

# NIH Public Access

**Author Manuscript** 

IEEE Trans Neural Netw. Author manuscript; available in PMC 2012 February 17.

# Published in final edited form as:

IEEE Trans Neural Netw. 2011 June ; 22(6): 829–844. doi:10.1109/TNN.2011.2123917.

# Causality Analysis of Neural Connectivity: Critical Examination of Existing Methods and Advances of New Methods

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# Abstract

Granger causality (GC) is one of the most popular measures to reveal causality influence of time series and has been widely applied in economics and neuroscience. Especially, its counterpart in frequency domain, spectral GC, as well as other Granger-like causality measures have recently been applied to study causal interactions between brain areas in different frequency ranges during cognitive and perceptual tasks. In this paper, we show that: 1) GC in time domain cannot correctly determine how strongly one time series influences the other when there is directional causality between two time series, and 2) spectral GC and other Granger-like causality measures have inherent shortcomings and/or limitations because of the use of the transfer function (or its inverse matrix) and partial information of the linear regression model. On the other hand, we propose two novel causality measures (in time and frequency domains) for the linear regression model, called new causality and new spectral causality, respectively, which are more reasonable and understandable than GC or Granger-like measures. Especially, from one simple example, we point out that, in time domain, both new causality and GC adopt the concept of proportion, but they are defined on two different equations where one equation (for GC) is only part of the other (for new causality), thus the new causality is a natural extension of GC and has a sound conceptual/ theoretical basis, and GC is not the desired causal influence at all. By several examples, we confirm that new causality measures have distinct advantages over GC or Granger-like measures. Finally, we conduct event-related potential causality analysis for a subject with intracranial depth electrodes undergoing evaluation for epilepsy surgery, and show that, in the frequency domain, all measures reveal significant directional event-related causality, but the result from new spectral causality is consistent with event-related time-frequency power spectrum activity. The spectral GC as well as other Granger-like measures are shown to generate misleading results. The proposed new causality measures may have wide potential applications in economics and neuroscience.

#### Keywords

Event-related potential; Granger or Granger-like causality; linear regression model; new causality; power spectrum

# I. Introduction

GIVEN a set of time series, how to define causality influence among them has been a topic for over 2000 years and is yet to be completely resolved [1]–[3]. In the literature, one of the most popular definitions for causality is Granger causality (GC). Due to its simplicity and easy implementation, GC has been widely used. The basic idea of GC was originally conceived by Wiener [4] and later formalized by Granger in the form of linear regression

model [5]. It can be simply stated as follows. If the variance  $(\sigma_{\epsilon_1}^2)$  of the prediction error for

the first time series at the present time is greater than the variance  $(\sigma_{\eta_1}^2)$  of the prediction error by including past measurements from the second time series in the linear regression model, then the second time series can be said to have a causal (driving) influence on the first time series. Reversing the roles of the two time series, one repeats the process to

address the question of driving in the opposite direction. GC value of  $\ln(\sigma_{\epsilon_1}^2/\sigma_{\eta_1}^2)$  is defined to describe the strength of the causality that the second time series has on the first one [5]–

[10]. From GC value, it is clear that: 1)  $\ln \left(\sigma_{\epsilon_1}^2 / \sigma_{\eta_1}^2\right) = 0$  when there is no causal influence

from the second time series to the first one and  $\ln(\sigma_{\epsilon_1}^2/\sigma_{\eta_1}^2) > 0$  when there is, and 2) the

larger the value of  $\ln(\sigma_{\epsilon_1}^2/\sigma_{\eta_1}^2)$ , the higher causal influence. In recent years, there has been significant interest to discuss causal interactions between brain areas which are highly complex neural networks. For instance, with GC analysis Freiwald et al. [7] revealed the existence of both unidirectional and bidirectional influences between neural groups in the macaque inferotemporal cortex. Hesse et al. [9] analyzed the electroencephalogram (EEG) data from the Stroop task and disclosed that conflict situations generate dense webs of interactions directed from posterior to anterior cortical sites and the web of directed interactions occurs mainly 400 ms after the stimulus onset and lasts up to the end of the task. Roebroeck *et al.* [11] explored directed causal influences between neuronal populations in functional magnetic resonance imaging (fMRI) data. Ova et al. [10] demonstrated causal interactions between auditory cortical fields in humans through intracranial evoked potentials to sound. Gow et al. [12] applied Granger analysis to MRI-constrained magnetoencephalogram and EEG data to explore the influence of lexical representation on the perception of ambiguous speech sounds. Gow et al. [13] showed a consistent pattern of direct posterior superior temporal gyrus influence over sites distributed over the entire ventral pathway for words, non-words, and phonetically ambiguous items.

Since frequency decompositions are often of particular interest for neurophysiological data, the original GC in time domain has been extended to spectral domain. Along this line, several spectral Granger or Granger-like causality measures have been developed such as spectral GC [6], [8], conditional spectral GC [6], [8], partial directed coherence (PDC) [14], relative power contribution (RPC) [15], directed transfer function (DTF) [16], and short-time direct directed transfer function (SdDTF) [17]. For two time series, spectral GC, PDC, RPC, and DTF are all equivalent in the sense that, when one of them is zero, the others are also zero. The applications of these measures to neural data have yielded many promising results. For example, Bernasconi and Konig [18] applied Geweke's spectral measures to describe causal interactions among different areas in the cat visual cortex. Liang *et al.* [19] used a time-varying spectral technique to differentiate feedforward, feedback, and lateral

dynamical influences in monkey ventral visual cortex during pattern discrimination. Brovelli *et al.* [20] applied spectral GC to identify causal influences from primary somatosensory cortex to motor cortex in the beta band (15–30 Hz) frequency during lever pressing by awake monkeys. Ding *et al.* [6] discussed conditional spectral GC to reveal that causal influence from area S1 to interior posterior parietal area 7a was mediated by the inferior posterior parietal area 7b during monkey visual pattern discrimination task. Sato *et al.* [21] applied PDC to fMRI to discriminate physiological and nonphysiological components based on their frequency characteristics. Yamashita *et al.* [15] applied RPC to evaluate frequency-wise directed connectivity of BOLD signals. Kaminski and Liang [22] applied short-time DTF to show predominant direction of influence from hippocampus to supramamilary nucleus at the theta band (3.7–5.6 Hz) frequency. Korzeniewska *et al.* [17] used SdDTF to reveal frequency-dependent interactions, particularly in high gamma (> 60 Hz) frequencies, between brain regions known to participate in the recorded language task.

In time domain, the well-known GC value defined by  $\ln(\sigma_{\epsilon_1}^2/\sigma_{\eta_1}^2)$  is only related to noise terms of the linear regression models and has nothing to do with coefficients of the linear regression model of two time series. As a result, this definition may miss some important information and may not be able to correctly reflect the real strength of causality when there is directional causality from one time series to the other. That is, the larger GC value does not necessarily mean higher causality, or vice versa, although in general this definition is very useful to determine whether there is directional causality between two time series, that

is,  $\ln(\sigma_{\epsilon_1}^2/\sigma_{\eta_1}^2) = 0$  means no causality and  $\ln(\sigma_{\epsilon_1}^2/\sigma_{\eta_1}^2) \neq 0$  means existence of causality. Therefore, the GC value may not correctly reflect real causal influence between two channels. In other words, GC values for different pairs of channels even from the same subject may not be comparable. As such, the common practice of using thickness of arrows in a diagram to represent the strength of causality for different pairs of channels even in the same subject may not be true. In the literature, the other GC value defined in [7] is only related to one column of the coefficient matrix of the linear regression model and has nothing to do with the terms in other columns and noise terms. This also makes this definition suffer from similar pitfalls. Therefore, a researcher must use caution when drawing any conclusion based on these two GC values. In the frequency domain, the spectral GC is defined by Granger [5] based on the inverse matrix of the transfer matrix and the noise terms of the linear regression model and called it causality coherence. This definition in nature is a generalization of coherence where researchers have already realized that coherence cannot be used to reveal real causality for two time series. For this reason, since then various definitions of GC in frequency domain have been developed. Among the most popular definitions are the spectral GC [6] and [8], PDC [14], RPC [15], and DTF [16]. The spectral GC can be applied to two time series or two groups of time series, PDC, RPC, and DTF can be applied to multidimensional time series. DTF and RPC are not able to distinguish between direct and indirect pathways linking different structures and as a result they do not provide the multivariate relationships from a partial perspective [21]. PDC lacks a theoretical foundation [23]. In general, the above spectral Granger or Granger-like causality definitions are based on the transfer function matrix (or its inverse matrix) of the linear regression model and thus may not be able to reflect the real strength of causality as pointed out later in detail in this paper. Note that the transfer function matrix or its inverse matrix is different from the coefficient matrix of the linear regression model (frequency model), on which we rely in this paper to propose new spectral causality.

In this paper, on one hand, in time domain we define a new causality from any time series Y to any time series X in the linear regression model of multivariate time series, which describes the proportion that Y occupies among all contributions to X. Especially, we use one simple example to show that both the new causality and GC adopt the concept of

proportion, but they are defined on two different equations where one equation (for GC) is only part of the other equation (for new causality), and therefore the new causality is a natural extension of GC and GC is not the desired causal influence at all. As such, even when the GC value is zero, there still exists a real causality which can be revealed by a new causality. Therefore, the popular traditional GC cannot reveal the real strength of causality at all and researchers must apply caution in drawing any conclusion based on the GC value. On the other hand, in frequency domain we point out that any causality definition based on the transfer function matrix (or its inverse matrix) of the linear regression model in general may not be able to reveal the real strength of causality between two time series. Since almost all existing spectral causality definitions are based on the transfer function matrix (or its inverse matrix) of the linear regression model, we take the widely used spectral GC, PDC, and RPC as examples and point out their inherent shortcomings and/or limitations. To overcome these difficulties, we define a new spectral causality that describes the proportion that one variable occupies among all contributions to another variable in the multivariate linear regression model (frequency domain). By several simulated examples, one can clearly see that our new definitions (in time and frequency domain) are advantageous over existing definitions. In particular, for a real event-related potential (ERP) EEG data from a seizure patient, the application of new spectral causality shows promising and reasonable results. But the applications of spectral GC, PDC, and RPC all generate misleading results. Therefore, our new causality definitions may open a new window to study causality relationships and may have wide applications in economics and neuroscience.

This paper is organized as follows. Causality analyses in time domain and frequency domain are discussed in Section II and Section III, respectively. Several examples are provided in Section IV. Concluding remarks are given in Section V.

# II. Granger Causality in Time Domain

In this section, we first introduce the well-known GC and conditional GC, and then we define a new causality.

We begin with a bivariate time series. Given two time series  $X_1(t)$  and  $X_2(t)$ , which are assumed to be jointly stationary, their autoregressive representations are described as

$$\begin{cases} X_{1,t} = \sum_{j=1}^{m} \mathbf{a}_{11,j} X_{1,t-j} + \epsilon_{1,t} \\ X_{2,t} = \sum_{j=1}^{m} \mathbf{a}_{22,j} X_{2,t-j} + \epsilon_{2,t} \end{cases}$$
(1)

and their joint representations are described as

$$\begin{cases} X_{1,t} = \sum_{j=1}^{m} a_{11,j} X_{1,t-j} + \sum_{j=1}^{m} a_{12,j} X_{2,t-j} + \eta_{1,t} \\ X_{2,t} = \sum_{j=1}^{m} a_{21,j} X_{1,t-j} + \sum_{j=1}^{m} a_{22,j} X_{2,t-j} + \eta_{2,t} \end{cases}$$
(2)

where t = 0, 1, ..., N, the noise terms are uncorrelated over time,  $\varepsilon_i$  and  $\eta_i$  have zero means and variances of  $\sigma_{\varepsilon_i}^2$  and  $\sigma_{\eta_i}^2$  i = 1, 2. The covariance between  $\eta_1$  and  $\eta_2$  is defined by  $\sigma_{\eta_1\eta_2}$ =  $\operatorname{cov}(\eta_1, \eta_2)$ .

