

BODIPY-Based Molecular Probe for Imaging of Cerebral β -Amyloid Plaques

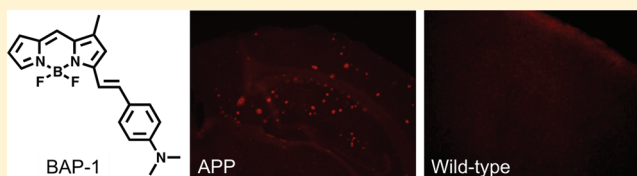
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Supporting Information

ABSTRACT: We designed and synthesized a BODIPY-based probe (BAP-1) for the imaging of β -amyloid plaques in the brain. In binding experiments *in vitro*, BAP-1 showed excellent affinity for synthetic $A\beta$ aggregates. β -Amyloid plaques in Tg2576 mouse brain were clearly visualized with BAP-1. In addition, the labeling of β -amyloid plaques was demonstrated *in vivo* in Tg2576 mice. These results suggest BAP-1 to be a useful fluorescent probe for the optical imaging of cerebral β -amyloid plaques in patients with Alzheimer's disease.

KEYWORDS: Alzheimer's disease, β -amyloid plaque, BODIPY, optical imaging



The formation of β -amyloid ($A\beta$) plaques is a critical neurodegenerative change in Alzheimer's disease (AD).^{1,2} Since the imaging of $A\beta$ plaques *in vivo* may enable the pre-symptomatic diagnosis of AD, several imaging technologies including positron emission tomography (PET),^{3–21} single photon emission computed tomography (SPECT),^{22–24} magnetic resonance imaging,^{25–28} and optical imaging^{29–33} have been applied for this purpose. In particular, several PET probes have shown the feasibility of imaging $A\beta$ plaques in AD brains. PET imaging is an established clinical modality that provides good sensitivity deep in tissue. However, it is limited by a time-consuming data acquisition process, exposure to radioactivity, the need for expensive equipment and highly skilled personnel, and a relatively poor spatial resolution.

Conversely, optical imaging with fluorescent probes is a relatively new modality that offers real-time, nonradioactive, and, depending on the technique, high-resolution imaging,³⁴ leading to a rapid, inexpensive, and nonradioactive drug screening system for AD. However, there have been fewer reports regarding the development of fluorescent probes than PET probes despite their significance, although AOI-987,²⁹ NIAD-4,³⁰ CRANAD-2,³² ANCA-11,³⁵ and BMAOI³⁶ have been reported for the imaging of $A\beta$ plaques.

Compounds containing a boron dipyrromethane (BODIPY) scaffold have widespread applications as dyes, fluorescent probes in biological systems, and materials for incorporation into electroluminescent devices.^{37–40} Their broad utility is due to their high thermal and photochemical stability, chemical robustness, and tunable fluorescence properties. We have previously reported a dual SPECT/fluorescent probe based on the BODIPY scaffold, for the imaging of $A\beta$ plaques *in vivo*.⁴¹ Despite good affinity for synthetic $A\beta(1–42)$ aggregates and the clear labeling of $A\beta$ plaques in sections of the mouse brain, the BODIPY-based probe was not suitable for imaging *in vivo* due to its poor uptake into the brain. Two other papers have

reported BODIPY-based probes targeting $A\beta$ plaques.^{42,43} However, these derivatives have not been applied to imaging *in vivo* perhaps due to their low brain uptake and short excitation/emission wavelength, though they showed high affinity for $A\beta$ plaques *in vitro*. The findings of these previous studies suggested that additional structural changes may modify the properties of BODIPY derivatives to improve their suitability for imaging *in vivo*.

Many $A\beta$ -imaging probes for PET applied in clinical trials possess a dimethylamino styryl group as a consensus structure as reported previously.^{3,22,44–46} Then, in the present study, we designed and synthesized a new BODIPY-based $A\beta$ probe (BAP-1) with a dimethylamino styryl group which plays an important role in binding to $A\beta$ aggregates. BAP-1 belongs to a class of dyes that are collectively called molecular rotors, where the dimethyl-aniline is the donor, and the BODIPY unit is the acceptor.⁴⁷ This motif is typical of $A\beta$ -imaging probes. Here, we report the *in vitro* and *in vivo* evaluation of BAP-1 as a new probe for the optical imaging of cerebral $A\beta$ plaques.

