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Mechanism of Decrease in Mitral Regurgitation After Cardiac Resynchronization Therapy:

Optimization of the Force–Balance Relationship

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Abstract

Background—Cardiac resynchronization therapy (CRT) has been shown to reduce functional mitral regurgitation (MR). It has been proposed that the mechanism of MR reduction relates to geometric change or, alternatively, changes in left ventricular (LV) contractile function. Normal mitral valve (MV) function relies on a balance between tethering and closing forces on the MV leaflets. Functional MR results from a derangement of this force–balance relationship, and CRT may be an important modulator of MV function by its ability to enhance the force–balance relationship on the MV. We hypothesized that CRT improves the comprehensive force balance acting on the valve, including favorable changes in both geometry and LV contractile function.

Methods and Results—We examined the effect of CRT on 34 patients with functional MR before and after CRT (209±81 days). MR regurgitant volume, closing forces on MV (derived from Doppler

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CLINICAL PERSPECTIVE

Cardiac resynchronization therapy (CRT) is associated with a reduction in functional mitral regurgitation (MR). However, the precise mechanism of MR reduction is incompletely defined. Normal mitral valve (MV) function results from a balance of both tethering and left ventricular (LV) closing forces on the MV. Tethering forces, transmitted via the chordae, keep the valve from prolapsing, whereas closing forces depend on the pressure generated by the ventricle to close the mitral valve. Functional MR results from a derangement in this force–balance relationship of tethering and closing forces. There are 2 potential mechanisms by which CRT may reduce MR. One mechanism relates to reverse remodeling effects of CRT on the LV and MV geometry, resulting in improved spatial relationships of the MV to the ventricle and reduction in leaflet tethering. A second mechanism relates to improved LV contraction with an increase in LV pressure generation after CRT and increased closing forces on the MV with improved leaflet coaptation. To better understand the mechanism of MR reduction after CRT, we examined LV and MV geometry using 3D echocardiography and the transmitral closing pressure pattern using Doppler echocardiography, at baseline and 6 months post-CRT. The latter is an integrated measure of LV force generation and reflects the coordinated impact of closing forces on the MV throughout systole. Our results show that MR reduction post-CRT is associated with both reduced tethering of the mitral valve through beneficial affects on LV remodeling and increased LV contraction forces on the mitral valve. It has been proposed that the mechanism of MR reduction relates to geometric change or, alternatively, changes in LV contractile function. Normal MV function relies on a balance between tethering and closing forces on the MV leaflets. Functional MR results from a derangement of this force–balance relationship, and CRT may be an important modulator of MV function by its ability to enhance the force–balance relationship on the MV. We hypothesized that CRT improves the comprehensive force balance acting on the valve, including favorable changes in both geometry and LV contractile function.

transmitral pressure gradients), including dP/dt and a factor (closing pressure ratio) expressing how long the peak closing gradient is maintained over systole (closing pressure ratio=velocity time integral/MR peak velocity \times mitral regurgitation time), and dyssynchrony by tissue Doppler were measured. End-diastolic volume, end-systolic volume, mitral valve annular area (MAA) and contraction (percent change in MAA from end-diastole to midsystole), leaflet closing area (leaflet area during valve closure), and tenting volume (volume under leaflets to annular plane) were measured by 3D echocardiography. After CRT, end-diastolic volume (253 ± 111 versus 221 ± 110 mL, $P<0.001$) and end-systolic volume (206 ± 97 versus 167 ± 91 mL, $P<0.001$) decreased and ejection fraction (19 ± 6 versus $27\pm 9\%$, $P<0.001$) increased. MR regurgitant volume decreased from 35 ± 17 to 23 ± 14 mL ($P<0.001$), MAA from 11.6 ± 3.5 to 10.5 ± 3.1 cm² ($P<0.001$), leaflet closing area from 15.4 ± 5 to 13.7 ± 3.8 cm² ($P<0.001$), and tenting volume from 5.7 ± 2.6 to 4.6 ± 2.2 mL ($P<0.001$). Peak velocity (and therefore transmitral closing pressure) was more sustained throughout systole, as reflected by the increase in the closing pressure ratio (0.77 ± 0.1 versus 0.84 ± 0.1 before CRT versus after CRT, $P=0.01$); dP/dt also improved after CRT. There was no change in dyssynchrony or MAA contraction.

Conclusions—Reduction in MR after CRT is associated with favorable changes in MV geometry and closing forces on the MV. It does so by favorably affecting the force balance acting on the MV in 2 ways: reducing tethering through reversal of LV remodeling and increasing the systolic duration of peak transmitral closing pressures.

