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Phototoxicity of Nano Titanium Dioxides in HaCaT Keratinocytes – Generation of Reactive Oxygen Species and Cell Damage

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Abstract

Nano-sized titanium dioxide (TiO₂) is among the top five widely used nanomaterials for various applications. In this study, we determine the phototoxicity of TiO₂ nanoparticles (nano-TiO₂) with different molecular sizes and crystal forms (anatase and rutile) in human skin keratinocytes under UVA irradiation. Our results show that all nano-TiO₂ particles caused phototoxicity, as determined by the MTS assay and by cell membrane damage measured by the lactate dehydrogenase (LDH) assay, both of which were UVA dose- and nano-TiO₂ dose- dependent. The smaller the particle size of nano-TiO₂ the higher the cell damage. The rutile form of nano-TiO₂ showed less phototoxicity than anatase nano-TiO₂. The level of photocytotoxicity and cell membrane damage is mainly dependent on the level of reactive oxygen species (ROS) production. Using polyunsaturated lipids in plasma membranes and human serum albumin as model targets, and employing electron spin resonance (ESR) oximetry and immuno-spin trapping as unique probing methods, we demonstrated that UVA irradiation of nano-TiO₂ can induce significant cell damage, mediated by lipid and protein peroxidation. These overall results suggest that nano-TiO₂ is phototoxic to human skin keratinocytes, and that this phototoxicity is mediated by ROS generated during UVA irradiation.

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Conflict of interest statement

The authors declare that there are no conflicts of interest.

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Keywords

TiO₂ nanoparticles; Phototoxicity; Reactive oxygen species (ROS); Lipid peroxidation; Human HaCaT keratinocytes; ESR; Oximetry; Immuno-spin trapping

Introduction

Nanomaterials have been recently developed that show great potential for use in the biomedical, optical, and electronic fields. They are currently manufactured on a large scale to be used in thousands of consumer goods and industrial products. However, nanomaterials are potentially toxic due to their unique properties including extremely high surface-to-volume ratios, which can make them very reactive or catalytic. Furthermore, the tiny size of nanomaterials makes it possible for them to pass through cell membranes and other biological barriers. Therefore, investigation of cellular toxicity and phototoxicity of nanomaterials is critically needed.

Nano-sized titanium dioxide (TiO₂) is among the top five nanomaterials widely used in paints, plastics, cosmetics, personal care products, and as food additives and drug delivery agents (Kangwansupamonkon *et al.*, 2009; Ray *et al.*, 2009). The usefulness of TiO₂ nanoparticles (nano-TiO₂) is primarily linked to two of its functions: absorbing and deflecting ultraviolet (UV) radiation and semiconductor photocatalysis (Fujishima *et al.*, 2000). Under UVA irradiation, electrons in the TiO₂ valence band absorb the photon energy and jump to the conduction band, leaving valence band holes that extract electrons from water or hydroxyl ions and generate hydroxyl radicals ([•]OH). Formation of other reactive oxygen species (ROS), including superoxide (O₂^{•-}) and singlet oxygen (¹O₂), by different mechanisms has also been reported (Hirakawa and Hirano, 2006; Daimon and Nosaka, 2007). The photocatalytic properties make TiO₂ nanoparticles successful candidates for degrading organic pollutants (Mura *et al.*, 1999) or killing microorganisms (Kangwansupamonkon *et al.*, 2009; Foster *et al.*, 2011). On the other hand, potential risks associated with exposure to nano-TiO₂ raise many concerns due to generation of ROS during UV irradiation; ROS are genotoxic or cytotoxic to organisms (Vevers and Jha, 2008; Ghosh *et al.*, 2010; Sycheva *et al.*, 2011).

