

Research Article

Theme: Pharmacokinetic/Pharmacodynamic Modeling and Simulation in Drug Discovery and Translational Research
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Pharmacodynamic Model of Sodium–Glucose Transporter 2 (SGLT2) Inhibition: Implications for Quantitative Translational Pharmacology

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ABSTRACT. Sodium–glucose co-transporter-2 (SGLT2) inhibitors are an emerging class of agents for use in the treatment of type 2 diabetes mellitus (T2DM). Inhibition of SGLT2 leads to improved glycemic control through increased urinary glucose excretion (UGE). In this study, a biologically based pharmacokinetic/pharmacodynamic (PK/PD) model of SGLT2 inhibitor-mediated UGE was developed. The derived model was used to characterize the acute PK/PD relationship of the SGLT2 inhibitor, dapagliflozin, in rats. The quantitative translational pharmacology of dapagliflozin was examined through both prospective simulation and direct modeling of mean literature data obtained for dapagliflozin in healthy subjects. Prospective simulations provided time courses of UGE that were of consistent shape to clinical observations, but were modestly biased toward under prediction. Direct modeling provided an improved characterization of the data and precise parameter estimates which were reasonably consistent with those predicted from preclinical data. Overall, these results indicate that the acute clinical pharmacology of SGLT2 inhibitors in healthy subjects can be reasonably well predicted from preclinical data through rational accounting of species differences in pharmacokinetics, physiology, and SGLT2 pharmacology. Because these data can be generated at the earliest stages of drug discovery, the proposed model is useful in the design and development of novel SGLT2 inhibitors. In addition, this model is expected to serve as a useful foundation for future efforts to understand and predict the effects of SGLT2 inhibition under chronic administration and in other patient populations.

KEY WORDS: diabetes; glucosuria; pharmacodynamics; pharmacokinetics; SGLT2; translational pharmacology; UGE.

INTRODUCTION

It has been estimated that more than 25 million Americans (8.3% of the population) have type 2 diabetes (T2DM) (1). In 2007 alone, the costs associated with diabetes amounted to greater than 280,000 lives and 170 billion dollars (2). As such, T2DM remains one of the largest therapeutic areas for research and development in the pharmaceutical industry. This therapeutic area is also one of the most

competitive, with the majority (*i.e.* 57%) of medicinal chemistry patent applications between 2008 and 2010 centered upon just eight molecular targets (3). Under these circumstances, clinical attrition of a lead molecule due to suboptimal pharmacokinetics, efficacy, or safety can be disastrous, as there are often multiple competitor programs in play against the same target. As such, early decisions regarding chemical optimization and candidate selection are critically important to success. To this end, considerable efforts have been made to develop and apply biologically based mathematical models in support of quantitative human pharmacokinetic predictions from *in vitro* and *in vivo* data generated preclinically (4–17). It is now commonplace for such predictive pharmacokinetic models to be used in the design and selection of drug candidates across the pharmaceutical industry. The decline in pharmacokinetic attrition observed in the pharmaceutical industry can be attributed, in part, to these efforts (18). In contrast, to date, far less attention has been paid to the development and application of biologically based mathematical models to support quantitative pharmacology

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predictions from *in vitro* and *in vivo* data generated preclinically. Such models are expected to be useful in reducing the relatively high rate of late-stage safety and efficacy-based attrition (18). This is expected to be particularly enabling in highly competitive areas, like diabetes, where the margin for error in the design and advancement of the best clinical candidate is relatively low.

Within the T2DM therapeutic area, the sodium–glucose co-transporter 2 (SGLT2) target represents one of the most competitive areas of R&D (3–19). Glucose entering the glomerulus through passive filtration is reabsorbed by the combined actions of SGLT2 and SGLT1 in the S1 and S3 segments of the proximal tubule, respectively. Genetic functional data suggest that the urinary glucose excretion (UGE) associated with impaired SGLT2 function represents a safe and effective approach for managing the hyperglycemia associated with T2DM (20–22). Other attractive features of this mechanism include its non-insulin-dependent nature and the potential for weight loss due to the caloric loss associated with UGE. As such, it is one of the top eight targets being pursued in the pharmaceutical industry and there are several novel SGLT2 inhibitors currently in clinical development (3–19). While several compounds have attrited in phase I and II, clinical results with the most advanced SGLT2 inhibitor, dapagliflozin, indicate that clinically significant HbA1c reductions are possible with this target (23,24). To date, dapagliflozin is also the only SGLT2 inhibitor for which extensive preclinical and clinical data have been disclosed. These data provide the opportunity to examine the quantitative translational pharmacology of SGLT2 inhibition. As such, the objective of this work is to quantitatively examine the translational pharmacology of SGLT2 inhibition between the preclinical and clinical setting using a simple, physiologically based pharmacokinetic/pharmacodynamic (PK/PD) model. The results of this work indicate that the acute clinical pharmacology of SGLT2-mediated UGE can be reasonably well predicted from preclinical data using the proposed PKPD model. This work highlights several important principles of general relevance to the quantitative scaling of preclinical information in support of the design and advancement of clinical candidates with the highest likelihood of clinical success.

