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Selective Modification of HK Peptides Enhances siRNA Silencing of Tumor Targets *In Vivo*

Szu-Ting Chou1,2, **Qixin Leng**1, **Puthupparampil Scaria**3, **Martin Woodle**3, and **A. James Mixson**¹

¹ Department of Pathology, University of Maryland Baltimore, MSTF Building, 10 South Pine Street, Baltimore, MD 21201, USA

² Department of Chemical and Biomolecular Engineering, University of Maryland, College Park, MD 20740

3 Aparna Biosciences Corporation, Rockville, MD, 20852

Abstract

Our research has focused on systemic delivery of small interference RNA (siRNA) by branched peptides composed of histidine and lysine, called HK peptides. After studying several HK peptides, one four-branched peptide, H3K(+H)4b, with a predominant repeating pattern of - HHHK-, was found to be an effective carrier of siRNA. Although the unmodified H3K(+H)4b carrier of siRNA targeting an oncogene was previously shown to have promise in a tumor-bearing mouse model, we sought to develop a more effective HK carrier of siRNA in the current study. Our primary goal was to determine whether different ligand (cyclic RGD)-pegylation patterns on the H3K(+H)4b peptide affect siRNA delivery *in vitro* and *in vivo*. We compared the unmodified H3K(+H)4b with two modified H3K(+H)4b peptides for their ability to deliver siRNA in a tumorbearing mouse model; one modified HK peptide, (RGD-PEG)⁴-H3K(+H)4b, had four cRGD-PEG conjugated to each molecule, while the other peptide, (RGD-PEG)-H3K(+H)4b, had one cRGD-PEG per molecule. Although the modified HK peptides by themselves did not form stable nanoplexes with siRNA, combination of a highly charged unmodified HK peptide, H2K4b, with either of the modified HK peptides did form stable siRNA nanoparticles. For *in vitro* experiments with MDA-MB-435 cells that expressed luciferase, the H3K(+H)4b siRNA nanoplexes targeting luciferase decreased its activity by 90% compared with negligible down-regulation by the modified $H3K(+H)4b$ nanoplexes (P<0.01). In contrast, the two modified $H3K(+H)4b$ siRNA nanoplexes administered intravenously were more effective than the H3K(+H)4b nanoplexes in silencing luciferase in a tumor xenograft model. The luciferase activity in tumor lysates of mice administered H3K(+H)4b, (RGD-PEG)-H3K(+H)4b, and (RGD-PEG)⁴-H3K(+H)4b nanoplexes decreased by 18%, 35%, and 75%, respectively. Thus, the siRNA nanoplex incorporating the highly modified peptide, $(RGD-PEG)^{\bar{4}}$ -H3K(+H)4b, was the most effective at silencing its target *in vivo* (P<0.01). These studies demonstrate that selectively modified HK polymers are promising candidates for targeting oncogenes with siRNA.

Keywords

non-viral; siRNA; MDA-MB-435 cells; xenograft; systemic; mouse model

Conflict of Interest Statement

Correspondence: Dr. A. James Mixson, Department of Pathology, University of Medicine School of Medicine, 10 South Pine Street, Room 759, Bldg. MSTF, Baltimore, MD, 21201; JMixson@som.umaryland.edu.

A. James Mixson has license agreements and/or equity with Aparna Biosciences, Sirnaomics Inc., and Silence Therapeutics

Introduction

RNAi silencing is a promising research and therapeutic strategy, utilized to down-regulate aberrant disease-causing genes and to study genes important for signal transduction pathways. The RNAi process is activated by incorporation of a 19 to 23-mer double stranded RNA fragment (siRNA) into the RISC complex $¹$. Together with the Argonaut 2</sup> endonuclease that is part of the RISC complex, the siRNA recognizes and cleaves the target mRNA in a catalytic manner $2-5$. Despite the potential of siRNA as a therapeutic agent, an effective delivery system for siRNA is essential to facilitate specific targeting and cellular uptake in the target tissue, particularly for systemic diseases such as cancer. Indeed, the development of an efficient delivery system for nucleic acids including siRNA has proved elusive and has been the rate-limiting step in developing siRNA-based therapeutics.

Nevertheless, there are many promising carriers for siRNA in various stages of pre-clinical and clinical trials, including synthetic polymers, aptamers, neutral and cationic liposomes, and peptides $6-14$. Currently, no systemic carrier of siRNA has fully been proven effective for clinical use against cancer, but evidence points to a need for ligand-mediated tissue targeting and a preference for nanoplex forms. Moreover, it is likely that non-viral carriers will continue to evolve for the foreseeable future, with progressive improvements. To this end, our lab has focused on developing an effective *in vitro* and *in vivo* vehicle for small interference RNA. To accomplish this, we have synthesized and screened a number of histidine-lysine rich peptides $(HK)^{15-18}$ testing their ability to carry and deliver siRNAto give effective gene inhibition. While lysines are essential for binding siRNA, histidines are important for buffering and may aid in the release of siRNA from endosomes. Altering the sequence of histidines and lysines within the branches of the HK polymer can affect its ability to transport siRNA within the cell. After studying several HK peptides, one 4 branched form, H3K(+H)4b, with predominant repeating patterns of -HHHK-, was determined to be an effective carrier of siRNA: H3K(+H)4b siRNA nanoplexes targeting the Raf-1 oncogene inhibited tumor growth by 60% ¹⁹.

