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Aminolevulinic Acid-Photodynamic Therapy Combined with Topically Applied Vascular Disrupting Agent Vadimezan Led to Enhanced Antitumor Responses

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Abstract

The tumor-vascular disrupting agent (VDA) vadimezan (5,6-dimethylxanthenone-4-acetic acid, DMXAA) has been shown to potentiate the antitumor activity of photodynamic therapy (PDT) using systemically administered photosensitizers. Here, we characterized the response of subcutaneous syngeneic Colon26 murine colon adenocarcinoma tumors to PDT using the locally applied photosensitizer precursor aminolevulinic acid (ALA) in combination with a topical formulation of vadimezan. Diffuse correlation spectroscopy (DCS), a non-invasive method for monitoring blood flow, was utilized to determine tumor vascular response to treatment. Additionally, correlative CD31-immunohistochemistry to visualize endothelial damage, ELISA assays to measure induction of tumor necrosis factor-alpha (TNF- α) and tumor weight measurements were also examined in separate animals. In our previous work, DCS revealed a selective decrease in tumor blood flow over time following topical vadimezan. ALA-PDT treatment also induced a decrease in tumor blood flow. The onset of blood flow reduction was rapid in tumors treated with both ALA-PDT and vadimezan. CD31-immunostaining of tumor sections confirmed vascular damage following topical application of vadimezan. Tumor weight measurements revealed enhanced tumor growth inhibition with combination treatment compared to ALA-PDT or vadimezan treatment alone. In conclusion, vadimezan as a topical agent enhances treatment efficacy when combined with ALA-PDT. This combination could be useful in clinical applications.

INTRODUCTION

Photodynamic therapy (PDT), a clinically useful curative or palliative treatment for a variety of solid malignancies acts through multiple mechanisms, including vascular damage, direct killing of tumor cells and stimulation of host anti-tumor immune responses (1). Initial PDT studies used the now FDA-approved, intravenously administered exogenous photosensitizer porfimer sodium (Photofrin®) but a major disadvantage of this agent was the prolonged cutaneous sensitivity that followed administration (2). Conversely, the prodrugs aminolevulinic acid (ALA) and its methyl ester form methyl aminolevulinate (Metvix™, MAL) can be applied topically and cause cells, in particular tumor cells, to accumulate

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increased amounts of the endogenous photosensitizer protoporphyrin IX (PpIX), which does not cause prolonged photosensitivity (3,4). Topical PDT using both ALA and MAL has gained considerable acceptance in the clinical setting due to the convenience of application, rapid clearance of the photosensitizer and the decreased period of skin photosensitivity following application compared to first generation photosensitizers (5). Furthermore, topical PDT was as effective as surgical excision of superficial dermal lesions, was not invasive, caused less cosmetic damage and had the advantage of treating multiple lesions simultaneously (6–10). While both ALA and MAL are used for treatment of dermatological lesions, our studies focused on ALA as the prodrug precursor for PpIX synthesis because of our greater experience with ALA-PDT in approved protocols in pre-clinical studies (11–13) and in clinical settings for treatment of BCC at Roswell Park Cancer Institute (14,15). Kuijpers *et al* found similar short-term therapeutic efficacy between ALA and MAL-PDT in treatment of nodular BCC lesions and multiple reports showed that there was no difference in photosensitizer distribution after topical application of either prodrug (16–18). Furthermore, a recent report by the British Association of Dermatologists of the guidelines for management of BCC recommended the use of ALA or MAL-PDT for treatment of superficial lesions (19). While ALA-PDT has demonstrated efficacy in treatment of numerous superficial skin lesions and malignancies (20–22), its efficacy in treatment of BCCs was highly dependent on lesion size and surgical excision of nodular BCC was found more effective than ALA-PDT (23,24). Therefore, it would be advantageous to find mechanisms that increases ALA-PDT efficacy in nodular lesions to maintain the advantages of PDT and reduce the need for surgical excision.

The presence of a functioning vascular network in tumors is essential to meet their metabolic demands for oxygen and nutrient supply. Indeed, it is well recognized that vascular destruction is one of the major consequences of PDT when performed using most systemically administered photosensitizers (25,26). Studies of the response to ALA-PDT suggest that the antitumor activity is primarily mediated by direct tumor cell toxicity rather than effects on the tumor vasculature (11,27). We therefore investigated the combination of topical ALA-PDT with topical application of vadimezan, a vascular disrupting agent. We previously showed that vadimezan caused a steady and rapid decrease in blood flow over time, resulting in a decrease to 50–55% of baseline at 2 hours post application and further decreasing to 65–70% of baseline at 3 hours post application, confirming that vadimezan causes a rapid disruption of tumor blood flow when used as a topical agent (12). Here, we expanded our studies to examine blood flow after combination treatment with ALA-PDT and vadimezan to test our hypothesis that direct cytotoxicity of ALA-PDT in conjunction with the potent vascular disruptive effects of vadimezan would enhance the antitumor activity *in vivo*.

We chose to use the subcutaneous Colon26 murine colon adenocarcinoma in BALB/c, rather than the transgenic Gli transcription factor overexpressing model used in our previous study (12) which develops spontaneous BCC-like tumors with a similar morphology to human BCC (28). Growth of subcutaneously inoculated Colon26 tumors is very reproducible and the blood supply is evenly distributed within the tumor. Tumor growth in the K5-Gli-2 mice is sporadic, sizes vary considerably and the blood supply of the tumors tends to be confined to the connective tissue surrounding the tumor nodules. For proof of principle, and to reproducibly demonstrate changes in blood flow, we decided to use a model in which differences in size and blood vessel distribution were minimal.

