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The differential effects of pathway- versus target-derived glial cell line–derived neurotrophic factor on peripheral nerve regeneration

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Abstract

Object—Glial cell line–derived neurotrophic factor (GDNF) has potent survival effects on central and peripheral nerve populations. The authors examined the differential effects of GDNF following either a sciatic nerve crush injury in mice that overexpressed GDNF in the central or peripheral nervous systems (glial fibrillary acidic protein [GFAP]–GDNF) or in the muscle target (Myo-GDNF).

Methods—Adult mice (GFAP-GDNF, Myo-GDNF, or wild-type [WT] animals) underwent sciatic nerve crush and were evaluated using histomorphometry and muscle force and power testing. Uninjured WT animals served as controls.

Results—In the sciatic nerve crush, the Myo-GDNF mice demonstrated a higher number of nerve fibers, fiber density, and nerve percentage $(p < 0.05)$ at 2 weeks. The early regenerative response did not result in superlative functional recovery. At 3 weeks, GFAP-GDNF animals exhibit fewer nerve fibers, decreased fiber width, and decreased nerve percentage compared with WT and Myo-GDNF mice ($p < 0.05$). By 6 weeks, there were no significant differences between groups.

Conclusions—Peripheral delivery of GDNF resulted in earlier regeneration following sciatic nerve crush injuries than that with central GDNF delivery. Treatment with neurotrophic factors such as GDNF may offer new possibilities for the treatment of peripheral nerve injury.

Disclosure

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Keywords

glial cell line-derived neurotrophic factor; chromophore; transgenic mouse; sciatic nerve crush; peripheral nerve injury; motor endplate; muscle force; power testing

> Surgical treatment of devastating peripheral nerve injuries currently relies on a combination of nerve grafting and nerve transfer procedures. A better understanding of neurotrophic factors and their effects on regeneration is likely to provide the next paradigm shift in the treatment of peripheral nerve injuries. Glial cell line–derived neurotrophic factor is a well-known member of the GDNF family of ligands, which has demonstrated neuroprotective and regenerative properties in a number of PNS and CNS disease and injury models.^{5,28,33,37,42,} ⁵⁵ The receptor complex for the GDNF family of ligands is composed of a signaling component Ret tyrosine kinase and 1 of 4 glycosylphosphatidylinositol-linked high-affinity ligand binding components designated as GFRα1–GFRα4. Glial cell line–derived neurotrophic factor has been extensively studied, especially with regard to its influence on neuronal populations including dopaminergic, central noradrenergic, sensory, and motoneurons.1,4,9,17,19,20,29,35, $39,52$ Designated as one of the most potent motoneuron survival factors, ¹⁷ GDNF promotes peripheral nerve regeneration in multiple experimental models.^{3,16,30,38}

> To study the in vivo effects of GDNF on different aspects of motoneuron biology in normal and pathological conditions, transgenic mice overexpressing GDNF either in the target, that is, in the skeletal muscle $(Myo-GDNF)^{34}$ or in the CNS and PNS (astrocytes and Schwann cells) (GFAP-GDNF) were generated.^{7,55} Using these transgenic animals, it has been shown that both target- and pathway-derived overexpression of GDNF rescues motoneuron subpopulations from developmental programmed cell death.^{33,35,55} Pathway-derived GDNF promotes complete survival of motoneurons following facial nerve axotomy in neonatal mice and nerve avulsion in adult mice.^{37,55} However, in a mouse model of amyotrophic lateral sclerosis, a disease isolated to spinal motoneurons, it has been demonstrated that only targetderived GDNF and not pathway-derived GDNF is neuroprotective.²⁸ Furthermore, it has been demonstrated that the expression of endogenous GDNF and its receptor $GFR\alpha1$ are upregulated both in the distal nerve stump and in skeletal muscle following a nerve injury.^{6,18,32,46} Moreover, it is known that GDNF is not homogeneously expressed throughout the axon in WT mice, and it is thought that its intracellular trafficking also affects its neuroprotective and regenerative properties.26,36,⁴⁹

> Significant previous work has been published, $2,16,38$ and based on the existing literature, we hypothesized that GDNF from different transgene sources would have different effects on peripheral nerve regeneration and functional recovery following nerve injury. To test this hypothesis, we performed a sciatic nerve crush injury in mice that overexpress GDNF in the CNS/PNS (GFAP-GDNF) or in skeletal muscle (Myo-GDNF). The present study was designed to further investigate the effects of pathway-derived versus centrally derived GDNF on injured peripheral nerves with respect to the rate of regeneration, myelination, fiber width distribution, and motor endplate reinnervation and their manifestation on muscle force production.