In the current study, we sought to develop a more effective ligand targeted form of the H3K(+H)4b siRNAnanoplex, particularly for use *in vivo*. In order to prevent aggregation and to selectively target the tumor with the nanoparticle, the H3K(+H)4b was modified by varying the number and location of cRGD-PEG conjugates. Two modifications of H3K(+H)4b were made: one highly modified HK polymer in which an cRGD-PEG was attached to each branch (four cRGD-PEG per molecule) and the other, a more limited HK modification in which the cRGD-PEG was attached to the (Lys) ₃ core that generates the branched polypeptide (one cRGD-PEG per molecule). Compared to the unmodified H3K(+H)4b, both modified HK peptides when combined with an unmodified HK peptide were markedly more effective carriers of siRNA to tumors in a murine model. Moreover, the siRNA nanoplex containing the highly modified HK was the most effective in silencing the target gene in tumor xenografts.

Materials and Methods

Animals

Female athymic mice (4–8 wk old) were purchased from NCI Frederick. The experiments were done in accordance with regulations by the Institutional Animal Care and Use Committee of the University of Maryland Baltimore.

Cell line

A human malignant cell line MDA-MB-435, stably expressing firefly luciferase, was cultured in Dulbecco's minimal essential medium (DMEM) containing 10% fetal calf serum (FCS) and 20mM glutamine.

Polymers

The branched HK polymer was synthesized on a Ranin Voyager synthesizer (PTI, Tucson, AZ) by the biopolymer core facility at the University of Maryland, as previously described. The unmodified four branched H3K(+H)4b and H2K4b polymers with a dominant repeating pattern of –HHK- and -HHHK-, respectively were synthesized as described previously ¹⁸. The four terminal branches of the HK polymers emanate from the 3-lysine core: for H3K(+H)4b, the branch sequence is KHHHKHHHKHHHHKHHHK and for H2K4b, the branch sequence is KHKHHKHHKHHKHHKHHKHK. For modified H3K(+H)4b, a cysteine was added to each of the four N-terminal branches or to the C-terminal end of the lysine core. Cyclic (c)RGD-PEG was conjugated to the HK polymer using a synthesis procedure similar to one previously described 12. Briefly, cyclic RGD peptide with the sequence c(RGDfK) (purchased from Peptides International, Louisville, KY) was coupled to 3.4Kd PEG using a heterobifunctional PEG, SCM-PEG-VS, from Nektar Therapeutics (Huntsville, AL), in dry DMSO in equimolar ratio. The cRGD-PEG conjugate was precipitated from DMSO by adding 10 fold excess of anhydrous cold ether. The resulting solid material was dried, characterized and used for coupling to H3K(+H)4b. The cRGD-PEG-VS conjugate obtained was then reacted with H3K(+H)4b consisting of cysteine at the N-terminus of each of the four branches (for RGD-PEG)⁴-H3K(+H)4b) or C-terminus (for RGD-PEG-H3K(+H)4b) at pH 7.3 (HEPES buffer), to obtain the cRGD-PEG modified polypeptides. The modified H3K(+H)4b peptides were purified by dialysis and characterized by amino acid analysis. The resulting conjugates on average had one (for RGD-PEG-H3K(+H)4b) or four (for (RGD-PEG)⁴-H3K(+H)4b)) cRDG-PEG moieties, based on amino acid analysis of the purified conjugates.

siRNA

The siRNA duplex targeting luciferase (Luc) was as follow: sense, 5′-CUG-CAC-AAG-GCC-AUG-AAG- A-dTdT-3′; antisense, 5′-UCU-UCA-UGG-CCU-UGU-GCA-G-dTdT-3′, targeting 5′-CUG-CAC-AAG-GCC-AUG-AAG-A-3′. The 2-O-methyl (2′OMe) siRNA for the luciferase was similar to the unmodified siRNA except that the uridines in the sense strand had 2-OMe modifications. The control siRNA was siGENOME Non-Targeting siRNA #3, sense 5′-AUG-UAU-UGG-CCU-GUA-UUA-G-dTdT-3′; antisense, 5′-CUA-AUA-CAG-GCC-AAU-ACA-C-dTdT-3′ (Dharmacon, Lafayette, CO).