Vadimezan is currently in Phase III clinical trials after successful Phase II trials in combination with standard chemotherapy for treatment of non-small cell lung cancer (29,30) and castration-refractory metastatic prostate cancer (31). Vadimezan has shown antivascular effects in both murine and human tumors, increasing vascular permeability and hemorrhagic

necrosis (32,33). The local synthesis of cytokine TNF- α within murine tumors was found in part to cause the tumor destruction (34,35). Our earlier studies indicated that addition of intraperitoneal vadimezan to PDT using the systemically-administered photosensitizers porfimer sodium (Photofrin™) and HPPH (Photochlor™) dramatically enhanced the destruction of solid tumors implanted in mice (34,36).

It is well established that to achieve the maximal benefit from photodynamic treatments, sufficient oxygen levels need to be present in the tumor to form the damaging reactive oxygen species. Therefore, the time of topical vadimezan administration must be optimized to ensure that the induced vascular collapse does not impede the photodynamic reaction. Based on the rapid decrease of tumor blood flow and tumor perfusion after topical vadimezan treatment observed in our previous study, we demonstrate that the combination of ALA-PDT and topical vadimezan decreases tumor size when vadimezan is applied 1 hour prior to irradiation (12).

MATERIALS AND METHODS

Reagents

5-Aminolevulinic acid hydrochloride was purchased from Sigma-Aldrich (St. Louis, MO). Solid 5,6-Dimethylxanthenone-4-acetic acid (courtesy of Gordon Rewcastle, University of Auckland, New Zealand) was stored at room temperature in the dark.

Tumor model, treatment groups, vadimezan treatment and photodynamic therapy

All experimental protocols were approved by Roswell Park Cancer Institute Institutional Animal Care and Use Committee. Six to eight-week-old female BALB/cAnNCr mice were obtained from Jackson Laboratory (Bar Harbor, ME). After removing mouse fur by shaving and use of a depilatory cream, mice were subcutaneously inoculated with 1×10^6 of the murine colon adenocarcinoma Colon26 on the upper right back. When tumors reached 5–6 mm in diameter, mice were randomly placed in each of the treatment groups: untreated controls, ALA-PDT alone, ALA-PDT plus topical DMSO, topical vadimezan alone and ALA-PDT plus topical vadimezan. ALA was prepared as a 20% (w/v) topical solution in the proprietary vehicle DUSA (DUSA Pharmaceuticals, Inc., Wilmington, MA). Twenty μ L of the 20% ALA solution was applied topically to the tumor in 5 μ L increments 3 hours prior to light treatment. The ALA incubation time was based on our prior experience with topical ALA in this tumor model at the sizes used in this study in which 3 hours is sufficient for PpIX synthesis throughout tumors of 1.5–2.5 mm thickness to the deepest part, the reported depth (1 to 2 mm) of measureable drug concentration in human BCC tumor biopsies after topical ALA application (18,37). Also, studies by Ericson *et al* showed a maximal gradient between normal skin and tumor tissue fluorescence at 3 hours after ALA application (38). OpSite transparent medical dressing (Smith & Nephew Medical Limited, Hull HU3 2BN England) was placed over the tumor to protect the area. Vadimezan solution, 1 mg vadimezan dissolved in 40 μ L of DMSO was applied to the tumor in a similar fashion in 5 μ L increments at one hour before laser treatment and OpSite was placed over the tumor. Three hours after application of ALA, mice were anesthetized with Ketamine/Xylazine (K/X, 100/10 mg/kg) and placed on a heated pad to maintain body temperature. A light spot diameter of 1.1 cm from a dye laser pumped by an argon ion laser tuned to 635 nm was used to irradiate the tumor at a fluence of 80 J/cm² and a fluence rate of 75 mW/cm². When tumors in the control group grew to the endpoint of 400 mm³, all mice were sacrificed and tumors were removed and weighed.

Immunohistochemical analysis

BALB/c mice bearing Colon26 tumors and mice without tumors were left untreated or were treated with ALA-PDT, topical vadimezan or the combination as described above. Twenty-four hours later mice were sacrificed and tumors removed. The tumors were cut in half to expose the deepest part of the tumor and placed in Zinc fixative (Formalin-free, BD Pharmigen, San Diego, CA) overnight, then transferred to 70% ethanol. The samples were then processed and embedded in paraffin. Sections were stained for CD31, an endothelial cell marker as described previously by Henderson et al (39). The mean tumor thickness of control (untreated) tumors at the time of treatment was 2.02 ± 0.20 (mean \pm standard deviation, range 1.8–2.3 mm) and the mean thickness of all tumors 24 h after treatment was 1.97 ± 0.16 mm.

Optical blood flow measurements (Diffuse Correlation Spectroscopy)

The DCS technique was used to non-invasively and continuously monitor blood flow. The DCS instrument was previously detailed in our published work (15,40–42). The DCS technique was also previously described in detail (43–49). Briefly, the instrument had a 785 nm long coherence length laser (CrystaLaser), a single photon-counting detector (Perkin-Elmer) and a custom built autocorrelator board (Correlator.com). The source-detector Photodetector outputs were fed into the correlator board with the resulting intensity autocorrelation functions and photon arrival times recorded by a computer (43). The normalized intensity autocorrelation function allowed for the diffuse electric field temporal autocorrelation function to be obtained (43), which was shown to satisfy the diffusion equation (46–48). Brownian or random flow models can be applied to extract information about the particle motion by solving the diffusion equation (50).

