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Assessment of Myocardial Triglyceride Oxidation with PET

and ¹¹C-Palmitate

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Abstract

Background—The goal of this study was to test whether myocardial triglyceride (TG) turnover including oxidation of TG-derived fatty acids could be assessed with PET and ¹¹C-palmitate.

Methods and Results—26 dogs were studied fasted (FAST), during Intralipid infusion (IL), during a hyperinsulinemic-euglycemic clamp without (HIEG) or with Intralipid infusion (HIEG +IL). ¹¹C-palmitate was injected, and 45 min were allowed for labeling of myocardial TG pool. 3-D PET data were then acquired for 60 min, with first 15 min at baseline followed by 45 min during cardiac work stimulated with constant infusion of either phenylephrine (FAST, n=6; IL, n=6; HIEG +IL, n=6) or dobutamine (FAST, n=4; HIEG, n=4). Myocardial ¹¹C washout during adrenergic stimulation (AS) was fitted to a mono-exponential function (Km(PET)). To determine the source of this ¹¹C clearance, Km(PET) was compared to direct coronary sinus-arterial measurements of total ¹¹C activity, ¹¹C-palmitate, and ¹¹CO₂. Before AS, PET curves in all groups were flat indicating absence of net clearance of ¹¹C activity from heart. In both FAST groups, AS resulted in negligible net ¹¹C activity and ¹¹CO₂ production higher than net ¹¹C-palmitate uptake. AS with phenylephrine resulted in net myocardial uptake of total ¹¹C activity and ¹¹C-palmitate in IL and HIEG+IL, and ${}^{11}CO_2$ production lower than ${}^{11}C$ -palmitate uptake. In contrast, AS with dobutamine in HIEG resulted in net clearance of all ¹¹C metabolites (total ¹¹C activity, ¹¹C-palmitate and ¹¹CO₂) with ¹¹CO₂ contributing 66% to endogenous FA oxidation. AS resulted in significant Km(PET) in all groups, except HIEG+IL. However, positive correlation between Km(PET) and ¹¹CO₂ was observed only in HIEG (R²=0.83, P=0.09).

Conclusions—This is the first study to demonstrate that using PET and pre-labeling of intracardiac TG pool with ¹¹C-palmitate, noninvasive assessment of myocardial TG use is feasible under metabolic conditions that favor endogenous TG use such as increased metabolic demand (β -adrenergic stimulation of cardiac work) with limited availability of exogenous substrate (HIEG).

Keywords

myocardial triglyceride turnover; 3-D PET; ¹¹C-palmitate; β -adrenergic stimulation; monoexponential clearance

Introduction

Long-chain fatty acids (FA) are the primary energy source for the heart 1,2 . In the healthy heart, 70–90% of the FA entering the cell are immediately oxidized, with the remaining 10–30%

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stored in the intracardiac triglyceride (TG) pool ³⁻⁵. These stores serve as a buffer that compensates for short-term differences in FA supply and lipid oxidative demand, and provide FA when plasma FA concentrations reach low levels ⁶. Due to its small mass, the turnover of myocardial TG is quick ⁷, and is inversely related to the concentration of exogenous FA ⁴, ⁸⁻¹⁰. In normal perfused rat hearts, 11% of mitochondrial ATP production is attributed to oxidation of the myocardial TG-derived FA ^{4,11}, increasing to 50% when exogenous energy sources are limited ⁴. Myocardial TG turnover can be rapidly accelerated by adrenergic stimulation ¹²⁻¹⁸.

The contribution of endogenous TG-derived FA to overall energy metabolism appears to be altered in various animal models of cardiac disease. For example, in failing rat hearts endogenous TG, measured with ¹³C-magnetic resonance spectroscopy, is not oxidized even though exogenous palmitate oxidation is unchanged ¹⁹. In contrast, TG turnover provides up to 70% of the ATP production in uncontrolled diabetes ^{10,20} and during reperfusion of ischemic hearts ⁵. High levels of TG in the heart cause diminished contractile function, hypertrophy, and myocyte death ²¹⁻²³. Therefore, lipolysis of intracardiac TG might also play an important physiologic role by protecting the heart from deleterious effects of surplus lipid accumulation.

Relatively little is known about regulation of myocardial TG metabolism in humans in either health or disease. This is primarily due to the lack of adequate methods for its measurement ^{7,24-26}. At least in theory, myocardial lipolysis can be quantified based on the rate of glycerol release from the heart measured with arterio - coronary sinus balance ²⁷. This method, however, requires the tenuous assumptions that all lipolysis is complete (i.e., hydrolysis of one TG molecule yields one glycerol molecule) and that the heart cannot oxidize glycerol. In any case, it is too invasive for routine use. Recently, ¹H-MRS was used to detect myocardial TG content and net lipolysis ²⁸⁻³². However, this approach does not allow for estimation of the rate of the TG turnover. On the other hand, to date the most common method for noninvasive measurement of myocardial FA metabolism is compartmental modeling of PET kinetics of ¹¹C-palmitate ³³⁻³⁷. However, this approach measures only metabolism of exogenous FA and does not account for the contribution from the intracardiac TG pool.

