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### Hypofractionation for Prostate Cancer

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#### Abstract

Hypofractionation for prostate cancer was originally carried out in the pursuit of efficiency and convenience, but has now attracted greatly renewed interest based upon a hypothesis that prostate cancers have a higher sensitivity to fraction size, reflected in a low  $\alpha/\beta$  ratio, then do late responding organs at risk such as the rectum or bladder.

Tumor control and acceptable toxicity outcomes from several hypofractionation or brachytherapy analyses do in fact support an  $\alpha/\beta$  ratio for prostate cancer that is low, perhaps even lower that that for the normal organs that ordinarily constrain the delivery of radiation therapy. However, many of these studies lack sufficient patient numbers and follow-up, are clouded by dose inhomogeneity issues in the case of brachytherapy, or delivered effective doses that were too low by contemporary standards. Thus, the clinical efficacy of the approach has yet to be fully validated.

However, a number of newer prospective trials, some randomized, are underway or have reached accrual await sufficient follow-up for analysis. These studies, which cover a wide range of doses per fraction, should ultimately be capable of validating the utility of prostate hypofractionation and the models that predict its effects. With hypofractionation's significant potential for therapeutic gain, cost savings and improved patient convenience, the future management of localized prostate cancer could be profoundly altered in the process.

#### Keywords

prostate cancer; hypofractionation; stereotactic body radiotherapy; fractionation

#### Introduction

Dose escalation, which has been demonstrated to improve biochemical control, can be accomplished with acceptably low toxicity using conformal radiotherapy techniques, but at the expense and inconvenience of delivering large number of fractions, often more than 40. An unusual prostate tumor radiobiology, however, an uncharacteristically high sensitivity to

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large fractions of radiation, may allow a radically different, radiobiologically-based approach to dose escalation.

The majority of results from clinical trials involving altered fraction size argue for a low  $\alpha/\beta$  ratio (a high fraction size sensitivity) for prostate cancer on the order of 1-3 Gy, a value lower than or similar to values typically ascribed to the adjacent organs at risk such as bladder and rectum. Such a relationship implies that the therapeutic ratio could be improved by treating prostate cancers with fewer but larger fractions of radiation, a hypofractionation approach.

This survey will discuss the rationale for prostate hypofractionation, review ongoing and completed clinical trials and describe promising future directions.

#### The Case for Hypofractionation

What is the fractionation response of prostate cancer?—Conventional fractionation schemes employing fraction sizes of 1.8-2.0 Gy are based upon the premise that tumors typically are less responsive to fraction size than are late-responding normal tissues. The  $\alpha/\beta$  ratio is a measure of fractionation response, with low ratios (high  $\alpha/\beta$ 's) associated with late responding normal tissues. A low  $\alpha/\beta$  is consistent with a greater capacity for repair between fractions, with an accompanying greater relative sparing with small fraction sizes, than for tumors with their typically higher  $\alpha/\beta$  ratios. Under these conditions, an improved therapeutic ratio is achieved with multiple small fractions for most types of tumors. The  $\alpha/\beta$  ratios thought to be associated with tumors, however, are typically 8 or greater, whereas for late responding normal tissues, values on the order of 3 or 4 or somewhat less for CNS are suggested from the analyses of numerous experimental and some clinical outcome studies.

**Tumors** other than prostate cancer have shown stronger than expected fraction size dependencies (low  $\alpha/\beta$  ratios) as well, including melanomas<sup>1</sup> and some sarcomas2.. Slow proliferation may be a hallmark of such a response and, in the case of prostate cancer, there is ample evidence for slow proliferation, based both upon direct measurement of potential doubling times and labeling indices3 and upon analysis of the kinetics of rising PSA during tumor recurrence.4 What is uncertain is whether all prostate cancers, particularly those with high grade and having possibly higher growth rates, share this characteristic.

