



Published in final edited form as:

Heart Rhythm. 2011 April ; 8(4): 599–605. doi:10.1016/j.hrthm.2010.11.038.

Bidirectional Ventricular Tachycardia: Ping Pong in the His-Purkinje System

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Abstract

Background—Bidirectional ventricular tachycardia (BVT), characterized by an alternating beat-to-beat electrocardiographic QRS axis, is a rare but intriguing arrhythmia associated with digitalis toxicity, familial catecholaminergic polymorphic ventricular tachycardia (CPVT), and several other conditions which predispose cardiac myocytes to delayed afterdepolarizations (DADs) and triggered activity. Evidence from human and animal studies attributes BVT to alternating ectopic foci originating from the distal His-Purkinje system in the left and/or right ventricles, respectively.

Objective—To evaluate a simple “ping pong” model of reciprocating bigeminy to explain BVT.

Methods—We constructed a 2D anatomic model of the rabbit ventricles with a simplified His-Purkinje system, in which different sites in the His-Purkinje system had different heart rate thresholds for DAD-induced bigeminy.

Results—When the heart rate exceeded the threshold for bigeminy at the first site in the His-Purkinje system, ventricular bigeminy developed, causing the heart rate to accelerate and exceed the threshold for bigeminy at the second site. Thus, the triggered beat from the first site induced a triggered beat from the second site. The triggered beat from the second site next reciprocated by inducing a triggered beat from the first site, and so forth. Bigeminy from two sites produced BVT, and from 3 or more sites, polymorphic VT.

Conclusions—This ping pong mechanism of reciprocating bigeminy readily produces the characteristic electrocardiographic pattern of BVT, and its degeneration to polymorphic VT if additional sites develop bigeminy.

Keywords

action potentials; arrhythmia (mechanisms); catecholaminergic polymorphic ventricular tachycardia; electrophysiology; ventricular tachycardia

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Disclosures. No conflicts of interest.

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Introduction

Bidirectional ventricular tachycardia (BVT) is characterized by beat-to-beat alternation of the QRS axis on the electrocardiogram (ECG). Although uncommon, it has fascinated clinicians since its original description in 1922 as a manifestation of digitalis toxicity^{1–4}. It has also been reported in the setting of hypokalemic periodic paralysis⁵, Andersen-Tawil syndrome⁶, and fulminant myocarditis⁷. More recently, BVT has also been recognized as a hallmark of catecholaminergic polymorphic ventricular tachycardia (CPVT) syndrome, a familial disorder with a high risk of sudden cardiac death during sympathetic stimulation⁸. During exercise testing, these patients typically develop premature ventricular complexes (PVCs) and sometimes ventricular bigeminy^{9–11} in association with BVT, which can self-terminate or degenerate into polymorphic VT and ventricular fibrillation (VF)^{8, 11, 12}. Although the most characteristic electrocardiographic pattern of BVT is right bundle branch (RBB) block with an alternating QRS axis⁸, other patterns, such as alternating RBB and left bundle branch (LBB) block or alternating QRS axis with a narrow QRS¹³ have also been observed. Recent genetic studies have attributed familial CPVT syndromes to defects in the cardiac ryanodine receptor (RyR2) or calsequestrin, an associated regulatory protein, in the sarcoplasmic reticulum (SR), and CPVT has been recapitulated in genetically-engineered mouse models incorporating the analogous RyR2 mutations^{14, 15}. In these mice, abnormal RyR2 regulation predisposes myocytes to delayed afterdepolarizations (DADs) and triggered activity, analogous to digitalis toxicity. A recent optical mapping study in a mouse CPVT model due to the mutation R4496C in RyR2 (RyR2- R4496C) showed that BVT was caused by two foci in the distal His-Purkinje system (HPS), one in the right ventricle (RV) and the other in the left ventricle (LV), alternately activating the ventricles¹⁶. Moreover, ablation of the RV HPS with Lugol's solution converted BVT to monomorphic VT. These authors went on to show in a computer model of the anatomic mouse ventricles that alternate pacing from the RV and LV septum produced a characteristic electrocardiographic pattern of BVT. However, they did not address the mechanism by which triggered activity spontaneously generated this pattern.

