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Longitudinal PET Imaging of Doxorubicin Induced Cell Death with ¹⁸F-Annexin V

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Abstract

Purpose—This study aims to apply longitudinal positron emission tomography (PET) imaging with ¹⁸F-Annexin V to visualize and evaluate cell death induced by doxorubicin in a human head and neck squamous cell cancer UM-SCC-22B tumor xenograft model.

Procedures—*In vitro* toxicity of doxorubicin to UM-SCC-22B cells was determined by a colorimetric assay. Recombinant human Annexin V protein was expressed and purified. The protein was labeled with fluorescein isothiocyanate (FITC) for fluorescence staining and ¹⁸F for PET imaging. Established UM-SCC-22B tumors in nude mice were treated with two doses of doxorubicin (10 mg/kg each dose) with 1 day interval. Longitudinal ¹⁸F-Annexin V PET was performed at 6 h, 24 h, 3 days, and 7 days after the treatment started. Following PET imaging, direct tissue biodistribution study was performed to confirm the accuracy of PET quantification.

Results—Two doses of doxorubicin effectively inhibited the growth of UM-SCC-22B tumors by inducing cell death including apoptosis. The cell death was clearly visualized by 18 F-Annexin V PET. The peak tumor uptake, which was observed at day 3 after treatment started, was significantly higher than that in the untreated tumors $(1.56 \pm 0.23 \text{ vs. } 0.89 \pm 0.31 \text{ %ID/g}, p < 0.05)$. Moreover, the tumor uptake could be blocked by co-injection of excess amount of unlabeled Annexin V protein. At day 7 after treatment, the tumor uptake of 18 F-Annexin had returned to baseline level.

Conclusions—¹⁸F-Annexin V PET imaging is sensitive enough to allow visualization of doxorubicin induced cell death in UM-SCC-22B xenograft model. The longitudinal imaging with ¹⁸F-Annexin will be helpful to monitor early response to chemotherapeutic anti-cancer drugs.

Keywords

¹⁸ F-Annexin V; doxorubicin; apoptosis; PET; chemotherapy	

Conflict of Interest

The authors declare they have no conflicts of interest.

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Introduction

Most of the chemotherapy agents, including the anthracycline antibiotic doxorubicin [1], cause tumor cell death primarily by induction of apoptosis [2]. Traditionally, apoptosis can be characterized in isolated cells by *in vitro* methods including DNA laddering and terminal deoxynucleotidyl transferase-mediated dUTP nick-end labeling (TUNEL) [3]. Histological methods play an important role in confirming apoptosis if tissue can be removed from the living system by biopsy or surgery. However, the selection bias and lack of ability to monitor the dynamic process of apoptosis limit the utility of such studies in clinical applications [4]. Therefore, there has been growing interest in the use of non-invasive functional and molecular imaging techniques to observe apoptosis [5].

As the cell undergoes apoptosis, there are a number of steps in the process that may be investigated using very different imaging modalities [6]. Among them, phosphatidylserine (PS) exposure occurs very early in the apoptotic chain of events, preceding such hallmark events as nuclear condensation and DNA laddering. Moreover, PS exposure is a near-universal event in apoptosis, and it presents a very abundant target (millions of binding sites per cell) that is readily accessible on the extracellular face of the plasma membrane [7].

Annexin V, an endogenous human protein with molecular weight of 36 kDa, has a high affinity ($k_d = 7 \text{ nM}$) for PS binding [8]. Due to the high affinity for apoptotic cells, no immunogenicity, and lack of *in vivo* toxicity, Annexin V is the dominant probe to detect and image apoptosis [9, 10]. Indeed, Annexin V has been labeled with 125 I, 123 I, 111 In and 99m Tc for single-photon emission computed tomography (SPECT) imaging [11, 12]. Clinical trials among patients with various tumor types demonstrated that Annexin V imaging is a promising technique to confirm the onset of apoptosis induced by chemotherapy and radiation therapy [13–15]. For example, 99m Tc-Annexin V scintigraphy applied to human tumors after the first course of chemotherapy showed increased tumor uptake proving that apoptosis had been initiated [16].

Compared with SPECT, positron emission tomography (PET) has the advantage that it is more sensitive and quantitative [17]. Annexin V has been labeled with positron emission radioisotopes including ¹²⁴I [18], ⁶⁸Ga [19] and ¹⁸F [20, 21] for PET imaging. It has been found that apoptosis induced by radiation therapy or chemotherapy could be distinguished with either *in vivo* imaging or *ex vivo* autoradiography [19, 20] using these agents. However, in most of the studies, only one time point imaging was performed. We hypothesized here that a longitudinal imaging at multiple time points would be helpful to reflect the dynamic nature of drug induced apoptosis.

