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Optimized Temporary Biventricular Pacing Acutely Improves Intraoperative Cardiac Output After Weaning From Cardiopulmonary Bypass – A Sub-study of a Randomized Clinical Trial

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Abstract

Objective—Permanent biventricular pacing benefits patients with heart failure and interventricular conduction delay, but the importance of pacing with and without optimization in patients at risk of low cardiac output after heart surgery is unknown. We hypothesized that pacing parameters independently affect cardiac output. Accordingly, we analyzed aortic flow measured with an electromagnetic flowmeter in patients at risk of low cardiac output, during an ongoing randomized clinical trial of biventricular pacing (n=11) vs. standard of care (n=9).

Methods—A sub-study was conducted in all 20 patients, in both groups, with stable pacing after coronary artery bypass grafting and/or valve surgery. Ejection fraction averaged 33±15%, QRS duration 116±19 msec. Effects were measured within one hour of the conclusion of cardiopulmonary bypass. Atrioventricular delay (7 settings) and interventricular delay (9 settings) were optimized in random sequence.

Results—Optimization of atrioventricular delay (171 ± 8 msec), at an interventricular delay of 0 msec, increased flow 14% vs. the worst setting (111 ± 11 msec, p < 0.001) and 7% vs. nominal atrioventricular delay (120 msec, p < 0.001). Interventricular delay optimization increased flow

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10% vs. the worst setting (p < 0.001) and 5% vs. nominal interventricular delay (0 msec, p < 0.001). Optimized pacing increased cardiac output 13% vs. atrial pacing at matched heart rate (5.5 \pm 0.5 vs. 4.9 \pm 0.6 L/min; p = 0.003) and 10% vs. sinus rhythm (5.0 \pm 0.6 L/min; p = 0.019).

Conclusions—Temporary biventricular pacing increases intraoperative cardiac output in patients with left ventricular dysfunction undergoing cardiac surgery. Atrioventricular and interventricular delay optimization maximizes this benefit.

Introduction

Biventricular pacing (BiVP) is an established therapy for congestive heart failure (CHF), and it is currently the standard of care for select patients with advanced CHF associated with left ventricular (LV) dysfunction and intraventricular conduction delay (IVCD).¹ Permanent BiVP improves LV dimension and function and decreases morbidity and mortality, although it is associated with a nonresponse rate of up to 30%.2⁻⁵ While the long-term benefits of BiVP are typically not appreciated until several months after implantation, hemodynamic effects of changes to pacing parameters are reflected acutely by metrics such as stroke volume, ventricular dyssynchrony, and the maximal first derivative of pressure (dP/dt_{max}). 6^{,7} These properties have facilitated the study of the optimization of programmable BiVP parameters, such as atrioventricular (AV) delay (AVD) and interventricular delay (VVD), to maximize the hemodynamic benefit of BiVP and to reduce its nonresponse rate. ^{8–}10

The acute hemodynamic effects of BiVP also enable the study of temporary BiVP as a treatment for low output states after cardiac surgery. Low LV ejection fraction (LVEF) is an independent risk factor for poor outcomes following cardiac surgery.¹¹ BiVP improves hemodynamics without increasing myocardial oxygen consumption,8 and, therefore, it is particularly appealing as a potential therapy in cardiac surgery patients. Prior studies have assessed temporary perioperative BiVP in heterogeneous groups of patients with varying results.12⁻²⁴ Moreover, the role of optimization of temporary BiVP parameters in the perioperative setting is unclear.^{25,26}

The BiVP After Cardiac Surgery (BiPACS) trial is a randomized clinical trial to study the effect of optimized temporary BiVP on cardiac output (CO) in postoperative cardiac surgery patients with preoperative LV systolic dysfunction and an IVCD. Patients undergo BiVP optimization at multiple time points in the intraoperative and postoperative periods and are randomized to continuous optimized BiVP vs. standard of care. The hypothesis underlying the BiPACS trial is that CO will increase 15% in patients undergoing temporary BiVP. In this sub-study of the BiPACS trial, we hypothesized that optimization of pacing parameters would increase CO. Accordingly, we assessed the contribution of AVD and VVD optimization to the effect of BiVP optimization in the intraoperative period, following separation from cardiopulmonary bypass (CPB), and evaluated the effect of optimized BiVP on CO as compared to atrial pacing (AAI) and to sinus rhythm with no pacing (NSR).

