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Endovascular coils as lung tumour markers in real-time tumour tracking stereotactic radiotherapy: preliminary results

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Abstract To evaluate the use of endovascular coils as markers for respiratory motion correction during high-dose stereotactic radiotherapy with the CyberKnife, an image-guided linear accelerator mounted on a robotic arm. Endovascular platinum embolisation coils were used to mark intrapulmonary lesions. The coils were placed in subsegmental pulmonary artery branches in close proximity to the target tumour. This procedure was attempted in 25 patients who were considered unsuitable candidates for standard transthoracic percutaneous insertion. Vascular coils (n=87) were successfully inserted in 23 of 25 patients. Only minor complications were observed: haemoptysis during the procedure

(one patient), development of pleural pain and fever on the day of procedure (one patient), and development of small infiltrative changes distal to the vascular coil (five patients). Fiftyseven coils (66% of total inserted number) could be used as tumour markers for delivery of biologically highly effective radiation doses with automated tracking during CyberKnife radiotherapy. Endovascular markers are safe and allow high-dose radiotherapy of lung tumours with CyberKnife, also in patients who are unsuitable candidates for standard transthoracic percutaneous marker insertion.

Keywords Stereotactic radiotherapy · Marker · Lung tumour

Introduction

Conventional radiotherapy for early stage non-small cell lung cancer (NSCLC) has poor clinical outcome [1]. New radiotherapy techniques have been developed to deliver a higher radiation dose to the lung tumour while sparing adjacent normal tissue [2–6]. Common to these new regimens is the control for respiratory motion in combination with the use of a stereotactic coordinate system [7, 8]. Target localisation can be further improved by the insertion of small metallic markers into the lung tumour, which are automatically detected by the image guidance of tumour tracking radiotherapy systems (TTRS) [8] or internal gating systems [6]. Both marker-based treatment systems enable a considerable reduction of the safety margin to avoid a geometric miss, resulting from tumour motion

outside the radiation beam. This limits the volume of nearby healthy tissues that will be irradiated, reducing the toxicity of the treatment. As a result, high biologic effective radiation doses shown to obtain local control rates on the order of 90% in stage I NSCLC can then be safely administered [9, 10].

The standard technique of marker insertion for tumour tracking is a direct percutaneous transthoracic puncture [8]. The insertion of a marker inside the lung tumour was shown to enable an accurate three-dimensional (3D) target localisation during the respiratory motion [6].

However, not all lung tumours (e.g., cavernous tumours or small, lesions without clear contours) are suitable for transthoracic percutaneous marker placement. Furthermore, the 22–45% risk of pneumothorax after transthoracic marker placement may be unacceptably high for some of



this generally frail patient population due to severe cardiopulmonary co-morbidity [8, 11–13]. Thus, many patients with NSCLC who might potentially benefit from curative radiotherapy currently cannot undergo such high-dose radiotherapy treatment because of the limitations inherent to marker placement by transthoracic puncture.

Therefore, we explored the use of vascular embolisation coils, positioned in small subsegmental pulmonary artery branches surrounding the tumour, as markers for tumour tracking. Endovascular marker placement would be an achievable alternative also in tumours difficult to reach for transthoracic puncture. This would also eliminate the risk of pneumothorax. Here, we report our initial results on the feasibility, effectiveness and complications of endovascular coils, as markers for the SynchronyTM [14], the respiratory tumour tracking system of the CyberKnife (Accuray, Sunnyvale, CA).

Materials and methods

Patients

From May 2005 to November 2006, 50 patients with a lung tumour were referred for frameless motion-corrected stereotactic radiotherapy with the SynchronyTM system of the CyberKnife. In 25 patients, metallic markers for tumour tracking were inserted using direct transthoracic puncture. In 25 other patients (18 male, 7 female), direct transthoracic puncture was considered not feasible or too risky due to: possible major clinical consequences of a pneumothorax for six patients (history of pneumonectomy (2 patients), bilobectomy (two, including one patient with a lesion without clear contours), lobectomy (one) and one oxygen dependent patient), a major risk to develop pneumothorax (two patients with one lesion in each lung, including one patient with a cavernous tumour; two patients with two lesions in the same lung), the combination of advanced age and/or cardiopulmonary toxicity (15 patients). The median age of these 25 patients was 79 years (range, 28-89). Twenty patients had primary NSCLC, which was biopsy proven in 12. Five patients were treated for metastatic lung disease: one of cervical carcinoma (two lesions, left-sided and right-sided), two of rectal carcinoma (including one patient with one lesion in each lung), one of malignant melanoma (two lesions in the left lung) and one of a breast carcinoma (two lesions in the right lung). Table 1 shows the diameter, number and localisation of the lung lesion(s). The Charlson Comorbidity Score [15], assessing the comorbidity of a given patient by accounting for several health disorders, is also shown in Table 1. Approval from the Ethics Committee was obtained for the use of vascular embolisation coils as marker for lung tumours, and all patients gave informed consent prior to the insertion of embolisation coils.

