SYMPOSIUM REPORT

The output from human inspiratory motoneurone pools

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Survival requires adequate pulmonary ventilation which, in turn, depends on adequate contraction of muscles acting on the chest wall in the presence of a patent upper airway. Bulbospinal outputs projecting directly and indirectly to 'obligatory' respiratory motoneurone pools generate the required muscle contractions. Recent studies of the phasic inspiratory output of populations of single motor units to five muscles acting on the chest wall (including the diaphragm) reveal that the time of onset, the progressive recruitment, and the amount of motoneuronal drive (expressed as firing frequency) differ among the muscles. Tonic firing with an inspiratory modulation of firing rate is common in low intercostal spaces of the parasternal and external intercostal muscles but rare in the diaphragm. A new time and frequency plot has been developed to depict the behaviour of the motoneurone populations. The magnitude of inspiratory firing of motor unit populations is linearly correlated to the mechanical advantage of the intercostal muscle region at which the motor unit activity is recorded. This represents a 'neuromechanical' principle by which the CNS controls motoneuronal output according to mechanical advantage, presumably in addition to the Henneman's size principle of motoneurone recruitment. Studies of the genioglossus, an obligatory upper airway muscle that helps maintain airway patency, reveal that it receives simultaneous inspiratory, expiratory and tonic drives even during quiet breathing. There is much to be learned about the neural drive to pools of human inspiratory and expiratory muscles, not only during respiratory tasks but also in automatic and volitional tasks, and in diseases that alter the required drive.

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Background

Neural control of the mammalian respiratory system must ensure adequate ventilation to provide continuous oxygenation, carbon dioxide removal and hydrogen ion regulation for survival. The system must function during sleep, in the absence of many behavioural drives, and also during wakefulness. The repertoire of the system must allow a range of non-ventilatory functions, some of which are involved with ventilation directly, such as coughing and vocalization, and some which are involved indirectly, such as movement and postural control of the axial skeleton. Added to this, parts of the upper airway must share the same space for the passage of air, for the ingestion of food and drink, and sometimes for vomiting. So while quiet breathing may be simple, the coordination of the multiplicity of respiratory-related tasks is not. No comparable multitasking exists for movements of the limbs.

One region of the medulla, the pre-Bötzinger complex, can act as a pacemaking rhythm generator (Smith *et al.* 1991), perhaps as a coupled oscillator with the nearby parafacial respiratory group (Onimaru & Homma, 2003). When these two regions remain intact after transection of the brainstem, rhythm generation persists *in vivo* (Feldman & Del Negro, 2006). This reductionist approach has focused attention on medullary generators rather than suprapontine, pontine and spinal contributors to the patterned output from the many motor nuclei that produce ventilatory movements.

Compared with the developments from studies in experimental animals including reduced neonatal preparations, views about human respiratory output seem somewhat primitive – muscles are 'obligatory' inspiratory

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muscles if they contract during tidal inspiration, and 'accessory' if they contract when inspiratory drive is increased during exercise or loading. Recent studies have revealed that if an inspiratory muscle has a major mechanical action to expand the rib cage, it is likely to be recruited during quiet breathing (De Troyer et al. 2005; see below). However, we know comparatively little about how a particular drive generated in the medulla is distributed to the many respiratory muscles. It must emanate from bulbospinal projections within so-called dorsal and ventral respiratory groups of medullary respiratory neurones, as has been confirmed using electrophysiological (e.g. Hilaire & Monteau, 1976; Davies et al. 1985; Merrill & Lipski, 1987; Segers et al. 1987) and anatomical tracing methods (e.g. Rikard-Bell et al. 1984; Feldman et al. 1985). The consensus is that the strength of the direct monosynaptic projections to the phrenic and thoracic motor nuclei is relatively weak, particularly for the external intercostal motor nuclei (see De Troyer et al. 2005). Estimates of the direct input to intercostal motoneurones suggest that it provides less than 10% of the depolarization observed in central respiratory drive potentials, and therefore it is likely that the bulk of the phasic input arrives via excitatory spinal interneurones (cf. Saywell et al. 2007). Populations of propriospinal interneurones which receive medullary inspiratory drive have been described in the cervical (e.g. Bellingham & Lipski, 1990) and thoracic cord (Kirkwood et al. 1988).