MATERIALS AND METHODS

Materials. (2S,3R,4R,5S,6R)-2-[4-Chloro-3-(4-ethoxybenzyl)phenyl]-6-(hydroxymethyl)-tetrahydro-2H-pyran-3,4,5-triol, referred to as dapagliflozin hereafter, was synthesized as described previously (25).

Preclinical Studies. All animal care and *in vivo* procedures were approved and conducted in accordance with guidelines of the Pfizer Animal Care and Use Committee. Male Sprague–Dawley rats (~300 g) were singly housed in metabolic cages for urine collection over 24 h ($n=4-5$ per group). A separate set of male Sprague–Dawley rats with indwelling jugular vein catheters were used for determination of pharmacokinetics ($n=3$ per group). Dapagliflozin was administered via oral gavage (1 ml/300 g body weight) at single doses of 0.1, 1, 3, and 10 mg/kg ($n=4-5$ per group). A subset of rats ($n=5$) was given control vehicle (0.5%

methylcellulose and 0.1% Tween 80). Blood (0.3 mL) was collected from jugular vein catheters at 0.25, 0.5, 1, 2, 4, 6, 8, and 24 h, centrifuged and the resultant plasma kept frozen at -20°C until analysis for dapagliflozin concentration via LC-MS/MS. Urine was collected following treatment administration over a duration of 24 h. Urinary glucose concentration was measured by UV absorbance spectrophotometry at 340 nm using a Roche Hitachi 917 spectrophotometer (Diamond Diagnostics, Holliston, MA, USA). The total amount of glucose excreted in the urine (UGE) was calculated as the product of urine concentration and urine volume.

Bioanalysis. Aliquots (50 μL) of plasma samples and standards were subjected to protein precipitation with acetonitrile containing an internal standard. Samples were vortexed and centrifuged to obtain supernatant which was analyzed by LC-MS/MS. Analyst (version 1.4.1) was used to measure peak areas, and peak area ratios of analyte to internal standard were calculated. A calibration curve was constructed from the peak area ratios of the standards to the internal standard by applying a weighted linear ($1/x^2$) regression. The linear range of the standard curve was 5.00 to 5,000 ng/mL. LC-MS/MS conditions were as follows: Mass Spectrometer+Source Type was Sciex API 4,000 – Turbo Spray; HPLC pump was Shimadzu; Autosampler was CTC PAL Autosampler; injection volume was 10 μL ; a gradient was used with mobile phase A, 10 mM ammonium acetate and 1% isopropyl alcohol in water; B, acetonitrile; flow rate 0.500 mL/min (column 2.0 \times 30 mm, 5 μm LUNA C18 column (phenomenex)). An initial condition of 90% A, 10% B was held for 0.25 min, ramped to 10% A, 90% B over 1 min, returned to the initial condition in a single step and held for 0.25 min prior to the next injection. Detection mode was negative.

Literature Reports on Human Studies. Mean human plasma dapagliflozin concentrations following single doses of 2.5, 10, 50, 100, and 250 mg and associated urinary glucose excretion over 120 h in healthy subjects were obtained from a literature report (26) via digitization using Grab It! XP 10 (DataTrend Software Inc.). Digitized data were electronically overlaid on figures from the original report to ensure concordance.

Rat PK/PD Model. The concentration-time profiles of dapagliflozin in rats were described using a one-compartment linear disposition model with first-order absorption:

$$\frac{dA_{po}}{dt} = -k_a \cdot A_{po}; A_{po}(0) = \text{Dose} \quad (1)$$

$$V_{c,app} \frac{dC_p}{dt} = k_a \cdot A_{po} - k_{el} \cdot C_p \cdot V_{c,app}; C_p(0) = 0 \quad (2)$$

where k_a is the first-order absorption rate constant after oral dosing and k_{el} is the first-order elimination rate constant. Equation 1 describes the amount of drug (A_{po}) at the site of absorption after oral dosing. The administered dose represents the initial condition at the site of absorption. Plasma drug concentration and apparent volume of distribution in the central compartment are denoted by C_p (initial condition=0) and $V_{c,app}$, respectively. The dynamic cumulative