Blood flow was monitored by DCS in Colon26 tumors on the upper right back of BALB/c mice. Tumors for DCS were slightly larger (6.5 – 7.5 mm in diameter) than those for histology and the PDT treatment tumor response. Tumors are measured with calipers which includes the overlying skin so the tumor tissue itself is somewhat smaller than this. To ensure that the projections onto the tumor of the source and detection fibers with the largest separation distances used could be positioned to monitor only tumor tissue, the slightly larger tumor size was used. Hypoxic areas (although not necrotic) are found within tumors at all the sizes we have used in this study, but do not appear to be greater in the larger tumors (possibly because the vasculature is slightly more mature). The slightly increased diameter of tumors used the DCS may have slightly changed the tumor vascular dynamics, and if the tumors from the DCS monitored groups had been grown to the endpoint, they may well have had a poorer response.

However, we believe that the differences in the conclusions drawn would also be minimal. The depth of penetration of the diffuse light corresponds to approximately one-third to one-half of the separation distance between the source and detector fibers (50). In these studies, 2 separation distances of 2 and 3.5 mm were used, which correlate to tumor depths of 1 to 1.33 mm and 1.75 to 2.33 mm, respectively. Two depths within the tumor were examined to monitor whether ALA-PDT and vadimezan caused vascular effects both close to the surface where the drugs were topically applied and at the deepest aspects of the tumor where topically applied drugs may be present at lower concentrations. Mice were anesthetized during DCS measurements and placed on a heating pad at 34.5°C to maintain body temperature. A thermal couple was inserted under the skin on the right flank of the mouse to monitor body temperature throughout DCS. To keep the mice immobilized, booster injections of K/X at 0.25 of the original dose (25/2.5 mg/kg) were administered every 30 minutes. Mice were sacrificed immediately after DCS was completed. To monitor normal tissue blood flow and the effect of anesthesia, data was collected from source and detector

fibers placed on depilated skin over the hip of the mouse and protected from light. For all DCS data, blood flow fluctuations in the tumor were first normalized to baseline measurements of tumor blood flow taken prior to treatment. The blood flow measurements were further normalized to the blood flow from the non-tumor, skin tissue region. Once the baseline measurements were made, treatment and DCS monitoring began.

Enzyme-linked immunosorbent assay

TNF- α protein expression in tumor tissue from BALB/c mice inoculated with Colon26 tumors treated with DMSO or vadimezan was determined using a Quantikine mouse TNF- α /TNFSF1A ELISA kit purchased from R&D Systems (Minneapolis, MN). Tumor tissues were excised at various time points after treatment and homogenized in 1ml per gram of tumor tissue of CellLytic MT Mammalian Tissue Lysis/Extraction Reagent (Sigma-Aldrich, St. Louis, MO) plus protease inhibitor cocktail (P-8340, Sigma-Aldrich, St. Louis, MO) at a ratio of 400:1. Supernatants were isolated by centrifugation and their protein concentration was determined using the Bio-Rad protein assay (Bio-Rad Laboratories, Hercules, CA). Samples containing 40 μ g of protein were analyzed for cytokine expression. Four to six mice were used for each test group (except 1 h DMSO, 2 mice only, since vehicle alone showed no histological or blood flow effects at 1 hour post application).

Statistical analysis

Unpaired two-tailed t-test analyses were carried out on parametric data using the GraphPad Prism software, version 5.01. (GraphPad Software, Inc.)

RESULTS

ALA-PDT caused a decrease in tumor blood flow

The reported literature shows that the extent of ALA-PDT induced vascular damage is highly variable. The vascular response can be altered by parameters which include but are not limited to route of ALA delivery, light dosimetry and wavelength of activating light used (8,11,51–53). We showed previously that ALA-PDT in tumor bearing mice led to a decrease in tumor blood flow immediately following the start of light delivery, but blood flow remained constant at 50 to 60% of baseline for the hour following irradiation (12). To confirm and extend these observations of the effect of topical ALA-PDT on blood flow, DCS was employed in the current study to non-invasively monitor tumor blood flow *in vivo* continuously before, during and after completion of light delivery (80 J/cm² delivered at a rate of 75 mW/cm²), but for a prolonged period of 3 hours. The average relative tumor blood flow was measured at two depths within the tumor of approximately 1 and 1.75 mm (n=2) (Figure 1). Immediately at the start of light delivery a drop in tumor blood flow was observed at both monitored depths within the tumor tissue, culminating in a maximal drop to approximately 50 to 70% of baseline levels during light delivery. Following completion of light delivery, the relative tumor blood flow did not recover to baseline levels or decrease further decrease for the 3 hours monitored. This demonstrates that ALA-PDT alone causes a measureable decrease in tumor blood flow, similar at both depths which is maintained for 3 hours but does not lead to complete stasis of tumor blood flow. Therefore, addition of the vascular disrupting agent vadimezan to the ALA-PDT treatment was proposed which may further enhance the antivasular effect and tumor response.

Topical vadimezan treatment reduces vascular density in tumors but not in normal skin tissue

Vadimezan and vehicle DMSO were applied topically to skin on the upper right back of naïve BALB/c mice or animals bearing subcutaneous Colon26 tumors. Twenty four hours

after treatment, mice were euthanized and skin or tumors were removed for immunohistochemical staining. An antibody against CD31 was used to stain the endothelial cells within the skin and Colon26 tumor samples. Vessel density was determined by counting the number of vessels in 5X magnification fields, at least 3 fields per sample. In Figure 2, compared to BALB/c skin treated with DMSO only, skin exposed to vadimezan did not demonstrate a significant decrease in CD31 stained vessel number (75.3 \pm 5.3 vessels for DMSO, 83.6 \pm 3.7 vessels for vadimezan, $p=0.2455$ using the unpaired two-tailed t-test, $n=4$). Furthermore, no change in vessel size or extravasation of red blood cells was observed in the blood vessels from vadimezan treated murine skin samples from BALB/c mice. This demonstrates that topically applied vadimezan does not cause damage to the normal blood vessels in the skin in this model.