In our previous study, we genetically engineered UM-SCC-22B human head and neck squamous cancer cells with a cyclic luciferase, an endogenous apoptosis marker. The apoptosis induced by Doxil was confirmed with multiple imaging strategies including bioluminescence imaging (BLI) and diffusion-weighted magnetic resonance imaging (DW-MRI) [22]. In this study, we applied longitudinal PET imaging to monitor the dynamics of cell death induced by doxorubicin using ¹⁸F-Annexin V as imaging agent.

Materials and Methods

Cell line and MTT assay

Human head and neck squamous cell line UM-SCC-22B was acquired from the University of Michigan [23] and cultured in Dulbecco's modified medium supplemented with 10% (v/v) heat-inactivated FBS, 100 unit/ml penicillin, and 100 μ g/ml streptomycin at 37°C in an atmosphere of 5% (v/v) CO₂.

The toxicity of doxorubicin to UM-SCC-22B cells was determined by a colorimetric assay with 3-(4, 5-dimethylthiazol-2-yl)-2, 5-diphenyl tetrazolium bromide (MTT; Sigma). All studies were performed with triplicate samples and repeated at least three times. Briefly, cells were harvested by trypsinization, resuspended in DMEM medium, and plated in a 96-well plate at 4,000 or 2,000 cells per well. After treatment with different doses of doxorubicin (ranging from 0.1 nM to 0.5 μ M) for 48 h, the culture medium was then replaced and 50 μ l of 1.0 mg/ml sterile filtered MTT was added to each well. The unreacted dye was removed after 4 h incubation and the insoluble formazan crystals were dissolved in 150 μ l of DMSO. The absorbance at 570 nm (reference wavelength: 630 nm) was measured with a Synergy II multimode microplate reader (BioTech Instruments, VT).

Purification and conjugation of Annexin V protein

Annexin V expressing plasmid was kindly provided by Dr. Seamus J. Martin (The Smurfit Institute, Trinity College, Dublin, Ireland) and Annexin V protein was expressed and purified according to the protocol previously reported [24]. Fluorescein isothiocyanate (FITC, Sigma-Aldrich) was dissolved in anhydrous DMSO immediately before use (3 μl at 10 mg/ml) and then added into Annexin V (500 μg) with a molar ratio of 5:1 in 500 μL borate buffer (20 mM, pH 8.5). The mixture was incubated and rotated at room temperature for 60 min for covalent conjugation. The unreacted dye molecules were removed by PD-10 column (GE Healthcare).

In vitro apoptotic staining

Cells were seed in 24 well plates and treated with doxorubicin (10 μ M) for 24 h. After rinsing twice with PBS, the cells were incubated with FITC-Annexin V for 15 min at room temperature. For blocking, 200 μ g/ml of unlabeled Annexin V was added 5 min before FITC-Annexin V was added. Then Hoechst 33342 was added to the solution and incubated for another 15 min at room temperature. The cells were rinsed three times and immediately observed with a fluorescence microscope (X81, Olympus).

Synthesis of radioactive materials

2-deoxy-2-[¹⁸F]fluoro-D-glucose (¹⁸F-FDG) was purchased from the Nuclear Pharmacy of Cardinal Health, and reconstituted with sterile saline. The average radiochemical purity of the product was 98.5% and specific activity was >1,000 Ci/mmol.

N-succinimidyl 4-¹⁸F-fluorobenzoate (¹⁸F-SFB) was synthesized with a modular system (Eckert & Ziegler Eurotope GmbH) as previously reported [25]. ¹⁸F-SFB was redissolved in 10 μl of acetonitrile and an Annexin V (100 μg) solution in 0.1 M NaHCO₃ buffer was added. The reaction was incubated at room temperature for 30 min. The reaction mixture was purified with a NAP-5 size exclusion column (GE Healthcare) according to the manufacture's procedure. The component was eluted with saline to give a fraction containing ¹⁸F-Annexin V after the void volume of about 0.75 ml. ¹⁸F-Annexin V was assayed by radio-TLC for the presence of small molecule impurities (R_f of ¹⁸F-SFB, 0.9; R_f of ¹⁸F-Annexin V, 0.09). The specific activity of ¹⁸F-Annexin V at the end of synthesis was 1.53 ± 0.66 mCi/nmol (n = 5).

