

The role of cardiac magnetic resonance imaging in differentiating the underlying causes of left ventricular hypertrophy

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The onset of sudden cardiac death and large inter- and intra-familial clinical variability of hypertrophic cardiomyopathy pose an important clinical challenge. Cardiac magnetic resonance imaging is a high-resolution imaging modality that has become increasingly available in the past decade and has the unique possibility to demonstrate the presence of fibrosis or scar using late gadolinium enhancement imaging. As a result, the diagnostic and prognostic potential of cardiac magnetic resonance imaging has been extensively explored in acute and chronic ischaemic cardiomyopathy, as well as in several nonischaemic cardiomyopathies.

This review aims to provide a critical overview of recently published studies on hypertrophic cardiomyopathy and discusses the role of cardiac magnetic resonance imaging in differentiating underlying causes of hypertrophic cardiomyopathy, such as familial hypertrophic cardiomyopathy, cardiac involvement in systemic disease and left ventricular hypertrophy due to endurance sports. Also, it demonstrates the use of cardiac magnetic resonance in risk stratification for the onset of sudden cardiac death, and early identification of asymptomatic family members of hypertrophic cardiomyopathy patients who are at risk for the development of hypertrophic cardiomyopathy. (Neth Heart J 2010;18:135-43.)

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This review will focus on the clinical applicability of cardiac magnetic resonance (CMR) to determine the underlying cause of different forms of hypertrophic cardiomyopathy (HCM). According to the recent position statement of the European Society of Cardiology, HCM is to be subdivided into familial and nonfamilial forms. Since considerable overlap in aetiology may exist between HCM and restrictive cardiomyopathy (RCM), several causes of RCM will also be briefly discussed.¹

Hypertrophic cardiomyopathy

The clinical diagnosis of HCM is based on the presence of left ventricular (LV) hypertrophy in the absence of increased afterload, such as systemic hypertension or aortic stenosis. The prevalence of HCM in the general population is estimated at 1:500, indicating that in the Netherlands, approximately 33,000 people have HCM. An overview of recent CMR studies on HCM is presented in table 1. The nonpathological form of LV hypertrophy, as observed in athletes, can be distinguished from pathological hypertrophy, based on the maximal end-diastolic wall thickness to volume ratio.² An end-diastolic wall thickness to volume ratio <0.15 mm⋅m²⋅ml⁻¹ – which was calculated by dividing the maximal end-diastolic wall thickness by indexed LV end-diastolic volume − was found to have a 99% specificity to differentiate an athlete's heart from pathological hypertrophy.

Familial HCM

Familial HCM is mainly caused by mutations in genes which encode for sarcomeric proteins that have an autosomal dominant pattern of inheritance. Histologically, HCM is characterised by myocyte disarray, hypertrophy and interstitial fibrosis, which predominantly results in diastolic dysfunction, and may serve as a substrate for ventricular arrhythmias.³ HCM accounts for at least 25% of sudden cardiac death (SCD) in young athletes, and is sometimes

Design=study design, n=patient number, SC=single centre, P=prospective, C=cross-sectional, LGE=late gadolinium enhancement, HCM=hypertrophic cardiomyopathy, LV=left ventricular, PPV=positive predictive value, NPV=negative predictive value, L=longitudinal, CMR= cardiac magnetic resonance.

the first symptom of disease.⁴ Since CMR has a high spatial and temporal resolution and may determine myocardial tissue characteristics such as lipomatous metaplasia and fibrosis, its role in early identification of HCM mutation carriers without LV hypertrophy, in diagnosing HCM, and in risk stratification for SCD in HCM patients has been extensively explored.

Early identification of HCM mutation carriers CMR cine imaging can be used to evaluate myocardial structure in HCM mutation carriers. With CMR cine imaging, structural abnormalities described as crypts of the inferoseptum were recently found in 80 to 90% of HCM mutation carriers, in whom no hypertrophy was present.^{5,6} These crypts were only visible on an end-diastolic dedicated image plane through the inferoseptum (figure 1A). While a single crypt or paired crypts have also occasionally been described in a referral-based population without HCM, it is likely, yet unproven, that crypts are the macroscopic representation of myocyte disarray since mild forms of disarray are known to occur in the inferoseptum in the general population.⁷ Additionally, very prominent crypts can also be observed with 2D echocardiography.⁸ Of note, as a sign of probable HCM mutation carriership, these crypts should be carefully discriminated from hypertrabecularisation of the myocardium, which is not typically found in HCM mutation carriers (figure 1B).

