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## Patch-clamp amplifiers on a chip

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### Abstract

We present the first, fully-integrated, two-channel implementation of a patch-clamp measurement system. With this “PatchChip” two simultaneous whole-cell recordings can be obtained with rms noise of 8 pA in a 10 kHz bandwidth. The capacitance and series-resistance of the electrode can be compensated up to 10 pF and 100 MΩ respectively under computer control. Recordings of hERG and Na<sub>v</sub> 1.7 currents demonstrate the system's capabilities, which are on par with large, commercial patch-clamp instrumentation. By reducing patch-clamp amplifiers to a millimeter size micro-chip, this work paves the way to the realization of massively-parallel, high-throughput patch-clamp systems for drug screening and ion-channel research. The PatchChip is implemented in a 0.5 μm silicon-on-sapphire process; its size is 3 × 3 mm<sup>2</sup> and the power consumption is 5 mW per channel with a 3.3 V power supply.

### Keywords

patch clamp; amplifier; series resistance; integrated circuit; voltage clamp

## 1. Introduction

The patch-clamp amplifier is a ubiquitous tool for characterizing ion-channel activity. For the screening of pharmaceutical compounds or the characterization of expressed channels, high-throughput patch-clamp systems are being developed, where recordings are made from cells in each well of a 96 or 384-well plate. In these systems the recording is made not with a glass pipette, but from a planar electrode at the bottom of each well (Fig. 1). An important part of such highly-parallel recording systems is a high-density array of patch-clamp amplifiers. We present here a highly-miniaturized patch-clamp amplifier with complete whole-cell measurement capabilities.

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Important constraints in building massively-parallel patch-clamp systems have been the size and cost of the amplifiers, heat dissipation - which restricts the proximity of the amplifiers to the cells - and crosstalk between channels. The integrated “PatchChip” amplifier presented in this paper solves all of these design requirements, and is based on experience from our prototypes [1,2,3,4,5,6]. The dual-channel patch-clamp system occupies  $3 \times 3 \text{ mm}^2$  of area and consumes just 5 mW of power per channel. It is fabricated using a standard silicon-on-sapphire fabrication process, which allows parasitic capacitances and cross-talk effects to be minimized.

## 2. Materials and methods

Figure 2 shows a block diagram of one channel of the PatchChip system. The two channels of the system are identical. The main signal path is from the membrane current  $I_{in}$  to the monitor voltage output  $V_{out} = I_{in}R_f$ , through operational amplifiers A1, A2, A3.

Cells are stimulated by controlling the voltage  $V_p = V_{clamp}$  at the electrode and measuring the resultant ionic current  $I_{in}$ . The goal of the compensation circuits is to allow step changes to be applied to the cell membrane potential  $V_m$  while the ionic current  $I_i$  is measured. The cell membrane can be modeled as a capacitance  $C_m$  in parallel with the membrane resistance  $R_m$ . The headstage of the patch-clamp recording system consists of a current-to-voltage transimpedance amplifier A1. The feedback resistor  $R_f$  is selectable in eight steps from 50 k $\Omega$  to 10M $\Omega$ . Small shunt capacitors stabilize the feedback loop while yielding a bandwidth of a minimum of 300 kHz (with  $R_f = 10 \text{ M}\Omega$ ) when the total capacitance on the input node is 30 pF. A difference amplifier A2 subtracts  $V_{clamp}$  from the transimpedance output. The resultant output voltage  $V_{out}$  is proportional to the input current,  $I_{in}$ .

The output filter A3 represents two poles of a three-pole, 20 kHz anti-aliasing filter. The third pole is presented by an external capacitor and is the only “glue” component required for the analog interface between the PatchChip and the external A-D converter. Similarly, the two-pole input reconstruction filter A6, critically-damped with a time constant of 2  $\mu\text{s}$ , smooths the input command signal  $V_{com}$  delivered directly from an external D-A converter and prevents rapid steps from causing nonlinearities and slew-limiting in the other amplifiers of the system.

### 2.1. Electrode compensation circuitry

The system compensates for the difference between the actual membrane voltage  $V_m$  and the clamping voltage  $V_{clamp}$  due to the voltage drop across the pipette electrode series resistance  $R_s$ . The circuit also compensates for the current  $i_{prs}$  drawn by the electrode parasitic capacitance  $C_{prs}$  and by and by the seal leakage-resistance  $R_L$ .

$R_s$  compensation is necessary for two reasons. First, it allows accurate voltage clamping of the membrane by reducing the errors from the voltage drop across the series access resistance  $R_s$ . Second, the compensation reduces the time needed to charge  $C_m$  enabling the circuit to monitor ion-channel events occurring immediately after changes in  $V_{com}$  is applied [7]. The drop across  $R_s$  is predicted by adding a fraction of  $V_{out}$  to the applied membrane-command potential  $V_{com}$  by means of amplifier A5, to obtain  $V_{clamp}$ . The fraction of compensated series-resistance is determined by the 9-bit mDAC3, which at full-scale yields compensation for a resistance of  $10 \times R_f$ . mDAC3 was designed as a hybrid weighted-resistor and R-2R device to minimize the noise gain of the A5 stage. A passive phase-lag compensation circuit is included in the positive-feedback loop if desired, to improve stability when a high percentage of  $R_s$ , e.g. more than 90%, is compensated.

For effective  $R_s$  compensation the measured current must be equal to the current  $I_m$  flowing through  $R_s$ . The charging current of the parasitic electrode capacitance  $C_{prs}$  and the current through the leakage conductance  $R_L$  therefore must first be subtracted from the measurement of  $I_{in}$ . The capacitive-current subtraction is done by injecting a current  $i_{inj}$  through an integrated capacitor  $C_{inj}$  of 10 pF. The gain  $\alpha_{inj}$  of the amplifier A7 is determined by the 8-bit mDAC1 to be between 1 and 2. The compensated capacitance is equal to  $(\alpha_{inj} - 1)C_{inj}$ .