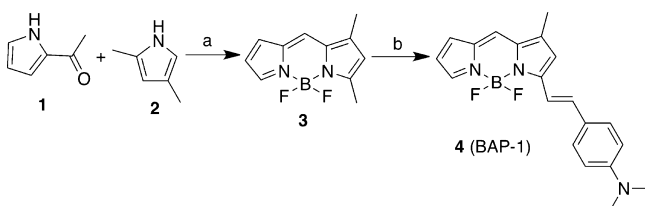
RESULTS AND DISCUSSION

The target BODIPY derivative (BAP-1) was synthesized as shown in Scheme 1. Although the synthetic route for this compound has been reported,³⁷ we made some modifications. The key step in the formation of the BODIPY backbone (3) was accomplished by the condensation of pyrrole 2-carboxyaldehyde (1) and 2,4-dimethylpyrrole (2) at low temperature, followed by the addition of $\text{BF}_3 \cdot \text{OEt}_2$ in a yield of 36.1%. Compound 4 (BAP-1) was successfully prepared by the condensation of 3 and 4-dimethylaminobenzaldehyde in the presence of piperidine and acetic acid (50.6% yield).

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Scheme 1. Synthetic Route for BAP-1^a

^aReagents: (a) CHCl_3 , POCl_3 , BF_3OEt_2 , Et_3N ; (b) toluene, 4-dimethylaminobenzaldehyde, piperidine, and AcOH .

First, we evaluated the fluorescent properties including absorption, excitation, emission wavelength, and quantum yield of BAP-1 in CHCl_3 . BAP-1 exhibited absorption, excitation, and emission wavelengths of 604, 614, and 648 nm, respectively, with a high fluorescent quantum yield (46.8%) (Table 1). Although

Table 1. Fluorescence Characterization of BAP-1^a

Abs (nm)	Ex (nm)	Em (nm)	quantum yield (%)
604	614	648	46.8

^aAbsorbance, fluorescence excitation and emission, and quantum yield of BAP-1 were determined with $10 \mu\text{M}$ of the compound in CHCl_3 .

BAP-1 showed slightly shorter wavelengths of excitation/emission at 614/648 nm than are appropriate for optical imaging in vivo, its high quantum yield was expected to enable the imaging of $A\beta$ plaques in shallow areas of the mouse brain.

Furthermore, when BAP-1 existed in a solution containing $A\beta$ aggregates or bovine serum albumin (BSA), its fluorescent intensity increased with the concentration of the aggregates, indicating affinity for $A\beta$ aggregates (Figure 1). However, we

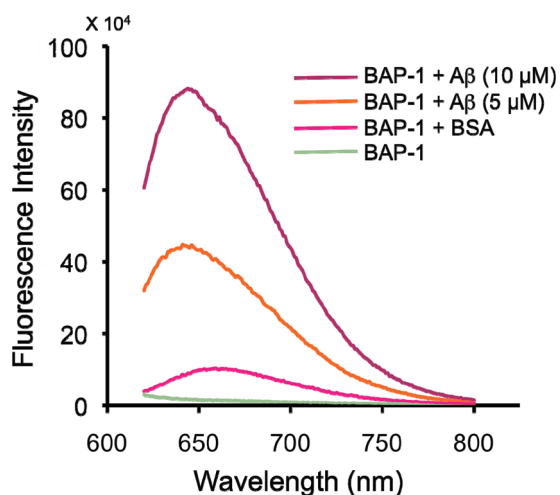


Figure 1. Fluorescence intensity of BAP-1 upon interaction with $A\beta$ 42 aggregates and BSA.

found no significant change in fluorescence during the incubation with BSA, indicating that there is little interaction between BAP-1 and BSA.

