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Elevated Cyclic Stretch Induces Aortic Valve Calcification in a Bone Morphogenic Protein-Dependent Manner

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Calcified aortic valve (AV) cusps have increased expression of bone morphogenic proteins (BMPs) and transforming growth factor- β 1 (TGF- β 1). Elevated stretch loading on the AV is known to increase expression of matrix remodeling enzymes and pro-inflammatory proteins. Little, however, is known about the mechanism by which elevated stretch might induce AV calcification. We investigated the hypothesis that elevated stretch may cause valve calcification via a BMP-dependent mechanism. Porcine AV cusps were cultured in a stretch bioreactor, at 10% (physiological) or 15% (pathological) stretch and 70 beats per minute for 3, 7, and 14 days, in osteogenic media supplemented with or without high phosphate (3.8 mmol/L), TGF- β 1 (1 ng/ml), as well as the BMP inhibitor noggin (1, 10, and 100 ng/ml). Fresh cusps served as controls. Alizarin red and von Kossa staining demonstrated that 15% stretch elicited a stronger calcification response compared with 10% stretch in a fully osteogenic medium containing high phosphate and TGF-β1. BMP-2, -4, and Runx2 expression was observed after 3 days on the fibrosa surface of the valve cusp and was stretch magnitude-dependent. Cellular apoptosis was highest at 15% stretch. Tissue calcium content and alkaline phosphatase activity were similarly stretchdependent and were significantly reduced by noggin in a dose dependent manner. These results underline the potential role of BMPs in valve calcification due to altered stretch. (Am J Pathol 2010, 177:49-57; DOI: 10.2353/ajpath.2010.090631)

Aortic valve calcification, long considered a passive process associated with risk factors such as age, hypertension, renal disease, and cardiovascular disease, is potentially an active inflammatory and degenerative process that is influenced by hemodynamic forces as well as dysfunction of normal cellular functions.^{1–3} Surgical replacement or repair is the primary treatment mode for valve calcification as there are currently few medical or pharmacological options available. Calcified valves demonstrate increased expression of cytokines such as transforming growth factor- β 1 (TGF- β 1),^{4,5} bone morphogenic proteins (BMPs),⁶ as well as alkaline phosphatase (ALP).^{7,8} Additionally, active osteogenesis was reported in calcified human valve cusps.¹

Several mechanisms have been proposed for valve calcification including osteogenic differentiation of valvular interstitial cells,^{8,9} calcification secondary to cellular apoptosis,^{4,10} and necrosis-related deposition of calcium.¹¹ Although a common feature of these processes is the disruption in the normal functioning of the endothelium and interstitial cells in the valve cusp,^{12,13} the exact mechanisms and factors that result in calcific disease initiation are not well understood. Apart from biochemical, atherogenic, and humoral factors, the mechanical/hemodynamic environment of the valve is thought to play an important role in the regulation of normal and pathological valve cell function.^{14,15}

The aortic valve functions in a complex mechanical environment, which includes cyclic stretch, bending, pressure, and shear stresses,¹⁴ and several authors have linked alterations in these hemodynamic forces to initiation and progression of valve dysfunction and disease.^{16–18} Hypertension, which is a known risk factor for calcific aortic valve disease,¹⁹ results in a situation of elevated stress and stretch of the valve cusp. Under physiological conditions, the normal valve experiences

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approximately 10% stretch in the circumferential direction and 30% in the radial direction, which can change depending on changes in pressure load.²⁰ Increased cyclic stretch has been linked to elevated expression of matrix remodeling proteins¹⁶ as well as pro-inflammatory markers²¹; however, the possible mechanisms of elevated stretch-induced valvular degeneration and specifically calcification are not well characterized.

We investigated the hypothesis that aortic valve calcification is induced by elevated cyclic stretch in a BMPdependent manner. The potential downstream effects of secreted BMP were blocked by using noggin. We found that the aortic valve can be calcified rapidly in a proosteogenic or atherogenic culture medium within 7 days, and that these responses were BMP-dependent.

