

Brief Communication

Cerebral formation of free radicals during hypoxia does not cause structural damage and is associated with a reduction in mitochondrial PO_2 ; evidence of O_2 -sensing in humans?

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Cellular hypoxia triggers a homeostatic increase in mitochondrial free radical signaling. In this study, blood was obtained from the radial artery and jugular venous bulb in 10 men during normoxia and 9 hours hypoxia (12.9% O_2). Mitochondrial oxygen tension ($P_{O_2}^{mit}$) was derived from cerebral blood flow and blood gases. The ascorbate radical ($A^{\bullet-}$) was detected by electron paramagnetic resonance spectroscopy and neuron-specific enolase (NSE), a biomarker of neuronal injury, by enzyme-linked immunosorbent assay. Hypoxia increased the cerebral output of $A^{\bullet-}$ in proportion to the reduction in $P_{O_2}^{mit}$, but did not affect NSE exchange. These findings suggest that neuro-oxidative stress may constitute an adaptive response.

Journal of Cerebral Blood Flow & Metabolism (2011) 31, 1020–1026; doi:10.1038/jcbfm.2011.2; published online 9 February 2011

Keywords: brain; free radicals; hypoxia; mitochondrial oxygen tension; oxygen sensing

Introduction

Although the human brain represents only 2% body weight, it accounts for a disproportionate 25% of

basal oxygen (O_2) consumption to support the demands of neuronal activity. This commitment to an obligatory high rate of O_2 consumption combined with limited glycolytic capacity renders the brain exquisitely sensitive to O_2 deprivation (hypoxia), with a correspondingly high vulnerability for failure (Bailey *et al*, 2009a). As a consequence, elaborate cellular O_2 -sensing mechanisms have evolved to preserve O_2 homeostasis and to ultimately prevent brain damage (Sharp and Beraudina, 2004).

However, despite considerable progress in our understanding of the cerebral pathways activated during hypoxia, a unified mechanism that allows the brain to sense and ultimately respond to O_2 remains elusive. Emerging evidence suggests that the mitochondrion may function as the primary O_2 'sensor', given its capacity to increase free radical and associated reactive oxygen–nitrogen species formation during hypoxia (Chandel *et al*, 1998). Although thermodynamically capable of causing structural

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This study was funded by The Danish National Research Council (File Number 22-04-0413), The Copenhagen Hospital Corporation, The Danish National Research Foundation (Grant 504-14), The Laerdal Foundation, The AP Møller Foundation, the Jensa La Cour Foundation, the Larsen Foundation, and the Hoejmosgaard Foundation. This study was conducted at the Centre of Inflammation and Metabolism supported by grants from the Danish National Research Foundation (DG 02-512-555) and the Commission of the European Communities (Contract No. LSHM-CT-2004-005272 EXGENESIS).

Received 7 November 2010; revised 20 December 2010; accepted 21 December 2010; published online 9 February 2011

damage when in excess, these oxidant signals can act as secondary messengers (Wright *et al*, 2004), which activate O₂ salvage genes through stabilization of the transcription factor hypoxia-inducible factor-1α (Guzy and Schumacker, 2006) in physiologically controlled, although as of yet undefined, amounts.

In support, human studies have documented an increased systemic formation of free radicals during hypoxia in proportion to arterial desaturation (Bailey *et al*, 2009b). However, whether any potential relationship exists between cerebral mitochondrial PO₂ and the focal (cerebral) formation of free radicals remains to be examined. This is clinically relevant, given the cerebral complications encountered in diseases defined by hypoxemia, notably obstructive sleep apnea and chronic obstructive pulmonary disease (Sharp and Bernaudin, 2004).

To investigate this, we combined electron paramagnetic resonance spectroscopy for direct detection of the ascorbate radical (A•⁻) with calculation of cerebral mitochondrial PO₂ ($\bar{P}_{O_2}^{mit}$) in a group of healthy volunteers exposed to hypoxia. We hypothesized that compared with normoxia, hypoxia would promote the cerebral formation and net output of A•⁻ as indicated by a negative arterio-jugular venous concentration difference (a-jv_D). As we considered this to reflect an adaptive response that preserves O₂ homeostasis, we further hypothesized that A•⁻ output would correlate against the reduction in $\bar{P}_{O_2}^{mit}$ in the absence of neurovascular tissue damage as indicated by a lack of exchange in the neuronal-parenchymal injury biomarker, neuron-specific enolase (NSE).