Methods

BiPACS Study Population

The study protocol was approved by the Columbia University Medical Center Institutional Review Board. Adult patients undergoing elective open-heart surgery on CPB were screened for eligibility to enroll in the BiPACS trial. All patients gave written, informed consent. Recruitment was done prior to the day of surgery by qualified and trained study coordinators and investigators on the study team with permission of the Attending surgeon. Inclusion criteria included: preoperative CHF, LVEF ≤40% and QRS duration ≥100 msec, or patients undergoing combined mitral and aortic valve surgery. LVEF and QRS criteria were

liberalized from values of 35% and 120 msec, respectively, in the original protocol. Exclusion criteria included: atrial fibrillation, second or third degree AV block, congenital heart disease, intracardiac shunts, or heart rate >120 beats per minute (bpm) after separation from CPB. Preoperative data obtained by chart review included: LVEF, as measured by echocardiogram or left ventriculogram; heart rhythm, QRS duration, and intraventricular blocks from electrocardiogram (EKG) tracings; the type of surgery performed; and demographic characteristics. The BiPACS trial is ongoing, and endpoints will not be examined until 212 patients have been randomized.

Study Design and Optimization Protocol

To avoid imbalances that may occur using simple randomization, patients in the BiPACS trial are randomized to the two treatment groups at the end of Phase I, using randomly permuted blocks of four, six, and eight. A treatment allocation ratio of one to one was used; each group will be of equal size. The Phase 1 testing described here occurs in all patients, prior to randomization. Optimization of AVD, ventricular pacing site, and VVD are tested in random sequence. Randomization and testing sequences are determined by forms in sealed envelopes that are not opened until needed. These forms were prepared prior to the enrollment of the first patient. Before separation from CPB, temporary epicardial pacing leads were sewn to the right atrial (RA) appendage, anterior right ventricle (RV), and two randomized sites, out of six possible sites, on the LV. One of the LV leads (LV1) was placed at the basal LV at either the obtuse margin, circumflex, or posterior regions; the second LV lead (LV2) was placed at either the mid infero-medial, mid infero-lateral or apical LV. Data from BiVP using LV1 were analyzed in this study. The leads were attached to a Medtronic InSync III permanent biventricular pacemaker (Medtronic, Inc, Minneapolis, MN), mounted in an external housing unit, and their sensing and pacing functions were tested and confirmed. An appropriately sized electromagnetic flow probe (Carolina Medical Electronics, East Bend, NC) was placed on the ascending aorta. After separation from CPB and establishment of stable inotrope and vasopressor dosing, the BiVP optimization protocol was initiated. The pacing rate was set at 90 bpm, or at 10 bpm above the patient's intrinsic heart rate if greater than 90 bpm to ensure atrial capture, up to a maximum of 120 bpm. These heart rates were selected empirically. A wider range of heart rates is studied in phase 3 of the BiPACS trial, including cardiac resynchronization therapy at the intrinsic heart rate.

Real-time aortic volume flow, EKG, and arterial pressure signals were collected with an analog-to-digital converter (PowerLab, ADInstruments, Inc., Milford, MA) and recorded on a personal computer (iMac, Apple Computer, Inc, Cupertino, CA) (Figure 5). CO was measured by integrating aortic volume flow tracings over one respiratory cycle using MacLab software (ADInstruments, Inc, Milford, MA) and custom designed routines in Matlab (The MathWorks, Inc, Natick, MA).

