Brief Review of Models of Ectopic Bone Formation

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Ectopic bone formation is a unique biologic entity—distinct from other areas of skeletal biology. Animal research models of ectopic bone formation most often employ rodent models and have unique advantages over orthotopic (bone) environments, including a relative lack of bone cytokine stimulation and cell-to-cell interaction with endogenous (host) bone-forming cells. This allows for relatively controlled in vivo experimental bone formation. A wide variety of ectopic locations have been used for experimentation, including subcutaneous, intramuscular, and kidney capsule transplantation. The method, benefits and detractions of each method are summarized in the following review. Briefly, subcutaneous implantation is the simplest method. However, the most pertinent concern is the relative paucity of bone formation in comparison to other models. Intramuscular implantation is also widely used and relatively simple, however intramuscular implants are exposed to skeletal muscle satellite progenitor cells. Thus, distinguishing host from donor osteogenesis becomes challenging without cell-tracking studies. The kidney capsule (perirenal or renal capsule) method is less widely used and more technically challenging. It allows for supraphysiologic blood and nutrient resource, promoting robust bone growth. In summary, ectopic bone models are extremely useful in the evaluation of bone-forming stem cells, new osteoinductive biomaterials, and growth factors; an appropriate choice of model, however, will greatly increase experimental success.

What Is Ectopic Bone Formation?

Eсторіс воле, from the Greek word *ektopos* or "away from a place," refers to the ossification of tissues outside their usual origins. Ectopic bone formation is most often experimentally induced, but does also have clinical relevance. For example, ectopic bone has long been described as a congenital or inherited malformation [1–4], or a complication of various conditions such as paraplegia [5,6], posthip arthroplasty [7,8], postburn, or traumatic injury [9–11]. Such pathologic formation of endochondral bone in soft tissues such as muscle, subcutaneous tissue, and fibrous tissue adjacent to joints is called heterotopic ossification (HO). Up to 10% of patients who have invasive surgery will develop this debilitating complication, which is thought to be caused by local inflammation followed by recruitment of skeletal progenitor cells [12,13]. Though less frequently observed, hereditary forms of ectopic bone formation also exist. One such disease entity is called fibrodysplasia ossificans progressiva resulting from a mutation in the ACVR1 gene that causes upregulation of BMP1 [14]. Experimental induction of bone tissue has been long-standing, first in muscle pouch and subcutaneous models [15,16], and more recently in the kidney capsule model. Each of these experimental entities offers distinct advantages and drawbacks that will be discussed below.

Ectopic Versus Orthotopic Bone Formation

The distinction between ectopic and orthotopic bone formation is an important one. Orthotopic bone formation is derived from the greek word *orthos* meaning "straight, right" and refers to studies in which bone is formed in its correct anatomical location. Such studies can either be nonsurgical (eg, the injection of materials into the long bone periosteum) or surgical (eg, a calvarial defect in which material is grafted in the defect site). In these instances, the distinct biochemical and mechanical environment of an orthotopic bone model should not be overlooked. Bone injury has long been understood to elicit a cascade of signaling pathway activation, including fibroblast growth factor [17], transforming growth factor-beta (TGF- β) [18], Hedgehog [19], and Wingless Protein (Wnt) signaling [20] among others. This upregulation of