The present review focuses on the detailed behaviour of populations of single motor units which are active during quiet breathing in awake human volunteers and patients. The motoneurones innervate obligatory inspiratory muscles. The advantage is that these recordings provide insights into how the descending inspiratory drive is sculpted *in vivo* during wakefulness in a way which is not known for other experimental preparations. The limitations are that the mechanisms driving motoneuronal discharge cannot be determined precisely. Despite this, the data lead to new questions about the brainstem output to respiratory muscles.

Studies of human respiratory muscle output

We can study the final output of the central nervous system to muscles by recording the electromyographic activity of single motor units. The timing of firing and the firing rates of a population of single motor units within a muscle indicate the descending and reflex neural drive to that motoneurone pool. We have studied the motor unit firing properties of five obligatory inspiratory muscles in humans to determine how neural drive is distributed across and within the pools during normal breathing (Saboisky *et al.* 2007*b*). Electromyographic activity was recorded using selective intramuscular electrodes from the diaphragm, scalene muscle, 2nd space parasternal intercostal, and both the 3rd and 5th space dorsal external intercostal muscles. The electrodes are moved to about 10 sites within each muscle and the electromyographic activity is decomposed to provide the spike trains from single motor units. Recordings are usually made during quiet breathing and there is little or no discomfort while they are made. The timing and amount of drive to each of the different muscles vary systematically during normal breathing (Saboisky et al. 2007b). Figure 1 illustrates the profiles of activation of populations of motor units recorded from the diaphragm and the 5th space dorsal external intercostal muscle. These muscles showed the most extreme patterns of inspiratory activity. The figure shows the times of recruitment and derecruitment, relative to inspiratory time, of each of the motor units during normal breathing. Activity of the motor units is ordered according to their onset times. The colours indicate the onset, peak and end firing frequencies of each unit. While both muscles were activated during inspiration, the motor units recorded from the diaphragm were recruited earlier, on average after 26% inspiratory time (T_{insp}) , and reached higher firing frequencies (mean 12.6 Hz), while units in the 5th space dorsal external intercostal were recruited significantly later in the breath, on average after 43% T_{insp} , and reached lower firing frequencies (mean 10.1 Hz). The remaining three muscles were recruited on average at distinct times falling between the diaphragm and 5th space dorsal external intercostal muscles. The 3rd space dorsal external intercostal muscle, scalene muscle and 2nd space parasternal intercostal muscles were recruited at 29%, 32%, 34% T_{insp} (respectively), and reached mean peak frequencies of 11.9 Hz, 9.3 Hz, 10.8 Hz, respectively. The distinct patterns of recruitment observed during normal quiet breathing in these five inspiratory muscles suggest a non-uniform activation of the different motoneurone pools that may be required to produce efficient ventilation.

The variation in the patterns of activation of inspiratory motor units across muscles begs the question: how is it organized? The simplest explanation would be that it may be organized at the level of the motoneurone. Henneman's size principle (Henneman, 1957: Henneman *et al.* 1965) states that motoneurone recruitment order depends largely on cell size as this is related to cell 'excitability'. Small-sized motoneurones are therefore recruited before large ones. This principle holds for most limb motoneurone pools (Cope & Pinter, 1995). It is possible that the different inspiratory motoneurone pools comprise different-sized motoneurones that might determine their recruitment profiles during inspiration. However, this is unlikely and there is some evidence from our data that this is not the case.