BiVP optimization was performed by optimization of AVD, followed by VVD. All pacing settings during optimization were conducted over 10-second intervals and were tested twice. The use of a rapid optimization protocol measuring changes in cardiac mechanics over brief intervals has been described previously.^{14, 27} AVD optimization was performed during sequential RA-BiVP, with a VVD of 0 msec. AVD was varied in 30-msec increments, ranging from 90-270 msec, in randomized order. AVDs that were longer than the patient's intrinsic paced AVD were not tested. The AVD yielding the highest CO was selected as the optimum AVD. AVD optimization data from a representative patient is shown in Figure 1. VVD optimization was then performed, using the optimum AVD, by varying VVD by 20-msec increments, ranging from -80 msec (LV first) to +80 msec (RV first), in randomized order. CO as a function of VVD was plotted, and the VVD yielding the highest CO was selected as the optimum VVD (Figure 2), thereby defining the optimum BiVP parameters for the patient. Optimized BiVP was then compared to RA pacing (AAI mode), at the same

heart rate, and to NSR with no pacing in randomized order, over 30-second intervals. The aortic flow probe was then removed and the temporary pacing leads were externalized for further BiVP optimization in subsequent phases of the BiPACS trial.

Statistical Analysis

For AVD and VVD optimization data and for the comparison among optimized BiVP, AAI, and NSR, descriptive statistics were calculated for each group. Differences among multiple groups (3) were tested using blocked, one-way Analysis of Variation (ANOVA). Post hoc comparisons to assess pairwise differences between groups were performed using the Tukey test adjusted for multiple comparisons. Differences between two groups were tested using a two-way paired Student's t-test. P values of <0.05 were considered significant. Statistical analysis was performed using SAS 9.1 (SAS Institute, Inc., Cary, NC).

Results

Patient flow for the BiPACS trial and this sub-study covers recruitment from 4/1/07 to 6/2/09. The number of patients screened was 2,261, and 60 were enrolled. Thirty-three patients received the intended testing in Phase 1 and were subsequently randomized to BiVP (Experimental Group) or standard of care (Control Group). There were no adverse events during Phase 1. The number of these patients for whom the primary endpoint was measured was 13 in the BiVP group and 13 in the standard of care group. The study has not been completed, however, so no analysis of primary and secondary outcomes has been done, and the present study only describes results for Phase 1. Accordingly, the data after randomization and the period of follow-up are not relevant and are not summarized.

Among the 33 patients who received Phase I testing in the BiPACS trial, 13 were eliminated from this sub-study because of frequent ventricular ectopy, an intra-aortic balloon pump, or noisy aortic flow tracings. Ultimately, of the 20 patients included in this sub-study, there were 13 without second or third degree AV block who completed comparison of optimized BiVP, AAI, and NSR. Baseline clinical characteristics are shown in Table O-1.

The majority of patients underwent valvular surgery, including double valve cases, as well as combination valve and coronary artery bypass graft (CABG) surgery. Average demographics were age 67±12 (S.D.) years, male gender 75%. LVEF averaged 33±15%, and average QRS duration was 116±19 msec. Nine patients underwent combined CABG and aortic and/or mitral valve replacement. Five underwent combined aortic and mitral valve surgery, three underwent aortic surgery alone, and three underwent isolated CABG.

Results of AVD and VVD optimization are shown in Figure 3. The intrinsic, paced AVD was >150 msec in all patients and >270 msec in 10 patients. The mean optimum AVD was 171 ± 8 msec vs. 111 ± 11 msec for the mean worst AVD (p < 0.001). The optimum AVD was >150 msec in 10 patients and >120 msec in all but two patients. Comparison of mean CO for the optimized, worst, and nominal (120 msec) AVD settings showed significant differences among groups (p < 0.001). In pairwise comparisons, mean CO was different in both the optimum and worst groups, compared to that of AVD 120 msec. BiVP with the optimum AVD differed from the worst AVD (p < 0.001), with a mean increase in CO of 14% (range: 2-34%). The optimal AVD differed from an AVD of 120 msec (p < 0.001), with a mean increase in CO of 7% (range: 0-34%).