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		TABLE 1.	RECENT STUDIES USING SUBCUTANEOU	S IMPLAI	NTATION		
Artic No.	le PMID Year Author	Cell type	Scaffold	Protein	Duration	Result	Host animal
1.	21702756 2011 Park ⁵²		bMBCP	BMP2	8 Weeks	Bone formation only observed with the combination of bMBCP	Rat
5	21118417 2011 Song ⁵³	hPDLSCs	Collagen	BMP2	5 Days	scaffold and BMP2 BMP2 promoted hPDLSCs to form mineralized cementum and downregulated organized	Mice
Э.	21710441 2011 Janicki ⁵⁴	Human BMSCs	B-TCP and fibrin glue		8 Weeks	PDL tissue Variable ectopic bone formation	Mice
4.	21303418 2011 Ma ²⁶	Predifferentiated cell sheets	s B-TCP cylinder	ı	8 Weeks	observed perween numan donors Highly mineralized bone tissue	Rabbit
ы.	20666615 2010 Kempen ⁵⁶		PLGA/poly(propylene fumarate)/ gelatin composites	BMP2	8 Weeks	Bone only seen in BMP2-loaded composites. Additional treatment with PTH enhanced bone formation	Rat
6.	20925348 2010 Seyedjafari ⁵⁷	Human cord blood derived MSCs	PLLA and HA-coated PLLA	I	10 Weeks	in BMP2 groups Higher ossification and formation of trabeculi observed in HA-coated	Mice
7.	20638718 2010 Wu ⁵⁸	l	Titanium coated discs (collagen,	BMP2	5 Weeks	Collagen and Ethisorb coating	Rat
×.	20149447 2010 Lee ⁵⁹	I	EULSOLD, FLOA OF FOLYACUVE) aCS	BMP2	8 Weeks	BMP2 increased bone formation and rate of bone growth across all	Rat
9.	19866334 2010 Eguchi ⁶⁰	Mouse osteoblasts/	Polymer discs	BMP2,	3 Weeks	ETN enhanced the bone-inducing	Mouse
10.	19918912 2010 Bahar ⁶¹	osteoclasts BMSCs	Demineralized (DBM), deproteinized (HABM) or nontreated (MBM) cortical bone cylinders		10 Weeks	capacity of DML2 Demineralized or nontreated cortical bone cylinders showed progressive mineralization, while deproteinized	Rat
11.	20636333 2010 Boos ⁶²	Sheep BMSCs	B-tricalcium phosphate/ hydroxyapatite granules	BMP2	12 Weeks	Ectopic bone could be generated using MSCs with β-TCP/HA granules	Sheep
12.	19580831 2010 Zhao ³⁵	I	DBM with or without BMP2 cross-linking	BMP2	4 Weeks	atome. Diver 2 increased point romation The addition of BMP2 cross-linking to DBM resulted in significant	Rat
13.	21478102 2010 Götz ⁶⁴	l	Nano-crystalline hydroylapatite		8 Months	bone tornauon As early as 5 weeks, new bone formation was observed	Mini pig
14.	20497064 2010 Cui ⁶⁵	D1 mouse osteoprogenitor cell line overexpressing	PLGA	Ι	3 Weeks	Forced overexpression of VEGF+BMP6 combination led to greatest bone	Mouse
15.	20438297 2010 Byeon ⁶⁶	V EGF OF BMP'6 cUCB MSCs	B-TCP		84 Days	tormation cUCB MSCs form significant osteoid matrix with ALP positive precursor	Dog

(Table continued \rightarrow)

			TABLE 1. (CONTINUED)				
Articl No.	e PMID Year Author	Cell type	Scaffold	Protein	Duration	Result	Host animal
16.	19540582 2009 Zhang ⁶⁷	C2C12 cells	Nanoparticulates of BSA/ polvethvlenimine for BMP2 release	BMP2	3 Weeks	cells Nanoparticulate coating was not effective due to cytoxicity. BMP2	Rat
17.	19828890 2009 Yang ⁶⁸	DPSCs transfected with	Ceramic		12 Weeks	alone induced robust ectopic bone Only BMP2 transfected cells showed	Mouse
18.	19842114 2009 Ben-David ⁶⁹	BMP2 Human BMSCs	Gelatin-based hydrogel and ceramic (CaC03/B-TCP)		8 Weeks	obvious mineralization BMSCs showed substantial new bone formation, while scaffolds	Mouse
19.	19890976 2009 Ma ³¹	Rabbit BMSCs	I		8 Weeks	without cells did not Sheets of BMSCs without scaffold	Mouse
20.	19335406 2009 Chang ⁷¹	Bovine BMSCs	Alginate		30 Weeks	and form ectopic bone BMSCs showed endochondral	Mouse
5		Hiiman BMSCs	HA ceramic or B-TCP		8 Weeks	bone formation, particularly at high densities Greater home formation observed	Raf
22.	18458439 2007 Liu^{73}	Human BMSCs	B-TCP	I	12 Weeks	with HA ceramic than B-TCP Predifferentiated BMSCs on B-TCP	Mouse
23.	17324591 2007 Cai ⁷⁴	Mouse BMSCs	Alginate	I	8 Weeks	resulted in woven bone as early as 4 weeks Predifferentiation of BMSCs	Mouse
			3			toward ostoegenesis or chondrogenesis resulted in ectopic bone or cartilage, respectively	
Md	BCP, macroporous biphasic calciur	n phosphate; BMP2, bone mor	phogenetic protein 2; hPDLSC, human period	lontal lig	ament ster	cell; BMSC, bone marrow derived mesenchyr	mal stem cell;