A number of earlier analyses and reviews of clinical outcomes after brachytherapy argue for a low  $\alpha/\beta$  ratio for prostate cancer.<sup>5, 6</sup> Brenner and Hall<sup>5</sup>, for example, analyzed dose response data for external beam radiation compared with I-125 brachytherapy data and estimated a very low  $\alpha/\beta$  ratio of 1.5 Gy for prostate cancer. Duschene and Peters<sup>6</sup> concluded in analogous fashion that the  $\alpha/\beta$  ratio for prostate cancer may be low and more similar to that expected for late responding normal tissue than for the typical, more rapidly proliferating tumor. These studies involved very simple calculational approaches comparing 145 Gy given at low dose rate to 70–74 Gy at fractionated high dose rates for patients with similar initial PSA levels and Gleason scores.

Fowler, Chappell and Ritter<sup>7</sup> also conducted a comprehensive analysis of clinical outcome in patients treated with external beam radiotherapy versus I-125 or Pd-103 implants in order to further test the above analyses. An  $\alpha/\beta$  ratio for prostate cancer well below 2 Gy was also estimated.

These perminent brachytherapy implant versus external beam comparisons are potentially weakened by questions about brachytherapy dose heterogeneity, effective RBE and repair rates during protracted exposure, but there is more rigorous evidence for a low  $\alpha/\beta$  in studies

such as that of Martinez at al<sup>8</sup> in which patients were treated with a standard external beam course of treatment followed by high dose rate temporary implant boost doses which were escalated by decreasing fraction number from 3 to 2 and by increasing fraction size from 5.5 to 10.5 Gy. Patients were grouped according to prognostic factors and biochemical control was modeled versus equivalent dose, as calculated via a linear quadratic model. An estimated  $\alpha/\beta$  ratio of 1.2 (95% CI: 0.03, 4.1 Gy) was derived, again very lowand potentially more reliable given that all patients were treated by the same modalities.

Another study utilizing both external beam and brachytherapy data is that of Williams et al<sup>9</sup>, who used a proportional hazards model to estimate the  $\alpha/\beta$  ratio from data on 3756 external beam and 185 high dose rate brachytherapy boost patients. An estimated ratio of 2.6 Gy was determined, but with a wide 95% confidence interval of 0.9 to 4.8 Gy. The limited range of external beam fraction sizes as well as patient and prescription dose heterogeneity restricted the precision with which the  $\alpha/\beta$  ratio could be estimated. Other efforts to estimate the  $\alpha/\beta$  ratio from published clinical outcomes of purely external beam studies will be described in detail later.

Challenges have been raised, however, regarding the low estimates of the  $\alpha/\beta$  ratio for prostate cancer. Some relate to the potential uncertainties surrounding permanent implant dosimetry <sup>10</sup>, as previously mentioned, others focus on the potential confounding role of tumor cell repopulation, <sup>11</sup> and still others suggest a confounding role of tumor hypoxia upon the estimation of  $\alpha/\beta$  <sup>12</sup>. There are arguments that at least partially counter these concerns, however, and, with all information considered, a low  $\alpha/\beta$  ratio for prostate cancer remains an attractive hypothesis supported by several lines of evidence. While clinical data supporting a low  $\alpha/\beta$  ratio is becoming more plentiful, derived estimates are still characterized by wide confidence intervals. These uncertainties will ultimately not be resolved until biochemical control data from large, preferably randomized hypofractionation studies with 5 or more years of follow-up become available.

#### Hyupofractionation has the potential for improving therapeutic ratio

If, contrary to most other tumors, prostate cancer has a lower  $\alpha/\beta$  ratio than late-responding normal tissue, the potential exists for hypofractionation to significantly improve the therapeutic ratio. The relationship between fraction size and therapeutic ratio can best be illustrated, at least over a range of fraction sizes between 1 and around 6 Gy, through use of linear quadratic modeling, which allows calculation of an equivalent dose delivered in 2 Gy fractions (EQD<sub>2</sub>) for any total dose, D, dose per fraction, d, and alpha-beta ratio,  $\alpha/\beta$ :

**EQD**<sub>2</sub>=D ×  $[(d+\alpha/\beta)/2 \quad Gy+\alpha/\beta)]$ 

An  $\alpha/\beta$  ratio for tumor less than that for at-risk normal tissues predicts an improved therapeutic ratio with hypofractionation. For example, the ratio of the EQD<sub>2</sub> doses for tumor (with an assumed  $\alpha/\beta$  of 1.5) to late normal tissue (an assumed  $\alpha/\beta = 3$ ) can be plotted as a function of increasing fraction size, while limiting total dose to maintain acceptable side effect risks. This therapeutic ratio is plotted as a function of fraction size in figure 1.