UGE response to SGLT2 inhibition was modeled as a function of the inhibitor concentration, C , as previously described (27):

$$\frac{d\text{UGE}}{dt} = \text{GFR} \cdot \text{PG} - f_{\text{reabs}} \cdot \text{GFR} \cdot \text{PG} \cdot \left(1 - \frac{I_{\text{max}} \cdot C}{IC_{50} + C}\right) \quad (3)$$

where GFR represents glomerular filtration rate and PG represents the plasma glucose concentration. The product of these parameters represents the rate of glucose filtration by the kidney. The f_{reabs} parameter represents the fraction of filtered glucose which is reabsorbed in the untreated condition. The I_{max} and IC_{50} parameters represent the maximum fractional inhibition of glucose reabsorption by the inhibitor and the concentration of inhibitor which achieves half-maximal inhibition of glucose reabsorption, respectively. For purposes of modeling, the physiologically relevant parameters of glucose filtration and reabsorption were fixed to independent estimates obtained from the literature. GFR was set to 0.55 ml/h/g consistent with that previously reported in rats (28). PG was fixed to a mean experimental estimate obtained in an independent, in-house study of 30 male Sprague–Dawley rats weighing 290 ± 50 g ($1.41 + 0.54$ mg/ml determined spectrophotometrically). This value is consistent with plasma glucose values reported in normal rats (29–31). The f_{reabs} parameter was fixed to 0.996 as previously estimated and is commensurate with near complete glucose reabsorption in normal rats (27). As such, only I_{max} and IC_{50} were estimated in the modeling process.

Human PK/PD Model. The reported mean concentration-time profiles of dapagliflozin in healthy subjects were described using a two-compartment linear disposition model with first-order absorption:

$$\frac{dA_{\text{po}}}{dt} = -k_a \cdot A_{\text{po}}; A_{\text{po}}(0) = \text{Dose} \quad (4)$$

$$V_{\text{c,app}} \frac{dC_p}{dt} = k_a \cdot A_{\text{po}} - (k_{\text{el}} + k_{\text{pt}}) \cdot C_p \cdot V_{\text{c,app}} + k_{\text{tp}} \cdot A_t; C_p(0) = 0 \quad (5)$$

$$\frac{dA_t}{dt} = k_{\text{pt}} \cdot C_p \cdot V_{\text{c,app}} - k_{\text{tp}} \cdot A_t; A_t(0) = 0 \quad (6)$$

where k_a is the first-order absorption rate constant after oral dosing, k_{pt} and k_{tp} are the first-order rate constants for non-specific distribution of the drug to and from a peripheral compartment, and k_{el} is the first-order elimination rate constant. Equation 4 describes the amount of drug (A_{po}) at the site of absorption after oral dosing and Eq. 6 describes the amount of drug in the peripheral compartment (A_t). Plasma drug concentration and apparent volume of distribution in the central compartment are denoted by C_p and $V_{\text{c,app}}$, respectively. Subsequent prediction and modeling of human UGE employed the pharmacokinetic parameters estimated in this step.

A slightly modified form of Eq. 3 was used to both predict and model the pharmacodynamics of SGLT2 inhibitor-mediated UGE in healthy subjects:

$$\frac{d\text{UGE}}{dt} = \text{GluFR} - f_{\text{reabs}} \cdot \text{GluFR} \cdot \left(1 - \frac{I_{\text{max}} \cdot C}{IC_{50} + C}\right) \quad (7)$$

where GluFR denotes glucose filtration rate as determined by the product of GFR and PG. GluFR was fixed to a population mean value of 7.5 g/h commensurate with typical mean plasma glucose concentrations (*i.e.* 100 mg/dl, 5 mM) and GFR (*i.e.* 125 ml/min) in healthy subjects (32–34). This simplification was performed in order to allow for a fixed 20% inter-cohort coefficient of variation around the assumed population mean GluFR in modeling the human data. As neither this parameter nor its composite parts (PG and GFR) were reported in the literature, this allowance provides for a reasonable degree of variability in this physiological parameter around the assumed population mean value across dose groups. In the modeling process, I_{max} , IC_{50} , and *post hoc* estimates of GluFR in each dose group were estimated. In addition to the modeling described above, prospective simulations of human UGE were performed from pharmacodynamic parameters estimated in rats. For this analysis, GluFR was assumed to be 7.5 g/h. The I_{max} and f_{reabs} parameters were assumed to translate 1:1 between rats and humans. Lastly, the IC_{50} parameter estimated in rats was translated to an expected human value by accounting for species differences in unbound fraction and *in vitro* potency as follows:

$$IC_{50,\text{human}} = IC_{50,\text{rat}} \times \frac{f_{\text{u, rat}}}{f_{\text{u, human}}} \times \frac{\text{hSGLT2 } IC_{50}}{\text{rSGLT2 } IC_{50}}$$

where hSGLT2 IC_{50} and rSGLT2 IC_{50} denote the potency against human and rat SGLT2 determined *in vitro*.