Based on the observation that PVCs and ventricular bigeminy are common precursors to BVT^{9–11}, it occurred to us that a simple “ping pong” mechanism, which we call reciprocating bigeminy, could readily account for the pattern of alternating foci observed during BVT. Although a number of mechanisms for BVT have been suggested^{10, 11, 17–19}, the straightforward, conceptually intuitive mechanism of reciprocating bigeminy has not, to our knowledge, been explicitly proposed previously, yet is fully consistent with well-known properties of triggered activity caused by DADs. We demonstrate its plausibility by incorporating these experimentally well-documented properties into computer simulations to reproduce the characteristics of BVT.

Methods

Ventricular and Purkinje AP cell models

For ventricular cells, we used the Mahajan *et al.* model²⁰, a detailed model of rabbit ventricular AP which includes intracellular Ca (Ca_i) dynamics (Fig. 1A, red trace). To model the Purkinje cell AP (Fig. 1A, black trace), we modified $I_{to,f}$, $I_{to,s}$, I_{kr} , I_{ks} , and I_{kl} as described by Cordeiro *et al.*²¹. We also added a background Ca current (adopted from the LRD model²²), using the following formulation:

$$I_{Ca,b} = \bar{G}_{Ca,b} (V - E_{Ca,b}) \quad (1)$$

$$E_{Ca,b} = \frac{RT}{2F} \ln \frac{c_o}{c_s} \quad (2)$$

where $\bar{G}_{Ca,b}$ is the maximal current conductance, c_s is submembrane Ca concentration in mM, c_o is extracellular Ca concentration in mM, F is Faraday's constant, R is the universal gas constant, and T is temperature in K. $\bar{G}_{Ca,b}$ was adjusted to produce physiological values of diastolic and systolic Ca in the Purkinje cells and ventricular myocytes (Fig. 1A and Table 1).

To produce DADs and triggered activity in Purkinje cells, we used the formulation of spontaneous SR Ca release described by Hufferaker *et al.*²³, with some modifications. Spontaneous release was triggered solely by the SR Ca load (and not cytosolic Ca concentration), as follows:

$$J_{spon} = \bar{G}_{spon} \cdot p \cdot (c_j - c_s) \quad (3)$$

where J_{spon} is the spontaneous Ca release flux, c_j is the SR Ca concentration, \bar{G}_{spon} is the conductance of the release and p is the gating variable obeying the following equation:

$$\frac{dp}{dt} = \frac{(p_\infty - p)}{\tau_p} \quad (4)$$

$$p_\infty = \begin{cases} 0 & \text{if } c_j < K_1 \\ \frac{c_j - K_1}{K_2 - K_1} & \text{if } K_1 < c_j < K_2 \\ 1 & \text{if } c_j > K_2 \end{cases} \quad (5)$$

where τ_p 10 ms is the time constant for spontaneous SR release, and K_2 , K_1 are the upper and lower thresholds for spontaneous SR Ca release, respectively (Table 2). With these additions, the differential equations for c_j and c_s become:

$$\frac{dc_j}{dt} = -J_{rel} - J_{spon} + J_{up} + J_{leak} \quad (6)$$

$$\frac{dc_s}{dt} = \beta_s \left[\frac{v_i}{v_s} (J_{rel} - J_d + J_{Ca} + J_{NaCa} + J_{Ca,b} + J_{spon}) - J_{trpn}^s \right] \quad (7)$$

where J_{rel} is Ca-induced Ca release from the SR, J_{spon} is the spontaneous release from SR due to Ca overload, J_{up} is Ca uptake by SERCA, and J_{leak} is the Ca leak from the SR into the cytoplasm. J_d represents diffusion of Ca from the submembrane compartment (c_s) into the cytoplasmic compartment (c_i), J_{Ca} is Ca flux into the c_s from the L-type Ca channel, and J_{NaCa} is the flux through the NaCa exchanger. β_s represents the time independent submembrane Ca buffering and J_{trpn}^s is the time dependent binding of Ca to troponin C. Finally, v_i/v_s represents the cytoplasmic-to-SR volume ratio.