Previous studies have suggested that nano-TiO₂ that has not been irradiated with UV has limited cytotoxicity (Rehn *et al.*, 2003). However, further reports have shown that TiO₂ particles without illumination affected cell-matrix adhesion, which is not associated with ROS damage to cells (Fujita *et al.*, 2009). Under UV irradiation, TiO₂ nanoparticles exhibit toxic effects to both normal tissue and cancer cells, such as human dermal and lung cells (Liao *et al.*, 2009), human keratinocyte cells (Shukla *et al.*, 2011; Simon *et al.*, 2011), rat lung alveolar macrophages (Afaq *et al.*, 1998), intestinal cells (Koenenman *et al.*, 2010) and HeLa cells (Cai *et al.*, 1992). The human skin and eye are of particular concern as target sites for phototoxic damage because these tissues are constantly exposed to direct daily ambient radiation. It was reported that although micron-sized TiO₂ cannot penetrate through the intact epidermal barrier (Kiss *et al.*, 2008), topical application of TiO₂ nanoparticles may induce dermal toxicity (Wu *et al.*, 2009). The photoreactivity of TiO₂ nanoparticles is largely dependent on their particle size, shape and crystal structure (Sharma, 2009; Liu *et al.*, 2010). It was demonstrated that smaller nano-TiO₂ particles tend to have higher phototoxicity, and anatase and amorphous forms of nano-TiO₂ show higher cytotoxicity than its rutile form (Xue *et al.*, 2010; Sanders *et al.*, 2011).

In the present studies, we have evaluated the phototoxicity of nano-TiO₂ with four different sizes (<25 nm, 31 nm, <100 nm, and 325 nm) and two crystal forms (anatase and rutile)

towards human skin keratinocytes under UVA irradiation. We observe that their differences in phototoxicity are highly correlated with the production of ROS. By employing polyunsaturated lipids in plasma membrane and human serum albumin (HSA) as model targets, our unique electron spin resonance (ESR) oximetry and immuno-spin trapping techniques indicate that UVA photoirradiation of nano-TiO₂ in biological systems can lead to significant cell damage.

Materials and methods

Chemicals

Nano-TiO₂ (A25, <25 nm anatase, catalog # 637254; A325, 325 mesh anatase, catalog # 248576; R100, <100 nm rutile, catalog # 637262), HSA, xanthine, superoxide dismutase (SOD), diethylenetriaminepentaacetic acid (DTPA), 2,2,6,6-tetramethyl-4-piperidone (TEMP) and dimethyl sulfoxide (DMSO, cell-culture grade) were all purchased from Sigma Chemical Co. (St. Louis, MO). Titanium dioxide (P25, 31 nm anatase/rutile, catalog # Aeroxide® TiO₂ P25) was from Degussa (Alpharetta, GA). Fetal bovine serum (FBS) was from Biofluids (Rockville, MD, USA). Dulbecco's modified Eagle's medium (DMEM), phosphate buffered saline (PBS, pH 7.4), trypsin-EDTA, penicillin, and streptomycin were purchased from Invitrogen Inc. (Grand Island, NY). The MTS assay kit (CellTiter 96® Aqueous) was purchased from Promega Co. (Madison, WI). ¹⁵N-labeled 4-oxo-2,2,6,6-tetramethylpiperidine-d16-1-oxyl (¹⁵N-PDT) was purchased from Cambridge Isotope Labs (Andover, MA). Xanthine oxidase (XOD) was from Roche Applied Science (Indianapolis, IN). The spin-trap 5-tert-butoxycarbonyl 5-methyl-1-pyrroline *N*-oxide (BMPO) was purchased from Applied Bioanalytical Labs (Sarasota, FL). Egg phosphatidylcholine was obtained from Avanti Polar Lipids, Inc. (Alabaster, AL). 5,5-dimethyl-1-pyrroline *N*-oxide (DMPO) was purchased from Dojindo laboratories (Japan).

Preparation of TiO₂ suspensions

The nano-TiO₂ suspensions were prepared by first dispersing the nanoparticles in ultrapure water using a sonicator for 30 min to produce a 10 mg/ml stock nano-TiO₂ suspension and then diluting according to the requirements of the experiments.