PLGA, poly-lactic-co-glycolic acid; TCP, tricalcium phosphate; PTH, parathyroid hormone; PLLA, poly-L-lactide acid; HA, hydroxyapatite; aCS, absorbable collagen sponge; ETN, etanercept; VEGF, vascular endothelial growth factor; cUCB, canine umbilical cord blood; ALP, alkaline phosphate; BSA, bovine serum albumin; DPSC, dental pulp stem cell.

pro-osteogenic signaling cascades has been shown to be critical for successful MSC-mediated osseous repair of bone injury [21]. The bone morphogenetic protein (BMP) signaling pathway, for example, is acutely upregulated in a mouse calvarial defect model. This upregulation enables adipose-derived stem cells to successfully ossify a criticalsized defect [21].

The mechanical forces exerted on a graft site should be considered as well. MSC transplantation into a long bone defect is subject to significant stress/strain forces with weight-bearing and locomotion [22]. In contrast, ectopic models are largely void of mechanical force (perhaps slight compression of the implant depending on its size can be observed, especially in the kidney capsule model). Biomechanical forces are well-studied, involving a cascade of signaling events leading to bone formation, or "mechanotransduction" [22–25]. It is important to realize that ectopic bone models allow for near-complete removal of this potential extraneous experimental variable. Thus, ectopic bone formation models reduce the number of variables involved in bone formation, eliminating (or reducing) the effects of bone stimulating cytokines, bone forming cells, endogenous stem cells, and potentially bone-stimulating mechanotransduction. Each of the commonly used models discussed below has significant advantages and drawbacks.

Models of Ectopic Bone Formation

Subcutaneous implantation

Subcutaneous implantation is the most simplistic of all experimental models of ectopic bone formation. Surgically, it is the easiest of all models and a novice can perform this procedure with success after learning basic suturing technique. Nearly any mammalian animal model can be chosen, ranging from mouse and rat to rabbit, dog, and pig among numerous others (see Table 1 for a review). Rodent models are preferable and most widely used due to their low cost, lax skin (which accommodates large-volume implants), and availability of immunodeficient rodents for xenograft-based experiments. Generally, incisions should be made on the dorsum of the rodent so as to prevent the animals from removing their own sutures. Alternatively, intradermal stitches can be placed which avoids the possible need to dress the wound. Classically, bone marrow derived mesenchymal stem cells (BMSCs) are the most commonly studied cell type (Table 1). The availability of immunodeficient rats and mice makes possible and practical the transplantation of humanderived cells for increased clinical relevance. Cells may be transplanted immediately after derivation, after culture expansion, or after predifferentiation [26]. In such cases, predifferentiation may ensure adequate in vivo bone formation. However, culture time and conditions may change the overall composition of a cell population [27,28]. Further, predifferentiation is less ideal for clinical translation as the barrier for regulatory approval is higher if cells are taken ex vivo before implantation. Mesenchymal cells have been shown to have the ability to form bone when placed in an osteogenic environment; however, subcutaneous implantation often requires cytokine supplementation or molecular modifications [29,30]. Cell delivery methods are widely variable, from stiff poly lactic glycolic acid, to composite gels and other matrices. As an alternative to material scaffolds, culture-expanded cell sheets can be rolled and implanted without a carrier, showing new bone formation [31]. In addition, various growth factors and other stimuli have been added such as BMP2 and vascular endothelial growth factor to name a few (see again Table 1).