Keywords

functional mitral regurgitation; 3D echocardiography; cardiac resynchronization therapy

Heart failure is a cause of significant morbidity and mortality, and its prevalence is increasing as the population ages.¹ Cardiac resynchronization therapy (CRT) results in improvement in symptoms and survival in patients with advanced heart failure and widened QRS.^{2–4} Functional mitral regurgitation (FMR) occurs in approximately 50% of patients with left ventricular (LV) dysfunction and also negatively affects survival.^{5,6} CRT is associated with a reduction in MR, and this decrease in MR probably influences the favorable effects of CRT.^{7–8} Although reduction in MR has been described, its precise mechanism has been only incompletely defined. Normal mitral valve (MV) function results from a balance of both tethering and closing forces on the mitral valve. Tethering forces are transmitted via the chordae and keep the valve from prolapsing, whereas closing forces depend on the pressure generated by the ventricle to close the mitral valve. FMR results from a derangement in this force–balance relationship of tethering and closing forces.^{9,10} There are 2 potential mechanisms by which CRT may reduce MR. One relates to improved LV contraction with an increase in LV pressure generation after CRT, resulting in increased closing forces on the MV and improved leaflet coaptation. A second mechanism relates to reverse remodeling effects of CRT on the LV and MV geometry, resulting in improved spatial relationships of the MV to the ventricle and reduction in leaflet tethering, an important determinant of FMR.

Because CRT has the potential to modulate both contractile function and LV remodeling, elucidating the effects of CRT on MV geometry and function will provide important insights toward optimizing the therapeutic benefits of CRT and improve echocardiographic assessment of the efficacy of CRT. We hypothesized that CRT results in favorable effects on the force–balance relationship of MV function, improving both tethering and closing forces on the MV by its dual effect on LV contraction and remodeling. To look at these effects on the force–balance relationship, we used the strength of 3D echocardiography to quantify MV geometry and analyzed transmitral flow velocities to provide insights into the dynamics of MV closing forces, specifically including an integrated measure of LV force generation based on transmitral Doppler velocities.

Methods

Subjects

Consecutive patients with congestive heart failure with FMR (mild or greater) who received CRT for standard indications (New York Heart Association [NYHA] class ≥ 3 despite optimized medical therapy, ejection fraction [EF] $\leq 35\%$, and QRS duration ≥ 120 ms) were studied. Patients with acute heart failure decompensation (< 3 months), echocardiographic evidence for organic mitral valve pathology, or aortic valve disease were excluded. Two- and three-dimensional baseline transthoracic echocardiography was performed before implant or within 24 hours after implant with biventricular pacing switched off. Follow-up studies were performed approximately 6 months after implant. Clinical status was assessed at baseline and at 6-month follow-up. The study was approved by an institutional review committee, and all patients gave informed consent.

Clinical Evaluation

Evaluation of clinical status included assessment of NYHA functional class, quality-of-life score (Minnesota Living With Heart Failure Questionnaire), and 6-minute walk test.

Echocardiography Protocol

Transthoracic echocardiography was performed at baseline (before CRT) and at 6 months (after CRT). All patients underwent 2D and 3D and color Doppler echocardiographic examination at rest in the lateral position. Tissue Doppler imaging (TDI) was used to assess intraventricular dyssynchrony. Three-dimensional echocardiography was used for the assessment of LV volumes, EF, and mitral valve geometry.

Imaging Acquisition

Full-volume 3D data sets were obtained in the apical 4-chamber view with either a Sonos 7500 or IE33 using a $\times 3$ transducer (Philips Medical Systems, Andover, Mass) with ECG gating and suspended respiration. Three-dimensional datasets were transferred to a computer for offline analysis with customized software.

Data sets for TDI were obtained by 2D Doppler echocardiography using a General Electric Vivid 7 cardiac ultrasound machine (General Electric, Milwaukee, Wis). Images were obtained with a 2- to 5-MHz transducer. Color tissue Doppler imaging from 3 consecutive cardiac cycles was obtained from apical views, and frame rate was optimized (> 140 frames/s).

Data Analysis

The quantification of MR was performed using the proximal isovelocity surface area method.^{11,12} Instantaneous peak velocity and dp/dt , defined as the slope traced between 1 and 3 m/s on the MR jet recorded at a sweep speed of 100 mm/s, were measured.¹³

In addition to standard segmental measures of dyssynchrony (see below), LV and transmitral force generation as influenced by CRT was measured. These include dp/dt and the closing pressure ratio, which is an index measure that integrates LV force generation during systole based on transmitral Doppler velocities. This ratio is based on physiological principles of Doppler echocardiography examining and integrating the time course of closing pressure forces on mitral function as a measure of LV coordination¹⁴⁻¹⁶; it is calculated as velocity time integral divided by the MR time period and multiplied by MR peak velocity (velocity time integral/MR time \times MR peak velocity) and is a measure of how sustained the maximum closing forces are on the MV during the MR time. The closing pressure ratio quantifies the impact of closing forces on the MV throughout systole and reflects an integrated measure of LV force

generation. Because it is an integrative measure, it better reflects the overall closing forces on the MV rather than the instantaneous peak transmitral pressure. A higher ratio represents a transmitral gradient that rises faster and remains high for a longer period during systole (Figure 1).