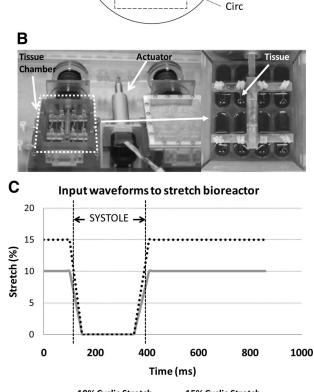
Materials and Methods

Tissue Harvest and Preparation

Fresh porcine hearts (12 to 24 months) were obtained from a local abattoir within 10 minutes of slaughter. The aortic valves were transported to the laboratory in sterile, ice-cold Dulbecco's Phosphate Buffered Saline (Sigma, St. Louis, MO). A rectangular section of tissue with dimensions of 15×10 mm was isolated from the central region of each valve cusp, proximal to the line of coaptation. Tissue sections were studied in circumferential orientation (Figure 1A) because this is the primary direction of the stress-bearing collagen fibers within the cusp.¹⁴ These samples were then randomized and assigned to treatment groups outlined below. We ensured that each cusp sample originated from a different animal and that there was a random mix of left, right, and noncoronary cusps for each treatment group. All samples were stretched in appropriate culture medium in a tensile stretch bioreactor (Figure 1B)²² maintained at 37°C in an incubator. Additionally, culture medium was replaced every 2 days during each experiment and was visually inspected for evidence of contamination. The waveforms imposed on the cusp are depicted in Figure 1C.²⁰ On completion of the stretching, samples were removed and immediately washed three times in ice-cold sterile Dulbecco's Phosphate Buffered Saline and either frozen in optimal cutting temperature compound (Electron Microscopy Sciences, Hatfield, PA) for histological and immunohistochemical analyses, or flash frozen in liquid nitrogen.

Experimental Groups and Conditions

Three mechanical treatment groups were explored in this study: (1) fresh tissue (acute control); (2) 10% stretch (physiological); and (3) 15% stretch (hypertensive). Static controls were not used because they are not representative of a realistic mechanical environment for the aortic valve. We have validated previously that stretch is the dominant force acting on the cusp samples and that any shear stresses induced on the leaflet due to the stretching motion are negligible.²² Five different modifications of



Α

10% Cyclic Stretch ••••• 15% Cyclic Stretch

Figure 1. Preparation of aortic valve cusps for the experiment. A circumferentially oriented 15 × 10 mm section was excised from the central region of porcine aortic valve cusps (**A**). An *ex vivo* tensile stretch bioreactor was used in this study (**B**).²² A magnified image of the tissue chamber is shown on the **right**. A loading curve was used in this study. The gradients of the extension and relaxation approximated those experienced *in vivo* (**C**).²⁰

Dulbecco's modified Eagle's medium (DMEM; Sigma) were initially used to understand their different pro-osteogenic and calcific potentials (Table 1). The high phosphate concentration (3.8 mmol/L) and inclusion of TGF- β 1 (1 ng/ml) in the osteogenic medium were based on pathophysiologically relevant conditions reported in hyperphosphatemia due to renal disease^{23,24} and previous studies on cells in culture.^{4,25}

To permit the characterization of the BMP-dependent pathway of aortic valve calcification, four different concentrations of the BMP-antagonist noggin (R&D Systems, Minneapolis, MN), -0, 1, 10, and 100 ng/ml, were added to the DMEM formulation that elicited the strongest calcific response (ie, DMEM formulation V as shown in the results). Noggin was selected because it is a well-established BMP antagonist with a weak dissociation constant (K_d) of 20 Picomolar.²⁶ This would allow noggin to bind any expressed BMP and prevent its downstream action. Additionally, noggin has been previously shown to block the pro-inflammatory effects of BMP-4 expression on vascular endothelial cells.²⁷ Therefore, it is an ideal candidate to evaluate the BMP-dependence of aortic valve calcification.

No.	Culture media	Composition
1	Normal medium	Normal DMEM supplemented with 10% fetal bovine serum
2	Base osteogenic medium	Normal medium supplemented with 1 mmol/L β -glycerophosphate, 10 μ mol/L dexamethasone, and 0.9 mmol/L PO ₄ ³⁻
3	Base osteogenic medium with high phosphates	Base osteogenic medium with 3.8 mmol/L PO_4^{3-}
4	Base osteogenic medium with TGF- β 1	Base osteogenic medium with 1 ng/ml TGF- β 1
5	Full osteogenic medium	Base osteogenic medium with 1 ng/ml TGF- β 1 Base osteogenic medium with 3.8 mmol/L PO ₄ ³⁻ and 1 ng/ml TGF- β 1

Table 1. Different Formulations of Culture Media Used in Order to Develop a Model for Calcification in an ex vivo System