There are several uncertainties that potentially limit the reliability of such models, however. The first, as previously discussed, is uncertainty over the tumor  $\alpha/\beta$ . If prostate cancer and late normal tissue damage  $\alpha/\beta$  ratios that were equal, for example, there would be no hypofractionation-related gain in therapeutic gain, although improvements in convenience and cost efficiency could still ensue.

Secondly, while the applicability of the linear quadratic model to fraction sizes ranging up to 5-6 Gy seems fairly secure, that is not the case for still larger dose fractions, a key factor when considering ultra hypofractionated, stereotactic body radiation therapy approaches. There is some support for applicability to very large fraction sizes, even 20-30 Gy<sup>13, 14</sup>, particularly with modifications as needed to account for processes such as reoxygenation and redistribution<sup>15</sup>. Other analyses, however, suggest thatapplication of the model to larger fraction sizes could under predict the total dose required to produce a given effect.<sup>16</sup>, resulting in a less toxic but also less effective treatment. Other uncertainties cited above such as reoxygenation and redistribution are also particularly relevant as the total number of fractions in a treatment course diminishes.

In spite of a significant number of remaining uncertainties, however, there remains sufficient supporting evidence to justify continuing to test the hypothesis that larger radiation fraction sizes will will be effective and safe. Although many were planned before prostate cancer's unusual large-fraction radiobiology was suspected, a number of prostate hypofractionation trials have been carried out and information regarding the efficacy and safety of such an approach is emerging. These trials will be detailed later.

#### **Clinical approaches using hypofractionation**

Two types of hypofractionation designs can be considered, using the linear quadratic model as a basis, that would exploit the hypothesized radiobiological advantages and increase the therapeutic ratio. Hypofractionation could be designed with the intent of either reducing the normal tissue toxicity while maintaining the same tumor control, or of increasing tumor control while maintaining constant toxicity risk.

Figure 1, presented earlier, is an example of the latter approach in which increasingly more effective tumor doses can be delivered while a constant level of side effect risk is maintained. Most hypofractionation studies to date have employed this type of design.

#### Hypofractionation for Prostate Cancer – Clinical Experience

There are a number of older, published experiences with hypofractionated, external beam radiotherapy for prostate cancer, particularly in the UK.<sup>17-19</sup> These treatments were generally well tolerated, but overall efficacy is difficult to assess, given the largely pre-PSA era these trials were conducted in. A number of more contemporary hypofractionation trials have either now been published or are currently underway. These are listed in Table I. In order to permit at least approximate comparisons of such diverse treatment schedules, EQD<sub>2</sub> doses were calculated and are shown in Table 1 for assumed  $\alpha/\beta$  ratios of 1.5 and 3 for prostate cancer and late responding normal tissue, respectively. It is apparent that although most of these trials have only modestly hypofractionated schedules, the EQD<sub>2</sub> doses range between about 4 and 8 % higher for tumor than for normal tissue, illustrating the potential for therapeutic gain even with relatively modest hypofractionation if prostate cancers indeed have a lower  $\alpha/\beta$  ratio than that for normal tissue.

The Princess Margaret<sup>20</sup>, Cleveland Clinic<sup>21</sup>, Manchester<sup>22</sup>, NCI-Canada<sup>23</sup> and Chiba carbon ion<sup>24</sup> trials are the only contemporary trial with published results that have sufficient numbers of patients and sufficient although still relatively short follow-up to enable preliminary estimates of biochemical control and toxicity. Of these, only the Princess Margaret, Cleveland Clinic and Chiba carbon ion trials delivered what would now be considered adequate EQD<sub>2</sub> doses and had sufficient patient numbers and follow-up to adequately estimate late toxicity.

