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# Association of Hip Strength Estimates by Finite Element Analysis with Fractures in Women and Men

Shreyasee Amin<sup>1,3</sup>, David L. Kopperdhal<sup>6</sup>, L. Joseph Melton III<sup>2,3</sup>, Sara J. Achenbach<sup>4</sup>, Terry M. Therneau<sup>4</sup>, B. Lawrence Riggs<sup>2</sup>, Tony M. Keaveny<sup>5,6</sup>, and Sundeep Khosla<sup>2</sup>

Shreyasee Amin: amin.shreyasee@mayo.edu; David L. Kopperdhal: david.kopperdahl@ondiagnostics.com; L. Joseph Melton: melton.j@mayo.edu; Sara J. Achenbach: achenbach@mayo.edu; Terry M. Therneau: therneau@mayo.edu; B. Lawrence Riggs: riggs.lawrence@mayo.edu; Tony M. Keaveny: tmk@me.berkeley.edu; Sundeep Khosla: khosla.sundeep@mayo.edu

<sup>1</sup>Division of Rheumatology, Department of Internal Medicine, Mayo Clinic, Rochester, MN

<sup>2</sup>Division of Endocrinology, Metabolism and Nutrition, Department of Internal Medicine, Mayo Clinic, Rochester, MN

<sup>3</sup>Division of Epidemiology, Department of Health Sciences Research, Mayo Clinic, Rochester, MN

<sup>4</sup>Division of Biomedical Statistics and Informatics, Department of Health Sciences Research, Mayo Clinic, Rochester, MN

<sup>5</sup>Departments of Mechanical Engineering and Bioengineering, University of California, Berkeley, CA

<sup>6</sup>O.N. Diagnostics, Berkeley, CA

# Abstract

Finite element (FE) analysis of quantitative computed tomography (OCT) scans can estimate sitespecific whole bone strength. However, it is uncertain whether the site-specific detail included in FE-estimated proximal femur (hip) strength can determine fracture risk at sites with different biomechanical characteristics. To address this question, we used FE analysis of proximal femur OCT scans to estimate hip strength and load-to-strength ratio during a simulated sideways fall, and measured total hip areal and volumetric bone mineral density (aBMD and vBMD) from QCT images, in an age-stratified, random sample of community adults, age  $\geq$  35 years. Among 314 women (mean age  $\pm$  SD: 61  $\pm$  15 years; 235 postmenopausal) and 266 men (62  $\pm$  16 years), 139 women and 104 men had any prevalent fracture, while 55 women and 28 men had a prevalent osteoporotic fracture that had occurred age  $\geq$  35 years. Odds ratios by age-adjusted logistic regression analysis for prevalent overall and osteoporotic fractures each were similar for FE hip strength and load-to-strength ratio, as well as total hip aBMD and vBMD. C-statistics (estimated areas under ROC curves) were also similar (e.g., 0.84-0.85 [women] and 0.75-0.78 [men] for osteoporotic fractures). In women and men, the association with prevalent osteoporotic fractures increased below an estimated hip strength of ~3000 N. Despite its site-specific nature, FEestimated hip strength worked equally well at predicting prevalent overall, and osteoporotic, fractures. Furthermore, an estimated hip strength below 3000 N may represent a critical level of systemic skeletal fragility in both sexes that warrants further investigation.

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Please address correspondence to: Dr. Shreyasee Amin, Division of Rheumatology, Mayo Clinic, 200 First Street SW, Rochester, MN 55905. Telephone: (507)-284-4277, Fax: (507)-284-0564, amin.shreyasee@mayo.edu.

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Keywords

finite element analysis; fractures; bone density; quantitative computed tomography; hip; proximal femur

### INTRODUCTION

There has been growing interest in the role of enhanced biomechanical analyses to improve fracture prediction. Quantitative computed tomography (QCT)-based finite element (FE) models mechanistically integrate all relevant bone density and geometry information from QCT scans to provide an estimate of whole bone strength, and such strength estimates have been used now by several groups in the study of osteoporosis and fracture risk (1–5), especially for the proximal femur (6–13). Proximal femur (hip) strength, as estimated by FE analyses, is of particular interest since hip fractures account for the greatest morbidity, mortality and cost of any fracture in both women and men (14). Furthermore, FE-estimated hip strength, when combined with estimated loads to the hip from a sideways fall (i.e., load-to-strength ratio), may offer improved hip fracture prediction (11).

