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## **Targeted modulation of reactive oxygen species in the vascular endothelium**

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## **Abstract**

Endothelial cells lining vascular luminal surface represent an important site of signaling and injurious effects of reactive oxygen species (ROS) produced by other cells and endothelium itself in ischemia, inflammation and other pathological conditions. Targeted delivery of ROS modulating enzymes conjugated with antibodies to endothelial surface molecules (vascular immunotargeting) provides site-specific interventions in the endothelial ROS, unattainable by other formulations including PEG-modified enzymes. Targeting of ROS generating enzymes (e.g., glucose oxidase) provides ROS- and site-specific models of endothelial oxidative stress, whereas targeting of antioxidant enzymes SOD and catalase offers site-specific quenching of superoxide anion or/and  $H_2O_2$ . These targeted antioxidant interventions help to clarify specific role of endothelial ROS in vascular and pulmonary pathologies and provide basis for design of targeted therapeutics for treatment of these pathologies. In particular, antibody/catalase conjugates alleviate acute lung ischemia/reperfusion injury, whereas antibody/SOD conjugates inhibit ROS-mediated vasoconstriction and inflammatory endothelial signaling. Encapsulation in protease-resistant, ROS-permeable carriers targeted to endothelium prolongs protective effects of antioxidant enzymes, further diversifying the means for targeted modulation of endothelial ROS.

## **Keywords**

endothelial cells; drug delivery; vascular immunotargeting; oxidative stress; antioxidant enzymes

## **Introduction: vascular oxidative stress and antioxidant interventions in the endothelium**

Abnormally high influx of reactive oxygen species (ROS) that exceeds normal cellular antioxidant capacity, collectively termed "oxidative stress", causes many pathological processes including inflammation, cellular dysfunction and tissue damage. Endothelial cell monolayer lining the vascular lumen controls vital integral functions (transport between organs, vascular permeability and tone, blood fluidity, host defense, angiogenesis and

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carcinogenesis) and represents arguably one of the most sensitive and important targets for oxidative stress [1, 2]. Excessive ROS cause pathological activation of endothelium including exposure of cell adhesion molecules (such as ICAM-1 and VCAM-1) and inhibitors of fibrinolysis [3-5], loss of transmembrane glycoprotein thrombomodulin that normally exerts anti-thrombotic and anti-inflammatory functions [6], disruption of the endothelial barrier and, in severe cases, cell death. These pathological changes lead to and propagate thrombosis, edema, inflammation, ischemia, abnormal vascular growth and functions. Further, ROS superoxide anion quenches NO· produced by endothelium, thereby aggravating vasoconstriction and thrombosis (Fig.1). Endothelial disorders and injury caused by ROS are implicated in ischemia, inflammation, stroke, acute lung injury, myocardial infarction, atherosclerosis, hypertension and diabetes, among other maladies [7, 8].

Therefore, design of effective and safe means for specific interventions in endothelial ROS, produced by abnormally activated endothelial cells or released by leukocytes, represents an important biomedical problem [9]. In acute settings, such interventions can be achieved by administration of antioxidant therapeutics. In theory, enzymatic antioxidants can provide highly specific and effective detoxification of endothelial ROS, on the condition that the formulations are properly delivered to the target cells. This specific aspect of vascular drug delivery and targeting attracts a considerable attention for several decades and has been reviewed in this journal ten years ago [10]. This article offers an updated analysis of the problem, focused on recent achievements in targeted delivery of antioxidant enzymes to endothelial cells.