Gel Retardation Assay

The amount of HK polymer (modified and/or unmodified) to neutralize siRNA was determined by the gel retardation assay. Varying amounts of HK peptides were mixed with 1 μg of siRNA and incubated for 30 minutes at room temperature. Specifically, the following HK:siRNA ratios (w/w or w/w/w) were prepared in water: 1) H3K(+H)4b:siRNA (1:1; 1.5:1; 2:1; 2.2:1; 2.5:1); 2) RGD-PEG-H3K(+H)4b/H2K4b:siRNA and 3) (RGD-PEG-H3K(+H)4b)⁴ /H2K4b:siRNA (3:0.6:1; 4:0.6:1; 6:0.6:1; 3:0.8:1; 4:0.8:1; 6:0.8:1). After the HK siRNA nanoplex was loaded onto the gel (3 % agarose), electrophoresis was carried out at a constant voltage of 75 V for 45 minutes in TBE buffer containing ethidium bromide. The siRNA band densities were then visualized under a UV transilluminator at a wavelength of 365 nm. On the basis of fluorescence (UN-SCAN-IT; Silk Scientific, Orem, UT) of siRNA that had migrated into each lane, the stability of HK siRNA nanoplex was determined. A gel retardation assay was also done on each *in vivo* HK siRNA preparation

Particle size and surface charge

Particle size was measured on all HK nanoplexes by dynamic light scattering (DLS) with the N4 plus particle size analyzer (Beckman Coulter Corp., Miami, FL). The zeta potential was measured by Delsa 440 SX instrument (Coulter) on HK siRNA nanoplexes that were used for *in vivo* studies.

HK:siRNA nanoparticle preparation

For *in vitro* experiments, HK siRNA nanoplexes were prepared as previously described 18 , 19 by briefly mixing siRNA (1 µg) in 50 µl of OptiMEM with various amounts of HK peptides. The siRNA nanoplexes were maintained at room temperature for 30 min prior to size measurements and/or incubation with cells or serum. The ratios for HK to siRNA were based on gel retardation assays with additional ratios tested for *in vitro* bioluminescent assays.

For tumor xenografts experiments *in vivo*, mice were treated by injection in the tail vein with HK nanoplexes containing 40 μg of luciferase or control siRNA. After the polymers were mixed with the siRNA, the resulting nanoplex formed at room temperature for 40 minutes. Each mouse was then treated by i.v. injection with 300 μl of the nanoplexes. The ratios of polymers to siRNA for *in vivo* bioluminescent studies were based on the gel retardation and particle size measurements.

Stability of HK nanoplexes in Serum

With one microgram of siRNA in complex with the optimal amount of unmodified $H3K(+H)4b$ or the two modified cRGD-PEG $H3K(+H)4b$ peptides, the nanoplexes (2 µl) were incubated with increasing concentrations (0%, 10%, 50% and 75%) of mouse serum (total volume 10 μl) for 1 h at room temperature. The gel retardation assay was used to test the stability of the nanoplexes in serum.

Cellular Uptake

Cells (1×10^5) were incubated with different carriers (H3K(+H)4b, (RGD-PEG)-H3K(+H)4b/H2K4b, or (RGD-PEG)⁴H3K(+H)4b/H2K4b) in complex with Cy3 labeledsiRNA (IDT, Coralville, IA). Four hours later, cells were fixed in formaldehyde for 5 min; the nuclei were stained with chromatin dye Hoechst 33342 (Invitrogen, Carlsbad, CA) in PBS for 5 min. Confocal images were obtained with Zeiss LSM510 laser scanning confocal microscope (Carl Zeiss, Thornwood, NY).

In vitro **bioluminescence assays**

MDA-MB-435 cells expressing luciferase were plated in a 24-well plate (0.5 ml of DMEM, 10% serum) at a density of 3×10^4 cells/well. Various peptides and peptide combinations (H3K(+H)4b, (RGD-PEG)-H3K(+H)4b, (RGD-PEG)⁴ -H3K(+H)4b, (RGD-PEG)- $H3K(+H)4b/H2K4b$, and $(RGD-PEG)^4-H3K(+H)4b$, in complex with Luc-siRNA (1 µg), were prepared as described previously, and nanoplexes were incubated with MDA-MB-435 cells for 48 h. The HK to siRNA ratios that were tested for *in vitro* bioluminescent experiments were as follows: H3K(+H)4b:siRNA, 2.2:1, 4:1, 6:1; (RGD-PEG)-H3K(+H)4b, 2:1, 4:1, 6:1; (RGD-PEG)⁴ -H3K(+H)4b, 2:1, 4:1, 6:1; (RGD-PEG)-H3K(+H)4b/H2K4b, 2:0.8:1, 3:0.8:1; 6:0.8:1; (RGD-PEG)⁴-H3K(+H)4b/H2K4b, 2:0.8:1, 4:0.8:1, 6:0.8:1. The cells were then exposed to lysis buffer (200 μl) (Promega, Madison, WI) followed by

centrifugation at 12,500 rpm for 5 min. The luciferase activities in the supernatant fraction were measured by a Turner TD 20/20 luminometer (Promega).