To validate the closing pressure ratio, we measured the ratio in an experimental model of ischemic mitral regurgitation¹⁷ with and without pacing. Pacing introduces ventricular dyssynchrony, and the closing pressure ratio should decrease with pacing. In this model, Dorsett sheep were placed under general anesthesia (12.5 mg/kg sodium thiopental IV) and ventilated at 15 mL/kg with a mixture of 2% isoflurane and oxygen. The hearts were exposed through a left thoracotomy and an epicardial pacing lead placed on the right ventricle to produce dyssynchrony. Epicardial scanning was performed to image the MV. The MR Doppler profile was obtained using continuous-wave Doppler with and without pacing. This protocol was reviewed and approved by our institutional animal care committee.

LV Volumes and MV Geometry

End-diastolic (EDV) and end-systolic (ESV) LV volumes were calculated by tracing the LV endocardial border using 6 imaging planes and applying a surface fitting algorithm to calculate volume.¹⁸ Mitral annular area (MAA) was measured at midsystole by tracing annular points. Mitral annular contraction was defined as percentage change in MAA from end-diastole (largest area) to midsystole (smallest area).¹⁹ The leaflet closing area is the surface area of the leaflets (midsystole using 6 planes, fitted to a surface fitting algorithm).²⁰ Leaflet closing area increases in patients with LV dysfunction and indicates significant tethering. The tenting volume of the leaflets, which reflects the common end point of the force–balance relationship, incorporating both tethering and closing forces, was measured as the volume under the leaflets to the plane of mitral annulus at midsystole.

Dyssynchrony

Dyssynchrony was assessed by offline analysis of color tissue Doppler imaging. Indices of mechanical dyssynchrony calculated included (1) maximal time delay (MTD) defined as the difference between the maximal and minimal times to peak longitudinal systolic velocity among 12 segments, (2) standard deviation of the time to peak longitudinal systolic velocity for all 12 segments evaluated as Ts-SD, and (3) septal to lateral wall delay (SLD) defined as difference between time to peak systolic velocity of the basal inferoseptal and lateral walls. Left ventricular dyssynchrony was present when $MTD \geq 100$ ms^{21,22} or $Ts-SD \geq 33$ ms,²³ or $SLD \geq 65$ ms.^{24,25} Interpapillary muscle dyssynchrony was defined as the difference in time to peak longitudinal systolic velocity between the myocardial segments underlying each of the papillary muscles.²⁶

Subgroup Analyses: MR Reduction and MR No-Reduction Subgroups and Nonresponder and Responder Subgroups

The patient population was subdivided into patients in whom MR RV was reduced $\geq 20\%$ from baseline after CRT (MR reduction group) and patients whose MR RV was not reduced (increase in MR RV or a $<20\%$ reduction in MR RV: MR no-reduction group). In addition, patients were divided into echocardiographic responder (ESV reduced $>15\%$) and nonresponder (ESV unchanged or increased) to CRT.²¹

Statistical Analysis

Continuous measurements are presented as mean \pm SD. Comparison between before and after CRT and were performed using a 2-tailed Student *t* test for paired continuous data. For paired ordinal variables, the Wilcoxon signed-rank test was performed. To assess the determinants of

MR improvement after CRT, a multivariate stepwise linear regression analysis was performed with percent change in MR RV as the dependent variable. Pre-CRT variables included in the multivariate analysis were ESV, MAA, leaflet area, tenting volume, and closing pressure ratio. These variables were selected as the most likely mechanistic and functional variables to affect MR. For comparisons of subgroups (MR reduction versus MR no-reduction subgroups and responder and nonresponder groups), unpaired *t* tests were used to compare between baseline and after CRT.

Intraobserver and interobserver variabilities were assessed by intraclass correlation coefficients.²⁷ All the statistical analyses were performed using SPSS 16.0 (SPSS, Inc, Chicago, Ill).

Results

Forty-seven patients with at least mild mitral regurgitation who underwent CRT were reviewed for inclusion. Twelve patients were excluded either for intrinsic mitral valve abnormalities (5 patients) or for suboptimal image quality for 3D analysis (7 patients). One patient died before the 6-month follow-up period. Thus, a total of 34 patients with a mean age of 66 ± 12 years and 209 ± 81 days of follow-up were included in the study. Baseline characteristic of these patients are summarized in Table 1. There were more men than women, although there were no differences in the underlying etiology (ischemic versus nonischemic) of cardiomyopathy.