Experimental Sterility, Tissue Structural Integrity, and Viability

For these studies, the valve tissue was being cultured in an ex vivo environment for up to 14 days. It was therefore important to verify that the tissue was not damaged and that there was no contamination of the culture media. Routine H&E staining was used to assess tissue structure. Apart from a qualitative assessment, mean tissue thickness was determined from these H&E micrographs by using the Image J software (NIH, Bethesda, MD). Tissue culture medium was analyzed microscopically every 2 days for evidence of bacterial or fungal growth. In addition, pH and media absorbance (at 364 nm)¹⁸ was tested at 3, 7, and 14 days and compared with fresh media, as well as media conditioned for the same duration but without tissue. Cell death was determined by carefully examining 4',6-diamidino-2-phenylindole stained cells after 3, 7, and 14 days of stretch culture under a $40 \times$ objective. Individual cells were inspected for evidence of DNA aggregation, smearing, or other abnormalities. The count of these cells was then normalized over the total number of cells in that particular micrograph and presented as percentage cell death for that particular culture duration.

Analysis of Calcification, Cell Apoptosis, and Bone Morphogenic Protein Expression

Frozen optimal cutting temperature blocks were cut into $5-\mu$ m sections in cross section. Alizarin Red and von Kossa staining were used to assay for tissue mineralization. Cell apoptosis was analyzed and quantified by using a terminal deoxynucleotidyl transferase-mediated dUTP nick-end labeling fluorescence kit (Roche Applied Science, Indianapolis, IN) as outlined before.¹⁶ Immunohistochemistry was used to identify cells positive for BMP-2 (1:25; Santa Cruz Biotechnology, Santa Cruz, CA) and BMP-4 (1:50; Santa Cruz Biotechnology). Semiquantitative assessments of BMP-2 and -4 expression were performed by using previously published methods.²⁸ Sections were also probed with von Willebrand Factor (1:100, Sigma) to identify the phenotype of the cells that were expressing BMPs.

Calcium Assay

Tissue samples were weighed and pulverized by using a mortar and pestle in liquid nitrogen, incubated in 1 M acetic acid for 24 hours at 4°C to solubilize calcium, and

centrifuged at 15,000 rpm. The supernatant as well as calcium standards were assayed for calcium content by using a calcium specific arsenazo dye reagent (Fisher-Scientific, Waltham, MA). The quantity of reaction product formed was determined by spectrophotometry at 650 nm. The calcium content was normalized with the weight of the sample and expressed as microgram calcium per milligram wet weight.

Alkaline Phosphatase Enzyme Activity Assay

Tissue samples were pulverized by using a mortar and pestle in liquid nitrogen and homogenized in ice-cold radioimmunoprecipitation assay buffer (Santa Cruz Biotechnology) before centrifuging at 15,000 rpm to pellet extracellular matrix debris. The supernatant was assayed for protein concentration by using the BCA protein assay (Pierce, Rockford, IL). ALP activity in the tissue lysate was assayed by adding 10 mmol/L pnitrophenyl phosphate as a substrate in 0.1 M glycine buffer (pH 10.4) containing 1 mmol/L ZnCl₂ and 1 mmol/L MgCl₂. The quantity of p-nitrophenol formed was determined by spectrophotometry at 405 nm and then monitored at 15, 30, 60, 120, and 180 minutes and after 24 hours. ALP activity was calculated from a standard and normalized with the protein concentration. The specific activity of ALP was reported as nanomole per minute per milligram protein.

Analysis of Downstream Transcription Factors for Bone Morphogenic Proteins

Immunoblotting was used to analyze expression of Runx2 (1:100; Santa Cruz Biotechnology), Osteocalcin (1:50; Millipore, Billerica, MA), and β -actin (1:1000, Sigma). Equal amounts (30 μ g) of tissue lysates were resolved by reducing SDS-polyacrylamide gel electrophoresis. After transfer to a polyvinylidene difluoride membrane (Millipore), the blots were blocked with 3% bovine serum albumin and probed with primary antibody and appropriate biotinylated secondary antibody. The membranes were finally incubated in horseradish peroxidase-conjugated streptavidin. Immunopositive bands were detected by using a luminol-based chemiluminescence reagent (Pierce) and analyzed by densitometry by using the Image J program (NIH).