In vivo **bioluminescence experiments**

- **a.** Tumor lysates: MDA-MB-435 xenografts that stably expressed luciferase were established by injecting 2×10^6 cells into midclavicular line of female nude mice (NCI Frederick). After tumor reached about 50 mm³, mice were separated into five treatment groups: untreated, H3K(+H)4b/Luc siRNA (w/w, 2.2:1), (RGD-PEG)H3K(+H)4b/H2K4b/Luc siRNA (w/w/w, 3:0.8:1), and (RGD- $PEG)^{4}H3K(+H)4b/H2K4b/Luc$ siRNA or control siRNA (w/w/w, 4:0.8:1). These HK nanoplexes containing 40 μg of siRNA were administered via the tail veins. Forty-eight hours after inoculation of the nanoplexes, the mice were euthanized and luciferase activity was then measured in tumor homogenates. After determining the most effective carrier, time course and 2′OMeLuc siRNA experiments were performed in a similar manner. Tumor volume was determined using the formula $1/2 \times \text{length} \times \text{width}^2$.
- **b.** Bioluminescence Imaging: Protocol for preparation and inoculation of HK siRNA nanoplexes in tumor- bearing mice were similar to tumor lysate experiments except that the IVIS-200 optical imaging system (Xenogen Corp., Almeda, CA) measured tumor luciferase activity in real-time in living mice. At the time of imaging, mice were anesthetized with a 2.5% isofluorane/oxygen mixture and injected i.p. with 150 mg/kg of D-Luciferin (Caliper LifeSciences, Hopkinton, MA); photon emission was measured 15 min after the administration of luciferin. To normalize the photon emission (i.e., RLU), the region of interest at times 0 and 48 h were of equal size.

Cytokine Measurements

A multiplex bead-based assay using Luminex technology was used to measure serum levels of mouse INF-γ, TNF- α, and IL-6 as described by manufacturer (Upstate Waltham, MA). Levels of mouse INF-α were measured with an ELISA kit as described by the manufacturer (PBL Biochemical Laboratories, Piscataway, NJ). These assays were done by the cytokine core facility at the University of Maryland School of Medicine.

Statistics

Results comparing multiple groups were analyzed by one-way analysis of variance followed by Bonferoni test (Sigma Plot, 11.0). Student t-test was used, where appropriate, for pairwise comparisons. Values shown represent means, and error bars represent standard deviation. In all cases, differences were considered to be statistically significant when the P values were <0.05.

Results

Optimization of HK-siRNA Nanoplexes

To determine appropriate HK and siRNA ratios for *in vivo* studies, gel retardation assays 20–22 and particle size measurements using dynamic light scattering (DLS) were used to facilitate development of siRNA nanoplexes. Moreover, we have previously found that plasmid nanoplexes formed with HK peptides that were approximately 100 to 150 nm in size were effective in transfection of tumor xenografts 23 . Therefore, we examined various ratios of HK to siRNA to determine the minimal amount of HK that would form nanoplexes retaining approximately 90% or more of the siRNA in the loading well and that would result in a nanoplex with a diameter of 150 nm or less (Figure 1). For H3K(+H)4b, the lowest ratio

to retard siRNA and still be associated with the smallest particle size was $2.2:1$ (w/w) (N/P ratio, 2.7:1). At this ratio, about 92% of the siRNA was retarded and the size of the siRNA nanoplex was 149 ± 41 nm. In contrast to the unmodified H3K(+H)4b, both modified HK were unable to retard siRNA, even at very high ratios (i.e., 7:1, N/P). Moreover, at any ratio of the modified HK polymers to siRNA, the particle size of the siRNA nanoplex could not be determined by DLS (data not shown). As a result, we combined an unmodified H2K4b peptide that has a high lysine content and greater condensing properties with the modified H3K(+H)4b polymers to enable greater siRNAbinding. For the modified polymer with only one cRGD-PEG conjugated to its core, the optimal (RGD-PEG)-H3K(+H)4b/H2K4b/siRNA ratio was 3:0.8:1 (w/w/w; N/N/P ratio, 3:1:1); this ratio resulted in 99% retardation of the siRNA and a nanoparticle size of 147 ± 51 nm. For the highly modified HK, the selected (RGD-PEG)⁴ -H3K(+H)4b/H2K4b/siRNA ratio was 4:0.8:1 (w/w/w; N/N/P ratio 2.7:1:1), the minimum amount of HK polymer to produce a stable nanoplex. These selected ratios for unmodified and modified polymers to siRNA were used in subsequent experiments although additional ratios were also evaluated for *in vitro* gene silencing experiments. At these selected ratios, nanoplexes containing the $H3K(+H)4b$, (RGD-PEG)-H3K $(+H)4b$, and $(RGD-PEG)^4-H3K(+H)4b$ had zeta potentials of 37, 17.3, and 16.7 mV, respectively. Notably, the amount of H2K4b used in siRNA nanoplexes that also incorporated modified H3K(+H)4b was not sufficient to neutralize the negatively charged siRNA; the H2K4b:siRNA ratio of 0.8 to 1 (w:w) retained only 35% of the siRNA in the gel retardation assay (data not shown).