Characterization of nano-TiO₂

X-ray diffraction (XRD) patterns were recorded on a Philips XPert PRO MPD X-ray diffractometer (Philips, Eindhoven, The Netherlands) operated at 35 kV and 45 mA with Cu-K α radiation. Scanning Electron Microscope (SEM) images were taken on a Hitachi S4800 field scanning electron microscope (FESEM, Japan) operating at 10 kV. Samples were suspended in ethanol solution by sonication first. Approximately 10 μ l of suspensions were spin-coated on a silicon wafer at 3000 rpm for 60 seconds. Dynamic light scattering (DLS) measurements of particle size were carried out using a light scattering Zetasizer Nano-S90 light scattering instrument (Malvern Instruments, Enigma Business Park, UK).

Cell culture and phototoxicity measurement

Human HaCaT keratinocytes, a transformed epidermal human cell line (Boukamp *et al.*, 1988), were grown to ~95% confluence in 96-well plates at 37°C in DMEM containing 10% FBS under 95% air/5% CO₂. For phototoxicity tests, cells were exposed in the dark for 4 h at 37 °C to different TiO₂s (50 and 100 μ g/ml) in DMEM (FBS free). Control cells were treated with DMEM alone. After incubation the medium was removed and replaced by sterile PBS containing 10 mM glucose. Cells were then irradiated with UVA from four fluorescent PUVA lamps (Houvalite F20T12BL-HO; National Biological Co. Twinsburg, OH). The maximum emission of the UVA light lamps was determined to be between 320–

390 nm. The light intensities at wavelengths below 315 nm (UVB light) and above 400 nm (visible light) are approximately two orders of magnitude lower than the maximum in the 320–390 nm spectral region (Zhao *et al.*, 2010). The UVA exposure doses were 0, 2.5, 5.0, and 10 J/cm² respectively, as measured with an YSI-Kettering Model 65A Radiometer (Yellow Springs Instrument Co., Yellow Springs, OH). After exposure the PBS/glucose solution was removed and replaced with DMEM containing 2% FBS and the cells were kept in the incubator overnight. Aliquots (10 μ l) were removed and LDH release into the medium was assayed using the Cytotox 96 kit (Promega Corp., Madison, WI) according to the manufacturer's directions. The remaining medium was removed and the cells were washed with PBS and replaced with 100 μ l/well of PBS/glucose containing the MTS reagent (CellTiter 96 Aqueous Proliferation Assay; Promega Cop.). After incubation for 2 h at 37 $^{\circ}$ C, the absorbance at 492 nm was recorded using a microplate reader (Spectrafluor Plus, Tecan US, RTP, NC).

ESR spectroscopy

Conventional ESR spectra were obtained with a Bruker EMX ESR Spectrometer (Billerica, MA). All spin trapping ESR measurements were carried out using the following settings for detection of the spin adduct between BMPO and O₂^{•-} (BMPO-OH): 10 mW microwave power, 100 G scan range and 1 G field modulation. All measurements were performed in replicates at ambient temperature. A light system consisting of a Xenon lamp coupled with a Schoeffel monochromator was used to generate UV light at 340 nm wavelength. All the samples for ESR measurements were freshly prepared in 100 mM phosphate buffer at pH 7.4. The buffer was treated with Chelex-100 resin for 24 h to remove traces of transition metal ions.

Spin label oximetry

ESR oximetry measurement is based on the bimolecular collision of molecular oxygen with a spin label which is a stable free radical. Collision of the spin label with O₂ produces a spin exchange, resulting in shorter relaxation times and ESR signals with broader linewidths and decreasing peak height. Thus, oxygen consumption by such mechanisms as lipid peroxidation results in decreased line widths and increased peak height for the spin probe. The oximetry method determines the oxygen concentration by measuring the hyperfine structural changes at the low field line of the ESR spectrum using ¹⁵N-PDT as the spin label (Halpern *et al.*, 1994; Swartz and Clarkson, 1998; Xia *et al.*, 2007; Yin *et al.*, 2008; Yin *et al.*, 2009). During lipid peroxidation, the levels of dissolved O₂ vary, with a time dependent decrease in linewidth and an increase in the peak intensity of the ESR signal indicating continuous O₂ consumption. The value of oxygen concentration was obtained from a calibrated curve of the ESR linewidth versus the oxygen concentration.