Accordingly, the goal of this study was to investigate the feasibility of assessing myocardial TG turnover non-invasively using PET and 1-¹¹C-palmitate. To do so, we pre-labeled the myocardial TG pool with ¹¹C-palmitate and, taking advantage of the higher sensitivity of 3-D (or septaless) PET ³⁸, measured the rate of ¹¹C washout from the myocardium during adrenergic stimulation in a well-controlled canine model studied over a wide range of substrate and hormonal conditions. To determine the source of the PET ¹¹C clearance, direct coronary sinus – arterial measurements of the total ¹¹C, ¹¹C-palmitate and ¹¹CO₂ counts were analyzed and compared with clearance rate of PET ¹¹C activity.

Materials and Methods

Animal Preparation

All animal experiments were conducted in compliance with the Guidelines for the Care and Use of Research Animals established by Washington University's Animal Studies Committee. Purpose bred 6.2-9.8 kg (7.65 $\pm 0.88 \text{ kg}$) male beagle dogs were fasted, anesthetized and instrumented as reported previously ^{39,40}. One femoral vein was cannulated to administer drugs. Catheters were placed in the thoracic aorta via the femoral arteries for arterial sampling and monitoring of arterial blood pressure. To obtain venous blood samples, a coronary sinus catheter was placed via the right external jugular vein under fluoroscopic guidance as previously described ³⁷. The ECG, arterial blood pressure and heart rate were monitored throughout the study.

To achieve a wide range in myocardial use and oxidation of endogenous TG, twenty six dogs were studied under various conditions established 60 min prior to tracer injection. Ten dogs were studied after overnight fasting (FAST). To increase myocardial FA uptake, a continuous infusion of 20% Intralipid (IL) (Fresenius Kabi Clayton, LP; 1 mL/min) was administered in six dogs. To switch myocardial substrate metabolism from primarily FA to glucose use, a hyperinsulinemic-euglycemic clamp (HIEG) was performed in ten dogs, using a continuous infusion of insulin (70 mU/kg/h) along with an adjustable infusion of 20% dextrose ³⁵. To assess the effect of competing exogenous substrates on the accuracy of the measurement of TG turnover, six of the ten HIEG dogs received concomitant administration of IL (HIEG+IL). Since we wanted to investigate whether an acute increase in cardiac work alone was sufficient to stimulate myocardial TG mobilization, or whether direct activation of lipolysis was required as well, cardiac work was stimulated with either phenylephrine or dobutamine. Accordingly, in six FAST, and all IL and HIEG+IL dogs, cardiac work was increased with phenylephrine (0.84 - 1.6 ug/kg/min). In four FAST and all HIEG dogs, cardiac work was increased with dobutamine (20 μ g/kg/min). The difference in these interventions was based on the fact that unlike phenylephrine, dobutamine stimulates lipolysis. Therefore to be able to compare these two groups, IL infusion was added to HIEG to mimic peripheral lipolysis during adrenergic stimulation with phenylephrine.

Experimental Protocol

All PET studies were performed on a microPET 220 (Concorde Microsystems Inc.) which operates solely in 3-D mode. After a position scan, a bolus of 1110 - 1480 MBq of ¹¹C-palmitate was injected, and 45 min were allowed ⁴¹ to minimize uptake and oxidation of ¹¹C-palmitate and maximize ¹¹C labeling of myocardial TG. Continuous dynamic PET data acquisition was started after this waiting period. To determine the basal rate of ¹¹C clearance from the myocardium, data were collected for 15 min while the heart was at rest. Cardiac work was then increased with a constant infusion of either phenylephrine (0.84 and 1.6 µg/kg/min) or dobutamine (20 µg/kg/min), which was continued throughout the rest of the study. Simultaneous arterial and coronary sinus blood samples for ¹¹C total activity and ¹¹C-palmitate administration during baseline (at 2, 10, and 45 min) and adrenergic stimulation (at 60, 62, 65, 70, 75, 85, 95 and 105 min). Another set of arterial and coronary sinus blood samples were collected at 0, 10, 45 and 85 min for plasma substrates (glucose, free FA, and lactate) and insulin levels, blood gases, pH, hematocrit and hemoglobin.

Measurements of Unlabeled Plasma Substrates

Plasma glucose and lactate levels were assayed enzymatically with a 2300 STAT Plus Analyzer (YSI Life Sciences, Yellow Springs, OH). Plasma free FA levels were measured using an enzymatic colorimetric method (Wako NEFA C kit, Wako Chemicals USA, Richmond, VA). Plasma insulin was measured by radioimmunoassay (Linco Research Co., St. Charles, MO).