In vitro **comparison of siRNA nanoplexes with cRGD-HK conjugates**

We also tested the ability of unmodified and modified HK siRNA nanoplexes to downregulate luciferase stably expressed in MDA-MB-435 cells. Of note, MDA-MB-435 cells have elevated levels of the $\alpha_v \beta_3$ integrin, the receptor for RGD ²⁴. The unmodified H3K(+H)4b or the two modified H3K(+H)4b with and without H2K4b were used as carriers of a luciferase-targeting siRNA *in vitro*. Unmodified H3K(+H)4b nanoplexes inhibited luciferase activity by approximately 90%, while the nanoplexes containing only modified HK peptides had minimal activity (Fig. 2a). In addition, the nanoplexes with the modified HK combined with H2K4b had no activity across several HK:siRNA ratios. These functional siRNA assays correlated with fluorescent uptake studies. We observed discrete intracellular particles in cells treated with unmodified H3K(+H)4b siRNA nanoplexes while we found a weak diffuse fluorescence pattern in cells treated with the siRNA control or modified HK siRNA nanoplexes (Fig. 2b). Over a range of time periods (1 to 8 hr) in which the siRNA was incubated with the cells, there was no discernable difference in the intracellular fluorescent patterns between siRNA control and the modified HK siRNA nanoplexes—that is, weak to no intracellular accumulation occurred in these groups (data not shown).

In vivo **evaluation of HK polymers as carriers of Luc siRNA**

Similar to the *in vitro* study, we screened numerous HK polymers in complex with Luc siRNA for their ability to inhibit luciferase in tumor xenografts. After MDA-MB-435 tumors expressing luciferase grew to approximately 50 mm^3 , the mice were divided into various treatment groups and treated by injection with the different HK Luc siRNA nanoplexes. Forty-eight hours later, the mice were euthanized and the tumor lysates were evaluated for luciferase activity. The group treated with $(RGD-PEG)^{4}H3K(+H)4b/H2K4b$ in complex with Luc siRNA was the most effective in silencing the tumor luciferase activity (Fig. 3), with activity reduced by about 75% (P< 0.01; (RGD-PEG)⁴H3K(+H)4b/H2K4b vs. other carriers and control groups). The unmodified $H3K(+H)4b$ and (RGD-PEG)- $H3K(+H)4b$ H2K4b nanoplexes reduced tumor luciferase activity by 18 and 35%, respectively ($P < 0.05$; (RGD-PEG)-H3K(+H)4b/H2K4b vs. unmodified H3K(+H)4b or untreated). Thus, the

highly modified HK nanoplex formulation was the most effective. To determine whether reduction of tumor luciferase was based on the specificity of the siRNA mechanism, a nontargeting siRNA in complex to the most effective carrier, $(RGD-PEG)^4$ -H3K(+H)4b/ H2K4b, was used as the negative control *in vivo*. There was approximately 20% inhibition for the non-targeting siRNA nanoplex, suggesting that the Luc siRNA specifically inhibited luciferase expression.

We also confirmed the tumor lysate studies with the Xenogen optical imaging system and demonstrated that highly modified H3K(+H)4b nanoplexes significantly suppressed luciferase activity in tumor xenografts (Fig. 4). Mice treated with the highly modified H3K(+H)4b-H2K4b combination in complex with Luc-siRNA had decreased luciferase activity in tumors of $63.14\% \pm 15.18$ compared to luciferase activity of tumors in untreated mice (P = 0.01, n = 3). For untreated mice, the RLU was $7.47 \pm 1.71 \times 10^5$ at time 0, and 9.43 $\pm 2.33 \times 10^5$ 48 h later, whereas for treated mice, the RLU was 7.78 $\pm 1.90 \times 10^5$ at time 0, and 3.08 \pm 0.59 \times 10⁵ at 48 h. The regions of interest at time 0 and 48 h for RLU determinations were equal in size.

Time Course of siRNA-mediated luciferase inhibition *in vivo*

To determine the duration of Luc silencing in the MDA-MB-435 xenografts, a time course was done with the most effective nanoplex, (RGD-PEG)⁴-H3K(+H)4b/H2K4b/Luc siRNA. After HK-siRNA nanoplex injection, inhibition of luciferase activity was 71% at 24 h, 75% at 48 h, and 46% at 72 h compared to untreated controls (Fig. 5). These findings suggest that the optimal time interval for dosing may be about 3 days for rapidly dividing tumor cells to obtain maximum tumor growth inhibition ^{6, 25, 26}.