To quantify the affinity for $A\beta$ aggregates, we measured the apparent binding constant (K_d) of BAP-1 by conducting a saturation assay (Figure 2). The fluorescent intensity of BAP-1 increased in a dose-dependent manner and was saturated at the higher concentration. Transformation of the saturation binding data to Scatchard plots provided linear plots, indicating that

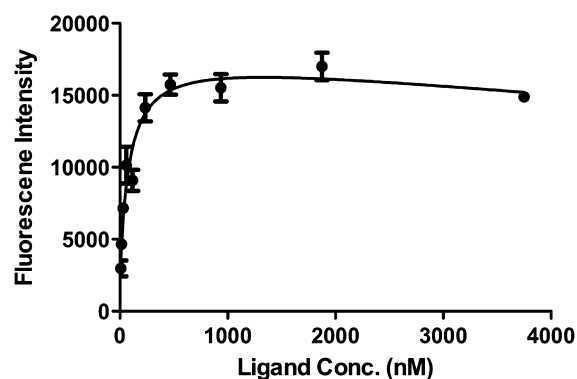


Figure 2. Plot of the fluorescence intensity ($E_m = 673 \text{ nm}$) as a function of the concentration of BAP-1 in the presence of $A\beta$ 42 aggregates ($2.2 \mu\text{M}$) in solutions.

BAP-1 has one binding site on $A\beta$ aggregates. BAP-1 showed excellent affinity for $A\beta$ aggregates at a K_d value of 44.1 nM .

To confirm the affinity of BAP-1 for $A\beta$ plaques in the brain, neuropathological fluorescent staining with BAP-1 was carried out using brain sections from Tg2576 mice (Figure 3). Tg2576 mice have been specifically engineered to overproduce $A\beta$ plaques in the brain⁴⁸ and frequently used to evaluate the specific binding of $A\beta$ plaques in experiments in vitro and in vivo.^{49–51} Many fluorescent spots were observed in the brain sections of Tg2576 mice (32-month-old, female) (Figure 3A), while no spots were observed in the wild-type mice (29-month-old, female) (Figure 3B). The staining pattern was consistent with that observed with thioflavin S (Figure 3C), a dye commonly used to stain $A\beta$ plaques,⁵² indicating that BAP-1 shows specific binding to $A\beta$ plaques in the mouse brain.

One important prerequisite for a probe for imaging of $A\beta$ plaques in the brain is to penetrate the blood–brain barrier after an i.v. injection. Furthermore, the ideal amyloid-imaging agent should be rapidly washed out from normal brain tissue in addition to having a high brain uptake. Since normal brain tissue has no amyloid plaques to trap the agent, the washout should be fast, providing a higher signal-to-noise ratio in the AD brain. To test the uptake into and washout from the brain, we determined the fluorescent intensity in the brain after the injection of BAP-1 into a normal mouse. BAP-1 showed high initial brain uptake at 2 min postinjection, but the fluorescence that accumulated in the brain was rapidly eliminated, both of which are highly desirable properties for $A\beta$ imaging probes (Figure 4).

To evaluate the potential of BAP-1 in living brain tissue, we carried out experiments ex vivo using a Tg2576 mouse (25-month-old male) and a wild-type mouse (25-month-old male) as an age-matched control. The fluorescence in whole brains removed at 1 h postinjection of BAP-1 was much higher in the Tg2576 mouse than wild-type mouse (Figure 5).

To further evaluate what the higher fluorescence in the Tg2576 mouse brain was derived from, we prepared frozen sections from both brains and observed them with a fluorescence microscope. The brain sections from the Tg2576 mouse showed distinctive staining of $A\beta$ plaques by BAP-1 (Figure 6A), while those from the wild-type mouse showed no such staining (Figure 6B). The staining pattern in the brain sections from the Tg2576 mouse was consistent with that observed on immunohistochemical staining with an antibody specific for $A\beta(1–42)$ (BC05) as shown by arrows in Figure 6C. The results suggest that BAP-1 penetrated the blood–brain



Figure 3. Neuropathological staining of BAP-1 in a 10- μ m section from a Tg2576 mouse brain (A) and a wild-type mouse brain (B). Labeled plaques were confirmed by staining of the adjacent section with thioflavin-S (C).