Materials and methods

Subjects and Design

Ten males aged 27 ± 4 years old provided written informed consent following approval by the Scientific Ethics Committee of Copenhagen and Frederiksberg Municipalities (Denmark). After local anesthesia (2% lidocaine), subjects received a retrograde catheter in the right internal jugular vein using the Seldinger technique under ultrasound guidance with the tip advanced to the bulb of the vein. A radial arterial catheter was placed in the nondominant arm. Baseline samples were collected during normoxia (21% O₂) and after 9 hours passive exposure to hypoxia (12.9% O₂).

Cerebral Oxygenation

Hemoglobin (Hb), Hct (hematocrit), partial pressure of oxygen and carbon dioxide (PO₂/PCO₂), oxyhemoglobin saturation (SO₂), pH, P50, temperature, and (whole-blood) glucose were determined using a blood gas analyzer (ABL 715; Radiometer Medical, Copenhagen, Denmark). Global cerebral blood flow (CBF) was measured using the Kety–Schmidt

technique in the desaturation mode using nitrous oxide (N₂O) as the tracer (Taudorf *et al*, 2009). In brief, subjects inhaled 5% N₂O and O₂ in N₂ (corresponding to both normoxic and hypoxic inspirates) for 30 minutes. From 2 minutes before the cessation of N₂O until 15 minutes thereafter, 12 sets of paired synchronized samples were drawn into gas-tight syringes from the arterial and venous catheters. Samples were equilibrated against air in a water bath at 37°C for 60 minutes, and N₂O concentration was measured by photoacoustic spectroscopy (Innova Photoacoustic Field Gas Monitor 1412; Brüel & Kjaer, Copenhagen, Denmark). Unlike our previous study (Taudorf *et al*, 2009), all tubing was presaturated using a syringe filled with pure N₂O, O₂, and N₂ corresponding to the inspired air mixtures before running experimental samples. Global CBF was subsequently derived by the Kety–Schmidt equation given as:

$$CBF = 100 \times \lambda \times \frac{c_{jv}(\text{equilibrium})}{\int_{t=0}^{t=\infty} (c_{jv}(t) \times dt) \int_{t=0}^{t=\infty} (c_a(t) \times dt)}$$

$$= 100 \times \lambda \times \frac{\text{height at equilibrium}}{\text{area between curves}},$$

where $c_{jv}(t)$ and $c_a(t)$ are the jugular venous and arterial concentration of the tracer at time (t) in minutes, respectively, and λ represents the brain–blood partition coefficient (mL/g) calculated from data reported previously (Kety *et al*, 1948):

$$\lambda = 1.167 - (0.0026 \times \text{Hct} (\%))$$

Cerebral plasma flow (CPF) was calculated as CBF × (1–Hct). Cerebral O₂ delivery was calculated as:

$$CBF \times caO_2,$$

where caO₂ refers to arterial oxygen content (mmol):

$$caO_2 = 0.60 \times SaO_2 \times Hb + 0.0013 \times PaO_2$$

The oxygen extraction fraction (EO₂) was determined by:

$$EO_2 = \frac{c_aO_2 - c_vO_2}{c_aO_2} \times 100 (\%)$$

The global cerebral metabolic rate of oxygen (CMRO₂) was calculated as:

$$CMRO_2 = CBF \times a-jv_D O_2,$$

where a-jv_DO₂ refers to the arterio-jugular venous O₂ content difference.