The muscles active in inspiration act on the chest wall in different proportions to create negative pressure and the inflow of air into the lungs. However, these muscles are also active in voluntary movements involving the trunk, and postural tasks requiring control of spinal stability while standing or sitting upright (e.g. Gandevia et al. 2002). In some cases, we recorded inspiratory motor units that continued to discharge throughout expiration (see also Butler et al. 2001; Gandevia et al. 2006; Saboisky et al. 2007b). These 'tonically firing' units presumably have an inspiratory and postural function. The proportion of these units in each of the five inspiratory muscles differs. Although the diaphragm was activated earliest and to the greatest extent during inspiration, it had no tonically active units. Conversely, the largest numbers of tonically firing units were in the 5th dorsal external intercostal muscles (see Fig. 1, tonic firing indicated by thin horizontal lines). Even though these tonic units in the 5th dorsal external intercostal muscle are active and therefore already at threshold, the inspiratory increase in firing can begin throughout inspiration. This late increase in activation of already-active units means that the differences in recruitment patterns of motor units across inspiratory motoneurone pools does not depend simply on differences in recruitment thresholds across pools (i.e. the size principle). Indeed, the distribution of inspiratory drive must be organized, even within a motoneurone pool, at a premotoneuronal level (Saboisky *et al.* 2007*b*).

Gradients of neural drive across intercostal muscles

Further evidence that the inspiratory drive is non-uniform comes from studies of the neural drive to intercostal muscles in humans and in dogs (De Troyer *et al.* 2003; Gandevia *et al.* 2006; for review see De Troyer *et al.* 2005). Drive is directed preferentially to those muscles or portions of muscles with the greatest mechanical advantage for inspiration. Inspiratory mechanical advantage (and respiratory effect) has been defined for respiratory muscles (Wilson & De Troyer, 1992, 1993) and measured directly for most inspiratory muscles in the dog (De Troyer & Legrand, 1995; De Troyer *et al.* 1996b; Legrand *et al.* 1996, 1997; Wilson *et al.* 1998). It has also been measured

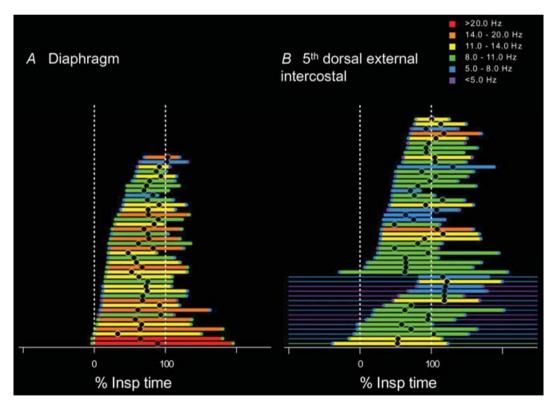


Figure 1. Time and frequency plot (TAFPLOT) of the discharge of motor units in two human inspiratory pump muscles

The firing time for each single motor unit recorded from the diaphragm (A) and the 5th dorsal external intercostal muscle (B) during quiet breathing, relative to the time of inspiration. For each unit, the thick horizontal line represents the time that the firing frequency increases in the inspiratory or expiratory phase of respiration. The thin horizontal line indicates tonic firing of the motor unit at other times. The units are ordered relative to their onset time. The colour of the thick horizontal line denotes the peak firing frequency (range 5–20 Hz; see colour scale). The onset and end firing frequencies are denoted by the coloured circles at the ends of the line. The time of the peak firing is indicated as a black circle. Data modified from Saboisky *et al.* (2007*b*) with permission of the American Physiological Society.

indirectly in the human using computed tomography imaging to derive the fractional shortening in muscle length over a standard lung volume (from functional residual capacity to total lung capacity, De Troyer *et al.* 1998; Wilson *et al.* 2001; Legrand *et al.* 2003).

Figure 2 illustrates the close relationship between mechanical advantage and neural drive for the inspiratory intercostal muscles in humans. The neural drive is given as a number of inspiratory motor unit spikes derived from the peak firing frequencies and the duration of inspiratory discharge. During inspiration, the external intercostal muscles in humans and dogs are activated earlier in each breath, and to a larger extent in the regions and spaces where inspiratory mechanical advantage is largest (for review see De Troyer et al. 2005). In humans, the motor units fire at higher frequencies in the rostral spaces (11.9 Hz in the 3rd dorsal space) than in the more caudal spaces (6.7 Hz in the 7th dorsal space). There are even differences in activation within a space; activation is greater dorsally, and less ventrally (6.0 Hz in the 3rd ventral space), which corresponds to the reduction in inspiratory mechanical advantage in the ventral portions of these muscles (Wilson et al. 2001; see Fig. 2).