HK siRNA Polyplexes do not induce cytokine response

Cationic carriers in complex with siRNA can induce cytokines which in turn can result in cellular toxicity and/or inhibit gene expression in tumors by an indirect mechanism $27-30$. Thus, luciferase activity may be reduced due to intra-tumoral cytokine induction and tumor cell apoptosis, non-specific mechanisms other than siRNA-mediated gene silencing. To minimize cytokine induction by the siRNA nanoplex *in vivo*, the sense strand of the siRNAcan be modified by cautious addition of a methyl group to the 2′-hydroxyl group of the ribose without significantly affecting the biological activity of the siRNA ³¹. In (RGD-PEG)⁴-H3K(+H)4b/H2K4b nanoplexes, a 2'O-methylated Luc siRNA was compared to unmodified Luc siRNA. If cytokine induction resulted in a non-specific cytotoxic effect from the nanoplexes, then the unmodified siRNA nanoparticle would likely be more effective at reducing luciferase activity compared to the 2′-OMe luciferase nanoparticle. As shown in Fig. 6a, however, there were no significant differences between the unmodified and 2′-OMe siRNAtumor-bearing treatment groups; the decrease in luciferase activity was 80% in the 2-OMe siRNA group vs. 75% in the unmodified siRNA group. Furthermore, the HK in complex with siRNA (unmodified or 2′-OMe modified) did not induce higher cytokine levels (IL-6, INF- α , INF- γ , and TNF- α) compared to the untreated groups (Fig. 6b). The cytokine levels in three groups were very low in comparison to DOTAP liposomal siRNA complexes, particularly for INF- α (INF- α , 754 pg/ml). Together, these data indicate that modified HK siRNA nanoplexes administered i.v. did not increase the level of cytokines in mice and cytokine induction by the HK siRNA nanoparticles did not have a significant role in decreased expression of luciferase in the tumors.

Nuclease Assay

The integrity of HK:siRNA polyplex may be sensitive to the serum components *in vivo* ³². Pegylated polymers may augment the stability of the polyplex, by reduced binding of serum components. To investigate their stability in mouse serum, HK nanoplexes were incubated

in the presence of varying amounts of serum for one hour at room temperature and then analyzed by gel electrophoresis (3% agarose). As shown in Table 1, increased dissociation of siRNA was observed from all carriers as the serum concentration was increased to 50% and above. Among the nanoplexes, the unmodified H3K(+H)4b siRNA nanoplexes were less stable than the modified HK nanoplexes. There was little difference in the stability in serum between the two modified HK nanoplexes suggesting that there may be other factors (e.g., number of cRGD) that affect their ability to silence their targets *in vivo*.

Discussion

To develop more effective carriers of siRNA, we compared two ligand modified HK peptides with an unmodified HK peptide. The two cRGD-PEG HK peptides differed in the number and location of cRGD-PEG conjugates on the polymer. One highly modified HK polymer with a cRGD-PEG conjugated to each branch was made that we thought would have greater tumor uptake and selectivity. Nevertheless, we were concerned that such a modification on each branch might interfere with binding to siRNA. To investigate this, an HK peptide with only one cRGD-PEG attached to its core was prepared and was expected to bind siRNA more effectively because the branching arms were not modified. Surprisingly, neither modified HK polymers by themselves effectively retarded siRNA, even at elevated N/P ratios (7:1). This data, together with the inability to determine their particle size by DLS, suggest that a stable nanoparticle was not formed.

Nevertheless, combining modified H3K(+H)4b with unmodified H2K4b when mixed with siRNA did form stable nanoparticles that could effectively silence their target *in vivo*. Because H2K4b alone previously was not an effective carrier of siRNAin silencing its targets¹⁸ and reduced amounts of H2K4b were used to form the nanoplex, it is likely that H2K4b has a supportive role in forming the nanoplex, but not a primary role in the siRNA nanoplex silencing role of the target. H2K4b was selected as a helper peptide because of its high content of lysines and its greater ability to condense nucleic acids compared to other HK peptides. It will be interesting to test nanoplexes using other unmodified HK peptides (i.e., H3K(+H)4b) that are significantly more effective as carriers of siRNA, even though they are less efficient in condensing nucleic acids compared with H2K4b. The data in this study are consistent with the notion that H2K4b binds tightly with siRNA and provides a central nidus to which the modified H3K(+H)4b then binds. Such a model is similar to what the results shown by Kim et al. with their carrier siRNA complexes. In that model, although the pegylated siRNA did not effectively silence its cellular target, a combination of PEI with the targeted PEGylated siRNA was effective; PEI was posited to form the central core and stabilize the siRNA nanoplex $8, 20$. Although the modified and unmodified HK peptides were mixed together before addition of the siRNA, we plan in future studies to determine whether sequential addition of H2K4b first to the siRNA, followed by the modified H3K(+H)4b might increase the efficacy of the carrier.