Data Analysis. The PK/PD model was implemented in NONMEM version 5, release 1.1 using the first-order method of approximation (35). Analysis was conducted in a sequential manner whereby pharmacokinetic parameters estimated in step 1 were fixed to population mean estimates during estimation of pharmacodynamic parameters in the second step. Residual error was characterized according to a proportional error model:

$$y_j = f(\theta, t_j) (1 + \varepsilon_j) \quad (8)$$

where $f(\theta, t_j)$ is the predicted value of the data from the model given the population mean PK and PD parameters (θ) and time (t_j). y_j denotes the j^{th} observation and ε_j accounts for the residual between the predicted and observed values. Goodness-of-fit was analyzed using the objective function, visual inspection of curve fits, predicted and observed plots, residual plots, and an assessment of parameter estimates and associated correlations of parameter estimates.

RESULTS

Rat Pharmacokinetics and Pharmacodynamics

Dapagliflozin exposure was dose proportional between 0.1 and 10 mg/kg. The proposed one-compartment model

with first-order absorption well characterized each dose level (Fig. 1a), and uncertainty (SEM%) associated with the parameter estimates was low (Table I). In addition, the proposed PK/PD model reasonably well fitted the observed 24-h UGE (Fig. 1b). Both the data and model indicate less than dose proportional increase in UGE at doses above 1 mg/kg. However, slightly greater increases in UGE were observed at the 3 and 10 mg/kg dose levels than were fitted by the model. Incorporation of a hill coefficient in the model did not improve the fit to the data further (data not shown). The I_{\max} parameter was estimated to be 0.32 and the associated uncertainty was low (Table I). A larger degree of uncertainty (51% SEM) was associated with the IC_{50} parameter estimate of 29 ng/ml (2.9 nM unbound).

Human Pharmacokinetics and Pharmacodynamics

Previously reported dapagliflozin pharmacokinetics were well characterized by the proposed linear two-compartment model (Fig. 2), and the uncertainty associated with parameter estimates was low (Table II). As described in the MATERIALS AND METHODS section, prospective predictions of human UGE assumed a 1:1 translation of I_{\max} and f_{reabs} from rats (0.32 and 0.996, respectively). An expected human IC_{50} of 6.6 ng/ml was obtained by accounting for species differences in unbound fraction and *in vitro* potency as follows:

$$IC_{50,\text{human}} = IC_{50,\text{rat}} \times \frac{f_{u,\text{rat}}}{f_{u,\text{human}}} \times \frac{h\text{SGLT2}IC_{50}}{r\text{SGLT2}IC_{50}}$$

$$= 29 \text{ ng/ml} \times \left(\frac{0.040}{0.064}\right) \times \left(\frac{1.1}{3.0}\right) = 6.6 \text{ ng/ml}$$

Assuming these parameter values, prospective predictions of human UGE were of consistent shape, but biased toward under-prediction (Fig. 3a). Overall, this bias was modest in nature, with the error in UGE prediction at 120 h being 23%, 28%, 7%, 28%, and 23% at dapagliflozin doses of 2.5, 10, 50, 100, and 250 mg, respectively. Not surprisingly, modeling of the data provided a better characterization, with no obvious bias across doses (Fig. 3b). The I_{\max} and IC_{50} parameters were estimated to be 0.35 and 3.5 ng/ml (0.55 nM unbound), and uncertainty associated with the parameter estimates was low (Table II). *Post hoc* estimates of glucose filtration rate in the 2.5, 10, 50, 100, and 250 mg dose groups were 6.6, 7.7, 6.8, 8.6, and 8.6 g/h, respectively. These estimates correspond to daily glucose filtrations of 158, 185, 163, 206 and 206 g, respectively.

DISCUSSION

Preclinical Pharmacokinetics and Pharmacodynamics

The proposed biologically based PK/PD model provided a reasonable characterization of observed dapagliflozin-mediated UGE in rats. Modest UGE under predictions at high doses and a 51% SEM on the IC_{50} estimate may be due, in part, to the relatively sparse, single time point, UGE data available for PK/PD modeling in the rat. Given the observed exposures of dapagliflozin in this study, it is also feasible that some modest degree of SGLT1 inhibition may confound the