## **Reactive oxygen species (ROS), antioxidant defense and spatiotemporal requirements for antioxidant interventions**

Resident and migrant cells in the vasculature including macrophages, white blood cells, smooth muscle cells and endothelial cells produce the ROS superoxide anion O<sub>2</sub><sup>-</sup> from oxygen using enzymes including mitochondrial respiratory chain [11], xanthine oxidase [8] and NADPH oxidase [12]. O<sub>2</sub><sup>-</sup> forms a strong oxidant, peroxinitrate (ONOO<sup>−</sup>), in a fast reaction with NO. , thereby inactivating this vasodilatory and anti-thrombotic mediator, or spontaneously transforms into  $H_2O_2$ . By accelerating the latter transformation, a family of enzymes superoxide dismutase (SOD) including mitochondrial MnSOD (86-88 kD), cytosolic CuZnSOD (32 kD) and extracellular SOD (135 kD) preserves NO. and blocks ONOO<sup> $-$ </sup> formation [13]. Freely diffusible  $H_2O_2$  is more stable than  $O_2^-$ , yet, in reactions with transition metals, myeloperoxidase, superoxide and NO it forms strong oxidants including ·OH radical and HOCl [14]. A highly potent enzyme catalase consisting of four identical 60 kD subunits localized predominantly in the cytosol and specific vacuoles (peroxisomes) decomposes  $H_2O_2$  into water. However, when ROS detoxification and repair of oxidized biomolecules are insufficient, cellular and tissue abnormality ensues, leading to pathology (Fig.2).

Direct effects of ROS, especially labile and poorly diffusible O**<sup>2</sup>** .− are compartmentalized within nanometers of generation site. Therefore, interventions in ROS mediated processes should be precisely controlled spatiotemporally, ideally at sub-cellular level. For example, unguided  $O_2$ <sup>--</sup> dismutation may be inefficient or even aggravate the injury if local  $H_2O_2$ reduction is not sufficient [15, 16]. These considerations emphasize the need for site-specific delivery of antioxidants. For example, treatment of oxidative stress caused by excessive ROS flux in mitochondria may be optimally served by mitochondrial interventions [17]. Membrane-permeable and mitochondria-directed SOD quenchers and mimetic consuming reducing cofactors to catalyze  $O_2$ <sup> $-$ </sup> dismutation show promising protective effects in cell culture and animal models [18, 19]. Mutant SOD2/3 chimera binding to cell surface via

negatively charged glycocalyx and cell transfection by SOD confer protective antioxidant and anti-inflammatory effects [20-24].

However, these antioxidant interventions including delivery using membrane permeating peptides [25], provide no endothelial targeting and act in diverse tissue and cellular compartments [26]. Such spatially promiscuous effects may be beneficial in treatment generalized forms of oxidative stress and inflammation, such as sepsis and radiation injury, but insufficiently targeted for site-specific endothelial interventions. As result, our understanding of where antioxidant interventions are required, which specific ROS need to be decomposed and means to achieve this goal are acutely incomplete, in part due to insufficiently effective and precise targeted delivery of antioxidants [27, 28]. Further, translation of many of these antioxidant delivery means into therapeutic domain is hindered by concerns of practicality, efficacy, specificity, safety and spatiotemporal control of the interventions. For example, the feasibility, expedience, and safety of gene therapy are suboptimal for use in most acute settings, whereas practicality of enzyme infusion is similarly limited for management of chronic oxidative stress. This article is focused on endothelial delivery of antioxidant enzymes for treatment of acute oxidative stress in the vasculature.

#### **Endothelial delivery of antioxidants: requirements and challenges.**

Prolonged and prophylactic administration of non-enzymatic antioxidants including ROS scavengers (e.g., vitamin E), reducing agents (e.g., N-acetylcysteine) and antioxidant inducers (e.g., curcumin), may confer some extent of alleviation of subtle and modest forms of chronic oxidative stress, but provides no tangible benefits in acute conditions (Table 1) [29]. Antioxidant enzymes can potentially afford more potent and specific effects. For example, intratracheal delivery of catalase and SOD and their transgenic expression alleviated oxidative stress occurring in the airways of animals [30-35]. Unfortunately, the adequate delivery of enzymes to the endothelium, that is not readily accessible from the airways, has not yet being achieved [36].

Endothelial delivery of antioxidant enzymes via the vascular route seems more suitable for this goal. Of note, the pulmonary vasculature represents about 20-25% of the total endothelial surface in the body, receives the entire venous blood ejected by the heart (i.e., 50% of the total cardiac blood output, whereas all other organs including pulmonary bronchial circulation share arterial blood) and thus represent the privileged vascular target [37, 38]. Therefore, compounds with high affinity to endothelium injected in the bloodstream quickly accumulate in the lungs [39]. Local infusion of such compounds including antibodies and antibody fragments directed to endothelial antigens and natural ligands of endothelial receptors, in a conduit artery greatly enhances uptake in the downstream vasculature of an organ of interest, whereas pulmonary vasculature takes up the lion share of the leftovers entering the systemic circulation [40-42].