Methods

Animal Population

The GFAP-GDNF mice were generated to facilitate a greater than 175-fold increase in CNS GDNF overexpression and a 20-fold increase in PNS (nonmyelinating Schwann cell) GDNF overexpression as driven by the astrocyte-specific GFAP promoter. 55 To study the effects of GDNF overexpression in the muscle target, we used adult Myo-GDNF mice that overexpressed GDNF in muscle at 2.7 times normal endogenous levels as driven by the myogenin promoter.

³³ Integration of the GDNF transgene in heterozygous Myo-GDNF and GFAP-GDNF mice was determined by polymerase chain reaction on genomic DNA extracted from mouse tail specimens.

All experimental animals were housed in a central animal facility and were maintained preand postoperatively in strict accordance with the National Institutes of Health guidelines and according to protocols approved by the Division of Comparative Medicine at Washington University School of Medicine.

Surgical Procedures

All surgical procedures were performed using aseptic and microsurgical techniques. Mice were anesthetized using subcutaneous injections of ketamine (75 mg/kg) and medetomidine (0.5 mg/kg). The right hind leg was then shaved and depilated prior to antiseptic skin preparation. For the sciatic nerve crush model, animals were positioned prone, and a skin incision was made approximately 1 mm posterior and parallel to the femur. The superior margin of the biceps femoris muscle was bluntly dissected and retracted laterally, to expose the medially coursing sciatic nerve. The sciatic nerve was then crushed 5 mm proximal to its trifurcation with No. 5 jeweler's forceps for 30 seconds. ⁸ The crush site was marked with an 11-0 epineurial suture. The wound was irrigated, and the skin was closed with interrupted 6-0 nylon. Anesthesia was reversed with atipamezole hydrochloride (1 mg/kg), and the animals recovered on a heated surface.

Light Microscopy and Histomorphometry

Single transgenic Myo-GDNF, GFAP-GDNF, and WT mice were used and nerves (4–7 mice/ group) were harvested at 0-, 2-, 3-, 4-, and 6-week time points. Segments of the sciatic nerves were harvested en bloc. Labeled nerve specimens from distinct regions proximal and distal to the site of crush injury were preserved in glutaraldehyde, postfixed in osmium tetroxide, and embedded in Araldite 502, and 1-μm cross-sections were obtained with an LKB III Ultramicrotome. Nerves were qualitatively assessed for the preservation of nerve architecture, quality and quantity of regenerated nerve fibers, extent of myelination, and the presence of ongoing wallerian degeneration. This proprietary semiautomated system used a series of algorithms to distinguish axons, myelin, nerve sheath, and debris from each other.²¹ Eightbitplane digital pseudocoloring and our algorithms were used to distinguish axons, myelin, and debris from one another. Processed cross-sections were digitized and assessed for total fascicular area and total fiber number. The mean \pm SD was used to present all data in this study. A 2-tailed ANOVA was made to determine the differences between individual groups. Histomorphometric calculations were performed using Statistica (StatSoft, Inc.). If significant, a Student-Newman-Keuls test was performed to compare groups. Statistical significance was established at $p < 0.05$.

Dynamic Muscle Force Measurement

Functional motor recovery following sciatic nerve crush was assessed in situ by measuring evoked force production in the EDL muscle. The Myo-GDNF, GFAP-GD-NF, and WT mice (2 or 3 mice/group) underwent sciatic nerve crush and were allowed to recover for 2, 4, and 6 weeks postoperatively. At the terminal time point, animals were anesthetized, as previously described, prior to microsurgical isolation of the sciatic nerve and EDL muscle. Specifically, the EDL muscle and distal tendons were exposed through a skin incision extending from the dorsum of the foot to the lateral knee. The distal EDL tendons were then severed, freed from the extensor retinacula, and sutured to a stainless steel S-hook. The sciatic nerve was subsequently exposed and proximally neurolysed prior to severing the tibial and sural nerves just distal to the point of trifurcation.