One of the more important considerations for subcutaneous bone models is a technical one. The physical identification of the implant can be challenging, especially as newlyformed bone can be similar in color to the surrounding dermal tissues. Moreover, the lax skin of rodents allows for potentially significant migration of an implant, a difficulty that can be compounded by small implant sizes. The authors suggest the use of colored scaffolds or the labeling of cells/ implants with a dye before implantation to facilitate identification upon removal. This becomes increasingly important with longer-term studies with months separating implantation and harvest.

Another consideration for subcutaneous bone formation is the theoretical lack of naturally bone-forming stem cells within the intradermal environment. This is in direct contrast to intramuscular bone formation (see below) in which striated muscle satellite progenitor cells are readily able to form bone, given an appropriate osteogenic stimulus. This lack of endogenous bone-forming cells may be a benefit or a disadvantage depending on the experimental design. For example, it may be a benefit if an exogenous stem cell is implanted, ensuring that in theory the predominant, newlyformed bone is from exogenous origin. On the other hand, it may be a detraction if the study is designed to expressly test a biomaterial scaffold, in which case an endogenous boneforming stromal cell may be needed to ensure adequate bone formation. A similar caveat should also be considered in subcutaneous models: skin injury has been shown to result in the honing of circulating progenitor cells to the defect site [32], and one cannot definitively exclude these progenitor cell types from participating in bone formation.

Finally, subcutaneous models may show inferior boneforming capacity in comparison to other experimental models of ectopic bone formation. In general, relatively greater ectopic bone formation is observed within the intramuscular compartment compared with intradermal compartment [33]. For example, in one study performed on dogs and pigs, bone formation could be histologically observed after 45 days after intramuscular transplantation in contrast to 60 days after subcutaneous implantation [34]. However, exceptions to this general observation do exist, where, for example, a particular nano-crystalline hydroxyapatite scaffold produced significantly more subcutaneous rather than intramuscular bone in minipigs [35]. In general, the reduced ectopic bone formation in subcutaneous models may be due to reduced vascularization and blood flow-which is especially striking in comparison to the infrarenal capsule model as discussed below. Therefore, a lack of robust subcutaneous bone formation and the need for extended in vivo "incubation" times may limit the utility of subcutaneous models.

Muscle pouch implantation

Muscle Pouch (or intramuscular) implantation has a rich history in bone formation. In fact, BMPs were first studied for their ability to induce bone formation in a muscle pouch model [36]. Like subcutaneous ectopic bone formation,

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TABLE 2.