The liver and kidney eliminate naked catalase and SOD within minutes after IV injection [10]. Conjugation with polyethylene glycol, PEG [43], encapsulation in PEG-liposomes [44] or PEG-coated polymeric carriers [45-47], conjugation with PEG-based pluronics [48, 49] and other modifications such as conjugation with compounds favoring binding to plasma albumin prolong the circulation time of catalase and SOD, thereby enhancing their potency in some forms of systemic oxidative stress in animals [50-55]. Due to enhanced aqueous solubility affording high doses in cell culture medium, PEG-enzymes enter intracellular vesicles via non-specific uptake of fluid phase after prolonged incubations in cell cultures [56]. However, efficacy of this pathway for intracellular delivery is limited *in vivo* due to lack of endothelial affinity [10, 38]. In fact, inhibition of interactions with cells provided by PEG corona is one of the key features of this stealth technology. Tracing of radiolabeled

PEG-catalase and PEG-SOD showed no better uptake by endothelial cells in culture and delivery to endothelium in vivo than achieved by naked enzymes [57].

Some SOD and catalase formulations bind to and enter cells due to hydrophobic or electrostatic interactions (e.g., enzymes coupled to cationic membrane-permeating peptides such as TAT) [52, 53, 58-60]. Further, constructs fusing cytosolic CuZnSOD with glycocalyx-binding peptides showed promising protective effects in animal models of inflammation [22]. However, endothelial targeting of these derivatives has yet to be proven in animal studies. They do not accumulate in the pulmonary vasculature and provide rather modest protective effects in animal models of acute endothelial oxidative stress [10, 38]. Using carriers with affinity to endothelial surface molecules enables more effective and specific targeting of antioxidant enzymes [2, 9].

#### **Vascular immunotargeting to endothelial surface molecules.**

In order to achieve specific targeting of antioxidant enzymes to endothelial cells, we and other labs devised a "vascular immunotargeting" strategy that employs conjugation of cargoes with antibodies (or their fragments) that bind to specific endothelial surface epitopes [2, 61-68]. Epitopes tested for this goal include constitutively expressed angiotensinconverting enzyme, ACE [39, 61, 69], aminopeptidase P [70], pan-endothelial Platelet-Endothelial Cell Adhesion Molecule-1 (PECAM) [2] and transferrin receptor [71] or Intercellular Adhesion Molecule-1 (ICAM-1) [72] (Table 2). ICAM-1 is constitutively exposed on endothelium in the vasculature and further up-regulated by inflammatory agents, abnormal blood flow and oxidative stress [73, 74]. Molecules exposed exclusively on activated endothelium (e.g., E- and P-selectins and VCAM-1) represent attractive targets for delivery of drugs and imaging probes to pathological sites in the vasculature [75-79].

Binding of antibodies and carriers carrying these antibodies may activate or inhibit target molecules, for example via their cross-linking, blocking or induced disappearance from the plasmalemma (shedding or internalization) [80-82]. This may lead to either beneficial or adverse side effects in the context of the therapeutic intervention. For example, antibodies to the constitutive endothelial protein thrombomodulin (TM) accumulate in the pulmonary vasculature [68, 83], but cannot be used for therapies, since TM inhibition leads to thrombosis and inflammation [84]. However, targeting of H**2**O**2**-generating enzyme glucose oxidase conjugated with anti-TM (anti-TM/GOX) provides useful animal models of acute oxidative stress in the pulmonary vasculature described in the next section [6, 85-87].