VVD optimization after AVD optimization yielded significant differences in CO when comparing the optimum, worst, and nominal (0 msec) VVD settings (p < 0.001) (Figure 3). In pairwise comparisons, both the optimum and worst VVD differed from the nominal VVD. BiVP with the optimum VVD differed from the worst VVD (p < 0.001), increasing

Distributions of optimal and worst AVDs and VVDs are shown in Figures O-6 and O-7, respectively. An AVD of 90 yielded the lowest CO in the majority of patients. In all but two patients, the optimal AVD was >120 msec, and, in three patients, an AVD of 120 msec was the worst setting. VVD optimization resulted in a pattern of optimum and worst VVD settings, ranging from RV-first to LV-first pacing, likely reflecting heterogeneity in the types of IVCD among patients. In two patients, the nominal VVD yielded the lowest CO.

Comparison of optimized BiVP to AAI and NSR is shown in Figure 4. The differences among the three groups were significant (p = 0.003), as were pairwise comparisons between optimized BiVP vs. AAI and NSR (p = 0.003 and 0.019, respectively). Optimized BiVP resulted in an increase in mean CO by 13% vs. AAI at the same heart rate (CO 5.5 ± 0.6 vs. 4.9 ± 0.6 L/min) and by 10% vs. NSR (5.0 ± 0.5 L/min). The paced heart rate was greater in the BiVP and AAI groups (97 ± 3 bpm), compared to the NSR group (80 ± 4 bpm) (p < 0.001).

Discussion

Defining the best modality and method for permanent BiVP optimization, in order to improve BiVP response rates and heart failure outcomes, is an active area of investigation. To our knowledge, the BiPACS trial is the first randomized clinical trial to assess the role of temporary BiVP optimization at multiple time points in the perioperative cardiac surgery setting. In this sub-study, which focused on intraoperative BiVP in the immediately post-CPB period, we found that BiVP optimization increased CO compared to both AAI and NSR (no pacing), with significant contributions from optimization of both AVD and VVD (Figure 3). The difference in CO between the best and the worst settings was considerable, ranging as high as 34% in an individual patient. Moreover, in five patients, programming a nominal AVD or VVD resulted in the least effective BiVP setting, which supports a rationale for routine optimization in all patients undergoing temporary BiVP.

AVD optimization represents a balance between optimizing LV filling and atrial emptying and minimizing diastolic mitral regurgitation. Nominal, "out of the box" AVD settings are typically programmed to short intervals, such as 120 msec, to ensure biventricular capture. However, empiric use of short AVDs may routinely underestimate the optimal AVD.²⁸ Longer intrinsic paced AVDs, in the post-CPB period, allowed for testing of AVDs greater than or equal to 240 msec in the majority of patients. AVD optimization alone resulted in a 14% increase in CO between the best and worst settings and a 7% increase compared to an AVD of 120. In all but two patients, the optimum AVD was longer than 120 msec (Figure O-6). Indeed, in the immediate post-CPB period, factors contributing to impaired diastolic function, such as myocardial ischemia and edema, may necessitate the use of longer AVDs in patients with impaired LV function. In this study, atrio-BiVP was achieved by pacing from the RA. RA pacing alters interatrial delay and the timing of left atrial-LV contraction, which implies that the optimum AVD would differ in RA paced, biatrially paced, and atrial-sensed BiVP modes.^{29, 30}

Modulation of VVD has been shown to reduce ventricular dyssynchrony and improve hemodynamic parameters.^{9, 10} In the present study, VVD optimization increased CO by 10% and 5% compared to the worst and nominal settings, respectively, underscoring the additional benefit of VVD optimization, even after AVD has been optimized. Whether the sequence in which AVD and VVD are optimized affects the determination of optimized BiVP parameters is uncertain and warrants further study.