Measurements of Plasma ¹¹C-Palmitate and its Metabolites

Plasma ¹¹C total activity was measured on a gamma counter in counts/mL/min. All directly measured arterial and coronary sinus ¹¹C data were normalized to injected dose as well as decay corrected by time lapsed from tracer injection to blood sampling time. The contribution of ¹¹CO₂ and ¹¹C-palmitate to total ¹¹C radioactivity in each of the arterial and coronary sinus samples was determined quantitatively as previously described ³⁵. As we were interested only in clearance of pre-labeled intramyocardial TG, total myocardial ¹¹C activity, ¹¹C-palmitate and ¹¹CO₂ were calculated as their coronary sinus minus arterial counts. The positive differences were considered as myocardial clearance of the corresponding measurements, while negative values indicated myocardial uptake of tracer.

PET Image Analysis

Myocardial ¹¹C-palmitate transaxial composite PET images (10-60 min) were summed to place myocardial regions of interest. To minimize contamination from septum and liver, eight regions of interest for each study were placed on the anterior (n=4) and lateral (n=4) walls and traced into each dynamic frame to generate myocardial ¹¹C time activity curves. To investigate whether myocardial clearance of PET ¹¹C-activity during adrenergic stimulation reflected oxidation of endogenous TG, time activity curves for each region corresponding to the first 30 min of adrenergic stimulation were fitted to a mono-exponential function. Due to low ¹¹C activity after 45 minutes of PET data acquisition which led to increased data noise, the last 10 to 15 min of data collection were excluded from analysis.

For each intervention, the estimated rate constants, Km(PET) (min⁻¹), were averaged to generate a mean rate constant per study and compared to myocardial net ¹¹C activity, ¹¹C-palmitate and ¹¹CO₂ direct measurements obtained from arterial and coronary sinus sampling.

Statistical Analysis

All data are presented as mean \pm SD. Differences in myocardial total ¹¹C activity, ¹¹C-palmitate or ¹¹CO₂ measurements between pre- and post adrenergic stimulation for a given intervention were compared by means of two-way analysis of variance (ANOVA) for repeated measurements, where the post-hoc Scheffé test was used to localize differences among measurements. Correlations between Km(PET) and ¹¹C-palmitate or ¹¹CO₂ measurements were done by linear regression. A P value of < 0.05 was considered statistically significant.

Results

Hemodynamics

Hemodynamic data are shown in Table 1. At baseline, heart rate and diastolic blood pressure were comparable across groups except in HIEG+IL, where both parameters were highest (P < 0.05 vs. dobutamine FAST). Systolic blood pressure was the highest in HIEG group (P < 0.05 vs. IL). There were no significant differences in rate pressure product among the study groups.

Adrenergic stimulation resulted in an overall increase in all hemodynamic measurements (Table 1, BL vs. AS P < 0.0001). Post-hoc analysis showed that compared to baseline, adrenergic stimulation resulted in (1) increased heart rate in dobutamine FAST only; (2) increased systolic blood pressure in all groups; (3) increased diastolic blood pressure in phenylephrine but not dobutamine groups, and (4) increased rate pressure product in all except HIEG group. Phenylephrine increased the rate pressure product via increases in blood pressure, while dobutamine-induced increases in rate pressure product were due to increases in both heart rate and systolic blood pressure. Rate pressure product was higher during dobutamine than during phenylephrine infusion (ANOVA P < 0.0001, 18,073 ± 5,840 vs. 12,503 ± 3,744, P < 0.01).

Plasma Substrate and Insulin Levels

Arterial plasma levels of substrate and insulin for all interventions are presented in Table 2. Adrenergic stimulation resulted in an overall increase in plasma glucose levels, with baseline levels lowest in the FAST groups (P < 0.05 vs. IL) and no differences among interventions during adrenergic stimulation. At baseline, plasma lactate concentrations were highest in the IL group (P < 0.005 vs. HIEG and both FAST groups). During adrenergic stimulation, while lactate levels remained significantly higher in the IL group, overall lactate levels were not different from baseline. There was a weak but significant increase in plasma FA during adrenergic stimulation (P=0.04). Plasma FA levels by design were highest in IL and HIEG+IL (P < 0.05 vs. HIEG and both FAST groups) during both baseline and adrenergic stimulation.

Plasma insulin levels by design were highest in HIEG and HIEG+IL groups (P < 0.05 vs. IL and both FAST groups) during both baseline and adrenergic stimulation. However, adrenergic stimulation did not alter baseline plasma insulin levels.

Direct Coronary Sinus - Arterial Measurements of Total $^{11}\mathrm{C}$ Activity, $^{11}\mathrm{C}$ -Palmitate and $^{11}\mathrm{CO}_2$

Figure 1 shows directly measured differences between coronary sinus and arterial plasma for total ¹¹C activity (black bars), ¹¹C-palmitate (open bars) and ¹¹CO₂ production (gray bars) as an average of values obtained at baseline (2, 10, and 45 min) pre-phenylephrine (Fig.1A) and pre-dobutamine (Fig.1C), and during adrenergic stimulation (60, 62, 65, 70, 75, 85, 95 and 105 min) with phenylephrine (Fig.1B) and dobutamine (Fig.1D).