However, all fractures, including osteoporotic fractures at skeletal sites other than the hip, generate a substantial socioeconomic burden (15,16). Currently, areal bone mineral density (aBMD) at the hip by dual-energy X-ray absorptiometry (DXA) is the assessment site and mode of choice in the osteoporotic fracture prediction model (FRAX<sup>®</sup>) developed by the World Health Organization (17). Even though BMD at the hip may be useful in fracture prediction at non-hip sites, it remains possible that estimates of hip strength from QCTbased FE models may not be. Certain characteristics captured by a FE model of the proximal femur, such as overall bone size, may represent a common trait across bones at different anatomic sites; however, other features, such as three-dimensional proximal femur shape, bone density and spatial distribution are likely to be biomechanically relevant only at the hip. Furthermore, the typical traumatic loading conditions, a sideways fall on the hip, are clearly specific to hip fracture. Thus, it is uncertain whether FE-derived estimates of hip strength, or load-to-strength ratio at the proximal femur, will be equally useful at estimating fracture risk at diverse skeletal sites with widely varying biomechanical and traumatic loading characteristics. If this potential limitation is not realized, then these FE-estimated strength measures generated at the hip may be of further potential clinical utility and would require additional study; otherwise, this limitation needs to be acknowledged and attention should remain focused instead on hip-specific fracture prediction from these FE models.

Our goal was to examine the ability of bone strength estimates by FE analysis, and the loadto-strength ratio, determined at the proximal femur, to predict prevalent overall and osteoporotic fractures in an age-stratified random community sample of adult women and men and to compare these findings with results using total hip aBMD and volumetric BMD (vBMD) measurements.

### **METHODS**

#### Study subjects

Subjects were participants in a population-based cohort study of bone health where bone imaging was performed in all subjects and fracture history was documented at their initial study visit. Following approval by Mayo Clinic's Institutional Review Board, 375 women and 325 men were recruited from age-stratified random samples of Rochester, Minnesota women and men, as previously described (18). Over half of the Rochester population is seen annually at some Mayo Clinic facility, and almost all are seen at least once in any three-year

period. Thus, the enumerated population (Rochester women seen in  $2001 \pm 1$  year and men seen in  $2002 \pm 1$  year) approximates the underlying population of the community, including both free-living and institutionalized individuals. All but 5 women and 12 men were white, reflecting the ethnic composition of the population (90% white in 2000). There were 127 premenopausal women (mean age  $\pm$  SD,  $38 \pm 9$  years; range, 21 to 55 years) and 248 postmenopausal women ( $68 \pm 12$  years; range, 39 to 97 years); the men ( $57 \pm 19$  years) ranged in age from 22 to 93 years. As we were interested in the association with prevalent fractures that would have occurred in adulthood, we restricted this analysis to those subjects  $\geq$  35 years of age at the initial study visit. Excluding 13 women and 8 men who did not have a measure of FE-estimated proximal femur strength, we therefore studied the remaining 314 women ( $61 \pm 15$  years), of whom 235 were postmenopausal, and 266 men ( $62 \pm 16$  years).

### Bone density assessments

Total hip vBMD measurements were made by single energy QCT using a multidetector Light Speed QX/i scanner (GE Medical Systems, Milwaukee, WI; slice thickness, 2.5 mm and in-plane pixel dimension,  $0.74 \times 0.74$  mm). Calibration standards scanned with the subject were used to convert CT numbers directly to equivalent vBMD (mg/cm<sup>3</sup>), and the correlation between bone density determined by our image processing algorithm and that of the European Spine Phantom was 0.998. We also used the QCT images to estimate total hip aBMD measurements using a software program (Version 3.1, Mindways Software Inc, Austin TX). A direct comparison of this equivalent QCT-derived measure of aBMD with a DXA-measured value was possible for 260 subjects for whom QCT and DXA scans (Lunar Prodigy, GE Medical Systems, Milwaukee, WI) were both available at a later date, and these data confirmed the validity of the QCT-derived measure (R<sup>2</sup>=0.93) [unpublished data].

#### Proximal femur strength and load-to-strength ratio

To estimate proximal femur strength, and as described in detail elsewhere (8,9,11), each QCT scan was converted into a three-dimensional FE model of the proximal femur, using 1.5 mm cube-shaped "voxel" 8-noded finite elements, in which the local material properties of cortical and trabecular bone were assigned from the spatially-varying calibrated Hounsfield units from the QCT scan using empirically-derived relations (19-21). Each subject-specific FE model was then virtually loaded to failure in simulation of an unprotected sideways fall with impact on the greater trochanter. Non-linear analyses were used in these simulations, assuming a modified von Mises-type failure criterion for the bone tissue in which the bone was stronger in compression than tension. Models were loaded to an overall deformation of 4% nominal strain in a sideways fall configuration, and the strength was taken as the maximum force from the overall force-deformation curve of the whole bone. Laboratory experiments on 76 elderly cadavers loaded in a sideways fall configuration at high speed have shown a strong correlation (R<sup>2</sup>=0.78, Y=X type correlation) between such estimates of proximal femur strength and direct measures from biomechanical testing (22).