Although the parasternal intercostal muscles are continuous with the internal layer of intercostal muscles, they are active in inspiration. For these muscles, there are similar rostrocaudal gradients of neural drive for both humans and dogs (Fig. 2; Gandevia *et al.* 2006; see also De Troyer *et al.* 2005). The average firing rate for parasternal intercostal motor units in the 1st space was 13.4 Hz compared with just 8.0 Hz in the 5th space. Although the mechanical advantage could not be derived for the 1st parasternal intercostal muscle, it can be estimated from the linear relationship between mechanical advantage and neural drive for the other four spaces. Along the parasternal intercostal space, for the dog, the neural drive is greatest medially and reduced more laterally (Legrand *et al.* 1996). However, in the human there is no difference in activation (Fig. 2; Gandevia *et al.* 2006), probably reflecting the differences in rib curvature and muscle fibre orientation between the human and the dog (De Troyer *et al.* 2005).

As argued above, across the intercostal muscles there is a recruitment principle related to 'neuromechanical' matching of central respiratory drive (Butler *et al.* 2007). It has been argued on theoretical grounds that the timing and degree of activation of these muscles by the neuromechanical matching principle may be metabolically efficient (De Troyer *et al.* 2005). But what is the mechanism for the control? The gradients of neural activity across the intercostal muscles are preserved in dogs even when all respiratory muscle, thoracic joint and skin feedback is removed by phrenic nerve section or dorsal rhizotomy (De Troyer & Legrand, 1995; De Troyer *et al.* 1996a). The lack of change in activation pattern despite disruption of

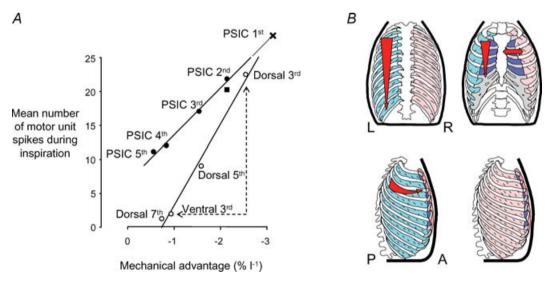


Figure 2. Neuromechanical matching in the human intercostal muscles

A, the mechanical advantage is plotted against the mean number of motor unit spikes during inspiration (i.e. neural drive) for different regions of the parasternal intercostals (\bullet) and external intercostals (O). There is a strong linear relation between the mechanical advantage and neural drive for each muscle ($r^2 = 0.99$). The line for parasternal intercostals has been extrapolated to predict the mechanical advantage of the muscle fibres in the first space (marked as a cross). Note that the medial and lateral (marked as a square) portions of the 2nd parasternal intercostal muscle have a similar mechanical advantage. Note also that there is an appropriately low neural drive to the ventral portion of the 3rd external intercostals, which has a low mechanical advantage compared to the dorsal portion. This figure is modified from Gandevia *et al.* (2006). *B*, the gradients of mechanical advantage and inspiratory drive are shown schematically for the parasternal intercostals and the external intercostals. The letters L, R, P and A refer to left, right, posterior and anterior, respectively.