Reported toxicity in these three, higher effective dose trials was low, with the actuarial RTOG Grade  $\geq 2$  late rectal and genitourinary toxicity rates all generally 6% or less (Table

1). Efficacy has been consistent with expectations for conventionally dose escalated radiation therapy. For intermediate risk patients, the Cleveland clinic trial yielded a 5 year biochemical control rate of 85%, similar to that attained with that institution's prior standard of 78 Gy in 2 Gy fractions.<sup>21</sup> The Chiba carbon ion trial<sup>24</sup> found a biochemical control rate of 97% at 5 years in intermediate risk patients and the Princess Margaret study<sup>20</sup>, reported a 36 month biochemical control rate of 85%, again in intermediate risk patients.

The Manchester study<sup>22</sup>, delivered an equivalent an EQD<sub>2</sub> of 66 Gy that, by today's standards, would be considered low and, accordingly, produced low late toxicities and relatively poor biochemical control rates. Similarly, the NCI-Canada and Edinburgh trials, each with an EQD<sub>2</sub> of only about 62 Gy, yielded biochemical control rates and toxicities that were were correspondingly low as well. However, results from these trials as well as the higher dose Princess Margaret, Chiba and Cleveland Clinic studies, provide a range of fraction size data, allowing valuable testing of  $\alpha/\beta$  ratio assumptions and of linear quadratic modeling.

Figure 2 is a graphical representation of biochemical control rates versus equivalent dose from these six studies (for intermediate risk prostate cancer, when specifically reported). Represented are 3-5 year actuarial bDFS rates using the ASTRO definition, the only definition uniformly available in these reports. The solid, dose response curve for radiation delivered in 2 Gy fractions is adapted from Fowler *et al*<sup>25</sup> and is based upon 5 year biochemical control data for intermediate risk patients from 5 conventionally fractionated prostate cancer trials. Biochemical control points from each hypofractionation trials are plotted relative to their equivalent dose (EOD<sub>2</sub>) for an assumed  $\alpha/\beta$  ratio of 1.5. If higher  $\alpha/\beta$ ratios had been assumed, all points would be plotted significantly further to the left of their indicated loations. The ratio of 1.5 produces plotted points that fit the standard fractionation curve reasonably well. However, there are many unaccounted for variables that prevent this from becoming a rigorous comparison, including potentially non-equivalent prognostic characteristics, treatment technique differences and variable use of androgen deprivation. Still, the degree of outcomes agreement between hypofractionated and conventional regimens when an  $\alpha/\beta$  of 1.5 is assumed does suggest that prostate cancer response can in fact be characterized by a low  $\alpha/\beta$  ratio.

More formalized estimates of the  $\alpha/\beta$  ratio from clinical data do, in fact, reveal the inherent uncertainties involved. Analysis by Bentzen and Ritter<sup>26</sup> of one of these trials, the NCI-Canada study<sup>23</sup>, estimated a quite low  $\alpha/\beta$  ratio of 1.2 Gy, but with a wide 95% confidence interval of from -3.3 to 5.6 Gy. Another study by Williams *et al*, <sup>9</sup> a retrospective analysis of 3756 patients treated with a modest range of external beam fraction sizes or with high dose rate brachytherapy, used a proportional hazards model stratified by risk severity to estimate an  $\alpha/\beta$  ratio of 2.6 Gy, but with a 95% confidence interval of from 0.9 to 4.8 Gy. A review by Dasu<sup>27</sup> extensively reviews  $\alpha/\beta$  analyses from a number of such clinical trials. It demonstrates significant variability and large confidence intervals, but again, does suggest that the ratio is low, on the order of 2 Gy or less. Thus, many studies have suggested a low  $\alpha/\beta$  ratio, but the relatively narrow range of fraction sizes employed in these external beam studies has significantly limited the accuracy with which it can be measured. Low dose rate or high dose rate brachytherapy studies have employed much larger fraction sizes but, from a modeling standpoint, are plagued by a concerns over dose inhomogeneity and, in the case of low dose brachytherapy, relative biological effectiveness.

