens capsule stretches when pulled by the zonulae to adopt its flattened shape for far distance focusing. There is no study that has conclusively determined what changes in the lens during accommodation: surface, volume or both. Strenk *et al.* (2004) in commenting on their MRI study of *in vivo* human lenses conclude: "a quite unexpected finding is that the lens CSA (cross sectional area) increases with accommodation. Because the CSA of the lens is larger in the accommodated state when external tension is minimal, the reduction in lens CSA must be produced by the increased zonular tension required to flatten the lens. These accommodative changes in lens CSA reflect accommodative changes in lens volume and suggest that the lens material is slightly compressed when accommodation is relaxed and the external forces exerted on the lens are greatest. These results challenge a long-held belief that the lens is incompressible, based on the fact that it contains a large amount of water which is incompressible." Despite the fact that the lens compressibility (i.e., Poisson's ratio) has never been measured, they suggest the possibility that the lens material may be compressed and uncompressed with elastic recovery during the two extremes of accommodation. Thus, they have demonstrated changes in volume during accommodation, but they do not consider the possibility that fluid may be moving in and out of the lens (our hypothesis) rather than being compressed. Their demonstration is based in a two-dimensional approach: the CSA changes during accommodation. Assuming symmetry around the anterior-posterior axis, the result can be extrapolated to the 3-dimensional lens.

As indicated before, the other report suggesting possible fluid movement during accommodation is that of Reiff (1995). Although his concern is the change in intraocular pressure during accommodation, he states: "Another factor in the lens' ability to regulate intraocular pressure during accommodation would be the effect of the change in shape of the lens during accommodation on the transport of water into and out of the lens. If, as described (Koretz & Handelman, 1988), the lens capsule were relatively constant in total surface area over a short period of time, a change in shape from approximately an oblate spheroid to one approaching a globular spheroid, as occurs during accommodation, would allow the lens to imbibe more water because the maximum volume for a given surface area is the sphere."

Contrary to this, Koopmans *et al.* (2003) reported that they were able to change the accommodative power of isolated, cortex-emptied and polymer-refilled human lens capsules, where volume was constant. However, it is possible that the postmortem capsule could be substantially stretched, which is the only way that the shape and curvature can be changed at constant volume. Given this contemporary interest to replace the content of the capsular bag of cataractous lenses with a gel-like material that could be deformed by the action of the ciliary muscle, thereby re-establishing accommodation after cataract surgery, it should be made clear

that if the surface area of the capsule does not change enough, then the change in shape of the “refilled lens capsule” will be limited because the internal gel will not get out of, or into, the lens. The natural lens has two important physical properties difficult to reproduce - its high protein content for a refraction index larger than that of the aqueous humor, and a fluid content that can permeate its capsule.

We recently described in detail our approach to calculate volume from lens CSA (Gerometta *et al.*, 2007). In this work we characterized 1) an *in vitro* model: the isolated iris-ciliary body-zonulae-lens complex (CB-Z-L) dissected from bovine, and 2) a theoretical model: the graphical construction of human lenses from structural parameters acquired from the literature. The bovine lens was chosen because it could be freshly procured, its large size allowed for calculation of small volume changes, and it could be abundantly obtained at a low cost. We are aware that the bovine lens has a limited accommodative amplitude given the structure of its internal fibers (Kuszak *et al.*, 2006), but it served our purpose.

Because of the complex geometric shape of the lens, an accurate measurement of its volume is not easy to determine with certainty. Hence, we developed a method to compute the volume of the lens from lateral photographs (Gerometta *et al.*, 2007). These photographs enabled the CSA to be computed with software. We calculated the volume of isolated bovine lenses in conditions simulating accommodation by forcing shape changes with a custom-built stretching device in which the CB-Z-L was placed. Two measurements were taken (CSA and center of mass) to calculate volume. Mechanically stretching the CB-Z-L increased the equatorial length, and decreased the anterior-to-posterior length, the CSA, and the lens volume. The control parameters were restored when the lenses were stretched and relaxed in an aqueous physiological solution, but not when submerged in oil, a condition with which fluid leaves the lens and does not re-enter. This suggests that changes in lens CSA previously observed in human could have resulted from fluid movement out of the lens. If the change in volume was due to compression of its content, as suggested by Strenk *et al.* (2004), the lens should have regained its rounded shape when tension was relaxed even when immersed in oil. In the bovine, our measurements indicated a reversible 6-8% change in the volume of the lens under the conditions simulating accommodation.