Moreover, since both cRGD-PEG modifications of H3K(+H)4b did not form an effective or a defined siRNA nanoparticle without the addition of an unmodified HK polymer (i.e., H2K4b), it is unclear whether any PEG modifications to the H3K(+H)4b polymer will result in a stable siRNA nanoplex. If binding alone were the sole determinant, we would expect that the singly modified H3K(+H)4b would form a more stable and defined particle, but there was no evidence to support this. Consequently, there may be other factors in addition to modification of $H3K(+H)4b$ that interferes with its binding with siRNA. For example, PEGylation of HK may interfere not only with binding, but also with the self-assembly of the nanoparticle; this may explain why unmodified HK peptides were needed to form stable nanoplexes. Of course, neither interference with binding nor nanoplex formation is mutually exclusive, but it is certainly plausible that the role of these mechanisms may vary with the

In contrast to most carriers *in vivo* that were identified from the most promising carriers *in vitro*, we found in this study that the most effective HK carrier *in vitro* was not the optimal carrier *in vivo*. Of the HK investigated, unmodified H3K(+H)4b was the most effective carrier *in vitro*, whereas the modified H3K(+H)4b/H2K4b carrier of siRNA had no observed silencing activity in cell culture experiments. In contrast, the silencing efficiency by siRNA in tumor xenografts was significantly greater with the modified HK nanoplexes *in vivo* and correlated with the number of cRGD-PEG per HK. Increased multivalency based on the ligand conjugated to the drug or complex is known to augment internalization $33,34$ and this provides the likely rationale for greatest activity by the highly modified $H3K(+H)4b$ nanoplex *in vivo*. It is not completely clear why efficient silencing of luciferase was observed *in vivo* but not *in vitro* with the modified HK nanoplexes. Although the literature is consistent with our results that PEGylation of the nanoplex may decrease uptake *in vitro* and enhance accumulation of the nanoplex within the tumor tissue, addition of cell-specific ligands such as cRGD to PEG usually augments uptake of nanoplexes not only *in vivo* but also *in vitro* 12, 35–39. Indeed, previous groups have found that cRGD conjugated nanoparticles (with or without PEG) selectively targeted $\alpha_{\nu}\beta_3$ integrins on the cell surfaces of MDA-MB-435 cells *in vitro* and *in vivo* 35, 36, 40–42. Although modification of H3K(+H)4b with cRGD-PEG did not enhance uptake or silencing with siRNA *in vitro*, the *in vivo* results demonstrating down-regulation of luciferase in tumors formed by MDA-MB-435 cells suggest that modification of HK greatly augmented silencing activity of the siRNA nanoplex. This is further bolstered by our finding that similarly modified HK were effective and specific carriers of luciferase-expressing plasmids to MDA-MB-435 tumor xenografts compared to other tissues (data not shown). Although it is common to observe carriers that are ineffective *in vivo* that were effective *in vitro*, there are few other studies 43–45 demonstrating that more efficient carriers *in vivo* were ineffective *in vitro*. The importance of this observation is that it suggests that until alternative screening methods to evaluate carriers are developed for *in vivo* models, it is likely many other carriers that are particularly effective *in vivo* will never be identified.

Delivery remains the major obstacle to achieving meaningful RNAi silencing. Consequently, our primary goal in this study was to develop a more effective carrier of siRNA to tumor xenografts. Previously, we determined that unmodified H3K(+H)4b in complex with a Raf-1 siRNA inhibited tumor size by approximately 60% after five injections 19. On the basis of the current results, we anticipate that the (RGD- PEG ⁴H3K(+H)4b/H2K4b combination will be significantly more effective carrier than the unmodified carrier for siRNA in targeting oncogenes of tumor xenografts. Furthermore, the silencing of luciferase by the cRGD-targeted HK siRNA nanoplex appears to be specific, as evidenced by the minimal silencing by the control siRNA and low induction of cytokines by the HK siRNA nanoparticle.

Our silencing tumor xenograft model examined whether targeted HK siRNA polyplexes could effectively traversed the endothelial cell barrier to silence luciferase expressed by tumor cells. Nevertheless, it is likely that the cRGD HK siRNA polyplexes will also target the more readily accessible $\alpha_v \beta_3$ -expressing endothelial cells of tumors. In addition to cyclic RGD peptides, other tumor-selective ligands could be conjugated to the HK peptides to target tumor cells and silence their oncogenes 46. Although the efficacy of cRGD-PEG targeted HK as a carrier of siRNA targeting tumors and angiogenesis requires further validation, the studies thus far have indicated that modified HK is a promising candidate for systemic delivery of siRNA.

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Abbreviations

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Ratio of HK to siRNA

Fig. 1. Gel Retardation Assay

To determine the amount of HK that retards siRNA migration, various ratios of unmodified H3K(+H)4b (a) or modified HK combinations (b, (RGD-PEG)-H3K(+H)4b/H2K4b; c, $(RGD-PEG)^4-H3K(+H)4b/H2K4b$) in complex with siRNA (1 µg) were prepared and then subjected to gel electrophoresis for 30 minutes (3% gel). Different ratios of HK polymers to siRNA are represented above the gel and the particle size is shown below the gel. For the modified HK groups (b,c), modified and unmodified polymers (H2K4b) were mixed for more complete retardation of siRNA. The ratio enclosed in the box represents the selected *in vitro* and *in vivo* silencing conditions based on the size of the particle (less than 150 nm) and siRNA retardation. NA represents nanoparticles in which the size could not be determined by dynamic light scattering.