To determine the load-to-strength ratio at the proximal femur, we related estimated loads experienced in a sideways fall to the bone strength derived from the FE models. Each subject's specific body mass and height information was used to estimate the in-vivo impact force, using biomechanical theory, for a simulated sideways fall with impact directly on the greater trochanter (9,11,23). A constant value of trochanteric soft tissue thickness (25 mm) was used for all subjects. Because subject-specific values of trochanteric soft tissue thickness were not measured in this study, we assumed the same value for all subjects. Further, because we did not have average values of trochanteric soft tissue tissues for the different sexes for this cohort, rather than assume average values from the literature (24,25) and perhaps introduce an unknown degree of bias, we opted instead to use the same values

of trochanteric soft tissue thickness for both women and men and in that way remove this variability from influencing results.

Proximal femur strength and load-to-strength ratio estimates by FE analyses were determined blinded to prevalent fracture status of the subjects.

### Fracture ascertainment

Based on self-report and subsequent review of complete (inpatient and outpatient) community medical records, we documented fractures that had occurred at any skeletal site at age 35 years or thereafter as of the time of each study subject's imaging studies (prevalent fracture). From all fractures identified, the subset of *osteoporotic fractures* was then defined as fractures of the proximal femur, lumbar or thoracic vertebrae (spine), distal forearm and proximal humerus that had resulted from low or moderate trauma (e.g., fall from a standing height or less) (26).

#### Statistical analysis

Age-adjusted logistic regression models were used to examine the association with prevalent overall and osteoporotic fractures for each measurement of interest: total hip aBMD, total hip vBMD, proximal femur strength by FE analyses and the load-to-strength ratio at the proximal femur. We also examined the c-statistic, which represents the area under the receiver operator characteristic (ROC) curve (AUC), for each logistic regression model. The probability of fracture associated with each measurement was further explored using a generalized additive model and results were graphed using a smoothing function. Analyses were performed using SAS version 9 (SAS Institute, Cary, NC, USA) and Splus (TIBCO Corporation, Palo Alto, CA).

# RESULTS

#### Women

For the 314 women age  $\geq$  35 years, the Pearson correlation between FE-estimated proximal femur strength and total hip aBMD was 0.92 while for total hip vBMD it was 0.93 (p<0.001 for both).

There were 139 of 314 women (44%) who had any prevalent fracture that occurred  $\geq$  age of 35 years, while 55 (18%) had a history of at least one osteoporotic fracture. The cause and distribution of fractures by skeletal site are delineated in Table 1 for women. The median duration from occurrence of first fracture to the time of bone imaging was 12 years (range: 96 days-54 years) for overall fractures and 7 years (range: 75 days to 45 years) for osteoporotic fractures.

As expected, women without a prevalent fracture were younger and had higher total hip aBMD, total hip vBMD, FE-estimated proximal femur strength and lower load-to-strength ratio at the proximal femur than those with fractures (Table 2). The associations between prevalent overall or osteoporotic fracture with each of total hip aBMD, total hip vBMD, FE-estimated proximal femur strength and load-to-strength ratio at the proximal femur were largely similar with respect to the age-adjusted odds ratios and, particularly, the estimated AUCs (Table 3). Our findings remained similar in sensitivity analyses where we restricted our analyses to women age  $\geq$  50 years or to prevalent fractures occurring within 5 years of the QCT scans (data not shown).

#### Men

For the 266 men age  $\geq$  35 years studied, the Pearson correlation between FE-estimated proximal femur strength and total hip aBMD was 0.87 while for total hip vBMD it was 0.89 (p<0.001 for both).

There were 104 of 266 men (39%) who had any prevalent fracture that occurred  $\geq$  age 35 years, while 28 (11%) had a history of at least one osteoporotic fracture. The cause and distribution of these fractures by site are outlined in Table 4 for men. The median duration from occurrence of first fracture to the time of bone imaging was 14 years (range: 83 days to 48 years) for overall fractures and 5 years (range: 178 days to 30 years) for osteoporotic fractures.

Similar to women, men without a prevalent fracture were younger and had higher total hip aBMD and vBMD, FE-estimated proximal femur strength and lower load-to-strength ratio at the proximal femur than those with fractures (Table 5). When we examined the age-adjusted associations between prevalent overall or osteoporotic fracture and each of total hip aBMD, total hip vBMD, FE-estimated proximal femur strength and load-to-strength ratio at the proximal femur, we found that the odds ratios and AUCs were, again, fairly similar (Table 6). For osteoporotic fractures, the odds ratio for total hip aBMD was slightly lower than for the other measurements, but the c-statistic was equivalent across all measures. As in women, our findings remained similar when we restricted our analyses to men age  $\geq$  50 years or to prevalent fractures occurring within 5 years of the scans (data not shown).

#### Differences between women and men

As noted in Tables 2 and 5, women without fractures had higher mean total hip vBMD than men without a fracture history, but lower mean total hip aBMD and proximal femur FEestimated strength, despite being of similar age. Furthermore, women with any prevalent or osteoporotic fracture also tended to have higher mean total hip vBMD values than men with corresponding fracture history, even though women with an osteoporotic fracture were slightly older than men with an osteoporotic fracture. Again, however, the mean total hip aBMD and proximal femur FE-estimated strength were lower in women than men with any prevalent or osteoporotic fractures. In contrast, the load-to-strength ratios at the proximal femur, which were calculated using the same value of trochanteric soft tissue thickness for both sexes, were of similar magnitude for women and men with the same fracture classification.