Now consider the first equalities in (1) and (2). According to the original formulations in [4] and [5], if  $\sigma_{\eta_1}^2$  is less than  $\sigma_{\epsilon_1}^2$  in some suitable statistical sense,  $X_2$  is said to have a causal influence on  $X_1$ . In this case, the first equality in (2) is more accurate than that in (1) to

estimate  $X_1$ . Otherwise, if  $\sigma_{\eta_1}^2 = \sigma_{\epsilon_1}^2$ ,  $X_2$  is said to have no causal influence on  $X_1$ . In this case, two equalities are same. Such kind of causal influence, called GC [6], [8], is defined by

$$F_{X_2 \to X_1} = \ln \frac{\sigma_{\epsilon_1}^2}{\sigma_{\eta_1}^2}.$$
(3)

Obviously,  $F_{X_2 \to X_1} = 0$  when there is no causal influence from  $X_2$  to  $X_1$  and  $F_{X_2 \to X_1} > 0$  when there is. Similarly, the causal influence from  $X_1$  to  $X_2$  is defined by

$$F_{X_1 \to X_2} = \ln \frac{\sigma_{\epsilon_2}^2}{\sigma_{\eta_2}^2}.$$
(4)

To show whether the interaction between two time series is direct or is mediated by another recorded time series, conditional GC [6], [24] was defined by

$$F_{X_2 \to X_1 \mid X_3} = \ln \frac{\sigma_{\epsilon_3}^2}{\sigma_{\eta_3}^2}$$
(5)

where  $\sigma_{\epsilon_3}^2$  and  $\sigma_{\eta_3}^2$  are the variances of two noise terms  $\varepsilon_3$  and  $\eta_3$  of the following two joint autoregressive representations:

$$X_{1,t} = \sum_{j=1}^{m} \mathbf{a}_{11,j} X_{1,t-j} + \sum_{j=1}^{m} \mathbf{a}_{13,j} X_{3,t-j} + \epsilon_{3,t}$$
(6)

and

$$X_{1,t} = \sum_{j=1}^{m} a_{11,j} X_{1,t-j} + \sum_{j=1}^{m} a_{12,j} X_{2,t-j} + \sum_{j=1}^{m} a_{13,j} X_{3,t-j} + \eta_{3,t}.$$
(7)

According to this definition,  $F_{X_2 \to X_1|X_3} = 0$  means that no further improvement in the prediction of  $X_1$  can be expected by including past measurements of  $X_2$ . On the other hand, when there is still a direct component from  $X_2$  to  $X_1$ , the past measurements of  $X_1$ ,  $X_2$ , and

 $X_3$  together result in better prediction of  $X_1$ , leading to  $\sigma_{\eta_3}^2 < \sigma_{\epsilon_3}^2$ , and  $F_{X_2 \to X_1 | X_3} > 0$ .

For GC, we point out some properties as follows.

Property 1:

i. Consider the following model:

$$X_{1,t} = a_{12,1} X_{2,t-1} + \eta_{1,t}$$

$$X_{2,t} = 0.8 X_{2,t-1} + \eta_{2,t}$$
(8)

where  $\eta_1$ ,  $\eta_2$  are two independent white noise processes with zero mean and variances  $\sigma_{\eta_2}^2 = 1$  Fig. 1 shows GC values in two cases: a)  $a_{12, 1} = -0.8$  and  $\sigma_{\eta_1}^2$  varies from 0.01 to 2; b)  $a_{12, 1}$  varies from -0.1 to -0.95 and  $\sigma_{\eta_1}^2 = 1$ . From Fig. 1(a) and (b), one can see that the GC value from  $X_2$  to  $X_1$  decreases as the variance  $\sigma_{\eta_1}^2$ 

increases (or increases as the amplitude  $|a_{12, 1}|$  increases). That means that increasing the amplitude  $|a_{12, 1}|$  or decreasing variance of the residual term  $\eta_1$  will increase the GC value from  $X_2$  to  $X_1$ . Thus, we conclude that GC is actually a relative concept, a larger GC value from  $X_2$  to  $X_1$  means that the causal influence from the first term  $a_{12, 1}X_{2,t-}$  occupies a larger portion compared to the influence from the residual term  $\eta_{1, t}$ , or vice versa.

ii. Consider the following model:

$$\begin{cases} X_{1,t} = a_{11,1} X_{1,t-1} - 0.8 X_{2,t-1} + \eta_{1,t} \\ X_{2,t} = a_{21,1} X_{1,t-1} + 0.8 X_{2,t-1} + \eta_{2,t} \end{cases}$$
(9)

where  $0 < a_{11,1}, a_{21,1} < 1$  and for simplicity  $\eta_1, \eta_2$  are assumed to be two

independent white-noise processes with zero mean and variances  $\sigma_{\eta_1}^2 = 1 = \sigma_{\eta_2}^2$ . Fig. 2 shows GC from  $X_2$  to  $X_1$  for (9) under different parameters  $a_{11,1}$  and  $a_{21,1}$ . When we calculate GC, it should be pointed out that for each specific (9) we generate a dataset of 200 realizations of 10 000 time points. For each realization, we estimate AR models [autoregressive representations (1) and joint representations (2)] with the order of 8 by using the least-squares method and calculate GC where the order 8 fits well for all examples throughout this paper [see Fig. 2(a) and (b) from which one can see GC keeps steady when the order of the estimated models is greater than 8]. Then we obtain the average value across all realizations and get GC from  $X_2$  to  $X_1$ . From Fig. 2, one can clearly see that GC from  $X_2$  to  $X_1$  has nothing to do with parameters  $a_{11,1}$  and  $a_{21,1}$  [of course, choices of parameters  $a_{11,1}$  and  $a_{21,1}$  are such that (9) does not diverge]. This property is consistent with the spectral GC result introduced later.

iii. For (2), if  $\eta_{2,t} \equiv 0$  or  $\eta_{1,t} = \eta_{2,t}$ , GC from  $X_2$  to  $X_1$  equals zero. This can be proved from (17.29), [6] and the spectral GC (32) introduced later.

Except for the two specific cases in (iii) of Property 1, in general GC and conditional GC are useful to show whether theoretically there is directional interaction between two neurons or among three neurons. When there exists causal influence, a question arises: does the GC value or the conditional GC value reveal the real strength of causality? to answer this question, let us consider the following simple model:

$$\begin{cases} X_{1,t} = a_{12,1} X_{2,t-1} + \eta_{1,t} \\ X_{2,t} = a_{21,1} X_{1,t-1} + \eta_{2,t} \end{cases}$$
(10)

where  $\eta_1$  and  $\eta_2$  are two independent white-noise processes with zero mean and  $a_{12, 1}a_{21, 1} \neq 0$ . From (10), one can get

$$X_{1,t} = a_{12,1} \left( \underbrace{a_{21,1} X_{1,t-2} + \eta_{2,t-1}}_{=a_{12,1} a_{21,1} X_{1,t-2} + a_{12,1} \eta_{2,t-1} + \eta_{1,t}}_{=a_{12,1} a_{21,1} X_{1,t-2} + a_{12,1} \eta_{2,t-1} + \eta_{1,t}} \right) + \eta_{1,t}$$

$$(11)$$

So, the GC value

$$F_{x_2 \to x_1} = \ln \frac{a_{12,1}^2 \sigma_{\eta_2}^2 + \sigma_{\eta_1}^2}{\sigma_{\eta_1}^2} = -\ln \left( 1 - \frac{a_{12,1}^2 \sigma_{\eta_2}^2}{a_{12,1}^2 \sigma_{\eta_2}^2 + \sigma_{\eta_1}^2} \right) \in [0, +\infty)$$
(12)

or equivalently

$$F_{x_2 \to x_1} = \frac{a_{12,1}^2 \sigma_{\eta_2}^2}{a_{12,1}^2 \sigma_{\eta_2}^2 + \sigma_{\eta_1}^2} \in [0, 1]$$
(13)

which is only related to the last two noise terms and has nothing to do with the first term. It is noted that all three terms make contributions to current  $X_{1,t}$ , and  $a_{12, 1}a_{21, 1}X_1$ , t-2 must have causal influence on  $X_{1,t}$  and must be considered to illustrate real causality. Especially,

when  $\sigma_{\eta_2}^2 = 0$ , we have  $X_{1, t} = a_{12, 1}a_{21, 1}X_{1, t-2} + \eta_{1, t}$  and  $F_{X_2 \to X_1} = 0$ . Since  $a_{21, 1}X_{1, t-2}$  comes from  $X_{2, t-1}$ , we can surely know that  $X_2$  has real nonzero causality on  $X_1$  because  $a_{12, 1}a_{21, 1} \neq 0$ . Thus, GC or conditional GC may not reveal real causality at all. As such, these two definitions have their inherent shortcomings and/or limitations to illustrate the real strength of causality. These comments are summarized in the following remark.

Remark 1:

i. When there is causality from  $X_2$  to  $X_1$ ,  $F_{X_2 \to X_1}$  varies in  $(0, +\infty)$ . GC may not correctly reveal the real strength of causality. Thus, it is hard to say how much influence is caused only based on the value of  $F_{X_2 \to X_1}$ . For example, for two sets of different time series  $\{X_1, X_2\}$  and  $\{\bar{X}_1, \bar{X}_2\}$  their GC values may not be comparable. When  $F_{X_2 \to X_1} = 1$  and  $F_{\bar{X}_2 \to \bar{X}_1} = 10$ , we cannot say that the influence caused from  $X_2$  to  $X_1$  in the set of time series  $\{X_1, X_2\}$  is smaller than that caused from  $\bar{X}_2$  to  $\bar{X}_1$  in the set of time series  $\{\bar{X}_1, \bar{X}_2\}$ . As such, a smaller value of  $F_{X_2 \to X_1}$  does not mean  $X_2$  has less causal influence on  $X_1$ . Thus, for actual physical data when one obtains a small value of  $F_{X_2 \to X_1}$  (e.g.,  $F_{X_2 \to X_1} = 0.1$ ), it does not mean that there is no causality from  $X_2$  to  $X_1$  and the causal influence from  $X_2$  to  $X_1$  can be ignored. On the contrary, when one obtains a large value of  $F_{X_2 \to X_1}$  (e.g.,  $F_{X_2 \to X_1} = 1$  which can be ignored compared to  $F_{X_2 \to X_1} = +\infty$ ), it does not mean that there is strong causality from  $X_2$  to  $X_1$ . Let us take a look at the following two models:

$$\begin{pmatrix} X_{1,t} = 0.8X_{1,t-1} - 0.8X_{2,t-1} + \eta_{1,t} \\ X_{2,t} = 0.8X_{2,t-1} + \eta_{2,t} \end{cases}$$
(14)

and

$$\begin{cases} X_{1,t} = -0.8X_{2,t-1} + \eta_{3,t} \\ X_{2,t} = 0.8X_{2,t-1} + \eta_{2,t} \end{cases}$$
(15)

where  $\eta_1$ ,  $\eta_2$ , and  $\eta_3$  are three independent white-noise processes with zero mean and variances  $\sigma_{\eta_1}^2 = 0.005$ ,  $\sigma_{\eta_2}^2 = 1$  and  $\sigma_{\eta_3}^2 = 0.01$ . For (14) we can obtain GC  $F_{X_2 \to X_1}$ = 4.86. For (15) we can obtain GC  $F_{X_2 \to X_1} = 4.18$ . In (14), the noise term  $\eta_1$  has smaller variance  $\sigma_{\eta_1}^2$  so that a snmall change (compared to  $\sigma_{\eta_1}^2$ ) of the variance of the residual  $\varepsilon_1$  of the estimated autoregressive representation model for  $X_1$  may lead to a bigger GC value [see GC definition in (3)] as shown in  $F_{X_2 \to X_1} = 4.86$ . A similar analysis holds for (15). Therefore, it seems that both of GC values are "intuitively reasonable" based on GC definition. Now a question arises: Does the "reasonable" GC value correctly reflect the real strength of causality? Unfortunately, the answer is no. Note that: 1)  $X_2$  is same in (14) and (15); 2)  $X_1$  is driven by  $X_2$  in (15); 3)  $X_1$  is driven by  $X_1$  and  $X_2$  in (14); and 4) influence from  $\eta_1$ or  $\eta_3$  is very small and can even be ignored because of their small variances, and

thus intuitively we can draw a conclusion that the real causality from  $X_2$  to  $X_1$  in (14) should be weaker than that from  $X_2$  to  $X_1$  in (15). However,  $F_{X_2 \to X_1} = 4.86$  for (14) is larger than  $F_{X_2 \to X_1} = 4.18$  for (15). As such, the traditional GC may not be reliable at least in the above two cases, that means that the resulting GC value may not be truely reflect the real strength of causality. Hence, in general, it is questionable whether the GC value reveals causal influence between two neurons.