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Prior to analysis, animals were placed on an adjustable warming bath where the target extremity was immobilized by transversely inserting a pin through the femoral condyles. The exposed sciatic nerve was bathed in mineral oil and proximally interfaced using a shielded bipolar silver wire electrode (Harvard Apparatus, Inc.). The distal tendons of the EDL muscle were then connected to the lever arm of a dual-mode lever system (model 300C, Aurora Scientific, Inc.) through the integrated S-hook. Simultaneous stimulation of the sciatic nerve and measurement of evoked active EDL muscle force was accomplished using a custom-built system consisting of a Grass S88× isolated pulse stimulator (Grass Technologies), model 300C dual-mode lever, model 604A interface board, and desktop PC running DMA/DMC software (Aurora Scientific, Inc.).

The amplitude of applied electrical impulses and the length of the EDL muscle required to produce maximum twitch force were determined for each muscle tested to standardize force measurements. The resulting optimal stimulus amplitude and optimal muscle length (L_o) were used for all subsequent measurements. Maximum isometric tetanic force was quantified by applying trains of electrical pulses (pulse width 0.2 msec, burst width 300 msec) of varying frequency (pulse frequency 30–400 Hz) to the sciatic nerve while recording resulting force production in the EDL muscle. Two-minute recovery periods were provided between trials to reduce muscle fatigue and data contamination.

Peak power produced by the EDL muscle was measured during isovelocity shortening contractions facilitated by preprogrammed rotation of the servo lever arm. The optimal fiber length (L_f) was calculated from L_o using an EDL-specific fiber length/muscle length ratio of 0.44.⁴⁷ The EDL muscles were allowed to contract at increasing velocities $(0.5-4.0 \, \text{L}_f/\text{second})$ through a constant displacement around L_0 (105 to 95% L_f) on stimulation of the sciatic nerve by trains of electrical pulses of varying frequency (pulse frequency 100–400 Hz). The average active force during isovelocity contraction was calculated from acquired force traces using custom data analysis software (MATLAB, MathWorks, Inc.). Power was subsequently calculated as the product of the average force and the velocity of contraction.

Maximum isometric tetanic force and peak power measurements were converted to maximum specific tetanic force (sF_0) and normalized peak power (nP_0) , respectively, to better compare measurements acquired from various animals and eliminate variability associated with muscle atrophy. Contralateral uninjured EDL muscles (5–8 mice/group) were quantitatively analyzed in a similar fashion and served as controls. Following analysis, all animals were killed.

Statistical Analysis

Data were analyzed using a Kruskal-Wallis ANOVA test on ranks. All values are displayed as mean \pm SD. Histomorphometry and muscle force and power testing were done following a post hoc Dunn test. Confocal imaging analysis was done following a post hoc Student-Newman-Keuls test. A p value < 0.05 was defined as significant for all groups.

Results

Sciatic Nerve Crush

Histomorphometry was performed on harvested sciatic nerves 5 mm distal to the crush site following crush injury (Fig. 1). As depicted in Fig. 1 at the 2- and 3-week time points postcrush, Myo-GDNF mice demonstrated a significantly higher total number of nerve fibers, fiber density, and nerve percentage $(p < 0.05)$ than the other genotypes. The Myo-GDNF mice had 4411 ± 1382 and 4733 ± 981 nerve fibers versus 1404 ± 157 and 3933 ± 489 fibers for WT and 1616 ± 780 and 2436 ± 795 fibers for GFAP-GDNF mice (Fig. 1A).

By the 4-week time point GFAP-GDNF mice had significantly more nerve fibers than either WT or Myo-GDNF animals ($p < 0.05$) (Fig. 1A). The GFAP-GDNF nerves contained 5954 \pm 931 nerve fibers in comparison with 3522 ± 1160 for WT and 3937 ± 1080 for Myo-GDNF animals. The GFAP-GDNF animals had a higher fiber density in comparison with WTs at this time point ($p < 0.05$).

At the 6-week time point, there were no significant differences in total nerve fibers, fiber width, density, or percent nerve (Fig. 1). In addition, the fiber width distribution no longer demonstrated any significant difference regardless of the presence or site of GDNF overexpression (Fig. 2E).