Inhibition of ACE leading to reduction of the level of Ang II, a potent vasoconstricting, proinflammatory and pro-oxidant mediator activating ROS production in endothelium, may provide beneficial effects in the context of treatment conditions associated with hypertension, ischemia, inflammation and oxidative stress [88]. On the other hand, inhibition of bradykinin metabolizing enzymes ACE and aminopeptidase P leads to elevated levels of bradykinin, which may cause hypotension, enhanced vascular permeability and edema [89, 90]. Thus, ACE inhibitory antibodies and ACE-targeted conjugates can be important ways to modulate ACE activity in lab animals and pilot human studies [91]. Cell adhesion molecules ICAM and PECAM are transmembrane glycoproteins involved in WBC adhesion and transmigration, cellular recognition and signaling [92, 93]. Pulmonary accumulation of WBC is generally viewed as a pro-inflammatory process implicated in pathogenesis of ALI, hyperoxia, ischemia and other diseases [94-96]. Cell adhesion blockade inhibits WBC transmigration and inflammation [97, 98]. Thus, drug targeting to ICAM and PECAM may suppress inflammation. Studies in diverse animal species revealed no harmful effects of drug targeting directed to ICAM-1 [99-101] and PECAM-1 [38, 81, 85, 102-106].

Endothelium constitutively stably expresses approximately  $1-3\times10^5$  copies of ACE and ICAM-1 and  $0.5$ -1.5 $\times$ 10<sup>6</sup> copies of PECAM-1, respectively, on the surface of one cell [39, 99, 102]. These endothelial determinants are among the most extensively studied as anchors for vascular immunotargeting and drug delivery [9, 38, 107, 108]. Endothelial cells internalize ACE antibodies, likely via the clathrin-related endocytosis [82], and multivalent conjugates carrying multiple copies of ICAM and PECAM antibodies [42, 102, 109], via an unusual endocytic pathway, CAM-mediated endocytosis distinct from phagocytosis, caveolar and clathrin endocytosis and remotely resembling macropinocytosis, in some aspects [110]. Of note, endothelial cells internalize relatively large conjugates and nanocarriers directed to ICAM and PECAM, with maximal dimension of several microns [111].

Enzymes, genetic materials, nanocarriers, liposomes and other cargoes and carriers conjugated or fused with antibodies to ACE, ICAM and PECAM (anti-ACE, anti-ICAM and anti-PECAM) bind to endothelial cells in cultures and, more importantly, in the vasculature in intact animals [38, 39, 99, 104, 112]. As result, drugs, enzymes, DNA, viruses, liposomes and diverse nanocarriers conjugated with anti-ACE, anti-ICAM and anti-PECAM accumulate in the lungs and other highly vascularized organs after intravascular injection**,** providing drug delivery to the endothelium [38, 81, 85, 102-106, 112-114]. Most studies of vascular immunotargeting of enzymes controlling ROS level in the endothelial cells employed antibodies to ACE, ICAM and PECAM [46, 108].

#### **Vascular immunotargeting of ROS generating enzymes: modeling of**

**endothelial oxidative stress.—**Studies of endothelial oxidative stress and testing of antioxidant interventions require well controlled models of elevated ROS influx in this cell type. Treatment of cells in culture with ROS or ROS generating enzymes offers a simple and straightforward approach. For example, exposure to glucose oxidase/glucose system generating  $H_2O_2$  or to xanthine oxidase/xanthine system generating both superoxide and  $H<sub>2</sub>O<sub>2</sub>$  can be employed in model studies [86, 115]. Further, abnormally high and low levels of oxygen and chemicals including quinones and paraquat cause intracellular ROS production in endothelial mitochondria [6]. Inflammatory agonists including Ang II, VEGF and cytokines, as well as abrupt changes in perfusion rate, cause endothelial ROS production via enzymatic systems including transmembrane NADPH oxidase [1, 116].

Of course, these agents cause very complex changes in animal studies, not limited to ROS influx in endothelial cells. Vascular immunotargeting of ROS generating enzymes helps to achieve this specific effect, useful for modeling and delineating the role of endothelial oxidative stress and testing means for its specific treatment. Thus, glucose oxidase (GOX) conjugated with anti-ACE, anti-PECAM and anti-TM binds to and enters endothelial cells, causing acute oxidative stress [87, 117, 118]. Further, these GOX conjugates accumulate in the pulmonary endothelium after intravenous injection and cause acute vascular oxidative stress manifested by dose-dependent pulmonary edema, thrombosis, inflammation, accumulation of oxidized molecules and, in most severe cases, mortality [6, 86, 115, 118]. Specific manifestations of vascular oxidative stress in these animal models vary depending on endothelial surface molecule or even epitope selected for GOX targeting. For example, anti-TM/GOX causes more severe, heavily thrombotic pulmonary injury than anti-PECAM/ GOX, likely due to thrombomodulin inhibition unleashing thrombin [87]. Anti-TM/GOX conjugates with higher avidity to endothelium provide more potent injury, whereas hyperoxia further augment oxidative stress caused by anti-TM/GOX by providing enhanced supply of the rate-limiting GOX substrate, oxygen [6]. Therefore, it is possible to finetune the extent and mechanism of acute vascular oxidative stress in models using antibody/GOX conjugates, by selecting optimal endothelial epitopes, conjugate avidity, dose and oxygen supply. Of interest, a model of acute pulmonary oxidative stress caused by GOX targeting to