The OGI (oxygen–glucose index) was calculated as:

$$OGI = \frac{c_aO_2 - c_vO_2}{c_a\text{glucose} - c_v\text{glucose}}$$

Using established formalism (Gjedde, 2005; Gjedde *et al*, 2005; Rasmussen *et al*, 2007), the mean capillary oxygen saturation ($\bar{S}_{O_2}^{cap}$) was calculated as:

$$\bar{S}_{O_2}^{cap} = SaO_2 \left(1 - \frac{c_aO_2 - c_vO_2}{2c_aO_2} \right),$$

assuming that O₂ extraction rises linearly with distance as blood traverses the capillary network. Solution of the Hill equation permitted calculation of the (mean) capillary PO₂ ($\bar{P}_{O_2}^{cap}$):

$$\bar{P}_{O_2}^{cap} = P_{50a}^{Hb} h_a \sqrt{\frac{S_{O_2}^{cap}}{1 - S_{O_2}^{cap}}},$$

where P_{50a}^{Hb} is the PO₂ when Hb is half-saturated (29 mmHg) and h_a is Hill's coefficient (2.84 for arterial blood). Given the absence of capillary recruitment in the brain, O₂ diffusibility (L) was calculated during hypoxia (in which mitochondrial oxygen tension could be assumed to be negligible) and given as:

$$L = \frac{CMRO_2}{\bar{P}_{O_2}^{cap}}$$

based on group mean values and assumed to be constant at 7.8 μmol/100 g/min/mmHg for any given CBF. The mean mitochondrial PO₂ ($\bar{P}_{O_2}^{mit}$) was subsequently given by:

$$\bar{P}_{O_2}^{mit} = \bar{P}_{O_2}^{cap} - \frac{CMRO_2}{L}$$

The assumptions and limitations associated with the formalism underlying the nonlinear flow–metabolism coupling model have been discussed in detail elsewhere (Gjedde, 2005).

Ascorbate (Antioxidant)

Exactly 100 μL of plasma was stabilized and deprotonated by adding 900 μL of 5% metaphosphoric acid (Sigma Chemical, Dorset, UK). Ascorbate was assayed by fluorimetry based on the condensation of dehydroascorbic acid with 1,2-phenylenediamine (Bailey *et al*, 2009d). The intraassay and interassay coefficients of variations were both <5%.

Ascorbate (Free Radical)

Exactly 1 mL of plasma was injected into a high-sensitivity multiple-bore sample cell (AquaX, Bruker Instruments Inc., Billerica, MA, USA) housed within a TM₁₁₀ cavity and analyzed by X-band electron paramagnetic resonance spectroscopy operating at 100 kHz modulation frequency, 0.65 Gauss (G) modulation amplitude, 10 mW microwave power, 2×10^5 receiver gain, and 41 milliseconds time constant for 3 incremental scans (Bailey *et al*, 2009b). Spectra were filtered identically using WINEPR (Version 2.11, Bruker, Karlsruhe, Germany), and the double integral of each doublet was calculated using the Origin software (Version 5.0, OriginLab[®], Northampton, MA, USA). The intraassay and interassay coefficients of variations were both <5%.

Neuron-Specific Enolase

Neuron-specific enolase was incorporated as a molecular biomarker of neuronal-parenchymal in-

jury using a commercially available enzyme-linked immunosorbent assay (CanAg, Ref 420-10) with a lower detection limit of <1 μg/L. The intraassay and interassay coefficients of variations were both <5%.

Cerebral Net Exchange

This was calculated as:

$$CPF \times a - jv_D$$

By convention, a negative value reflects net cerebral output or gain, whereas a positive value reflects consumption or loss.

Cephalalgia

Symptoms of acute mountain sickness (AMS) were assessed using the LL (Lake Louise) (Roach *et al*, 1993) and ESQ-C (Environmental Symptoms Questionnaire Cerebral) (Sampson *et al*, 1983) scoring systems. A clinically validated visual analog scale was used to measure headache (Iversen *et al*, 1989). Clinical AMS was diagnosed if a subject presented with a combined total LL score (self assessment + clinical score) of ≥ 5 points and ESQ-C score ≥ 0.7 points (Bailey *et al*, 2009b).