We also modified the equation for c_p , the effective Ca concentration sensed by the L-type Ca channel accounting for L-type Ca current inactivation due to spontaneous SR Ca release as follows:

$$\frac{dc_p}{dt} = \tilde{J}_{spon} + \tilde{J}_{SR} + \tilde{J}_{Ca} - \frac{c_p - c_s}{\tau_s} \quad (8)$$

$$\tilde{J}_{spon} = \gamma \cdot J_{spon} \quad (9)$$

where \tilde{J}_{SR} and \tilde{J}_{Ca} are the effective fluxes from SR and Ca channel respectively and \tilde{J}_{spon} is the effective flux from spontaneous SR calcium release and $\gamma = 200$ is the conversion factor.

With these modifications, the Purkinje AP model developed DADs of sufficient amplitude to cause a single triggered AP at a critical heart rate. Parameters were adjusted such that the critical heart rate at which DADs occurred could be varied (Fig. 1B, green versus purple traces).

Tissue model—We used rabbit ventricular anatomy and fiber-orientation data obtained from the Cardiac Mechanics Research Group at the University of California (San Diego, CA), as described previously^{24, 25}, to extract a 2D sagittal section of the ventricles, as shown in Fig. 2A. We added a His-Purkinje network (with a thickness of 5 Purkinje cells), consisting of a His bundle dividing into a RBB and LBB, each forming further branches until inserting into the ventricular myocardium to generate a physiological activation sequence.

Wave propagation in 2D tissue was modeled using a reaction-diffusion partial differential equation:

$$\frac{\partial V_m}{\partial t} = -\frac{I_{ion}}{C_m} + \tilde{I}_{nbr} \quad (10)$$

where V_m is the membrane voltage, I_{ion} is the sum of the membrane currents and C_m is the membrane capacitance. \tilde{I}_{nbr} is the diffusive flow from the neighbor cells as described below, which is solved by a partial differential equation. The partial differential equation was solved using operator splitting and an adaptive time step method^{26, 27}. We used a variable time step between 0.001 and 0.01 ms. All simulations were performed on a 128-node Beowulf cluster.

The diffusive flow between neighboring cells was defined as:

$$\tilde{I}_{nbr} = D \left(\frac{V_{i+1,j} + V_{i-1,j} - 2V_{i,j}}{dx^2} \right) + D \left(\frac{V_{i,j+1} + V_{i,j-1} - 2V_{i,j}}{dy^2} \right) \quad (11)$$

where $D = 0.001$ cm²/ms if the neighboring cell was a ventricular myocyte and $D = 0.006$ cm²/ms if the neighboring cell was a Purkinje cell, and $dx=dy=0.015$ cm. Each cell could have up to 4 neighbors. Purkinje cells were coupled to ventricular myocytes at a total of 27 sites in the terminal His-Purkinje branches (where the 5 terminal Purkinje cells were coupled to 5 adjacent ventricular cells) and at a few points within the septum (where 2 Purkinje cells

were coupled to 2 adjacent ventricular cells). The diffusion at Purkinje-myocyte interfaces was defined as:

$$\tilde{I}_{nbr} = D_p \left(\frac{V_{i+1,j} - V_{i,j}}{dx^2} \right) + D_v \left(\frac{V_{i-1,j} - V_{i,j}}{dx^2} \right) \quad (12)$$

where $D_p = 0.006$ and $D_v = 0.001$ cm²/ms.

When the His bundle was paced (simulating a sinus beat), the resulting activation sequence is shown in Fig. 2B. Activation was earliest at the left septum, followed by right septum, ventricular apex and lateral ventricular walls, generally consistent with the ventricular activation sequence during sinus rhythm^{28,29}. Within the HPS, regions of the RBB and LBB (labeled *a* and *b*, respectively) were assigned the DAD-generating Purkinje cell AP models (corresponding to the two traces in Fig. 1B), with the remainder of the HPS comprised of the standard Purkinje cell AP model without DADs (Fig. 1A). In some simulations, a 3rd area (labeled *c*) was also assigned DAD-generating Purkinje cell AP models.