Beside structural abnormalities, HCM mutation carriers also exhibit reduced systolic and early diastolic mitral valve annulus velocities in septal and lateral segments prior to the development of manifest HCM. These characteristics can be measured by both echocardiography (using tissue Doppler imaging) and CMR (using a phase-contrast imaging technique).⁹⁻¹¹ With phase contrast imaging, static tissue remains grey and tissue that moves at relatively high velocities appears as very bright or dark, depending on the direction of movement (figure 3). This technique is generally used for blood flow quantification, but can also be accurately employed to measure (diastolic) myocardial velocities.12 Therefore, this CMR technique may serve as an alternative to echocardiographic tissue Doppler imaging.

Measurement of LV wall thickness in hypertrophic cardiomyopathy

Although HCM is generally diagnosed with 2D echocardiography, a direct comparison between CMR and 2D echocardiography revealed that the diagnostic accuracy of CMR to identify HCM patients among a group of patients with suspected HCM was higher than 2D echocardiography.¹³ CMR identified HCM in 6% of patients who would otherwise remain undetected by 2D echocardiography. With echocardiography, the magnitude of hypertrophy in the basal lateral wall and the presence of extreme hypertrophy (>30 mm) were underestimated in 20 and 10% of patients respectively.

Risk assessment of sudden death in hypertrophic cardiomyopathy

Risk stratification for SCD involves the assessment of five clinical risk factors:

- 1. Extreme LV hypertrophy (>30 mm);
- 2. Blunted blood pressure response to exercise in patients younger than 40 years;
- 3. A family history of SCD;
- 4. Unexplained syncope;
- 5. Nonsustained ventricular tachycardia on 24 hour Holter monitoring.¹⁴

The occurrence of ventricular arrhythmias and subsequent SCD in HCM patients has been reported to be associated with an increased amount of fibrosis per LV segment.³

Fibrosis can be detected *in vivo* with CMR using late gadolinium enhancement (LGE) imaging. The most widely used CMR contrast agent is gadolinium chelate. This contrast agent is readily washed out of normal myocardium, but resides in areas of myocardium with increased extracellular space, e.g. where large amounts of interstitial fibrosis or scar tissue are present.¹⁵

In HCM patients, the areas with contrast enhancement (LGE) are predominantly localised at the insertion points of the right ventricle into the LV and are related to increased amounts of local collagen deposits and oedema.^{16,17} The pattern of LGE is often described as patchy or confluent and found in approximately 80% of HCM patients

Figure 1. Cardiac magnetic resonance cine images. A) Modified two-chamber end-diastolic cine image through the inferoseptum of a hypertrophic cardiomyopathy mutation carrier. Crypts are present in the basal inferoseptum (denoted by white arrowheads) penetrating compact myocardium and can easily be distinguished from noncompaction cardiomyopathy. B) Two-chamber cine imaging in a patient with noncompaction cardiomyopathy. The noncompacted layer aligning a compact layer is most profound in the apical region, and sometimes extends towards the inferior and/or lateral regions, as illustrated by the white arrowheads. LV= left ventricle.

Figure 2. Short-axis left ventricular late gadolinium enhancement images of two HCM patients. Note that the fibrotic burden in patient B (confluent type LGE) is much more extensive than in patient A (patchy type LGE), which is related to increased risk of ventricular arrhythmias. Typically, late gadolinium enhancement (white arrowheads) is located at the insertion points of the right ventricle into the septum, see patient A. This pattern is observed in approximately 80% of HCM patients. LV=left ventricle.