- ii. The same problem as (i) exists for conditional GC.
- iii. Consider Fig. 3 where 2 or 10 are direct GC values. The total causal influence from *Y* to *X* is the summation of the direct causal influence from *Y* to *X* (i.e., 2) and the indirect causal influence mediated by *Z*. Obviously, the indirect causal influence mediated by *Z* does not equal to  $2 \times 10 = 20$  since this influence must less than the direct causal influence 2 from *Y* to *Z*. This implies that the indirect causality along the route  $Y \rightarrow Z \rightarrow X$  does not equal  $F_{Y \rightarrow Z} \times F_{Z \rightarrow X}$ .

Because of the above-mentioned shortcomings and/or limitations of GC, we next give a new causality definition of multivariate time series. Let us consider the following general model:

$$\begin{cases} X_{1,t} = \sum_{j=1}^{m} a_{11,j} X_{1,t-j} + \dots + \sum_{j=1}^{m} a_{1n,j} X_{n,t-j} + \eta_{1,t} \\ X_{2,t} = \sum_{j=1}^{m} a_{21,j} X_{1,t-j} + \dots + \sum_{j=1}^{m} a_{2n,j} X_{n,t-j} + \eta_{2,t} \\ \vdots \\ X_{n,t} = \sum_{j=1}^{m} a_{n1,j} X_{1,t-j} + \dots + \sum_{j=1}^{m} a_{nn,j} X_{n,t-j} + \eta_{n,t} \end{cases}$$
(16)

where  $X_i(i = 1, ..., n)$  are *n* time series, t = 0, 1, ..., N,  $\eta_i$  has zero mean and variance of  $\sigma_{\eta_i}^2$  and  $\sigma_{\eta_i\eta_k} = \operatorname{cov}(\eta_i, \eta_k)$ , *i*, k = 1, ..., n. Based on (16), Fig.4 clearly shows contributions to  $X_{k,t}$ , which include  $\sum_{j=1}^{m} a_{k1,j} X_{1,t-j}, ..., \sum_{j=1}^{m} a_{kn,j} X_{n,t-j}$  and the noise term  $\eta_{k,t}$  where the influence from  $\sum_{j=1}^{m} a_{kk,j} X_{k,t-j}$  is causality from  $X_k$ 's own past values. Each contribution plays an important role in determining  $X_{k,t}$ . If  $\sum_{j=1}^{m} a_{ki,j} X_{i,t-j}$  occupies a larger portion among all those contributions, then  $X_i$  has stronger causality on  $X_k$ , or vice versa. Thus, a good definition for causality from  $X_i$  to  $X_k$  in time domain should be able to describe what proportion  $X_i$  occupies among all these contributions. This is a general guideline for proposing any causality method (i.e., all contributions must be considered). For (11), let us define

$$\bar{\eta}_t \stackrel{\Delta}{=} a_{12,1} \eta_{2,t-1} + \eta_{1,t} \tag{17}$$

which is the summation of two noise terms and each noise term makes contributions to  $\overline{\eta}$ . To describe what proportion  $\eta_2$  occupies in  $\overline{\eta}$ , we define

$$\frac{a_{12,1}^{2}\sum_{t=1}^{N}\eta_{2,t-1}^{2}}{a_{12,1}^{2}\sum_{t=1}^{N}\eta_{2,t-1}^{2}+\sum_{t=1}^{N}\eta_{1,t}^{2}}=\frac{a_{12,1}^{2}\sigma_{\eta_{2}}^{2}}{a_{12,1}^{2}\sigma_{\eta_{2}}^{2}+\sigma_{\eta_{1}}^{2}}$$
(18)

which is the same as the GC defined in (13). Therefore, here, in nature, GC is actually defined based on the noise (17) and follows the above guideline. Motivated by this idea as

well as (i) of Property 1, we can naturally extend the noise (17) to the *k*th equation of (16) and define a new direct causality from  $X_i$  to  $X_k$  as follows:

$$n_{\substack{X_{i} \longrightarrow X_{k}}} = \frac{\sum_{t=m}^{N} \left(\sum_{j=1}^{m} a_{ki,j} X_{i,t-j}\right)^{2}}{\sum_{h=1}^{n} \sum_{t=m}^{N} \left(\sum_{j=1}^{m} a_{kh,j} X_{h,t-j}\right)^{2} + \sum_{t=m}^{N} \eta_{k,t}^{2}}.$$
(19)

When N is large enough

$$\sum_{t=m}^{N} \eta_{k,t}^{2} = \sum_{t=1}^{N} \eta_{k,t}^{2} - \sum_{t=1}^{m} \eta_{k,t}^{2} = N\sigma_{\eta k}^{2} - \sum_{t=1}^{m} \eta_{k,t}^{2} \approx N\sigma_{\eta k}^{2}.$$

Then, (19) can be approximated as

$$\frac{\sum_{t=m}^{N} \left(\sum_{j=1}^{m} a_{ki,j} X_{i,t-j}\right)^{2}}{\sum_{h=1}^{n} \sum_{t=m}^{N} \left(\sum_{j=1}^{m} a_{kh,j} X_{h,t-j}\right)^{2} + N\sigma_{\eta k}^{2}}.$$
(20)

Throughout this paper, we always assume that N is large enough so that  $n_{x_i \to x_k}$  is always defined as (20).

When n = 2 in (16), in his early work [8] Geweke stated that GC  $F_{X_2 \to X_1} = 0$  if and only if  $a_{12,j} \equiv 0$ . According to this statement, if  $a_{12,j} \equiv 0$ , then there is no causality (or GC). If  $a_{12,j} \neq 0$ , then there is GC. Similarly, for (20) we can make the following statement:  $n_{x_2 \to X_1} = 0$  if and only if  $a_{12,j} \equiv 0$ . If  $n_{x_2 \to X_1} \neq 0$ , then  $a_{12,j} \neq 0$ , which implies that there is causality from  $X_2$  to  $X_1$ . If  $n_{x_2 \to X_1} = 0$ , then  $a_{12,j} \equiv 0$  and there is no causality from  $X_2$  to  $X_1$  As such, the new causality  $n_{x_1 \to X_k} = 0$ , then  $a_{12,j} \equiv 0$  and there is no causality from  $X_2$  to  $X_1$  As such, the new causality  $n_{x_1 \to X_k} = 0$  and there is very important because pairwise treatments of signals can lead to errors in the estimation of mutual influences between channels [25] and [26].

New causality based on (11) can be written as

$$n_{X_{2} \xrightarrow{D} X_{1}} = \frac{\sum_{t=1}^{N} (a_{12,1} X_{2,t-1})^{2}}{\sum_{t=1}^{N} (a_{12,1} X_{2,t-1})^{2} + \sum_{t=1}^{N} \eta_{1,t}^{2}} = \frac{\sum_{t=1}^{N} (a_{12,1} X_{2,t-1})^{2}}{\sum_{t=1}^{N} (a_{12,1} X_{2,t-1})^{2} + N \sigma_{\eta_{1}}^{2}}$$
(21)

which describes what proportion  $X_2$  occupies among two contributions in  $X_1$  [see (11)]. Note that for (11) GC  $F_{X2} \rightarrow X_1$  is proposed based on (17) and describes what proportion  $\eta_2$  occupies among two contributions in  $\overline{\eta}$  [see (18)]. Thus GC actually reveals causal influence from  $\eta_2$  to  $\overline{\eta}$ , but it does not reveal causal influence from  $X_2$  to  $X_1$  at all by noting that  $\overline{\eta}$  is

only partial information of  $X_1$ , i.e., the noise terms  $a_{12, 1}\eta_{2,t-}+\eta_{1,t}$ . Any causality definition by using only partial information of  $X_1$  may inevitably be questionable. As such, new causality is totally different from GC. In general, we can make some key comments in the following remark.

Remark 2:

i.

It is easy to see that  $0 \le n_{x_i \to x_k} \le 1$ . Moreover, it is meaningful and understandable that a larger new causality value reveals a larger causal influence for different sets of bivariate time series. Thus, in this way, the thickness of arrows in Fig. 13(a) representing the strength of the connections makes much sense. As pointed out in (i) of Remark 1, a larger GC value does not necessarily reveals a larger causal influence for different sets of bivariate time series. Hence, if one uses thickness to represent strength of connections based on GC values for different sets of bivariate time series, it may not make sense. However, unfortunately almost all researchers did in this way after calculating GC values for different sets (pairs) of bivariate time series.

ii.

For (14) and (15), we can get  $n_{x_2 \to x_1}^{\text{D}} = 0.110$  and 0.994, respectively. For (15),

 $n_{X_2 \xrightarrow{D} X_1} = 0.994$  means that influence from the noise term  $\eta_3$  to  $X_1$  is very small and  $X_1$  is almost completely driven by  $X_2$ . Hence, the real causality from  $X_2$  to  $X_1$  for (15) is very close to that for the following model:

$$\begin{cases} X_{1,t} = -0.8X_{2,t-1} \\ X_{2,t} = 0.8X_{2,t-1} + \eta_{2,t} \end{cases}$$
(22)

whose real causality from  $X_2$  to  $X_1$  obviously equals 1. The causality value  $n_{12} = 0.994$ 

 $n_{x_2 \to x_1} = 0.994$  correctly reveals the real causality from  $X_2$  to  $X_1$  for (15), which is close to 1. For (14), we can easily show that influence from the noise term  $\eta_1$  to  $X_1$  is very small compared to the causal influence from  $X_2$  to  $X_1$  and  $X_1$  is almost completely driven by  $X_1$  and  $X_2$ . Hence, the real causality from  $X_2$  to  $X_1$  for (14) is very close to that for the following model:

$$\begin{cases} X_{1,t} = 0.8X_{1,t-1} - 0.8X_{2,t-1} \\ X_{2,t} = 0.8X_{2,t-1} + \eta_{2,t} \end{cases}$$
(23)

where  $X_1$ 's past value also makes a contribution to  $X_1$ 's current value. Comparing (22) to (23), one can clearly see that the real causality from  $X_2$  to  $X_1$  for (23) is surely weaker than that for (22). By noting small variances of the noise terms, this is why we mention the intuitive conclusion for (14) and (15) pointed in (i) of

Remark 1. The causality value  $n_{x_2 \to x_1}^{p} = 0.110$  for (14) is smaller than causality value  $n_{x_2 \to x_1}^{p} = 0.994$  for (15). This result is consistent with the above analysis. However, the GC value  $F_{X_2 \to X_1} = 4.86$  for (14) is larger than the GC value  $F_{X_2 \to X_1}$ = 4.18 for (15), which violates the above analysis. In fact, from  $n_{x_2 \to x_1}^{p} = 0.110$  for (14), one can see that  $X_1$ 's past value makes a rather major contribution to  $X_1$ 's current value. But this contribution is not considered in the GC as pointed in (ii) of Property 1 where the GC value from  $X_2$  to  $X_1$  has nothing to do with the parameters

 $a_{11,1}$  and  $a_{21,1}$ . Therefore, the causality definition in (20) is much more reasonable, stable, and reliable than GC.

iii. Consider the following two models:

$$\begin{cases} X_{1,t} = -0.99X_{2,t-1} + \eta_{1,t} \\ X_{2,t} = 0.99X_{1,t-1} + 0.1X_{2,t-1} + \eta_{2,t} \end{cases}$$
(24)

and

$$\begin{cases} \bar{X}_{1,t} = -0.99\bar{X}_{2,t-1} + \bar{\eta}_{1,t} \\ \bar{X}_{2,t} = 0.1\bar{X}_{2,t-1} + \bar{\eta}_{2,t} \end{cases}$$
(25)

where  $\eta_1$  and  $\eta_2$  are two independent white-noise processes with zero mean and

variances  $\sigma_{\eta_1}^2 = 1$ ,  $\sigma_{\eta_2}^2 = 0.1$ ,  $\eta_{1,t} = \bar{\eta}_{1,t}$ ,  $\eta_{2,t} = \bar{\eta}_{2,t}$  and the initial conditions  $X_{1,0} = \bar{X}_{1,0}$ and  $X_{2,0} = \bar{X}_{2,0}$ . We can obtain  $F_{X_2 \to X_1} = 0.092$  for both (24) and (25),  $n_{X_2 \to X_1} = 0.964$  for (24), and  $n_{X_2 \to X_1} = 0.090$  for (25). Fig. 5 shows trajectories –

 $0.99X_2$ ,  $-0.99X_2$  and  $\eta_1$  for one realization of (24) and (25). From Fig. 5(a) and (c), one can clearly see that amplitudes of  $-0.99X_2$  are much larger than that of  $\eta_1$  and the contribution from  $-0.99X_2$ , t-1 occupies much larger portion compared to that from  $\eta_1$ , t, as a result, the causal influence from  $X_2$  to  $X_1$  occupies a major portion compared to the influence from  $\eta_1$  and the real strength of causality from  $X_2$  to  $X_1$ 

should have higher value. This fact is real. Our causality value  $n_{x_2} \xrightarrow{D} X_1 = 0.964$  for (24) is consistent with this fact. Similarly, from Fig. 5(b) and (c), one can clearly see that amplitude of  $-0.99X_2$  is much smaller than that of  $\eta_1$  and the contribution from  $-0.99X_2$ ,  $t_{t-1}$  occupies much smaller portion compared to that from  $\eta_{1, t}$ , as a result, the causal influence from  $X_2$  to  $X_1$  occupies a rather small portion compared to the influence from  $\eta_1$  and the real strength of causality from  $X_2$  to  $X_1$  should

have a smaller value. This fact is also real. Our causality  $n_{x_2 \to x_1} = 0.090$  for (25) is consistent with this fact. However, GC always equals 0.092 for both of (24) and (25) and does not reflect such kind of changes at all, and violates the above two real facts.

iv. For the two specific cases in (iii) of Property 1 and for any nonzero  $a_{12,j}$ , we have

 $F_{X_2 \to X_1} = 0$  for (2). However, one can easily check  $n_{X_2 \to X_1} \neq 0$  if  $X_2 \neq 0$ , that is, there is real causality. Thus, GC  $F_{X_2 \to X_1} = 0$  does not necessarily imply no real causality, but new causality  $n_{X_2 \to X_1} = 0$  must imply no real causality (no GC). So, new causality reveals real causality more correctly than GC.