Liposomes were prepared as previously described (Kusumi *et al.*, 1986). Briefly, a suspension of 30 mg/ml egg PC liposomes and 0.1mM ¹⁵N-PDT with or without TiO₂ was added to a quartz capillary tube. The lipid peroxidation was initiated by UV (340 nm) irradiation. The ESR spectra were then recorded at 4 min intervals for 16 min. Signals were obtained with a 0.05 G scanning width, 0.5 mW incident microwave power and with 100 kHz field modulation. All ESR spectra were recorded at the low field line of ¹⁵N-PDT and at ambient temperature.

ELISA and Western Blot

HSA protein samples were typically prepared by treating 600 μ M HSA with 0.1 mg/ml TiO₂, and 50 mM DMPO in 100 mM phosphate buffer (Chelex-treated with 25 μ M DTPA) at pH 7.4 in a 6-well plate in the absence or presence of UVA irradiation (10 J/cm²). After treatment, samples were frozen at -80 $^{\circ}$ C for further experiments.

The ELISA assay to measure DMPO nitron adducts was performed essentially as described by Ehrenshaft and Mason (Ehrenshaft and Mason, 2006) with minor modifications. Two microgram aliquots of protein diluted in bicarbonate buffer, pH 9.4, were allowed to adsorb to the wells of a 96-well microtiter plate (Grenier Labortechnik) for 1.5 h. After washing once with wash buffer (1×PBS with 0.1% tween), the microtiter plate was incubated for 1 h in a 1:5000 dilution of rabbit polyclonal anti-DMPO antiserum, washed 4 times with wash buffer, incubated for 1 h more in a 1:5000 dilution of an alkaline phosphatase anti-rabbit secondary antibody, again washed 4 times with wash buffer, and finally washed once with 1×TBS, pH 9.6. After addition of CDP-Star (25 μM) (Roche Laboratories), the chemiluminescent product was detected using a microplate reader (Spectrafluor Plus, Tecan US, RTP, NC).

For Western Blot analysis, 10 μg of HSA protein from each reaction were electrophoresed under reducing conditions through a 4–12% BisTris NuPAGE acrylamide gel (Invitrogen) followed by electroblotting to a nitrocellulose membrane. Western Blot analysis was then performed as described (Ehrenshaft and Mason, 2006) except that DMPO-containing proteins were visualized using the Odyssey infrared imaging system (Licor).

Results

Characterization of nano-TiO₂

The XRD results shown in Fig. 1A reveal the crystal structure of nano-TiO₂ samples, which are consistent with the crystallinity provided by the vendors. The crystalline composition of P25 was evaluated to be around 86% anatase and 14% rutile by the ratios of the integral areas of the three main diffraction peaks of the two phases (Zhao *et al.*, 2008). SEM was used to visualize the particle size and shape of nano-TiO₂. The SEM images of four nano-TiO₂ samples are shown in Fig. 1B. The sizes are roughly consistent with the sizes claimed by the vendors. From the SEM images we also find that aggregates or big clusters are formed for all samples, especially for the smallest A25 sample. DLS measurements show the size and distribution of TiO₂ aggregates in the aqueous medium, which are largely dependent on the concentration, dispersant, and primary particle size (Sanders *et al.*, 2011). As shown in Fig. 1C, aggregates of the smallest A25 sample were between 150–500 nm and the other three were between roughly 250–700 nm at the lower concentration (50 μg/mL) tested in the phototoxicity experiments.