Table 1 Charlson Comorbidity Score and tumour characteristics

Patient number	Diameter of nodule(s) (mm)	Number of nodules, lung side	Charlson Comorbidity Score
1	36	1, R	3
2	31/28	2, L	6
3	32	1,R	3
4	44	1,R	5
5	27	1,R	8
6	23/27	1 L; 1 R	6
7	23	1, R	7
8	34	1, L	1
9	20	1, L	3
10	50	1, R	1
11	32	1, R	1
12	24	1, L	3
13	40	1, R	2
14	30	1, R	5
15	29	1, L	3
16	55	1, R	1
17	26	1, R	2
18	17/20	2, R	6
19	16/6	1 L, 1 R	3
20	40	1, R	5
21	30	1, R	2
22	11	1, R	3
23	24	1, L	4
24	15	1, L	2
25	29	1,R	3

^{*}Failure to insert coil, L = left lung, R = right lung

Technique of endovascular marker insertion

The patient was installed in the supine position, and the procedure was performed in the interventional suite.

A 7-F pulmonary angiography catheter (Grollman-type angled pigtail) was inserted through the femoral vein (although both sides can be used, the right femoral vein was habitually punctured) and positioned in the left or right main pulmonary artery under ECG monitoring (Fig. 1). Over a .035" guide wire, the catheter was exchanged for a 5-F angled tipped general-purpose catheter with a single end hole. The catheter was advanced over the guide wire into one of the subsegmental pulmonary artery branches in the vicinity of the lung tumour. Larger but not smaller tumours could be well seen with fluoroscopy during the procedure. The position of smaller tumours was inferred from the pre-procedural CT examination of the lungs, and catheter placement was then based on segmental anatomy of the pulmonary arteries. When in the desired position, the catheter was wedged into a small subsegmental pulmonary

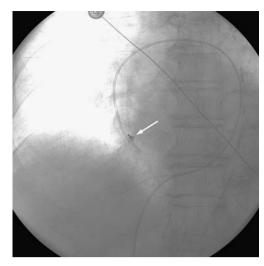


Fig. 1 A pulmonary arterial catheter used to place a coil. The inserted coil is indicated by the arrow: $179 \times 179 \text{ mm}$ ($96 \times 96 \text{ DPI}$)

artery branch and a 3–4-mm tapered platinum embolisation coil was placed (Tornado Embolization coils, Cook, Bloomington, IN). Platinum coils were used because of their high radio-opacity. Ideally, three coils were placed.

After the procedure, we recorded any clinical symptoms suggestive of immediate pulmonary complications. After an average period of 7 days (range, 2–19 days), a noncontrast-enhanced four-dimensional multislice planning CT (4-D CT) examination was performed, which was evaluated for possible complications of coil placement. The 4-D CT was also used to appreciate the extent of synchronous motion of the tumour with coils on a given distance.

Complications were classified according to the Society of Interventional Radiology (SIR) reporting standards [16]. The SIR standards of the practice committee classifies the complications by outcome: type A complications are minor complications that require no therapy and have no consequence; type B complications are minor complications requiring nominal therapy, including overnight admission, for observation only and have no consequence; type C complications are major complications requiring therapy and include minor hospitalization (< 48 h); type D complications are major complications that require major therapy, causing an unplanned increase in level of care, and include a prolonged hospitalization (>48 h); type E complications are major complications resulting in permanent adverse sequelae, and type F complications result in death of the patient.