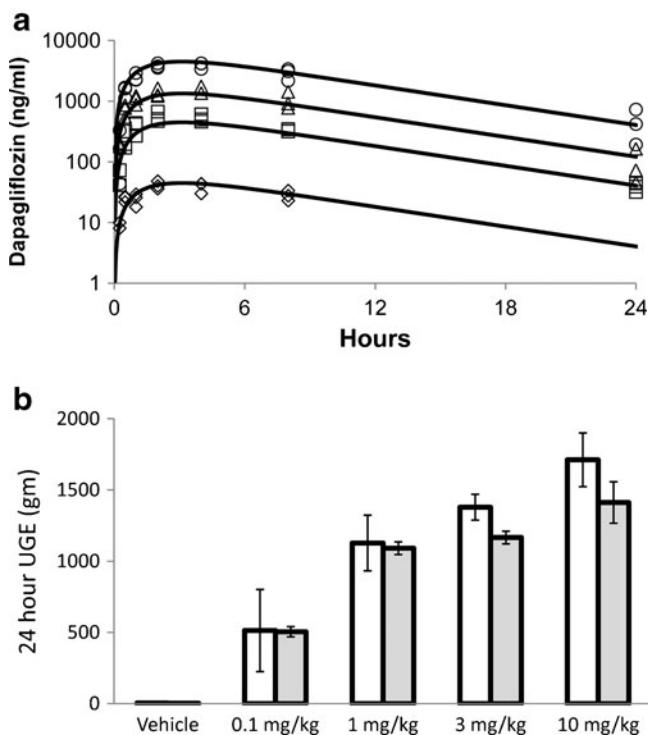


Fig. 1. Single-dose plasma pharmacokinetics **a** and UGE pharmacodynamics **b** of dapagliflozin at four dose levels in rats. Lines of **a** and shaded bars of **b** represent model fits. Open symbols of **a** represent individual observations at doses of 0.1 (triangle), 1 (square), 3 (triangle), and 10 mg/kg (circle). Open bars of **b** (mean \pm S.D.) represent mean experimental observations (\pm S.D.). UGE over 24 h in the vehicle group was 4.1 ± 0.6 g

analysis of rat data. As reported previously, the IC_{50} of dapagliflozin for rat SGLT1 is 620 nM (36). Model-predicted maximum, average and minimum dapagliflozin concentrations at the highest dose tested (10 mg/kg) were 4,458 ng/ml (436 nM unbound), 2,055 ng/ml (201 nM unbound), and 409 ng/ml (40 nM unbound), respectively. As such, the fractional inhibition of SGLT1 at 10 mg/kg could vary between 6% and 40% over the 24-h UGE determination. Although relatively less important to glucose reabsorption in normal conditions (\sim 10% vs. 90% for SGLT2) (37), SGLT1 may play a more important fractional role as SGLT2 is increasingly inhibited. Factoring in the relative contribution of these two transporters under various degrees of pharmacological inhibition will require a more mechanistic model and is outside the scope of the current work. Nevertheless, additional confidence that the PK/PD model predominantly represents SGLT2 inhibition can be derived from the concordance between the estimated unbound IC_{50} and that previously reported for rSGLT2 *in vitro* (2.9 vs. 3 nM, respectively) (36). In addition, we have recently reported a similar *in vitro*-*in vivo* concordance of IC_{50} in applying this PK/PD model to new SGLT2 inhibitor, PF-04971729 (27). It is interesting to note that the I_{\max} of dapagliflozin was estimated to be 0.32, indicating that maximum SGLT2 inhibition is associated with only a 32% reduction in glucose reabsorption. Again, this observation is consistent with the potential that other transporters (e.g., SGLT1) may play an increasing important role in glucose reabsorption as SGLT2 is inhibited.

Table I. Estimated PK/PD Model Parameters for Dapagliflozin in Rats

Parameter (units)	Definition	Final estimate	% SEM
Pharmacokinetic parameters			
k_{el} (1/hr)	First-order elimination rate constant	0.13	7.6
k_a (1/hr)	First-order absorption rate constant	0.67	11.9
$V_{c,app}$ (L/kg)	Apparent volume of distribution	1.5	6.7
Pharmacodynamic parameters			
$IC_{50, total}$ (ng/ml)	Total plasma concentration associated with half-maximal inhibition of SGLT2-mediated glucose reabsorption	29	51
$IC_{50, unbound}$ (nM)	Unbound plasma concentration associated with half-maximal inhibition of SGLT2-mediated glucose reabsorption	2.9 ^a	–
I_{max}	Maximum fractional inhibition of glucose reabsorption	0.32	6.3

^a Calculated based on a molecular weight of 409 Da and a rat unbound plasma fraction of 0.040 estimated by standard equilibrium dialysis techniques

Human Pharmacokinetics and Pharmacodynamics

Though generally consistent, prospective prediction of human UGE from the pharmacodynamic parameters obtained in rats were modestly biased toward under prediction (Fig. 3a). In contrast, the proposed biologically based PK/PD model for SGLT2 inhibitor-mediated UGE provided an excellent characterization of mean UGE in healthy subjects taken from the literature (Fig. 3b). Unlike the rat studies, an extensive amount of pharmacokinetic and UGE data were available to support precise parameter estimation. In addition,

the improved selectivity of dapagliflozin for human SGLT2 over human SGLT1 (1.1 vs. 1,391 nM) (36), removes the potentially confounding influence of SGLT1 inhibition at the doses examined herein. The estimated I_{max} of 0.35 was similar to that estimated in rats (0.32) and that reported previously in humans (26). In addition, as was observed in rats, the unbound IC_{50} estimate was very similar to that previously reported for dapagliflozin against hSGLT2 *in vitro* (0.55 vs. 1.1 nM, respectively) (36). *Post hoc* estimates of GluFR were slightly different among dose groups with no obvious trend. These results suggest that the observed bias in prospective predictions is likely a function of slight errors in the assumed values of IC_{50} , I_{max} , and *GluFR*. Overall, these results indicate an excellent quantitative translation of dapagliflozin pharmacology across species.