Nano-TiO₂-induced phototoxicity in human HaCaT keratinocytes

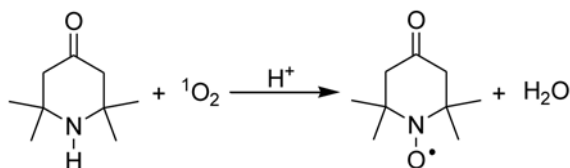
The phototoxicity of the four different sizes of nano-TiO₂ towards HaCaT keratinocytes was determined using two different assays. The MTS assay measures the activity of (mainly mitochondrial) dehydrogenases, while cell membrane damage is measured by the release of cytosolic LDH. As measured by the MTS assay, no decrease in viability was observed when HaCaT cells were exposed to TiO₂ samples or to UVA alone (Fig. 2A and 2B). However, in the presence of UVA radiation, two anatase TiO₂ samples (A325 and A25) and P25 TiO₂ caused UVA dose- and concentration-dependent damage to HaCaT cells. The rutile TiO₂ sample (R100) showed much less phototoxicity towards HaCaT cells even at a high concentration of 100 μg/ml and 10 J/cm² UVA exposure (Fig. 2B). The extent of photocytotoxicity to cells irradiated at 7.5 or 10 J/cm² was in the following order: P25>A25>A325>R100. A similar result was seen with the LDH release assay (Fig. 3A and 3B).

ESR measurement of ROS generation

ESR spin trap spectroscopy was employed to determine whether or not nano-TiO₂ under UVA light irradiation has the capability to generate ROS chemically. Generation of

hydroxyl radicals was detected by the ESR spin trapping technique using BMPO. BMPO is a newly developed spin trap offering more advantages over the existing spin traps, such as greater stability and sensitivity (Zhao *et al.*, 2001). The BMPO/ \cdot OH adduct has an ESR signal pattern similar to that of DMPO/ \cdot OH, which exhibits a characteristic set of four lines (1:2:2:1) in its ESR spectrum. In the absence of UVA irradiation, the ESR signal of the hydroxyl radical spin adduct was not detectable from the mixture of BMPO and nano-TiO₂ (data not shown). No such ESR profile was generated when BMPO was irradiated under UVA light (340 nm) in the absence of nano-TiO₂ (Fig. 4A) or in the presence of the rutile R100 TiO₂ sample (Fig. 4B). However, UVA irradiation of BMPO in the presence of A325 nano-TiO₂, A25 nano-TiO₂, or P25 nano-TiO₂ all produced the characteristic ESR profile (Fig. 4C, 4D, and 4E). As shown in Fig. 4, UVA irradiation of P25 nano-TiO₂ resulted in the strongest signal of BMPO/ \cdot OH signal (Fig. 4E), followed by two anatase TiO₂ samples, A325 nano-TiO₂ and A25 nano-TiO₂ (Fig. 4C and 4D). This signal was largely inhibited by the addition of 20% DMSO (Fig. 4F), further confirming the generation of OH radicals during the UVA irradiation.

We tested the generation of singlet oxygen by the ESR trapping technique using TEMP. It has been previously reported that 4-oxo-2,2,6,6-tetramethylpiperidine-N-oxyl (TEMPONE), a nitroxide radical detectable by EPR spectra, is generated from TEMP and singlet oxygen (Eq. 1) (Lion *et al.*, 1976).



(1)

Irradiation of different nano-TiO₂ samples (0.1 mg/ml) containing 20 mM TEMP resulted in ESR spectra of three lines with equal intensities ($a_N = 16.0$ G), typical of nitroxide radicals (Fig. 5, inset). The hyperfine splitting constant and g factor of the photosensitized oxidation product of TEMP were identical to those of commercial TEMPONE. Fig. 5 shows the ESR intensity of the TEMPONE signal as a function of time during irradiation of different nano-TiO₂ samples. The P25 nano-TiO₂ solution (Fig. 5, curve A) showed the rate that increased the fastest, followed by the A25 nano-TiO₂ sample (Fig. 5, curve B). The rates of production of singlet oxygen were much slower for A325 nano-TiO₂ and R100 nano-TiO₂ (Fig. 5, curves C and D). A control solution with TEMP only (data not shown) indicated no ESR signal increase. For P25 nano-TiO₂, addition of a singlet oxygen quencher, NaN₃, caused a substantial decrease in the rate of increase of the EPR signal (Fig. 5, curve E).

