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COCHLEAR EFFERENT INNERVATION AND FUNCTION

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Abstract

Purpose of review—This review covers topics relevant to olivocochlear-efferent anatomy and function for which there are new findings in papers from 2009 to early 2010.

Recent findings—Work within the review period has increased our understanding of medial efferent (MOC) mechanisms in outer hair cells, MOC reflex tuning, MOC effects on distortion product otoacoustic emissions, the time course of MOC effects, MOC effects in psychophysical tests and on understanding speech, MOC effects in attention and learning, and lateral efferent function in binaural hearing. In addition, there are new insights into efferent molecular mechanisms and their effect on cochlear development.

Summary—Techniques for measuring efferent effects using otoacoustic emissions are now well developed and have promise in clinical applications ranging from predicting which subjects are susceptible to acoustic trauma to characterizing relationships between efferent activation and learning disabilities. To realize this promise, studies are needed in which these techniques are applied with high standards.

Keywords

medial olivocochlear; hearing; auditory psychophysics; descending control; auditory development

INTRODUCTION

This review will cover papers that significantly enhance understanding about olivocochlear (OC) efferents. Most of the papers studied medial OC (MOC) efferents, the myelinated efferents that innervate outer hair cells (OHCs) in mature animals. However, there is work on lateral OC (LOC) efferents that innervate auditory-nerve fibers under inner hair cells (IHCs), and on acetylcholine receptors -- the receptors for the main efferent neurotransmitter. For more detailed background see previous reviews [1,2].

MOC Mechanisms

One way MOC synapses may inhibit is by shunting OHC receptor currents [3]. Although measurements in isolated OHCs suggested that the OHC capacitance would severely limit this shunting [4], a new model that includes both piezoelectric and elastic OHC properties shows that the OHC capacitance is not as limiting as was believed [5**]. This model demonstrates that, in OHCs driving a load, the capacitance is strongly coupled to OHC

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In the cochlear base, MOC activity reduces basilar-membrane responses to sound by reducing the gain of cochlear amplification [6]. Recordings from auditory-nerve fibers show that MOC effects are different in the apical and basal halves of the cochlea [7]. To understand the mechanical basis for apical MOC effects, responses to sound were measured in the organ of Corti from Hensen cells in the guinea-pig apex [8]. MOC stimulation slightly reduced AC responses and had a larger, but still small (3 dB), effect on DC responses. Much remains to be learned about apical cochlear mechanics and MOC effects.

MOC reflex properties

The signature events of the "MOC reflex" are MOC excitation by sound and the resulting cochlear changes. Because MOC fibers have narrow tuning curves and innervate the cochlea tonotopically, the MOC reflex has been thought to provide narrowly-tuned negative feedback to cochlear places excited by sound [9]. MOC reflex effects can be noninvasively assayed using otoacoustic emissions (OAEs), which are ear-canal sounds whose amplitude depends on cochlear amplification. MOC-induced reductions of OAEs are sometimes called "suppressions," but because the reduction is due to MOC synaptic effects, not two-tone suppression, we refer to these reductions as MOC inhibition.

MOC-reflex tuning was recently measured using stimulus-frequency OAEs (SFOAEs) near 1 kHz, with MOC activity elicited by half-octave bands of noise varied over a 5 octave range [10*]. The MOC reflex had broad frequency tuning, and in some subjects noise bands centered 2.5 octaves above or below the probe tone produced significant MOC effects. For probes near 1 kHz, the most effective elicitor was 0.5–1 octave below the probe frequency (not at the probe frequency as expected). Similar tests using 0.5 and 4 kHz probes also showed broad tuning, but for 0.5 kHz the most effective elicitor was above the probe frequency (opposite the direction for 1 kHz probes), while for 4 kHz, the most effective elicitor was centered at the probe frequency, and, in addition, elicitors in a broad, lowfrequency region produced MOC activation [11, Lilaonitkul and Guinan, unpublished data]. These human results are similar to the pattern of inhibition versus characteristic frequency for auditory-nerve fibers found in cats [12], taking into account that the range of hearing in cats is 1–1.5 octaves higher than in humans. In another human study, MOC effects were measured by a method that extracts nonlinear SFOAE components plus changes in the linear component [13*]. This study found that elicitor-noise frequencies below the 4 kHz probe were primarily responsible for producing MOC activity, consistent with the above results.