After CRT, patients had a clinical improvement in terms of NYHA functional class ($P<0.0001$), 6-minute walk test (284 ± 143 to 408 ± 100 meters; before versus after CRT, $P<0.001$), and quality-of-life score (54 ± 17 to 21 ± 15 ; $P<0.001$). There were no significant changes in heart rate (70 ± 11 to 69 ± 10 bpm; $P=0.8$) or mean blood pressure (85 ± 12 to 86 ± 12 mm Hg; $P=0.9$) between baseline and 6-month follow-up.

Table 2 shows the changes in echocardiographic measures before and after CRT. There was a significant reduction in MR regurgitant volume after CRT. LV volumes decreased and EF increased. There were favorable changes in MV geometry after CRT, with a decrease in MAA, leaflet closing area, and tenting volume (Figure 2). The closing pressure ratio increased after CRT, consistent with more sustained closing forces on MV during systole (Figure 3). In addition, in an experimental validation model, the closing pressure ratio was measured with and without pacing (pacing would introduce a more dyssynchronous contraction and hence decrease the ratio). In the paced heart, there was a significant decrease in closing pressure ratio compared with nonpaced hearts (0.85 ± 0.03 to 0.72 ± 0.03 , nonpaced versus paced, $P<0.001$) (Figure 4), without significant change in heart rate. Mitral annular contraction and dyssynchrony by TDI did not change significantly despite improvement in LV function. After adjusting for closing pressure ratio ($R^2=0.17$; $B=-0.42$; $P=0.03$), no other variable was significantly associated with percent decrease in MR.

MR Reduction Versus MR No-Reduction Subgroups

Table 3 compares changes in echocardiographic parameters before and after CRT within each subgroup. Fifty-three percent of the patients had a $>20\%$ reduction in MR RV after CRT (MR reduction) and 47% had lesser reduction or increases in MR RV after CRT (MR no reduction). Both groups showed a reduction in LV volumes; however, the EF increased by 53% in the MR reduction group and only by 20% in the MR no-reduction group. Importantly, only in the MR reduction group were there associated beneficial MV geometry remodeling changes. Both groups demonstrated a significant increase in dP/dt. However, only the MR reduction group was associated with a significant increase in the closing pressure ratio compared with after CRT versus before CRT (Table 3).

Responder Versus No-Responder Subgroups

Table 4 compares changes in echocardiographic parameters before and after CRT within each subgroup. Among the 34 patients, there were 62% responders to CRT and 38% nonresponders. The responders had significant beneficial changes in MV geometry and improvement in closing forces after CRT compared with before CRT, whereas the nonresponder group did not have similar improvements in mitral valve geometry after CRT compared with before CRT (Table 4).

Intraobserver and Interobserver Differences

The intraobserver variability as assessed by intraclass correlation coefficient (r) were 0.93 (95% CI, 0.75 to 0.98) for MAA, 0.94 (95% CI, 0.77 to 0.98) for leaflet closing area, and 0.93 (95% CI, 0.76 to 0.98) for tenting volume for interpapillary muscle dyssynchrony and MTD. The interobserver variability on these measurements were 0.90 (95% CI, 0.35 to 0.99), 0.91 (95% CI, 0.42 to 0.99), and 0.88 (95% CI, 0.41 to 0.98), respectively. The intravariability and intervariability values for the closing pressure ratio were 0.93 (95% CI, 0.53 to 0.99) and 0.90 (95% CI, 0.28 to 0.98), respectively. The intraobserver variability for dyssynchrony measurements were MTD, 0.83 (95% CI, -0.19 to 0.97); Ts-SD, 0.9 (95% CI, 0.3 to 0.98); and opposite wall delay (OPWD), 0.96 (95% CI, 0.61 to 0.99). The interobserver variability for these measurement were 0.86 (95% CI, 0.3 to 0.98), 0.93 (95% CI, 0.61 to 0.91), and 0.96 (95% CI, 0.69 to 0.99), respectively.

Discussion

The main finding of this study is that the reduction in FMR after CRT is associated with beneficial changes in MV geometry and improved LV closing pressures on the MV.

Force–Balance Relationship

Normal MV function relates to a balance between tethering and closing forces. The tethering forces are transmitted through the chordae to prevent mitral leaflets from prolapsing and are dependent on normal LV-MV spatial relationships.^{10,28,29} This spatial relationship depends on the position of the papillary muscle relative to the mitral valve leaflets, and LV geometry is a major determinant of this. Closing forces depend on the pressure generated by the ventricle to close the MV. FMR results from imbalance between tethering and closing forces. Apical displacement of the papillary muscles caused by a dilated or ischemically distorted LV wall increases tethering forces. Decreased LV contractility decreases closing forces.¹⁶ Both lead to incomplete mitral leaflet coaptation and mitral regurgitation. We demonstrated that CRT results in favorable effects on the force–balance relationship of MV function, improving both tethering and closing pressures on the MV by its dual effect on LV contraction and remodeling. These favorable effects result in a greater coaptation zone for closure. Our results suggest that CRT results in more sustained peak closing pressures on the MV during systole as demonstrated by a higher closing pressure ratio after CRT. A higher closing pressure ratio may result from either improved LV contractility or improved coordination of LV contraction or both. In our study, dP/dt also improved after CRT, suggesting that enhanced LV contractility plays a role in enhancing the closing pressures on the valve.