One study that, when mature, may provide a more useful range of fraction sizes is the final non-randomized study listed in Table 1, which is a multi-institutional trial (University of Wisconsin, M.D. Anderson-Orlando, Wayne State University, Medical college of Wisconsin and JT Vucurevich Cancer Inst., Rapid City). This is a phase I/II study<sup>28</sup> that escalates dose-

per-fraction in three steps, with late rectal bleeding the escalation-limiting factor. The design results in predicted late effects expected to remain relatively constant (at a level consistent with about 76 Gy delivered in 2 Gy fractions) even as fraction size escalates. The trial design also includes a nested fractions-per-week escalation/de-escalation to monitor for and prevent unacceptable acute toxicities that might result from too extreme a shortening of treatment duration and that might lead to consequential late toxicities.<sup>25</sup>

Preliminary results from this phase I/II trial<sup>28</sup> have indicated acceptably low rates of GI and GU toxicity (2 years grade 2 GI and GU toxicity rates of 8.8 and 3%, respectively, and preliminary biochemical control rates that are high and in the expected range. The trial is nearing completion with 280 of a target 300 patients accrued. Centrally analyzed dose-volume data and the trial's wide range of doses-per-fraction may permit solid estimates of  $\alpha/\beta$  ratios both for prostate cancer as well as for adjacent organs at risk.

Thus, outcomes from a variety of hypofractionation trials provide support for a low  $\alpha/\beta$  ratio for prostate cancer and justify further investigation of large fraction sizes, preferably via randomized clinical trials. Several such randomized trial that deliver acceptably high EQD<sub>2</sub> doses have either recently completed accrual and are awaiting reporting or are currently underway (Table I), and should provide a rigorous evaluation of this treatment approach. Collection within such trials of detailed dose-volume information should be encouraged as well to permit as well an accurate analysis of the fractionation response of regional organs at risk.

#### **Extreme Hypofractionation**

Shorter hypofractionation schedules, consisting of only 4-5 fractions, are now also beginning to be explored, although not always exclusively within the context of clinical trials. Five total fractions have typically been used with fraction sizes of greater than 6-7.5 Gy are typically given, although significantly higher doses per fractions have been used in some cases. A number of uncertainties, however, make it essential that such efforts be carried in a clinical trial setting so that monitoring and reporting guidelines are established and met. Efforts to so shorten the treatment depend to some extent upon extrapolation from results obtained using more modest hypofractionation which, themselves, are not yet fully mature. In addition, significant uncertainties remain over the validity of the linear quadratic model, modified or otherwise, for predicting the biological effectiveness of these higher doses per fraction. For example, the relative contribution of differing radiation damage mechanisms likely changes with increasing fraction size<sup>29</sup>, rendering predictions from standard models unreliable.

Furthermore, in theory, the potential tumor control enhancing contributions of reoxygenation and redistribution could diminish as the number of fractions decreases and treatment duration shortens. In addition, treatment delivery accuracy-associated quality control issues such as immobilization, target motion and image guidance must be given increasing attention as the number of delivered treatments decreases,. These requirements can best be addressed in the context of prospective trials that ensure patient safety and proper documentation ofoutcomes..

Several prospective trials of extreme hypofractionation are currently underway. Five are listed in Table 2, with only the Madsen *et al* trial <sup>30</sup> having sufficient follow-up (median 48 months) to allow meaningful evaluation of biochemical control. Reported outcomes from this trial were acceptable, with actuarial late GU and GI grade 2 toxicities at 48 months of 16.1 and 9.4% respectively, and an actuarial freedom from biochemical relapse at 48 months of 90% (nadir plus 2). The Tang *et al* phase I/II trial<sup>31</sup> has only reported on 30 patients and only on acute toxicities, which were acceptably low. The Timmerman *et al* study listed in

Table 2, is an ongoing phase I/II study notable for the higher dose fractions it employs, specifically 5 fractions of either 9.5, 10 or 10.5 Gy each. Another study recently opened, this one industry sponsored (ClinicalTrials.gov Identifier: <u>NCT00643617</u>), delivers 38 Gy in 4 fractions of 9.5 Gy each using Cyberknife delivery. Were standard linear quadratic modeling to remain valid at these much larger fraction sizes, these regimens could produce extraordinarily high tumor and normal tissue EQD<sub>2</sub> doses. There is evidence, however, that the linear quadratic model significantly overestimates biological effect at very large fraction sizes<sup>16</sup>. Furthermore, normal tissue volume restrictions during treatment planning could also reduce the potential for toxicity from these high dose fractions, although, unlike some tumors such as the mid-lung, for example, the prostate has an unavoidable organ at risk, the urethra, tolerance for which must be considered.