Pseudo-ECG calculation

A pseudo-ECG (Φ_e) was computed from membrane voltage using the following integral expression³⁰:

$$\varphi_e(x', y', z') = D \int \left[-\nabla V_m \cdot \left(\nabla \frac{1}{r} \right) \right] dx + D \int \left[-\nabla V_m \cdot \left(\nabla \frac{1}{r} \right) \right] dy \quad (13)$$

$$r = [(x - x')^2 + (y - y')^2 + (z - z')^2] \quad (14)$$

where ∇V_m is the spatial gradient of V_m and r is the distance from a source point (x, y, z) to the location of the “electrode” at (x', y', z') .

Results

The proposed “ping pong” mechanism of BVT is based on the following two commonly observed behaviors of DAD-mediated triggered activity: i) above a certain threshold heart rate, a DAD triggers a single AP after each paced AP, initiating ventricular bigeminy (Fig. 1B); ii) the threshold heart rate for bigeminy varies at different locations in the heart (Fig. 1Ba and 1Bb, respectively). From the experimental evidence indicating that BVT arises from the bundle branches of the HPS¹⁶, we assume that the sites from which bigeminy arises are located in the HPS, where source-sink relationships are more favorable for DAD formation than in ventricular muscle^{31,32}. The different heart rate thresholds for bigeminy are a natural assumption, since if the rate thresholds were the same everywhere, all rate-dependent DAD-mediated PVCs arising from the HPS would have a narrow QRS complex, which is not true. We arbitrarily chose the RBB to have the lower heart rate threshold for bigeminy, set at 67 bpm, and the LBB to have the higher threshold, set at 100 bpm (Fig. 3, and movie in online supplement). Thus, when the heart rate exceeded 67 bpm, the paced AP with a normal activation sequence (top row) was followed by a triggered AP from the RBB, producing a QRS morphology resembling LBB block (middle row). With the onset of ventricular bigeminy, however, the average heart rate now doubled, exceeding the 100 bpm threshold for bigeminy to develop in the LBB. Thus, the triggered beat from the RBB elicited a triggered beat from the LBB, producing a QRS morphology resembling RBB

block (bottom row). The arrival of this beat in the RBB then caused a triggered AP arising from the RBB, with LBB block morphology, and so forth, in a ping pong fashion. Fig. 3B shows that the computed ECG from the model closely resembles that recorded from a patient during BVT¹². Thus, each triggered AP from the RBB reciprocally triggers an AP from LBB, and vice versa, producing VT with an alternating LBB/RBB block pattern, as shown by the orange symbols in Fig. 4. In the example in Fig. 3, BVT terminated spontaneously, as often occurs clinically, but sustained BVT was also simulated with different parameter settings. Had we chosen the LBB to have the lower heart rate threshold for bigeminy, the results would be the same, except that the BVT would have begun with a RBB block QRS morphology instead of LBB block.

This same scenario can also account for the classical human CPVT pattern of RBB block with alternating QRS axis, assuming that the two bigeminal foci are located in distal regions of the left anterior and left posterior fascicles of the LBB (Fig. 4, blue symbols). Thus, the reciprocating bigeminal beats arising from the distal left posterior and anterior fascicles would exhibit RBB block with left and right axis deviation, respectively. Cases of BVT have also been reported in which the axis alternates, but the QRS is narrow¹³. This variant could be explained by bigeminal beats arising alternately from the anterior and posterior fascicles, but conducting retrogradely and blocking antegradely (Fig. 4, brown symbols). Thus, retrograde conduction to the contralateral fascicle and RBB would result in a narrow QRS with right or left axis deviation.

Finally, we simulated the degeneration of BVT into polymorphic VT, by assuming that when BVT further increases heart rate, additional sites in the HPS are recruited to develop bigeminy. Fig. 5 shows a scenario where an additional site exists at a Purkinje-myocyte junction in the RV free wall. When this third site developed triggered ventricular bigeminy, the earliest activation occurred irregularly among the three sites, creating a polymorphic VT pattern on the computed ECG, similar to that observed in a patient¹². Similar patterns developed when more than three sites develop spontaneous SR Ca release activity (data not shown).