Studies have shown that FMR varies during the cardiac cycle and that it is determined by changes in the transmitral pressure gradient.^{30,31} A biphasic pattern has been described with early and late systolic peaks and a midsystole minimum.¹⁵ CRT may act to improve closing forces by improving the temporal pattern of closing forces on the MV throughout systole. Breithardt et al¹⁶ demonstrated that CRT acutely reduces the severity of FMR in patients with heart failure with left bundle-branch block. LV contractility improves; as a consequence,

transmitral pressure gradient rises faster and to a higher maximal, as reflected by increases in dP/dt .

Beneficial remodeling changes in MV geometry and closing forces occurred despite the apparent lack of improvement in intraventricular or inter papillary muscle dyssynchrony after CRT in our study. Tissue velocity–derived dyssynchrony indices did not improve after CRT, even in patients who respond favorably to CRT. Neither patients who had an improvement in LV volume after CRT nor patients in whom the degree of MR improved exhibited a resolution of mechanical dyssynchrony after CRT. Other investigators have noted similar findings.³² The principal objective of this study was to examine the effects of CRT on the mitral valve and not to demonstrate improvements in dyssynchrony.

Assessment of cardiac force generation by transmitral pressure may provide an alternate window to examine the benefit of CRT in synchronizing LV contraction.

There are a number of measures to assess dyssynchrony that are inherently segmental in nature. However, none currently integrate the effect of LV contraction as a whole. The closing pressure ratio is a measure of global and coordinated LV contraction and may provide a unique index that is a complementary or independent measure of CRT benefit.

Comparison of the MR reduction and MR no-reduction groups provided confirmatory support for the importance of improving the force–balance relationship in reducing MR. Despite similar reductions in LV volumes and improvements in LVEF, patients in the MR reduction group had significant decreases in MV geometric measures after CRT compared with before CRT, whereas patients without MR reduction did not have favorable changes in MV geometry. Both groups demonstrated a significant increase dP/dt , but the MR reduction group also had a significant increase in the closing pressure.

Patients who were responders to CRT, defined as an ESV reduction of $>15\%$, had corresponding beneficial changes compared with pre-CRT levels, in MV geometry, closing pressure ratio, and dP/dt , whereas nonresponders did not have these beneficial changes after CRT versus before CRT. These changes in responders support the notion that the MV geometric and closing forces changes mirror the LV remodeling and function changes.³³

Mechanistic Insights and Clinical Implications

Our findings demonstrated the importance of closing pressure ratio as a measure of success of CRT on MV function. An increase in closing pressure ratio after CRT reflects a more coordinated and integrated LV force generation across the MV. The closing pressure ratio mirrored favorable effects of CRT in terms of LV volume and MR reduction, and this ratio may be an important echocardiographic target to assess the efficacy of CRT.

Limitations

This study had a small sample size, and all variables considered for multivariate analyses could not be entered into the same model.

Matrix-array 3D probes have reduced frame rates and image resolution compared with 2D imaging. A reduction in frame rates may result in decreased image quality to assess complex mitral valve changes. However, image quality is typically adequate or better in patients with cardiomyopathy due to the proximity of the heart to the chest wall, especially in the apical windows.

Mitral regurgitation and LV ejection fraction can be affected by differences in loading conditions. However, the effects of different loading conditions should be minimized because

these patients were stable outpatients on an optimal medical regimen. All studies were performed in the outpatient setting, not during a hospitalization for acute exacerbation, which may change loading conditions. In addition, there were no significant differences in heart rate and blood pressure among the patient visits.

We did not directly assess the acute effects of CRT on MV function. Prior studies have demonstrated that improved interpapillary muscle dyssynchrony plays an important role in beneficial acute effects after CRT.^{8,26,34} Our study did not examine acute effects, focusing on late remodeling effects of CRT.

Conclusion

CRT is associated with a reduction in MR. The mechanism relates to optimization of the force–balance relationship, with favorable changes in both closing and tethering forces on MV function. It does so by favorably affecting the force balance acting on the MV in 2 ways: reducing tethering through reversal of LV remodeling and increasing the systolic duration of high transmitral closing pressures.