When we graphically displayed the probability of prevalent osteoporotic fractures in relation to total hip aBMD, total hip vBMD, and proximal femur FE-estimated strength (Figure 1), we noted that for both women and men, there was a steep increase in probability of prevalent osteoporotic fractures below a given threshold of BMD or FE-estimated hip strength. This threshold, however, appeared to be of similar value in both women and men for total hip aBMD and proximal femur FE-estimated strength, but not for total hip vBMD. For example, at a 20% probability of osteoporotic fracture for women vs. men, respectively, total hip aBMD was 0.77 g/cm<sup>2</sup> (95% CI: 0.74, 0.82 g/cm<sup>2</sup>) vs. 0.78 g/cm<sup>2</sup> (95% CI: 0.73, 0.83 g/cm<sup>2</sup>) and FE-estimated proximal femur strength was 3034 N (95% CI: 2804, 3689 N) vs. 3174 N (95% CI: 2717, 3714 N) (Figure 1). In contrast, for the same probability of fracture, women had a higher total hip vBMD, (247 mg/cm<sup>3</sup>, 95% CI: 237, 260 mg/cm<sup>3</sup>) than men, (191 mg/cm<sup>3</sup>, 95% CI: 177, 209 mg/cm<sup>3</sup>) as also shown in Figure 1.

### DISCUSSION

We found that estimates of proximal femur bone strength and load-to-strength ratio derived by FE analysis identify women and men with prevalent overall and osteoporotic fractures

equally well as total hip aBMD, the site frequently used in standard clinical practice (27,28). Thus, even though the FE-based bone strength estimate and load-to-strength ratio were specifically derived for the geometry, spatial density distribution and other biomechanical features unique to the proximal femur, each of these hip-specific biomechanical outcomes provided similar estimates of prevalent fracture risk at all skeletal sites combined, including those traditionally considered osteoporotic, when compared with total hip aBMD or vBMD measures. This is noteworthy because our analysis included only 3 hip fractures (2 in women and 1 in men), where the hip strength estimate would be expected to perform the best. In contrast to fracture site-specific studies of the hip, wrist and spine (3–5,11,29,30), estimating a load-to-strength ratio at the proximal femur was not superior at overall or osteoporotic fracture discrimination. This is not surprising since osteoporotic fractures as a group, as well as fractures generally, are associated with a diverse array of circumstances that may result in traumatic loads very different from the one simulated in this analysis. Nevertheless, the load-to-strength ratio performed comparably well to the other measures.

Interestingly, while the thresholds below which the probability of prevalent osteoporotic fractures increased substantially were similar in women and men for total hip aBMD and FE-estimated proximal femur strength, it was higher for total hip vBMD in women than men. Since aBMD measurements are influenced by size, the larger bone size in men likely accounts for their greater FE-estimated proximal femur strength despite the lower total hip vBMD in men compared with women, as has been previously recognized (30). These data further underscore the underlying differences in bone structure between women and men who fracture (9).

We also demonstrated that for both women and men, proximal femur estimates of strength below ~3000 N were associated with a steep increase in the probability of prevalent osteoporotic fractures. These findings suggest that women and men may have a similar threshold of proximal femur strength below which their risk of osteoporotic fractures in general is substantially increased. Our observations are in keeping with recent findings from a longitudinal prospective study of incident hip fractures in men (MrOS-US) in which all subjects with proximal femur strength estimates < 2900 N fractured over the approximate 5-year follow-up (11). Nevertheless, men with fractures in our cohort had a mean FE-estimated proximal femur strength that was comparable to women who had no fractures. This could be explained if the men with fractures had experienced trauma with higher bone loads. Although the proportion of men with fractures due to severe trauma was no greater than that among the women in our cohort, we do not know the exact loads experienced at time of fracture occurrence. Yet, as demonstrated by our results depicted in Figure 1, when bone strength is low enough (i.e., less than 3000 N) the probability of prevalent fractures increases for both men and women.