Net uptake of total ¹¹C activity and ¹¹C-palmitate, shown as negative values, as well as ¹¹CO₂ production, shown as positive values, were observed in all five groups at rest, before adrenergic stimulation of cardiac work (Fig.1A and 1C), as well as in IL and HIEG+IL during phenylephrine stimulation (Fig. 1B). Interestingly, ¹¹CO₂ production in these groups never exceeded ¹¹C-palmitate uptake, suggesting that most if not all of the ¹¹CO₂ production was likely due to oxidation of exogenous FA. However, in both FAST groups, stimulation with either phenylephrine or dobutamine resulted in negligible total ¹¹C-activity exchange while ¹¹C-palmitate uptake was lower than ¹¹CO₂ production in both groups, suggesting oxidation of both exogenous ¹¹C-palmitate and endogenous myocardial TG-derived ¹¹C-palmitate. In contrast, in HIEG group (Fig.1D) we observed net release for all three ¹¹C measurements (total ¹¹C activity, ¹¹C-palmitate and ¹¹CO₂), with 2/3 of ¹¹C release accounted for by ¹¹CO₂ apparently produced from oxidation of myocardial TG-derived ¹¹C labeled FA.

PET Measurements during Adrenergic Stimulation

Figure 2 shows representative PET myocardial time activity curves (dots) before and during adrenergic stimulation with phenylephrine (Fig.2A-C) and dobutamine, mono-exponential fitting to PET clearance of myocardial ¹¹C activity during adrenergic stimulation (solid lines), and the corresponding clearance rates (Km, min⁻¹) (Fig. 2D-E). Before adrenergic stimulation, PET curves in all groups were nearly flat demonstrating a lack of net clearance of ¹¹C activity. During adrenergic stimulation with phenylephrine, PET Km(min⁻¹) rates were comparable in FAST and IL (0.002 ± 0.001 and 0.003 ± 0.003 , respectively, P = NS), and negligible in HIEG +IL (0.0004 ± 0.0005 , P = NS from zero).

In contrast, during dobutamine stimulation, PET Km(min⁻¹) rates were significantly higher than during phenylephrine stimulation of cardiac work (0.006 ± 0.003 vs. 0.002 ± 0.002 , P < 0.001) with comparable rates in both FAST and HIEG groups (0.006 ± 0.003 and 0.006 ± 0.003 , respectively, P = NS).

During phenylephrine stimulation, there was no significant positive correlation between Km (min⁻¹) and either ¹¹C activity, ¹¹C-palmitate or ¹¹CO₂ exchange (not shown). However, when individual dogs were examined, three in FAST, two in IL and two in HIEG+IL studies showed net clearance of ¹¹C activity with ¹¹CO₂ release greater than ¹¹C-palmitate uptake. Thus, in these studies ¹¹CO₂ production must have been due, at least in part, to oxidation of endogenous FA.

Figure 3 shows correlation between PET Km(min⁻¹) (y-axis) and the difference in directly measured coronary sinus and arterial plasma net myocardial ¹¹C activity (Fig. 3A, 3D), ¹¹C-palmitate (Fig. 3B, 3E) and ¹¹CO₂ (Fig. 3C, 3F) during cardiac work stimulated with dobutamine in FAST (Fig. 3A-C) and HIEG (Fig. 3D-F) groups.

In FAST studies, there was a strong trend toward significant correlation between Km(min⁻¹) and directly measured net total ¹¹C activity (Fig. 3A, P = 0.06), with no correlation between Km(min⁻¹) and ¹¹C-palmitate (Fig. 3B) or ¹¹CO₂ (Fig. 3C). While FAST studies averaged net uptake of ¹¹C-palmitate (Fig. 3B) and production of ¹¹CO₂ (Fig. 3C), ¹¹C-total net uptake was observed in two of the animals and net release in the other two (Fig. 3A). In the two studies with ¹¹C-activity release, uptake of net ¹¹CO₂ was also greater than ¹¹C-palmitate uptake, indicating that there was oxidation of both exogenous and endogenous sources of FA.

In contrast, in HIEG group in all four dogs, there was ¹¹C clearance resulting in correlative trend between PET Km(min⁻¹) and total ¹¹C activity (Fig. 3D, $R^2 = 0.64$, P = 0.2), but not with ¹¹C-palmitate (Fig. 3E). However, there was strong but not significant correlation between PET Km(min⁻¹) and ¹¹CO₂ (Fig. 3F: $R^2 = 0.83$, P = 0.09). These data in conjunction with the observations obtained from directly measured differences in coronary sinus and arterial plasma corroborate that PET clearance of ¹¹C activity during dobutamine-induced cardiac work in HIEG group can be attributed to myocardial ¹¹CO₂ production from oxidation of intracardiac ¹¹C labeled TG.

Discussion

To the best of our knowledge, to date non-invasive measurements of myocardial FA metabolism using PET and radionuclide tracers have been limited to measurements of exogenous FA uptake and metabolism, including oxidation and esterification of FA. In this study, we investigated for the first time whether TG turnover including TG degradation and oxidation could be assessed non-invasively with PET and ¹¹C-palmitate.