The differential amplifier A2 is unbalanced when the voltage-output mDAC2 is set to a gain different from its minimum value of 0.5. As its gain increases, subtraction is provided for the excess  $I_{in}$  on the input. The maximum gain of the 10-bit mDAC2 is unity, allowing for compensation of a leakage resistance as high as  $R_f$ . All three compensation circuits are controlled using a serial digital control bus. A 64-bit shift register and buffer register store the bit patterns for the mDACs and various switches in one patch-clamp channel.

## 2.2. Voltage swings and $R_f$

Modern patch-clamp amplifiers contain an additional ‘‘C-Slow’’ compensation circuit to remove the large current transients due to the charging of the membrane capacitance  $C_m$ , which is typically in the range of 20-40 pF. These circuits have been implemented as a first-order state-variable filter [7,8] in which the time constant is roughly 100  $\mu$ s to 1 ms. Due to the limited capacitor sizes, and therefore short time constants, that can be realized in a monolithic circuit, we decided not to provide this ‘‘slow capacitance’’ compensation. Instead, this compensation will be provided in software. We rely on the use of a 16-bit or higher resolution A-D converter to digitize the current-monitor signal  $V_{out}$  so that the large charging transients can be subtracted digitally.

In the absence of slow-capacitance compensation, the entire charging current of the membrane capacitance must be injected through the feedback resistor  $R_f$ . Thus the voltage swing available at the output of amplifier A1 becomes an important issue. We have used a 3.3 volt silicon-on-sapphire (SOS) process, so that the analog power-supply voltages are  $\pm 1.6$  V. Although the typical membrane-potential excursions are only in the range  $\pm 150$  mV, when  $R_s$  compensation is in use the excursions of  $V_p$  can be an order of magnitude larger.

Consider the case in which a fraction  $k$  of the series resistance is compensated. When a voltage step of magnitude  $\Delta V_{com}$  is applied to  $V_{com}$  the effect of the  $R_s$  compensation feedback is to produce an initial step  $\Delta V_p = \Delta V_{com}/(1 - k)$ . For example, a 150 mV step with  $k=0.8$  (80% compensation) yields an initial step of 750 mV. Even ignoring the current through  $R_L$  the initial current will be  $I_{in} = \Delta V_p/R_s$  and will have to be sourced through the feedback resistor  $R_f$ . Thus the initial voltage at the output of A1 ( $V_{out,A1}$ ) will need to be

$$V_{out,A1} = \frac{\Delta V_{com}(R_s + R_f)}{(1 - k)R_s} \quad (1)$$

If  $R_f$  is chosen to be equal to  $R_s$  in this example, the initial value of  $V_{out,A1}$  must be 1.5V, very close to the available supply voltage of 1.6V. To avoid amplifier saturation therefore, two steps must be taken. First,  $R_f$  must be kept to a low value, typically 5-10 M $\Omega$  in cases where  $R_s$  is in this resistance range. Second, amplifier A1 (and also other amplifiers in the circuit) must have a rail-to-rail output swing capability. The characteristics of the operational amplifiers are described in section 2.4.

The low value of the feedback resistor  $R_f$  means that the current-monitor signal of the PatchChip will have a substantial contribution from the resistor's thermal noise; in a 10 kHz

bandwidth this noise is 4 pA rms when  $R_f = 10\text{M}\Omega$ . The thermal noise arising in  $R_s$  is also large, and when its value is equal to  $R_f$ , its noise is equal to that from  $R_f$  at high frequencies  $f > f_c$ , where  $f_c = 1/(2\pi R_s C_m)$ . When  $R_s$  compensation is in use, which in effect increases the recording bandwidth beyond  $f_c$ , the two resistances  $R_f$  and  $R_s$  make nearly equal contributions to the noise variance. Thus the low value of  $R_f$  does result in increased noise, but the increase is moderate, about a factor of  $\sqrt{2}$  over the theoretical minimum noise due to  $R_s$  alone.

### 2.3. Silicon-on-sapphire technology

The PatchChip was implemented using the silicon-on-sapphire (SOS) technology. SOS offers several advantages over conventional bulk CMOS technology, as is illustrated in Figure 3. First, the absence of a conducting substrate greatly reduces parasitic capacitance and allows the fabrication of large, nearly-ideal resistors. In conventional bulk-CMOS processes the source and drain of each transistor is isolated from the substrate by a reverse-biased diode; these diodes contribute a considerable capacitance to each such node in the circuit. Even resistor elements, which are isolated from the bulk silicon by oxide layers, show considerable parasitic capacitance because the oxide layers are relatively thin. In SOS on the other hand, transistors and resistors are fabricated on top of the thick sapphire substrate (Figure 3) and therefore experience vastly smaller parasitic capacitances [9]. Second, the non-conducting substrate provides a better means of isolating devices on the substrate, yielding better cross-talk performance between patch-clamp channels. Third, the insulating substrate allows the power supplies for digital and analog parts of this mixed-signal circuit to be separated to obtain better noise performance. Fourth, the lower parasitic capacitance allows SOS devices to perform at faster speeds and lower power than those made using conventional bulk CMOS technology [10]. The final layout of the micro-chip implementing the two-channel patch-clamp system is shown in Figure 4. This layout is the physical implementation of the circuits reported in Figure 2.