Discussion

Both supraventricular or ventricular mechanisms of BVT have been proposed in the past, involving either focal or reentrant mechanisms¹⁰. A supraventricular mechanism with alternating left anterior and left posterior fascicular block¹⁷ was largely excluded with the advent of intracardiac recordings, which failed to show a His bundle potential preceding the alternating QRS complexes during BVT^{18, 19}. Postulated ventricular mechanisms have included a single focus in the proximal His bundle or bundle branches with alternating left fascicular block, or single or double foci in the distal HPS. In the single focus case, there is no obvious explanation for why fascicular or bundle branch block should alternate during BVT. Usually, concealed retrograde conduction perpetuates block in the fascicle/bundle branch that initially develops conduction block. Even if a conduction gap prevents concealed retrograde conduction from perpetuating block, both fascicles/bundle branches would have to exhibit the same conduction gap phenomena, which seems highly unlikely. In the double foci case, if neither focus is protected by entrance block, the faster focus should overdrive the slower focus, producing monomorphic VT rather than BVT. If both foci are protected by entrance block, then they would have to have identical cycle lengths, phase-shifted by exactly 180° to produce a constant cycle length during BVT, which also is improbable. If only one focus is protected by entrance block, then it could induce a second focus to fire at a fixed coupling interval, but the coupling interval would have to be exactly half of the first focus's cycle length to produce a constant cycle length during BVT.

In contrast to these complicated mechanisms, reciprocating bigeminy solves the puzzle of alternating QRS morphology by a simple “ping pong” mechanism in which DAD-induced triggered activity develops at different heart rate thresholds in different regions of the HPS or ventricles, consistent with known cellular properties of DAD-induced triggered activity^{28, 33, 34}. To produce a constant (i.e. nonalternating) cycle length during BVT requires only that the coupling intervals of the triggered beats be similar at the two sites.

Although we have modeled the bigeminy to be due to triggered activity from DADs, the same results are predicted for any mechanism inducing ventricular bigeminy (including automaticity or reentry) at more than one location in the ventricles. In addition, there is no strict requirement for the two bigeminal foci to be located in the distal HPS in opposite fascicles or ventricles. For example, two reciprocating triggered foci located in the same ventricle⁸, or at sites in the endocardium and epicardium, could also produce BVT by this mechanism³⁵, although the QRS axis and morphology changes would be different. However, in humans, the most common BVT pattern during digitalis toxicity and CVPT is RBB block with alternating right and left axis deviation, consistent with reciprocating ectopic foci located in the distal left anterior and posterior fascicles of the left bundle. In mouse, due to its smaller heart size, the more common pattern may be foci located on opposite sides of the interventricular septum.

Finally, we show that if the increased heart rate during BVT induces a third bigeminal focus in the HPS, the interactions between the three foci can produce irregular activation patterns resulting in polymorphic VT (Fig. 5). Since the model is deterministic, the irregularity may be due to chaos, which is a common scenario observed with coupled oscillators³⁶. As heart rate progressively accelerates, we speculate that additional regions develop DADs, making the conversion to VF progressively more likely.

In summary, we conjecture that the full spectrum of arrhythmias described electrocardiographically in acquired and familial conditions associated with BVT can be accounted for based on the known properties of DAD-triggered arrhythmias, as follows:

- i. Ventricular bigeminy, when a single site in the HPS or ventricular myocardium develops a single DAD-triggered beat following each sinus beat;
- ii. BVT, when a second site develops ventricular bigeminy, and reciprocally activates the first site by the ping-pong mechanism described above;
- iii. Polymorphic VT, when 3 or more sites concurrently develop bigeminy. Note that these first 3 mechanisms specifically require bigeminy, i.e. that DADs are capable of triggering only a single PVC following each sinus or paced beat, so that the subsequent beat has to arise from a different location (thereby altering the QRS morphology/axis).
- iv. Monomorphic VT, when bigeminy progresses to repetitive DADs which generate a run of triggered activity, such that the site with most rapid rate of the triggered activity overdrives the other slower sites, producing a monomorphic QRS complex.
- v. Degeneration to VF, when any of these VT forms results in wavebreak and initiation of reentry, which is then likely to be maintained by a mixture of reentry and DAD-triggered focal activations.