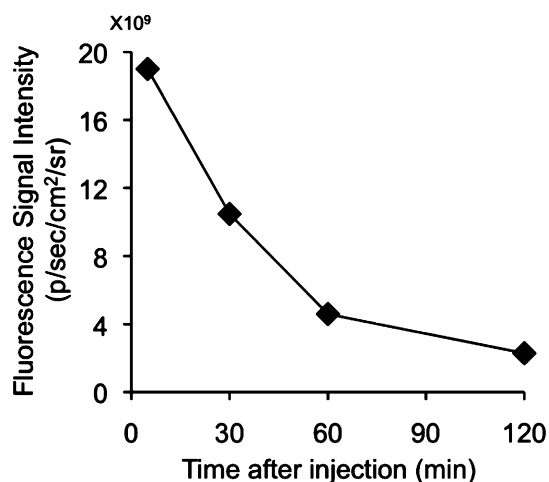


Figure 4. Fluorescence intensity after injection of BAP-1 into ddY mice with an IVIS spectrum.

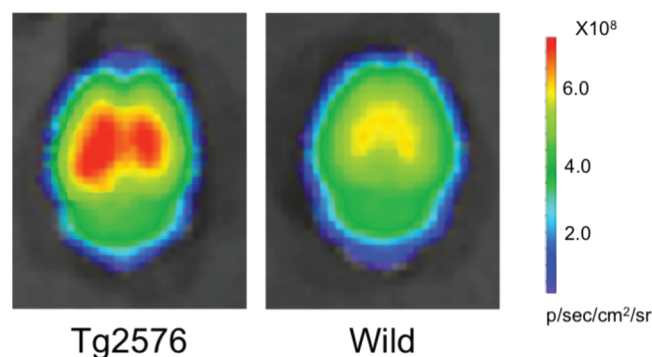


Figure 5. Comparison of the fluorescence intensity in the brain after the injection of BAP-1 into a Tg2576 mouse (A) and wild-type mouse (B).

barrier and selectively labeled the $A\beta$ plaques in the brain, as reflected by the biodistribution experiments and *in vitro* binding assays. To our knowledge, this is the first report that BODIPY-based probes can function as $A\beta$ imaging probes *in vivo*. However, the excitation and emission wavelengths of BAP-1 were still shorter than the ideal wavelengths for optical imaging *in vivo*. Several BODIPY derivatives with longer wavelengths in the near-infrared region have recently been reported.^{53–55} On the basis of these findings, we may develop more appropriate BODIPY-based probes for the imaging of $A\beta$ plaques *in vivo*.

We also conducted *in vivo* imaging experiments using Tg2576 mice and age-matched controls. However, we could not find a significant difference between the two groups, because the fluorescence of BAP-1 accumulated nonspecifically in the scalp in both groups. To improve nonspecific accumulation in the scalp, further modification of the BODIPY scaffold will be needed in the future.

In conclusion, we successfully designed and synthesized a BODIPY-based $A\beta$ probe, BAP-1, for optical imaging *in vivo*. In binding experiments *in vitro*, BAP-1 showed high affinity for $A\beta$ aggregates. BAP-1 clearly stained $A\beta$ plaques in the mouse brain, reflecting its affinity for $A\beta$ aggregates *in vitro*. In animal experiments using normal mice, BAP-1 displayed good uptake into and fast washout from the brain. In addition, *ex vivo* fluorescent staining of brain sections from Tg2576 mice after the injection of BAP-1 showed selective binding of $A\beta$ plaques with little nonspecific binding. These findings suggest BAP-1 to be a useful molecular probe for the detection of $A\beta$ plaques in AD brains and also provide useful information for the development of new BODIPY-based probes in the future.

METHODS

General. All reagents were obtained commercially and used without further purification unless otherwise indicated. ¹H and ¹³C NMR spectra were obtained on a JEOL JNM-LM400 spectrometer with TMS as an internal standard. Coupling constants are reported in hertz. Multiplicity was defined by s (singlet), d (doublet), and m (multiplet). Mass spectra were obtained on a SHIMADZU GC-2010. HPLC was performed with a Shimadzu system (a LC-20AD pump with a SPD-20A UV detector, $\lambda = 254$ nm) using a Cosmosil C18 column (Nacalai Tesque, SC₁₈-AR-II, 4.6 \times 150 mm) and acetonitrile/water (3/2) as the mobile phase at a flow rate of 1.0 mL/min. The target compound was proven by this method to show >95% purity.