Animal model and treatment plan

All animal studies were conducted in accordance with the principles and procedures outlined in the NRC Guide for the Care and Use of Laboratory Animals and were approved by the Institutional Animal Care and Use Committee (IACUC) of the Clinical Center, National Institutes of Health. The UM-SCC-22B tumor model was generated by subcutaneous injection of 5×10^6 cells into the right shoulder of female athymic nude mice (Harlan

Laboratories). Tumor size was monitored with digital caliper and tumor volume was calculated as $vol = ab^2/2$, where a is the longest diameter and b is the shortest diameter. Two weeks after inoculation, 10 mice each with a volume around 300 mm³ were randomized into two groups. One group (n = 5) received 2 doses of 10 mg/kg of doxorubicin (ALZA Corporation, USA) through intravenous administration with an interval of 1 day. The control group (n = 5) received PBS only. The acute liver apoptosis model was induced by tail vein injection of 10 mg/kg of cycloheximide (Sigma-Aldrich) [26]. Three hours later, PET scans were performed with 18 F-Annexin V.

PET imaging

At day 0, 6 hours, day 1, 3, and 7 after treatment initiation, PET scans were performed with the tumor-bearing mice using ¹⁸F-Annexin V. Each UM-SCC-22B tumor-bearing mouse, under isoflurane anesthesia, was injected via a tail vein with 3.7 MBq (100 μCi) of ¹⁸F-Annexin V. Ten-minute static scans were acquired at 0.5, 1 and 2 h after injection, respectively (n = 5/group). For blocking experiments, 500 µg of unlabeled Annexin V was coinjected with 3.7 MBq (100 µCi, around 3 µg) of ¹⁸F-Annexin V, and 10-min static PET images were acquired at 60 min after injection (n = 3) with a dedicated small animal Inveon PET scanner (Preclinical Solution, Siemens). For ¹⁸F-FDG scan, mice were maintained under isoflurane anesthesia during the injection, accumulation, and scanning periods and were fasted for 6 h before tracer injection. Body temperature was maintained before and during imaging using a thermostat controlled circulating warm water pad. The images were reconstructed using a two-dimensional ordered-subset expectation maximization (2D OSEM) algorithm without correction for attenuation or scattering. For each scan, regions of interest (ROIs) were drawn over the tumor and major organs using vendor software (ASI Pro 5.2.4.0) on decay-corrected whole-body coronal images. The radioactivity concentrations (accumulation) within the tumors, muscle, liver, and kidneys were obtained from mean pixel values within the multiple ROI volume and then converted to MBq/ml/min using the calibration factor determined for the Inveon PET system. These values were then divided by the administered activity to obtain (assuming a tissue density of 1 g/ml) an image-ROI-derived percent injected dose per gram (%ID/g).

Biodistribution study

Immediately after PET imaging, the tumor-bearing mice were sacrificed and dissected. Blood, tumor, major organs, and tissues were collected and wet-weighed. The radioactivity in the wet whole tissue was measured with a γ -counter (1480 Wizard 3 gamma counter, Perkin–Elmer). The results were expressed as percentage of injected dose per gram of tissue (%ID/g). Values were expressed as mean \pm SD for a group of four animals.

Histological staining

Tumor samples were collected and sectioned after the animals were sacrificed. DNA fragmentation was analyzed by terminal deoxynucleotidyl transferase mediated dUTP nick end labeling (TUNEL) assay using a commercial kit (Maxin-Bio) according to the manufacturer's protocol. For the staining of Ki-67, frozen tumor tissue slices were fixed with cold acetone for 20 min and dried in the air for 30 min at room temperature. After blocking with 1% bovine serum albumin for 30 min, slices were incubated with rabbit anti-mouse Ki-67 antibody (1:200; BD Biosciences) and then incubated with Dylight488-conjugated goat anti-rabbit secondary antibody (1:300; Jackson ImmunoResearch Laboratories). After being washed 3 times with PBS, the slices were mounted with 4'-6-diamidino-2-phenylindole (DAPI)-containing mounting medium and observed under an epifluorescence microscope (X81; Olympus). Each experiment was performed in pairs, and the pairs were then repeated twice.

Statistical analysis

The data were described as means \pm standard deviation. Student's t test was applied to compare the statistical difference among groups. P value < 0.05 was considered statistically significant.

Results

Doxorubicin treatment induces apoptosis

Consistent with our previous study, UM-SCC-22B cells are sensitive to doxorubicin treatment [22]. The IC $_{50}$ value of doxorubicin to the cells is 10 μ M after 24 h incubation (Fig. 1a). Doxorubicin also effectively inhibited the growth of the established UM-SCC-22B tumors in nude mice. After being treated with doxorubicin for 24 h, UM-SCC-22B cells were stained with FITC-Annexin V. The strong green fluorescence signal was identified on the cell membrane of the treated cells but not on the untreated cells (Fig. 1b), indicating doxorubicin treatment induced PS externalization. Besides, the fluorescent signal was effectively blocked by co-incubation with excess amount of unlabeled Annexin V. As shown in Fig.1c, at day 7 with two doses of 10 mg/kg of doxorubicin treatment, the tumor size in the treated group was significantly smaller than that in control group (p < 0.01). Some tumors in the treated group were completely cured. It has been demonstrated previously that the tumor growth inhibition was apoptosis related [22].