Limitations

Several limitations of our study should be recognized. Our Purkinje AP model is an approximation that does not replicate all experimental details such as a lowered AP plateau²¹. We did not attempt to build a complete “bottom up” model linking Ca waves and DADs

at the subcellular-cellular levels to DADs and triggered activity at the tissue-whole heart levels. In particular, Ca waves and DADs at the cellular level are strongly influenced by stochastic factors. How they overcome source-sink mismatches in well-coupled tissue to produce regular behaviors such as ventricular bigeminy is not well-understood. Nevertheless, periodic arrhythmias attributed to DADs, such as ventricular bigeminy are commonly observed in cardiac tissue^{28, 33, 34} in the setting of glycoside toxicity and in association with BVT^{9–11}. The experimental observation that PVCs with wide QRS complexes arise from the HPS during or after rapid pacing also implies that different regions of the heart must have different rate thresholds for DAD-mediated triggered activity, since otherwise, PVCs would all have a narrow QRS complex. This is not surprising, since many factors which influence the precise rate threshold at which DADs cause triggered activity, including cell properties, intercellular coupling, geometrical factors influencing the source-sink relationship in the bundle branches and HPS, etc. To illustrate the general feasibility of the reciprocating bigeminy mechanism, we therefore phenomenologically introduced these well-documented experimental features into our computer model, rather than a building a highly detailed model from the bottom up incorporating stochastic elements, etc. To simplify the computer modeling, we also simulated a ventricular slice, rather than the full 3D anatomic heart. This is not likely to change the findings, however, since the ventricular myocardium acts simply as a passive electrical conduit for the ping pong dynamics occurring in the HPS.

Supplementary Material

Refer to Web version on PubMed Central for supplementary material.

Acknowledgments

Funding Sources. This study was supported by NIH/NHLBI grants P01 HL078931 and R01 HL103662, and the Laubisch and Kawata Endowments.

We thank Tannaz Tebbi for technical assistance.

Non-standard Abbreviations and Acronyms

BVT	bidirectional ventricular tachycardia
CPVT	catecholaminergic polymorphic ventricular tachycardia
DAD	delayed afterdepolarization
EAD	early afterdepolarization
ECG	electrocardiogram
HPS	His-Purkinje system
LBB	left bundle branch
LV	left ventricle
PVC	premature ventricular complex
RyR2	Ryanodine receptor
RBB	right bundle branch
RV	right ventricle

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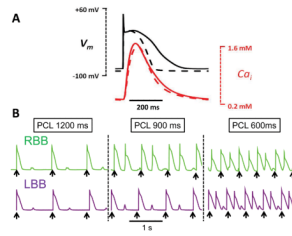


Fig. 1.

A. Comparison of simulated rabbit ventricular (dashed line) and Purkinje (solid line) APs and Ca_i transients, during pacing at 600 ms. **B.** Rate dependence of DADs and bigeminy in the Purkinje cell AP models. In the green trace *a*, the rate threshold for DAD-induced bigeminy was 67 bpm (PCL 900 ms), such that pacing (black arrows) at both 900 and 600 ms induced bigeminy. In purple trace *b*, the bigeminy rate threshold was 100 bpm (PCL 600 ms), such that pacing at 600 ms, but not 900 ms, induced bigeminy.