Implications for Applied Translational Research

This work suggests that the acute clinical pharmacology of SGLT2 inhibitors in healthy subjects can be predicted from preclinical data using the proposed biologically based PK/PD model of UGE with sufficient accuracy to support decision making (compound rank ordering, candidate selection, early clinical trial design). More specifically, this work suggests that SGLT2 inhibitor-mediated UGE can be predicted in humans from the following data which can be obtained preclinically: (1) a prediction of human pharmacokinetics, (2) parameters describing the normal physiological process of glucose filtration and reabsorption (GFR, plasma glucose concentration, f_{reabs}), and (3) parameters describing the intrinsic efficacy (I_{max}) and potency (IC_{50}) of the SGLT2 inhibitor for UGE. Key principles and limitations underlying how each of these key areas of translation was handled in the current work are discussed below.

Translational Pharmacokinetics. The prediction of human pharmacokinetics will usually serve as the foundation upon which pharmacodynamics are predicted. Many reports have demonstrated that reasonably accurate pharmacokinetic predictions from preclinical data are feasible and common in the pharmaceutical industry (4–17). In a previous report, we have utilized these approaches to support a pharmacodynamic prediction for a new SGLT2 inhibitor, PF-04971729 (27). Since

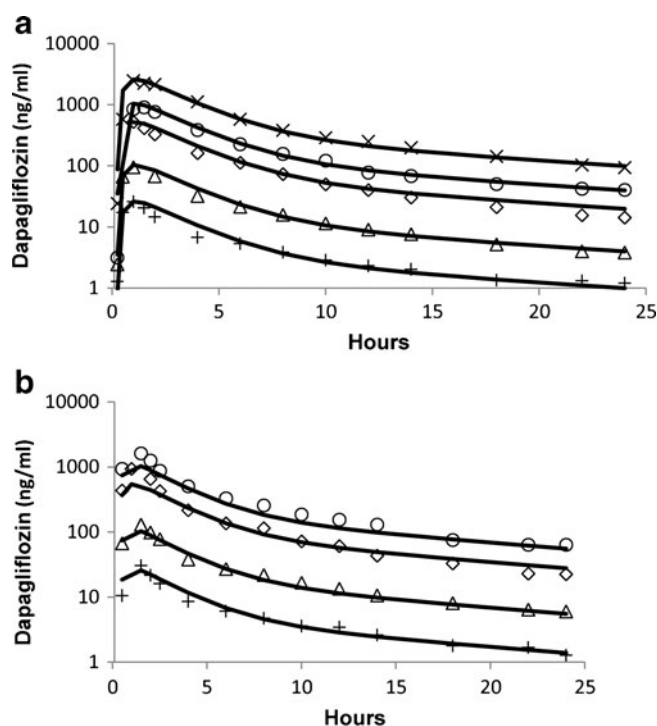


Fig. 2. Mean dapagliflozin pharmacokinetics in healthy subjects following single **a** and multiple daily doses **b** as obtained from the literature (26). Symbols represent doses of 2.5 (plus sign), 10 (triangle), 50 (diamond), 100 (circle), and 250 mg (multiplication sign). Lines represent model fits

Table II. Estimated PK/PD Model Parameters for Dapagliflozin in Healthy Subjects

Parameter (units)	Definition	Final estimate	% SEM
Pharmacokinetic parameters			
k_{el} (1/hr)	First-order elimination rate constant	0.26	7.7
k_a (1/hr)	First-order absorption rate constant	2.7	14.8
k_{pt} (1/hr)	First-order rate constant for distribution of drug from plasma to tissues	0.14	14.3
k_{tp} (1/hr)	First-order rate constant for distribution of drug from tissues to plasma	0.09	22.2
$V_{c,app}$ (L)	Apparent central volume of distribution	70	8.5
Pharmacodynamic parameters			
$IC_{50, total}$ (ng/ml)	Total plasma concentration associated with half-maximal inhibition of SGLT2-mediated glucose reabsorption	3.5	17.1
$IC_{50, unbound}$ (nM)	Unbound plasma concentration associated with half-maximal inhibition of SGLT2-mediated glucose reabsorption	0.55 ^a	–
I_{max}	Maximum fractional inhibition of glucose reabsorption	0.35	5.7

^a Calculated based on a molecular weight of 409 Da and a human unbound plasma fraction of 0.064 estimated by standard equilibrium dialysis techniques. GluFR was assumed to be 7.5 g/h with a 20% inter-cohort coefficient of variation. GluFR was estimated to be 6.6, 7.7, 6.8, 8.6, and 8.6 g/h in the 2.5, 10, 50, 100, and 250 mg dose cohorts