A large proportion of all fractures occur among both women and men who are considered "osteopenic" based on aBMD T-scores that lie between -1.0 and -2.5 (31,32). Determination of overall bone strength in these individuals, as estimated from FE models at the hip, may be one way of better distinguishing those with clinically relevant bone fragility (9), particularly if FE-estimated proximal femur bone strength is below 3000 N. In our cohort, a FE-estimated proximal femur strength less than 3000 N was seen in only 2 of 109 women (~2%) with a total hip aBMD T-score > -1.0 (normal) but in 84 of 93 women (90%) with a T-score < -2.5 (osteoporotic). Among the women with a T-score between -1.0 and -2.5, 30% had a FE-estimated hip strength less than 3000 N. Similarly, in men, a FE-estimated proximal femur strength less than 3000 N. Similarly, in total hip aBMD T-score (male-specific) > -1.0 and in 28 of 31 men (90%) with a T-score < -2.5. On the other hand, 22% of men with a T-score between -1.0 and -2.5 had a FE-estimated hip strength less than 3000 N. It may be that when DXA T-scores are in the

Amin et al.

osteopenic range, using FE-derived proximal femur strength may help to better identify those at particularly high fracture risk, in general. Unfortunately, the number of fractures in those who would be considered osteopenic in our cohort was too few to explore this possibility in depth. While controversy exists on whether female or male specific T-scores should be used for men in fracture prediction models (33), our findings suggest that FE-derived estimates of hip strength do appear to be a reasonable surrogate for overall bone strength, and so such estimates of bone strength may be able to enhance our ability to identify both women and men with bone fragility at greatest risk for fracture, regardless of how the T-score is derived (9). However, further work to examine this prospectively would be required.

Our study is cross-sectional in nature. However, our ability to capture overall and osteoporotic prevalent fractures with a very high degree of case ascertainment (34) in a community-based sample of women and men remains a notable strength. While we did not have direct measurements of total hip aBMD as measured by DXA scans in this study, our QCT-derived aBMD measurements were highly correlated with those from DXA in our validation study [unpublished data]. Our load-to-strength estimates were all derived for a fall to the side on the greater trochanter, and are not necessarily the loads that would be experienced at other bone sites. Furthermore, in estimating our load-to-strength ratio, we used a constant value of trochanteric soft tissue thickness (25 mm) for all subjects. There is well recognized individual variability in trochanteric soft tissue thickness, as well as general differences between men and women (24,25). Greater values of soft tissue thickness, seen on average for women compared to men, would attenuate the force at impact, thus reducing the load-to-strength ratio, theoretically reducing the risk of fracture. Since we did not have reliable measurements of soft tissue thickness data for this cohort, we removed the influence of soft tissue thickness from our analysis by assuming the same value for all subjects, both women and men. Our results indicate that our estimated load-to-strength-ratio, at least under such an assumption, does appear to be a comparable predictor of prevalent overall and osteoporotic fractures. That being said, if estimates of the actual loads experienced with falls or relatively low-trauma events causing fractures at other bone sites can be improved, the load-to-strength ratio, derived using bone strength as estimated at the proximal femur, may further enhance prospective non-hip fracture prediction models. That remains a topic of ongoing research.

Our findings suggest that FE-derived estimates of proximal femur strength are comparable in determining the probability of prevalent overall and osteoporotic fractures to total hip aBMD or vBMD. Thus, the characteristics specific to the proximal femur in the FE model did not appear to jeopardize its ability to assess fracture risk at other skeletal sites. Furthermore, the increase in probability of prevalent osteoporotic fractures in both women and men with FE-derived proximal femur strength values of less than 3000 N suggests that such low levels of proximal femur strength may represent a critical level reflective of systemic skeletal fragility. More work is warranted on determining whether an absolute bone strength value such as this, derived from the proximal femur by FE analysis, may serve as a clinically relevant threshold below which both women and men at highest risk for an osteoporotic fracture can be better identified.

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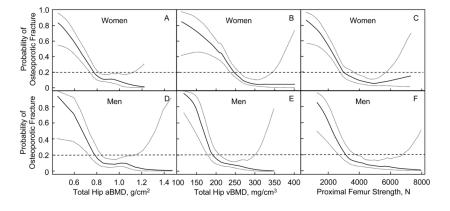
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Amin et al.



### Figure 1.

Probability of prevalent osteoporotic fracture (solid line) with 95% confidence intervals (dotted lines) for women (top panel, A–C) and men (bottom panel, D–F) associated with total hip aBMD, total hip vBMD and FE-derived estimates of proximal femur strength.

Distribution of all prevalent fractures occurring after age 35 years among of an age-stratified sample of 314 Rochester, Minnesota women over the age of 35 years.