CyberKnife

The CyberKnife is a frameless image-guided radiotherapy system. The 6-MV linear accelerator is mounted on a robotic arm possessing six degrees of motion freedom. The

CyberKnife therapy unit is equipped with an imageguidance system that consists of two kV X-ray tubes attached to the ceiling of the treatment room and a pair of orthogonally positioned flat-panel imagers mounted on the floor. A marker extraction algorithm automatically detects the position of the markers in the X-ray images. Basically, the algorithm searches for areas with high contrast in both images that could originate from a single marker. These areas are candidate markers. On the basis of the expected characteristics of the markers and their expected relative positions from the planning CT, the algorithm determines which candidates are true markers and reconstructs the marker locations in 3D. Finally, the 3D marker locations are registered to the marker locations that were determined in the planning CT to obtain the translations and rotations. Although one marker is sufficient to reduce translational setup errors of the target [17], three markers were required to distinguish marker migration from true tumour motion. As long as the three markers do not migrate in the same direction to the same extent, their migration can be detected by the change in the mutual distance between the markers. The probability that the three markers would migrate an identical distance and direction may be considered sufficiently small to warrant the use of this three marker method for the detection of marker migration.

The SynchronyTM is the respiratory tumour tracking system of the CyberKnife. The system automatically compensates for the tumour motion by continuously adjusting the position of the beam. The actual motion of the linear accelerator is determined by a correspondence model that relates the respiratory signal, registered by lightemitting diodes placed on the skin, with the internal metallic markers that are localised by the kV X-ray system. The correspondence model is built at the start of the treatment by acquiring kV X-ray images at different phases of the breathing cycle. During the treatment this model is continuously updated by acquiring X-ray images every 3 to 5 min.

Results

Coil placement

Endovascular coils (n=87) were succesfully inserted in 23 of 25 patients in whom the procedure was attempted. A median number of 3 coils for each tumour was inserted (range, 1–5). Table 2 depicts the number of coils for each nodule and the total number of coils for each patient. Coils could also be safely inserted in the two patients with a lesion in each lung as well as in one patient with a medical history of pneumonectomy. In five cases the ideal number of three coils was not inserted due to: haemoptysis during the procedure after insertion of the 2nd coil (n=1), a centrally located tumour difficult to access (n=2), long duration of the procedure and fatigue of the patient (n=2).

Table 2 Number of coils inserted per nodule and per patient

Patient number	Coil per nodule	Total coils inserted
1	5	5
2	3	6
3	2	2
4	4	4
5	3	3
6	2 R, 3 L	5
7	*	*
8	*	*
9	2	2
10	4	4
11	4	4
12	3	3
13	4	4
14	4	4
15	3	3
16	3	3
17	3	3
18	2, 3	5
19	2 R, 1 L	3
20	5	5
21	4	4
22	3	3
23	4	4
24	3	3
25	5	5

^{*}Failure to insert coil, R = right lung, L = left lung.

These last two patients included a patient in whom two tumours were marked. In this patient, the procedure was halted after inserting the fifth coil, that is, the second coil for the second tumour.

The procedure time was on average approximately 60 min. All the interventions, including also the patients with multiple lesions, could be performed at once.

The procedure failed in two patients. Here, it proved difficult to negotiate the angiography catheter through the pulmonary valve also whenever the Grollman catheter had been exchanged for a balloon-tipped flow-guided catheter. Catheter manipulation in the right ventricle induced ventricular arrhythmias, which was the reason to terminate the procedure. In both patients, we chose to resort to CT-guided transthoracic puncture despite the anticipated risk of pneumothorax rather than proceeding with the endovascular approach and increase the complications risk angiographically by using full narcosis, more extensive protection against arrhythmia and more sophisticated angiography devices including guiding catheters. Trans-

thoracic marker placement was successful in both patients, but resulted in the development of a small pneumothorax in one case.

Complications

There were no immediate procedure-related complications except for one patient who had limited haemoptysis (type A complication), probably caused by wedging the catheter too forcefully in the pulmonary artery end branches during placement of the second coil. The procedure was stopped and the haemoptysis resolved within 10 min without ensuing clinical sequelae. One other patient, who had two lung metastases from cervical cancer marked, developed chest pain and fever suggestive for pulmonary infarction, on the day of coil insertion (type C complication). The patient was treated with standard analgetics and was admitted more than 2 days in the hospital to exclude other complications such as pneumonia or pulmonary embolism. The pain was probably pleuritic because two coils were placed against the visceral pleura and caused pleuritic friction and inflammation. All the other patients were discharged from the day-care facilities after a 2-h postprocedural observational period.

During the interval between the coil insertion and the start of the CyberKnife radiotherapy (average 15 days, range, 7–29), none of the patients reported (an increase of) dyspnea or fever, except the single patient with type C complication. The radiation planning CT scan of the lungs showed no procedure-related abnormalities in 18 of 23 patients. In five patients there were small infiltrative changes distal to one of the coils suggestive for small areas of pulmonary infarction (type A complication).