To do so, we used ¹¹C-palmitate to pre-label the myocardial TG pool of dogs studied under a wide range of substrate and hormonal conditions, and using 3-D PET, measured the rate of ¹¹C washout from the myocardium at baseline and during adrenergic stimulation. To determine whether the latter in fact represented mobilization of the intracardiac TG pool, we correlated the PET rate of ¹¹C clearance (Km(min⁻¹)) with directly measured arterial and coronary sinus total ¹¹C, ¹¹C-palmitate, and ¹¹CO₂ counts.

We found that before adrenergic stimulation, there was net uptake of total ¹¹C activity and ¹¹C-palmitate that exceeded ¹¹CO₂ production in all groups (Fig. 1A and 1C). In addition, flat PET curves were also observed in all groups indicating absence of net clearance of ¹¹C activity from heart (Fig. 2). Adrenergic stimulation with phenylephrine resulted in net myocardial uptake of total ¹¹C activity and ¹¹C-palmitate in IL and HIEG+IL while ¹¹CO₂ production was less than ¹¹C-palmitate uptake. This pattern suggested exogenous FA as the main source of FA oxidation. Adrenergic stimulation with either phenylephrine or dobutamine in FAST groups resulted in negligible net ¹¹C activity with net ¹¹C-palmitate uptake lower than ¹¹CO₂ production, suggesting oxidation from both exogenous and endogenous sources independent of the adrenergic stimulation used. In contrast, adrenergic stimulation with dobutamine in HIEG resulted in net clearance of all ¹¹C metabolites (total ¹¹C activity, ¹¹Cpalmitate and ¹¹CO₂), with ¹¹CO₂ contributing 2/3 to total ¹¹C washout suggesting that in this case ¹¹CO₂ production could be attributed exclusively to oxidation of endogenous TG.

To our knowledge, this is the first attempt to label the myocardial TG pool with ¹¹C by injection of ¹¹C-palmitate for subsequent imaging with PET. This approach differs significantly from how early kinetics of PET ¹¹C clearance have historically been used to assess myocardial oxidation of exogenous FA, in that we sought to quantify the very late kinetics of the tracer representing the metabolism of myocardial TG. This presented a challenge due to the short half-life of the tracer (20.2 min) compared to the time required to label the TG pool as well as to clear the heart of ¹¹CO₂ derived from direct oxidation of the injected ¹¹C-palmitate.

However, the 45-min waiting period between the injection of ¹¹C-palmitate and the beginning of the 3-D PET data acquisition was sufficient, as seen from the practically flat time activity curves before adrenergic stimulation during the first 15 min of each scan (Fig. 2A-E). This was true in all animals regardless of the conditions under which they were studied, e.g., in the fasted state vs. infused with glucose and insulin and/or Intralipid. This allowed us to determine whether adrenergic stimulation increased the rate of ¹¹C clearance from the myocardium. Since we wanted to investigate whether an acute increase in cardiac work alone was sufficient to stimulate myocardial TG mobilization, or whether direct activation of lipolysis was required as well, cardiac work was stimulated with either phenylephrine or dobutamine. Dobutamine, as a β_2 -agonist, has a direct lipolytic effect^{42,43} while the α_1 -agonist phenylephrine is an inhibitor of lipolysis ⁴⁴.

Although both agents increased cardiac work and stimulated PET clearance of ¹¹C from myocardium, phenylephrine infusion resulted in very low Km(PET) in FAST and IL groups (Fig.2A and 2B), with no significant PET clearance in HIEG+IL group (Fig.2C). In contrast, PET Km(min⁻¹) was 3 - 4 folds higher during dobutamine infusion (Fig.2D and 2E). At least in theory, this difference could be due to the fact that phenylephrine increased the rate pressure product by only ~40%, with this being mostly due to an increase in blood pressure, whereas dobutamine more than doubled the rate pressure product, as a result of increases in both heart rate and systolic blood pressure. These findings are expected given the higher inotropic effect of β -adrenergic agents⁴⁵. However, this differential response cannot explain the observed differences in PET clearance, because PET Km(min⁻¹) was still significantly higher (P < 0.05) in dobutamine-infused animals (0.006 ± 0.003 min⁻¹) than in phenylephrine-infused animals (0.002 ± 0.002 min⁻¹) even when the analysis was restricted to those with comparable rate-pressure products (16,526 ± 3,826 and 14,059 ± 3,915 beats/min/mmHg for seven dobutamine-and 13 phenylephrine-treated animals, respectively). Thus, these differences could be attributed to lipolytic effect of dobutamine that results in higher TG turnover.

Since the PET clearance of ¹¹C during adrenergic stimulation of cardiac work could have resulted from utilization of either exogenous ¹¹C-palmitate taken up from plasma or from endogenous intracardiac TG pre-labeled with ¹¹C-palmitate, we calculated the directly measured coronary sinus – arterial difference in total ¹¹C activity to determine whether there was a net uptake or net release of tracer. To determine the extent to which any net release of ¹¹C could be attributed to oxidation vs. egress of non-metabolized ¹¹C-palmitate released from endogenous TG, we also calculated coronary sinus - arterial differences in ¹¹CO₂ and ¹¹C-palmitate.