Statistical Methods

All quantitative data were expressed as mean \pm SE. The sample size was n = 6 to 8 (all from different animals) for all analyses. The data were first analyzed by using analysis of variance to determine whether there was significant contribution by a particular treatment on the measured parameters, followed by the Tukey posthoc test. A P value of less than 0.05 was used as a measure of statistical significance. All statistical analyses were performed by using Minitab (Minitab Inc., State College, PA).

Results

Tissue Structure, Viability, and Media Sterility is Maintained under Cyclic Stretch

H&E staining (Figure 2A) demonstrated that the tissue morphology and structure was comparable between fresh valve cusps and cusps stretched for 3, 7, and 14 days. Tri-layered morphology was maintained, and characteristic features such as the ridged fibrosa layer and sparse spongiosa layer was maintained between the stretched groups and fresh tissue. In addition, tissue thickness was statistically similar (P > 0.4; n = 10) between fresh controls and cusp samples stretched for 3, 7, and 14 days (Figure 2B). Analysis of cell death showed that the number of dead cells was less than 3.5% of number of total cells (Figure 2, C and D), indicating that the bioreactor system did not induce significant cell death. The number of cells that appeared to be necrotic were statistically similar (P > 0.1) between 3, 7, and 14 days of stretch culture.

There was no significant (P > 0.5; n = 6) difference in absorbance at 364 nm between fresh DMEM (0.408 ± 0.025), conditioned medium with tissue after 3 (0.432 ± 0.035), 7 (0.427 ± 0.036), and 14 days (0.421 ± 0.031), and conditioned medium without tissue after 3 (0.408 ± 0.025), 7 (0.415 ± 0.029), and 14 days (0.420 ± 0.029). Media pH was also statistically unchanged (P > 0.5; n =12) over the course of experiment, indicating good media sterility. In addition, examination of the media under the microscope every 2 days did not demonstrate evidence of bacterial or fungal contamination.

Cyclic Stretch Induced Aortic Valve Calcification

It has not been previously demonstrated whether aortic valve cusp tissue can be calcified *ex vivo* in an experimentally feasible timeframe. We tested the hypothesis that porcine aortic valve cusps can be calcified by a combination of pathological levels of stretch (15%) and a pathophysiologically relevant humoral environment (high concentrations of phosphate and TGF- β 1). Fresh porcine valve samples and samples cultured for 7 days at 10% stretch (physiological) or 15% stretch (pathological) in normal DMEM (Figure 3, A and E), osteogenic medium (Figure 3, B and F), or osteogenic medium supplemented with high phosphate (Figure 3, C and G) did not show positive Alizarin red staining for calcification. Calcific

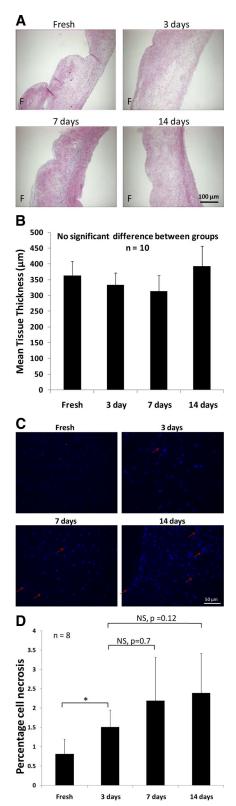


Figure 2. Normal tri-layered morphology of aortic valve cusps was maintained in stretch experiments. Tissue morphology and structure was comparable between fresh controls and samples stretched for 3, 7, and 14 days (**A**). There was no significant difference in tissue thickness between fresh controls and samples stretched for 3, 7, and 14 days (**B**) [n = 10]. Samples cultured to 3, 7, and 14 days showed some evidence of DNA deterioration as demoss strated by **arrows** (**C**); however, the number of necrotic cells was less than 3.5% of the total number of cells (**D**) [n = 8] F indicates fibrosa. *P < 0.05.