Chemistry. *1,3-Dimethyl-4,4-difluoro-4-bora-3a,4a-diaza-s-indacene (3)*. A solution of pyrrole 2-carboxyaldehyde (**1**) (368 mg, 3.87 mmol) and 2,4-dimethylpyrrole (**2**) (368 mg, 3.87 mmol) in CHCl_3 (10 mL) was cooled to 0 °C. After POCl_3 (360 μL) was added with caution, the mixture was stirred at room temperature for 2 h. $\text{BF}_3 \cdot \text{OEt}_2$ (3 mL) and Et_3N (3 mL) were added sequentially, and the resulting mixture was stirred at room temperature for 10 min. The solution was washed with H_2O and dried with Na_2SO_4 . The solvent was removed, and the residue was purified by silica gel column chromatography (hexane/ethyl acetate = 2:1) to give 308 mg of **3** (36.1%). ¹H NMR (400 MHz, CDCl_3) δ 2.28 (s, 3H), 2.59 (s, 3H), 6.16 (s, 1H), 6.43 (m, 1H), 6.93 (d, $J = 3.6$ Hz, 1H), 7.20 (s, 1H), 7.65 (s, 1H). ¹³C NMR (100 MHz, CDCl_3) δ 11.3, 15.0, 116.2, 121.2, 124.8, 126.5, 132.5, 136.5, 138.9, 146.0, 163.1. MS m/z 220 (M^+).

4,4-Difluoro-3-((E)-[2-(4-dimethylaminophenyl)ethenyl]-1-methyl-4-bora-3a,4a-diaza-s-indacene (4, BAP-1). Compound **3** (120 mg, 0.55 mmol) and 4-dimethylaminobenzaldehyde (82 mg, 0.55 mmol) were dissolved in toluene (10 mL) with piperidine (350 μL) and AcOH (350 μL). The mixture was stirred under reflux for 1 h. After the mixture cooled to room temperature, H_2O was added and extracted with ethyl acetate. The organic phase was dried over Na_2SO_4 and filtered. The solvent was removed, and the residue was purified by silica gel chromatography (hexane/ethyl acetate = 1:2) to give 97 mg of **4** (50.6%). ¹H NMR (400 MHz, CDCl_3) δ 2.30 (s, 3H), 3.09 (s, 6H), 6.42 (m, 1H), 6.73 (m, 3H), 6.84 (d, $J = 3.9$ Hz, 1H), 7.06 (s, 1H), 7.36 (d, $J = 16.6$ Hz, 1H), 7.46 (d, $J = 16.3$ Hz, 1H), 7.54 (d, $J = 8.8$ Hz, 2H), 7.60 (s, 1H). ¹³C NMR (100 MHz, CDCl_3) δ 11.4, 40.1,

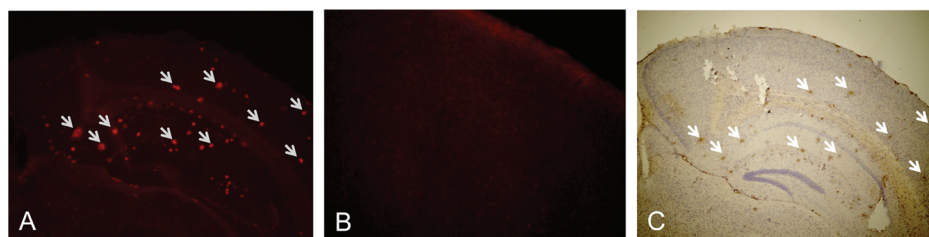


Figure 6. Ex vivo fluorescence observation of brain sections from a Tg2576 mouse (A) and wild-type mouse (B) after an injection of BAP-1. The presence of A β plaques in the section from the Tg2576 mouse was confirmed with immunohistochemical staining using a monoclonal A β antibody (C). Arrows show A β plaques stained by both BAP-1 (A) and immunohistochemical labeling (C).

111.9, 113.4, 115.2, 117.4, 120.4, 123.4, 123.8, 130.1, 132.6, 136.2, 138.4, 141.9, 144.4, 151.7, 160.6. MS m/z 351 (M^+).