Although the lens can swell or shrink under the influence of osmotic forces, there are no studies showing that a few microliters can be expelled across the anterior face in less than a second, which is the time required in accommodation. We don't know the force developed inside the lens when stretched, but it should be sufficient to move fluid at the rate required. For technical reasons related to the design of our “stretching apparatus” (rotating a wheel), it took several seconds to stretch the lens, but we felt no particular resistance (Gerometta *et al.*, 2007). With a more advanced technology, we were able to determine that the bovine lens regains its volume in less than 200 milliseconds after the release of the stretching tension (unpublished data). Although we demonstrated a change in volume of the lens, it turned out from our analysis that a change in the surface area of the lens during accommodation is also required (Gerometta *et al.*, 2007). We are presently in the processes of developing an approach to quantify the extent to which the lens surface area might also change.

In short, accommodation could involve changes in capsular surface, but it also clearly involves changes in lens volume. During accommodation, the shape and arrangement of the lens fibers should change (Kuszak *et al.*, 2006) and the fibers maybe compressed somewhat. This could result in fluid movement from the more internal fibers towards the periphery, each layer contributing a minute amount of the volume that finally emerges at the lens surface. As such, this requires good communication between fibers laterally, as described by Zampighi *et al.* (2002) for the extensive interconnection of fibers with aquaporins. Presumably, the rich



expression of aquaporins within the lens may have a role during accommodation and their possible impairment could be one more factor contributing towards presbyopia.

## General Summary

Overall, we have presented in this article unresolved issues related to fluid transport in distinct ocular tissues that we have studied over the past decade. Perhaps others might find the phenomena discussed herein sufficiently intriguing to merit complementary study and comment. Clearly an important future advance would be the development of non-toxic aquaporin inhibitors, the use of which could provide insight on each of the three subject areas that we have highlighted.

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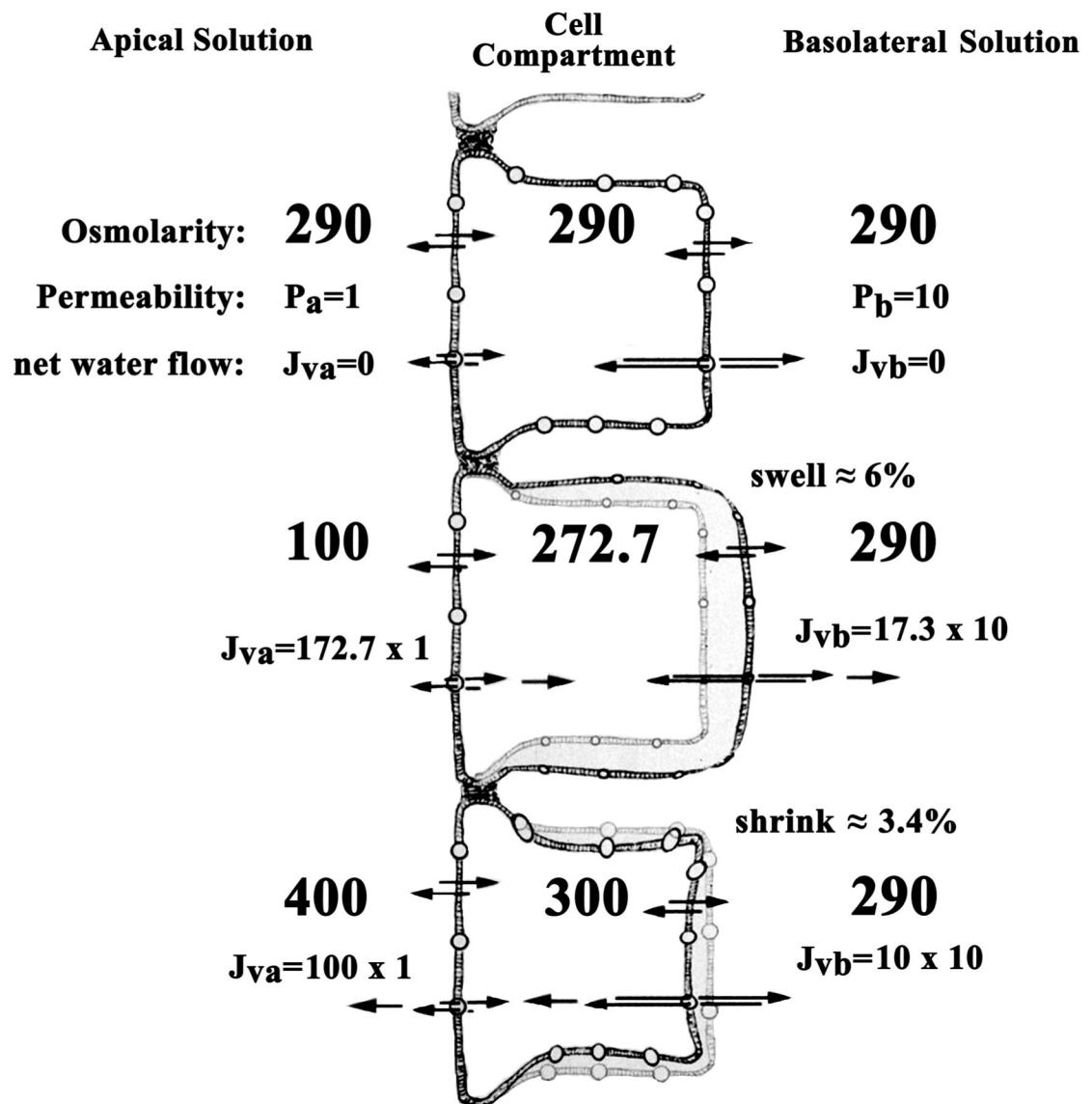
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**Figure 1.** Immediate effects of changes in osmolarity of the apical-side solution. See text for explanation.