- **v.** Once (16) is evaluated based on the *n* time series  $X_1, \ldots, X_n$ , from (20) the direct bidirectional causalities between any two channels can be obtained. This process can save much computation time compared with the remodeling and recomputation by using conditional GC to compute the direct causality.
- vi. Based on this definition, one may define the indirect causality from  $X_i$  to  $X_k$  via  $X_l$  as follows:

$$n_{\substack{X_i \longrightarrow X_k \text{ via } X_l}} = n_{\substack{D \\ X_i \longrightarrow X_l}} \times n_{\substack{X_l \longrightarrow X_l}}.$$

This cascade property does not hold for the previous GC definition as discussed in (iii) of Remark 1.

**vii.** Given any route  $R: X_i \to X'_{l_1} \to X'_{l_2} \to \cdots, \to X'_{l_h} \to X_k$  where

 $\{X'_{l_1}, \ldots, X'_{l_h}\} \subseteq \{X_1, \ldots, X_n\} - \{X_i, X_k\}$ , the indirect causality from  $X_i$  to  $X_k$  via this route R may be defined as

$$n_{\substack{x_i \longrightarrow x_k \text{ via route } R}} = n_{\substack{x_i \longrightarrow x'_{l_1}}} \times \prod_{s=1}^{h-1} n_{\substack{x'_{l_s} \longrightarrow x'_{l_{s+1}}}} \times n_{\substack{x'_{l_h} \longrightarrow x_k}}.$$
(26)

Let  $S_{ik}$  be the set of all such kind of routes, we may define the total causality from  $X_i$  to  $X_k$  as

$$n_{X_i \to X_k} = n_{X_i \to X_k} + \sum_{R \in S_{ik}} n_{X_i \to X_k} \quad \text{via route} \quad R.$$
(27)

Let  $n_{X_i \to X_k}$  be the causality calculated based on the estimated AR model of the pair  $(X_i, X_k)$ . The exact relationship between  $n_{X_i \to X_k}$  and  $\stackrel{n}{\underset{x_i \to x_k}{\longrightarrow}}$ in (27) keeps unknown to us.

viii. For the three time series as shown in Fig. 3, conditional GC can help to obtain the

direct causality from *Y* to *X* (i.e.,  $F_{y \to X}^{\text{D}}$ ). As a result, the indirect causality from *Y* to *X* via *Z* (i.e.,  $F_{y \to X}^{\text{D}}$ ) equals  $F_{y \to X}^{\text{T}} - F_{y \to X}^{\text{D}}$ , where  $F_{y \to X}^{\text{T}}$  is the total causality from *Y* to *X*. For multiple time series, given a route, one may not obtain the indirect causality based on previous GC definition. For example, in Fig. 6 the indirect causality via the route  $R': Y \to W \to Z \to X$  cannot be obtained based on previous GC definition. However, using (26) we can get the indirect causality via the route *R'*.

For a given model, in general we do not know exactly what the real causality is. But as shown in (i)–(iv) of Remark 2, we point out that new causality value more correctly reveals the real strength of the causality than GC, and traditional GC may give misleading interpretation result.

# III. GC in Frequency Domain

In the preceding section, we discussed causality in the time domain. In this section, we move to the counterpart: frequency domain. We first introduce a new spectral causality. Then we list three widely used Granger-like causality measures and point out their shortcomings and/ or limitations.

Consider the general (16). Taking Fourier transformation on both side of (16) leads to

$$X_{1}(f) = a_{11}(f)X_{1}(f) + \dots + a_{1n}(f)X_{n}(f) + \eta_{1}(f)$$

$$X_{2}(f) = a_{21}(f)X_{1}(f) + \dots + a_{2n}(f)X_{n}(f) + \eta_{2}(f)$$

$$\vdots$$

$$X_{n}(f) = a_{n1}(f)X_{1}(f) + \dots + a_{nn}(f)X_{n}(f) + \eta_{n}(f)$$
(28)

where

$$a_{lj}(f) = \sum_{k=1}^{m} a_{lj,k} e^{-i2\pi fk}, i = \sqrt{-1}, l, j = 1, \dots, n.$$
(29)

From (28), one can see that contributions to  $X_k(f)$  include not only  $a_{k1}(f)X_1(f), \ldots, a_{kk-1}(f)X_{k-1}(f) a_{kk+1}(f)X_{k+1}(f), \ldots, a_{kn}(f)X_n(f)$  and the noise term  $\eta_k(f)$ , but also  $a_{kk}(f)X_k(f)$ . Fig. 7 describes the contributions to  $X_k(f)$ , which include  $a_{k1}(f)X_1(f), \ldots, a_{kn}(f)X_n(f)$  and the noise term  $\eta_k(f)$  where the influences from  $a_{kk}(f)X_k(f)$  are causality from  $X_k$ 's own past contribution. So, it motivates us to define a new direct causality from  $X_i$  to  $X_k$  in the frequency domain as follows:

$$N_{\substack{x_i \to x_k}}(f) = \frac{|a_{ki}(f)|^2 S_{x_i x_i}(f)}{|a_{k1}(f)|^2 S_{x_1 x_1}(f) + \dots + |a_{kn}(f)|^2 S_{x_n x_n}(f) + \sigma_{nk}^2}$$
(30)

*i*, k = 1, ..., n,  $i \neq k$ , where  $S_{X_l X_l}(f)$  is the spectrum of  $X_l$ , l = 1, ..., n. Similar to previous new causality definition, the causality defined in (30) is called by new spectral causality.

# Remark 3: i.

It is easy to see that  $0 \le N_{x_i \to x_k}$   $(f) \le 1$ .  $N_{x_i \to x_k}$   $(f) \equiv 0$  if and only if  $a_{ki}(f) \equiv 0$ , which means all coefficients  $a_{ki, 1}, \ldots, a_{ki, m}$  are zeros.  $N_{x_i \to x_k}$   $(f) \equiv 1$  if and only if  $\sigma_{\eta_k}^2 = 0$  and  $a_{kj}(f) \equiv 0, j = 1, \ldots, n, j \neq i$ , which means there is no noise term  $\eta_k$ and all coefficients  $a_{kj, 1}, \ldots, a_{kj, m}$  are zeros  $j = 1, \ldots, n, j \neq i$ , i.e., the *k*th equality in (28) can be written as

$$X_{k,t} = \sum_{j=1}^{m} a_{ki,j} X_{i,t-j}$$

from which one can see that  $X_k$  is completely driven by  $X_i$ 's past values.

ii. Once (16) is evaluated based on the *n* time series, from (30) the direct bidirectional causalities between any two channels can be obtained. Based on this definition, the indirect causality from  $X_i$  to  $X_k$  via  $X_l$  may be defined as

$$N_{\substack{X_i \longrightarrow X_k \text{ via } X_l}} (f) = N_{\substack{X_i \longrightarrow X_l}} (f) \times N_{\substack{X_l \longrightarrow X_k}} (f) .$$

**iii.** Given any route  $R: X_i \to X'_{l_1} \to X'_{l_2} \to \cdots, \to X'_{l_h} \to X_k$  where

 $\{X'_{l_1}, \ldots, X'_{l_k}\} \subseteq \{X_1, \ldots, X_n\} - \{X_i, X_k\}$ , the indirect causality from  $X_i$  to  $X_k$  via this route R may be defined as

$$N_{\substack{X_i \xrightarrow{\mathrm{ID}} X_k \quad \text{via route} \quad R}}(f) = N_{\substack{X_i \xrightarrow{\mathrm{D}} X'_{l_1}}}(f) \times \prod_{s=1}^{h-1} I_{\substack{X'_{l_s} \xrightarrow{\mathrm{D}} X'_{l_{s+1}}}}(f) \times N_{\substack{X'_{l_h} \xrightarrow{\mathrm{D}} X_k}}(f) \,.$$

Let  $S_{ik}$  be the set of all such routes, we may define the total causality from  $X_i$  to  $X_k$  is

$$N_{X_i \xrightarrow{\mathrm{T}} X_k} (f) = N_{X_i \xrightarrow{\mathrm{D}} X_k} (f) + \sum_{R \in S_{ik}} N_{X_i \xrightarrow{\mathrm{ID}} X_k} \quad \text{via route} \quad R (f) .$$
(31)

Let  $N_{X_i \to X_k}(f)$  be the causality value calculated based on estimated AR model of the pair  $(X_i, X_i)$ 

 $X_k$  in frequency domain. The exact relationship between  $N_{X_i \to X_k}(f)$  and  $\sum_{X_i \to X_k}^{N}(f)$  in (31) is unknown to us as for unknown to us so far.

In the literature, there are several other measures to define causality of neural connectivity in the frequency domain. In the following, we will introduce these measures and point out their shortcomings and/or limitations.

1) Spectral GC ([6], [8], [24], [25], [27]): Given the bivariate (2), the Granger casual influence from  $X_2$  to  $X_1$  is defined by

$$I_{X_2 \to X_1}(f) = -\log\left(1 - \frac{\left(\sigma_{\eta_2}^2 - \frac{\sigma_{\eta_1 \eta_2}^2}{\sigma_{\eta_1}^2}\right)|H_{12}(f)|^2}{S_{X_1 X_1}}\right) \in [0, +\infty)$$
(32)

where the transfer function is  $H(f) = A^{-1}(f)$  whose components are

$$H_{11}(f) = \frac{1}{\det(A)}a_{22}(f), \quad H_{12}(f) = -\frac{1}{\det(A)}a_{12}(f)$$

$$H_{21}(f) = -\frac{1}{\det(A)}\bar{a}_{21}(f), \quad H_{22}(f) = \frac{1}{\det(A)}\bar{a}_{11}(f)$$
(33)

$$A = \left[\bar{a}_{ij}\right]_{2 \times 2}, \bar{a}_{kk}(f) = 1 - \sum_{j=1}^{m} a_{kk,j} e^{-i2\pi f j}, k = 1, 2, \bar{a}_{hl}(f) = -\sum_{j=1}^{m} a_{hl,j} e^{-i2\pi f j}, h, l = 1, 2, h \neq l.$$

This definition has shortcomings and/or limitations as shown in the following remark.

#### Remark 4:

- i. The same problems exist as in (i) and (iii) of Remark 1.
- **ii.** For the two specific cases in (iii) of Property 1 and for any coefficients  $a_{11,j}$ ,  $a_{12,j}$ ,  $a_{21,j}, a_{22,j}$ , we can check  $I_{X_2} \rightarrow X_1$  (f)  $\equiv 0$  based on (32). However, one can easily

check  $N_{X_2 \xrightarrow{D} X_1}(f) \neq 0$  for (2) if  $a_{12}(f)X_2(f) \neq 0$ : that is, there is real causality. Thus spectral GC  $I_{X_2} \rightarrow X_1(f) = 0$  does not necessarily imply no real causality for the

given frequency *f*, but new spectral causality  $N_{x_2} \xrightarrow{D} x_1$  (*f*) =0 must imply no real causality (of course, no spectral GC). As such, new spectral causality definition reveals real causality more correctly than spectral GC.