Optimized BiVP improved CO by 13% compared to AAI at the same heart rate, indicating that the mechanism of hemodynamic benefit in BiVP was not explained solely by an increased paced rate compared to the patient's intrinsic sinus rate (Figure 4). This finding is consistent with previous studies of temporary BiVP.^{13, 17}

In this study, the mean preoperative LVEF (33.4%) was higher and the mean QRS (115.7 msec) was narrower than in permanent BiVP trials (Table O-1).²⁻⁵ Although the criteria for permanent BiVP implantation are established,¹ the predictors of acute response to temporary perioperative BiVP have yet to be defined and are an area of ongoing investigation. Cardiac surgery and extracorporeal circulation cause transient myocardial depression and edema and may exacerbate conduction abnormalities. Patients with pre-existing LV dysfunction are among the highest risk cardiac surgery patients and are an appropriate group in which to assess the benefit of temporary BiVP. Recent evidence suggests that ambulatory CHF patients with narrow QRS complexes do not benefit from permanent BiVP, despite exhibiting echocardiographic evidence of dyssynchrony.³¹ Whether this applies to temporary perioperative BiVP remains to be seen, especially in a heterogeneous population of ischemic and valvular heart surgery patients.

The mechanism by which BiVP acutely reduces dyssynchrony and improves hemodynamics is not fully understood, particularly in perioperative ventricular failure. We have previously described animal models of acute right- and left-sided heart failure and found BiVP to be beneficial in those settings.³²⁻³⁴ The mechanism of action appears to be synchronization of pressure development across the interventricular septum, which allows the less impaired ventricle to assist the failing one.³⁴ These findings provide further rationale for studying temporary BiVP in the perioperative setting and will serve as a guide for future studies examining the mechanism behind the effect demonstrated in this study.

Another area of uncertainty lies in selecting the best metric by which to assess BiVP optimization, including: measures of ventricular dyssynchrony, mitral inflow, stroke volume, and dP/dt_{max}. The present study optimized BiVP based on CO, which is an important short-term endpoint for end-organ perfusion, particularly in critically ill, postoperative patients with low output states. Further study is needed to evaluate the relationship between hemodynamic responses to temporary BiVP, changes in ventricular synchrony, and patient outcomes.

Outcomes data including morbidity, mortality, ICU length of stay, and hospital costs are important secondary objectives of the BiPACS trial. Though the absolute changes in CO reported here during BiVP are relatively modest, the clinical impact may be important if amplified by a reduced requirement for beta agonists and vasopressors, with secondary improvements in peripheral organ function, fluid requirements, and incidence of arrhythmias.

Accumulating data indicate differences between patients in the BiPACS trial and those undergoing permanent BiVP for chronic heart failure. The optimal BiPACS protocol changes over time, and the effect also changes, with benefits being primarily rate-related on postoperative day number one but primarily related to stroke volume increases in the early post-CPB period. Absolute increases in CO during BiVP also tend to be larger in BiPACS patients with higher preoperative EFs, contradicting observations in chronic heart failure.³⁵ These differences suggest that the effects of BiVP in BiPACS are primarily mediated through effects on reversible myocardial injury rather than chronic dysfunction. These differences provide a rationale for expanding the selection of patients in our trial beyond the current recommendations for permanent BiVP. Digital transesophageal echo data capable of

defining changes in regional wall motion abnormalities is an important research goal of the BiPACS trial.

The BiPACS trial is being done under an Investigational Device Exemption from the Food and Drug Administration because, as this is written, there is no biventricular pacemaker approved for temporary pacing in the operating room. Similarly, until our trial is completed, we will not have definitive information regarding optimum LV lead locations. Empirically, temporary BiVP can be implemented by adding a temporary bipolar lead configuration to the lateral basal segment of the LV. These leads can be connected to the output terminals of a standard external temporary pacemaker in conjunction with bipolar temporary RV leads connected to the same terminals. This will result in BIVP with a VVD of zero. AVD can then be optimized empirically, using MAP or aortic flow criteria. Our current observations indicate that the optimum AVD may be as long as 300 msec in the early postoperative period, particularly in patients with atrial latency in excess of 100 msec (Rusanov A, et al., unpublished data).

In conclusion, optimization of temporary BiVP improves CO in patients undergoing cardiac surgery with preoperative evidence of LV systolic dysfunction and an IVCD. Individualized optimization of AVD and VVD each contributes to the overall benefit of optimized BiVP, and optimization should be considered as a routine step in temporary BiVP protocols. Temporary BiVP to treat low output states after cardiac surgery is a promising area of investigation. Further studies with larger numbers of patients will better define patient selection criteria and refine optimization techniques.