Vadimezan caused a significant decrease in the number of tumor blood vessels (85.1 \pm 12.0) to the full depth of the tumor of 1.78 \pm 0.17 mm (mean \pm standard deviation, $n = 3$) compared to untreated (158.4 \pm 32.4) or vehicle treated tumor samples harvested 24 hours after application ($p=0.0175$, unpaired two-tailed t-test, $n = 3$), Figure 3 and Table 1. It is important to note that the vascular damage caused by vadimezan was not confined to the region of tumor nearest to the epidermis, the site of topical application, but was observed throughout the tumor including at the tumor base (Figure 3B) which is well vascularized in the untreated control (Figure 3A). The enlarged and magnified images in Figure 3 show the extensive damage to the endothelial cells induced by vadimezan at the base of the Colon26 tumors in the region furthest from the skin (Figure 3B) compared to the untreated tumor (Figure 3A). Increased vascular leakiness also was observed at 24 hours post vadimezan application by the extensive extravasation of red blood cells into the tumor tissue (black arrows, Figure 3B), which was not observed in untreated samples. Also, some regions of nuclear condensation were observed at 24 h post topical vadimezan treatment, which may be indicative of apoptosis. These results provide proof of concept that vadimezan is effective at damaging blood vessels when applied topically.

Topically applied vadimezan induced TNF- α production in Colon26 tumors

The hemorrhagic necrosis observed in murine tumors in response to vadimezan treatment has been reported to be a response to tumor cell production of cytokines, largely TNF- α (35,54,55). To determine if topically applied vadimezan induced TNF- α within treated tumors, the cytokine levels in tumor lysates prepared at different time points after topical vadimezan treatment were measured by ELISA. Control lysates were from tumors treated with DMSO only. Topical application of vadimezan led to a significant and maximal increase in tumor TNF- α levels by 3 hours post application compared to vehicle treated tumors (Figure 4, * $p=0.0338$, unpaired two-tailed t-test), demonstrating a probable role of this cytokine in vascular damage with topical use of vadimezan.

The combination treatment of ALA-PDT and topical vadimezan caused a rapid decrease in blood flow

In a previous section we showed that ALA-PDT alone caused an immediate decrease in tumor blood flow during irradiation that did not recover during the 3 hours of monitoring. Previous data showed that topical vadimezan induced a rapid and steady drop in tumor blood flow to about 25% of baseline over 4 h, and that the optimal application time to maintain tumor perfusion during ALA-PDT was probably 1 hour prior to illumination (12). Next, we monitored the effect of the combined treatments on tumor blood flow ($n=2$), with the vadimezan applied 1 hour before light delivery. In the combination study, blood flow was monitored at one depth (approximately 1 mm) within the tumor, because there was no apparent difference in the blood flow changes at the two depths. When vadimezan was applied topically, a net decrease in blood flow of approximately 20% was observed by 1

hour when light delivery began (Figure 5A). Blood flow then steadily decreased over time to reach approximately 55 to 60% of baseline at 2 hours post topical application, when monitoring ceased (Figure 5A). This was similar to that observed at 2 hours post topical treatment of vadimezan as a single therapy (12) and greater than at any time after light delivery with the ALA-PDT single therapy (Figure 1). The combination therapy therefore decreased tumor blood flow consistent with the effect contributed by the vadimezan, but with no additional contribution from the ALA-PDT. It is possible that the vadimezan induced fluctuations in tumor blood flow and damage to tumor endothelial cells might interfere with the ALA-PDT vascular response. Topical vadimezan alone eventually decreased blood flow to 30–35% of baseline by 3 hours post application (12) and it is possible that extended monitoring of the combination might eventually show a greater decrease in blood flow than the 40% achieved after 2.5 hours of monitoring the combination treatment in Figure 5A.

The tumor samples treated with ALA-PDT alone (Figure 5B, left) show a slight increase in vessel diameter as well as blood vessel number (216.4 ± 21.9) compared to the untreated tumors (158.4 ± 32.4) at 24 hours post-treatment, Table 1. Destruction of tumor vasculature, extravasation of red blood cells into the tumor stroma and some nuclear condensation was observed in tumor samples exposed to the combined treatment (Figure 5B, right, black arrows, extravasated red blood cells), although the number of vessels remaining intact at 24 hours (159.8 ± 33.0) was higher than in tumors treated with vadimezan alone (85.1 ± 12.0).

Combination treatment with vadimezan and ALA-PDT decreases tumor weight

Compared to ALA-PDT alone, the combination of ALA-PDT and vadimezan caused a substantial decrease in tumor blood flow up to 2 hours following light delivery. We hypothesized that the combined treatment of ALA-PDT direct tumor cell destruction with the vascular disrupting agent vadimezan would enhance treatment outcome. Colon26 tumors were treated with ALA-PDT (80 J/cm^2 delivered at 75 mW/cm^2) alone or in combination with topical vadimezan applied 1 hour prior to PDT light delivery. At the endpoint (tumor growth of controls to 400 mm^3), mice were sacrificed and all tumors were resected and weighed. In Figure 6, it is shown that the combination led to a significant decrease in tumor weight compared to ALA-PDT treatment (***, $p=0.0006$) or vadimezan treatment alone ($p<0.0001$), unpaired two-tailed t-test). No significant decrease was observed when DMSO was applied one hour prior to ALA-PDT ($p=0.3261$, unpaired two-tailed t-test).