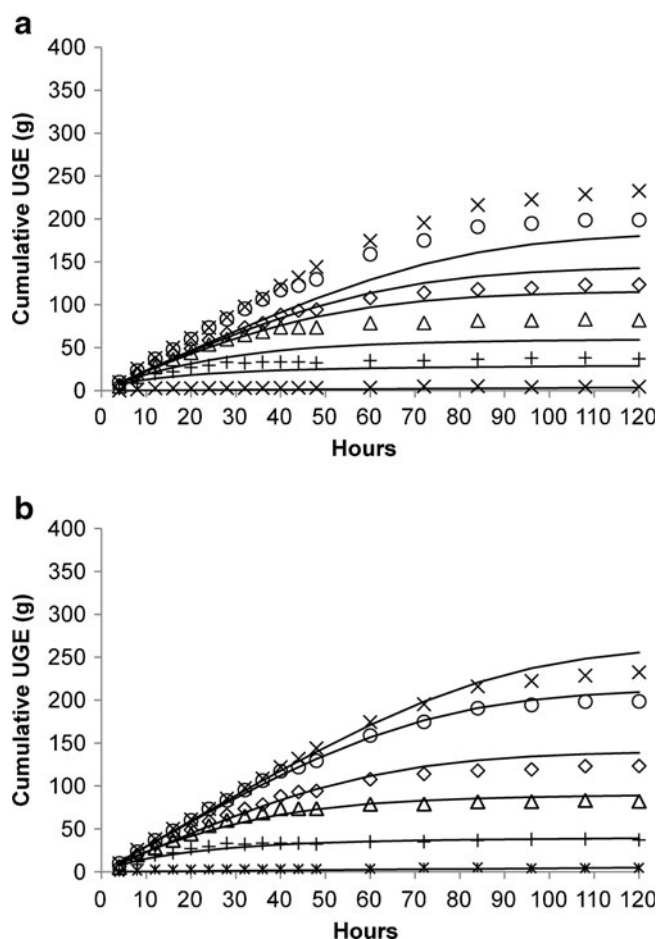


Fig. 3. Model-based prediction **a** and description **b** of mean UGE pharmacodynamics of dapagliflozin in healthy subjects following single doses as obtained from the literature (26). Symbols represent doses of 0 (asterisk), 2.5 (plus sign), 10 (triangle), 50 (diamond), 100 (circle), and 250 mg (multiplication sign). Lines represent model predictions **a** and fits **b**

the focus of the current work is upon an examination of translational pharmacology, human pharmacokinetics of dapagliflozin were simply obtained from the literature (26).

Translational Physiology. Physiologically, both the circulating concentration of glucose and the rate at which the circulation is filtered will govern the rate at which glucose is filtered by the kidney. This basic concept is codified in the model as the product of GFR and plasma glucose concentration. GFR is an independent physiological parameter that can be experimentally estimated at the subject level or approximated at the level of a population (e.g., mean GFR in healthy subjects). Plasma glucose concentration can also be determined either experimentally at the subject level or approximated at the level of a population (e.g., mean plasma glucose concentration in healthy subjects). As described in the **MATERIALS AND METHODS** section, GFR and plasma glucose values were chosen to be consistent with population mean values as obtained from the literature for the current exercise. While this simplification is appropriate to support the goals of the current study-level analysis, inter-patient variability in these parameters would be important to understand in many cases as this would certainly contribute to variability in response among individuals. This may be particularly important in the diabetic population where there is a large degree of inter-patient variability in glycemic control and renal function. Another simplification was made in the current analysis such that these physiological parameters were fixed to stationary (time-invariant) values. Although GFR does follow a circadian pattern, the variation around the mean value over 24 h appears to be small in healthy rats and humans (28–38). In addition, although plasma glucose profiles would be expected to vary with time and meals, there also appears to be little variation around the mean value in healthy rats and humans (29–31,39). As such, fixing GFR and plasma glucose to mean and stationary parameters for characterization of healthy rats and humans is likely a reasonable approximation. Because these simplifying

assumptions are less accurate in diabetic patients, particular attention should be paid to the time dependency of these parameters when extending this model to this patient population. Another potentially confounding variable with regard to the stationarity of plasma glucose concentrations is the effect of SGLT2 inhibitors to lower plasma glucose through UGE. However, as the amount of glucose excreted following a single dose of an SGLT2 inhibitor is small in healthy subjects, acute changes in plasma glucose are neither expected nor observed (26). In contrast, treatment of diabetic patients clearly lowers blood glucose concentration in studies of longer duration (23,24–40). As such, treatment-related changes in plasma glucose with time should be considered when extending this model to the chronic treatment of diabetics. This would require an accounting for the impact of UGE on the whole body physiology of glucose homeostasis. Lastly, the f_{reabs} parameter is an empirical descriptor of the fraction of filtered glucose that is reabsorbed. This descriptor is likely determined by the dynamic interplay of physiological rates (e.g., filtrate flow), SGLT1 and SGLT2 transport kinetics (e.g., V_{max}/K_m), plasma glucose concentrations and target biology (e.g. dynamics of SGLT2 expression). Accordingly, this parameter would be expected to vary greatly from patient to patient according to the level of disease and treatment. As such, codifying this aspect of the physiology may be critically important in extending this model to diabetics under chronic treatment. However, this is unlikely to significantly confound the current analysis as glucose is almost completely reabsorbed in healthy rats and humans.