¹⁸F-Annexin V PET imaging

After radiolabeling of Annexin V protein with 18 F, we first applied the tracer in a well-established acute liver apoptosis model [21]. Three mice were injected with cycloheximide (10 mg/kg) to induce apoptosis in the liver before imaging. Three hours later, about 3.7 MBq of 18 F-Annexin V was administered via tail vein for PET imaging. As shown in Fig. 2, significantly higher uptake of 18 F-Annexin V was observed in the treated liver than in the liver of the untreated control animals. The liver of the control mice showed a tracer uptake of 5.51 ± 0.77 % ID/g while the liver of the treated mice showed a tracer uptake of 5.51 ± 0.77 % ID/g while the liver of the treated mice showed a tracer uptake of 23.66 ± 3.33 %ID/g (p < 0.001). A 4.29-fold increase was observed, which is consistent with previously reported data [27].

It is well-known that apoptosis is a dynamic process, especially in the tumor environment [6]. With the UM-SCC-22B model, we performed PET imaging at different time points following the initiation of treatment. PET images demonstrated that $^{18}\text{F-Annexin V}$ was excreted from both hepatic and renal urinary routes, reflected by both high liver and kidney accumulations of the radioactivity. As shown in Table 1, within 2 hrs, the kidney uptake was decreased from $19.2 \pm 10.2 \text{ %ID/g}$ to $2.57 \pm 0.32 \text{ %ID/g}$ and liver uptake from $10.4 \pm 3.50 \text{ %ID/g}$ to $2.43 \pm 0.49 \text{ % ID/g}$. Based on the major organs uptake and ratios of tumor/non-tumor, we selected 1 h time point for the quantification of longitudinal PET images.

The tumor uptake in the control group barely exceeded the background, primarily due to the high perfusion and permeability of the tumor vasculature. At baseline, the tumors showed a tracer uptake of 0.97 ± 0.23 % ID/g (day 0). After treatment with doxorubicin, the tumor uptake of $^{18}\text{F-Annexin V}$ increased with time. As early as 6 hr after therapy, a trend of increased tumor uptake was already observed in the treated group which failed to meet our requirement for statistical significance (p = 0.057). At day 3, the treated tumors showed a tracer uptake of 1.56 ± 0.23 % ID/g, which was significantly higher than control tumors (0.89 \pm 0.31 % ID/g. p < 0.05). At day 7 after treatment, the difference between the two groups disappeared (Fig. 3).

In order to confirm the specificity of tumor uptake of $^{18}\text{F-Annexin V}$, another set of mice were treated with doxorubicin with the same dose and time interval. At day 3 after treatment, animals underwent PET imaging using $^{18}\text{F-Annexin V}$ with or without a blocking dose of unlableled Annexin V (500 µg per mouse). The tumor uptake of $^{18}\text{F-Annexin V}$ was partially blocked with extra amount of unlabeled protein (1.98 \pm 0.26 vs. 1.41 \pm 0.54 % ID/g, p < 0.05) (Fig. 4a & b).

¹⁸F-FDG PET imaging

We also performed PET imaging using $^{18}\text{F-FDG}$ to evaluate tumor metabolism changes after doxorubicin treatment [28]. The tumors were clearly visualized on PET images and the uptake of $^{18}\text{F-FDG}$ of control tumors was 7.23 \pm 1.88 %ID/g (Fig. 4c & d). At day 3 after doxorubicin treatment, $^{18}\text{F-FDG}$ uptake decreased significantly to 5.26 \pm 0.46 %ID/g (p < 0.05).

Biodistribution of ¹⁸F-Annexin V

In order to further confirm the PET imaging quantification, the biodistribution of 18 F-Annexin V was evaluated in tumor-bearing nude mice immediately after PET imaging. As shown in Fig. 5, the tumor uptakes were 1.51 ± 0.21 , 2.26 ± 0.37 and 1.42 ± 0.25 % ID/g in the control, treated and blocked group, respectively. As shown on PET images, both liver and kidneys showed high radioactivity uptake. It is worth noting that the tracer uptake in spleen increased dramatically from 4.17 ± 1.53 % ID/g in the control group to 17.28 ± 3.45 % ID/g in the treatment group. After blocking, the spleen uptake decreased to 8.32 ± 1.90 % ID/g. At 1 hr after tracer injection, the radioactivity in blood circulation remained relative high, with % ID/g value around 3 in all groups.