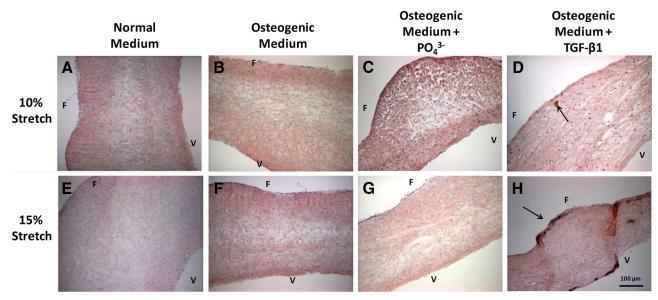


Figure 3. Alizarin red staining of porcine aortic valve cusps that were cultured for seven days under 10% (A–D) or 15% (E–H) stretch in normal DMEM, osteogenic DMEM, osteogenic DMEM with 1 ng/ml TGF- β 1, as indicated. Small calcific nodules were found only in G and H as marked with arrows. F indicates fibrosa; V, ventricularis.

nodule formation could be observed on the aortic surface in cusp samples exposed to both 10% and 15% stretch in osteogenic media with TGF- β 1 (Figure 3, D and H).

Treatment of valve cusps in fully osteogenic medium under 10% (physiological) or 15% stretch (pathological) for 7 days resulted in calcification in a stretch-dependent manner (Alizarin Red, Figure 4, A and C; von Kossa, Figure 4, B and D). The fibrosa side showed more intense staining than the ventricularis side of the cusp when exposed to 15% stretch. These results suggest that calcification of aortic valve cusps required both stretch and the fully osteogenic medium containing high phosphate and TGF- β 1 levels, whereas neither stretch nor the fully osteogenic medium alone was sufficient. In addition, the fibrosa side appeared to be preferentially susceptible to calcification.

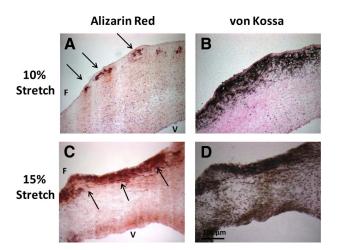


Figure 4. Cyclic stretch induced calcification of porcine aortic valve cusps. Aortic valve cusps were exposed to 10% (**A** and **B**) or 15% (**C** and **D**) cyclic stretch for seven days in fully osteogenic medium containing both high phosphate and TGF-*B*1. Cusps were then stained with Alizarin Red (**A** and **C**) or Von Kossa (**B** and **D**). Calcific nodules are marked with **arrows**. F indicates fibrosa; V, ventricularis.

Cellular Apoptosis was Highest for the 15% Stretch and Lowest for 10% Stretch

Because previous authors have linked valve calcification to cellular apoptosis,⁴ we tested if exposing cells to physiological and/or pathological stretch for 7 days in the fully osteogenic medium induced apoptosis of aortic valve cusp cells. Terminal deoxynucleotidyl transferase-mediated dUTP nick-end labeling assay (Figure 5, A and B) showed significantly larger numbers of apoptotic cells when cusps were cultured with 15% stretch (180.6 ± 49.5) in the fully osteogenic medium compared with 10% stretch (22.4 ± 4.3) and fresh controls (4.2 ± 0.9). In addition, cellular apoptosis was significantly reduced when samples were cultured with 100 ng/ml noggin (10% stretch: 3.2 ± 0.9 ; 15% stretch: 12.7 ± 1.9). For the 10% stretch with noggin group, the number of apoptotic cells was statistically similar to fresh controls.

Pathological Stretch Increased BMP-2/-4 Expression in Aortic Valve Cusps

To determine whether BMP expression was increased by cyclic stretch in the fully osteogenic medium, BMP-2 and -4 expressions were examined in aortic cusps that were stretched to 10% and 15% and in fresh controls (Figure 6). Fresh samples did not show any discernable amount of BMP-2 or BMP-4 as detected by immunohistochemistry. Both 10% and 15% cyclic stretch significantly increased BMP-2 and -4 expressions. In addition, BMP expression was significantly higher at 15% stretch compared with 10% stretch (Figure 6B). BMP-2 and BMP-4 expression was remarkably higher on the fibrosa side of the cusps compared with the ventricularis (Figure 6A). In addition, double immunostaining on the same valve sample with BMP-2 and von Willebrand Factor (Figure