			<b>Fracture Cause</b>			
	Severe Trauma	Falls from Standing	Spontaneous	Pathological Uncertain	Uncertain	All Causes
Fracture Site	N (%)	N (%)	N (%)	N (%)	N (%)	N (%)
Skull/face	2 (66.7%)	0(0.0%)	0 (0.0%)	0(0.0%)	1 (33.3%)	3 (1.1%)
Hands/fingers	13 (56.5%)	6 (26.1%)	0 (0.0%)	0(0.0%)	4 (17.4%)	23 (8.2%)
Distal Forearm	10 (22.2%)	34 (75.6%)	0(0.0%)	0(0.0%)	1 (2.2%)	45 (16.1%)
Proximal Humerus	4 (30.8%)	8 (61.5%)	0 (0.0%)	0(0.0%)	1 (7.7%)	13 (4.7%)
Other Arm	4 (40.0%)	6 (60.0%)	0 (0.0%)	0(0.0%)	(%0.0)	10 (3.6%)
Clavicle/scapula/sternum	7 (100%)	0(0.0%)	0(0.0%)	0(0.0%)	0(0.0%)	7 (2.5%)
Ribs	4 (16.7%)	2 (8.3%)	17 (70.8%)	0(0.0%)	1 (4.2%)	24 (8.6%)
Thoracic/Lumbar Vertebrae	10 (19.6%)	4 (7.8%)	33 (64.7%)	2 (3.9%)	2 (3.9%)	51 (18.3%)
Cervical Vertebrae	2 (50.0%)	0(0.0%)	2 (50.0%)	0(0.0%)	0~(0.0%)	4 (1.4%)
Pelvis	3 (75.0%)	1 (25.0%)	0 (0.0%)	0(0.0%)	0~(0.0%)	4 (1.4%)
Proximal Femur	0 (0.0%)	2 (100%)	0 (0.0%)	0(0.0%)	0(0.0%)	2 (0.7%)
Other Leg	22 (57.9%)	12 (31.6%)	0 (0.0%)	0(0.0%)	4 (10.5%)	38 (13.6%)
Feet/toes	33 (60.0%)	11 (20.0%)	6(10.9%)	0(0.0%)	5(9.1%)	55 (19.7%)
All Sites	114 (40.9%)	86 (30.8%)	58 (20.8%)	2 (0.7%)	19 (6.8%)	279

Bone density, strength estimates and load-to-strength ratio at the proximal femur in an age-stratified sample of 314 Rochester, Minnesota women over the age of 35 years.

No Fracture (n=175)Any Fracture (n=139)No Osteoporotic Fracture (n=259)Osteoporotic Fracture (n=55)Age (years) $56 \pm 13$ $68 \pm 14^{***}$ $59 \pm 14$ $74 \pm 12^{***}$ Age (years) $56 \pm 0.14$ $0.75 \pm 0.14^{***}$ $0.84 \pm 0.14$ $74 \pm 12^{***}$ Total Hip aBMD (g/cm <sup>3</sup> ) $0.86 \pm 0.14$ $0.75 \pm 0.14^{***}$ $0.84 \pm 0.14$ $0.70 \pm 0.14^{***}$ Total Hip vBMD (mg/cm <sup>3</sup> ) $267.1 \pm 45.8$ $232.5 \pm 44.2^{***}$ $259.9 \pm 45.3$ $213.6 \pm 43.4^{***}$ Proximal Femur Strength (N) $386.9 \pm 1186.6$ $3054.9 \pm 1186.5^{***}$ $3704.9 \pm 1178.8$ $2577.7 \pm 1172.2^{***}$ Load-to-Strength Ratio $0.98 \pm 0.33$ $1.26 \pm 0.45^{***}$ $1.03 \pm 0.36$ $1.43 \pm 0.50^{***}$	BMD (g/cm²)	=175) Any Fracture (n=139) 68 ± 14 *** 1 0.75 ± 0.14 *** 8 0000 0.000 0.000 0.000	No Osteoporotic Fracture (n=259) $59 \pm 14$ $0.84 \pm 0.14$ $259.9 \pm 45.3$	Osteoporotic Fracture (n=55)
$\begin{array}{cccccccccccccccccccccccccccccccccccc$	BMD (g/cm <sup>2</sup> )		$59 \pm 14$ $0.84 \pm 0.14$ $259.9 \pm 45.3$	*** 07 - 71
) $0.86 \pm 0.14$ $0.75 \pm 0.14^{***}$ $0.84 \pm 0.14$ $n^3$ $267.1 \pm 45.8$ $232.5 \pm 44.2^{***}$ $259.9 \pm 45.3$ hh (N) $3866.9 \pm 1186.6$ $3054.9 \pm 1186.5^{***}$ $3704.9 \pm 1178.8$ 0.98 \pm 0.33 $1.26 \pm 0.45^{***}$ $1.03 \pm 0.36$			$0.84 \pm 0.14$ $259.9 \pm 45.3$	$/4 \pm 1.2$
$n^3$ $267.1 \pm 45.8$ $232.5 \pm 44.2^{***}$ $259.9 \pm 45.3$ In $N$ $3866.9 \pm 1186.6$ $3054.9 \pm 1186.5^{***}$ $3704.9 \pm 1178.8$ $0.98 \pm 0.33$ $1.26 \pm 0.45^{***}$ $1.03 \pm 0.36$			$259.9\pm45.3$	$0.70 \pm 0.14^{***}$
Ih (N) $3866.9 \pm 1186.6$ $3054.9 \pm 1186.5^{***}$ $3704.9 \pm 1178.8$ $0.98 \pm 0.33$ $1.26 \pm 0.45^{***}$ $1.03 \pm 0.36$				$213.6 \pm 43.4^{***}$
$0.98 \pm 0.33 \qquad \qquad 1.26 \pm 0.45^{***} \qquad \qquad 1.03 \pm 0.36$			$3704.9 \pm 1178.8$	$2577.7 \pm 1172.2^{***}$
			$1.03\pm0.36$	$1.43 \pm 0.50^{***}$
	* p<0.01			

p<0.001 companing any fracture versus no fracture and osteoporotic fracture versus no osteoporotic fracture