Histological staining

At day 3 after treatment started, the treated tumors showed significant increased uptake of ¹⁸F-Annexin V, although the tumor size showed no apparent change. We collected tumor samples and performed Ki-67 staining to evaluate tumor proliferation and TUNEL staining to determine the DNA damage. As shown in Fig. 6a, in the control tumor sections, a relatively high percentage of cells were stained positively for Ki-67. Significantly reduced cell proliferation was observed in the doxorubicin treated tumor. A TUNEL assay is one of the traditional *in vitro* methods to characterize cell apoptosis, and TUNEL-positive nuclei confirm DNA fragmentation. Compared to the control group, the group that received 2 doses of doxorubicin treatment showed significantly more cell apoptosis (Fig. 6b).

Discussion

The early assessment of tumor response is of tremendous, but substantially unmet, need to assist oncologists to manage the quality of patient life versus intensive chemotherapy [29, 30]. Owing to high binding affinity with PS, Annexin V has been widely used as an imaging probe for non-invasive molecular imaging of apoptosis. However, an optimal imaging time frame following initiation of treatment still needs to be determined due to the dynamic nature of apoptosis. In this preclinical study with an established tumor apoptosis model, we determined the optimal imaging time point to reflect tumor early response of tumors to doxorubicin with longitudinal PET imaging using ¹⁸F-Annexin V.

Annexin V could be conjugated with an average of two mole equivalents of fluorobenzoate (FBA) without decreasing its affinity for red blood cells with exposed PS. However, an average conjugation of 7.7 decreased the binding by 3-fold [31]. In this study, we used ¹⁸F-SFB as the prosthetic group for Annexin V labeling and the average specific activity of ¹⁸F-

Annexin V was 1.53 ± 0.66 mCi/nmol (n=5). Thus, on average only one FB group was present on each Annexin V protein, which will not affect its binding affinity.

The treatment and imaging schedule was presented in Fig. 1B. We treated the UM-SCC-22B tumors with two doses of doxorubicin at one day interval and imaged the mice at day 0, 6 hr, day 1, 3 and 7 after treatment started. The results showed tumor uptake of ¹⁸F-Annexin V increased as early as at 6 hour after therapy and peaked at day 3. It is interesting to note that the tumor size showed no significant change at day 3 after therapy started, indicating the increase of ¹⁸F-Annexin V uptake in tumors precedes the size change. Moreover, the cell toxicity also has been confirmed by Ki-67 staining and TUNEL staining.

It has been pointed out that Annexin V uptake by tumor cells heavily depends on the exact time after the start of chemotherapy and there might be two peaks of Annexin V uptake. One occurs early within several hours and another probably appears in 24–72 hours after the treatment [32]. However, our data demonstrated that the cell death induced by doxorubicin occurred in a different pattern. It appears that cell death in doxorubicin treated UM-SCC-22B tumors occurs very soon after treatment begins and persists for several days. Tumor growth curves showed complete eradication of several tumors by day 7.

Using apoptosis reporter gene BLI imaging, we observed strong caspase 3 activity in Doxil treated tumors at day 5 after therapy initiation [22]. Thus, we speculate that at least in the current model, the ratio of apoptotic cells among the tumor kept increasing with time within the first several days. At day 7, the treated tumor showed decreased Annexin V uptake, partially due to the removal of the majority of apoptotic and necrotic cells. However, we cannot exclude the possibility that disruption of the tumor vasculature affected the delivery of the tracer to tumor region.

When untreated, even if the tumors grow to a size around 600 to 800 mm³, there is no apparent apoptosis or necrosis, which is confirmed by both optical and PET imaging [22] (Fig. 3). It is worthy of note that UM-SCC-22B tumors are highly vascularized with high permeability [33, 34]. Consequently, $^{18}\text{F-Annexin V}$ showed a tumor uptake of 1.04 ± 0.26 %ID/g in untreated tumors, which is mostly likely attributed to the non-specific accumulation of $^{18}\text{F-Annexin V}$. Thus, further studies will expand to more tumor models with various vascularization and receiving different therapeutic interventions.

Besides tumors, we found that the tracer uptake in spleen increased dramatically in treated group compared with that in the control group (17.28 ± 3.45 vs. 4.17 ± 1.53 % ID/g, p < 0.01), which reflected the toxicity of doxorubicin. Increased spleen and bone marrow uptake of Annexin V has been observed in a rat model treated with cyclophosphamide [35]. One possible explanation is that doxorubicin exerted toxic effect on bone marrow and hematopoietic progenitor cells. Consequently, damaged blood cells were captured by spleen. Specific binding of 18 F-Annexin V to those cells resulted in high radioactivity uptake in spleen. The spleen uptake could be blocked by an excess amount of unlabeled Annexin V protein, further confirming the specific binding of 18 F-Annexin V to apoptotic cells.