MOC reflex frequency selectivity was also measured as a function of noise bandwidth for constant-SPL elicitors presented ipsilateral, contralateral or bilateral relative to the measurement ear [14*]. Probe frequencies of 0.5, 1 and 4 kHz were used. As noise bandwidth was increased up to 4–6.7 octaves, MOC effects, measured by the change in SFOAEs, grew even though noise spectral density in the frequency region of the probe decreased (Fig. 1). These results indicate that sound excitations over almost the whole range of hearing summate to elicit the MOC effects seen at a single frequency. The experiments also revealed an interesting aspect of reflex laterality. For narrow-band noises, ipsilateral effects were twice as large as contralateral effects, whereas for broad-band noises, ipsilateral and contralateral elicitors had similar effects (Fig. 1). Perhaps strong MOC reflexes produce similar ipsilateral and contralateral effects on low-frequency responses so that binaural sound localization abilities are preserved.

The potential for the MOC reflex to affect binaural sound localization is shown by the large latency change it can produce. Changes in OAE latencies were measured to determine the

change in cochlear tuning produced by the MOC reflex (filter theory indicates that broader filters have shorter delays) [15*]. Significant reductions in OAE delays (5% for 0.5–2 kHz) were found, which indicates that MOC activity slightly widens cochlear tuning. The large change in cochlear response latency implied by the measured 0.5 ms change in OAE delay would have a profound effect on binaural localization if it were not balanced, e.g. by the MOC system producing similar changes in both ears.

MOC effects on DPOAEs

One common method for measuring MOC effects is by the change in distortion product OAEs (DPOAEs) at the frequency 2f1-f2 (where f2>f1). MOC activity typically reduces DPOAEs, but sometimes it enhances them. Two recent papers [16*,17*] show how these different effects are produced by interference from the two kinds of OAE sources (distortion and reflection sources [18]). These studies used DPOAE measurements with fine frequency steps to separate the distortion and reflection source components, and found that: (1) MOC stimulation inhibits (i.e. reduces) both components and shifts their phase, with the reflection component affected more than the distortion component, (2) DPOAE dips are produced by phase cancellation of the two components, and MOC-induced phase changes move the cancellation frequencies upward, (3) reduction of cancellations, particularly at dips, produces MOC-induced DPOAE enhancements, and (4) consistent DPOAE reductions (~2 dB) are found if measurements are made at fine-structure peaks [16*,17*].

Recent measurements show that larger MOC changes are found in the DPOAEs at f2-f1 than at 2f1-f2 [19*]. Unfortunately, f2-f1 DPOAEs are too small to measure in most human subjects. The relative sizes of f2-f1 and 2f1-f2 DPOAEs are controlled by the OHC-stereocilia operating point which can be varied using a low-frequency "bias" tone. The MOC effect on f2-f1 DPOAEs was found to interact with the bias-tone effect in a way that indicates that MOC action slightly changes the operating point of cochlear amplification [20*].

The time course of MOC effects

Two papers studied the effects of prolonged sound stimulation in producing MOC effects. In awake humans, 16 minutes of contralateral noise (interrupted twice for measurements) produced sustained inhibition of transient-evoked OAEs (TEOAEs) with perhaps a small increase in inhibition over the 16 minutes [21*]. In anesthetized guinea pigs, the MOC inhibition of ipsilateral cochlear responses (compound action potentials, DPOAEs, and round-window noise) began at the onset of the elicitor and showed an increase over 2–3 minutes that was partially sustained during the 15 minute contralateral noise [22*]. The slow increase in MOC inhibition was interpreted as not being due to the MOC slow effect [23,24], which decreases after a few minutes of stimulation. The slow change might be due to an increase in MOC firing during the sustained noise [22*]. After termination of the noise, the human data showed a significant enhancement of TEOAE amplitude [21*]. After-stimulation enhancement was also seen in experiments demonstrating the slow effect [23,24], but these enhancements may have an entirely different origin than the slow effect [25].

A problem in OAE tests for MOC effects is that the sound that evokes the OAE may also evoke MOC activity [26]. One way of avoiding this confound is by studying MOC effects on spontaneous OAEs (SOAEs). MOC effects elicited by contralateral sound on SOAEs showed onset and offset time constants in the few hundred ms range (similar to those seen in SFOAEs [27]) as well as slower changes and an SOAE enhancement after the sound burst. [28*]

MOC effects on Speech in Noise

It is hypothesized that MOC inhibition enhances the ability to discriminate signals in noise [29]. One way to gain understanding of this is by making a cochlear model that includes MOC effects (i.e. lower cochlear-amplifier gain) and by determining how MOC effects change perceptual abilities. Two recent studies did this using cochlear models as inputs to computerized speech recognition systems [30*,31*]. Although the model systems differed significantly, with no MOC activation both showed that speech in silence was recognized well, but speech in background noise was not. The addition of MOC effects improved speech recognition errors produced by real people shows an efferent enhancement of performance [30*]. Interestingly, optimum performance was obtained when the amount of efferent activity was proportional to the noise level [31*]. Such models show how MOC inhibition may improve speech in noise detection in humans [32].