It has been reported that $\text{O}_2^{\cdot-}$ can be oxidized to ${}^1\text{O}_2$ during TiO₂ photocatalytic reactions (Lipovsky *et al.*, 2012). Superoxide ($\text{O}_2^{\cdot-}$) undergoes dismutation to produce H_2O_2 , from which the \cdot OH radical can also be formed through the Fenton reaction. To further elucidate the mechanisms of \cdot OH and ${}^1\text{O}_2$ generation, we studied the effect of SOD on the production of \cdot OH and ${}^1\text{O}_2$ by P25 nano-TiO₂ during UVA irradiation. As a control study, addition of 1.25 U/ml SOD significantly inhibited the production of $\text{O}_2^{\cdot-}$ generated in a Xanthine system (Fig. 6A and 6B). However, no obvious effect was observed on \cdot OH generation by P25 nano-TiO₂ under UVA irradiation even at a high concentration of SOD (6 U/ml, Fig. 6C and 6D), indicating that nano-TiO₂-generated \cdot OH radicals were not evolved from $\text{O}_2^{\cdot-}$, at least for the most part. In contrast, the ${}^1\text{O}_2$ generation was markedly reduced in the presence of 1.25 U/ml SOD (Fig. 6E and 6F), confirming that $\text{O}_2^{\cdot-}$ may be a main pathway

in UVA-induced $^1\text{O}_2$ generation by nano-TiO₂ (Lipovsky *et al.*, 2012). It is noteworthy that although $\text{O}_2^{\bullet-}$ was formed from UVA irradiation of nano-TiO₂ and was attributed to the formation of $^1\text{O}_2$, no obvious $\text{O}_2^{\bullet-}$ production was detected in our ESR study using BMPO as a trapping agent (Fig. 4), which is actually consistent with a previous report (Konaka *et al.*, 2001). Its short lifetime under our experimental conditions warrants further investigation.

ESR oximetry measurement of lipid peroxidation

It is well known that ROS can produce a time-dependent peroxidation of the polyunsaturated lipids in plasma membrane. In this study, lipid peroxidation produced by UVA irradiation of different nano-TiO₂ was assessed using ESR oximetry recorded at 4-min intervals for 16 min. The consumption of oxygen accompanying lipid peroxidation was measured as a time-dependent narrowing of the ESR signal for the spin probe ^{15}N -PDT. As shown in Fig. 7, narrowing of the ESR signal was necessarily accompanied by an increase in the peak height of the ESR signal within the scan range. The results of lipid peroxidation produced by different nano-TiO₂ samples (R100, A325, A25, and P25) after UVA irradiation are shown in Fig. 7B–7E, respectively. The final ESR signal intensities of R100 nano-TiO₂ (Fig. 7B), A325 nano-TiO₂ (Fig. 7C), A25 nano-TiO₂ (Fig. 7D), and P25 nano-TiO₂ (Fig. 7E) were approximately 7.5, 11.7, 16.2, and 26.3% higher than in the control (Fig. 7A). The progressive increases in peak-to-peak signal intensity (and accompanying progressive narrowing of line width) in each panel were due to time-dependent oxygen consumption resulting from lipid peroxidation. Fig. 6F presents the data as a decrease in oxygen concentration, reflecting the variations in the slope (oxygen concentration versus time) with different nano-TiO₂, which decreases in the order of P25 > A25 > A325 > R100.

Immuno-spin trapping measurement of protein radicals

To further characterize the ability of ROS to oxidize target proteins, the most abundant plasma protein (human serum albumin, HSA) was incubated with DMPO and different nano-TiO₂ samples with and without UVA irradiation. The reaction products were analyzed by ELISA and Western blotting using an anti-DMPO polyclonal antibody. Immunochemical detection of HSA-DMPO nitron adducts was performed according to our previous studies (Ranguelova *et al.*, 2010). As measured by both ELISA and Western blotting, HSA with DMPO exposed to different nano-TiO₂ samples or UVA alone produced nitron adducts at background levels (Fig. 8A–8E). While in the presence of UVA irradiation, P25 nano-TiO₂ resulted in a significant increase in HSA-DMPO-derived nitron adducts (Fig. 8I). The other three nano-TiO₂ samples caused modest increases in adduct formation (Fig. 8F–8H). The order of the extent of nitron adducts is the same as for photocytotoxicity, hydroxyl radical, singlet oxygen, and lipid peroxidation measurements.