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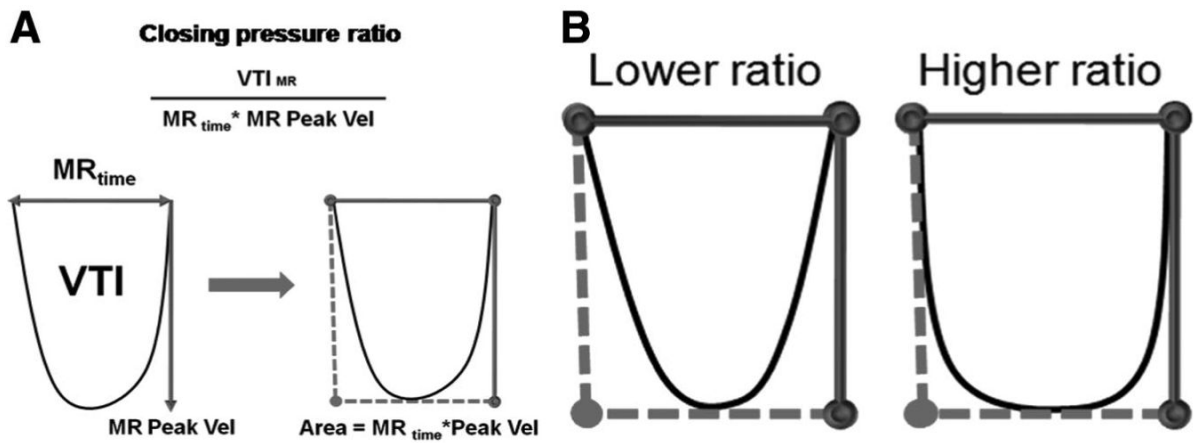


Figure 1.

The ratio of velocity time integral (VTI) divided by the MR time period (MR time) and multiplied by MR peak velocity reflects the shape of the closing forces on the MV and is a measure of how sustained the maximum closing forces are on the MV during the MR time. A higher ratio represents a transmitral gradient that rises faster and remains high for a longer period during systole.

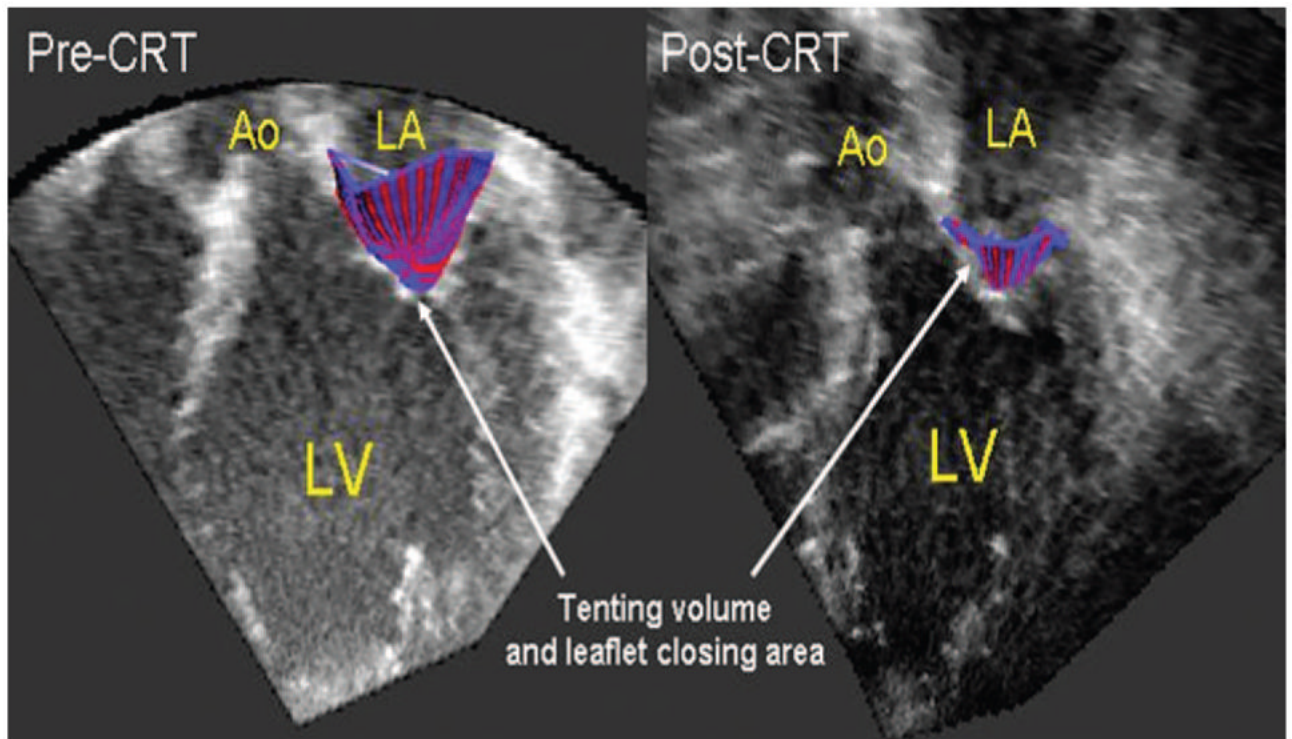


Figure 2. Three-dimensional reconstruction of the tenting volume and leaflet closing area in midsystole superimposed on 2D imaging slice from the 3D dataset. Both tenting volume and leaflet closing area decrease after CRT. Ao indicates aorta; LA, left atrium; LV, left ventricle.