Translational Pharmacology. As pharmacokinetics and physiology are major determinants of SGLT2 inhibitor-mediated UGE, the translation of the primary pharmacology data can only be examined once these aspects have been accounted for as described above. In the current exercise, translational pharmacology can be examined with respect to efficacy (the maximal inhibitor-induced UGE) and potency (the concentration of inhibitor which produces half-maximal UGE). The current work suggests that the *in vivo* potency of SGLT2 inhibitors can be reasonably well predicted from *in vitro* assays and mechanism-based PK/PD modeling of UGE data obtained in rats. One important principle in examining the *in vivo* translation of potency from *in vitro* systems is proper accounting for the unbound fraction of drug between systems. This is important as typically only the unbound fraction is available to interact with the target. This is particularly true for SGLT2 as: (1) only unbound drug is available for filtration to the site of the transporter and (2) the *in vitro* assays are conducted under protein-free conditions. The importance of this correction can be seen with the current results. For example, the estimated rat *in vivo* IC_{50} of dapagliflozin is 29 ng/ml. Converting this to molar units and correcting for an unbound plasma fraction of 0.040, one obtains an unbound IC_{50} estimate of 2.9 nM (vs. 3.0 nM *in vitro*). Likewise, converting the estimated human *in vivo* IC_{50} (3.5 ng/ml) using unbound fraction in human plasma (0.064), one obtains an unbound IC_{50} estimate of 0.55 nM (vs. 1.1 nM *in vitro*). These results suggest that the potency of SGLT2 inhibitors in humans can be reasonably well predicted from *in vitro* assays by accounting for unbound fraction. However, in the current exercise, human potency was predicted via scaling of the IC_{50} estimated obtained from PKPD

modeling of data obtained in rats. In this approach, differences in unbound fraction and *in vitro* potency are considered in relative terms in order to afford scaling of an estimate of IC_{50} obtained in rats. This approach may be useful when unknown factors are suspected of confounding the absolute translation of *in vitro* potency or unbound fraction. Again, this approach yields a predicted IC_{50} that is comparable to that estimated from the human data (6.6 vs. 3.5 ng/ml, respectively).

With regard to efficacy, these results similarly indicate the utility of preclinical data for predicting maximum UGE. The estimated I_{max} of dapagliflozin from the data in healthy subjects was 0.35. This is consistent with previous reports which indicate dapagliflozin is capable of acutely reducing glucose reabsorption up to approximately 30% in healthy subjects (26). This is also similar to the 34.5–43.2% maximum inhibition of glucose reabsorption produced by sergliflozin, another SGLT2 inhibitor, in non-diabetic subjects (41). Similarly, we estimate the I_{max} of dapagliflozin be 0.32 in rats. This estimate is also generally consistent with the value of 0.49 we have previously reported for another SGLT2 inhibitor, PF-04971729, in rats (27). These small differences across compounds and species suggest that maximum UGE is a property of the system, which is reasonably well conserved across rats and humans. As such, we speculate that the I_{max} parameter employed in the current model predominately represents an empirical descriptor of the biological system rather than the maximal level of SGLT2 inhibition. On a mechanistic level, this inhibitory limitation of about one third may reflect the activity of SGLT1 transporters located further downstream in the distal tubule of the nephron. Although outside the scope of the current work, a model that explicitly accounts for these aspects may be useful in providing a better understanding of these observations.

CONCLUSION

A simple biologically based PK/PD model has been developed, which was useful in characterizing the PK/PD data of dapagliflozin in rats and humans. This model provides a structure by which species differences in pharmacokinetics, physiology, and pharmacology can be accounted in order to support clinical pharmacology predictions from preclinical data. Application of this model to preclinical and clinical dapagliflozin data indicates the general predictive utility of *in vitro* pharmacology assays and rat pharmacology. These findings suggest that this model would be useful in supporting the design of SGLT2 inhibitors (early in drug discovery) that are capable of producing a robust proof-of-mechanism (i.e., UGE in the clinic). Future extensions of this model may also provide: (1) a more granular representation of glucose filtration and reuptake, (2) the ability to take additional endpoints of relevance to SGLT2 inhibition (e.g., HbA1c) into consideration, (3) the ability to characterize different patient populations, and (4) the ability to capture dynamic changes with chronic therapy.

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