MOC activity may enhance speech perception even when there is no background noise. Following identification tests of speech that was partially time reversed, subjects with the best identification scores had larger MOC inhibition of CEOAEs than subjects with the worst scores [33*]. The difference was strongest in the right ear. MOC cochlear effects may have directly aided performance, or alternately, both MOC activation and speech performance may be correlated (e.g. from left-hemisphere mechanisms) without MOC activity actually aiding performance.

MOC effects in psychophysics

The psychophysical phenomena called the "temporal effect" or "overshoot" has been suggested to be due to MOC inhibition. Overshoot is the phenomena that a brief sound has a lower threshold when presented 100 ms or more after the start of a noise burst compared to its threshold near the start of the noise burst. It is hypothesized that (1) the noise burst elicits MOC activity that builds up slowly and eventually decreases cochlear-amplifier gain, and (2) the decrease in cochlear-amplifier gain reduces the response to the low-level noise more than it reduces the response to the brief, high-level tone. If this is true, MOC activity during overshoot should decrease OAEs, and two recent studies looked for such a change. One study [34*] did not find an OAE change that corresponded to overshoot, while another did [35**]. The different results appear attributable to the different methods used. Overall, the results indicate that overshoot is due, at least in part, to MOC activity.

The amount and frequency specificity of MOC activity must vary continually in response to the recent history of sound stimulation and subject attention. Thus, cochlear amplifier gain can be expected to vary during psychophysical tests. Recent papers provide evidence for this [36,37,38].

Attention, learning and plasticity

A recent study found a reduction in MOC reflex activity (compared to passive, no-task listening) when a subject performed a task requiring attention to a sound [39*]. Tasks have been reported to produce both increases and decreases in MOC activity, but clear rules for which occurs have not emerged. An attractive hypothesis is that MOC activity increases in tasks when the MOC activity confers a benefit, but it decreases in tasks when it confers no benefit. Data are needed that test this hypothesis.

Over the last few years evidence has built up for a role of efferents in learning and plasticity. [40]. New evidence for a role in learning comes from the finding that MOC effects on OAEs were significantly lower at some frequencies in children with auditory listening problems compared to normal children [41]. A role of the descending auditory system in neural

was greatly reduced after selective destruction of cortical cells that project to the inferior colliculus. Whether this plasticity involves MOC neurons is not known. It is noteworthy, however, that MOC neurons exhibit immunofluorescence that indicates they contain enzymes that are involved in producing neural plasticity [43]. Furthermore, in frogs, nitric oxide (which helps produce neural plasticity) may slowly enhance efferent synaptic effects on hair cells, which suggests that nitric oxide might be involved in producing the MOC slow effect [44].

MOC tests in various populations

MOC tests, done by eliciting MOC activity with contralateral noise and measuring changes with OAEs, have been used in a variety of circumstances. Two papers indicate that OAE amplitudes and/or MOC effects on OAEs decrease in older subjects [45,46]. One paper indicates that smoking lowers TEOAEs and MOC effects on TEOAEs [47], while another found MOC effects on TEOAEs went down with age in smokers, but not in non-smokers [48]. MOC effects were reported to be generally lower in subjects with tinnitus than in normals [49,50]. Finally, in children with type-I diabetes mellitus, MOC inhibition of TEOAEs was lower than normal, which may be an early manifestation of diabetic neuropathy [51]. These results should be interpreted cautiously because the methods were often weak [2], e.g. the OAEs had low signal-to-noise ratios (only 3 dB), or OAE differences were not normalized thereby biasing the results.

LOC function in binaural hearing

LOC efferents have been suggested to have a role in balancing the outputs of the right and left cochleae to achieve optimum binaural hearing [1,52]. However, following manipulations that lowered the output of one cochlea, the output of the other cochlea remained constant, which argues against the hypothesis [53*].

Manipulations of cochlear neuroreceptors

MOC inhibition involves multiple steps that have been targets for manipulation and study. The efferent neurotransmitter, acetycholine (ACh), has receptors (AChRs) in the cochlea that are composed of $\alpha 9$ and $\alpha 10$ subunits [54]. Acetylcholine released by MOC terminals acts on $\alpha 9\alpha 10$ AChRs that allow entry of Ca²⁺ ions into the OHC. These Ca²⁺ ions activate nearby calcium-activated potassium channels, called SK2 channels, that allow potassium to exit and hyperpolarize the OHC. A study using animals with a mutation in α 9AChRs that increased AChR sensitivity found that this increased protection from acoustic trauma [55**]. This result provides a strong confirmation of the role of MOC synapses in trauma protection and the potential value of MOC reflex testing for predicting which subjects are susceptible to acoustic trauma. A study using SK2-null mice confirmed that electrically driven MOC effects are lost without functional SK2 channels, and also found downregulation of OHC ryanodine receptors that normally increase the SK2 activation [56]. This study also found, in double-null mice lacking both α 10AChR and SK2 genes, that there was a down regulation of α 9nAChR expression [56]. These results indicate that there are interlocking developmental signals such that SK2 channels are necessary for long-term survival of olivocochlear fibers and synapses. Another study showed a range of developmental anomalies in a9AChR knockout animals [57].