Animal	Sheep	Rabbit	Pig	Mouse	Mouse	Rat	Dog	Goat	Mouse	Goat	Rabbit
Results	Bone formation was seen with BCP alone or with most polymeric gel formulation excepting polyvinvl alcohol	Use of novel bilayer implant and BMSCs produced a neocartilage with subchondral bone like structure	Early osteogenesis detected as early as 5 weeks	Nano hydroxyapatite yielded higher bone density than other	Combination HA/DBM showed more robust ectoric home formation	B-TCP addition significantly enhanced hone formation	40% calcium apatite content resulted in significant bone formation in comparison	Larger porosity of scaffold led to greater ectopic home formation	Intramuscular injection of COMP-Angl dose- dependently enhanced BMP2-induced ectopic hone formation	BMSC sected implants showed 21% bone formation in comparison to minimal bone formation with scaffold alone	New bone formation was observed at 8 weeks with degradation of the
Duration	12 Weeks	12 Weeks	8 Months	4 Weeks	8 Weeks	3 Weeks	12 Weeks	12 Weeks	2 Weeks	12 Weeks	8 Weeks
Scaffold(s)	Biphasic calcium phosphate particles combined with 5 different polymeric gels	Poly vinyl alcohol/ gelatin-nano- hydroxyapatite/ polyamide6 scaffold	Nano-crystalline hydroxyapatite/ silica gel matrix	β-tricalcium phosphate compared with 4 different ceramics	Hydroxyapatite/DBM combined or alone	Chitosan hydrogel with or without B-TCP	Nano-sized calcium phosphate apatite particles in poly (D,L-lactide)	Porous CA ceramics	I	Biphasic calcium phosphate porous blocks	TCP ceramics
Protein(s)	I	I	I	BMP2	I	BMP2	I	I	Adenoviral delivered Cartilage Oligomeric Matrix Protein- Angiopoletin 1 or BMP7		I
Cell(s)	I	Rabbit neonatal BMSCs	I		Human BMSCs	I	I		I	Goat BMSCs	Rabbit BMSCs
Year Site	2011 Dorsum	2011 Hind limb	2011 Trapezius	2011 Thigh	2011 Abdominal Muscle	2010 Quadriceps	2010 Paraspinal	2010 Paraspinal	2010 Thigh	2010 Paraspinal	2010 Dorsum
PMID Author	21241835 Barbieri ⁷⁵	20967773 Qu ⁷⁶	21478102 Götz ³⁵	21569871 Billström ⁷⁸	21205997 Lee ⁷⁹	21105153 Luca ⁸⁰	20526989 Barbieri ⁸¹	19944783 Habibovic ⁴⁸	19782780 Jeong ⁸³	19769525 van Gaalen ^{s4}	19582839 Nan ⁸⁵
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659

	Animal	Mouse	Goat	Mouse	Mouse	Mouse	Mouse	Dog	Sheep	Goat	Mouse
	Results	TCP ceramic scaffold Hyaluronan based scaffolds showed greater bone formation than	Up to 16 weeks, ectopic bone forming activity was observed with either autologous or	allogenetic BMSCs ERRy alone had no effect, BMP2 alone increased bone formation. ERRy significantly decreased BMP2-induced houe	Vascular endothelial cells responded to BMP2 administration with chondrogenic and	osteogenic differentiation caALK2 induces ectopic ossification only in the setting of inflammation	Pulsed ultrasound led to accelerated BMP4 induced ectopic bone formation	ASCs showed significant enhancement of bone formation in comparison	to ceramic alone Mature ectopic bone was observed within the MRCP/fihvin composites	Abundant and homogenous bone formation observed with BMSCs in comparison to little bone in controls	Gender of cell derivation and host influences BMP4 induced osteogenesis. Male donors and hosts induce greater and more consistent bone formation
Table 2. (Continued)	Duration	3 Weeks	16 Weeks	5 Weeks	2 Weeks	1 Week	3 Weeks	12 Weeks	6 Months	9 Weeks	3 Weeks
	Scaffold(s)	Chitosan and hyaluronan hydrogels	Ceramic scaffold	I	Matrigel	I	I	BCP ceramic	Biphasic calcium phosphate (MBCP) ceramic oranules /fibrin olue	Porous BCP disks	Sterile gelatin sponge
	Protein(s)	BMP2	Platelet-leukocyte gel	I	BMP2	Adenoviral delivered constitutively active ATK2 (ca ATK2)	BMP4 expressing plasmid	I	I	I	I
	Cell(s)	I	Goat BMSCs	MC3T3-E1 or C2Cl2 cells overexpressing ERR? or BMP2	I	l	I	Dog ASCs	I	Goat BMSCs	BMP4 overexpressing Mouse skeletal muscle derived stem cells
	Year Site	2010 Quadriceps	2009 Paraspinal	2009 Thigh	2009 Tibialis anterior	2009 Hind limb	2009 Gastrocnemius	2009 Dorsum	2008 Paraspinal	2007 Paraspinal	2007 Hind limb
	PMID Author	20600403 Luca ⁸⁶	19374487 Geuze ⁸⁷	19324883 Jeong ⁸⁸	19255227 Lounev ⁸⁹	19029982 Yu ³⁹	19961269 Watanuki ⁹¹	19386665 Yao ⁹²	17619955 Le Nihouannen	17182096 Kruyt ⁹⁴	17605633 Corsi ⁹⁵
	Article No.	12.	13.	14.	15.	16.	17.	18.	19.	20.	21.