Statistical Analysis

The Shapiro-Wilk *W*-tests confirmed distribution normality. Cerebral oxygenation and exchange data were analyzed using a combination of paired samples *t*-tests and two-way repeated-measures ANOVA (analysis of variance). Relationships were examined using a Pearson product moment correlation. Significance was established at $P < 0.05$ and data are presented as mean \pm s.d.

Results

Cerebral Oxygenation

Hypoxia was associated with a reduction ($P < 0.05$ versus normoxia) in PaO₂ (107 \pm 6 mmHg to 46 \pm 3 mmHg), PaCO₂ (43 \pm 2 mmHg to 35 \pm 2 mmHg), SaO₂ (99% \pm 1% to 83% \pm 3%), and corresponding cerebral O₂ delivery (Table 1). As a consequence, $\bar{S}_{O_2}^{cap}$, $\bar{P}_{O_2}^{cap}$, and $\bar{P}_{O_2}^{mit}$ were also shown to decrease. An increase in EO₂ and (tendency towards) CBF counteracted hypoxemia, thus preserving CMRO₂. By contrast, the OGI was not altered during hypoxia (6.11 \pm 0.79 versus 5.86 \pm 0.95 in normoxia, $P > 0.05$).

Free Radicals

Hypoxia did not affect the $a-jv_D$ or subsequent exchange of ascorbate (hypoxia: 0.052 \pm 0.250 mmol/100 g/min versus normoxia: 0.120 \pm 0.249 mmol/100 g/min, $P > 0.05$). In contrast, hypoxia decreased the $a-jv_D$

Table 1 Cerebral oxygenation

	Normoxia	Hypoxia
CBF (mL/100 g/min)	85 ± 15	94 ± 17
CPF (mL/100 g/min)	51 ± 9	57 ± 11
O ₂ delivery (μmol/100 g/min)	728 ± 145	666 ± 108
a-jv _D O ₂ (mmol)	2.8 ± 0.3	2.7 ± 0.4
EO ₂ (%)	33 ± 3	38 ± 6 [†]
CMRO ₂ (μmol/100 g/min)	243 ± 55	249 ± 34
$\bar{S}_{O_2}^{cap}$ (%)	82.7 ± 1.3	66.9 ± 3.6 [†]
$\bar{P}_{O_2}^{cap}$ (mm Hg)	43.3 ± 2.0	33.3 ± 2.0 [†]
$\bar{P}_{O_2}^{mit}$ (mm Hg)	14.6 ± 4.1	1.4 ± 5.5 [†]

a-jv_DO₂, arterio-jugular venous O₂ content difference; CBF, cerebral blood flow; CMRO₂, cerebral metabolic rate of oxygen; CPF, cerebral plasma flow; EO₂, oxygen extraction fraction; $\bar{P}_{O_2}^{cap}$, mean capillary PO₂; $\bar{P}_{O_2}^{mit}$, mean mitochondrial PO₂; $\bar{S}_{O_2}^{cap}$, mean capillary O₂ saturation.

Values are mean ± s.d.; [†]different ($P < 0.05$).

of A^{•-} (-522 ± 471 AU/100 g versus -148 ± 256 AU/100 g, $P < 0.05$) primarily caused by an increase in jugular venous outflow ($P < 0.05$). Typical examples of A^{•-} spectra ($a^{H^{14}} \approx 1.76$ G, $\Delta H_{pp} \approx 0.6$ G, and $g = 2.0052$) observed with corresponding signal intensities are illustrated in Figure 1A. This translated into an increased cerebral output in hypoxia ($-29,283 \pm 25,852$ AU/100 g/min versus $-7,131 \pm 12,260$ AU/100 g/min, $P < 0.05$), which correlated directly against the reduction in $\bar{P}_{O_2}^{mit}$ (Figure 1B).

Neurovascular Integrity

There was no evidence of neuronal-parenchymal injury because hypoxia affected neither the a-jv_D nor the exchange of NSE (34.6 ± 40.2 μg/100 g/min versus normoxia: 30.2 ± 36.3 μg/100 g/min, $P > 0.05$).