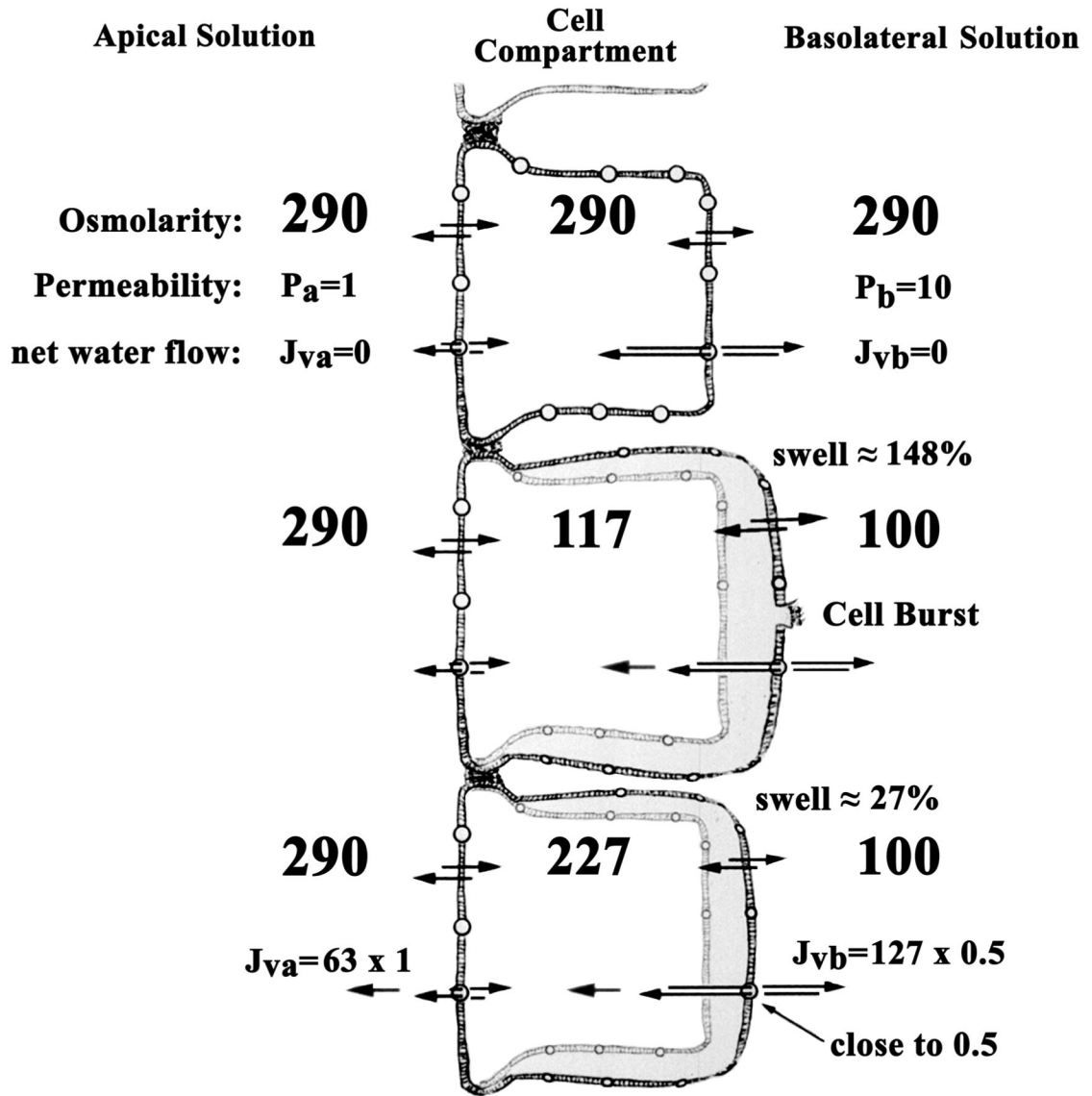
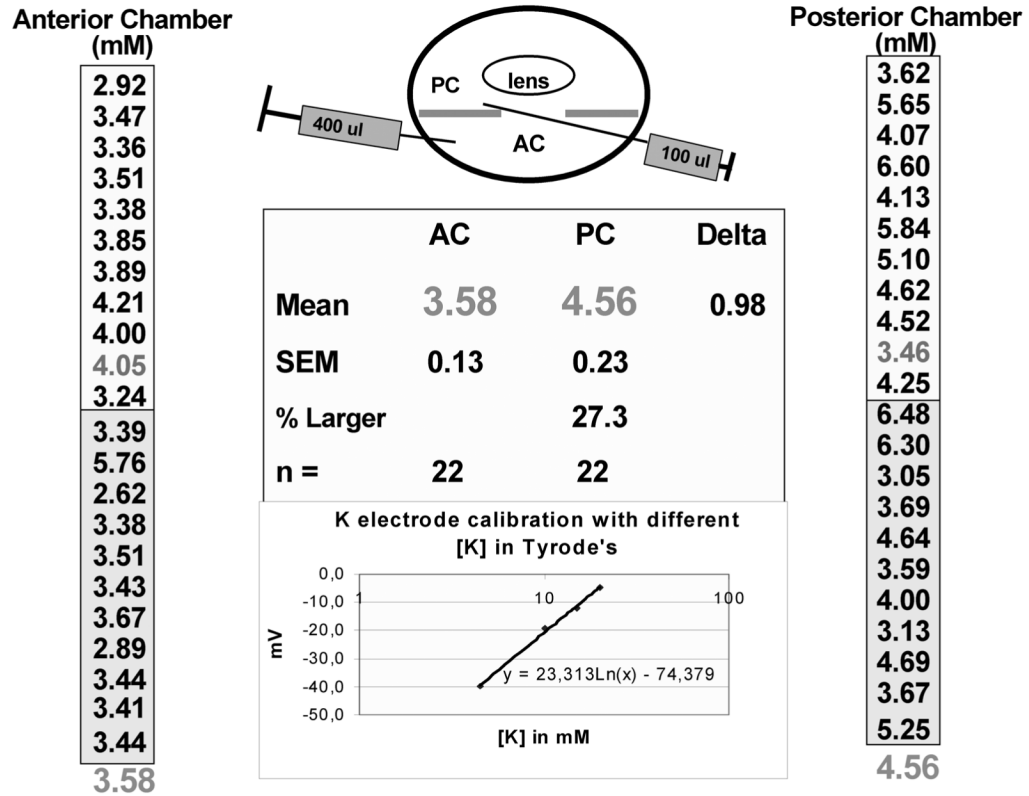
