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Assessing the Photoreceptor Mosaic Over Drusen Using Adaptive Optics and SD-OCT

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Abstract

Drusen are extracellular deposits that accumulate between the retinal pigment epithelium and Bruch's membrane. They are one of the earliest clinical manifestations of age-related macular degeneration and it is thought that they disrupt the overlying photoreceptors, leading to subsequent vision loss. The purpose of this study was to illustrate how spectral domain optical coherence tomography and adaptive optics fundus imaging can be used to quantitatively analyze the integrity of the overlying photoreceptors in a single subject with macular drusen. This imaging approach and the image analysis metrics introduced may serve as the foundation for valuable imaging-based biomarkers for detecting the earliest stages of disease, tracking progression, and monitoring treatment response.

INTRODUCTION

Spectral domain optical coherence tomography (SD-OCT) enables non-invasive, highresolution visualization of the normal and pathological retina.¹ This imaging modality has been used extensively to characterize drusen structure in age-related macular degeneration (AMD).²⁻⁵ It has been shown histologically that photoreceptors overlying and distal to drusen undergo degeneration.⁶ Using SD-OCT, photoreceptor layer thinning over drusen has recently been reported and proposed to reflect photoreceptor degeneration.⁷ More direct visualization of the photoreceptor mosaic is afforded by the use of adaptive optics.⁸ This technique has been used to image the cone mosaic surrounding drusen, but no quantitative analysis was undertaken.⁹ We used adaptive optics imaging to directly quantify the integrity of the cone photoreceptor mosaic in a patient with drusen, and used SD-OCT to assess the thickness of the inner segment/outer segment (IS/OS) layers compared with previous normative data.¹⁰

CASE REPORT

A 45-year-old asymptomatic woman was found to have retinal features consistent with basal laminar drusen on clinical examination. Blood pressure, urine dipstick, and renal function were all normal. Visual acuity without correction was 6/5 bilaterally. Fundus fluorescein

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angiography revealed multiple hyper-fluorescent soft and hard drusen scattered throughout the fundus (more numerous and extensive than seen ophthalmoscopically), with a greater concentration temporal to the macula (Fig. 1). Macular thickness and retinal nerve fiber layer thickness measured on the Cirrus HD-OCT (Carl Zeiss Meditec, Dublin, CA) was within the system's normal limits. High-resolution images of the macula were obtained using a Bioptigen SD-OCT (Bioptigen, Durham, NC) equipped with a 878-nm (186-nm bandwidth) light source.¹¹ A high-density 6×6 -mm volume scan (1,000 A-scans/B-scan, 150 B-scans) from the patient's left eye revealed a small, discrete drusen at 1.75° temporal to the fovea. At this location, images of the cone photoreceptor mosaic were obtained using a high-speed adaptive optics fundus camera.^{10,12,13} Individual frames were registered and averaged to increase the signal-to-noise ratio for the final image, as previously described.¹⁴ Figure 2 illustrates the co-registered fundus fluorescein angiography and adaptive optics images over the drusen, along with the corresponding SD-OCT image, performed using i2k Align Retina software (DualAlign, LLC, Clifton Park, NY) and Adobe Photoshop (Adobe Systems Inc., San Jose, CA).

Individual cones were identified using automated software,¹⁵ and cone density was subsequently analyzed using previously described methods.¹⁴ Although the contrast of the cone mosaic appears reduced over the drusen, cone density at this location (39,133 cones/mm²) was not significantly decreased compared with previously published normative data from our group (mean ± 2 standard deviation [SD] = 41,974 $\pm 6,972$ cones/mm²).¹³ We used a previously described Voronoi analysis¹⁶ to examine mosaic regularity (Fig. 3), comparing the geometry of the cones within 50 µm of the drusen and cones within 50-µm wide annular rings moving away from the drusen (ie, cones between 50 and 100 µm, between 100 and 150 µm, and so on). For the cones within 50 µm of the drusen, 45% had 6-sided Voronoi domains. For each of the other 50-µm annular rings, between 32% and 53% of the cones had 6-sided Voronoi domains (mean = 46%). In addition, the mean number of sides to the Voronoi domains for the cones within each 50-µm annular ring compared with that of the cones within 50 µm of the drusen the mosaic immediately overlying the drusen is regularly arranged, consistent with no significant cone loss.

Longitudinal reflectivity profile analysis of the SD-OCT images (Fig. 4) revealed that the inner-segment layer (distance between the external limiting membrane and IS/OS layer) was of normal thickness both directly above the druse and immediately adjacent to it, compared with 167 previously published normals.¹⁰ The outer-segment layer (distance between IS/OS and retinal pigment epithelium layers) was normal (30 μ m) immediately adjacent to the druse, but significantly thinner (18.2 μ m, normal mean \pm 2 SD is 32 \pm 1.11 μ m) directly above the druse. Although outer-segment shortening has been reported using fundus reflectometry techniques,¹⁷ the apparent thinning of the outer segment we observed on SD-OCT could be due to a shortening of the outer segment or to a splaying of the outer segment that is secondary to the volume occupied by the druse itself.