Dynamic Muscle Force Measurement of the EDL

To correlate histological findings with functional motor recovery following sciatic nerve crush, the maximum specific tetanic force (sF_0) and normalized peak power (nP_0) evoked in the EDL muscle (Fig. 3) were measured in situ. Examination of sF_0 measurements acquired from Myo-GDNF, GFAP-GDNF, and WT mice revealed progressive, monotonic recovery of EDL function in all groups over the 6-week time course. Two weeks after sciatic nerve crush, EDL muscles of GFAP-GDNF mice demonstrated lower sF_0 levels (104.45 kN/m²) than those of Myo-GDNF mice (172.87 kN/m^2) , which were generally equivalent to levels in WT mice (180.22 kN/m²). The GFAP-GDNF mice continued to demonstrate lower average sF_0 levels at 4 weeks (147.40 kN/m²) than Myo-GDNF and WT mice (206.85 and 228.58 kN/m²). All experimental groups demonstrated sF_0 values indistinguishable from control measurements at the terminal time point. Further examination of postoperative sF_0 recovery suggests that all experimental groups recovered motor function at similar rates prior to reaching preinjury levels.

Examination of nP_0 measurements acquired from all experimental groups revealed progressive, monotonic recovery of dynamic EDL function in Myo-GDNF and GFAP-GDNF mice. The WT mice did not exhibit this characteristic, progressive recovery due to an unexplained spike in nP_0 production at the 4-week time point. Assessment of nP_0 data collected 2 weeks after sciatic nerve crush demonstrated greater power production in EDL muscles of WT mice (107.87 W/kg) compared with Myo-GDNF and GFAP-GDNF mice (81.20 and 67.10 W/kg). Decreased power production in GFAP-GDNF mice at 2 weeks mirrored decreased force production at the same time point. By 6 weeks, all groups had persistent nP_0 production deficits compared with baseline controls (Fig. 3), suggesting a greater functional deficit than that predicted by sF_0 measurements.

Discussion

Significant clinical and laboratory research has been devoted to GDNF applications. Glial cell line–derived neurotrophic factor enhances nerve regeneration,^{2,16,38} is an important trophic factor for motor neuron survival, $17,34$ and has demonstrated significant potential as a neuroprotective agent.^{10,11,33,35,55} Despite these advances, a major obstacle in GDNF utilization has been the method and site of delivery that will optimize its benefits.40 Transgenic animals that overexpress GDNF in the CNS and nonmyelinating Schwann cells (GFAP-GDNF) or in peripheral skeletal muscle (Myo-GDNF) have enabled investigators to study sitespecific endogenous delivery. In this study, we examined CNS and pathway- versus targetderived GDNF in regard to peripheral nerve regeneration, and evaluated recovery after injury with histological, functional, and imaging outcome measures.

We have shown that Myo-GDNF animals demonstrate an earlier regenerative response 2 weeks after sciatic nerve crush. In contrast, GFAP-GDNF animals demonstrated a delayed neuroregenerative response with more nerve fibers and fiber density occurring by 4 weeks and

maintained for at least 6 weeks. The histomorphometric analysis of the harvested sciatic nerves does not distinguish between axonal sprouting or motor and sensory fiber regeneration.^{14,21} The increased number of fibers noted at the 2- and 3-week time points in the Myo-GDNF group may represent any combination of these variables; however, the high percentage of smallcaliber fibers at this early time point relative to uninjured controls (Fig. 2B) is most consistent with increased axonal sprouting. The high percentage of small-diameter fibers in the GFAP-GDNF sciatic nerves at 4 weeks (Fig. 2D) suggests delayed axonal sprouting, sensory nerve regeneration, or small-diameter intrafusal fiber regeneration. This observation supports the claim that GFAP-GDNF animals demonstrate a delayed regenerative response.

It is possible that the increase in fiber counts seen in this study is a result of the experimental model (Myo-GDNF and GFAP-GDNF) rather than the delivery modality of GDNF. Previously, it has been shown that the overexpression of GDNF in the muscle seen in Myo-GDNF mice used in this study results in a larger population of fusimotor neurons or γmotoneurons during development.50 The increase in this neuron subpopulation correlates with an increase in the percentage of small-diameter γ-motoneuron fibers following development, which can be seen in the fiber distribution plots of our controls (γ -motoneuron fibers are $\lt 3.5$ μm in diameter⁵⁰). It could be argued that the presence of an increased percentage of γmotoneurons results in an inflated number of nerves observed 2 weeks following injury seen in the Myo-GDNF group in the current study. However, this inflation would then be accompanied by a statistical increase in the percent of γ-motoneuron fibers (< 3.5 μm in diameter), and no such difference is seen between our control and Myo-GDNF groups at any time point except for the 4th week. We believe that the lack of differences in small-diameter fiber distribution between the control and Myo-GDNF groups validates the conclusion that target-derived GDNF delivery increases early nerve fiber regeneration.