**iii.** From in (17.22), (17.23), (32), and (33) above, we can derive

$$I_{x_{2} \to x_{1}}(f) = \frac{\Delta}{\sigma_{\eta_{1}}^{2} |\bar{a}_{22}(f)|^{2} - 2\sigma_{\eta_{1}\eta_{2}} \operatorname{Re}\left(\bar{a}_{12}(f)\bar{a}_{22}^{*}(f)\right) + \frac{\sigma_{\eta_{1}\eta_{2}}^{2}}{\sigma_{\eta_{1}}^{2}} |\bar{a}_{12}(f)|^{2} + \Delta}$$
(34)

where  $\Delta = \left(\sigma_{\eta_2}^2 - \sigma_{\eta_1\eta_2}^2/\sigma_{\eta_1}^2\right) |\bar{a}_{12}(f)|^2$ . Its detailed derivation is omitted here for space reason. One can see that  $I_{X_2 \to X_1}(f)$  has nothing to do with  $\bar{a}_{11}(f)$  and  $\bar{a}_{21}(f)$ , or, the real casuality from  $X_2$  to  $X_1$  in (2) has nothing to do with  $a_{11, j}$  and  $a_{21, j}$ .

This is not true [similar to the analysis in (ii) and (iii) of Remark 2]. Thus, in general, spectral GC in (32) does not disclose the real casual influence at all.

**iv.** GC was extended to conditional GC in frequency domain [6] and [8]. So, there exists the same problem as in (ii) above for conditional spectral GC.

2) PDC [14] and [28]: Let

$$a_{ij}(f) = \delta_{ij} - a_{ij}(f) \tag{35}$$

where  $a_{ij}(f)$  is as in (29), and  $\delta_{ij} = 1$  if i = j and 0 otherwise. Then in (16), PDC is defined to show frequency domain causality from  $X_i$  to  $X_i$  at frequency f as

$$\pi_{i \leftarrow j}(f) = \frac{\bar{a}_{ij}(f)}{\sqrt{\sum_{i=1}^{n} |\bar{a}_{ij}(f)|^{2}}}, \quad i, j = 1, \dots, n.$$
(36)

The PDC  $\pi_{i \leftarrow j}(f)$  represents the relative coupling strength of the interaction of a given source, signal  $X_j$ , with regard to signal  $X_i$ , as compared with all of  $X_j$ 's causing influences on other signals. Thus, PDC ranks the relative strength of causal interaction with respect to a given signal source and satisfies the following properties:

$$0 \le |\pi_{i \leftarrow j}(f)|^2 \le 1$$
 and  $\sum_{i=1}^n |\pi_{i \leftarrow j}(f)|^2 = 1, j = 1, ..., n.$ 

 $\pi_{i \leftarrow i}(f)$  represents how much of  $X_i$ 's own past contributes to the evolution on itself that is not explained by other signals (see [29]). Fig. 8 describes contributions of signal  $X_j$  to all signals  $X_1, \ldots, X_n$  and can help the reader to better understand the definition of PDC. Comparing Fig. 8 with Fig. 7, one can see that these two figures have different structures. It is notable that  $\pi_{i \leftarrow j}(f) = 0$  ( $i \neq j$ ) can be interpreted as absence of functional connectivity from signal  $X_j$  to signal  $X_i$  at frequency f. Hence, PDC can be used to multivariate time series to disclose whether or there exists casual influence from signal  $X_j$  to signal  $X_i$ . However, some researchers [30] already noted that PDC is hampered by a number of problems. In the following remark, we point out its shortcomings and/or limitations in a particular way.

#### Remark 5:

- Note that π<sub>i←i</sub>(f) represents how much of X<sub>i</sub>'s own past contributes to the evolution on itself (see [29]). Then, π<sub>i←i</sub>(f) = 0 means no X<sub>i</sub>'s own past contributes to the evolution on itself. However, π<sub>i←i</sub>(f) = 0 implies ā<sub>ii</sub>(f) = 0, that is, 1 a<sub>ii</sub>(f) = 0 or a<sub>ii</sub>(f) = 1(≠ 0), which means that there is X<sub>i</sub>'s own past contributes to the evolution on itself. A contradiction! On the other hand, π<sub>i←i</sub>(f) = 1 implies ā<sub>ki</sub>(f) = 0 (i.e., a<sub>ki</sub>(f) = 0), k = 1, 2, ..., n, k ≠ i, and ā<sub>ii</sub>(f) ≠ 0 (i.e., a<sub>ii</sub> ≠ 1). Given a frequency f, now we further assume X<sub>j</sub>(f) = X<sub>i</sub>(f) = 1 and a<sub>ij</sub>(f) = 1, a<sub>ii</sub>(f) = 0.01 for some j ≠ i. Then, a<sub>ij</sub>(f)X<sub>j</sub>(f) = 1 and a<sub>ii</sub>(f)X<sub>i</sub>(f) = 0.01. Thus, based on the *i*th equality of (28) we know that X<sub>i</sub>'s own past contributes to the evolution to X<sub>i</sub>'s evolution (i.e., a<sub>ii</sub>(f)X<sub>i</sub>(f) = 1) and can even be ignored. Thus, the number 1(= π<sub>i←i</sub>(f)) is not meaningful and PDC π<sub>i←i</sub>(f) is not reasonable.
- ii. High PDC  $\pi_{i \leftarrow j}(f)$ ,  $j \neq i$ , near 1, indicates strong connectivity between two neural structures (see [21]). This is not true in general. For example, assume  $\pi_{1 \leftarrow j}(f) = 1(j)$

 $\neq 1, 2$ ), which implies  $\bar{a}_{kj}(f) = 0, k = 2, ..., n$  and  $\bar{a}_{1j}(f) \neq 0$  (or  $a_{1j}(f) \neq 0$ ). Given a frequency *f*, now we further assume  $X_j(f) = X_2(f) = 1$  and  $a_{12}(f) = 1, a_{1j}(f) = 0.01$ . Then,  $a_{1j}(f)X_j(f) = 0.01$  and  $a_{12}(f)X_2(f) = 1$ . Thus, based on the first equality of (28) we know that  $X_j$ 's past contributes to  $X_1$ 's evolution (i.e.,  $a_{1j}(f)X_j(f) = 0.01$ ) is much smaller than  $X_2$ 's past contribution to  $X_1$ 's evolution (i.e.,  $a_{12}(f)X_2(f) = 1$ ) and can even be ignored. This demonstrates that there exists a very weak connectivity between  $X_j$  and  $X_1$ . However,  $\pi_{1 \leftarrow j}(f) = 1$  indicates strong connectivity between  $X_j$  and  $X_1$ . A contradiction!

- iii. Small PDC  $\pi_{i \leftarrow k}(f)$  does not means causal influence from  $X_k$  to  $X_i$  is small. For example, assume  $a_{ik}(f) = 0$ , i = 2, ..., n and  $\bar{a}_{1k}(f) = 0.1$ . Then, in terms of (36) one can see that  $\pi_{1\leftarrow k}(f) \approx 0.1$ , which is a small number. However, note the first equality of (28), if  $X_k(f)$  is a big number such that  $\bar{a}_{1k}(f)X_k(f)$  is much larger than any one of  $\bar{a}_{1j}(f)X_j(f)$ ,  $j \neq k$ . Then,  $X_k$  has major causal influence on  $X_1$  compared with other signals on  $X_1$ .
- iv.  $\pi_{i \leftarrow j}(f) > \pi_{i \leftarrow k}(f)$  cannot guarantee that causality from  $X_j$  to  $X_i$  is larger than that from  $X_k$  to  $X_i$  where  $j \neq i$ ,  $k \neq i$ . Actually (ii) and (iii) above support this statement.
- **v.** Consider (2) and further assume  $a_{21,j} = 0, j = 1, ..., m$ . One can clearly see that  $\pi_{1 \leftarrow 2}(f)$  has nothing to do with  $\bar{a}_{11}(f)$ , or, the real casual influence from  $X_2$  to  $X_1$  in (2) has nothing to do with  $a_{11,j}, j = 1, ..., m$ . This is not true [similar to the analysis in (ii) and (iii) of Remark 2].
- vi. The same problems as in (i) above ~(v) exist for a form of PDC called generalized PDC (GPDC) [31], [32].

3) RPC [15]: From (28) it follows that the transfer function  $H(f) = [H_{ij}(f)] = A^{-1}(f)$  where  $A = [\bar{a}_{ij}(f)]_{n \times n}$  and  $\bar{a}_{ij}(f)$  is as (35). When all noise terms are mutually uncorrelated, a simple RPC is defined as

$$R_{i \leftarrow j}(f) = \frac{|H_{ij}(f)|^2 \sigma_{\eta_j}^2}{S_{\chi,\chi}(f)}$$
(37)

where the power spectrum

$$S_{\chi_{i}\chi_{i}}(f) = \sum_{j=1}^{n} |H_{ij}(f)|^{2} \sigma_{\eta_{j}}^{2}, (i=1,\ldots,n).$$
(38)

Equation (38) indicates that the power spectrum of  $X_{i,t}$  at frequency *f* can be decomposed into *n* terms  $|H_{ij}(f)|^2 \sigma_{\eta_j}^2$ , (j = 1, ..., n), each of which can be interpreted as the power contribution of the *j*th innovation  $\eta_{j,t}$  transferring to  $X_{i,t}$  via the transfer function  $H_{ij}(f)$ . Thus,  $|H_{ij}(f)|^2 \sigma_{\eta_j}^2$  can be regarded as the power contribution of the innovation  $\eta_{j,t}$  on the power spectrum of  $X_{i,t}$ . RPC  $R_{i \leftarrow j}(f)$  defined in (37) can be regarded as a ratio of the power contribution of the innovation  $\eta_{j,t}$  on the power spectrum of  $X_{i,t}$  to the power spectrum  $S_{X_iX_i}(f)$ . Hence, RPC gives a quantitative measurement of the strength of every connection for each frequency component and always ranges from 0 to 1. The ratio is used to define  $X_j$ 's past contributes to  $X_i$ 's evolution. Fig. 9 describes contributions to signal  $X_i$ 's evolution from all signals  $X_k$ 's past values (k = 1, ..., n) and can help the reader to better understand the definition of RPC. Comparing Fig. 9 with Fig. 8, one can see that these two figures have different structures. Although RPC can be applied to multivariate time series, it has its shortcomings and/or limitations as pointed out in the following remark.

#### Remark 6:

- i. RPC  $R_{i \leftarrow i}(f)$  defined in (37) can only be regarded as a ratio of the power contribution of the innovation  $\eta_{i,t}$  on the power spectrum of  $X_{i,t}$  to the power spectrum  $S_{X_i}X_i(f)$ . In the literature, all researchers who use RPC to study neural connectivity view the ratio as  $X_i$ 's past contribution to  $X_i$ 's evolution. Unfortunately, the ratio cannot be used to define  $X_i$ 's past contribution to  $X_i$ 's evolution. It does not disclose real causal influence from  $X_i$  to  $X_i$  at all. For multivariate time series,  $R_{i \leftarrow i}(f) = 0$  does not mean no causal influence from  $X_i$  to  $X_i$ ,  $R_{i \leftarrow i}(f) = 1$  does not mean strong causality from  $X_i$  to  $X_i$ . For example, given a frequency f, let the transfer function  $H(f) = [H_{ij}(f)] = A^{-1}(f)$  satisfy  $H_{1i}(f) = 0$  and  $\bar{a}_{1i}(f) \neq 0$  (or  $a_{1i}(f) \neq 0$ 0),  $j \neq 1$ .  $H_{1i}(f) = 0$  indicates  $R_{1 \leftarrow i}(f) = 0$ . However, from the first equality of (28) and  $a_{1i}(f) \neq 0$ , one can see that there exists causality from  $X_i$  to  $X_1$ . Let the transfer function  $H(f) = [H_{ij}(f)] = A^{-1}(f)$  satisfy  $H_{1j}(f) \neq 0, H_{1k}(f) = 0, k = 1, ..., n, k \neq j$  and  $\bar{a}_{1i}(f) = 0$  (or  $a_{1i}(f) = 0$ ),  $j \neq 1$ . From  $H_{1i}(f) \neq 0$ ,  $H_{1k}(f) = 0$ ,  $k = 1, ..., n, k \neq j$ , it can be seen that  $R_{1 \leftarrow i}(f) = 1$ . However, from the first equality of (28) and  $a_{1i}(f) = 0$ , one can see that there exists no direct causality from  $X_i$  to  $X_1$  at all. Hence, RPC value  $R_{i \leftarrow i}(f)$  is not meaningful as far as causality from  $X_i$  to  $X_i$  is concerned.
- ii. In general, RPC  $R_{i \leftarrow j}(f)$  in (37) is unreasonable. The same analysis as (v) of Remark 5 leads to this statement.
- iii. When noise terms are mutually correlated, extended RPC (ERPC) was proposed in [15], and [33]. The same problems as above (i) and (ii) exist for ERPC.