### 2.4. High-performance operational amplifier design

A low-noise, rail-to-rail, constant-transconductance operational amplifier was designed specifically for this system [12]. SOS transistors have low output resistance and therefore yield low voltage gains; we therefore made extensive use of cascode circuits, obtaining with this three-stage design a DC gain of 75 db and a gain-bandwidth product of 12 MHz for unity-gain operation. Figure 5 shows the fabricated operational amplifier, which occupies an area of less than  $0.1\text{ mm}^2$ . Rail-to-rail operation of the amplifier is needed to maximize voltage swings with the small power-supply voltages. The amplifier reported a  $3\text{ nV}/\sqrt{\text{Hz}}$  of input-referred voltage noise in a bandwidth of 10 kHz, and  $< 1\text{ mV}$  of input-referred offset, while consuming 1.4 mW of power. Table 1 reports a summary of the amplifier characteristics.

## 3. Results

We have extensively tested the electrical properties of the two-channel patch-clamp system, and its functionality in patch-clamp recordings from cells. In these tests the system was controlled and data were acquired using the JClamp patch-clamp software ([www.scisoftco.com](http://www.scisoftco.com)). The results are comparable to those from commercial non-integrated patch clamp amplifiers.

Figure 6-A shows the measured step responses of the series resistance compensation circuit. The time constant  $\tau$  associated with charging the membrane capacitance  $C_m$  through a compensated resistance ( $R_S - R_{comp}$ ) when a step  $V_{com}$  is applied (inset), is given by  $\tau = C_m(R_S - R_{comp})$ . Increasing compensation,  $R_{comp}$  approaches  $R_S$  and  $\tau$  decreases, increasing

recording bandwidth. Using the series resistance compensation circuit, we compensated 3-4 M $\Omega$  of the 4 M $\Omega$  electrode series resistance, decreasing the time needed to charge  $C_m$  from  $\tau = 200 \mu\text{s}$  to  $50 \mu\text{s}$  (75% compensation) and about  $120 \mu\text{s}$  (100% compensation). Full resistance compensation can only be obtained with the phase-lag compensation circuit, which yields complete compensation at low frequencies but slows the settling time of the system.

Figure 6-B shows the measured step response of the electrode capacitive compensation circuit. When uncompensated, the headstage provides the current  $i_{prs}$  needed to charge the parasitic capacitance. This current appears as spikes in the current-monitor signal with the same polarity as  $V_{com}$ . When properly compensated, the spikes are greatly reduced in size.

Figure 7 shows measured simultaneous data from both channels of the system. We applied a large voltage step (100 mV) to one channel with a model cell connected to its input terminal. The cross-talk on the adjacent non-measuring channel is 40 dB lower even with 80% series resistance compensation in use.

Figure 8 shows a whole-cell recording from an HEK293 cell expressing hERG channels. We compensated the 6.5 pF parasitic capacitance, and 80% of the 4.2 M $\Omega$  series resistance present at the input.  $R_f$  was set to 5 M $\Omega$ . The peak tail current curve in part C shows the standard voltage dependence of inactivation and activation in the channels.

Sodium-channel currents present a particularly demanding test for a whole-cell recording system. The rapid kinetics and negative-resistance characteristic of these currents requires good  $R_s$  compensation. Figure 9 A shows single-sweep recordings from an HEK293 cell expressing Na $_v$  1.7 channels. Linear leak and residual capacitance artifacts were subtracted using the -P/6 method. This protocol (using six inverted pulse sequences scaled down by a factor of 6, delivered at negative membrane potentials) increases the net rms noise in the traces about three-fold. Despite the large cell capacitance ( $C_m = 40 \text{ pF}$ ) the clamp time constant was  $40 \mu\text{s}$ , giving a faithful current time course. The peak current-voltage curve (Figure 9 C) shows steep activation of the channel currents with no evidence of series-resistance error [11].

Table 2 summarizes the key features of the PatchChip. The 2-channel system occupies  $3 \times 3 \text{ mm}^2$  of area and consumes 5 mW of power per channel. The low power consumption allows the amplifiers to be placed in close proximity to the cells under test. The input-referred noise is 8 pA rms at 10 kHz bandwidth.

## 4. Discussion

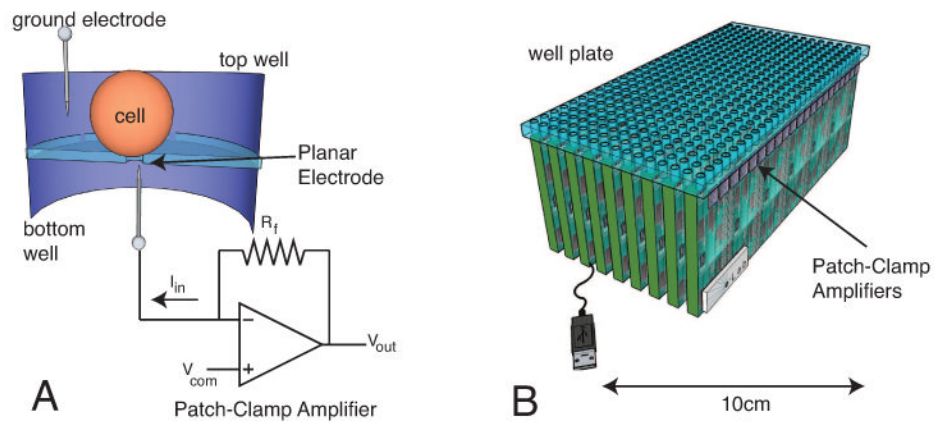
We have implemented a two-channel patch-clamp system in silicon-on-sapphire on a  $3 \times 3 \text{ mm}$  chip area. The system reports below  $-40 \text{ dB}$  of cross talk between adjacent channels and the input-referred current noise of the system is 8 pA rms in a 10 kHz bandwidth. The appropriate setting of the feedback resistor, 5-10M $\Omega$  for typical whole-cell recordings, means that the resistor's thermal noise makes a contribution; however this contribution is moderate in comparison to the thermal noise from the series resistance of the electrode-and-cell combination. The system is able to compensate series resistances and parasitic capacitances up to 100 M $\Omega$  and 10 pF respectively. The power consumption of the device is 5 mW per channel at 3.3 V. This accurate, low-noise system with electrode compensation can replace a commercial rack-mounted patch-clamp system; more importantly it can also be integrated into a massively parallel, high-throughput, patch-clamp system that can significantly advance the state-of-the-art in drug screening and ion-channel research.