these inputs suggests that the pattern is preset. Although equivalent experiments cannot be done as in experimental animals, it is likely that the pattern is also preset in humans. This is supported by the observation that the pattern of activation of inspiratory muscles in the neck is constant across a wide range of lung volumes and muscle lengths during voluntary inspiratory efforts (Hudson et al. 2007). Studies in patients with limited respiratory output would be consistent with this view (Estenne et al. 1998). A preset activation of different motoneurone pools or parts of a motoneurone pool may be organized partly at a spinal level via different-sized motoneurones, through a network of inhibitory interneurones, or at a higher level, but this is not yet known. Propriospinal interneurones at the upper cervical level (C1-C3) (Lipski & Duffin, 1986; Lipski et al. 1993) as well as Renshaw cells may be involved (Lipski et al. 1985). If we think of the different portions of intercostal muscles, with different mechanical advantages for different tasks, as separate muscles (even within the same intercostal space), then the neuromechanical principle of motoneurone recruitment is superimposed on the Henneman's size principle of recruitment. This is not likely to be a feature unique to respiratory muscles. There are some examples of task-dependent changes in motoneurone recruitment within the biceps brachii motoneurone pool which would be consistent with this proposal (ter Haar Romeny et al. 1982; Tax et al. 1989). Due to wide variation in mechanical advantage within many axial respiratory muscles, the ability to deliver drive differentially across the motoneurone pool may be especially important. This would also apply to muscles with a wide origin which can produce different directions of movement (e.g. the deltoid and trapezius; see Herrmann & Flanders, 1998).

Multiple neural drives in the human genioglossus

The genioglossus is a major upper airway dilator and it provides a dramatic example of a muscle that receives a heterogeneous combination of drives even during eupnoea. In the cat, recordings from the medial branch of the hypoglossal nerve have revealed that some motoneurones are active in inspiration while others are active in expiration (Hwang et al. 1983), although whether these fibres innervated the same muscle was not known. We became interested in the single motor unit activity of the genioglossus in humans during normal breathing, as multiunit EMG recorded by intramuscular electrodes suggests that the muscle is activated throughout respiration (Mezzanotte et al. 1992; Tangel et al. 1992), and hence the pattern of activation may resemble that in the cat. This pattern contrasts with that of the diaphragm and other pump muscles, which are not usually active during expiration, with the exception of a small proportion of tonically firing motor units (Fig. 1). In addition, in humans, the genioglossus contracts ~ 100 ms prior to the onset of airflow (Strohl *et al.* 1980).

Recordings of single motor unit activity from the genioglossus in healthy human subjects during quiet breathing reveal that its activity differs from that in 'pump' muscles in several ways. Figure 3 depicts the firing profiles of the population of genioglossus motor units (adapted from Saboisky et al. 2007a). First, we identified several different classes of motor unit behaviour (Saboisky et al. 2006; see also Tsuiki et al. 2000; Eckert et al. 2007). As in the pump muscles, many units were active either in inspiration only, or throughout respiration but with an increased discharge in inspiration and a tonic discharge throughout expiration. However, we also found motor units that increased their discharge in expiration, and a large number of motor units that fired continuously without any respiratory modulation. The different types of firing could be recorded simultaneously from the same intramuscular electrode, so although units could be active during opposite phases of the respiratory cycle, they are likely to have a complementary role in maintaining airway patency. Second, the firing rates of motor units in the genioglossus are on average twice as high as those of the pump muscles. Firing rates reach up to \sim 25 Hz on average for tonically active genioglossus units (Saboisky et al. 2006) compared with 12.6 Hz for the diaphragm and 10.1 Hz for the 5th dorsal external intercostal motor units. Third, genioglossus motor units are recruited prior to or at the beginning of inspiration, significantly earlier (on average $\sim 5\% T_{\text{insp}}$ for inspiratory phasic units) than the inspiratory pump muscles (26% T_{insp} for the diaphragm) where motor units continue to be recruited throughout the breath.

Figure 3 highlights the differences in the timing and distribution of inspiratory and expiratory drive across the hypoglossal motoneurone pool, as well as the differences outlined above from the inspiratory pump muscles. The neural output from and within these respiratory motoneurone pools is not uniform and may be controlled spinally or supraspinally, but this has not yet been established.