DISCUSSION

AMD is a progressive degenerative disorder leading to gradual deterioration of central vision over many years and represents the most common cause of blindness in the developed world. One of the early clinical features in the progression of AMD is the appearance of drusen. Patients with early stages of AMD often have no symptoms and the ability to predict the rate of progression is currently markedly limited. Accurate, high-resolution biomarkers are needed to help in the identification of individuals in the earliest stages of macular degeneration and also those who are likely to progress rapidly and may benefit most from more intensive observation and management. The development of imaging-based

biomarkers to detect AMD at its earliest stages may also have an important role in the assessment of early preventative interventions that are likely to become available in the near future. By monitoring early drusen over time using imaging tools such as SD-OCT and adaptive optics, their progression both in terms of size and their direct effect on the overlying retinal layers and photoreceptor mosaic can be quantified. In our case, we imaged an undisrupted photoreceptor mosaic overlying the early druse with normal regularity and cone density, giving us valuable information about the status of the photoreceptors at an early stage.

When trying to detect a druse, OCT or polarization imaging¹⁸ may be superior to adaptive optics imaging. However, when trying to directly examine the integrity of the photoreceptor mosaic at the single cell level, then adaptive optics imaging is needed. Accepting that these imaging modalities are complementary, one can shift focus to the challenge of developing image processing tools that enable easy and accurate integration of data from multiple imaging modalities. An alternate approach is to physically combine the two imaging modalities. Although not available commercially, several have developed adaptive optics-OCT systems capable of imaging the cone photoreceptor mosaic.¹⁹⁻²² Recently, one of these devices was used to evaluate the integrity of the cone mosaic at various depths throughout the length of the cone in a case where there was disruption of the cone mosaic.²³ In addition, high-speed OCT systems without adaptive optics have been shown to be able to resolve the peripheral cone mosaic.²⁴ The fact that the mosaic in our patient was visible across the entire surface of the druse shows that, despite morphological disruption on OCT (secondary to either outer-segment shortening or splaying), the cones were still present. Thus, in our case adaptive optics was used to interpret the SD-OCT images. There may be cases where SD-OCT can be used to interpret adaptive optics images or where polarization images could be used to interpret adaptive optics or SD-OCT images.

Obtaining functional data to correlate with the high-resolution structural information that can now be obtained represents an important area of research, including the use of microperimetry²⁵ to determine whether cone function has been altered. Microperimetry techniques that incorporate adaptive optics may be required to spatially constrain the stimulus to a specific subset of cones.^{26,27} In addition, it would be of interest to examine adaptive optics autofluorescence images in such patients to examine the integrity of the retinal pigment epithelium mosaic, especially in light of the fact that it has been shown that drusen can be associated with retinal pigment epithelium damage even peripheral to the drusen.²⁸ The rapid continued advances in imaging and image analysis, together with the potential to correlate this with novel functional techniques, is likely to have an important role both in patient selection and in the evaluation of current and future treatments for AMD.

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Figure 1.

Fundus fluorescein angiography montage of the patient's left eye. Individual images were montaged using i2k Align Retina software (DualAlign, LLC, Clifton Park, NY). The white box indicates the area of the cone mosaic displayed in Figure 2 and the dashed line indicates the location of spectral domain optical coherence tomography scan shown in Figure 2.



Figure 2.

Multimodal imaging of the retina. (A) Fundus fluorescein angiography and (B) adaptive optics images of the same patch of retina. (C) High-resolution spectral domain optical coherence tomography (SD-OCT) images using a broadband illumination with the Bioptigen SD-OCT system (Bioptigen, Durham, NC) showing retinal pigment epithelium excrescences with underlying moderately reflective material consistent with drusen. Image was taken at the location of the horizontal line (A). Thin vertical arrows (C) represent the boundary of the retinal area imaged (A and B). The blood vessel temporal to the drusen (A and B) can be seen in the SD-OCT image (C) as a vertical shadow above the large arrow, especially visible between the external limiting membrane and retinal pigment epithelium layers.



Figure 3.

Analysis of mosaic regularity analysis. Shown are the Voronoi boundaries associated with each cone identified using the automated program of Li and Roorda.¹⁵ Green color indicates Voronoi domains with 6 sides, reflecting hexagonal/triangular packing of the cone mosaic. Other colors indicate domains with greater or fewer than 6 sides and qualitative disruption can be seen overlying the larger vertical blood vessel where the cone mosaic was not completely resolved. White circles represent the boundaries of the 50-µm wide annular rings used to compare the regularity of the mosaic directly over the drusen with that elsewhere in the image.



Figure 4.

Disruption of the inner segment/outer segment (IS/OS) layers. On the left is a segment of the spectral domain optical coherence tomography (SD-OCT) image centered on the 65- μ m wide druse. Longitudinal reflectivity profiles have been plotted for the area of retina between the arrowheads. The middle plot shows normal-appearing retinal layers just temporal to the druse. In the SD-OCT images, the gray scale represents signal amplitude: low reflecting layers indicate nuclear layers, whereas high reflectivity typically comes from synaptic layers in the healthy retina. Assignment of layers is based on literature consensus.²⁹⁻³¹ The right plot shows significant thinning of the outer segment layer (distance between IS/OS and the first retinal pigment epithelium [RPE1] layers). The distance between RPE1 and Bruch's membrane (BM) is presumably occupied by the druse. The IS/OS layer itself appeared attenuated or "pinched," being 30% thinner (full-width half maximum) directly above the druse compared to immediately adjacent to the druse. ILM = inner limiting membrane; OPL = outer plexiform layer; ELM = external limiting membrane; IPL = inner plexiform layer; ONL = outer nuclear layer; a. u. = arbitrary units.