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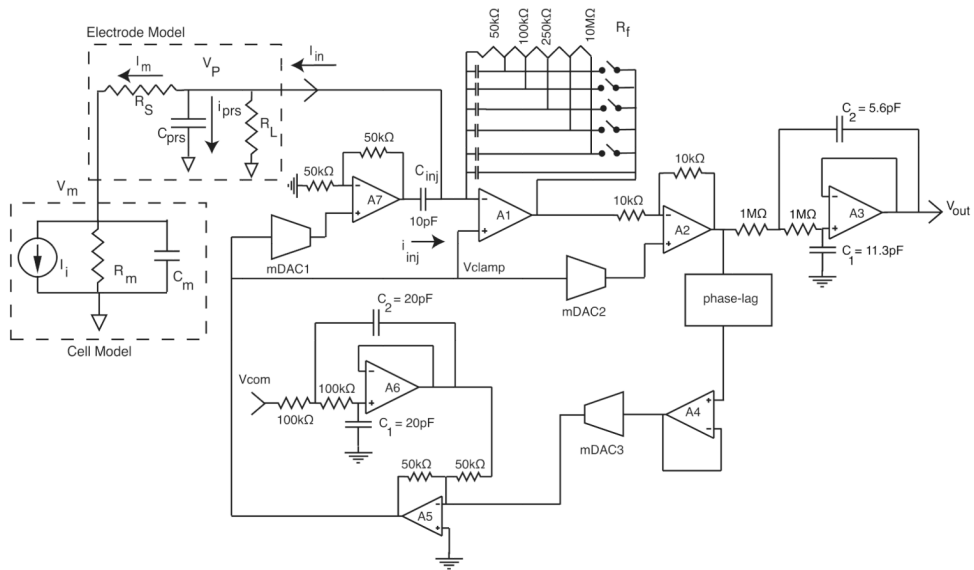
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**Figure 1.**

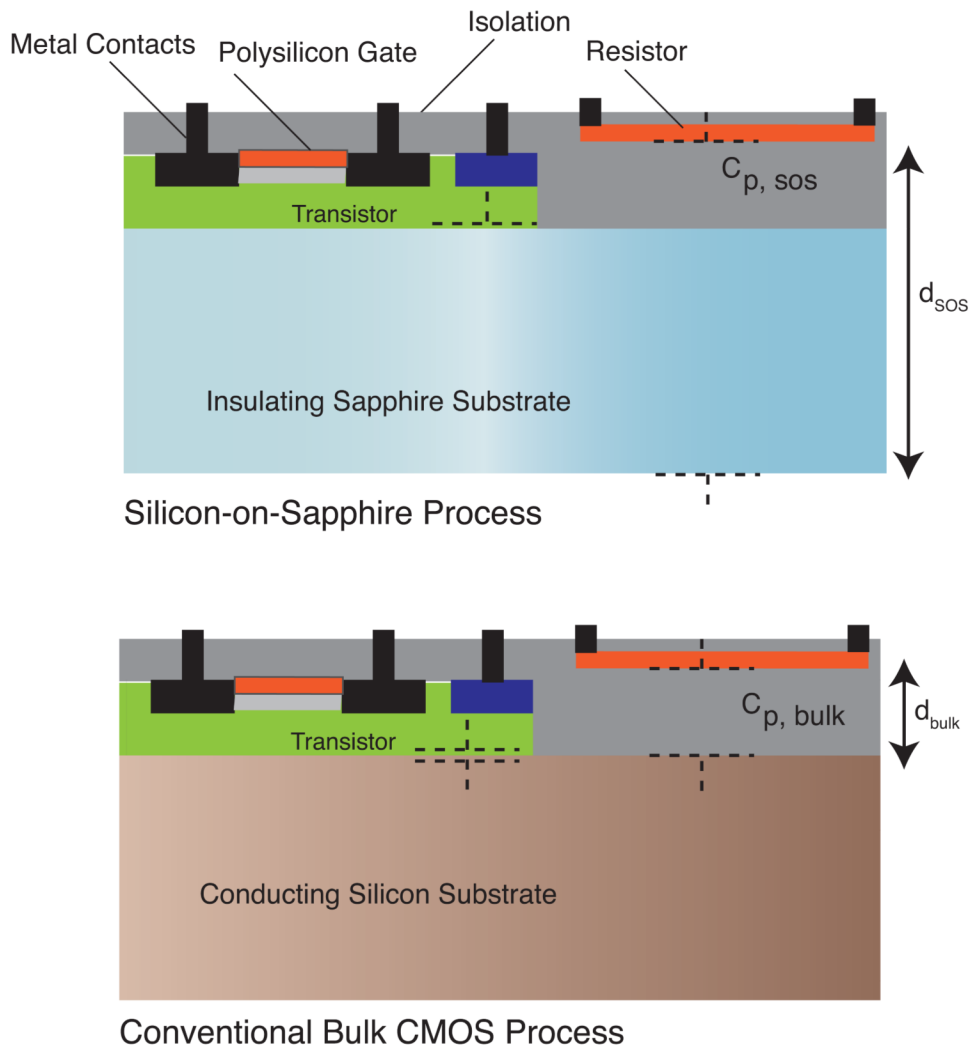
A - Patch-clamp amplifier performing whole-cell membrane current recording using a planar electrode. The planar electrode replaces the traditional glass micro pipette with a micron sized-aperture that is topologically equivalent to the glass tip of the pipette. Cells are introduced into a well, and when suction is applied, the cells seal into the aperture. Further suction is applied to rupture the cell so that a whole-cell configuration is established. B - Using the amplifiers presented in this paper, it is possible to design a high-throughput, automatic patch-clamp system that operates on entire 384 well plates. The wells on B are identical to the one in A. Requirements for the amplifier are millimeter-size dimensions and minimized heat dissipation, crosstalk and low fabrication cost.