Cephalalgia

Hypoxia increased AMS (LL: 3 ± 2 points versus normoxia: 0 ± 0 points, $P < 0.05$; ESQ-C: 0.803 ± 0.674 AU versus normoxia: 0.000 ± 0.000 AU, $P < 0.05$) and headache (visual analog scale: 29 ± 23 mm versus normoxia: 0 ± 0 mm, $P < 0.05$) scores, which correlated modestly against the increased cerebral output of A^{•-} (LL: $r = -0.61$, $P = 0.06$; ESQ-C: $r = -0.56$, $P = 0.09$; visual analog scale: $r = -0.65$, $P = 0.04$). Furthermore, the one subject diagnosed with clinical AMS exhibited the greatest reduction in $\bar{P}_{O_2}^{mit}$ (-30.9 mmHg) and increase in the a-jv_D ($-1,334$ AU/100 g) and subsequent cerebral output of A^{•-} ($-75,424$ AU/100 g/min) during hypoxia.

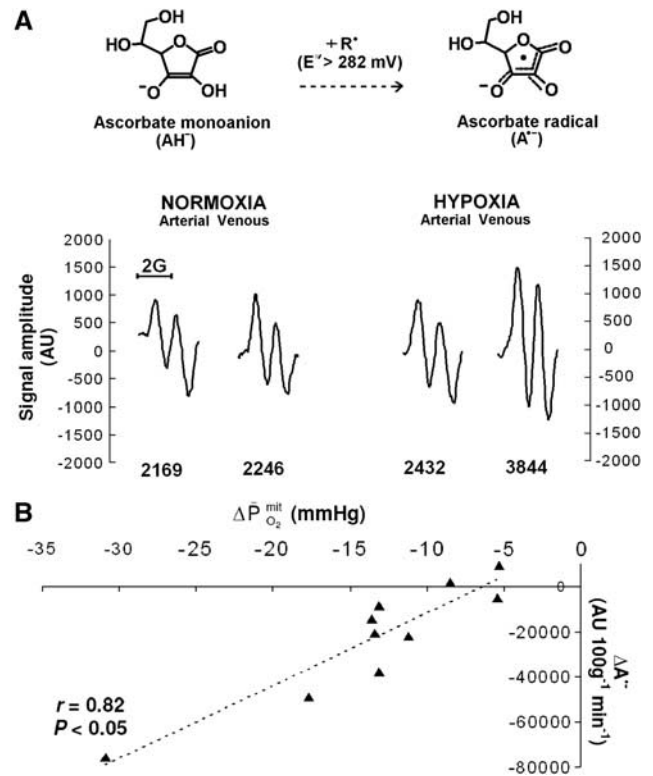


Figure 1 Cerebral formation of the ascorbate radical (A^{•-}) during hypoxia. **(A)** Oxidation of the ascorbate monoanion (AH⁻) by an initiating species (R[•]) with a one-electron reduction potential (E°) greater than +282 mV yields the domesticated ascorbate radical (A^{•-}). The unpaired electron is delocalized over a highly conjugated tricarbonyl π -system rendering it resonance stabilized, facilitating direct detection by electron paramagnetic resonance (EPR) spectroscopy. Note the increase in the systemic and cerebral formation of A^{•-} during 9 hours passive exposure to hypoxia. Digits below each spectrum represent EPR signal intensities in arbitrary units (AU) (double integral, which is directly proportional to the concentration of A^{•-}). **(B)** Relationship between the reduction (Δ , calculated as the hypoxic minus the normoxic control value) in mitochondrial PO₂ ($\bar{P}_{O_2}^{mit}$) and increase in the cerebral output of ascorbate radicals (A^{•-}).

Discussion

The major finding in this study was that the increased cerebral output of free radicals in the form of A^{•-} observed during hypoxia did not compromise neuronal-parenchymal integrity and correlated directly against the reduction in $\bar{P}_{O_2}^{mit}$. Although this does not disassociate cause from effect, it points towards an adaptive mechanism by which mitochondria potentially 'sense' changes in cerebral O₂ tension through free radical formation with the capacity to activate signaling pathways that serve to defend O₂ homeostasis in the face of a reduced PO₂.