DISCUSSION

While topical ALA-PDT has been useful for the treatment of precancerous actinic keratosis lesions and superficial BCC lesions, its use for treatment of nodular BCC skin cancers has to date been less successful (8,23,24). Therefore, approaches to enhance ALA-PDT efficacy would be beneficial for treatment of nodular lesions. It is understood that the choice of photosensitizer used can influence the mechanism of cell death induced by PDT. While some photosensitizers rely on vascular damage (56–58), ALA-PDT causes minimal damage to the vasculature and relies mostly on direct cytotoxicity to tumor cells (8,59). Peng et al applied a dual photosensitizer approach with non-vascular ALA-PDT plus low dose vascular destructive Photofrin-PDT, resulting in a significant decrease in tumor growth due to the lethal combination of microcirculatory shut down and direct cell toxicity (27). In the present study, a similar approach was employed by combining the small molecule vascular destructing agent vadimezan in place of anti-vascular PDT with the cytotoxic ALA-PDT treatment.

Unlike antiangiogenics which target neovascular growth, vadimezan leads to the selective destruction of tumor blood vessels (60). The specific tumor vascular collapse results in tumor hypoxia, hemorrhagic necrosis and ultimately tumor cell death (60–62). The selectivity of vadimezan is in part due to the direct and rapid induction of apoptosis of the tumor endothelial cells and induction of cytokines including TNF- α (55,63). In our studies, tumor samples removed at 24 hours after topical application of vadimezan demonstrated a significant decrease in the number of tumor blood vessels and a substantial decrease in CD31 endothelial cell staining, similar to the response observed by Seshadri *et al* with i.p. delivered vadimezan (32). DCS monitoring demonstrated a decrease in blood flow early after the application of vadimezan, which continued to decline over the monitored period and we believe that the early changes in blood flow are ultimately reflected in the blood vessel damage, which is seen in the histology of samples removed at 24 hours after treatment. A potential benefit to the combination treatment is that vadimezan and ALA-PDT would act in a complementary manner if timed correctly, targeting tumor tissue with non-overlapping toxicity by different mechanisms of action. While vadimezan selectively damages tumor vessels, it is less effective in targeting tumor cells of the periphery which are supplied by the normal tissue vasculature. This is often observed after single treatment among many vascular disrupting agents as a viable rim of tumor which persists at the periphery (64,65). To the contrary, PDT is highly effective in treatment of the outer, well perfused rim of tumor but often the inner, hypoxic and less-perfused central region of tumor has increased resistance to PDT (66).

The order of drug application is critical for a response to combination therapy. With PDT, the best tumor response was observed when cellular damage occurs first followed by vascular damage (66). As oxygen is critical for the photodynamic reaction during light irradiation, vadimezan needs to be administered such that blood vessels remain functional during light delivery to maintain blood flow and oxygen delivery. Previously we found that blood flow decreased gradually to 50–55% of baseline levels 2 hours after topical application of vadimezan (12) similar to that observed with ALA-PDT (Figure 1). We considered that a later application of vadimezan one hour prior to light delivery in ALA-PDT would not interfere with blood flow during light delivery as the vascular damage is a more gradual response and will occur after light delivery is complete. A previous report of the vascular damage induced by vadimezan using MRI showed that at 24 hours after treatment a significant extravasation of the contrast agent was observed in the tumors, indicative of vascular leakiness and damage (67). This corresponds to our studies of CD31 immunostained tumors, which showed red blood cell extravasation and a marked decrease in endothelial cell staining 24 hours after topical vadimezan application (Figure 3B). Previously by using DCS, we were able to monitor tumor blood flow in real time immediately after application of topical vadimezan (12). This technique was beneficial in this study as it permitted simultaneous monitoring of the tumor perfusion response without interrupting the laser irradiation and provided significant information about the rapid response to vadimezan and ALA-PDT of decreasing tumor blood flow at the monitored depths within the tumor tissue. Previous observations suggested that the optimal time for topical vadimezan application to tumors should be approximately 1 to 2 hours prior to PDT treatment such that decreased blood flow and vascular damage would follow the PDT induced cellular damage (12). This timeframe matched our previous report in which the combination of systemic vadimezan and Photofrin-PDT had maximal efficacy when vadimezan was administered 1–3 hours prior to light delivery, presumably because some time was required before the vadimezan effects occurred (34). Here, we found a successful decrease in tumor weight when topical vadimezan was applied 1 hour prior to ALA-PDT treatment. However, blood vessel numbers with the combination were similar to untreated controls at 24 h post treatment, which is of some concern despite the delay in tumor growth

found, so 1 hour prior to light delivery still may not be the optimal application time for topical vadimezan and further studies are required to determine this.

The immunohistochemical staining of tumor sections and DCS monitoring of blood flow at two tissue depths show that topically applied vadimezan affects blood vessels throughout the tumor and is not limited to the surface region. While we have used Colon26 tumors as a reproducible model of a nodular subcutaneous lesion, topical vadimezan applied to the spontaneous tumors of the K5-Gli-2 mouse model, which are a closer histological and morphological representation of human BCC, also caused extensive vascular destruction, red blood cell extravasation and tumor damage (12). While further studies need to be carried out to determine the usefulness of topical vadimezan in clinical treatment of cutaneous disease, especially nodular BCC, the positive response in the K5-Gli-2 model supports further investigation. Interestingly, it was observed that ALA-PDT caused a slight increase in vessel diameter and vessel numbers at 24 hours post-treatment as observed in Figure 5B. Previously, it was reported that ALA-PDT increased the number of blood vessels in the capillary beds of psoriasis plaques during and after ALA-PDT treatment (68). Increased expression of VEGF after ALA-PDT was also reported (69). It has been proposed that the post-PDT induction of VEGF may be responsible for the tumor recurrence observed after sub-curative PDT treatments as it provides a survival stimulus for the tumor cells (69,70). It is also possible that indirect effects of ALA-PDT, including inactivation of cytokines and hypoxia (due to the photochemical consumption of oxygen during the photochemical reaction) may stimulate endothelial cell proliferation (71–73). The intact blood vessels observed 24 h after treatment both in the ALA-PDT and combination treatments may help with re-oxygenation of the treated area and cause reperfusion injury which may contribute to ALA-PDT mediated damage, which has been shown in normal colon (74). However, there is a balance between pro- and anti-tumor effects and we currently do not know whether the blood vessels in the combination treatment would decrease at later time points, before recovering and sustaining tumor growth. This scenario could support a later, and/or additional application of vadimezan to inhibit the regrowth of blood vessels as tumor growth recovers.