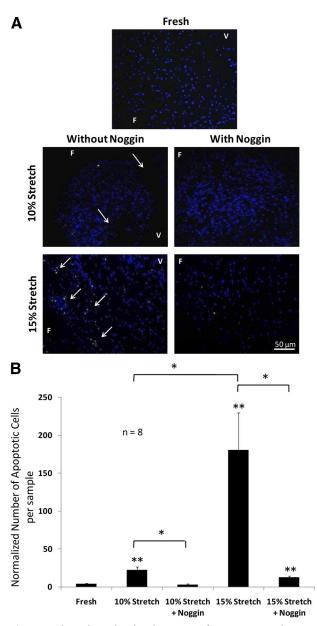


Figure 5. Elevated stretch-induced apoptosis of porcine aortic valve cusp cells. Fresh valve cusps and cusps exposed to 10% or 15% cyclic stretching in fully osteogenic medium were assayed for apoptosis by terminal deoxynucleotidyl transferase-mediated dUTP nick-end labeling staining (green) with 4',6-diamidino-2-phenylindole nuclei counterstain (blue), with apoptotic cells detected marked with **arrows** (**A**). The normalized number of apoptotic cells primage field was then quantified for each treatment condition (**B**). F indicates fibrosa; V, ventricularis. *P < 0.05; **P < 0.05 vs. fresh control.

7, A–D) revealed strong colocalization of these two proteins (Figure 7).

Calcification of Aortic Valve Cusps Occur in a BMP-Dependent Manner

Next, we examined whether cusp calcification induced by pathological cyclic stretch was mediated in a BMPdependent manner. To test this hypothesis, cusps were exposed to 10% or 15% cyclic stretch for 14 days in the fully osteogenic medium supplemented with or without

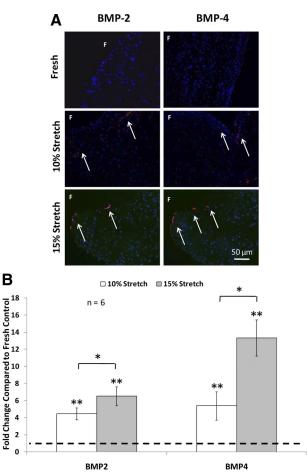


Figure 6. Representative micrographs of BMP-2 and BMP-4 immunohistochemical staining (**A**) and semiquantification (**B**) after three days of culture (10% or 15% stretch) in fully osteogenic DMEM compared with fresh controls. Expression of BMP was primarily observed on the fibrosa surface of the valve cusp. **Arrows** represent immunopositive cells. F indicates fibrosa. *P < 0.05; **P < 0.05 vs. fresh control.

the BMP inhibitor noggin. Then, total calcium content in each cusp was determined by calcium arsenazo assay (Figure 8A). Exposure of cusps to pathological stretch (15%) increased the calcium content by fivefold com-

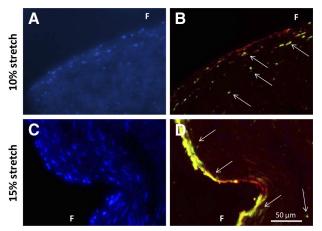


Figure 7. Representative micrographs of BMP-2 (green) and von Willebrand Factor (red) double immunohistochemical staining for samples stretched at 10% (A and B) and 15% (C and D) in fully osteogenic media. Cell nuclei are stained with 4',6-diamidino-2-phenylindole (blue) and presented in a separate image for clarity of viewing. Arrows represent immunopositive cells. F indicates fibrosa.

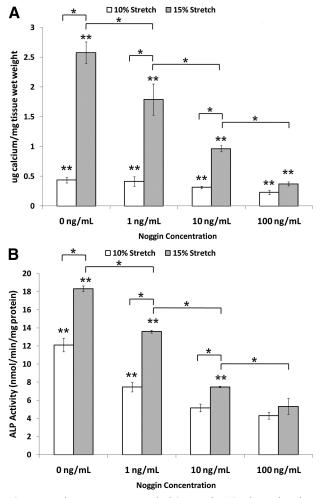


Figure 8. Calcium content in stretched (10% and 15%) valves cultured in fully osteogenic DMEM in 0, 1, 10, and 100 ng/ml noggin for 14 days (**A**) [n = 8]. ALP activity in stretched (10% and 15%) valves cultured in fully osteogenic DMEM in 0, 1, 10, and 100 ng/ml noggin for seven days (**B**) [n = 8]. *P < 0.05; **P < 0.05 versus fresh control.

pared with normal stretch (10%). Moreover, noggin blocked stretch-induced calcium increase in a concentration dependent manner (Figure 8A). As low as 1 ng/ml of noggin showed a significant inhibition (P < 0.05), reaching a maximum inhibition level at 100 ng/ml.