(figure 2).18 Indeed, LGE is more often found in HCM patients with documented ventricular arrhythmias on Holter monitoring and is associated with an increased number of contrast enhanced LV segments and lower LV ejection fractions.¹⁹⁻²¹ Moon and colleagues found that the extent of LGE was higher in patients with two or more clinical risk factors for SCD.20 Interestingly, LGE, as well as clinical risk factors for SCD, are also found in HCM mutation carriers without overt hypertrophy.5,22 Although these data suggest a relation between LGE and the onset of ventricular arrhythmias/SCD, only single-centre, cross-sectional data are available. To further elucidate the prognostic value of LGE in HCM patients, longitudinal, multicentre studies are warranted. At this point, HCM patients with LGE cannot be considered at increased risk for ventricular arrhythmias/ SCD per se, but the presence of LGE in HCM may be used as an arbitrator when ambiguity on ICD implantation remains after consideration of clinical risk factors.

Nonfamilial HCM

Many systemic disorders are associated with HCM, of which diabetes, end-stage renal disease, amyloidosis and lysosomal storage diseases are most frequently reported as underlying causes. The most important role of CMR in the diagnosis of patients with acquired HCM lies within the differentiation of the underlying systemic diseases, which is important for the choice of treatment and prognosis.

Diabetic cardiomyopathy

Diabetic cardiomyopathy is diagnosed by finding LV hypertrophy and diastolic dysfunction in the absence of obstructive coronary artery or valvular disease in patients with diabetes. The proposed mechanisms through which cardiomyopathy develops in patients with diabetes include a deranged cardiomyocyte metabolism and calcium homeostasis, concomitant systemic hypertension and endothelial dysfunction.²³

The findings of recent CMR studies suggest that the development of LV hypertrophy in diabetics is race dependent and coheres with systemic hypertension and obesity.23-25 This may not only result in subclinical diastolic, but also systolic dysfunction in type 1 and type 2 diabetes patients, as demonstrated in CMR studies using a dedicated CMR technique called myocardial tissue tagging.^{26,27} Myocardial tissue tagging allows visualisation and quantification of the regional deformation of the myocardium as well as global twist/untwist dynamics of the LV, and has proven to be more sensitive in the evaluation of regional function than wall thickening (figure 3).28 In patients with type 1 diabetes, a CMR tagging study evaluating the twist/untwist dynamics found that twisting rate was increased irrespective of heart rate, and may represent the early detrimental effects of diabetes on myocardial function. Thus far, no studies describe typical patterns of LGE in diabetics. Although the capability to detect subclinical myocardial disease in diabetics with CMR may allow timely initiation of therapy, the relation between subclinical LV dysfunction and clinical outcome in diabetic patients is yet to be elucidated.

Figure 3. Cardiac magnetic resonance functional images. A) Short-axis, phase-contrast magnitude image, displaying the anatomical information. Magnitude images are used to define the regions of interest for velocity quantification. B) Matching flow encoded, phase-contrast image. Tissue moving at low velocities has an intermediate signal intensity (grey) and tissue moving at high velocities has either a low signal intensity (black) or high signal intensity (white), depending on the direction of movement. Regions of interest can be drawn on the myocardium (dashed circle) and in the mitral valve orifice (solid circle) in every phase of the cardiac cycle. C) From these data, myocardial velocity (dashed line) and mitral valve inflow curves (solid line) can be derived for analysis of systolic and diastolic function. D) Short-axis end-diastolic myocardial tissue tagging image. At this point in the cardiac cycle, a horizontal and vertical tagging pattern is applied on the myocardium. E) This tagging pattern deforms concomitantly with the in plane deformation of the myocardium throughout the entire cardiac cycle. The temporal resolution may reach up to 14 ms. From the deformation in two orthogonal directions, strain and rotation in every direction can be calculated. F) Circumferential strain is most frequently used for analysis of myocardial deformation. LV=left ventricle.