**Figure 2.**

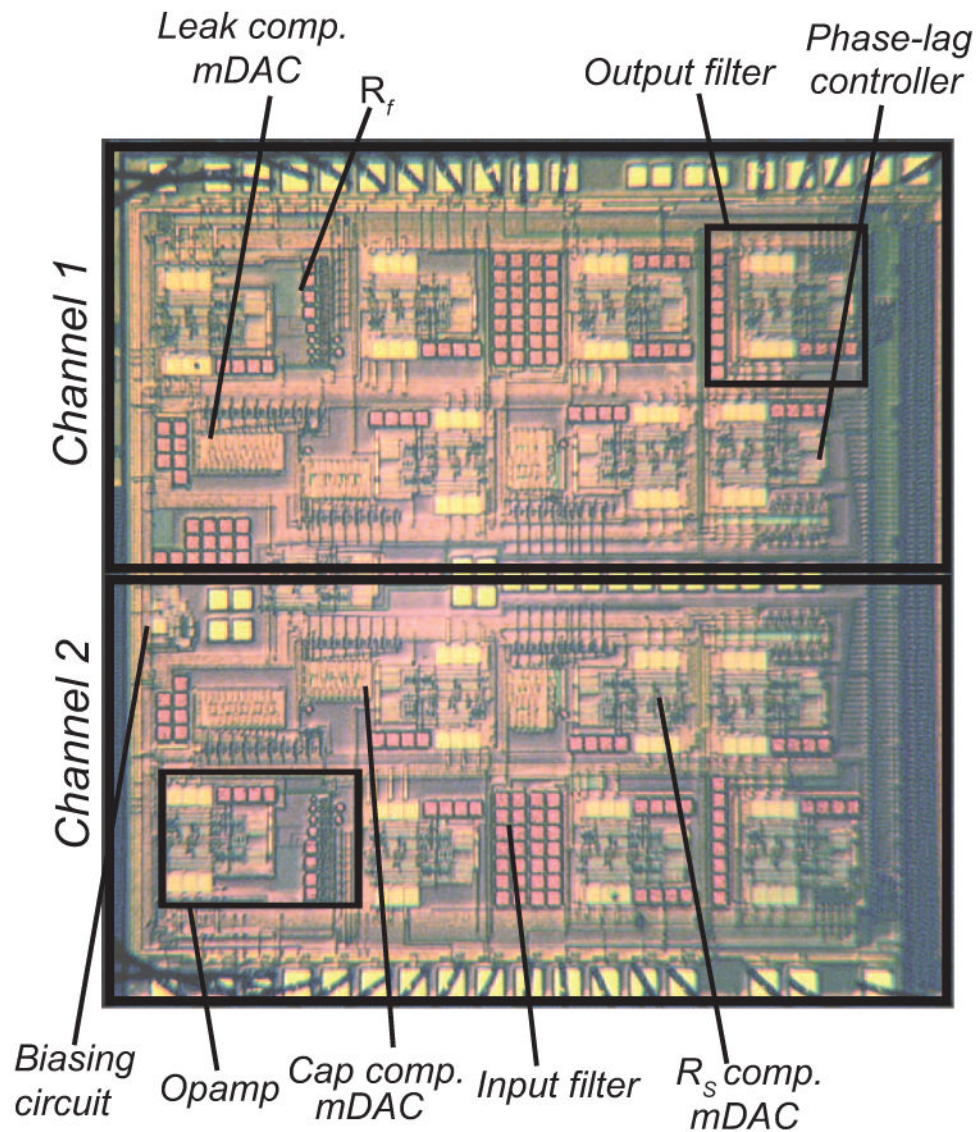
One channel of the two-channel integrated patch-clamp system and the electrical model of a cell and pipette electrode. The main signal path is from the membrane current  $I_m$  to the monitor voltage output  $V_{out} = I_m R_f$  through operational amplifiers A1, A2 and A3. Multiplying digital to analog converter mDAC 1 controls the parasitic capacitive compensation, mDAC 2 provides leak subtraction, mDAC 3 and the phase-lag controller circuit provides series resistance compensation. Input reconstruction and output anti-aliasing filters are also integrated. mDAC 1 and mDAC 2 are voltage-mode, R-2R DACs with  $R=50$  k $\Omega$ , minimum gains of 0.5, and resolutions of 8 and 10 bits, respectively. mDAC 3 is a 9-bit hybrid transconductance-mode DAC with a maximum transconductance of 0.2 mS. Typical values of the electrode and cell elements are  $C_{prs}=5$  pF,  $R_L=100$  M $\Omega$ ,  $R_S=10$  M $\Omega$ ,  $C_m=30$  pF,  $R_m=100$  M $\Omega$  and peak values of  $I_i$  are 1-10 nA.