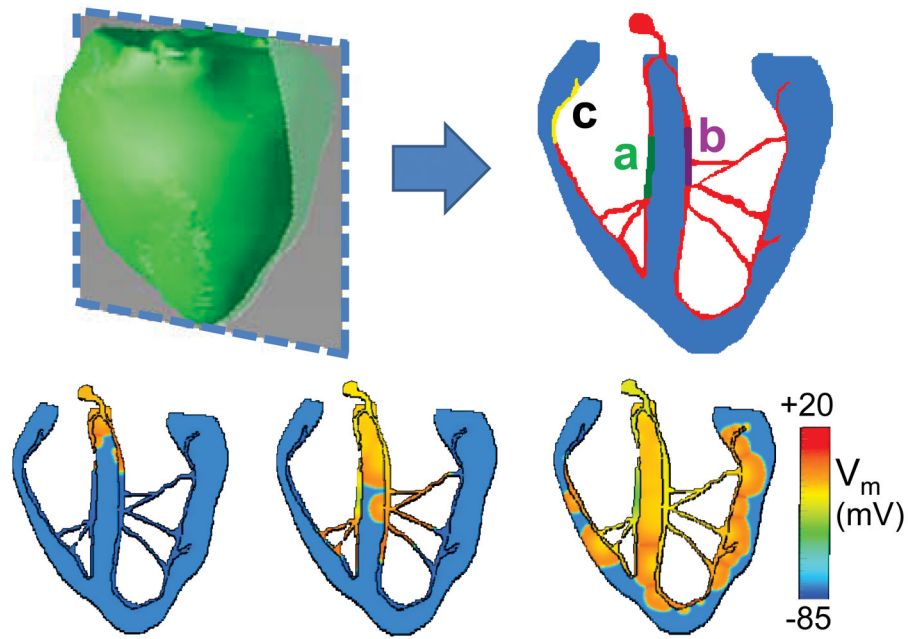


Fig. 2.
A. The anatomic rabbit ventricles model (green), showing a 2D section (blue) of myocardium with the HPS (red) incorporated. Regions of the HPS susceptible to DAD-induced bigeminy in the RBB (*a*, green) and LBB (*b*, purple) are indicated. In some simulations, a third region (yellow) also developed DAD-induced bigeminy. **B.** Voltage snapshots of normal activation when the His bundle is paced.

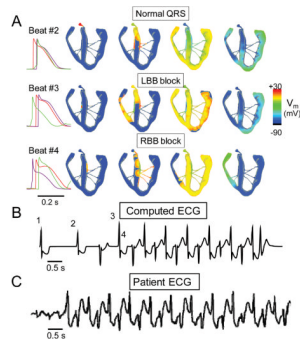


Fig. 3. Simulated BVT

A. Voltage snapshots showing the activation sequence at the onset of BVT. Beat #2 is the last paced beat, with normal activation. Beat #3 is the 1st beat of BVT, due to a DAD-triggered AP arising in the RBB, resulting in a QRS with LBB block pattern. Beat #4 is the 2nd beat of BVT, due to a DAD-triggered AP arising in the LBB, resulting in a QRS with RBB block pattern. Traces on right show the timing of APs recorded from the His bundle (red), RBB (green), and LBB (purple). **B.** The computed ECG from the simulation in A, showing BVT. **C.** ECG recorded in a patient during BVT ¹².