The lack of net ¹¹C release from the myocardium following phenylephrine administration in either of study group (Fig. 1B) did not allow for definitive identification of the source of the PET clearance under these conditions. However, analyzing the individual studies we found that in almost 1/3 of the studies there was ¹¹C clearance from myocardium with ¹¹CO₂ production greater than ¹¹C-palmitate uptake, suggesting that at least in part myocardium utilized endogenous intracardiac TG. Moreover, in two out of these seven dogs, we observed release from myocardium of not only total ¹¹C and ¹¹CO₂ but also intracardiac TG-derived ¹¹C-palmitate. Further attempts to determine under which metabolic conditions or level of cardiac work phenylephrine stimulated myocardial TG turnover fell short due to significant variability of metabolic and hemodynamic parameters among these experiments.

On the other hand, either negligible (FAST) or net release (HIEG) of total ¹¹C activity from the heart was observed during dobutamine stimulation (Fig. 1D), in keeping with the higher values for Km(PET) observed in these experiments (Fig. 2D and 2E). Further analysis of individual FAST dogs showed that in two animals with the highest levels of insulin (102 and 180 μ U) there was total ¹¹C net uptake, and in the other two with significantly lower insulin

levels (10.3 and 60 μ U) there was net ¹¹C release (Fig. 3A) ⁴⁶. ¹¹CO₂ production in FAST dogs was also greater than ¹¹C-palmitate uptake, indicating that there was oxidation of both exogenous and endogenous sources of FA. In contrast, release of all ¹¹C-metabolites in HIEG combined with correlation between Km and ¹¹CO₂ production, but not with either total ¹¹C or ¹¹C-palmitate, demonstrate that myocardial TG turnover could be successfully measured under conditions of enhanced cardiac work in the presence of low levels exogenous FA available for oxidation. Of note, the assumption that if there is net uptake, there could not be net clearance of tracer is valid only for averaged net measurements. However, it does not apply to PET dynamic data presented here, where myocardial tracer uptake is mostly represented in the early kinetics of the PET ¹¹C time-activity curves, while oxidation, as measured by the production of ¹¹CO₂, and potentially TG turnover, are mostly represented in the late kinetics of the PET curves. The fitting of a mono-exponential function to the late kinetics of PET ¹¹C activity should then be representative of these clearances, even in the presence of net tracer uptake.

There are, however, certain limitations to this method. This approach measures only clearance of the labeled TG and does not allow for the upstream estimation of myocardial TG pool. Therefore, this method provides only an index of myocardial TG turnover. However, we showed that PET clearance curves do reflect the myocardial TG turnover, and combined with the conventional PET protocol for measurement of myocardial exogenous FA metabolism, it may provide additional valuable information regarding the contribution of the endogenous myocardial TG to overall lipid metabolism in heart. Another limitation is the fact that due to confounding effects of continued myocardial uptake of exogenous ¹¹C-palmitate, the current method is unable to measure back-diffusion of TG-derived ¹¹C-palmitate originating from lipolysis. As a consequence, the assessment of total TG lipolysis (as opposed to the component that undergoes oxidation) is underestimated. The third limitation is the high dose/kg of 11 Cpalmitate used in this study that greatly exceeds the dose allowed for humans. In our study, we had to use high dose of short half-life tracer ¹¹C-palmitate (i.e., 20 min) because of the rather long (105 min = over 5 half-lives) protocol of this study. However, by the end of 45 min waiting period the ¹¹C curve reached the plateau, and it is possible that a shorter period could be sufficient for pre-labeling of myocardial TG pool. We also observed that the tracer washout in response to adrenergic stimulation occurred very fast, within approximately first 15 min. Therefore, it is possible to shorten the current protocol time to 60 min (35-40 min of pre-labeling of the TG pool, and data acquisition for 10 min at baseline and 20 min during adrenergic stimulation), and hence, the dose sufficient for this study could be decreased to a more acceptable 20-25 mCi. Further studies are required to determine whether these measurements can be obtained using a lower dose and imaging with newer and more sensitive human 3-D PET devices. Proven successful, this method can become useful as part of noninvasive basic research and human clinical studies designed to understand the role of myocardial TG turnover in the healthy and diseased heart, using metabolic interventions that result (1) in the storage and (2) in subsequent use of endogenous TG, such as HIEG + dobutamine. Thus, in order to detect alterations in myocardial TG turnover among different populations, clinical (or basic) metabolic studies, such as diabetic or obese patients vs. healthy controls, young vs. aging, or male vs. female subjects, could be implemented after pre-labeling of the TG pool and under the same metabolic intervention (i.e. HIEG clamp and β -adrenergic stimulation of cardiac work). The approach implemented in this study is a first and critical step for the future development of more sophisticated imaging and modeling approaches. These approaches may include multi-imaging/multi-tracer approaches that would combine established imaging methods to measure the TG pool, such as ¹H-MRS, and more advance PET kinetic approaches to assess the fate of the myocardial TG pool including back-diffusion of ¹¹C-palmitate derive from TG degradation and TG oxidation.