(a) Several HK or combination of HK carriers (H3K(+H)4b, (RGD-PEG)H3K(+H)4b, $(RGD-PEG)^4H3K(+H)4b$, $(RGD-PEG)H3K(+H)4b/H2K4b$, $(RGD-PEG)^4H3K(+H)4b$ H2K4b) of Luc siRNA were tested for their abilities to inhibit luciferase expression in MDA-MB-435 cells compared with the untreated group. H3K(+H)4b was the most effective carrier down- regulating expression by nearly 90%, whereas inhibition by other carriers was negligible. The data represent the mean \pm SD of luciferase of six determinations for each carrier. $*, P < 0.01$; H3K(+H)4b vs. modified HK carriers. (b) Comparison of uptake of different HK siRNA nanoplexes. A number of discrete intracellular fluorescent particles of siRNA were observed with unmodified H3K(+H)4b carriers, whereas the combination of modified and unmodified HK siRNA nanoplexes showed diffuse intracellular fluorescencesimilar to the fluorescence pattern observed with the siRNA alone. Images were obtained by a Zeiss LSM510 laser scanning confocal microscope. The HK to siRNA ratios were as follows: H3K(+H)4b:siRNA, 4:1; (RGD-PEG)-H3K(+H)4b, 4:1; (RGD-PEG)⁴-H3K(+H)4b, 4:1; (RGD-PEG)-H3K(+H)4b/H2K4b, 3:0.8:1; (RGD-PEG)⁴ -H3K(+H)4b/H2K4b, 4:0.8:1.

Treatment Group

Fig. 3. *In vivo* **evaluation of HK polymers to determine most effective carrier for Luc-siRNA** Four HK siRNA preparations (three HK-Luc siRNA; one HK-control siRNA) were compared for their ability to silence luciferase expression in MDA-MB-435 xenografts. The modified HK peptide, (RGD-PEG)⁴H3K(+H)4b/H2K4b, of Luc siRNA was the most effective, reducing luciferase expression in tumor xenografts by 75%. HK:siRNA ratios used in this experiment were based on the gel retardation assays. The data represent the mean \pm SD of luciferase of six determinations for each carrier. *, P< 0.01; (RGD-PEG)⁴H3K(+H)4b/H2K4b carrier vs. other carriers and control groups.

Fig. 4. Bioluminescence Imaging

Bioluminescence imaging was performed with the Xenogen IVIS 200 system. Mice bearing tumor xenografts were separated into two groups after the tumor size reached 50 mm³ and this experiment was repeated three times. (a) and (b) show tumor images of representative mice taken before treatment and 48 h after treatment, respectively. The mouse on the right in (a) and (b) was untreated; the mouse on the left of (a) and (b) was treated with (RGD- PEG ⁴H3K(+H)4b/H2K4b/Luc siRNA nanoplex (designated HK/Luc siRNA) by tail vein injection. The mouse treated with siRNA showed a marked down-regulation of luciferase. (c) shows the mean of the experiments comparing untreated mice with treated mice (n=3). In mice treated with luciferase siRNA, luciferase activity was reduced by $63.14 \pm 15.18\%$. $*$, P $= 0.01$; siRNA treated vs. untreated.

Fig. 5. Time course of siRNA induced luciferase activity reduction

Tumor-bearing mice were injected with the optimal HK-Luc siRNA nanoplex and luciferase activity was determined from tumor lysates at 24, 48, or 72 h. Compared to activity before treatment, luciferase activity was down-regulated by 71%, 75% and 46% at 24 h, 48 h, and 72 h respectively. *, P< 0.05; 72 h vs. 24 and 48 h time point. The data for each time point represent the mean \pm SD of luciferase.

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Fig. 6. Effect of induced cytokines on luciferase activity

(a) Unmodified and 2′OMeLuc siRNA in complex with the optimal HK combination were compared for their ability to reduce luciferase activity in tumor xenografts. The reduction in luciferase activity was similar in the two groups (75% with unmodified vs. 80% with 2′OMeLuc siRNA), indicating that silencing was not due to induction of cytokines. The data represent the mean \pm SD of luciferase activity of five determinations for each carrier. $*$, P < 0.01; siRNA treated vs. untreated. (b) Serum cytokine levels in MDA-MB-435 bearing mice were measured in untreated, optimal HK-Luc siRNA and optimal HK-2′O Me-Luc siRNA treatment groups. No differences were detected in the cytokine levels among the different treatment groups.

Table 1

Stability of HK siRNA nanoplexes in Serum

Unmodified H3K(+H)4b and modified H3K(+H)4b/H2K4b carriers in complex with siRNA were incubated at various concentrations of mouse serum (0%, 10%, 50% and 75%) for 1 hr. Gel retardation was then used to measure the stability of the nanoplexes as described in the Methods section. Compared to unmodified H3K(+H)4b siRNA nanoplexes, the two pegylated HK nanoplexes had greater stability at high serum concentration (50%, 75%);

*** , P < 0.01. The data represent the mean ± SD of measurement of 3 determinations for each carrier.

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