4) *DTF or Normalized DTF* [16]: DTF is directly based on the transfer function H(f). It is defined as (37) where  $\sigma_{\eta_j}^2 = 1, j = 1, ..., n$ . So, the same problems as (i) and (ii) of Remark 6 exist for normalized DTF.

In conclusion, for four widely used Granger or Granger-like causlity measures (spectral GC, PDC, RPC, and DTF), we clearly point out their inherent shortcomings and/or limitations. One of reasons for causing those shortcomings and/or limitations is the use of the transfer function H(f) or its inverse matrix. In fact, Fig. 7 gives a rather intuitive description for the contributions to  $X_k(f)$ , which are summations of all causal influence terms  $a_{k1}(f)X_1(f), \ldots, a_{kn}(f)X_n(f)$  and the instantaneous causal influence noise term  $\eta_k(f)$  where  $a_{kk}(f)X_k(f)$  is the

causal influence from  $X_k$ 's past value.  $N_{x_k \xrightarrow{D} x_k}(f)$  defined in (30) describes how much causal influence of all influences on  $X_k(f)$  comes from  $X_i(f)$ . Thus, new spectral causality defined in (30) is mathematically rather reasonable and understandable. Any other causality measure not directly depending on all these causal influence terms and the instantaneous causal influence noise term may not truly reveal causal influence among different channels. Note that the new definition is totally different from all existing Granger or Granger-like causality measures which are directly based on the transfer function (or its inverse matrix) of the AR model. The difference mainly lies in two aspects: 1) the element  $H_{ii}(f)$  of the transfer function H(f) is totally different from  $a_{ij}(f)$  in (28) and as a result any causality measure based on H(f) may not reveal real causality relations among different channels, and 2) as pointed out in (iii) of Remark 4, (v) of Remark 5, and (ii) of Remark 6, Granger or Grangerlike causality measures use only partial information and some information is missing [e.g.,  $I_{X_2 \to X_1}(f)$  in (34) has nothing to do with  $\bar{a}_{11}(f)$  or  $-a_{11}(f)$ ] unlike new spectral causality defined as (30) in which all powers  $S_{X_i}X_i$  (*i* = 1, ..., *n*) (including all available information) are adopted. As such, spectral GC, PDC, RPC, DTF, and many other extended or variant forms like GPDC [31], extended RPC (ERPC) [33], normalized DTF [16], direct directed transfer function (dDTF) [34], SDTF [35], short-time direct directed transfer function

(SdDTF) [17], to name a few, suffer from the loss of some important information and inevitably cannot completely reveal true causality influence among channels.

## IV. Examples

In this section, we first compare our causality measures with the existing causality measures in the first four examples and in particular we show the shortcomings and/or limitations of the existing causality measures. In Examples 1–4, we always assume all noise terms are mutually independent and normal distribution with variance of 1 except for Example 4 which has a variance of 0.3. In the last example, we then conduct event-related causality analysis for a patient who suffered from seizure in left temporal lobe and was asked to recognize pictures viewed. In this example, we calculate new spectral causality, spectral GC, PDC, and RPC for two intracranial EEG channels where one channel is from left temporal lobe and the other channel is from right temporal lobe. The simulation results show that all measures clearly reveal causal information flow from right side to left side, but new spectral causality result reflects event-related activity very well and spectral GC, PDC, and RPC results are not interpretable and misleading.

*Example 1:* Comparison between spectral GC and new spectral causality. Consider the following model:

$$\begin{array}{l} X_{1,t} = a_{11,1} X_{1,t-1} - 0.8 X_{2,t-1} + \eta_{1,t} \\ X_{2,t} = 0.8 X_{2,t-1} + \eta_{2,t}. \end{array}$$

$$\tag{39}$$

We consider two cases:  $a_{11, 1} = 0.1$  and  $a_{11, 1} = 0.8$ . Obviously,  $X_2$  should have different causal influence on  $X_1$  in these two cases. Fig. 10(b) shows the new spectral causality results in these two cases from which one can see that  $X_2$  has totally different causal influence on  $X_1$  in these two cases. However, based on (34),  $X_2$  has the same GC on  $X_1$  in these two cases [see Fig. 10(a)] because (34) has nothing to do with the coefficient  $a_{11, 1}$ . Hence, we confirm that in general spectral GC may not reflect real causal influence between two neurons and may lead to wrong interpretation.

*Example 2:* Comparison between new spectral causality and PDC. Consider the following model with three time series:

$$\begin{cases} X_{1,t} = 0.1X_{1,t-1} - 0.2X_{2,t-1} - 0.2X_{3,t-1} + \eta_{1,t} \\ X_{2,t} = -0.1X_{1,t-1} + 0.8X_{2,t-1} - 0.2X_{3,t-1} + \eta_{2,t} \\ X_{3,t} = 1.5X_{1,t-1} - 0.2X_{2,t-1} + 0.8X_{3,t-1} + \eta_{3,t}. \end{cases}$$
(40)

For (40), it is easy to check that  $\pi_{1\leftarrow 2}(f) = \pi_{1\leftarrow 3}(f)$  for any frequency f > 0 based on PDC definition of (36). This is not true. The reason is that  $X_2(f) \neq X_3(f)$  for most frequency f > 0 and, as a result,  $\bar{a}_{12}(f)X_2(f) \neq \bar{a}_{13}(f)X_3(f)$  by noting  $\bar{a}_{12}(f) = \bar{a}_{13}(f)$  for any frequency f > 0. Thus, in the frequency domain,  $X_2$  and  $X_3$  should have different causal influence on  $X_1$ . The new spectral causality plotted in Fig. 11 shows that the causality from  $X_2$  to  $X_1$  is indeed totally different from that from  $X_3$  to  $X_1$  for most frequency f > 0. So, we confirm that in general PDC value may not reflect real causality between two neurons and may be misleading.

*Example 3:* Comparison between new spectral causality and RPC. First consider the following model with three time series:

$$X_{1,t}=0.5X_{1,t-1} - 0.2X_{1,t-2} + 0.5X_{2,t-1} + \eta_{1,t}$$

$$X_{2,t}=0.8X_{1,t-1} - 0.5X_{1,t-2} + 0.2X_{2,t-1} + 0.4X_{3,t-1} + \eta_{2,t}$$

$$X_{3,t}=0.6X_{1,t-1} - 0.5X_{3,t-1} + 0.5X_{3,t-2} + \eta_{3,t}.$$
(41)

From (41), one can get the transfer function  $H(f) = A^{-1}(f)$ ,  $H_{11}(f) = (1 - 0.2e^{-i2\pi f})(1 + 0.5e^{-i2\pi f} - 0.5e^{-i4\pi f})/\det(A)$ ,  $H_{12}(f) = 0.5e^{-i2\pi f} (1 + 0.5e^{-i2\pi f} - 0.5e^{-i4\pi f})/\det(A)$ ,  $H_{13}(f) = 0.5e^{-i2\pi f} \times 0.4e^{-i2\pi f}/\det(A)$ . We compute

$$R_{1\leftarrow 3}(f) = \frac{|H_{13}(f)|^2}{|H_{11}(f)|^2 + |H_{12}(f)|^2 + |H_{13}(f)|^2}.$$
(42)

The curve of RPC  $R_{1\leftarrow 3}(f)$  based on (42) is shown in Fig. 12 from which one can see that there always exists direct causal influence from  $X_3$  to  $X_1$  for f > 0. Especially, when f = 100Hz,  $R_{1\leftarrow 3}(100) = 1$ , which indicates that there is very strong direct causal influence from  $X_3$ to  $X_1$ . However, from the first equality of (41), one can see that there is no real direct causal influence from  $X_3$  to  $X_1$  at all.

We then consider the following model with three time series:

$$\begin{cases} X_{1,t}=0.2X_{1,t-1}-0.2X_{1,t-2}+0.8X_{2,t-1}-0.4X_{3,t-2}+\eta_{1,t} \\ X_{2,t}=0.3X_{1,t-1}-0.2X_{1,t-2}-0.6X_{2,t-1}+0.5X_{3,t-1}+0.3X_{3,t-2}+\eta_{2,t} \\ X_{3,t}=0.4X_{1,t-1}+0.3X_{2,t-1}-0.4X_{3,t-1}+0.3X_{3,t-2}+\eta_{3,t}. \end{cases}$$
(43)

From (43), one can get the transfer function  $H(f) = A^{-1}(f)$  with  $H_{13}(f) = 0$ ,  $\forall f > 0$ . As a result, RPC  $R_{1 \leftarrow 3}(f) \equiv 0$ ,  $\forall f > 0$ , which indicates no direct causal influence from  $X_3$  to  $X_1$ . However, from (43) one can see that  $X_3$  indeed has causal influence on  $X_1$ . Moreover, every two time series have bidirectional connectivities, which are shown in Fig. 13(a). Causality in frequency domain from  $X_3$  to  $X_1$  is plotted in Fig. 13(b), from which one can see that there always exists causal influence from  $X_3$  to  $X_1$  for a given frequency f > 0.

Hence, by above two models, we confirm that in general RPC value may not reflect real causal influence between two neurons and, as a result, may yield misleading results.

*Example 4:* Comparison among new spectral causality, conditional spectral GC, PDC, and RPC together. Consider the following model with three time series:

 $\begin{cases} X_{1,t} = 0.3X_{1,t-1} - 0.1X_{1,t-2} + 0.4X_{2,t-1} - 0.2X_{2,t-2} + 0.3X_{3,t-1} - 0.4X_{3,t-2} + \eta_{1,t} \\ X_{2,t} = 0.3X_{1,t-1} - 0.4X_{1,t-2} + 0.3X_{2,t-1} - 0.1X_{2,t-2} + 0.4X_{3,t-1} - 0.2X_{3,t-2} + \eta_{2,t} \\ X_{3,t} = 0.4X_{1,t-1} - 0.2X_{1,t-2} + 0.3X_{2,t-1} - 0.4X_{2,t-2} + 0.3X_{3,t-1} - 0.1X_{3,t-2} + \eta_{3,t} \end{cases}$ (44)

where the noise terms are normal distribution with variance of 0.3 and all noise terms are mutually independent. For each realization (200 realizations of 10 000 time points) of (44), we estimated AR model [as mentioned in (ii) of Property 1] and calculated power, new spectral causality, conditional spectral GC, PDC, and RPC values in frequency domain. Then average values across all realizations are reported in Figs. 14 and 15. Power spectra of  $X_1, X_2$ , and  $X_3$  are plotted in Fig. 14(a), from which one can see that  $X_1, X_2$ , and  $X_3$  have almost same power spectra across all frequencies and have an obvious peak at f = 29.5 Hz. New spectral causality, conditional spectral GC, PDC, and RPC are shown in Fig. 15. The first, third, and fourth columns in Fig. 15 shows direct new spectral causality, PDC, and RPC, respectively, from  $X_1$  to  $X_1$ , from  $X_2$  to  $X_1$ , and from  $X_3$  to  $X_1$ . It is notable that new

spectral causalities from  $X_1$  to  $X_1$ , from  $X_2$  to  $X_1$ , and from  $X_3$  to  $X_1$  are similar and have peaks at the same frequency of 29.5 Hz, which is consistent with the peak frequency of power spectra in Fig. 14(a). So, these new spectral causality results are rather interpretable and reasonable by noting the almost same power spectra in Fig. 14(a) for  $X_1$ ,  $X_2$ , and  $X_3$ . On the contrary, conditional GC in the second cloumn of Fig. 15, PDC, and RPC (from  $X_2$  to  $X_1$ , and from  $X_3$  to  $X_1$ ) have peaks at different frequencies which are all different from 29.5 Hz. These results are not interpretable by noting the same peak frequency (29.5 Hz) of power spectra in Fig. 14(a). More specifically, PDC and RPC (from  $X_1$  to  $X_1$ ) achieve minimum at peak frequencies of PDC and RPC (from  $X_2$  to  $X_1$  or from  $X_3$  to  $X_1$ ). Obviously, these results are incorrect and misleading. N(f) and  $N_T(f)$  are presented in Fig. 14(b), where  $N(f) = N_{X_3 \to X_2} (f) \times N_{X_2 \to X_1} (f)$  based on (44) and  $N_T(f) = N_{X_3 \to X_1}(f)$  based on the estimated AR model of the pair ( $X_1, X_3$ ). One can see that  $N_T(f)$  (i.e., the total causality from

estimated AR model of the pair  $(X_1, X_3)$ . One can see that  $N_T(f)$  (i.e., the total causality from  $X_3$  to  $X_1$ ) is very close to N(f) (i.e., summation of causalities along all routes from  $X_3$  to  $X_1$ ) before 40 Hz. But after 40 Hz,  $N(f) > N_T(f)$ . For a general model, the exact relationship between N(f) and  $N_T(f)$  is unknown.