Conclusion

This is the first study to demonstrate that using PET and pre-labeling of intracardiac TG pool with ¹¹C-palmitate, noninvasive assessment of myocardial TG use is feasible under metabolic conditions that increase demand for substrate (β -adrenergic stimulation of cardiac work) while limit availability of exogenous FA (HIEG).

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Figure 1.

Directly measured averaged coronary sinus - arterial difference (CS-ART) for total ¹¹C activity (black bars), ¹¹C-palmitate (white bars) and ¹¹CO₂ (grey bars) before (A and C) and during adrenergic stimulation of cardiac work (B and D) with phenylephrine (A and B) and dobutamine (C and D). Data is presented as group mean \pm SD.



Figure 2.

Representative myocardial PET time activity curves (dots) and mono-exponential fitting (lines) of total PET ¹¹C activity (y axes) during adrenergic stimulation of cardiac work with phenylephrine (A-C) and dobutamine (D-E). Km - rate of ¹¹C clearance from myocardium.

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Figure 3.

Correlation between total ¹¹C clearance measured by PET (Km(PET) (y axes) (A-F) and averaged coronary sinus – arterial difference (x axes) of total ¹¹C activity (A and D), ¹¹C-palmitate (B and E), and ¹¹CO₂ (C and F) during adrenergic stimulation of cardiac work with dobutamine in FAST (A-C) and HIEG (D-F) studies. Negative values on x-axes indicate tracer uptake and positive values tracer clearance.

Table 1

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Fast (a=6) IL (a=6) HEG+IL (a=6) Fast (a=4) BL vs.AS HR bpm BL 96 ± 28 103 ± 17 $125 \pm 20^{\circ}$ 77 ± 15 92 ± 13 $P<0.0001$ HR bpm BL 96 ± 28 103 ± 17 $125 \pm 20^{\circ}$ 77 ± 15 92 ± 13 $P<0.0001$ As $92 \pm 18^{\circ}$ 112 ± 18 134 ± 19 149 ± 29 134 ± 55 $P<0.0001$ Sub multi BL 90 ± 13 79 ± 12 83 ± 11 101 ± 14 $103 \pm 21^{**}$ $P<0.0001$ Sub multi BL 90 ± 13 79 ± 12 83 ± 11 101 ± 14 $103 \pm 21^{**}$ $P<0.0001$ Sub multi BL 136 ± 31 102 ± 24 112 ± 24 117 ± 6 $P<0.001$ But multi BL 55 ± 8 49 ± 10 $44 \pm 10^{**}$ 52 ± 9 $P<0.001$ All multi BL 55 ± 8 $92 \pm 10^{**}$ $P<0.001$ $P<0.001$ All multi BL 92 ± 10 102 ± 24 $P<0.001$ $P<0$			AS: Phenylephr	ine		AS: Dobutamin	e	2-way ANO	VA	
HR bpm BL 96 ± 28 103 ± 17 $125\pm20^{*}$ 77 ± 15 92 ± 13 $P<0.0001$ AS $92\pm18^{*}$ 112 ± 18 12 ± 12 12 ± 12 21 ± 55 $P<0.0001$ SBP mm Hg BL 90 ± 13 79 ± 12 83 ± 11 101 ± 14 $103\pm21^{**}$ $P<0.0001$ SBP mm Hg BL 90 ± 13 79 ± 12 83 ± 11 101 ± 14 $103\pm21^{**}$ $P<0.0001$ AS 136 ± 31 102 ± 24 112 ± 24 117 ± 6 $142\pm11^{**}$ $P<0.0001$ DBP mm Hg BL 55 ± 8 49 ± 10 $41\pm10^{*}$ 62 ± 9 $60\pm15^{*}$ $P<0.0001$ AS 85 ± 24 61 ± 17 63 ± 22 58 ± 9 77 ± 11 $P<0.0001$ APP SBP*HR BL 8.01 ± 2.759 7.53 ± 1.744 0.461 ± 2.764 7.837 ± 2.669 9.201 ± 498 $P<0.0001$ APP SBP*HR BL 8.01 ± 2.759 7.590 ± 4.081 7.412 $P<0.0001$ APP SBP*HR BL 8.01 ± 2.759 7.837 ± 2.669 <t< th=""><th></th><th></th><th>FAST (n=6)</th><th>IL (n=6)</th><th>HIEG+IL (n=6)</th><th>FAST (n=4)</th><th>HIEG (n=4)</th><th>BL vs. AS</th><th>Intervention</th><th>Interaction</th></t<>			FAST (n=6)	IL (n=6)	HIEG+IL (n=6)	FAST (n=4)	HIEG (n=4)	BL vs. AS	Intervention	Interaction
	HR bpm	BL	96 ± 28	103 ± 17	$125 \pm 20^{*}$	77 ± 15	92 ± 13	P < 0.0001	P = 0.06	P < 0.001
SBP mmHg BL 90 ± 13 79 ± 12 83 ± 11 101 ± 14 $103\pm21^{**}$ $P<0.0001$ AS 136 ± 31 00 ± 24 112 ± 24 117 ± 6 $142\pm11^{**}$ $P<0.0001$ BP mm Hg BL 55 ± 8 49 ± 10 $44\pm10^{*}$ 62 ± 9 60 ± 15 $P<0.0001$ BP mm Hg BL 55 ± 8 49 ± 10 $44\pm10^{*}$ 52 ± 9 77 ± 11 $P<0.0001$ AS 85 ± 24 61 ± 17 63 ± 22 58 ± 9 77 ± 11 $P<0.0001$ AP SBP*HR BL 8.601 ± 2.759 7.593 ± 1.744 10.461 ± 2.764 7.837 ± 2.669 9.201 ± 498 $P<0.0001$ AS 11.798 ± 5.022 14.590 ± 4.081 17.462 ± 4.299 18.685 ± 7.382 $P<0.0001$		AS	$92 \pm 18^*$	112 ± 18	134 ± 19	149 ± 29	134 ± 55			
	SBP mm Hg	BL	90 ± 13	79 ± 12	83 ± 11	101 ± 14	$103\pm21^{**}$	P < 0.0001	P < 0.05	SN
		AS	136 ± 31	102 ± 24	112 ± 24	117 ± 6	$142\pm11^{**}$			
	DBP mm Hg	BL	55 ± 8	49 ± 10	$44 \pm 10^*$	62 ± 9	60 ± 15	P < 0.0001	SN	P < 0.05
$ \begin{array}{ c c c c c c c c c c c c c c c c c c c$		AS	85 ± 24	61 ± 17	63 ± 22	58 ± 9	77 ± 11			
AS $11,798 \pm 5,101$ $11,128 \pm 2,052$ $14,590 \pm 4,081$ $17,462 \pm 4,299$ $18,685 \pm 7,382$	RPP SBP*HR	BL	$8,601 \pm 2,759$	$7,593 \pm 1,744$	$10,461 \pm 2,764$	$7,837 \pm 2,669$	$9{,}201\pm498$	P < 0.0001	SN	SN
		AS	$11,798 \pm 5,101$	$11,128 \pm 2,052$	$14,590 \pm 4,081$	$17,462 \pm 4,299$	$18,685 \pm 7,382$			