Discussion

TiO₂ is regarded as an inert and non-toxic substance by many regulatory bodies; e.g., the FDA approved TiO₂ as a food color additive in 1996, and the Material Safety Data Sheets (MSDS) indicate that there are no exposure hazards to the health of occupational workers and public health. However, there have been several studies that have shown that TiO₂ is a potential carcinogen and photocatalyst in biological tissues (Burnett and Wang, 2011). The cytotoxicity and/or phototoxicity of nano-TiO₂ is still debated. Also, there is uncertainty about whether the properties of nano-TiO₂ differ with its particular form and size. Human skin and ocular tissues are most affected by ambient radiation. In vitro studies have shown that when irradiated, the smallest form of TiO₂, anatase (<25 nm), is phototoxic to human retinal cells (Sanders *et al.*, 2011). UV-induced production of ROS and the resultant oxidative stress exposure plays an important role in photocarcinogenesis caused by UV

irradiation. ROS are believed to be involved in many inflammatory skin disorders, skin cancer formation, and skin aging (He *et al.*, 2005). Thus we report here a study of the photocytotoxicity and phototoxicity of nano-TiO₂ towards human HaCaT keratinocytes.

Our results show that all nano-TiO₂ tested in this paper caused UVA and nano-TiO₂ dose-dependent phototoxicity in HaCaT cells. As expected, smaller particles resulted in higher phototoxicity than larger particles. Rutile nano-TiO₂ showed less phototoxicity than anatase nano-TiO₂. Moreover, small mixed anatase/rutile nano-TiO₂ (P25) showed the highest phototoxicity, which is consistent with previous reported results (Hurum *et al.*, 2003). The cellular toxicity of nano-TiO₂ mainly depends on its ROS generation under UVA irradiation. Using ESR and spin trapping technique, a “gold standard” and state-of-the-art tool for detecting and quantifying ROS, we confirmed the generation of hydroxyl radicals and singlet oxygen. ROS generation by these four nano-TiO₂ particles is consistent with the phototoxicity studies, further confirming our hypothesis that ROS production was probably involved in the phototoxic mechanism.

In addition to measurement of ROS generation with ESR, we explored two other assays to further characterize the phototoxicity of nano-TiO₂. ROS are known to produce a time-dependent peroxidation of the polyunsaturated lipids in plasma membrane (Yin *et al.*, 2008; Yin *et al.*, 2009) as well as peroxidation of lipids and proteins inside the cells (Girotti, 1998). To mimic oxidation reactions with substrates in biological systems, we used polyunsaturated lipids in plasma membranes and human serum albumin as model targets for ROS. Using innovative ESR oximetry and immune-spin trapping techniques, we easily detected ROS-induced peroxidation, which was found to be in agreement with the ESR-detected ROS production. These results indicate that both methods are useful for qualitative screening of the phototoxicity of nano-TiO₂.

Based on the results reported in this study, we propose the mechanism shown in Fig. 9. UVA irradiation results in electron-hole pairs in nano-TiO₂. The photoexcited nano-TiO₂ serves as the initiating species to transfer energy to molecular oxygen and generate singlet oxygen (¹O₂) or to extract electrons from water or hydroxyl ions to generate hydroxyl radicals ([•]OH). Our experimental results also indicate that part of the ¹O₂ formation proceeds via a superoxide-dependent mechanism, whereas the OH formation is not via superoxide (Fig. 6). It is well established that in the presence of a lipid or protein, the generated ROS can initiate lipid and/or protein peroxidation. Both ROS and lipid peroxidation are associated with aging-related diseases, including cancer (Aust *et al.*, 1993; Xia *et al.*, 2007).

In conclusion, the studies presented here give an overall *in vitro* assessment of the phototoxicity by various nano-TiO₂ particles towards HaCaT cells under UVA irradiation. This phototoxic damage was apparently mediated by production of ROS by photo-activated nano-TiO₂. According to our results ROS are generated by UVA irradiation of nano-TiO₂ with anatase and/or mixed anatase/rutile forms. Moreover, the phototoxicity of nano-TiO₂ was less with larger particle size and surface areas, indicating that coarse particles of nano-TiO₂ may consistently produce less ROS.