Accuracy of vascular coils as tumour markers

All patients could be successfully treated with the Cyber-Knife, based on the recognition of minimally one marker per lesion. Of the 87 coils initially placed, 57 were used as tumour markers for automated tracking during CyberKnife radiotherapy. Coils that were deemed unsuitable markers (see below) were not used by the human operator during treatment.

Twenty-four coils were not used as markers because they did not complete their winding and thus did not have a completely rounded shape. Six coils were disabled based on a distance judged to be too large (range, 56–123 mm) to guarantee a similar motion of the coils as the tumour. The median distance between all the inserted coils and the tumour border was 18 mm (range, 0–123 mm). Eighteen coils (21%) were directly abutting the tumour. In one patient, none of the coils was in an acceptable position. In retrospect, this was due to erroneous placement of coils in an entirely wrong position based on imaging during

placement in the anterior-posterior view only. In this patient, satisfactory coil position was achieved in a second angiographic procedure (not counted in this analysis as an index procedure).

It is of note that all inserted coils were detected during planning CT and showed no migration, which means the coils were in a stable, fixed position, during the interval between the planning CT and the completion of treatment, which was partitioned over the course of several days.

Discussion

Our results show that endovascular coils can be used as reliable markers for automated tumour tracking during high-dose radiotherapy for lung tumours with the Cyber-Knife. Markers are placed in the interventional radiology suite by using standard, off-the-shelf angiography equipment and embolisation coils and by using local anaesthesia only. The procedure is well tolerated, safe and may be performed on an outpatient basis. After placement, the coils remain in a stable position and do not migrate as these are wedged in small pulmonary artery branches.

The endovascular route, therefore, is a valuable alternative to the standard method of marker placement by percutaneous transthoracic puncture. The percutaneous method, on the other hand, is associated with a 22–45% risk of pneumothorax, which requires a chest tube insertion in 27% of the patients with obstructive lung disease, a particularly frequent disease in this patient population [8, 11–13].

Also, the endovascular approach is feasible whenever transthoracic puncture is difficult or not possible whenever the tumour mass is not well defined (e.g., cavernous tumours, Fig. 2) or whenever the lesion is in a hard to reach lung area by direct puncture. By also applying endovascular coils as possible tumour markers, many more patients with lung tumours can now be treated with CyberKnife radiotherapy. This enables the administration of high radiation doses, reported to offer excellent clinical results similar to radical surgery for early stage NSCLC [9, 10, 18]. Although not specifically adressed in this report, we may expect the use of embolisation coils for marking lung tumours to be of benefit for every radiotherapy system using image guidance to detect markers in order to improve the target localisation.

We did not encounter clinically relevant complications after endovascular coil placement. One patient experienced an episode of transient pleural pain, one patient had short-lived haemoptysis during coil placement, and in two patients we saw clinically silent CT findings suggestive of small pulmonary infarction. This was in accordance with the anticipated complication rate based on previous experience with coil placement in the pulmonary arteries for other indications, notably, pulmonary arteriovenous malformations. Based on this, one would expect to

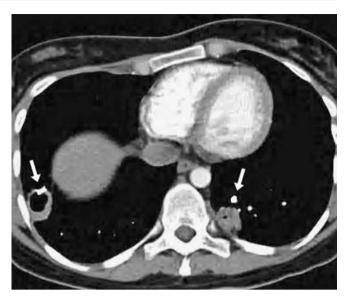


Fig. 2 Patient with two lung metastases (left and right sided) from a cervical carcinoma. Transthoracic marker insertion in the right cavernous lesion is not feasible. Furthermore, transthoracic placement in both lesions would be related to a major risk for pneumothorax. After endovascular marker placement (coils are indicated by an arrow), both lesions could be treated with CyberKnife. $98 \times 83 \text{ mm}$ ($96 \times 96 \text{ DPI}$)

encounter pulmonary infarction in 6%, pleuritic chest pain in 33% and groin haematoma in 3% [19].

Another alternative method for marker placement is the endobronchial placement using video flexible bronchoscopy with a modified transbronchial needle aspiration. The rationale to develop this method was the reduction of the risk of pneumothorax. However, bronchoscopic marker placement is performed under general anaesthesia (44%) or conscious sedation (56%) [20].