Pre-CRT

Post-CRT

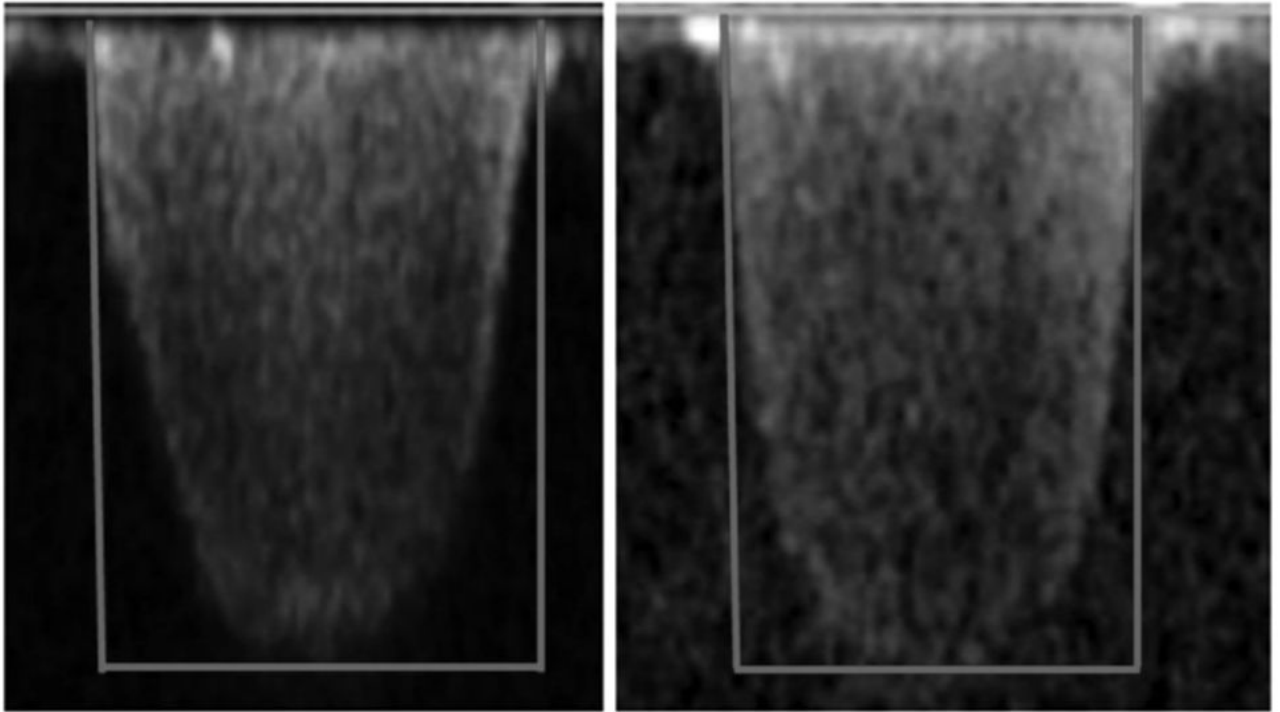


Figure 3. Continuous-wave Doppler regurgitant jet in a patient before CRT (right) and after CRT (left). Estimated closing pressure ratio increases from 0.682 to 0.894.

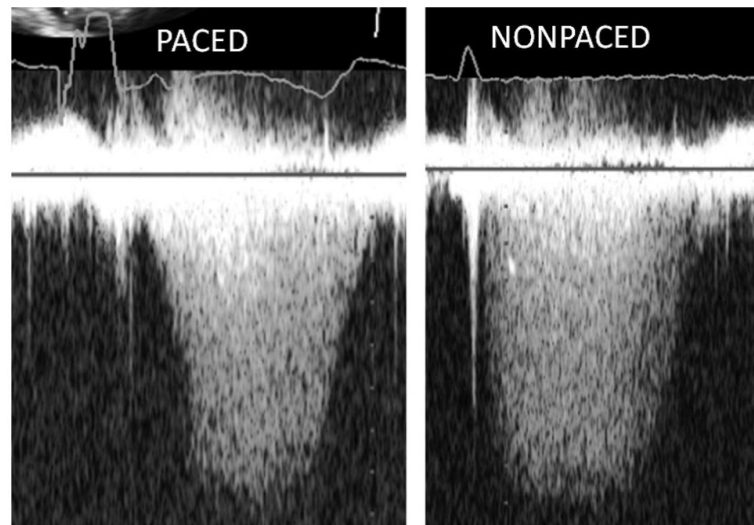


Figure 4. Continuous-wave Doppler regurgitant jet in paced (left) and nonpaced (right) patients. Estimated closing pressure ratio increases from 0.638 (paced) to 0.899 (nonpaced).