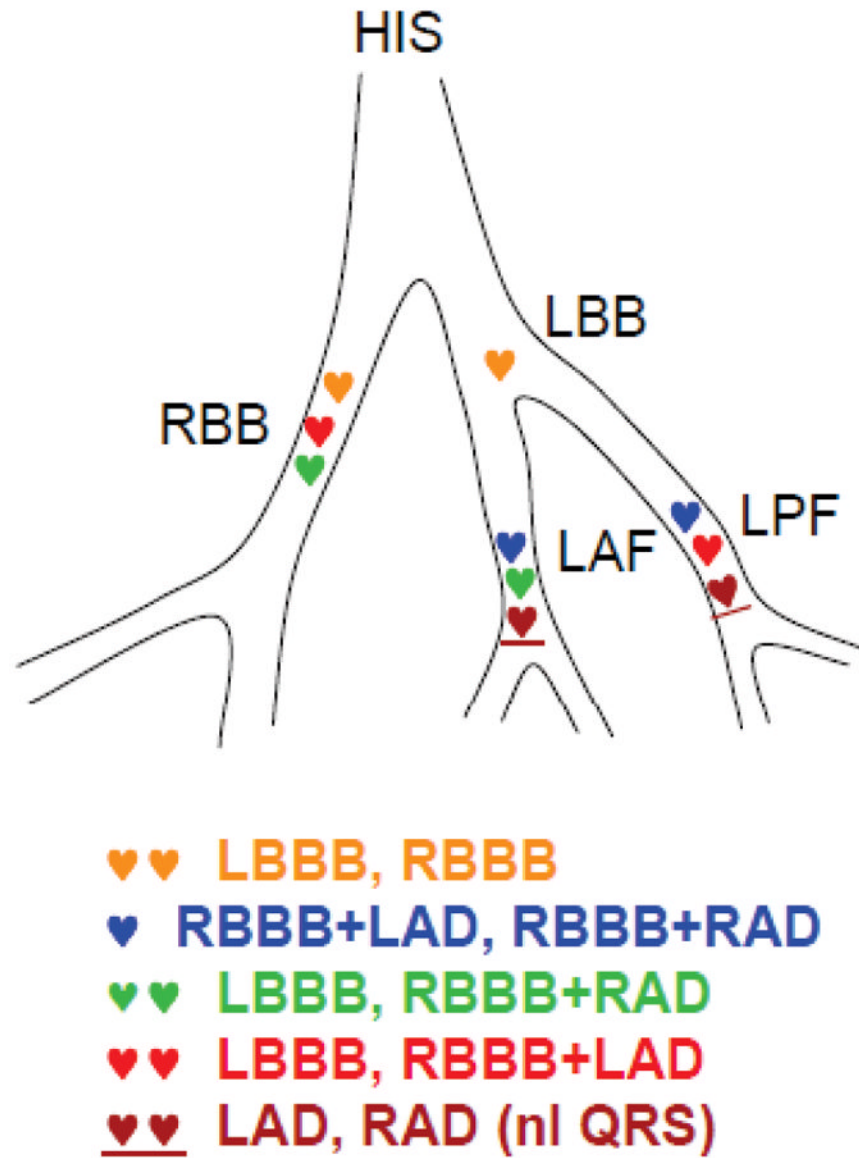


Fig. 4. ECG patterns of BVT corresponding to locations of pairs of foci with reciprocating bigeminy. HIS, His bundle; LBB, left bundle branch; RBB, right bundle branch; LAF, left anterior fascicle; LPF, left posterior fascicle; LBBB, left bundle branch block; RBBB, right bundle branch block; LAD; left axis deviation; RAD, right axis deviation. See text for details.

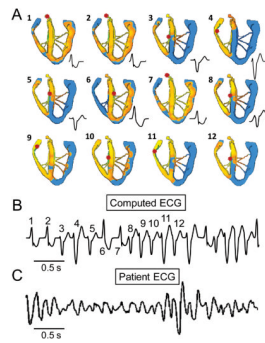


Fig. 5. Simulated polymorphic VT

A. Voltage snapshots showing the activation sequences corresponding to different QRS morphologies during polymorphic VT caused by 3 foci with reciprocating bigeminy. Red dot in each panel indicates the earliest activation site. **B.** The computed ECG from the simulation in A, showing polymorphic VT (with beat numbers corresponding to snapshots in A). **C.** ECG recorded in a patient with CPVT¹².

Table 1

Current conductances used in Purkinje and ventricular myocyte AP models.

	Purkinje	Myocyte
$\bar{G}_{o,f}$	0.165	0.11
$\bar{G}_{to,s}$	0.06	0.04
$\bar{G}_{ca,L}$	364.0	273.0
$\bar{G}_{ca,b}$	0.0010556	0.001508
\bar{G}_{kr}	0.0041625	0.0125
\bar{G}_{ks}	0.04615	0.1386
\bar{G}_{kl}	0.15	0.3
\bar{G}_{Na}	24.0	12.0

Table 2

I_{spon} parameters for the Purkinje AP model exhibiting DADs, located in the LBB, RBB, and distal Purkinje muscle junction (PMJ), as shown in Fig. 2.

	G_{spon}	K_1	K_2	τ_p
<i>RBB</i>	250.0	110.0	110.1	10.0
<i>LBB</i>	180.0	111.5	111.6	10.0
<i>PMJ</i>	215.0	111.0	111.1	10.0