Decreased ¹⁸F-FDG uptake in tumor at day 3 after treatment reflected the decreased tumor metabolism and growth inhibition, which was confirmed by the tumor growth curve retrospectively (Fig. 1b). With a different drug and different tumor model, we have observed different ¹⁸F-FDG PET imaging results. For example, contrary to these results, we have observed that ¹⁸F-FDG uptake increased at day 3 after paclitaxel therapy in a MDA-MB-435 tumor model resulting from inflammation and white blood cell infiltration [28].

Conclusion

¹⁸F-Annexin V PET imaging allows sensitive visualization of cell death induced by doxorubicin treatment. The longitudinal imaging with ¹⁸F-Annexin will be helpful to monitor tumor response to chemotherapy at early stage when used alone or combined with other molecular imaging modalities.

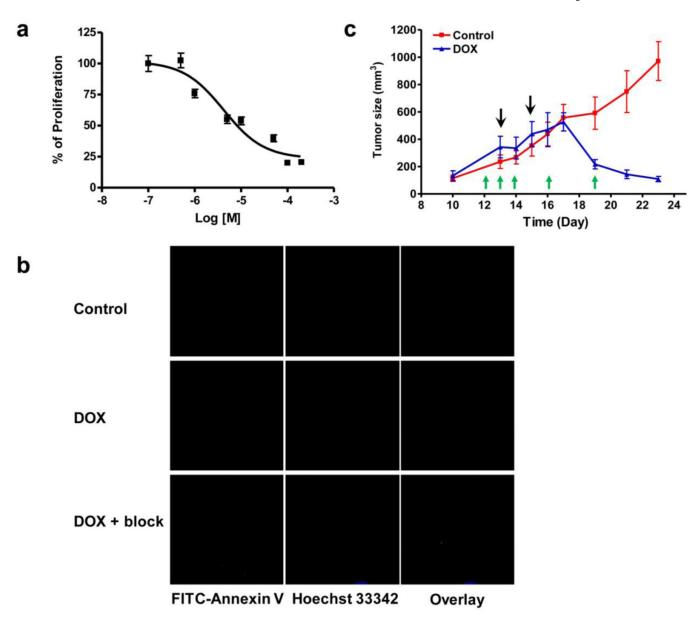
Acknowledgments

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Doxorubicin treatment induces apoptosis in UM-SCVC-22B cells ant tumors. **a** Cytotoxicty of doxorubicin on UM-SCC-22B cells determined by MTT assay. The IC₅₀ is determined as 10 μM after 24 hr incubation. **b** Fluorescence staining of UM-SCC-22B cells with FITC-Annexin V (green) after treatment with doxorubicin for 24 hr. The cells were co-stained with Hoechst 33342 (blue) for nuclei presentation. **c** The growth of UM-SCC-22B tumors was effectively inhibited by doxorubicin. The black arrows indicate the time for the two doses of doxorubicin (10 mg/kg for each dose). The green arrows indicate the time for PET imaging studies using ¹⁸F-Annexin V.

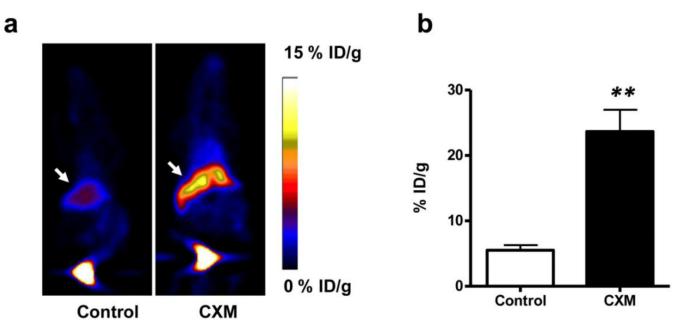
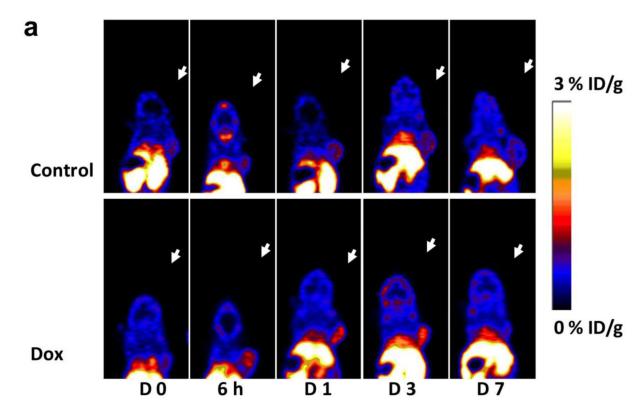