We next examined ALP activity in cusps exposed to 10% or 15% cyclic stretch for 7 days in the fully osteogenic medium. ALP activity in fresh cusp tissue was 1.7 \pm 0.8 nmol/min/mg protein. Fifteen percent stretch significantly increased ALP activity above that of 10% stretch at all concentrations of noggin (Figure 8B). Importantly, noggin treatment inhibited stretch-induced ALP activity in a concentration-dependent manner. These results suggest that calcification induced by a pathological level of stretch is mediated in a BMP-dependent manner.

Runx2 is a key transcription factor associated with osteoblast differentiation and is also a downstream transcription factor for BMP-2 and -4. Immunoblotting studies (Figure 9) demonstrated that Runx2 expression (Figure 9A) of aortic cusps was significantly increased by 7 days of 15% stretch in the fully osteogenic medium, in comparison with fresh controls (2.24-fold) and 10% stretch

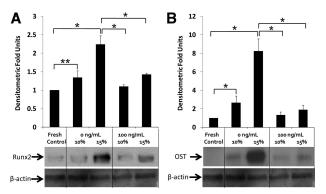


Figure 9. Runx2 expression in stretched (10% and 15%) valves cultured in fully osteogenic DMEM in 0 and 100 ng/ml noggin for three days (**A**) [n = 6]. Osteocalcin (OST) expression in stretched (10% and 15%) valves cultured in fully osteogenic DMEM in 0 and 100 ng/ml noggin for seven days (**B**) [n = 6]. *P < 0.05; **P < 0.01.

(1.67-fold). One hundred nanograms per milliliter noggin treatment inhibited stretch-induced expression of Runx2. The importance of stretch is also emphasized by the fact that there was no significant difference between fresh controls and normal (10%) stretch groups.

Identical trends were observed for osteocalcin expression (Figure 9B). Osteocalcin expression was significantly increased by both 10% (2.67-fold) and 15% (8.25fold) stretch when compared with fresh controls. These fold changes were greater than those observed for Runx2, which may be attributed to low basal levels of osteocalcin in a native aortic valve. In the presence of 100 ng/ml noggin, there was significant reduction in osteocalcin expression for both 10% (0.50-fold) and 15% (0.23-fold) stretched groups.

Discussion

The novel contributions of this study are the following: (1) we have demonstrated that the aortic valve can be calcified preferentially on the fibrosa side within a week in response to a pathologically relevant level of cyclic stretch and pro-osteogenic humoral conditions in ex vivo tissue culture; (2) pathological stretch induced apoptosis and BMP expression preferentially on the fibrosa side; and (3) the BMP antagonist noggin was able to block osteogenic and calcification events (ALP activity, calcium content, Runx2, and osteocalcin expression in the valve cusps/tissue) that were induced by stretch. This study therefore points to the BMPs, particularly BMP-2 and/or BMP-4 as key players in stretch-induced aortic valve calcification in a pro-osteogenic environment. These findings also suggest a potential importance of BMP antagonists in aortic valve calcification.

One of the most important findings of this current work is that aortic valve cusps can be calcified within a week by treating with a pathologically relevant level of stretch (15%) in fully osteogenic medium containing both high phosphate content (3.8 mmol/L) and TGF- β 1 (1 ng/ml). Neither the stretch nor the fully osteogenic medium alone could induce valve calcification within an experimental time frame of up to 14 days (data not shown). These results suggest that stretch and the fully osteogenic medium act in an additive manner. Although full mechanistic insights need additional studies, initial data suggest increased BMP-4 expression, cellular apoptosis, subsequent Runx2 and osteocalcin expression, and ALP activity as potential mechanisms. Reaching a threshold level of BMP by the additive actions of the mechanical (stretch) and atherogenic (TGF- β 1 and phosphate concentration) factors may be a key event in determining if the aortic valve undergoes calcification. A recent review article revealed that the specific atherogenic factors studied in the present study are especially important to the progression of valve calcification.¹⁵

The *ex vivo* tissue culture system used in this study is an accelerated model for calcification, obtaining expression of BMPs and ALP after 3 and 7 days, respectively, and significant increases in tissue calcium content after 14 days. It did not induce contamination and was able to maintain tissue viability for the experimental durations studied. An important contribution of this study is that this *ex vivo* system could be used to study valvular disease mechanisms on the bench-top before more detailed studies are done *in vivo*. Indeed, our studies may provide insight into possible mechanisms for stretch-induced/hypertension-induced valve disease. BMP-blockers appear to be a potential exciting target for future studies toward pharmacological treatment of aortic valve calcification.