Attempts to increase ALA-PDT efficacy with penetration enhancers such as dimethyl sulfoxide (DMSO) and iron chelators such as ethylenediamine tetraacetic acid (EDTA) in the application vehicle to increase the delivery of topically applied ALA to deeper sections of the tumor improved the complete response rates of nodular BCCs (20). In this report, the vehicle used for topical application of vadimezan was DMSO. However, DCS monitoring showed that DMSO alone did not affect tumor blood flow after topical application. Additionally, topical DMSO applied one hour prior to ALA-PDT did not significantly decrease tumor growth compared to ALA-PDT alone. Therefore the increased efficacy of the combination treatment is not due to any increased penetration of ALA that may occur with a topical DMSO application, but rather is due to the vascular damage caused by vadimezan.

In summary, this is a preliminary study exploring the use of vadimezan as a topical vascular disrupting agent, and whether this approach would be feasible combined with topical ALA-PDT. The experiments demonstrated a clear enhancement of the PDT effect with the addition of topical vadimezan, inducing a significant decrease in tumor weight compared to the single therapies alone and suggest that the combined approach deserves further investigation. Based on previous studies with topical and systemic vadimezan we considered that application of vadimezan 1 hour before light delivery for PDT would be optimal. However, taking into account the topical vadimezan mediated decreased blood flow that occurs before light delivery, application closer to or even after the light delivery might enhance the effects further. We were concerned that the damage caused by ALA-PDT to the

tumor, including edema, swelling, dilation of tumor vessels and altered microenvironment responses might impair the vadimezan effect if it were applied topically immediately following illumination. However, future studies exploring the temporal importance of single or multiple applications of vadimezan with PDT, should address these possibilities. Also, using a more representative model for nodular BCC, in which the vascular supply is confined to the periphery of the nodules rather than throughout the tumor (as occurs in the subcutaneous Colon26 model), may further increase the clinical applicability of these studies.

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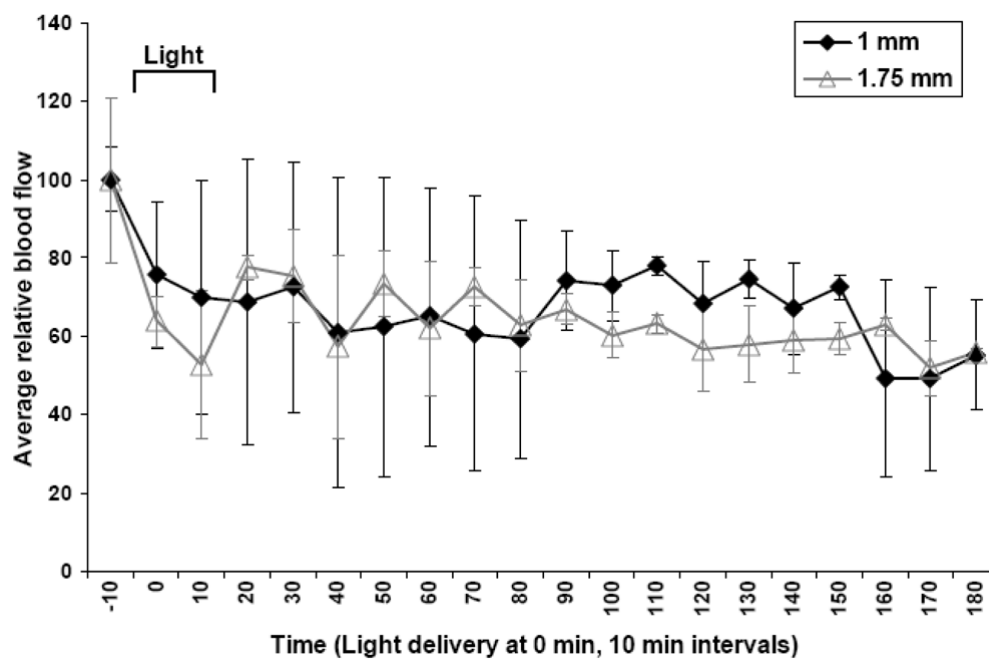


Figure 1. Diffuse correlation spectroscopy measurement after ALA-PDT

Tumor blood flow was monitored by DCS in response to ALA-PDT treatment before, during and after light delivery (80 J/cm^2 at 75 mW/cm^2). Graph represents mean blood flow measurements \pm standard error of the mean (SEM) of replicate experiments ($n=2$) over a period of 190 min (blood flow was measured for 10 min prior to light delivery). Two source-detector distances were used of 2 and 3.5 mm, correlating to measurements at approximately 1 and 1.75 mm deep. Light delivery began at time = 0 min and was complete at 18 min.