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660

	Animal	Mouse	Rat	Mouse	Rat, rabbit, dog	Rat	Human	Human
	Results	BMP4 induced endochondral bone formation with 100% efficiency by 2 weeks	Low concentration FGF2 promotes BMP2-induced ectopic bone formation	Undifferentiated BMSCs with novel composite scaffold induced significant woven bone	Biphasic calcium phosphate scaffolds induced greater bone formation in comparison to HA scaffolds	BMP2 induced endochondral bone formation and induced VEGF expression. VEGF increased BMP2-induced ectopic bone	Hydroxyapatite coated with BMP7 can form a replacement mandible	Successful ossification of a replacement mandible
	Duration	2 Weeks	3 Weeks	8 Weeks	3 Months	3 Weeks	6.5 Months	7 Weeks
	Scaffold(s)	I	Atelopeptide type I collagen	HA/TCP particles in self-hardening HPMC hydrogel	Biphasic calcium phosphate and HA scaffolds	Atelopeptide type I collagen (CL)	Hydroxyapatite implant	Titanium mesh with recombinant BMIP7 and bovine bone
TABLE 2. (CUNTINU	Protein(s)	BMP4 expressing plasmid	FGF2 and/or BMP2	I	I	BMP2±VEGF	Human BMP7	Human BMP7
	Cell(s)	I		Mouse BMSCs	I	I		Human BMSCs
	Year Site	2006 Gastrocnemius	2006 Hind limb	2006 Hind limb	2006 Thigh (rabbits and rats), gluteus (dogs)	2006 Calf	2006 Left Pectoralis Major	2004 Latissimus Dorsi
	e PMID Author	16961179 Kotajima ⁹⁶	16808813 Kakudo ⁹⁷	16510180 Trojani ⁹⁸	16846356 Yuan ⁹⁹	16857215 Kakudo ¹⁰⁰	16257511 Heliotis ³⁸	15337402 Warnke ³⁷
	Articl No.	22.	23.	24.	25.	26.	27.	28.

ASC, adipose-derived stem cell; CA, carbonated apatite; FGF2, fibroblast growth factor 2.

TABLE 2. (CONTINUED)

intramuscular bone formation may also be used in nearly any animal model (see Table 2). Although the mainstay remains rodent models, intramuscular implantation is readily translatable to larger animals (dog, pig, goat, and sheep). Intramuscular implantation has also been used in the human patient to successfully generate bone. For example, in 2004 Warnke et al. reported the intramuscular growth of a replacement human mandible using autologous bone marrow and BMP7 [37]. As another example, Heliotis et al. determined that even without added stem cells, BMP7 with hydroxyapatite can lead to replacement mandible ossification [38].

In small animal models, the hind limb is preferentially used. Generally, the authors suggest implantation in the thigh complex that affords space for a large-volume implant. In the thigh muscles of a mouse, for example, a maximum volume of up to $\sim 150 \,\mu$ L can be implanted. By contrast, the lower leg can be used for smaller volume implants. Benefits of using the lower leg are a readily palpable implant that can be monitored for growth or imaged by surface ultrasound if desired. Intramuscular implantation in a large animal is most often in the dorsal musculature, including paraspinal muscles or trapezius.

In recent years, BMP2 and other BMPs have been widely studied in intramuscular ectopic bone models [39]. BMPs are known to stimulate the osteogenic differentiation of native skeletal muscle satellite cells. This reinforces an important distinction between the intramuscular implantation model and other ectopic bone models: the presence of a native skeletal progenitor cells. If another osteoprogenitor cell source is experimentally implanted in a muscle pouch environment, it becomes critical to identify the cells on later histological analysis. This can be achieved by transfection with a reporter system, by gender mismatch of host and donor, or by xenografting and detection of species-specific antigens among other techniques. These techniques will allow for definitive identification of hosts from donor-derived bone. This extra step in analysis is vital for valid interpretation of intramuscular bone formation and could be a consideration to opt for another ectopic bone formation assay.