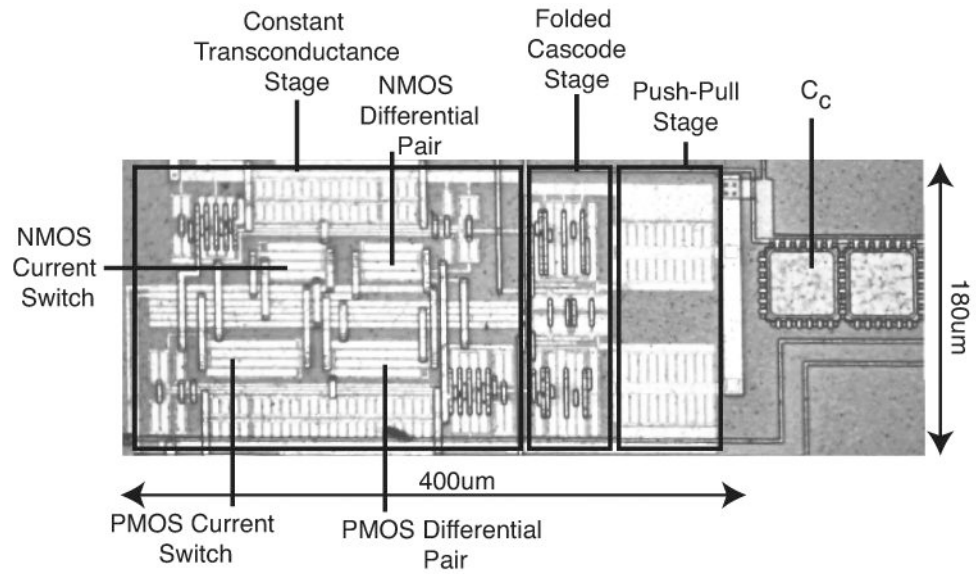
**Figure 3.**

The patch-clamp system was implemented using silicon-on-sapphire (SOS) technology. The insulating substrate in SOS (top) reduces parasitic capacitance and allows fabrication of large resistors to implement  $R_f$  with no degradation in frequency response. The insulating substrate reduces crosstalk between channels and allows devices to operate at faster speeds than conventional bulk CMOS technology (bottom).



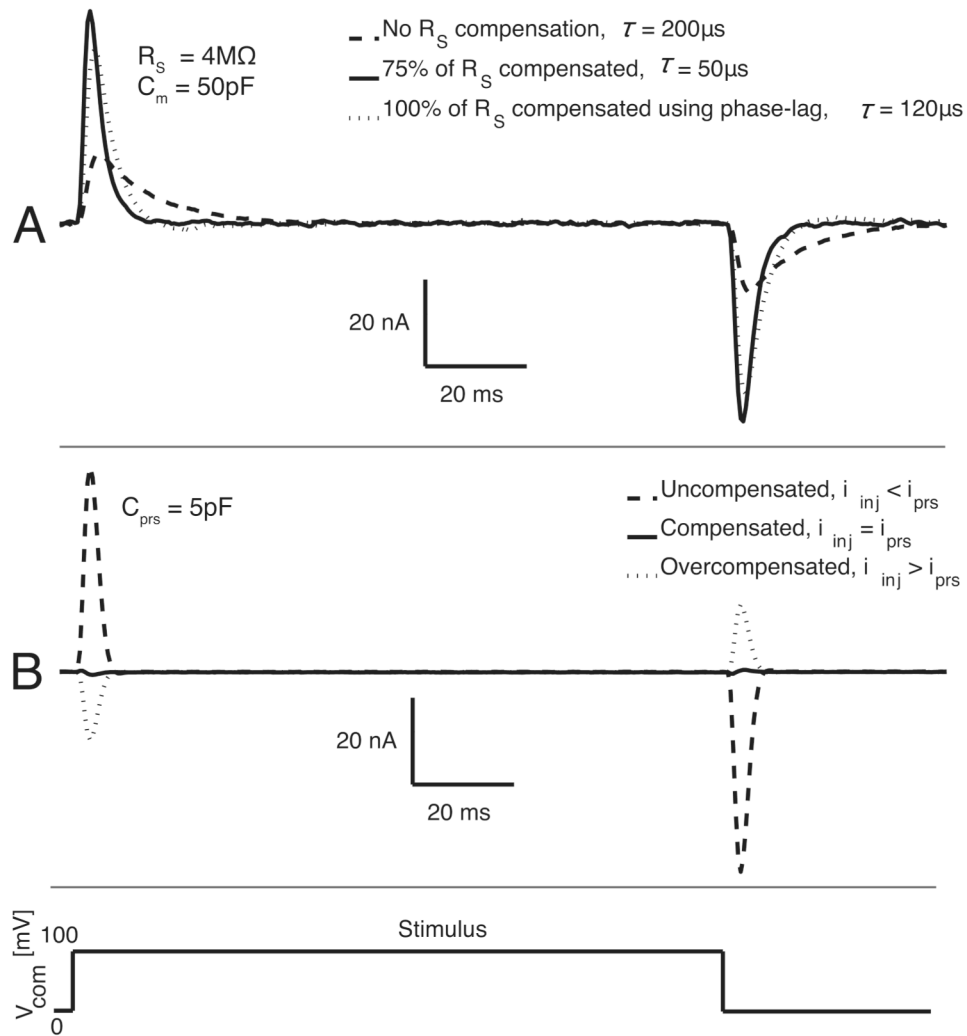
**Figure 4.**

A micrograph of the test circuit in silicon-on-sapphire technology. The fabricated die contained two channels and occupied just  $3 \times 3 \text{ mm}^2$ . Each channel has series resistance, parasitic capacitance and leak compensation capability. After initial setup expenditures, each amplifier costs just a few dollars to manufacture.