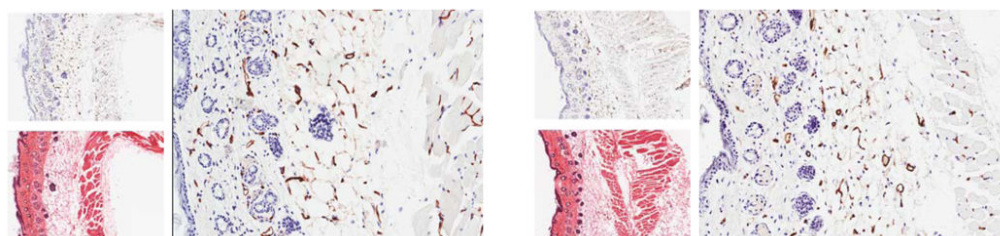


Figure 2. Vadimezan effects on blood vessels in normal mouse skin

Normal BALB/c mouse skin lacking hair was untreated (left panel) or treated with topical vadimezan (right panel). Skin was harvested at 24 h, fixed in zinc fixative and processed for embedding in paraffin. Sections were stained with anti-CD31 antibody. No decrease in the number of skin blood vessels was observed with vadimezan treatment. In each panel, top left: anti-CD31, 5X magnification, bottom left: H&E, 5X magnification, right: anti-CD31, 20X magnification. Figure is representative of replicate samples (n= at least 3).

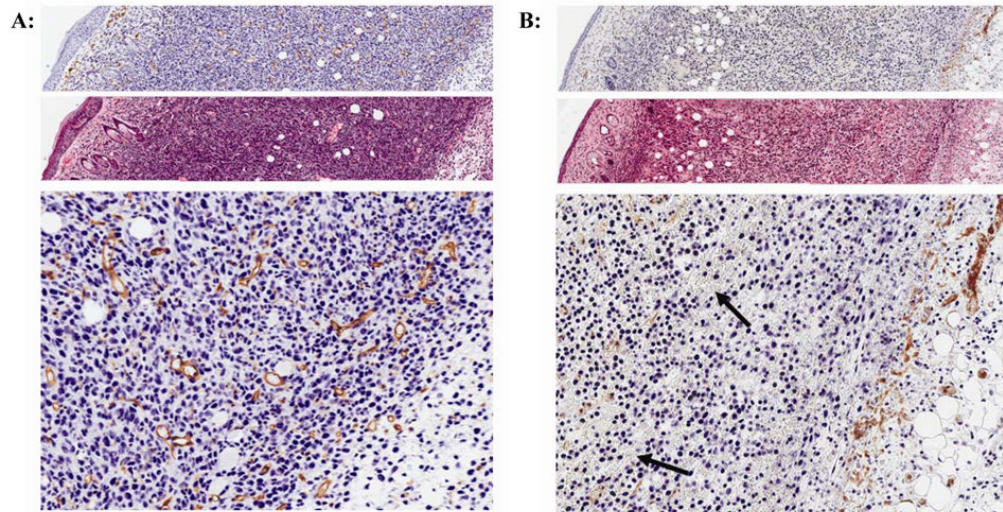


Figure 3. Topical vadimezan causes damage to blood vessels throughout Colon26 tumors

A: Untreated or B: topical vadimezan treated tumor samples from mice sacrificed at 24 h after vadimezan application. Top (anti-CD31) and middle (H&E) panels are at 20X magnification; bottom panel is an enlarged field of the region of tumor furthest from the skin. Figures are representative of replicate samples (n = at least 3). Black arrows indicate red blood cell extravasation in the vadimezan treated sample, not present in the untreated tumor samples. Note: the CD31 and H&E panels (top and middle) are composed of a sequence of adjoining images taken from the stratum corneum to the base of the tumor to show the extent of the vadimezan effect on tumor blood vessels.

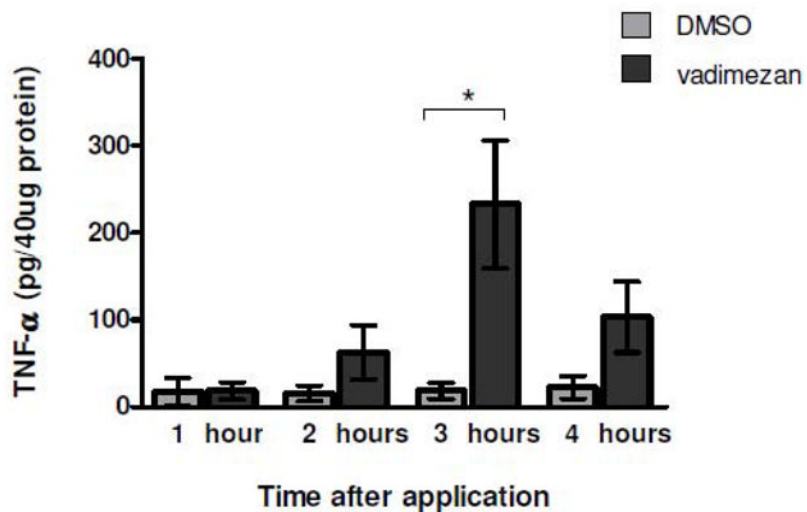


Figure 4. Topical vadimezan leads to increased TNF- α

Topical application of vadimezan induces TNF- α , reaching maximal levels at 3 h as determined by ELISA. Tumor lysates were prepared at various times after topical application. The values reported are the mean \pm SEM of 4–6 mice per group (1 h DMSO, n= 2).