Fig. 2. Small animal PET imaging of liver apoptosis. **a** Typical decay-corrected whole-body coronal images are shown with liver indicated by white arrows. The acute liver apoptosis model was established by i.v. injection of cycloheximide (CXM, 10 mg/kg). **b** Liver uptake of ^{18}F -Annexin V was quantified from PET scans (n = 3). CXM treated mice show significantly higher liver uptake of ^{18}F -Annexin V than untreated mice (p < 0.001).



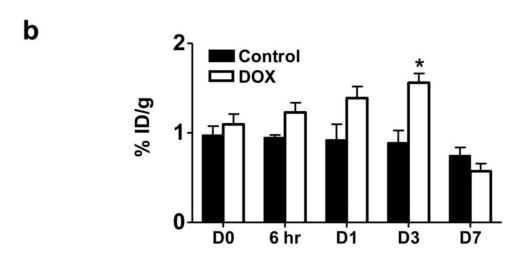


Fig. 3. $^{18}\text{F-Annexin V}$ PET imaging of UM-SCC-22B tumor bearing mice with or without doxorubicin treatment. **a** Representative decay corrected whole body coronal PET images at different time points after treatment started are shown. $^{18}\text{F-Annexin V}$ (3.7 MBq, 100 µCi) was injected via tail vein and ten-minute static scans were acquired at 1 h after injection. Tumors are indicated by arrows. **b** Tumor uptake of $^{18}\text{F-Annexin V}$ was quantified from PET scans (n=5). After doxorubicin treatment, tumor uptake increased to a peak at day 3 after treatment started (p < 0.05).

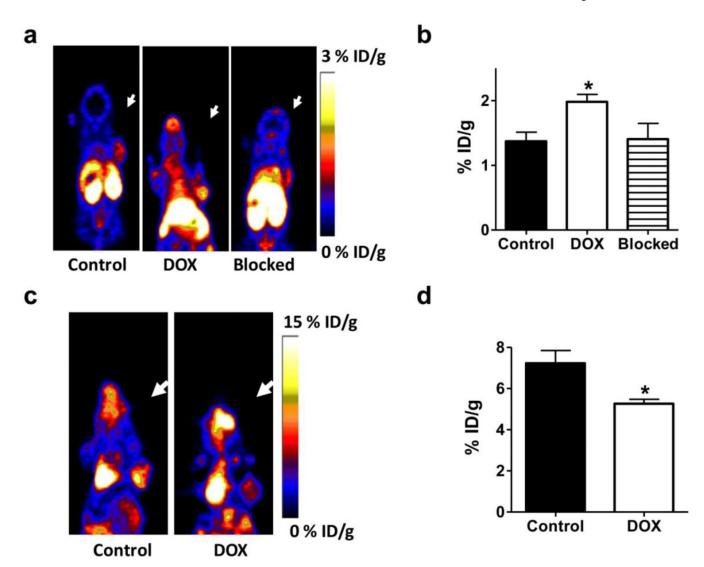


Fig. 4. a Representative decay corrected whole body coronal PET images at day 3 after treatment started. 18 F-Annexin V (3.7 MBq, $100 \,\mu\text{Ci}$, around 3 μg) was injected via tail vein and tenminute static scans were acquired at 1 h after injection (n=5). For blocking experiments, 500 μg of unlabeled Annexin V was coinjected with 3.7 MBq ($100 \,\mu\text{Ci}$) of 18 F-Annexin V (n = 3). Tumors were indicated with arrows. **b** Tumor uptake of 18 F-Annexin V was quantified by PET images. With excess unlabeled Annexin V, the tumor uptake of 18 F-Annexin V could be blocked (p < 0.05). **c** & **d** PET imaging of doxorubicin treated UM-SCC-22B tumor bearing mice at day 3 after treatment started using 18 F-FDG. The mice were maintained under isoflurane anesthesia during the injection, accumulation, and scanning periods and were fasted for 6 h before tracer injection. 18 F-FDG uptake in doxorubicin treated tumors was significantly lower than that in control tumors (n =5, p< 0.05).