Another critical distinction to make for intramuscular implantation experiments is that of the pro-osteogenic cytokine elaboration from sites of muscle injury. BMP signaling has been shown to be naturally upregulated postmuscle injury via Smad activation [40,41]. Normally this is important for the regulation of proliferation and myogenic differentiation of skeletal muscle satellite cells and their descendants. However, this heightened BMP signaling postmuscle injury theoretically represents a potentially confounding factor in intramuscular ectopic bone models. Like BMP signaling, other signaling pathways known to be important in osteogenesis are also upregulated by muscular injury. These include TGF-β1 and insulin-like growth factor 1 to name a few [42,43]. In light of these findings, it is important to utilize blunt dissection rather than traumatic sheering of muscle fibers when creating the potential space for implant insertion. A relatively atraumatic muscle pocket creation will theoretically minimize this natural upregulation of BMP and other pro-osteogenic cytokines. On that note, similar cytokines are upregulated after cutaneous injury (most prominently TGF-\u00b31), and may also play a confounding role in subcutaneous ectopic bone models.

Kidney capsule implantation

The kidney capsule model is a less frequently used method of ectopic bone formation, primarily owing to its relative technical difficulty in comparison to subcutaneous or intramuscular transplantation. Material is placed between the thin, fibrous capsule of the kidney and the underlying renal parenchyma. This material can be inserted either directly by injection with a small gauge needle, or surgically by creating a small incision in the capsule and gently inserting the material underneath the capsule. For the insertion method, a space should be created using blunt dissection (eg, using a melted Pasteur pipette). Unlike in primates, the kidney of rodents is an intraperitoneal organ and so the peritoneum must be incised before visualization of the kidney. The surgical insertion method is more technically challenging than the injection method, so prior practice is advisable. Most importantly, the capsule should remain intact to ensure that the implant stays in place and that proper vascularization will ensue. Material should not be injected into the parenchyma of the organ. Both the peritoneum and skin should be sutured after implantation.

A list of recent citations using the kidney capsule model for bone formation can be found in Table 3. The majority of studies utilize mice (either wild-type or immunocompromised), while a few use rats. BMSCs are the most commonly studied cell type, while cells derived from the tooth are often studied as well. A wide array of materials can be used for implantation including gels, bone matrices, and biodegradable sponges. A cell suspension or cell pellet can be injected as well, without any scaffold or carrier. The majority of implants are thereafter analyzed from 1 to 4 weeks postimplantation, but studies even up to 10 months in length have been described [44].

Significant features of the renal capsule model include: (1) increased blood flow to the implant, (2) theoretical lack of endogenous bone-forming stem cells, (3) size limitations of the implant, and (4) compressive force on the implant. Each will be considered in turn below. First, implants placed in the subrenal capsular assay are exposed to significant blood flow and likewise blood-borne nutrients. This has led in reports to supraphysiologic bone growth in comparison to native bone samples [45]. However, this can be considered a benefit rather than a detraction as engrafted cells are likely to survive and proliferate once in place. Moreover, the highly vascular environment may allow for the development of complex tissue types such as tooth-like structures in the field of dental research [46-48] and calvarial suture-like structures [45]. Secondly, the subrenal capsule microenvironment is theoretically free of bone-forming endogenous stem cells. While trafficking of endogenous stem cells is theoretical, it is almost certain that the engrafted cells are responsible for any observed bone formation. Third, limitations on the size of implant can be of concern, as larger volumes can inadvertently tear the capsule. While mice are most often used, rats can be substituted for larger implants (Table 3). Fourth and finally, the capsular tissue overlying the engrafted cells may be fairly taut, especially if large-volume implants are used. This can relay a compressive force onto the implant itself, which may predispose to cartilage over bone formation depending on the cell type [49-51].