Age-adjusted odds ratio and area under the receiver operator characteristic (c-statistic) for bone density, strength estimates and load-to-strength ratio at the proximal femur in an age-stratified sample of Rochester, Minnesota women over the age of 35 years.

	No Fracture (n=175)	Any Fracture	: (n=139)	Any Fracture (n=139) Osteoporotic Fracture (n=55)	cc=u) anno
		OR (95% CI)* c-statistic	c-statistic	OR (95% CI)*	c-statistic
Total Hip aBMD (g/cm <sup>2</sup> )	referent	1.3 (1.1, 1.5)	0.74	1.5 (1.1, 1.9)	0.84
Total Hip vBMD (mg/cm <sup>3</sup> )	referent	1.6 (1.1, 2.2)	0.74	2.0 (1.2, 3.3)	0.85
Proximal Femur Strength (N)	referent	1.3(1.0, 1.9)	0.73	1.8 (1.1, 2.9)	0.84
Load-to-Strength Ratio	referent	1.6 (1.1, 2.2)	0.74	1.8 (1.2, 2.8)	0.84

[OR (95% CI) and c-statistic for Osteoporotic Fracture when referent group is considered No Osteoporotic Fractures: Hip aBMD, 1.4 (1.1, 1.8), 0.81; Total Hip vBMD, 1.9 (1.2, 3.1), 0.81; Proximal Femur Strength, 1.8 (1.1, 3.0), 0.81; Load-to-Strength Ratio 1.6 (1.2, 2.4), 0.81]

\* Odds ratio per SD decrease for all variables except load-to-strength ratio, which is per SD increase.

Distribution of all prevalent fractures occurring after age 35 years among of an age-stratified sample of 266 Rochester, Minnesota men over the age of 35 years.

Amin et al.

			Fracture Cause			
	Severe Trauma	Falls from Standing	Spontaneous	Pathological	Uncertain	All Causes
Fracture Site	N (%)	N (%)	N (%)	N (%)	N (%)	N (%)
Skull/face	1 (50.0%)	0 (0.0%)	0 (0.0%)	0(0.0%)	1 (50.0%)	2 (1.2%)
Hands/fingers	18 (64.3%)	4 (14.3%)	0 (0.0%)	0(0.0%)	6 (21.4%)	28 (16.5%)
Distal Forearm	10 (52.6%)	7 (36.8%)	2 (10.5%)	0(0.0%)	0 (0.0%)	19 (11.2%)
Proximal Humerus	2 (66.7%)	1 (33.3%)	0(0.0%)	0(0.0%)	0 (0.0%)	3 (1.8%)
Other Arm	1 (33.3%)	1 (33.3%)	0(0.0%)	0(0.0%)	1 (33.3%)	3 (1.8%)
Clavicle/scapula/sternum	3 (33.3%)	2 (22.2%)	2 (22.2%)	0(0.0%)	2 (22.2%)	9 (5.3%)
Ribs	9 (27.3%)	5 (15.2%)	16 (48.5%)	0(0.0%)	3 (9.1%)	33 (19.4%)
Thoracic/Lumbar Vertebrae	7 (25.0%)	1 (3.6%)	20 (71.4%)	0(0.0%)	0 (0.0%)	28 (16.5%)
Cervical Vertebrae	1 (33.3%)	1 (33.3%)	1 (33.3%)	0(0.0%)	0 (0.0%)	3 (1.8%)
Pelvis	0 (0.0%)	1 (33.3%)	0(0.0%)	0(0.0%)	2 (66.7%)	3 (1.8%)
Proximal Femur	0 (0.0%)	1 (100%)	0 (0.0%)	0(0.0%)	0 (0.0%)	1 (0.6%)
Other Leg	9 (47.4%)	7 (36.8%)	1 (5.3%)	0(0.0%)	2 (10.5%)	19 (11.2%)
Feet/toes	11 (57.9%)	2 (10.5%)	2 (10.5%)	0(0.0%)	4 (21.1%)	19 (11.2%)
All Sites	72 (42.4%)	33 (19.4%)	44 (25.9%)	0(0.0%)	21 (12.4%)	170

Bone density, strength estimates and load-to-strength ratio at the proximal femur among of an age-stratified sample of 266 Rochester, Minnesota men over the age of 35 years.