These findings extend previous electron paramagnetic resonance spin-trapping reports of an increased cerebrospinal fluid concentration (Bailey *et al*, 2006) and net cerebral output of blood-borne alkoxy-alkyl radicals during hypoxia (Bailey *et al*, 2009d). In the

current study, we took advantage of $A^{\bullet-}$ as a biomarker to determine the brain's 'global' rate of free radical flux *in vivo* rather than focus on select species trapped *ex vivo* whose individual contributions to the neuro-oxidative cascade remain, as a consequence, uncertain. Given that the one-electron reduction potential associated with the $A^{\bullet-}$ /ascorbate monanion (AH^-) couple is so low ($E^{o'} = +282$ mV at pH 7.0), any radical generated across the cerebral circulation will react endogenously with this terminal small-molecule antioxidant to form the distinctive doublet $A^{\bullet-}$ that is readily detectable by electron paramagnetic resonance [($R^{\bullet} + AH^- \rightarrow A^{\bullet-} + R-H$) (Buettner, 1993)]. The fact that hypoxia did not affect ascorbate exchange further emphasizes that the increased output of $A^{\bullet-}$, detectable even within the time constraints of a single arterio-venous transit, likely reflects *de novo* radical formation (and not simply increased ascorbate auto-oxidation) by any number of oxidizing species whose identities remain to be established.

Although beyond the scope of this study, the source, mechanisms, and functional significance of free radical formation in hypoxia remain to be established. Given its modest antioxidant defenses, abundance of catalytic transition metals, auto-oxidizable neurotransmitters, and neuronal membrane lipids rich in polyunsaturated fatty acid side chains exposed to a disproportionately high O_2 flux, the human brain has traditionally been considered especially vulnerable to molecular attack (Bailey *et al*, 2009a). To examine this, we measured exchange of the dimeric enzyme NSE, the neuronal form of the glycolytic enzyme enolase (2-phospho-D-glycerate hydrolase), which is located almost exclusively within neuronal cell bodies, axons, and neuroendocrine cells (Schmechel *et al*, 1978). Its appearance across the cerebral circulation would therefore reflect parenchymal tissue injury in direct proportion to the extent of damage (Schoerhuber *et al*, 1999). Thus, the lack of exchange observed in the current study combined with previous reports that have consistently failed to document any increase in the systemic (Bailey *et al*, 2009b), cerebrospinal fluid (Bailey *et al*, 2006), and transcerebral (Bailey *et al*, 2009d) concentration of the astrocytic protein S100 β , a peripheral biomarker of blood-brain barrier damage, confirms that cerebral free radical formation proceeds in hypoxia without compromising neurovascular integrity.

As anticipated, hypoxia was associated with AMS and headache with modest correlations observed between symptom scores and the increased cerebral output of $A^{\bullet-}$. Similar correlations have been observed between the increase in (cephalic) venous $A^{\bullet-}$ and cephalgia which could be explained, at least in part ($\approx 30\%$ of the variance) by the reduction in arterial oxyhemoglobin saturation (Bailey *et al*, 2009b). Thus, if AMS is indeed associated with more marked arterial hypoxemia as suggested previously (Ge *et al*, 1997), symptoms may simply prove the

consequence of more marked $\bar{P}_{O_2}^{mit}$ -induced cerebral reactive oxygen-nitrogen species formation, which although controversial (Bailey *et al*, 2009c), have the capacity to sensitize perivascular sensory nerves and activate trigeminovascular nociceptors (Sanchez del Rio and Moskowitz, 1999). Follow-up exchange studies using 'brain-specific' targeted antioxidants are warranted to confirm whether neuro-oxidative nitrosative stress is indeed a causal or merely a consequential event, and its corresponding impact on cerebral oxygenation.