TABLE 3. RECENT STUDIES USING PERIRENAL IMPLANTATION

Animal	Rat	Mouse	Mouse	Mouse	Mouse	Mouse		Mouse	Rat	Mouse	Mouse	e Mouse
Results	Mature appearance and organized structure of enamel-dentin like fissue	ESTP-treated tooth buds developed normal morphology whereas untreated controls developed abnormally	Structural similarity to normal bone was identified with regions of cartilaginous, compact, and trabecular bone	Structural similarity to normal cranial sutures was identified amono transulanted hone	All MSC types showed ectopic bone	Chronic blood loss led to	hematopoietic microenvironment, reduction in bone formation and activation of the bone resorption	All dental mesenchymal/follicle	Dental pulp stem cell/apical cell combinations showed normal morphology while BMSC/apical bud cell showed atypical	morphology without ename Transplanted tissues contained mineralized islands with osteocyte - like cells embedded within the atubular - mineralized matrix	BMSCs without expansion sporadically formed bone, while BMSCs after expansion on fibrin- based microbeads reliably formed bone	BMSCs derived from male and female donors and transplanted in the kidney capsule respond to sex hormones with gender specific properties
Duration	8 Weeks	4 Weeks	4 Weeks	2 Weeks	2 Weeks	10 Months		3 Weeks	2 Weeks	2 Weeks	4 Weeks	3 Weeks
Scaffold	Nanoscale B-TCP/ collagen particles	Fibrin glue	Matrigel		DBM	I			Gelatin	I	Fibrin-based microbeads	
Protein	BMP2	EDTA soluble tooth proteins (ESTP)	I	l					I	I	1	Estradiol 17β, dihydrotestosterone
Year Cell(s)	2011 Rat tooth germ cells	2011 Embryonic tooth-forming primordia] and xenogenic murine apical bud epithelium/human dental pulp stem cell composites	2009 Mouse fetal osteoblasts	2009 Embryonic and early postnatal calvarial bone	2008 Mouse MSCs from bone marrow,	placenta, or unimilical coru 2007 Mouse BMSCs		2007 Mouse dental follicle cells	2007 Rat dental pulp stem cells, rat BMSCs/apical bud cells	2003 Mouse dental pulp cells	2002 Rat and Mouse BMSCs	2001 Mouse BMSCs
PMID Author	21427841 Zhang ⁴⁶	20695775 Chun ⁴⁷	19078959 Chan ¹⁰⁵	19590164 Lenton ⁴⁵	18619727 Prigozhina ¹⁰⁷	17198881 Gurevitch ⁴⁵		17618464 Kim ¹⁰⁹	17371295 Yu ⁴⁸	12755333 Braut ¹¹¹	12202005 Gurevich ¹¹²	11341327 Berger ¹¹³
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EDTA, ethylenediaminetetraacetic acid.

Summary

Experimentally induced ectopic bone formation is a wellstudied, well-described entity with subcutaneous, intramuscular, and kidney capsule transplantation being the most common models. Briefly, the most pertinent concern for subcutaneous implantation is the potential lack of robust bone growth, potentially attributable to poor blood flow. Intramuscular implantation exposes the implant to satellite progenitor cells, which theoretically makes distinguishing host from donor osteogenesis difficult. The kidney capsule method allows for supraphysiologic blood and nutrient resource, allowing for robust bone growth despite being a technically challenging assay. All 3 models are valid experimental entities; however, their distinct differences should be taken into account when either constructing or analyzing an experiment. Analyses of such models are crucial to understand the osteogenic differentiation of cells independent from an osseous environment. Thus, as skeletal tissue engineering progresses and the use of osteogenic progenitor cells becomes more commonplace, such models will hopefully allow for optimization of bone formation. Conversely, understanding the biology of ectopic bone formation might also allow for improved treatments of debilitations such as HO.

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ECTOPIC BONE FORMATION

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