No Fracture (n=162)         Any Fracture (n=104)         No Osteoporotic Fracture (n=238)         Osteoporotic Fracture (n=28)         Osteo In 1017 ****         Osteo In 1017 ****         Osteo In 1010 *****         Osteo In 1010 *****				Mean (SD)	
ears) $57 \pm 5$ $70 \pm 14^{***}$ Hp aBMD (g/cm <sup>2</sup> ) $0.95 \pm 0.14$ $0.85 \pm 0.16^{***}$ Hp vBMD (mg/cm <sup>3</sup> ) $239.1 \pm 36.8$ $209.9 \pm 43.4^{***}$ al Femur Strength (N) $4602.0 \pm 1287.4$ $3674.7 \pm 1310.5^{***}$ o-Strength Ratio $1.02 \pm 0.31$ $1.27 \pm 0.49^{***}$		No Fracture (n=162)	Any Fracture (n=104)	No Osteoporotic Fracture (n=238)	Osteoporotic Fracture (n=28)
<b>ip aBMD (g/cm²)</b> $0.95 \pm 0.14$ $0.85 \pm 0.16^{***}$ <b>ip vBMD (mg/cm³)</b> $239.1 \pm 36.8$ $209.9 \pm 43.4^{***}$ <b>al Femur Strength (N)</b> $4602.0 \pm 1287.4$ $3674.7 \pm 1310.5^{***}$ <b>o-Strength Ratio</b> $1.02 \pm 0.31$ $1.27 \pm 0.49^{***}$	Age (years)	57 ± 5	$70\pm14^{***}$	$61 \pm 16$	$69 \pm 16^*$
Hp vBMD (mg/cm³) $239.1 \pm 36.8$ $209.9 \pm 43.4^{***}$ nal Femur Strength (N) $4602.0 \pm 1287.4$ $3674.7 \pm 1310.5^{***}$ o-Strength Ratio $1.02 \pm 0.31$ $1.27 \pm 0.49^{***}$	Total Hip aBMD (g/cm <sup>2</sup> )	$0.95\pm0.14$	$0.85 \pm 0.16^{***}$	$0.93\pm0.15$	$0.81 \pm 0.17^{***}$
al Femur Strength (N) $4602.0 \pm 1287.4$ $3674.7 \pm 1310.5^{***}$ o-Strength Ratio $1.02 \pm 0.31$ $1.27 \pm 0.49^{***}$	Total Hip vBMD (mg/cm <sup>3</sup> )	$239.1 \pm 36.8$	$209.9 \pm 43.4^{***}$	$232.0\pm39.5$	$191.6\pm 45.0^{***}$
<b>o-Strength Ratio</b> $1.02 \pm 0.31$ $1.27 \pm 0.49^{***}$	Proximal Femur Strength (N)	$4602.0 \pm 1287.4$	$3674.7 \pm 1310.5^{***}$	$4359.7 \pm 1334.2$	$3217.4 \pm 1270.9^{***}$
* p<0.05 **	Load-to-Strength Ratio	$1.02 \pm 0.31$	$1.27 \pm 0.49^{***}$	$1.07 \pm 0.36$	$1.50 \pm 0.57^{***}$
** 	* p<0.05				
P<0.01	$^{**}_{p<0.01}$				
$^{**}_{n<0.001}$ comnaring any fracture versus no fracture and osteonorotic fracture versus no osteonorotic fracture	*** n<0.001 comnaring any fracture	versus no fracture and o	steonorotic fracture versus	no osteonorotic fracture	

Age-adjusted odds ratio and area under the receiver operator characteristic (c-statistic) for bone density, strength estimates and load-to-strength ratio at the proximal femur in age-stratified sample of Rochester, Minnesota men over the age of 35 years.

	No Fracture (n=162)	Any Fracture (n=104)	e (n=104)	Osteoporotic Fracture (n=28)	icture (n=28)
		OR (95% CI) <sup>*</sup> c-statistic	c-statistic	OR (95% CI)*	c-statistic
Total Hip aBMD (g/cm <sup>2</sup> )	referent	1.4 (1.1, 1.8)	0.75	2.0 (1.3, 3.0)	0.75
Total Hip vBMD (mg/cm <sup>3</sup> )	referent	1.6 (1.2, 2.2)	0.75	3.4 (1.9, 6.3)	0.78
Proximal Femur Strength (N)	referent	1.5 (1.1, 2.1)	0.74	3.2 (1.7, 6.2)	0.78
Load-to-Strength Ratio	referent	1.5 (1.1, 2.0)	0.74	2.5 (1.6, 4.1)	0.77

4D, 1.7 (1.2, 2.4), 0.69; Total Hip vBMD, 2.8 (1.7, 4.8), 0.74; Proximal Femur Strength, 2.8 (1.5, 5.1), 0.74; Load-to-Strength Ratio, 2.1 (1.4, 3.1), 0.74] 5

\* Odds ratio per SD decrease for all variables except load-to-strength ratio, which is per SD increase.