It was observed that calcification and tissue expression of BMP was preferentially expressed on the fibrosa side of the valve. Although the reason for this occurrence is not clear, potential reasons could be the fact that the cells on the fibrosa side are genetically more prone to calcification,²⁹ or that the local *in vivo* hemodynamic conditions on the aortic side of the valve cusps prime them to be more procalcific in nature.²⁸ Additionally, most of the expression of BMPs was observed on the endothelial layer of the valve cusps (Figure 6). This is in agreement with previous results on the effects of pathological shear stresses on valve cusps.²⁸ It is speculated that the endothelial layer acts as the mechanosensor in the case of cyclic stretch.

Other studies have also demonstrated that addition of BMP and TGF- β 1 can independently result in osteogenic differentiation of aortic valve cells cultured in vitro.4.8 BMP-2 specifically can induce calcific nodule formation of aortic valve fibroblasts.³⁰ This study demonstrated that BMPs and TGFs are more closely related than previously thought, with addition of exogenous TGF- β 1 directly resulting in expression of BMP-2 and -4 after only 3 days. We reported recently that altered shear stresses result in aortic valve inflammation via a BMP-dependent pathway,²⁸ indicating a strong link between altered mechanical forces on the valve tissue and BMP-influenced valve dysfunction. This study is also in agreement with in vitro studies on mesenchymal cells where BMP signaling activated the chondro-osteogenic Runx2/Cbfa pathway.15 Increased serum phosphate concentrations have also been linked to activation of the Runx2/Cbfa pathway,¹⁵ which was also observed in this study.

It is believed that calcification could occur via either an apoptosis-driven pathway^{10,11,31} or via an osteogenic and more matrix-dependent pathway.^{10,11} Some studies

have also demonstrated that depending on the mechanical and biochemical environment both processes can potentially occur.^{4,11} These studies also demonstrated that TGF- β 1 stimulates cellular apoptosis.^{4,11} We demonstrated that cellular apoptosis was present for samples stretched to 15%, but to a lesser extent in 10% stretch. Apoptotic cells were predominantly expressed on the fibrosa, matching the observed pattern of preferential calcification on that same surface of the valve. This finding further lends strength to the speculation that valve calcification is side-specific. In addition, ALP activity, which is a marker for osteogenic differentiation was also higher at 15% stretch compared with 10% stretch. It is believed that both apoptosis- and osteogenic-driven calcification could be occurring, but further study is needed to confirm this.

It was demonstrated that noggin can effectively inhibit BMP-induced aortic valve calcification. Noggin was used in this study as an antagonist for BMPs. Other BMP antagonists include chordin and follistatin.³² Although these other molecules were not investigated, noggin is well established as a specific BMP antagonist with a weak dissociation constant (K_d) of 20 pM,²⁶ making it a good candidate for this study. Noggin has been shown to block the pro-inflammatory effects of BMP-4 expression on vascular endothelial cells.²⁷ Indeed, the value of noggin in this study is its ability to interfere with the action of BMPs while not affecting the expression of BMPs per se. Ultimately, valve calcification could be a result of a breakdown of this delicate balance between agonists (BMPs) and antagonists (noggin) for calcific progression.

The importance of mechanical cues on tissues such as the aortic valve is clearly underlined in this study, both for normal homeostasis as well as the progression of pathology. Matrix remodeling enzymes, which are also involved in valve calcification, and investigated in a previous studies, were also seen to be modulated by altered cyclic stretch.^{16,33} From these results, it can be speculated that elevated cyclic stretch primes the aortic valve to an activated state, which is more prone to disease. Indeed, in this study, the presence of pro-osteogenic conditions readily induced progression of valve calcification. In addition, altered shear stress increased BMP-dependent inflammation on the fibrosa surface of aortic valve cusps.²⁸ In a recent study, it was shown that matrix stiffness can modulate the differentiation of valve interstitial cells to a pathological phenotype.¹¹

In conclusion, this study strongly suggests the importance of BMPs in aortic valve calcific progression resulting from elevated stretch. Moreover, the importance of studying valve pathology in close relation with its mechanical environment is also clearly demonstrated. Further studies should focus on understanding the detailed mechanobiological signaling of BMP-induced valve cell osteogenic differentiation.

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