Conclusions

As measured from the firing of populations of single motor units, the respiratory output from obligatory inspiratory muscles in human subjects breathing quietly when awake is not homogeneous in its respiratory timing, its distribution between and within particular muscles, and its amount. Furthermore, while the activity is usually phasic, especially in the diaphragm, tonic firing with an inspiratory modulation occurs particularly in the lower intercostal muscles, which have an inspiratory action on the rib cage. When the genioglossus, an upper airway muscle, is subjected to the same form of study, a greater number of firing patterns is encountered, including purely tonic firing and even firing with expiratory modulation. The classification of firing patterns observed during quiet breathing is simple, but the magnitude of any respiratory 'linkage' of firing patterns can be assessed formally by correlation of firing rate change with lung volume changes (Saboisky et al. 2006). This linkage is likely to change with posture, respiratory drives, and behavioural state (sleep versus wakefulness; see Bailey et al. 2007). Hence, the temptation to link the patterns of firing with the type of motoneurone studied under one condition should be resisted, as the patterns are likely to be labile, dependent on respiratory, postural and other motor demands. Furthermore, the presence of firing in single motor units does not reveal the source of all the extrinsic and intrinsic factors contributing to motoneuronal depolarization. Recent studies in the cat have shown that respiratory activity can appear even in lower limb muscles, but this may not occur through traditional respiratory bulbospinal pathways (Ford & Kirkwood, 2006).

The present studies are limited in several ways. First, so far, they have focused on the motoneuronal output during quiet (presumably non-volitional) breathing, in which there is little detectable activity linked to inspiration in primary and premotor cortical areas (e.g. Macefield & Gandevia, 1991; Raux et al. 2007). During volitional breathing, which does involve the motor cortex (e.g. Colebatch et al. 1991), it remains to be determined whether there is a similar temporal and spatial distribution of motoneuronal output to inspiratory motoneurone pools. If there is, it may suggest the presence of a spinal or subcortical network which is capable of the required coordination of inputs to, and outputs from, the motoneurones. However, it is possible that a mechanism to distribute drive 'efficiently' has evolved independently for both corticospinal and respiratory bulbospinal drives to motoneurone pools. Second, drive to expiratory muscles

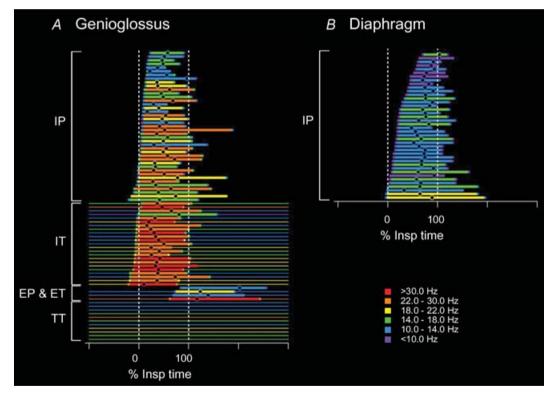


Figure 3. Time and frequency plot (TAFPLOT) of the discharge of motor units in the genioglossus and the diaphragm in humans

The firing time for populations of single motor units recorded in a group of subjects from the genioglossus, an upper airway muscle (A) and the diaphragm, a pump muscle (B) during quiet breathing, relative to the time of inspiration. For each unit, the thick horizontal line represents the time that the firing frequency increases in the inspiratory or expiratory phase of respiration. The thin horizontal line indicates tonic firing of the motor unit at other times. The units are ordered relative to time of the onset of their increased firing. Phasically firing units during inspiration (IP) are shown on top, followed below by tonically firing units that increased their discharge during units that did not increase their firing in time with respiration (TT). Data modified from Saboisky *et al.* (2007*a*,*b*) with permission of the American Physiological Society.

has not been assessed in detail, yet even during eupnoea, rhythmic activity can be recorded from human triangularis sterni muscles during stance (e.g. Estenne *et al.* 1988) and sitting (unpublished observations).

Notwithstanding these limitations, our approach has highlighted that conventional views of motor control will need to be expanded to explain the recruitment of axial muscles according to their measured mechanical advantage for inspiratory (and possibly other) tasks. Studies in patients with increased respiratory drive due to chronic obstructive pulmonary disease have shown that drive can be elevated to obligatory inspiratory muscles, especially the diaphragm (De Troyer et al. 1997; Gorman et al. 2005), and that this may form quite a stereotyped output. However, we know little about how the respiratory drives to the axial muscles develop, how they can be modified, and how they are limited during postural and volitional tasks. Such information will help define the neural substrate that ensures respiratory homeostasis and ultimately our survival.

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