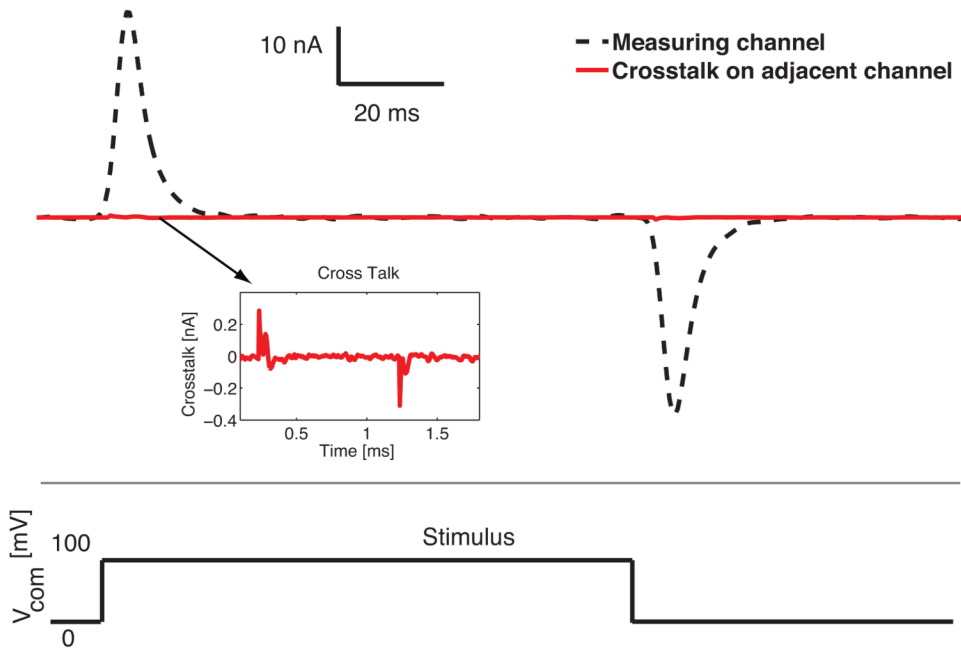
**Figure 5.**

A die micrograph of the fabricated operational amplifier. The operational amplifier occupies an area of  $0.08 \text{ mm}^2$  providing rail-to-rail output voltage and constant gain-bandwidth product over the entire rail-to-rail common-mode range. The capacitor  $C_c$  is the frequency-compensation capacitor.

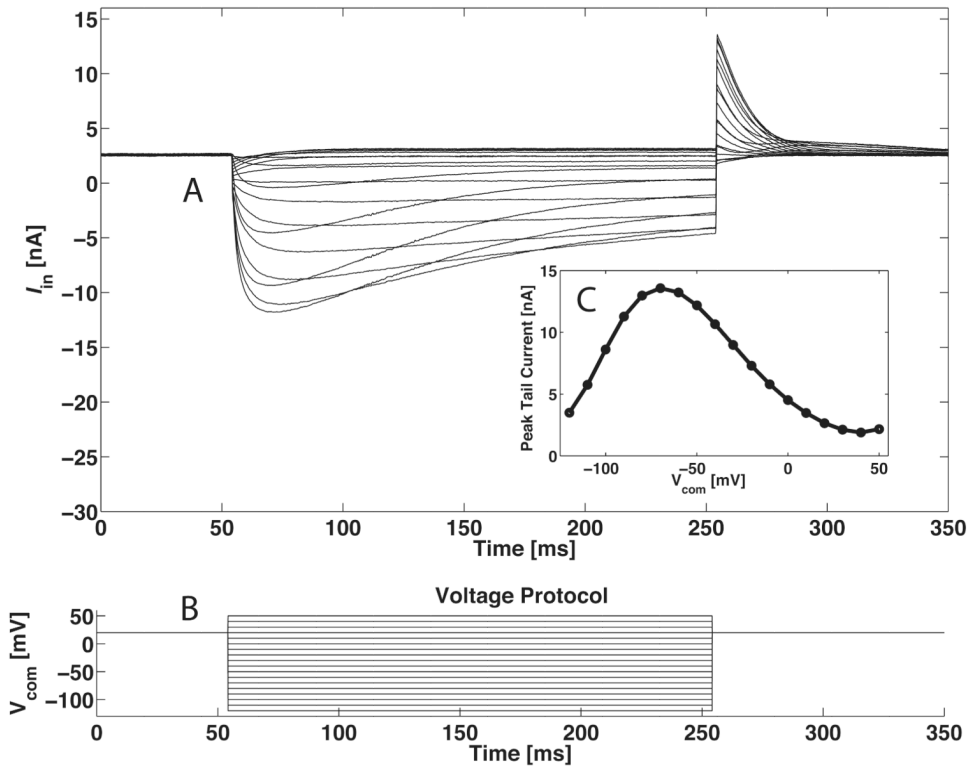


**Figure 6.**

A- measured response of the series resistance compensation circuit when compensating a 4  $\text{M}\Omega$  electrode series resistance. The time needed to charge  $C_m$  was reduced from  $\tau = 200\ \mu\text{s}$  to  $50\ \mu\text{s}$  (75% compensation) and  $120\ \mu\text{s}$  (100% compensation with phase-lag). B- measured step response of the electrode capacitive compensation circuit when compensating 5 pF at the input. When uncompensated, the headstage provides the current  $i_{prs}$  needed to charge the parasitic capacitance. This current appears as spikes in the current monitor signal. When properly compensated,  $i_{prs} = i_{inj}$  and the spikes do not appear. When overcompensated,  $i_{inj} > i_{prs}$  and the spikes reverse polarity.