Hence, by this example, we confirm that in general spectral GC, PDC, and RPC may not reflect real causality.

*Example 5:* In this example, we conduct ERP analysis for one seizure patient who suffered from seizure in left temporal lobe and was asked to recognize pictures viewed. There are two sessions for testing. During the first session, stimuli was presented and evaluated for their emotional impact (valence, arousal) and autonomic effects. Stimuli were chosen that are known to activate the amygdala from functional imaging studies. A second session was a recall task in which the subject was asked to recognize pictures viewed in session 1. The subject was comfortably seated in front of a computer monitor projecting and imaging from the International Affective Picture System (IAPS) every 22 s according to the above schema. Forty images were selected that span the range of emotional valence and arousal according to previously published standards. The image was held on the screen for 6 s, and then the subject was asked to rate the image on an emotional valence (0 = not emotionally intense to3 = extremely emotionally intense). Reaction time to the rating was measured. After rating, the screen went blank for 15 s. Twenty-four hours later, a second session was held in which pictures were presented in random order. All 40 of the previously viewed pictures as well as another 80 pictures from the IAPS with similar overall valence and arousal ratings were presented. Each image was presented for 3 s and then the patient was asked if it had been previously seen or not and to what degree of certainty this can be stated (e.g., not seen before very certain to not seen before very unsure). Reaction time to the response was measured. A blank screen followed the response for 2 s. We recorded intracranial EEG and behavioral data (response times and choices) from 16 electrodes consisting of right and left temporal depth electrodes (RTD and LTD, the locations of these electrodes can be seen in [36, Fig. 2]) composed of eight platinum/iridium alloy contacts spaced at 10 mm intervals on an XLTek EEG 128 system which digitizes each channel at 625 Hz with a 0.01-100 Hz analog band-pass digital filter. All channels (16) were referred to the scalp suture electrode. Individual stimulus response trials were visually inspected and those with artifacts were excluded from subsequent analysis. After visual inspection, the remaining analyzed data involves 7500 sample points and 78 epochs.

As in many researchers have done, we use the average referenced iEEG. ERP images in Fig. 16(a) clearly show cortical activity changes after stimulus onset in most channels. To study task-related causality relationship between different channels, we use the moving window technique where the window size is 150 samples (240 ms) and overlap is 75 samples (120 ms). After a complete analysis for the MVAR model order in each window by using the

Akaike information criterion [37]–[39] we found the chosen order of 8 fits well and thus a common model order of 8 was applied for all windows in our data set.

We took R5 and L4 as an example and calculated their causality relationship based on new spectral causality, spectral GC, PDC, and RPC. The power spectra for R5 and L4 averaged over all trials are shown in Fig. 16(b), from which one clearly sees that delayed lower frequency band (<8 Hz) activities are enhanced after stimulus onset (about 250 ms time delay). This result is consistent with previous findings that theta (2–10 Hz) oscillations have been observed to be prominent during a variety of cognitive processes in both animal and human studies [40]–[44] and may play a fundamental role in memory encoding, consolidation, and maintenance [45]-[47]. Time-frequency causality [or event-related causality (see, [17])] relationship between R5 and L4 based on new spectral causality, spectral GC, PDC, and RPC are shown in Fig. 16(c)-(f) respectively, from which one can find that: 1) the causal influence from R5 to L4 is significantly enhanced after stimulus onset (about 250 ms time delay) for all four measures (we use the statistical testing framework in [17] to test significance level for each measure). But only new spectral causality discloses the enhanced frequency band (<8 Hz), which is consistent with the delayed enhanced lower frequency band (<8 Hz) activities of R5 and L4 as shown in Fig. 16(b) and thus the result should be real. The enhanced frequency bands revealed by the other measures (spectral GC, PDC, RPC) are always less than 2 Hz and the enhanced lower frequency band (2-8 Hz) activities shown in Fig. 16(b) cannot be reflected and thus these results lead to misinterpretation, and 2) the causal influence from L4 to R5 is much smaller than that from R5 to L4 for each measure. These results indicate that interaction between the pair of R5 and L4 is not symmetric and R5 has a strong directional interaction on L4. A possible reason for this phenomenon is that the patient had left temporal lobe epilepsy and therefore some of brain functions were lost, which kept information flow in left temporal lobe from normally transmitting to right temporal lobe.

Hence, by this real neurophysiological data analysis, we further verify that new spectral causality may truly reveal causal interaction between two areas and the other measures like spectral GC, PDC, and RPC cannot do and thus may lead to wrong interpretation results.

# V. Conclusion

In human cognitive neuroscience, researchers are now not limited to only the study of the putative functions of particular brain regions, but are moving toward how different brain regions (such as visual cortex, parietal or frontal regions, amygdala, or hippocampus) may causally influence on each other. These causal influences with different strengths and directionalities may reflect the changing functional demands on the network to support cognitive and perceptual tasks. Direct evidence to show the existence of causality among brain regions can be achieved from the activity changes of brain regions by using brain stimulation approach. Brain stimulation affects not only the targeted local region but also the activity in remote interconnected regions. These remote effects depend on cognitive factors (e.g., task-condition) and reveal dynamic changes in interplay between brain areas. GC, one of the most popular causality measures, was initially widely used in economics and has recently received growing attention in neuroscience to reveal causal interactions for neurophysiological data. Especially in frequency domain, several variant forms of GC have been developed to study causal influences for neurophysiological data in different frequency decompositions during cognitive and perceptual tasks.

In this paper, on one hand, in time domain we defined a new causality from any time series Y to any time series X in the linear regression model of multivariate time series, which describes the proportion that Y occupies among all contributions to X (where each

contribution must be considered when defining any good causality tool, otherwise the definition inevitably cannot reveal well the real strength of causality between two time series). In particular, we used one simple example to clearly show that both of new causality and GC adopt the concept of proportion, but they are defined on two different equations where one equation (for GC) is only part of the other equation (for new causality). Therefore, new causality is a natural extension of GC and has a sound conceptual/theoretical basis, and GC is not the desired causal influence at all. As such, traditional GC has many pitfalls, e.g., a larger GC value does not necessarily mean higher real causality, or vice versa; even when GC value is zero, there still exists real causality which can be revealed by new causality. Therefore, the popular traditional GC cannot reveal the real strength of causality at all, and researchers must apply caution in drawing any conclusion based on GC value. On the other hand, in frequency domain we pointed out that any causality definition based on the transfer function matrix (or its inverse matrix) of the linear regression model in general may not be able to reveal the real strength of causality between two time series. Since almost all existing spectral causality definitions are based on the transfer function matrix (or its inverse matrix) of the linear regression model, we took the widely used spectral GC, PDC, and RPC as examples and pointed out their inherent shortcomings and/or limitations. To overcome these difficulties, we defined a new spectral causality which describes the proportion that one variable occupies among all contributions to another variable in the multivariate linear regression model (frequency domain). By several simulated examples, we clearly showed that our new definitions (in time and frequency domains) are advantageous over existing definitions. Moreover, for a real ERP EEG data from a patient with epilepsy undergoing monitoring with intracranial electrodes, the application of new spectral causality yielded promising and reasonable results. But the applications of spectral GC, PDC, and RPC all generated misleading results. Therefore, our new causality definitions appear to shed new light on causality interaction analysis and may have wide applications in economics and neuroscience. Apparently, before our methods can be widely used in economics and neuroscience, application of our methods to more time series data should be further investigated: 1) to evaluate our methods' usefulness and advantages over other existing popular methods; 2) to do statistical significance level testing; and 3) to study bias issue in time domain [48] and frequency domain, i.e., whether the resulting causality is biased by using appropriate surrogate data.

# Acknowledgments

This work was supported in part by the National Natural Science Foundation of China under Grant 61070127, and the International Cooperation Project of Zhejiang Province, China, under Grant 2009C14013, Grant NIH R01 MH072034, Grant NIH R01 NS054314, and Grant NIH R01 NS063039.

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### References

- 1. Seth A. Granger causality. Scholarpedia. 2007; 2(7):1667.
- Sun R. A neural network model of causality. IEEE Trans. Neural Netw. Jul.; 1994 5(4):604–611. [PubMed: 18267833]

- Zou C, Denby KJ, Feng J. Granger causality versus dynamic Bayesian network inference: A comparative study. BMC Bioinf. Apr..2009 10(1):401.
- 4. Wiener, N. The theory of prediction. In: Beckenbach, EF., editor. Modern Mathematics for Engineers. McGraw-Hill; New York: 1956. ch. 8
- 5. Granger CWJ. Investigating causal relations by econometric models and cross-spectral methods. Econometrica. Jul.; 1969 37(3):424–438.
- Ding, M.; Chen, Y.; Bressler, SL. Granger causality: Basic theory and applications to neuroscience. In: Schelter, B.; Winterhalder, M.; Timmer, J., editors. Handbook of Time Series Analysis. Wiley-VCH; Weinheim, Germany: 2006. p. 437-460.
- Freiwald WA, Valdes P, Bosch J, Biscay R, Jimenez JC, Rodriguez LM, Rodriguez V, Kreiter AK, Singer W. Testing non-linearity and directedness of interactions between neural groups in the macaque inferotemporal cortex. J. Neurosci. Methods. Dec.; 1999 94(1):105–119. [PubMed: 10638819]
- Geweke J. Measurement of linear dependence and feedback between multiple time series. J. Amer. Stat. Assoc. Jun.; 1982 77(378):304–313.
- Hesse W, Möller E, Arnold M, Schack B. The use of time-variant EEG Granger causality for inspecting directed interdependencies of neural assemblies. J. Neurosci. Methods. Mar.; 2003 124(1):27–44. [PubMed: 12648763]
- Oya H, Poon PWF, Brugge JF, Reale RA, Kawasaki H, Volkov IO. Functional connections between auditory cortical fields in humans revealed by Granger causality analysis of intra-cranial evoked potentials to sounds: Comparison of two methods. Biosystems. May–Jun.; 2007 89(1–3): 198–207. [PubMed: 17184906]
- 11. Roebroeck A, Formisano E, Goebel R. Mapping directed influence over the brain using Granger causality and fMRI. Neuroimage. Mar.; 2005 25(1):230–242. [PubMed: 15734358]
- Gow DW, Segawa JA, Alfhors S, Lin FH. Lexical influences on speech perception: A Granger causality analysis of MEG and EEG source estimates. Neuroimage. Nov.; 2008 43(3):614–623. [PubMed: 18703146]
- Gow DW, Keller CJ, Eskandar E, Meng N, Cash SS. Parallel versus serial processing dependencies in the perisylvian speech network: A Granger analysis of intracranial EEG data. Brain Lang. Jul.; 2009 110(1):43–48. [PubMed: 19356793]
- 14. Baccal LA, Sameshima K. Partial directed coherence: A new concept in neural structure determination. Biol. Cybern. Jun.; 2001 84(6):463–474. [PubMed: 11417058]
- Yamashita O, Sadato N, Okada T, Ozaki T. Evaluating frequency-wise directed connectivity of BOLD signals applying relative power contribution with the linear multivariate time-series models. Neuroimage. Apr.; 2005 25(2):478–490. [PubMed: 15784427]
- Kaminski M, Ding M, Truccolo-Filho W, Bressler SL. Evaluating causal relations in neural systems: Granger causality, directed transfer function and statistical assessment of significance. Biol. Cybern. Aug.; 2001 85(2):145–157. [PubMed: 11508777]
- 17. Korzeniewska A, Crainiceanu CM, Kus R, Franaszczuk PJ, Cronel NE. Dynamics of event-related causality in brain electrical activity. Human Brain Mapp. Oct.; 2008 29(10):1170–1192.
- Bernasconi C, Konig P. On the directionality of cortical interactions studied by structural analysis of electrophysiological recordings. Biol. Cybern. Sep.; 1999 81(3):199–210. [PubMed: 10473845]
- Liang H, Ding M, Nakamura R, Bressler SL. Causal influences in primate cerebral cortex during visual pattern discrimination. Neuroreport. Sep.; 2000 11(13):2875–2880. [PubMed: 11006957]
- Brovelli A, Ding M, Ledberg A, Chen Y, Nakamura R, Bressler SL. Beta oscillations in a largescale sensorimotor cortical network: Directional influences revealed by Granger causality. Proc. Nat. Acad. Sci. United States Amer. Jun.; 2004 101(26):9849–9854.
- Sato JR, Takahashi DY, Arcuri SM, Sameshima K, Morettin PA, Baccal LA. Frequency domain connectivity identification: An application of partial directed coherence in fMRI. Human Brain Mapp. Feb.; 2009 30(2):452–461.
- Kaminski M, Liang H. Causal influence: Advances in neurosignal analysis. Crit. Rev. Biomed. Eng. 2005; 33(4):347–430. [PubMed: 15982186]
- Guo S, Wu J, Ding M, Feng J. Uncovering interactions in the frequency domain. PLoS Comput. Biol. 2008; 4(5):e1000087–1–e1000087-5. [PubMed: 18516243]