Mice with the α 9AChR gene deleted have no MOC cochlear inhibition [58] and provide a way of assessing MOC function. In signal-in-noise sound-localization tests, α 9AChR-knockout mice had surprisingly normal behavior, and the authors suggested that central compensation via MOC collateral branches to the cochlear nucleus was responsible [59].

Page 6

However, a recent study of α9AChR-knockout mice found no obvious changes in the central morphology of OC neurons [60*]. Perhaps, as later suggested [61], MOC activity normally aids sound localization in noise, but knockouts showed no deficit because long training allowed them to develop alternate listening strategies. Whether such compensation involves MOC collaterals to the cochlear nucleus is unknown, but recent studies support older anatomical work indicating that MOC collaterals excite certain classes of cochlear-nucleus neurons [62]. Furthermore, animals that were unilaterally deafened indicate that MOC collaterals provide a slow excitation to cochlear-nucleus neurons [63*].

Efferent feedback that releases ACh on hair cell organs is phylogenetically old. New data indicate that the ACh receptors in mammals ($\alpha 9\alpha 10$ AChRs) evolved recently, presumably to control the phylogenetically-new, prestin-based cochlear amplification [64]. Two papers point out that AChRs are a possible pharmacotherapeutic target in conditions such as noise-induced hearing loss, tinnitus and auditory processing disorders [65,66].

GABA

A variety of data indicate that gamma-aminobutyric acid (GABA) is a second neurotransmitter released at LOC and MOC synapses, at least in some species. In α9AChRknockout animals, there was an unexpected increased expression of genes encoding GABA receptor subunits and the GABA synthetic enzyme [67]. These data suggest a developmental association in the cochlea between nicotinic cholinergic and GABAergic systems. In animals with a GABA receptor subunit (GABAb1) knocked out, MOC function assessed by DPOAE inhibition was normal, but these animals showed *increased* resistance to permanent (but not temporary) acoustic trauma [68*]. Immunostaining indicates that GABAb1 receptors are located in type II afferents that synapse on OHCs, which indicates a role for type II synapses in acoustic trauma and perhaps in cochlear amplification [68*].

MOC fibers and development

During mammalian development, MOC fibers briefly form synapses on IHCs (with $\alpha 9\alpha 10$ ACh receptors) before detaching and continuing on to innervate OHCs [69]. The role of this transient MOC innervation of IHCs is not clear. $\alpha 10$ ACh receptors on IHCs normally disappear with the disappearance of MOC innervation. Genetically-manipulated mice that have $\alpha 10$ AChRs in adulthood do not show ACh currents, presumably because IHC SK2 channels are also down-regulated [70]. Experiments in $\alpha 10$ AChR-knockout animals show that the development of basic IHC properties does not require the $\alpha 10$ AChR subunit [71]. Another study showed that while hearing was severely impaired in mice lacking the Ca²⁺ channel subunit CaVbeta2, the transient MOC innervation of IHCs still occurs during development [72].

CONCLUSION

Recent work provides a new understanding of MOC reflex tuning during passive listening but more work is needed to provide an understanding of MOC tuning during active listening. The interpretation of OAE changes in terms of MOC effects is now well understood for all OAE types. The main challenge in applying OAE methods to clinically relevant questions is the need for good methodology, e.g. the signal-to-noise ratio required for measuring MOC effects is much higher than what is required for simply measuring OAEs [2]. Measuring MOC effects and relating them to learning and disabilities seems particularly ripe for exciting new work. Finally, continued use of animals with new molecular knock-outs can be expected to provide important insights into cochlear development and how efferents produce their effects.

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Figure 1.

Medial olivocochlear (MOC) inhibition increases as the bandwidth of a constant-level elicitor increases, showing that sound excitations over almost the whole range of hearing are integrated in activating the efferents that affect one cochlear frequency region. For narrow-band elicitors (0.5 octaves), ipsilateral noise was approximately twice as effective as contralateral noise, but for wide-band elicitors (>6 octaves), ipsilateral and contralateral elicitors were equally effective. Patterned after the data Lilaonitkul and Guinan [14] for probe frequencies near 1 kHz, and 60 dB SPL elicitors centered on the probe frequency.