#### Conclusions

A number of hypofractionation trials have suggested a low  $\alpha/\beta$  ratio for prostate cancer that increases the therapeutic ratio when radiation fraction size is increased beyond the typical 1.8 to 2 Gy. However, precise determination of the  $\alpha/\beta$  ratio both for prostate cancer and for late responding normal tissue remains difficult, while uncertainties also exist in models that seek to extrapolate biological effects seen at lower fraction sizes to the larger doses per fraction that are seeing an increasing investigational focus. Given that standard fraction size radiation therapy is already highly effective when given to sufficiently high doses, it is imperative that ongoing and future studies of hypofractionation be carried out in prospective and, ideally randomized fashion. Several such randomized trials are underway or ahave completed accrual and are awaiting sufficient follow-up for analysis. Studies such as these will have the power to ultimately validate the utility of prostate hypofractionation, making available its potential for significant therapeutic gain, cost savings and improved patient convenience. The future management of localized prostate cancer could be profoundly altered as a result.

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#### Figure 1. Increasing therapeutic advantage with increasing hypofractionation

The equivalent total doses if delivered in 2 Gy fractions for prostate tumor ( $\alpha/\beta = 1.5$ ) and normal tissue late effects ( $\alpha/\beta = 3$ ) are shown versus fraction size-number combinations that preserve similar late effect levels, as would be predicted by the linear quadratic model. A reduction in total dose is required with increasing hypofractionation to maintain similar predicted late effects. The difference between the solid lines and dotted extensions on the right indicate in non-quantitative fashion a potential, over-prediction of biological effect by the linear quadratic model for very large fraction sizes.



#### Figure 2.

Biochemical disease-free survival (bDFS) rates versus equivalent doses from six hypofractionation studies identified in Table 1 (for intermediate risk prostate cancer, when separately reported in the publications). Shown are 3-5 year actuarial bDFS rates using the ASTRO definition, which was the only method consistently available for all reports. The solid line dose response curve for radiation delivered in 2 Gy fractions is adapted from Fowler *et al*<sup>18</sup> and is based upon 3-5 year biochemical control data for intermediate risk patients from 5 conventionally fractionated prostate cancer trials. Biochemical control points from the hypofractionation trials are plotted relative to their equivalent dose for an assumed prostate cancer  $\alpha/\beta$  ratio of 1.5.

Legend: NCIC<sup>32</sup>: Hypofx  $\Box$ , Standard **•**; Edinburgh<sup>33</sup>: **•**; Adelaid<sup>34</sup>: Hypofrx  $\Delta$ , Standard **>**; Manchester<sup>22</sup>: **>**; Princess Margaret<sup>20</sup>:  $\circ$ ; Cleveland Clinic<sup>21</sup>: •; Chiba<sup>24</sup>:  $\Delta$ .