While transcutaneously placed Visicoil gold localisation markers (RadioMedCorp., Tyngsboro, MA) were shown to be stable within tumours throughout the treatment duration [21], markers placed under bronchoscopy guidance tend to have less stable fixation. In 3 out of 6 central lung lesions and 3 out of 41 peripheral lesions, Shirato et al. encountered a dropping of the marker out of the lesion [22]. Another study reported that 21% of the inserted markers could not be detected on the planning CT scan made at 0-5 days after insertion and probably were coughed up [23]. Furthermore, the variation in the position of bronchoscopically implanted markers exceeded 2 mm in 9% of the treatment sessions, necessitating more frequent reexamination with CT scanning. In our study population, no gross migration was observed between the planning CT and during treatment delivery period.

Radiofrequency ablation (RFA) is another treatment recently investigated in the care of medically inoperable lung cancer and was shown to obtain promising results. Simon et al. reported 3-year local control rates of 57% and 25% for T1 and T2 NSCLC tumours, respectively [24].



Fig. 3 Non-coiling of the coil because of mismatch between the too large coil windings relative to the small vessel diameter. The coil is therefore unsuitable for automated tracking. The arrows indicate two coils that were unsuitable for tracking due to noncoiling: $137 \times 112 \text{ mm } (96 \times 96 \text{ DPI})$

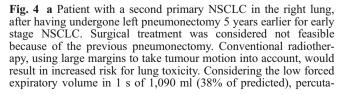
The 36% overall 3-year survival rate for stage I NSCLC was comparable to those obtained with standard external beam radiation therapy as reported in the review of Qiao et al [25]. The report of Simon highlighted the role of tumour size in the prediction of the local tumour progression rate of tumours smaller than 3 cm being more effectively treated with RFA than larger tumours. This observation confirmed the encouraging results of previous reports showing complete tumour necrosis in 69%–100% in the tumours

smaller than 3 cm [26, 27]. However, although these results are very promising, these appear to be inferior to the local control rates on the order of 90% obtained in stage I NSCLC with high-dose stereotactic radiotherapy [10].

Radiofrequency ablation was also shown by Simon et al. [24] to have an acceptable toxicity profile in patients who refused or who were not candidates for surgery with an overall pneumothorax rate of 28% with 10% requiring a chest tube insertion. Of concern is the procedure-specific 30-day mortality rate of 2.6% (4 of 153 patients). Of note, two of the patients with procedure-related deaths had previously undergone a pneumonectomy. De Baere et al. reported a pneumothorax rate of 54% with 9% requiring a chest tube [28]. Similar morbidity data were reported in other RF ablation reports [29, 30]. Randomised trials are required to accurately determine the place of radiofrequency ablation in the treatment of medically inoperable NSCLC patients.

Some limitations of our results need further attention. In this preliminary study we used standard, commercially available platinum embolisation coils of a tapered shape with gradually increasing diameter of the individual coil windings from 3 to 4 mm. These proved to be useful, but not ideal markers for the CyberKnife. In 24 of 87 cases (27%) the 4-mm diameter windings proved too big for the small subsegmental artery branches in which the angiography catheter was wedged. These windings remained stretched (non-coiling), which rendered these coils unsuitable for automated tracking (Fig. 3). Obviously, smaller winding coils are needed, but still on a .035" wire-based platform to ensure adequate radio-opacity and for ease of delivery through standard angiography catheters. As a further advantage, smaller coils may allow even more distal insertion







neous insertion of markers with its risk of pneumothorax was considered potentially life-threatening. Endovascular markers were placed (indicated by the arrow) and the patient was treated with CyberKnife by using a total dose of 45 Gy (administered in three treatment sessions). **b** Follow-up at 10 weeks. Showed complete tumour response. *Arrow* indicates the coil without remaining tumour): 84×76 mm (96×96 DPI)

in the pulmonary artery branches to further reduce the complication rates of pulmonary infarction and pleural pain.

Smaller coils may also be inserted closer to the tumour than larger coils. In our study, six coils could not be used as the distance from the tumour was too large to guarantee a synchronous motion. We used 4D CT to evaluate the relationship between both motions. A coil-tumour distance smaller than or approximating 40 mm was shown to be adequate. The smallest coil-tumour distance to be found unacceptable on 4D CT was 56 mm.

Based on our initial results, dedicated coils for marker purposes are currently being designed in close collaboration with the coil manufacturer. With this development we may expect to increase the proportion of coils that can be used during a CyberKnife treatment. In conclusion, the vascular insertion of coils is a valuable and safe method for marker implantation for lung tumours. This alternative route for placement is also feasible whenever percutaneous (or bronchoscopic) insertion of markers is not possible or undesirable. As a result, many more patients with lung tumours may now benefit from high-dose high-precision radiotherapy with CyberKnife (Fig. 4).

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