Despite the increase in nerve fiber counts, the early regenerative response in Myo-GDNF mice did not directly correlate with superlative functional recovery. Muscle force testing at 2 weeks was equivalent between Myo-GDNF and WT mice. At 4 weeks, GFAP-GDNF mice demonstrated a dramatic increase in total nerve fibers, yet functional data lagged behind with force and power not returning to WT and Myo-GDNF levels until 6 weeks. The discrepancy between estimates of functional recovery based on maximum specific tetanic force (sF_0) and normalized peak power (nP_0) measurements noted previously,⁵³ specifically demonstrates the complexity of peak power measurements. While maximum specific force values primarily measure functional reinnervation of muscle fibers by regenerating axons, normalized peak power measurements are simultaneously affected by variable reinnervation of muscle fibers, muscle fiber type switching, and muscle fibrosis.^{23,48} Comparison of sF_0 and nP_0 measurements suggests that CNS- and pathway-derived GDNF in GFAP-GDNF mice and target-derived GDNF in Myo-GDNF mice may delay and expedite acute nerve regeneration and functional reinnervation of distal motor targets, respectively. This variable GDNF production has little effect on dynamic muscle function or clinical outcomes in such an acute setting. Furthermore, these findings reinforce the principle that enhanced nerve regeneration alone is unable to overcome the many pathological processes limiting functional motor recovery following peripheral nerve injury and muscle denervation.

The Role of GDNF Gradients in Peripheral Nerve Regeneration

The presence of an enhanced gradient of GDNF expression when regenerating toward denervated muscle tissue may influence axonal regeneration in Myo-GDNF animals. In WT animals, the concentration of GDNF in adult mice is higher in peripheral nerves than in the fore-brain, brainstem, cerebellum, and spinal cord, suggesting that endogenous expression by peripheral Schwann cells and muscle tissue is greater than expression in the CNS.⁵⁵ This physiological pattern of endogenous GDNF being concentrated in the periphery versus the

CNS is preserved and increased in the Myo-GDNF animals.33 In contrast to this, GFAP-GDNF mice, created with the GFAP construct, were optimized for transgene expression to reside predominantly in glial cells, leading to much higher GDNF expression in the CNS. Although these animals have a higher CNS concentration of GDNF relative to peripheral expression, their peripheral expression is still 20-fold higher than that found in WT animals as measured by enzyme-linked immunosorbent assay (ELISA) of pooled sciatic nerve tissues.⁵⁵ Regardless of this increase, the physiological pattern of endogenous GDNF being higher in the periphery than in the CNS is not preserved in the GFAP-GDNF mice. In light of our results following sciatic nerve crush, these known concentration differences may explain some of our findings.

The GFAP and Myogenin Regulatory Elements

Other factors to consider in the interpretation of our results are the regulatory elements of the transgenic animals studied (GFAP and myogenin). The GFAP is expressed by astrocytes, in addition to nonmyelinating Schwann cells and reactive Muller cells.^{15,21,22,40} The mechanisms of GFAP regulation in vivo are not fully understood, but it is known that endogenous murine GFAP expression coincides with early neural development and astroglial differentiation, with an increase in GFAP mRNA until 1–2 weeks after birth, followed by a slow decline.^{7,27,44} Similar to this expression trend in development, it has also been shown that GFAP expression is increased after nerve injury, 25 and immunoreactivity of the promoter following facial nerve axotomy in neonates peaks at 1 week and begins to decline after 2 weeks toward normal levels. ⁴³ Although the *GFAP* gene activation mechanism may differ in distinct lesions,⁴⁵ it is possible that its upregulation and the resulting spike in GDNF concentration in the nerve pathway at 1 and 2 weeks were responsible for the delay seen in sciatic nerve regeneration in GFAP-GDNF animals compared with Myo-GDNF animals at these time points, presumably because of the loss of gradient to the muscle target. Additionally, upregulation of GDNF by Schwann cells in the GFAP-GDNF animals may have induced axonal sprouting and maintenance at the motor endplate, as seen in the EDL confocal images at 1 and 2 weeks.