AS - adrenergic stimulation; BL - baseline; FAST - fasted; IL - Intralipid; HIEG - hyperinsulinemic-euglycemic clamp; HR - heart rate; SBP - systolic blood pressure; DBP - diastolic blood pressure; RPP - rate pressure product.

 * P < 0.05 vs. FAST in dobutamine study;

** P < 0.05 vs. IL; NS - not significant.

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Table 2

Arterial Plasma Substrate and Insulin Concentrations

		AS: Phenyleph	rine		AS: Dobutamine		2-way ANO	VA	
		FAST (n=6)	IL (n=6)	HIEG+IL (n=6)	FAST (n=4)	HIEG (n=4)	BL vs. AS	Intervention	Interaction
GLUCOSE µmol/mL	BL	3.01 ± 1.28 #	3.88 ± 0.68	6.51 ± 3.15	2.82 ± 0.28 #	5.83 ± 1.27	P < 0.0005	P < 0.05	NS
	AS	$4.22\pm1.06^{\#}$	5.00 ± 0.04	8.55 ± 4.97	5.11 ± 1.23	5.43 ± 0.90			
LACTATE nmol/mL	BL	$1,013 \pm 321$ *	$1,572 \pm 289$	$1,303 \pm 199$	$805 \pm 51^*$	$717 \pm 81^*$	NS	P < 0.0005	NS
	AS	$1,215 \pm 673$ *	$1,633\pm432$	$1,218\pm403$	568 ± 125 *	785 ± 142 *			
FFA nmol/mL	BL	$586 \pm 368 * \#$	$4,027 \pm 2,117$	$4,767 \pm 3,792$	$1,126 \pm 814$ *#	$381 \pm 244 $ *#	P < 0.05	P < 0.05	NS
	AS	$508 \pm 197 * \#$	$6,102\pm807$	$6,605 \pm 3,900$	$1,922 \pm 714 $ *#	$765 \pm 330^{*} \#$			
INSULIN µU/mL	BL	$2 \pm 0 # **$	8 ± 10	$177 \pm 111^*$	$2 \pm 0^{**}$	$375 \pm 144 $ *#	NS	P < 0.0001	NS
	AS	$2 \pm 0 # **$	5 ± 3	$199 \pm 139^{*}$	88 ± 72 **	$373 \pm 121 $ *#			
S – adrener <i>wic</i> stimulation	BI.	- haseline: FAST	– facted: II . – Intr	alinid: HTFC – hvn	vlans-2 menilusuire	remic clamn. FF	A _ free fatty s	ride	

S. auy nype) adrenergic s - SA

* P < 0.05 vs. IL;

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 $^{\#}$ P < 0.05 vs. HIEG+IL;

** P < 0.05 vs. HIEG;

NS - not significant.