- Geweke JF. Measures of conditional linear dependence and feedback between time series. J. Amer. Stat. Assoc. Dec.; 1984 79(388):907–915.
- Blinowska KJ, Kus R, Kaminski M. Granger causality and information flow in multivariate processes. Phys. Rev. E. Nov.; 2004 70(5):050902(R)-1–050902(R)-4.
- 26. Kus R, Kaminski M, Blinowska KJ. Determination of EEG activity propagation: Pair-wise versus multichannel estimate. IEEE Trans. Biomed. Eng. Sep.; 2004 51(9):1501–1510. [PubMed: 15376498]
- 27. Cui J, Xu L, Bressler SL, Ding M, Liang H. BSMART: A MATLAB/C measurebox for analysis of multichannel neural time series. Neural Netw., Spec. Issue Neuroinf. Oct.; 2008 21(8):1094–1104.
- Schelter B, Winterhalder M, Eichler M, Peifer M, Hellwig B, Guschlbauer B, Lucking CH, Dahlhaus R, Timmer J. Testing for directed influences among neural signals using partial directed coherence. J. Neurosci. Methods. Apr..2005 152:210–219. [PubMed: 16269188]
- 29. Allefeld, C.; Graben, PB.; Kurths, J. Advanced Methods of Electrophysiological Signal Analysis and Symbol Grounding. Nova; Commack, NY: Feb. 2008 p. 276-296.
- Schelter B, Timmer J, Eichler M. Assessing the strength of directed influences among neural signals using renormalized partial directed coherence. J. Neurosci. Methods. Apr.; 2009 179(1): 121–130. [PubMed: 19428518]
- Baccal, LA.; de Medicina, F. Proc. 15th Int. Conf. Digital Signal Process. Cardiff, U.K.: Jul.. 2007 Generalized partial directed coherence; p. 163-166.
- Baccal, LA.; Takahashi, YD.; Sameshima, K. Handbook of Time Series Analysis. Wiley-VCH; Berlin, Germany: 2006. Computer intensive testing for the influence between time series; p. 365-388.
- 33. Tanokura Y, Kitagawa G. Power contribution analysis for multivariate time series with correlated noise sources. Adv. Appl. Stat. 2004; 4(1):65–95.
- 34. Korzeniewska A, Mańczak M, Kamiński M, Blinowska KJ, Kasicki S. Determination of information flow direction among brain structures by a modified directed transfer function (dDTF) method. J. Neurosci. Methods. May; 2003 125(1–2):195–207. [PubMed: 12763246]
- Ginter JJ, Blinowska KJ, Kaminski M, Durka PJ, Pfurtscheller G, Neuper C. Propagation of EEG activity in beta and gamma band during movement imagery in human. Methods Inf. Med. 2005; 44(1):106–113. [PubMed: 15778801]
- 36. Hu S, Stead M, Dai Q, Worrell G. On the recording reference contribution to EEG correlation, phase synchorony, and coherence. IEEE Trans. Syst., Man, Cybern., Part B: Cybern. Oct.; 2010 40(5):1294–1304.
- 37. Akaike H. A new look at the statistical model identification. IEEE Trans. Autom. Control. Dec.; 1974 19(6):716–723.
- Seghouane A-K, Amari S-I. The AIC criterion and symmetrizing the Kullback–Leibler divergence. IEEE Trans. Neural Netw. Jan.; 2007 18(1):97–106. [PubMed: 17278464]
- Seghouane A-K. Model selection criteria for image restoration. IEEE Trans. Neural Netw. Aug.; 2009 20(8):1357–1363. [PubMed: 19596633]
- Anderson KL, Rajagovindan R, Ghacibeh GA, Meador KJ, Ding M. Theta oscillations mediate interaction between prefrontal cortex and medial temporal lobe in human memory. Cereb. Cortex. Jul.; 2010 20(7):1604–1612. [PubMed: 19861635]
- 41. Hwanga DY, Golby AJ. The brain basis for episodic memory: Insights from functional MRI, intracranial EEG, and patients with epilepsy. Epil. Behav. Feb.; 2006 8(1):115–126.
- Kahana MJ, Seelig D, Madsen JR. Theta returns. Curr. Opin. Neurobiol. Dec.; 2001 11(6):739– 744. [PubMed: 11741027]
- 43. Kirk IJ, Mackay JC. The role of theta-range oscillations in synchronising and integrating activity in distributed mnemonic networks. Cortex. Mar.; 2003 39(4):993–1008. [PubMed: 14584563]
- 44. Liu D, Pang Z, Lloyd SR. A neural network method for detection of obstructive sleep apnea and narcolepsy based on pupil size and EEG. IEEE Trans. Neural Netw. Feb.; 2008 19(2):308–318. [PubMed: 18269961]
- 45. Buzsaki G. Theta rhythm of navigation: Link between path integration and landmark navigation, episodic and semantic memory. Hippocampus. 2005; 15(7):827–840. [PubMed: 16149082]

- Raghavachari S, Lisman J, Tully M, Madsen J, Bromfield E, Kahana M. Theta oscillations in human cortex during a working-memory task: Evidence for local generators. J. Neurophysiol. Mar.; 2006 95(3):1630–1638. [PubMed: 16207788]
- 47. Siapas AG, Wilson MA. Coordinated interactions between hippocampal ripples and cortical spindles during slow-wave sleep. Neuron. Nov.; 1998 21(5):1123–1128. [PubMed: 9856467]
- 48. Palus M, Vejmelka M. Directionality of coupling from bivariate time series: How to avoid false causalities and missed connections. Phys. Rev. E. May; 2007 75(5):056211–1–056211-14.



# Fig. 1.

(a) GC values from  $X_2$  to  $X_1$  in (8) as the variance  $\sigma_{\eta_1}^2$  changes from 0.01 to 2 where  $a_{12, 1} = -0.8$ . (b) GC values from  $X_2$  to  $X_1$  in (8) as  $a_{12, 1}$  changes from -0.1 to -0.95 where  $\sigma_{\eta_1}^2 = 1$ . From (a) one can see that GC value from  $X_2$  to  $X_1$  decreases as the variance  $\sigma_{\eta_1}^2$  increases. From (b) one can see that GC value from  $X_2$  to  $X_1$  increases as the amplitude  $|a_{12, 1}|$ 

increases.



#### Fig. 2.

(a) GC from  $X_2$  to  $X_1$  as a function of the order of the estimated models for (9) when  $a_{11, 1} = 0.2$  and  $a_{21, 1}$  changes from 0.1 to 0.9. (b) GC from  $X_2$  to  $X_1$  as a function of the order of the estimated models for (9) when  $a_{21, 1} = 0.2$  and  $a_{11, 1}$  changes from 0.1 to 0.9. From (a) and (b), one can see that: 1) GC from  $X_2$  to  $X_1$  keeps steady and converges to 0.67 when the order p > 8, and 2) GC from  $X_2$  to  $X_1$  has nothing to do with parameters  $a_{11, 1}$  and  $a_{21, 1}$ .



**Fig. 3.** Connectivities among three time series.







# Fig. 5.

Plot of trajectories for  $-0.99X_{2,t}$ ,  $-0.99\overline{X}_{2,t}$ , and  $\eta_{1,t}$  for one realization of (24) and (25) where  $X_{i,0} = \overline{X}_{i,0}$  and  $\eta_{i,t} = \overline{\eta}_{i,t}$ , i = 1, 2: (a)  $-0.99 X_{2,t}$  's trajectory for (24). (b)  $-0.99\overline{X}_{2,t}$  's trajectory for (25)(c)  $\eta_{1,t}$  's or  $\overline{\eta}_{1,t}$ 's trajectory.







**Fig. 7.** Contributions to  $X_k(f)$ .



**Fig. 8.**  $X_j$ 's contributions to all signals  $X_i$ , i = 1, 2, ..., n.









(a) Spectral GC results:  $I_{X_2 \to X_1}(f)$  based on (34) for (39) of two time series in two cases:  $a_{11, 1} = 0.1$  and  $a_{11, 1} = 0.8$ . (b) New spectral causality results:  $N_{X_2 \to X_1}(f)$  for (39).



Fig. 11. New spectral causality results:  $N_{x_2 \xrightarrow{D} x_1}(f)$  and  $N_{x_3 \xrightarrow{D} x_1}(f)$  for (40).



**Fig. 12.** Curve of RPC  $R_{1 \leftarrow 3}(f)$  calculated based on (42).



# Fig. 13.

(a) Results of new causality based on (20) for (43) of three time series in time domain. Selfcontributions are neglected. The resulting strength of the connections is schematically represented by the thickness of arrows. (b) New spectral causality from  $X_3$  to  $X_1$  is shown for (43) in frequency domain.



#### Fig. 14.

(a) Power spectra of  $X_1$ ,  $X_2$ ,  $X_3$ . It can be seen that  $X_1$ ,  $X_2$ ,  $X_3$  have almost same powers across all frequencies and have an obvious peak at f = 29.5 Hz. (b)

 $N(f) = N_{X_3 \to X_2} (f) \times N_{X_2 \to X_1} (f)$  based on (44) and  $N_T(f) = N_{X_3 \to X_1} (f)$  based on the estimated AR model of the pair ( $X_1, X_3$ ). One can see that  $N_T(f)$  (i.e., the total causality from  $X_3$  to  $X_1$ ) is very close to N(f) (i.e., summation of causalities along all routes from  $X_3$  to  $X_1$ ) before 40 Hz. But after 40 Hz,  $N(f) > N_T(f)$ . For a general model, the exact relationship between N(f) and  $N_T(f)$  is not known.



#### Fig. 15.

Comparison among new spectral causality, conditional spectral GC, PDC, and RPC together. The first, third, and fourth columns show direct new spectral causality, PDC, and RPC, respectively, from  $X_1$  to  $X_1$ , from  $X_2$  to  $X_1$ , and from  $X_3$  to  $X_1$ . The second column shows conditional GC. It is notable that: 1) new spectral causality from  $X_1$  to  $X_1$ , from  $X_2$  to  $X_1$ , and from  $X_3$  to  $X_1$  to  $X_1$  are similar and have peaks at the same frequence of 29.5 Hz, which is consistent with the peak frequency of power spectra [see Fig. 14(a)], and 2) conditional GC, PDC, and RPC (from  $X_2$  to  $X_1$ , and from  $X_3$  to  $X_1$ ) have peaks at different frequencies which are all different from 29.5 Hz.



#### Fig. 16.

(a) ERPs for eight left Macrowire channels (LMacro1–LMacro8) and eight right Macrowire channels (RMacro1–RMacro8) where average reference is applied. (b) Power spectra for LMacro4 (or L4) and RMacro5 (or R5). (c) New spectral causality results between L4 and R5. (d) GC results between L4 and R5. (e) PDC results between L4 and R5. (f) RPC results between L4 and R5.