Uraemic cardiomyopathy in end-stage renal failure In patients with end-stage renal failure (ESRF), LV hypertrophy is commonly diagnosed in the presence of conventional risk factors for the development of LV hypertrophy. Uraemic cardiomyopathy is defined by the presence of LV hypertrophy, dilation and systolic dysfunction. Also, increased interstitial fibrosis is found in ESRF patients.29,30 Experimental studies suggest direct cardiotoxicity of uraemia, but the circulatory abnormalities associated with ESRF such as aortic stiffening, coronary atherosclerosis with prominent calcification, and volume overload due to anaemia, may well account for the specific phenotype of uraemic cardiomyopathy. LGE is present in 29% of ESRF patients, and related to an increased number of conventional risk factors for ischaemic heart disease.29

Although these data illustrate that LGE imaging may serve as a valuable adjunct to the diagnostic work-up of ESRF, recent reports show that the use of gadolinium-based contrast agents is associated with increased prevalence of nephrogenic systemic sclerosis in these patients.³¹ Therefore,

LGE imaging should only be performed in ESRF patients when no diagnostic alternatives are available. Then, it may be prudent to institute prompt dialysis after LGE imaging. Of notice, increased LV mass and dimensions are strongly associated with increased risk of cardiovascular death in ESRF patients; therefore, CMR may be used for LV volume and mass measurement in the clinical follow-up of ESRF patients.³²

Amyloidosis

Cardiac amyloid protein deposition frequently involves primary (AL-type) and secondary amyloidosis and is a major determinant of prognosis. Approximately 50% of patients with amyloidosis die from heart failure or ventricular arrhythmias.³³ In senile amyloidosis, which results from wild-type transthyretin deposition, cardiomyopathy is usually the sole manifestation of disease. When cardiac involvement with heart failure is present, median survival in AL-type amyloidosis is 0.8 years and in senile amyloidosis approximately five years.^{34,35} The gold standard for diagnosing cardiac involvement of amyloidosis is endomyocardial biopsy, but the procedure exposes the patient to a small but considerable risk. Observing an increased intraventricular wall thickness with echocardiography or CMR in combination with a low voltage electrocardiogram has a sensitivity of 72% and specificity of 91%, and yields a positive predictive value of 79% and negative predictive value of 88% to diagnose cardiac involvement in amyoloidosis.36

In addition, cardiac involvement of amyloidosis displays a characteristic pattern of LGE on LGE imaging if the images are acquired four minutes after injection of contrast agent (figure 4). LGE is found in approximately 70% of patients.37,38 This ill-defined, generally subendocardial pattern of LGE matches the distribution of the amyloid deposition.39 Although most profound in the subendocardial layer of the myocardium, amyloid deposition occurs throughout the entire myocardium, and therefore has a higher T1 signal than normal myocardium. The typical pattern of late enhancement on LGE imaging, together with the increased T1 signal of myocardium, yield a diagnostic accuracy of 97% in patients with cardiac involvement in biopsy-proven amyloidosis, as determined with echocardiography.39

Whether CMR is more sensitive than echocardiography in detecting cardiac involvement in amyloidosis remains to be explored. To detect LV hypertrophy in patients suspected with cardiac involvement in amyloidosis, CMR can be considered an alternative to echocardiography. However, to additionally perform LGE imaging in these patients has shown to be clinically relevant, since the presence of LGE helps to confirm the diagnosis and

also the difference in T1 signal between epicardial and subendocardium is of prognostic importance in cardiac amyloidosis.37,38 A higher T1 signal in LGE imaging indicates higher amyloid deposition. When amyloid deposition is mainly present subendocardially, than T1 difference between subendocardium and subepicardium is high. When amyloid burden increases, amyloid deposition in the subepicardium occurs, and as a result the difference in T1 signal is lower. Maceira and colleagues found that patients with a T1 difference higher than 23 ms had an improved survival.37

Anderson-Fabry disease

Anderson-Fabry disease is the second most prevalent lysomal storage disease resulting from an Xlinked recessive disorder of glycosphingolipid metabolism. Cardiac involvement is common, resulting from glycosphingolipid within the cardiomyocytes, valves and vascular endothelium, ultimately resulting in HCM. Although generally believed to be a rare disorder, recent studies on the prevalence of this treatable cause of HCM showed that Anderson-Fabry disease was the underlying cause of disease in 3 to 6% of middle-aged men in an HCM referral population.^{40,41}

Histological studies on cardiac involvement mainly report intra-cardiomyocytal inclusions within the lysosomes with typical concentric lamellar configuration. However, LGE in Andersen-Fabry disease likely represents replacement scarring and typically occurs in the midventricular and epicardial layers of basal inferolateral wall in 92% of patients.⁴² Again, the pattern of LGE is more ill defined compared with scarring found after myocardial infarction.