These findings force a reappraisal of free radicals as simply damaging or toxic 'accidents of chemistry' and argue that their formation by the human brain may represent an adaptive response to hypoxia. It is tempting to speculate that the increases in CBF and EO_2 observed in the current study were subject to redox regulation and served to maintain global cerebral oxygenation in the face of severe hypoxemic hypocapnia. This concept is consistent with earlier work implicating (mitochondrial) reactive oxygen-nitrogen species as signaling molecules that coordinate the intrinsic mitochondrial cell death pathway in response to a diverse range of cellular stressors (Wright *et al*, 2004). More recently, *in vitro* studies that have identified the electron transport chain as the primary O_2 sensor, with complex III-derived reactive oxygen species released to the intermembrane space and cytosol as signals capable of triggering transcriptional and post-translational responses to hypoxia, notably stabilization of hypoxia-inducible factor-1 α , which ultimately preserve cellular O_2 supply (Waypa *et al*, 2010). In support, antioxidant prophylaxis was recently associated with a reduction in brachial artery vasodilation in exercising humans (Richardson *et al*, 2007), further establishing the functional importance of free radical formation in controlled, although as of yet undefined, amounts.

It is important to recognize that our findings reflect 'global' as opposed to 'regional' cerebral responses to hypoxia and the techniques used lack the temporal resolution required to assess dynamic change. The regional variation in the CBF response to acute (although isocapnic) hypoxia (8 minutes at 10% O_2) was confirmed by $H_2^{15}O$ positron emission tomography (Binks *et al*, 2008). The authors identified that phylogenetically older structures of the brain (nucleus accumbens, putamen, pallidum, caudate, and thalamus) exhibited greater increases in CBF during hypoxia compared with evolutionary younger (cortical) regions, which they speculated may represent an adaptive response that serves to protect regions responsible for (the more) essential homeostatic functions. Thus, like the skeletal and pulmonary circulatory response to hypoxia, the cerebral tissue is equally defined by marked diffusion-perfusion heterogeneity and as a consequence, one must therefore assume that the $\bar{P}_{O_2}^{mit}$ response to hypoxia follows a similar pattern in that regional variations likely predominate.

The values obtained for CBF and CMRO₂ (and thus by consequence the derivation of L) were noticeably higher than those reported in previous studies using the same technique, although with ¹³³Xe as the tracer (Madsen *et al*, 1993; Moller *et al*, 2002). The reasons for this discrepancy are not clear, although we remain confident that they were not caused by the contamination of samples with blood from extracerebral regions or as a consequence of inadequate desaturation.

Extracranial contamination would lead to a higher CBF, but would probably not affect CMRO₂ or even decrease the measured values, given the low metabolic rate and oxygen extraction of extracranial tissues. This is further supported by the observed OGIs, which would have been expected to be significantly greater than the observed values of ≈ 6 , given that such tissue would not be expected to be fueled exclusively by glucose. Finally, in the absence of radiographic evidence, all subjects reported a 'purl' during saline injection into the catheter, which indirectly confirms correct line placement.

In terms of desaturation, because N₂O is less soluble in biologic tissues than ¹³³Xe (Kety *et al*, 1948), the corresponding washout phase should theoretically be shorter and thus the error of measurement less. Furthermore, the sampling period was expanded from the original 10 minutes as applied with ¹³³Xe (Madsen *et al*, 1993; Moller *et al*, 2002) to 15 minutes to confirm a complete washout. Finally, our choice of N₂O as the tracer did not influence blood-borne nitric oxide metabolites, thus arguing against nitric oxide-mediated vasodilatation as a potential contaminant (Taudorf *et al*, 2009). Although the reasons underlying these atypically high CBF and CMRO₂ values remain unknown, the repeated-measures design ensured precision with our primary interest focused on the qualitative changes incurred by hypoxia.

In conclusion, the observation that hypoxia triggers a net cerebral output of free radicals in the absence of neurovascular tissue damage and in direct proportion to the reduction in $\bar{P}_{O_2}^{mit}$ provides the first tentative evidence for O₂-sensing by the human brain. It would be of interest to determine whether antioxidant prophylaxis ablates the cerebral adaptive response to hypoxia in future studies.

Acknowledgements

The authors acknowledge Mrs R Rousing and H Villumsen (University of Copenhagen, Denmark) for their technical assistance and Drs DM Murphy and E Carter (University of Cardiff, UK) for informed discussions.

Disclosure/conflict of interest

The authors declare no conflict of interest.

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