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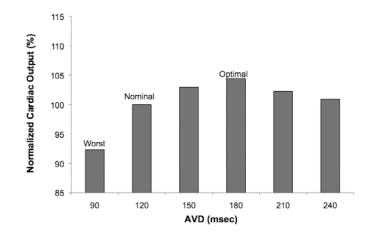
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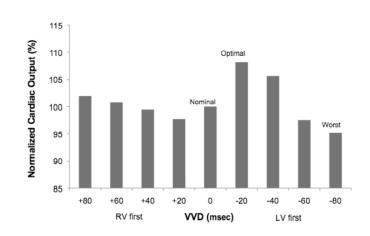
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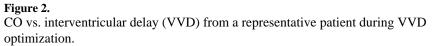
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Cardiac output (CO) vs. atrioventricular delay (AVD) from a representative patient during AVD optimization.





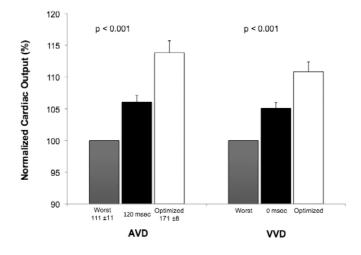


Figure 3.

BiVP optimization profiles for AVD and VVD. Mean COs are normalized to a scale of 100, with the worst parameter as the reference group. Error bars depict one standard error of the mean.

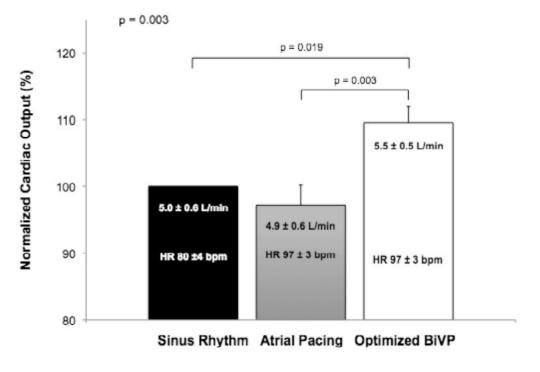


Figure 4.

Comparison of CO with optimized BiVP vs. right atrial pacing or sinus rhythm. Error bars depict one standard error of the mean.

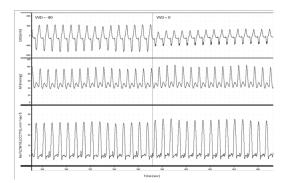
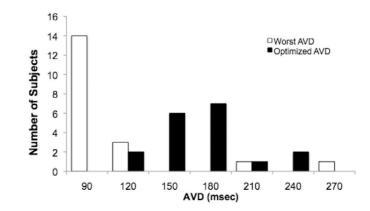


Figure 5.

Intraoperative recordings from a representative patient displaying changes in electrocardiogram (EKG), arterial pressure (AP), and aortic flow velocity during biventricular pacing (BiVP) optimization.





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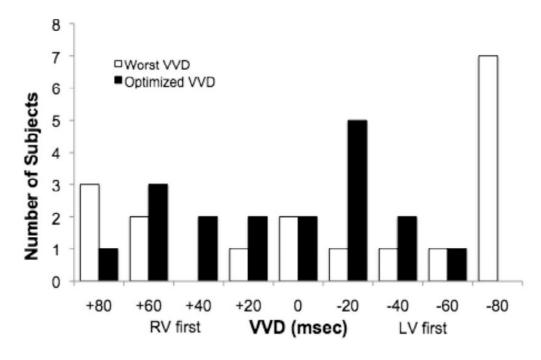


Figure 0-7. Distribution of optimal and worst VVD settings determined during VVD optimization.

Table O-1

Baseline Characteristics (ON LINE ONLY)

20
20
13
67.6 ± 12.2
33.4 ± 15.4
115.7 ± 19.1
75
9
5
3
3

BiVP, biventricular pacing; AAI, atrial pacing; SD, Standard Deviation; CABG, coronary artery bypass grafting; AVR, aortic valve replacement; MVR, mitral valve replacement or repair.