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endothelium in the presence of elevated oxygen level imitates clinical settings of acute lung injury in the patients on mechanical ventilation.

These features of endothelial targeting of ROS generating enzymes lend themselves to use for modeling specific endothelial components of acute endothelial oxidative stress in animals, which may have mechanistic value. In theory, this strategy might also prove useful for targeted eradication of certain types of endothelial cells such as tumor endothelium. However, animal models of anti-TM/GOX induced vascular oxidative stress found their primary application in testing protective effects of endothelial targeting of antioxidant enzymes, catalase and SOD.

**Endothelial delivery and protective effects of antibody conjugated catalase**

**and SOD.—**SOD and catalase have been conjugated with anti-ACE [69], anti-ICAM [72] and anti-PECAM [119] using diverse cross-linking chemistries including streptavidin-biotin [102] and SATA-SMCC [120]. These supramolecular conjugates (which will be called hereafter collectively Ab/SOD or Ab/catalase, unless specified otherwise), but not control IgG/SOD or IgG/catalase conjugates as well as PEG-modified enzymes, specifically bound to and entered endothelial cells, but not control cell types lacking the target antigen [57, 102, 115]. Accordingly, Ab/catalase and Ab/SOD, but not untargeted formulations protect endothelial cells against toxic effects of  $H_2O_2$  [102, 121] and  $O_2$ <sup>--</sup> [115] flux in the medium, thereby inhibiting ROS-induced cellular necrosis and apoptosis [115] (Fig.3). Further, these conjugates protect from oxidative stress induced by ROS produced intracellularly in endothelial cells treated with paraquat [115].

Radiolabeled Ab/AOE targeted to ACE, ICAM and PECAM, but not IgG/AOE or PEG/ AOE accumulate in the pulmonary vasculature in rats, mice, pigs and dogs after intravenous injection [57, 69, 72]. Confocal fluorescent microscopy revealed that Ab/SOD conjugate accumulates in endothelial intracellular vesicles in the pulmonary vasculature after systemic injection [57]. Optimal size of the Ab/AOE conjugates for highly specific endothelial targeting in vivo is within the range 30-500 nm diameter, which does not cause excessive non-specific retention in the capillaries (and coincides with the optimal size range for endothelial avidity and uptake of conjugates). In particular, anti-PECAM/AOE conjugates with diameter close to 300 nm show optimal efficacy and specificity of targeting to the pulmonary vasculature [120].

Functional activity of the injected conjugates has been initially validated in animal studies involving artificial influx of ROS in the pulmonary vasculature. In the first model, Ab/ catalase conjugates detoxify  $H_2O_2$  infused in lung isolated from rats pre-injected with the conjugate, thus protecting the pulmonary vasculature against oxidative injury and affirming the functionality of delivered antioxidant [85, 102, 106]. In the second, more challenging and physiologically relevant model, Ab/catalase, but not PEG-catalase or IgG/catalase, coinjected in mice with anti-TM/GOX (a conjugate that accumulates and generates  $H_2O_2$  in the pulmonary vasculature) attenuated oxidative stress in lungs, markedly attenuated edema and reduced lethality from 100% to <20% [85]. As expected, Ab/SOD did not protect against anti-TM/GOX induced pulmonary injury, since  $H_2O_2$  is the injurious ROS directly produced by GOX [122].