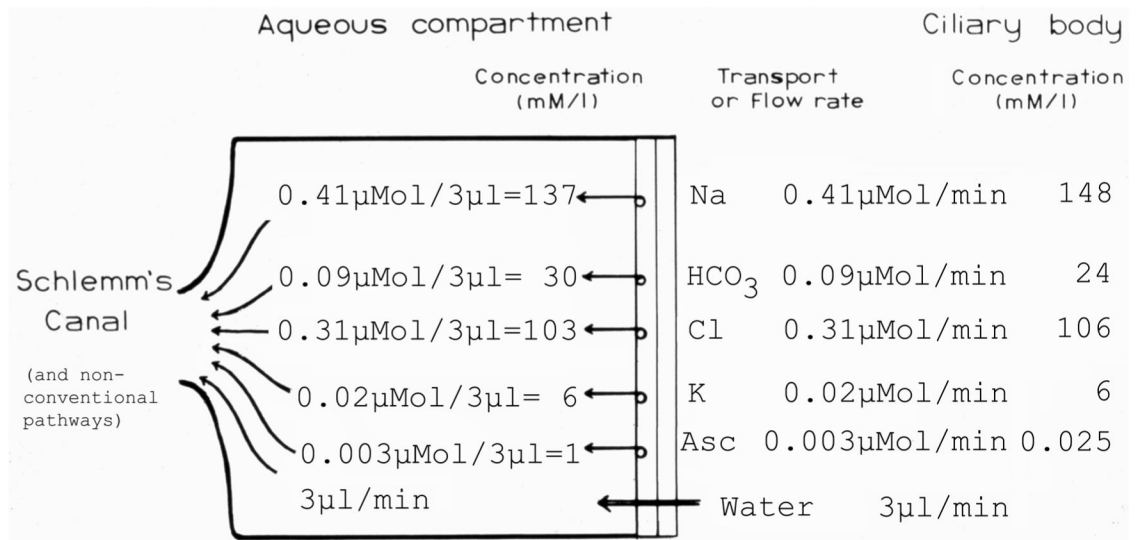