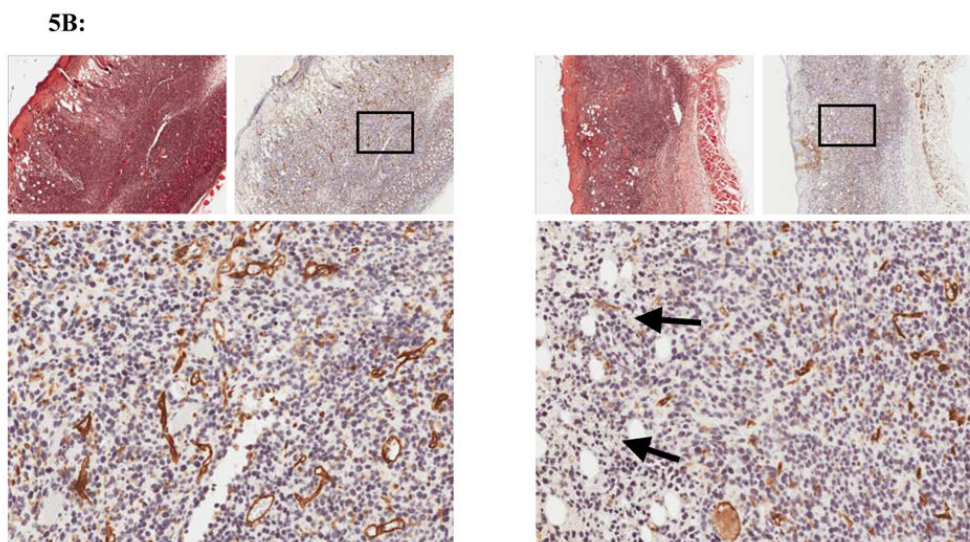
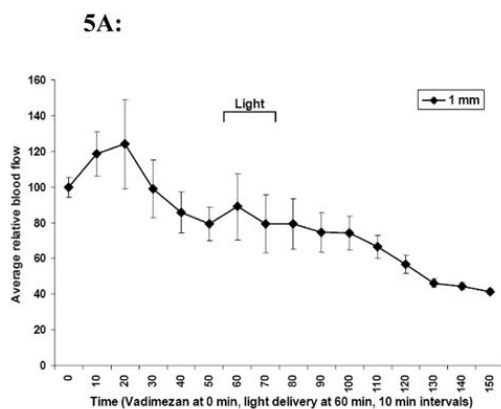


Figure 5.
A: ALA-PDT plus topical vadimezan. DCS was used to monitor blood flow in response to combination treatment. Vadimezan was applied 1 h prior to light delivery (2 h post ALA application). The graph is representative of the average tumor blood flow \pm SEM at 1 mm depth within the tumor (n=2). **B: IHC stain of endothelial cells in response to ALA-PDT with or without topical vadimezan.** 24 h after ALA-PDT alone (left panel) or in combination with vadimezan treatment (right panel), mice were sacrificed and tumors excised. Within each panel: Left-top: H&E, right top, anti-CD31: both at 5X magnification. Bottom: anti-CD31 at 20X magnification. Figures are representative of replicate tumor samples (n = at least 3). Black arrows indicate red blood cell extravasation.

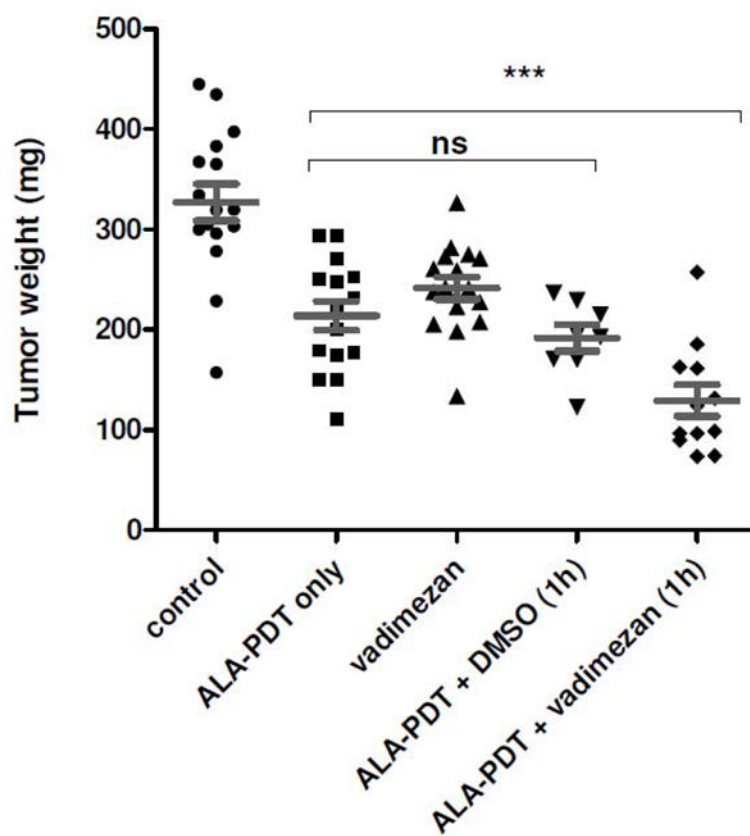


Figure 6. Tumor response to combination therapy

Tumor weights were measured post *in vivo* ALA-PDT, vadimezan, DMSO or combination therapy. Vehicle DMSO and vadimezan were applied 1 h prior to light delivery. The combination of ALA-PDT and vadimezan caused a significant decrease in tumor weight ($p < 0.001$) compared to ALA-PDT alone. No significant change in tumor weight was observed in the ALA-PDT alone, vadimezan alone or ALA-PDT plus DMSO treated groups ($p > 0.05$). Groups contained 8 to 12 mice.

Table 1
Blood vessel density in Colon26 tumors

CD31 stained blood vessels were counted in untreated or treated (ALA-PDT, topical vadimezan or the combination) Colon26 tumors removed 24 h after treatment. At least 8 fields (5X magnification) per group of 3 mice were counted. Values are the mean \pm standard error of the mean (SEM).

	Avg. # vessels per 5X field	S.E.M.
Untreated control	158.4	32.4
Vadimezan	85.1	12.0
ALA-PDT	216.4	21.9
ALA-PDT + Vadimezan	159.8	33.0