Myogenin, a helix-loop-helix transcription factor, plays a role in the differentiation of progenitor cells into mature myocytes and is localized in myonuclei after denervation.²⁴ It is transcriptionally repressed by electrical activity provided by motor innervation, and it is rapidly induced following the loss of function, as occurs in denervation.^{12,31,41,51} In a rat sciatic nerve transection model, myogenin RNA as measured in EDL muscles, has a 50-fold induction 3 days after injury and remains at a 30-fold induction level by 2 weeks.⁵⁴ In a mouse denervation study, a 40-fold increase of myogenin mRNA is noted in the gastrocnemius muscle with a rapid accumulation of myogenin mRNAs occurring as early as 8 and 16 hours after denervation.¹³ The rapid on/off of the myogenin regulatory element is one possible explanation for the observed early increase in the total number of nerve fibers in Myo-GDNF animals after sciatic nerve crush, as compared with the other genotypes. Additionally, this early production of GDNF by the Myo-GDNF animals after denervation may have promoted axonal sprouting and maintenance at the motor endplate, as observed on confocal imaging.

Conclusions

In the present study, the end point or target overexpression of GDNF (Myo-GDNF) was characterized by an increase in the number of regenerating axons 2 weeks after injury and a more rapid reinnervation of motor end-plates by terminal axons. Significant differences between these parameters in end point versus pathway GDNF over-expression were not evident at later time points and did not translate to significant differences in muscle isometric force or power production. While findings from this study suggest that the end point overexpression of GDNF may stimulate nerve regeneration, the results must be interpreted in the context of a transgenic mouse model. It will be necessary to both investigate the exogenous peripheral

delivery of GDNF and apply our findings to a large animal model. This will enable more sensitive measures of muscle force production following reinnervation and facilitate the evaluation of longer peripheral nerves, which translate to later experimental time points that are more clinically relevant to human peripheral nerve injury.

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Abbreviations used in this paper

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Fig. 1.

Bar graphs. Histomorphometry was performed on harvested sciatic nerves following crush injury. Compared with WT and GFAP-GDNF mice, Myo-GDNF demonstrated a statistically significantly higher total number of nerve fibers **(A**), fiber density **(C)**, and nerve percentage **(D)** at 2 weeks after sciatic nerve crush injury. At the 3-week time point Myo-GDNF demonstrated a significantly higher total number of nerve fibers, fiber width, fiber density, and nerve percentage compared with GFAP-GDNF mice. The GFAP-GDNF animals demonstrated a delayed regenerative response; at 4 weeks they had significantly more total nerve fibers and fiber density than WT controls. At 6 weeks, there was no statistical difference between any of the groups or measured parameters. *Asterisks* denote statistical differences (p < 0.05) between measurements.

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Fig. 2.

Bar graphs showing the distribution of fiber width as a percentage of the total fibers. At each time point following sciatic nerve crush, fiber width data were stratified according to animal genotype. Stratification data are represented as a percentage of the total mean fiber width within each genotype. **A:** In uninjured control animals, there are statistical differences in fiber width distribution of smaller-diameter fibers. **B:** At 2 weeks after nerve crush, WT animals show a statistically significant increase in 4–5-μm fibers. **C and D:** The GFAP-GDNF animals show an increase in small-diameter fibers at 3 weeks **(C)**, with significantly lower numbers of largerdiameter fibers compared with both WT and GFAP-GDNF. **E:** By 6 weeks, there are no differences between fiber distributions between genotypes. *Asterisks* denote statistical differences ($p < 0.05$) between measurements.

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Fig. 3.

Bar graphs. Functional motor recovery following crush injury was assessed through an in situ measurement of maximum specific tetanic force production and normalized peak power production in the EDL muscle. *Left:* The Myo-GDNF mice demonstrated a greater recovery of specific force production compared with GFAP-GDNF mice at 2 weeks postoperatively, equivalent to WT mice. *Right:* At a similar time point, recovery of power production in Myo-GDNF and GFAP-GDNF mice was indistinguishable, although both Myo-GDNF and GFAP-GDNF mice demonstrated a lower power production than WT mice.