Anti-PECAM/catalase, but not control formulations injected in donor rats prior to lung harvest, markedly attenuated acute oxidative stress, edema, tissue injury and leukocyte sequestration in lungs transplanted to recipient rats after 18 h of cold ischemia and improved blood oxygenation [106]. This encouraging result has been independently reproduced using anti-ACE/catalase in rat model of lung transplantation in heart beating and non heart beating

donor rats [123, 124]. Furthermore, anti-PECAM/catalase alleviated lung ischemiareperfusion injury in situ in ventilated mice [122] (Fig.3).

These animal studies affirmed targeted delivery to and protective effects of antioxidant enzyme conjugates in the pulmonary endothelium and provided means to define selectively role of given ROS in animal models of acute oxidative stress. For example, Ab/catalase, but not Ab/SOD conferred protection in models of pulmonary ischemia/reperfusion injury implicating  $H_2O_2$  as a main damaging ROS [122]. However, the acuteness and severity of tissue injury in this type of animal model could overshadow more subtle effects of Ab/SOD.

Indeed, Ab/SOD, but not Ab/catalase or untargeted SOD formulations, inhibited vasoconstriction induced by Angiotensin II in mice, thereby confirming the key role of superoxide produced by endothelial NADPH oxidase in quenching NO [122]. Furthermore, Ab/SOD, but not Ab/catalase or untargeted SOD formulations including PEG-SOD, inhibited pathological endothelial activation induced by cytokines and manifested by expression of VCAM-1 in the pulmonary endothelium in mice [57]. Studies in cell culture revealed that anti-PECAM/SOD accumulating in the endosomes quenches superoxide anion produced into vesicular lumen by NADPH oxidase, thereby intercepting specific proinflammatory signaling by intracellular superoxide inaccessible to other SOD formulations [57].

**Control of duration of effects and endothelial delivery of antioxidant enzymes loaded into protective carriers.—**Endothelial cells internalize AOE conjugates anchored to ACE, ICAM and PECAM. This enables site-specific quenching of ROS in endosomal compartment, critically important for interception of pro-inflammatory signaling [57]. However, due to vesicular trafficking involving a series of sodium-proton exchangers, within few hours internalized conjugates reach lysosomes and proteolytic degradation limits duration of antioxidant effects [125]. Of note, ICAM molecules delivering anchored conjugates dissociate from them in the endosomes and recycle to the cell surface, thereby allowing sustained intracellular delivery and effect of circulating anti-ICAM conjugates [126]. Further, auxiliary drugs disrupting microtubules and lysosome maturation prolongs antioxidant effects of the internalized catalase conjugates [100, 126]. These findings provide a basis for pharmaceutical regulation of the duration of therapeutic effects of targeted AOE.

Using nanocarriers offers an additional approach to modulate endothelial delivery and effects of AOE. First, geometry (size and shape) of nanocarriers affect their circulation, interaction with targets and intracellular processing [46, 127, 128]. This, elongated carriers offer higher degree of endothelial targeting specificity, while decelerating arrival of the lysosomes, thereby prolonging effect of ICAM-targeted catalase formulations [111].

An alternative approach is to encapsulate AOE into nanocarriers permeable for small molecules of ROS, but not proteases (proteins with MW in tens of kD). For example, a freeze-thawing double emulsion technique allows fairly efficient (~10%) encapsulation of active catalase into spherical polymer nanocarriers (200-400 nm diameter) based on PEG-PLGA and similar di-block copolymers, permeable for H2O2 and protecting catalase from proteases [129]. Using PEG-catalase further enhances the encapsulation efficacy and protection against proteases [45], whereas modulating molar ratio and size of PEG and PLGA chains in copolymer allows to produce catalase-loaded nanocarriers of spherical or filamentous shape [47]. Isotope-labeled catalase encapsulated in PEG-PLGA nanocarriers is protected from proteolysis and circulates for a prolonged period of time in mice, similarly to PEG-catalase, yet PEG-catalase is degraded by proteases [45].