Figure 2. Immediate effects of hypo-osmolarity in the basolateral-side solution. See text for explanation.

# Potassium Concentrations in Eye Chambers of live cows



**Figure 3.** Aqueous humor potassium concentrations of the anterior and posterior chambers of the *in vivo* bovine eye. Cows at an Argentinean corral were immobilized within a narrow passage ending in a yoke that loosely closed around the neck separating the body from the head and allowing manipulations of head and neck without discomfort to the animal. These animals were destined to imminent slaughter under the supervision of a local veterinarian according to approved procedures. Two drops of topical proparacaine 0.5% (Alcon, Argentina) were instilled on the eyes as an anesthetic. Following this, an ophthalmologist (R. Gerometta of the Departamento de Oftalmología, Facultad de Medicina, Universidad Nacional Del Nordeste (UNNE), Corrientes, Argentina) performed paracentesis drawing about 0.1 ml from the posterior chamber and 0.4 ml from the anterior chamber. These samples were immediately stored on ice in capped vials for analysis with a K<sup>+</sup>-sensitive electrode at UNNE, which was done upon returning to the lab. Paired posterior and anterior samples from individual eyes were collected over the course of 2 days (distinct shaded backgrounds for each date of collection) and one mean for the posterior and anterior chambers was tabulated. The potassium concentration of the posterior chamber was higher than that of the anterior in 21 of the 22 eyes assayed.



**Figure 4.**

Model of the transport rates that would have to occur across the *in vivo* rabbit bilayered ciliary epithelium to maintain steady-state electrolyte concentrations of the aqueous compartment, given an aqueous humor flow rate of  $3\mu\text{l}/\text{min}$ . In the case of sodium, for example, the continuous loss of  $3\mu\text{l}$  of aqueous through the outflow pathways each minute requires  $0.41\mu\text{mole}$  of Na to cross the ciliary epithelium per minute to maintain aqueous [Na] at  $137\text{mM}$ . In the rabbit, only bicarbonate and ascorbate (Asc) are actively transported “uphill” into the aqueous compartment from lower plasma levels, which equal the levels within the ciliary body stroma (shown on the right-side column of the figure). Na, Cl and K values are from Gerometta *et al.* (2005), bicarbonate and ascorbate values are from Kinsey (1953), and the  $3\mu\text{l}/\text{min}$  rate of aqueous humor flow in rabbits is from Murray and Bartels (1993).

**Table 1**

Ascorbate concentrations (mM) of aqueous humor in anterior and posterior chambers of rabbit eye

Rabbit sample	Anterior Chamber	Posterior Chamber
1R	1.05	1.32
1L	0.97	1.53
2R	1.30	1.32
2L	1.24	1.82
3R	1.10	1.45
3L	1.07	1.37
4R	1.01	1.32
4L	0.98	1.41
5L	0.94	1.04
6L	0.99	1.17
7R	0.91	1.56
7L	0.85	1.30
8R	1.13	1.77
8L	1.13	1.56
Mean:	1.05	1.42*
SEM:	0.03	0.06
n:	14	14
Posterior : Anterior ratio		1.36

\* Significantly larger than the anterior chamber value as paired data,  $P < 0.001$ . Rabbits were pretreated with bilateral, topical applications of 0.5% proparacaine HCl. After 15 min, 30  $\mu$ l and 50  $\mu$ l of aqueous were drawn from the posterior and anterior chambers respectively as described by Kinsey (1953). Twenty microliter aliquots of these samples were used in the ascorbate assay of Liu *et al.* (1982). In two cases the aqueous samples were not used because the iris was punctured; injured rabbits were immediately sacrificed by placement under general anesthesia and CO<sub>2</sub> asphyxiation.