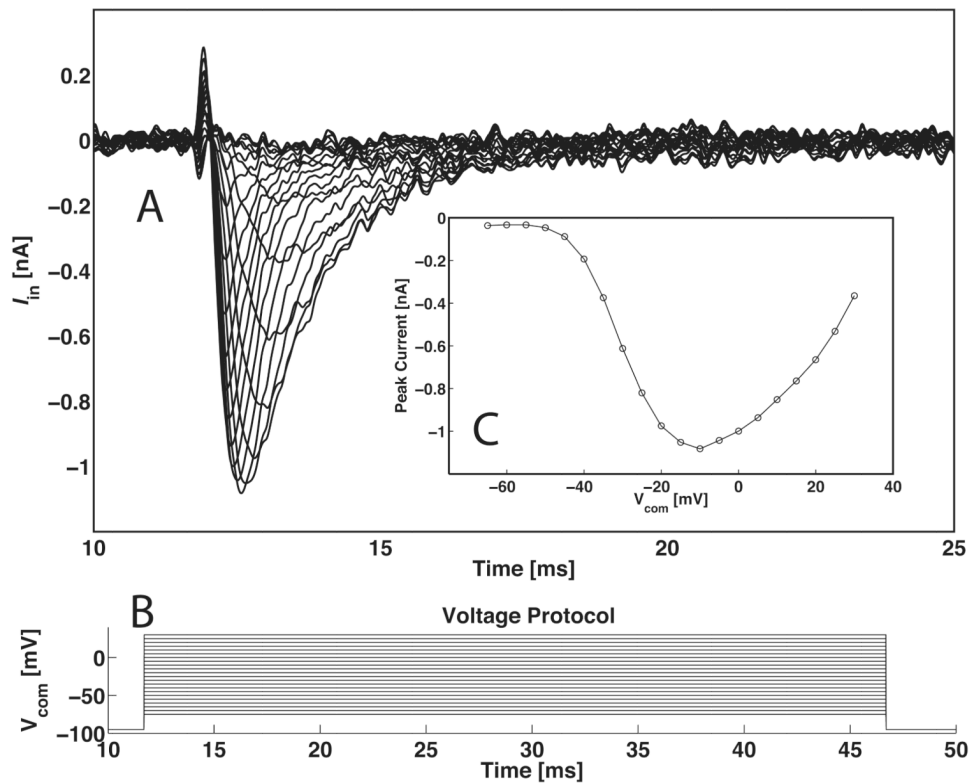


**Figure 7.** Measured crosstalk between channels. A voltage step of 100 mV was applied to one channel, which was driving a model circuit with 80% series-resistance compensation. The current-monitor signal in the adjacent non-measuring channel is at least 40 dB lower.



**Figure 8.**

A, single-sweep responses from an HEK 293 cell expressing hERG channels.  $R_s$  was 4.2 M $\Omega$  of which 80% was compensated.  $C_{prs}$  of 6.5 pF was fully compensated.  $C_m$  was 40 pF. B, the cells were held at 20 mV and stepped to potentials of -130 mV to 50 mV in 10 mV increments for 200 ms. C, the tail currents at +20 mV are plotted vs.  $V_{com}$  from A. The extracellular solution contained (mM) 117 NaCl, 13 KCl, 10 HEPES, 5 EGTA. The pipette solution contained 160 KCl, 1 EGTA, 10 HEPES. Currents were recorded at 100 kHz and filtered at 10 kHz.



**Figure 9.**

A, single-sweep responses of HEK 293 cells expressing Na<sub>v</sub> 1.7 sodium channels, after linear leak subtraction using the -P/6 protocol. The leak subtraction increases the net rms noise in the traces about three-fold.  $R_S$  was 4.5 M $\Omega$  of which 80% was compensated.  $C_{prs}$  of 7 pF was fully compensated.  $C_m$  was 40 pF. B, to generate activation curves, the cells were held at -100 mV and stepped to potentials of -75 mV to 30 mV in 5 mV increments for 35 ms. C, the peak currents vs.  $V_{com}$  from A. The current-monitor signal was filtered at 10 kHz and sampled at a 100 kHz rate. The recording was made at room temperature. The extracellular solution contained (in mM) 127 NaCl, 13 KCl, 10 HEPES. The pipette solution contained 10 NaCl, 140 CsF, 10 HEPES, 1 EGTA.

**Table 1**

Measurement results for the operational amplifier designed for the patch-clamp system. A load resistance of 15k $\Omega$  and a 3.3V power supply was used in the measurements. The operational amplifier met all design specifications.

Die Area	0.08 mm <sup>2</sup>
Open Loop Gain	75 dB
Gain-Bandwidth Product	12 MHz
Input-Referred Offset Voltage	0.4 mV
Input Common-Mode Range	0-3.3 V
Output Swing	0-3.3V
Slew Rate	10V/ $\mu$ s
Input-Referred Voltage Noise at 10 kHz	$3 \times 10^{-9} \text{V} \cdot \text{Hz}^{-1/2}$
Quiescent Current	430 $\mu$ A
Input Capacitance	2.6 pF



**Table 2**

Key features of the two-channel patch-clamp system.

Technology	0.5 micron Silicon-on-Sapphire
Number of channels	2 per die
Silicon area	3 × 3 mm per die 1.5 × 3 mm per channel
Power consumption	5 mW per channel at 3.3V
Capacitive compensation	10 pF max
Series resistance compensation	80% up to 10× $R_f$ , or 100% with phase-lag compensation
Leak compensation	conductance up to 1/ $R_f$
Current noise	8 pA rms input-referred in a 10kHz bandwidth ( $R_f=10\text{ M}\Omega$ )
Variable feedback resistor $R_f$	50, 100, 250, 500 k $\Omega$ 1, 2.5, 5, 10 M $\Omega$
Dynamic range	± 20 $\mu$ A
Reconstruction filter	2 poles, 60 kHz cutoff
Anti-aliasing filter	3 poles, 20 kHz cutoff
Nonlinearity	< 0.1 %
Cross talk between adjacent channels	−40 dB (at 80 % series resistance compensation)