Coating of catalase-loaded PEG-PLGA nanocarriers by anti-PECAM conjugated with PEG end groups provides highly specific and effective endothelial targeting of isotope-labeled cargo in vitro and in vivo and prolonged antioxidant protection of the endothelium [130]. Of note, PEG-PLGA polymer matrix is readily diffusible for  $H_2O_2$ , but not superoxide; hence encapsulation into PEG-PLGA nanocarriers practically obliterates effective enzymatic activity of SOD [130]. In contrast, encapsulation of either catalase or SOD into micelles formed by controlled precipitation of magnetic nanoparticles using calcium and oleate provides composite nanocarriers (200-300 nm diameter) containing active catalase or SOD accessible for either  $H_2O_2$  of superoxide and protected from proteases [131]. Targeting this formulation to endothelial cells using magnetic delivery [131] or anti-PECAM conjugated to surface of the micelles confers endothelial targeting and antioxidant protection.

## **CONCLUSION**

There was an impressive progress in design of antioxidant interventions targeted to the vascular endothelium in the last decade. A series of animal studies have demonstrated superiority of targeting catalase and SOD to endothelial markers including ACE and cell adhesion molecules over non-targeted formulations. Identification of alternative markers including those typical of specific endothelial phenotypes is underway and will even further diversify our arsenal of new means for targeted antioxidant interventions. These new means will help to dissect mechanisms of vascular oxidative stress and, hopefully, eventually translate into the clinical domain, thereby improving management of disease conditions involving this pathological mechanism. Ischemia-reperfusion injury in organ transplantation represents a clinical setting especially well posed to this development. Of course, industrial development of such complex drug delivery system will be modulated by commercial, regulatory and practical aspects. In this context, treatment of acute oxidative stress represents a more plausible therapeutic target than prolonged management of subtle chronic conditions.

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#### **Fig. 1.**

Vascular oxidative stress. Pro-inflammatory insults cause endothelial exposure of cell adhesion molecules (selectins, ICAM or VCAM) and cytokine production. Cell adhesion molecules facilitate white blood cell (WBC) adhesion and transmigration. Activation of Nox (for example by angiotensin II) leads to generation of superoxide that quenches NO and thus causes vasoconstriction. Activated WBCs bind to endothelium via cell adhesion molecules and produce reactive oxygen species (ROS) and other aggressive molecules that can result in oxidative damage and death of endothelial cells. ICAM, intercellular adhesion molecule; Nox, NADPH oxidase; PMN, polymorphonuclear neutrophils; TM, thrombomodulin; ICAM, intercellular cell adhesion molecule; VCAM, vascular cell adhesion molecule; TNF, tumor necrosis factor, IL, interleukin.

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## **Fig. 2.**

Reactive oxygen species pathways, antioxidant enzymes and their role in vascular oxidative stress. Superoxide is produced by several cellular enzyme systems including NADPHoxidases, xanthine oxidase, etc. It can react with NO producing aggressive peroxynitrite anion ONOO− and decreasing NO pool. Superoxide spontaneously or by action of superoxide dismutase may be reduced into hydrogen peroxide  $H_2O_2$ . Hydrogen peroxide can produce extremely reactive hydrogen radical ·OH in the presence of transition metals or hypochlorous acid by myeloperoxidase. Catalase and glutathione peroxidases protect cells against hydrogen peroxide. ALI/ARDS, acute lung injury/acute respiratory distress syndrome; COX, cyclooxygenase; GSHPx, glutathione peroxidases; MPO, myeloperoxidase; ROS, reactive oxygen species; SOD, superoxide dismutase; XO, xanthine oxidase.



### **Fig. 3.**

Protective effects of targeted formulations of AOEs in models of oxidative stress in vitro and in vivo. Catalase and SOD were conjugated to antibodies against endothelial target. AngII, angiotensin II; GOX, glucose oxidase; LPS, lipopolysaccharide; PQ, paraquat; SOD, superoxide dismutase.

#### **Table 1**

Classes of antioxidants tested for therapeutic use.



*\** BHA, butylated hydroxyanisole; t-BHQ, t-butylhydroquinone 5; ROS, reactive oxygen species.

#### **Table 2**

Targets for endothelial drug delivery.



ACE, angiotensin-converting enzyme; APP-2, aminopeptidase 2; EC, endothelial cell; ICAM, intercellular adhesion molecule; MM, molecular mass; PECAM, platelet-endothelial cell adhesion molecule; TfR, transferrin receptor; TM, thrombomodulin; VCAM, vascular cell adhesion molecule.