Table 1
Baseline Characteristics of the Study Population

Age, y	66±12
Sex, n (%)	
Male	23 (68)
Female	11 (32)
Origin, n (%)	
Ischemic	16 (47)
Nonischemic	18 (53)
NYHA functional class	
III	30 (88)
IV	4 (12)
Quality-of-life score	54±17
6-Minute walk test, m	284±143
Heart rate (BPM)	70±11
Mean blood pressure (mm Hg)	85±12

BPM indicates beats per minute.

Table 2
Echocardiographic Parameters at Baseline (Pre-CRT) and 6-Month Follow-Up (Post-CRT)

	Pre-CRT	Post-CRT	<i>P</i>
MR (RV-ml)	35±17	23±14	<0.001
EDV, mL	253±111	221±100	<0.001
ESV, mL	206±97	167±91	<0.001
EF, %	19±6	27±9	<0.001
MAA, cm ²	11.6±3.5	10.5±3.1	<0.001
MAA contr, %	4±0.9	8±0.6	0.1
TV, mL	5.7±2.6	4.6±2.2	<0.001
Leaflet closing area, cm ²	15.4±4	13.7±3.8	<0.001
Closing pressure ratio	0.77±0.1	0.84±0.1	0.01
dP/dt, mm Hg/s	534±202	794±362	<0.001
MTD, ms	102±34	108±36	0.2
Ts-SD, ms	36±13	40±14	0.07
SLD, ms	43±30	53±42	0.1
PMs Dys, ms	54±36	60±33	0.4

RV indicates regurgitant volume; TV, tenting volume; PMs Dys, interpapillary muscle dyssynchrony.

Table 3
Comparison of Echocardiographic Parameters at Baseline and 6-Month Follow-Up After CRT in the MR Reduction Group and the MR No-Reduction Group

	MR Reduction (n=18)		MR No-Reduction (n=16)		P
	Pre-CRT	Post-CRT	Pre-CRT	Post-CRT	
MR (RV-ml)	43±13	18±10	26±17*	29±15	0.008
EDV, mL	265±88	228±77	239±134	215±134	0.02
ESV, mL	216±78	167±81	195±118	168±113	0.004
EF, %	19±5	28±10	20±7	24±12	0.03
MAA, cm ²	12.4±3.2	11±3.4	10.8±3.9	10±2.8	0.1
MAA contr, %	3.9±0.7	7.8±0.5	4.2±1	8.8±0.7	0.3
TV, mL	6.4±2.5	4.8±2.4	5±2.8	4.6±2.1	0.1
Leaflet closing area, cm ²	16.9±3.8	14.5±4.1	14.2±4	13.1±3.6	0.2
Closing pressure ratio	0.77±0.04	0.85±0.1	0.78±0.1	0.81±0.1	0.2
dP/dt, mm Hg/s	548±227	867±447	519±181	750±264	0.01

RV indicates regurgitant volume; TV, tenting volume.

P compares pre-CRT versus post-CRT

* P<0.05 (pre-CRT MR reduction versus pre-CRT MR no reduction).

Table 4
Comparison of Echocardiographic Parameters at Baseline and 6-Month Follow-Up After CRT in Responders and Nonresponders to LV Reverse Remodeling

	Responder (n=21)		P	Nonresponder (n=13)		P
	Pre-CRT	Post-CRT		Pre-CRT	Post-CRT	
MR (RV-ml)	38±17	23±17	<0.001	29±10	24±6	0.2
EDV, mL	247±84	195±66	<0.001	262±148	265±130	0.6
ESV, mL	203±73	140±54	<0.001	212±130	210±120	0.7
EF, %	19±6	29±10	<0.001	20±6	22±9	0.2
MAA, cm ²	11.5±3	9.9±2.6	<0.001	11.7±4.4	11.3±3.8	0.3
MAA contr, %	4±0.4	7±0.5	0.2	4±1	9±0.7	0.3
TV, mL	5.9±2.4	4.5±1.8	<0.001	5.3±3.1	4.8±2.4	0.1
Leaflet closing area, cm ²	15.6±3.8	13±3.2	<0.001	15.1±5.3	14.6±4.5	0.5
Closing pressure ratio	0.74±0.11	0.81±0.11	0.04	0.82±0.08	0.87±0.13	0.1
dP/dt, mm Hg/s	491±191	838±357	0.01	590±211	729±230	0.1

RV indicates regurgitant volume; TV, tenting volume.

P compares pre-CRT versus post-CRT.