Figure 4. Cardiac magnetic resonance late gadolinium enhancement imaging. A) Two-chamber view of an amyloidosis patient with cardiac involvement. Note the global, subendocardial, ill-defined late gadolinium enhancement that is found in approximately 70% of patients (see arrowheads). B) Short-axis T2 weighted image of the left ventricle. Signal intensity of the septum has rapidly decayed, yielding a dark tone (solid circle) while signal intensity of the liver (dashed circle) is preserved. This demonstrates the poor correlation between T2* values of the liver and the heart.*

Restrictive cardiomyopathy

Cardiac iron overload

In patients with iron overload, caused by increased intestinal iron absorption (haemochromatosis) or by increased erythrocyte destruction and transfusional siderosis in thalassaemia, heart failure is the most common cause of death.⁴³ Cardiomyopathy probably results from the toxic effects of nontransferrin bound iron on the mitochondrial respiratory chain when the cardiac iron storage capacity is exhausted. This form of cardiomyopathy is reversible with chelate therapy, provided therapy is initiated before heart failure develops.44,45

However, the diagnosis of cardiac iron overload is often delayed due the relatively late onset of symptoms, echocardiographic abnormalities and unpredictability of development. Additionally, the extent of iron overload in the heart does not correlate with iron overload in the liver, which is usually employed in clinical practice as an indicator of systemic iron overload.44,45

With the CMR, the concentration of iron within the myocardium can be estimated by measuring the T2* relaxation time. This represents the velocity by which signal decay of tissue occurs on T2* weighted images (figure 4). The more rapid the signal decay, the more iron present. In myocardium, $T2*$ relaxation times $\langle 20 \rangle$ ms are found in patients with substantial cardiac iron overload and are strongly related to a decrease in LV ejection fraction.^{44,46} Therefore, repetitive T2* time measurement in patients at risk of cardiac iron overload allows timely initiation of chelate therapy and may prevent the development of heart failure.

Endomyocardial fibrosis

In hypereosinophilic syndrome, eosinophil-mediated endomyocardial fibrosis and subsequent RCM evolves through three stages: an acute necrotic stage which develops five to six weeks after the onset of illness, an intermediate stage in which thrombus formation along necrotic endocardium occurs in often asymptomatic patients, and a fibrotic stage. In the fibrotic stage, LV wall thickening by endomyocardial replacement scarring and thrombus formation can be observed with CMR, and warrants anticoagulation therapy. Also, this form of LV wall thickening can by discriminated from LV myocardial hypertrophy using LGE imaging, which reveals thickening of the endocardium and increased signal intensity, accompanied by LV cavity thrombus formation, indicated by black spots aligning the endocardium.47

Conclusions

Within the last decade, a large body of research has demonstrated the diagnostic accuracy of CMR, and the development of new sequences and techniques

holds promise for an increasing role of CMR in the diagnostic work-up and monitoring of nonischaemic cardiomyopathies. However, the majority of previous studies were single centre, and therefore its diagnostic accuracy in common practice is currently unknown. With the use of CMR, it is possible to noninvasively visualise crypts, fibrosis and oedema in HCM, to determine the cardiac involvement in systemic diseases including amyloidosis, and to measure the severity of iron overload. However, scarcity remains regarding the prognostic value of these findings and warrants further research.

To date, an increasing number of medical centres have embraced CMR as a standard diagnostic tool for diagnosis of both ischaemic and nonischaemic cardiomyopathies. Combined efforts of multiple medical centres to conduct the necessary long-term follow-up studies in patients with nonischaemic cardiomyopathies will ultimately allow us to answer the questions on the accuracy and prognostic value of CMR in patients with overt disease and those at risk to develop disease in day-to-day practice.

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E.E. van der Wall Chief Editor Netherlands Heart Journal