Fluorescence Measurements Using A β (1–42) and BSA. A solid form of A β (1–42) was purchased from Peptide Institute (Osaka, Japan). Aggregation was carried out by gently dissolving the peptide (0.25 mg/mL) in PBS (pH 7.4). The solution was incubated at 37 °C for 42 h with gentle and constant shaking. A mixture (100 μ M of 10% EtOH) containing BAP-1 (10 μ M) and A β (1–42) aggregates (0, 5, and 10 μ M) or BSA (45 μ g/mL) was incubated at room temperature for 30 min. After incubation, fluorescence emission spectra were collected between 645 and 800 nm with excitation at 614 nm.

Measurement of the Constant for Binding of A β Aggregates in Vitro. A mixture (100 μ L of 10% EtOH) containing BAP-1 (final conc. 0–3.75 μ M) and A β (1–42) aggregates (final conc. 2.2 μ M) or BSA (10 μ M) was incubated at room temperature for 30 min. Fluorescence intensity at 673 nm was recorded (Ex: 614 nm). The K_d binding curve was generated by GraphPad Prism 5.0 (GraphPad Software, Inc., La Jolla, CA, USA).

In Vitro Fluorescent Staining of Mouse Brain Sections. The experiments with animals were conducted in accordance with our institutional guidelines and approved by the Kyoto University Animal Care Committee. The Tg2576 transgenic mouse (female, 32-month-old) and wild-type mouse (female, 29-month-old) were used as the AD model. After the mouse was sacrificed by decapitation, the brain was removed and sliced into serial sections 10 μ m thick. Each slide was incubated with a 50% EtOH solution of BAP-1 (100 μ M). Finally, the sections were washed in 50% EtOH for 1 min two times and examined using a microscope (BIOREVO BZ-9000, Keyence Corp., Osaka, Japan) equipped with a Texas Red filter set (excitation filter, Ex 540–580 nm; dichroic mirror, DM 595; barrier filter, BA 600–660). Thereafter, the serial sections were also stained with thioflavin S, a pathological dye commonly used for staining A β plaques in the brain, and examined using a microscope equipped with a GFP-BP filter set (excitation filter, Ex 450–490; dichroic mirror, DM 495; barrier filter, BA 510–560).

Ex Vivo Imaging of Brains from Normal Mice. A mixed solution consisting of 20% DMSO and 80% propylene glycol (100 μ L) of BAP-1 (500 μ M) was injected intravenously directly into the tail of ddY mice (5-week-old). The mice were sacrificed at 2, 10, 30, and 60 min postinjection. The brain was removed and weighed, and fluorescence images of brains were acquired with an IVIS SPECTRUM imaging system (Caliper Life Sciences Inc., Hopkinton, MA, USA) with a 0.1-s exposure (f -stop = 2) and a customized filter set (excitation, 605 nm; emission, 660 nm). The fluorescence intensity in each region of interest covering an entire tissue was expressed as photons/sec per g after the subtraction of background signals obtained in a region of interest set over an area without any tissue.

Ex Vivo Imaging Using a Tg2576 Mouse and an Age-Matched Control. A 25-month-old Tg2576 mouse and a wild-type mouse were intravenously injected with 200 μ L of BAP-1 (133 μ M, 10% EtOH). After 1 h, the mice were sacrificed, and the brain was removed and frozen in powdered dry ice. Fluorescence images of the brains were acquired with an IVIS SPECTRUM imaging system (Caliper Life Sciences Inc., Hopkinton, MA, USA) with a 0.1-s exposure (f -stop = 2) and a customized filter set (excitation, 605

nm; emission, 660 nm). The frozen blocks were sliced into serial sections, 20 μ m thick, and examined using a microscope equipped with a Texas Red filter set. Thereafter, the presence and distribution of plaques in the same sections were confirmed with immunohistochemical staining using a monoclonal A β antibody (BC05) (Wako Pure Chemical Industries, Ltd., Osaka, Japan).

■ ASSOCIATED CONTENT

📄 Supporting Information

Data for ^1H and ^{13}C NMR spectra and HPLC analyses of BAP-1. This material is available free of charge via the Internet at <http://pubs.acs.org>.

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Author Contributions

M.O. and H.S. designed all experiments. H.W. performed the synthetic chemistry work and in vitro and in vivo experiments. H.K. performed the synthetic chemistry work.

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Notes

The authors declare no competing financial interest.

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