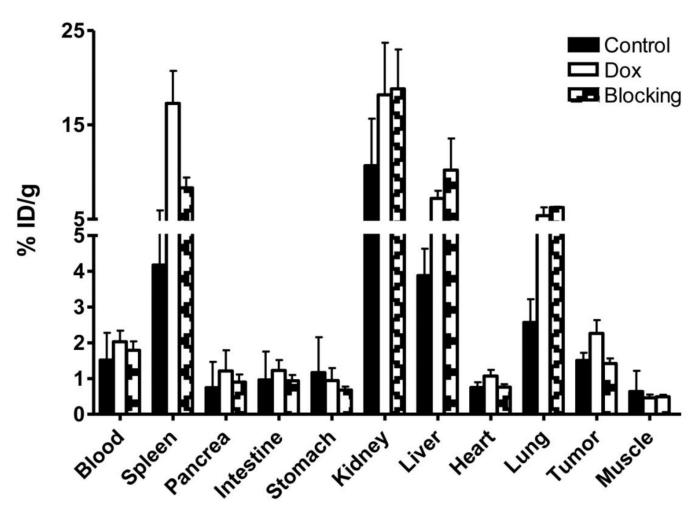


Fig. 5. Biodistribution of ¹⁸F-Annexin V at 1 hr after injection in UM-SCC-22B tumor bearing nude mice. The mice have been treated with 2 doses of doxorubicin with 10 mg/kg for each dose. At day 3 after treatment started, mice were injected intravenously with 3.7 MBq (100 μ Ci) of ¹⁸F-Annexin V alone (n=5) or with 500 μ g of unlabeled Annexin V (n=3). Data are presented as mean % ID/g \pm SD.

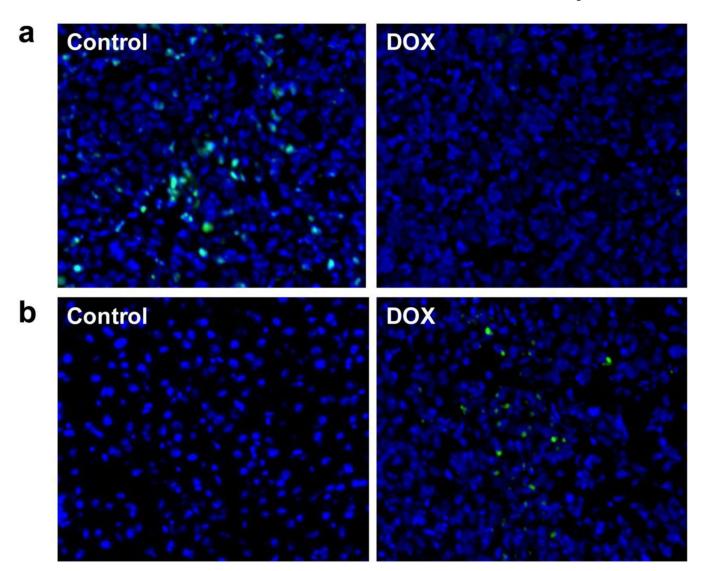


Fig. 6.
Histologic analyis of tumor response to doxorubicin. a Proliferation of UM-SCC-22B tumor cells at day 3 after doxorubicin treatment as assessed by Ki-67 immunofluorescence staining. Ki-67 are shown in green. Normal cell nuclei are shown in blue, stained by DAPI. b TUNEL staining of UM-SCC-22B tumor section after treatment with doxorubicin. Apoptotic nuclei are shown in green. Normal cell nuclei are shown in blue, stained by DAPI.

Table 1

Decay-corrected in vivo distribution of 18 F-Annexin V in UM-SCC-22B tumor bearing mice quantified by PET imaging (n = 9).

Organ	30 min	60 min	120 min
Kidneys	19.2 ± 10.2	7.57 ± 3.08	2.57 ± 0.32
Liver	10.4 ± 3.50	5.23 ± 2.37	2.43 ± 0.49
Blood*	2.98 ± 0.56	1.77 ± 0.46	0.85 ± 0.12
Tumor	1.52 ± 0.31	1.04 ± 0.26	0.59 ± 0.08
Muscle	0.69 ± 0.17	0.52 ± 0.24	0.23 ± 0.06
T/K	0.09 ± 0.03	0.15 ± 0.03	0.23 ± 0.04
T/L	0.15 ± 0.04	0.19 ± 0.01	0.25 ± 0.07
T/B	0.51 ± 0.08	0.59 ± 0.06	0.71 ± 0.14
T/M	2.27 ± 0.53	2.20 ± 0.67	2.76 ± 0.82

The results were presented as mean \pm SD (n = 9). Uptake is expressed in %ID/g tissue. Tumor/non-tumor ratios are unitless.

 $^{{}^*}$ Radioactivity in blood was determined by ROI over heart.

T, tumor; K, Kidneys; L, Liver; B, Blood; M, Muscle.