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# Table 1

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			Equivale Gy fracti	nt Dose in 2 ions (EQD <sub>2</sub> )		Intermed. risk	≥ Grade Toxici	: 2 Late y (%)
REFERENCE	No. PTS	Dose/fx size/# fxs	$\alpha/\beta = 1.5$ (tumor)	$\alpha/\beta = 3$ (late effects)	Med .F/U (mo.)	% bPFS	19	GU
Livsey <i>et al</i> 22 Manchester	705	50 Gy/3.13 Gy/16 fx	66 Gy	61.3 Gy	60	56 (5 yr)	5	6
Akimoto <i>et al</i> <sup>3</sup> 5 Gumma	52	69 Gy/3 Gy/23 fx	88.7 Gy	82.8 Gy	33	ł	25	1
Tsuji <i>et al</i> 24 Chiba	201	66 GyE/2/3 GyE/20 fx (carbon ions)	90.5 Gy	83.1 Gy	30	97	5	9
Higgins <i>et al</i> <sup>33</sup> Edinburgh	300	52.5Gy/2.625Gy/20 fx	61.9 Gy	59.1 Gy	12	55	1	-
Soete <i>et al</i> <sup>36</sup> Jette, Belgium	36	56 Gy/3.5 Gy/16	80 Gy	72.8 Gy		-	-	ł
Martin <i>et al</i> 20 Princess Margaret	92	60 Gy/3 Gy/20 fx	77.2 Gy	72 Gy	36	85	4	3
Kupelian <i>et al</i> 21, 37 Cleveland Clinic	770	70 Gy/2.5 Gy/28 fx	80 Gy	77 Gy	45	85	4.5	5.3
Ritter <i>et al</i> 28 Wisconsin	100 100 80 (active)	64.7 Gy/2.94Gy/22 fx 58.1 Gy/3.63Gy/16 fx 51.6 Gy/4.3Gy/12 fx	82.6 Gy 85.1 Gy 85.5 Gy	77 Gy 77 Gy 75 Gy	38 24 14	95	8.5	1
Lukka <i>et al</i> 23 NCIC	466 470	52.5/2.625 Gy/20 fx 66 Gy/2 Gy/33 fx	61.9 Gy 66 Gy	59.1 Gy 66 Gy	89	40	1.3	1.9
Y eoh <i>et al</i> <sup>38</sup> Adelaid	108 109	55 Gy/2.75 Gy/20 fx 64 Gy/2 Gy/32 fx	66.8 Gy 64 Gy	63.2 Gy 64 Gy	48	57.4 55.5	Alternate scoring	Alternate scoring
Pollack <i>et al</i> <sup>39</sup> Fox Chase	150 150	70.2 Gy/2.7Gy/26 fx 76 Gy/2 Gy/38 fx	84.2 Gy 76 Gy	80 Gy 76 Gy		1	-	
RTOG www.rtog.org/members/protocols/0415/0415.pdf	Ongoing (to 1067 pts)	70 Gy/2.5 Gy/28 fx 73.8 Gy/1.8 Gy/41 fx	80 Gy 69.6 Gy	77 Gy 70.8 Gy				
Khoo <i>et al</i> <sup>40</sup> MRC	Ongoing (to 2100 pts)	57 Gy/3 Gy/19 fx 60 Gy/3 Gy/20 fx	73.3 Gy 77.2 Gy	68.4 Gy 72 Gy				

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Grade 2 Late Ioxicity (%)	31 GU		15 29		13 13	
AL.	Med. F/U (mo.) (	41	33		12	
Total Equivalent Dose in 2 Gy fractions (EQD <sub>2</sub> )	$\alpha/\beta = 3$ (late effects)	64.9 Gy	74.3 Gy	77.7 Gy	70 Gy	118 Gy 130 Gy 142 Gy
	$\alpha/\beta = 1.5$ (tumor)	78 Gy	90.6 Gy	92.7 Gy	85.1 Gy	149 Gy 164 Gy
	Dose/fx size/# fxs	33.5 Gy/6.7 Gy/5 fx	36.25 Gy/7.25 Gy/5 fx	42.7 Gy/6.1 Gy/7 fx	35 Gy/7 Gy/5 fx	47.5 Gy/9.5 Gy/5 fx 50 Gy/10 Gy/5 fx
	No. PTS	40	41	105	30	15 10 (ongoing)
	REFERENCE	Madsen <i>et al</i> <sup>3</sup> 0 Virginia Mason	King <i>et al</i> <sup>4</sup> 1 Stanford	Widmark (personal communication, 2008) Umea	Tang <i>et al</i> 31 Univ. Toronto	Timmerman (personal communication, 2008)

\* NTD calculations are based upon standard linear quadratic modeling, which may over predict NTD doses for large fraction sizes such as used in the UTSW trial.