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Abbreviations

¹⁵N-PDT	4-Oxo-2,2,6,6-tetramethylpiperidine-d16-1-oxyl
BMPO	5-tert-butoxycarbonyl 5-methyl-1-pyrroline <i>N</i> -oxide
DLS	dynamic light scattering
DMEM	Dulbecco's modified Eagle's medium
DMPO	5,5-dimethyl-1-pyrroline <i>N</i> -oxide
DMSO	dimethyl sulfoxide
ESR	electron spin resonance
FBS	fetal bovine serum
DTPA	diethylenetriaminepentaacetic acid
HSA	human serum albumin
LDH	lactate dehydrogenase
MTS	3-(4,5-dimethylthiazol-2-yl)-5-(3-carboxymethoxyphenyl)-2-(4-sulfophenyl)-2H-tetrazolium
PBS	phosphate buffered saline
ROS	reactive oxygen species
SEM	scanning electron microscopy
SOD	superoxide dismutase
TEMP	2,2,6,6-tetramethyl-4-piperidone
UVA	ultraviolet A (315-400 nm)
XOD	xanthine oxidase
XRD	X-ray diffraction

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Highlights

- We evaluate the phototoxicity of nano-TiO₂ with different sizes and crystal forms.
- The smaller the particle size of nano-TiO₂ the higher the cell damage.
- The rutile form of nano-TiO₂ showed less phototoxicity than anatase nano-TiO₂.
- ESR oximetry and immuno-spin trapping techniques confirm UVA-induced cell damage.
- Phototoxicity is mediated by ROS generated during UVA irradiation of nano-TiO₂.

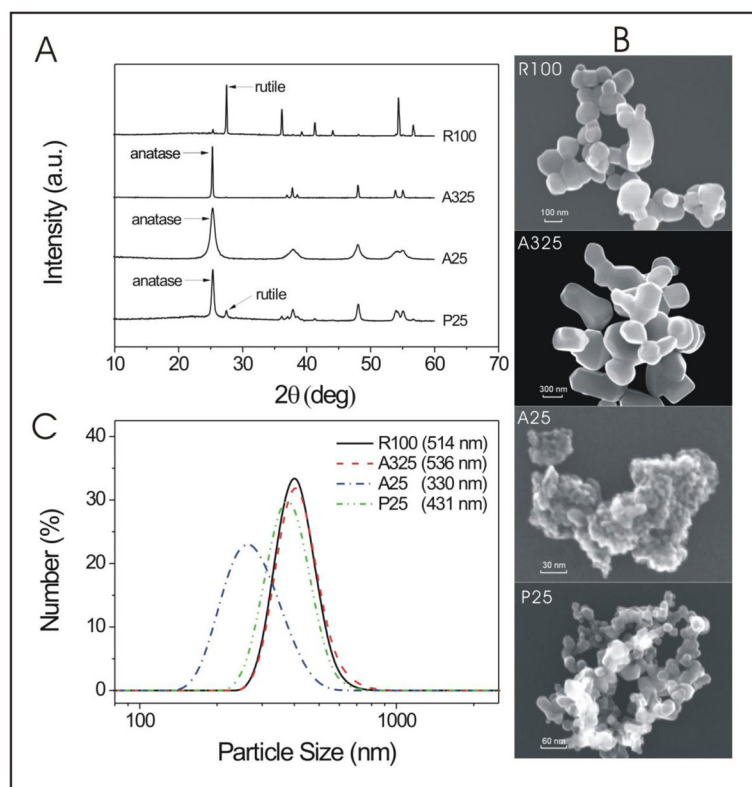


Figure 1. Characterization of Nano-TiO₂ samples. (A) XRD patterns of various TiO₂ samples; (B) SEM images of various TiO₂ samples; (C) DLS determination of particle size and distribution of 50 µg/ml nano-TiO₂ samples in DMEM medium (FBS free).

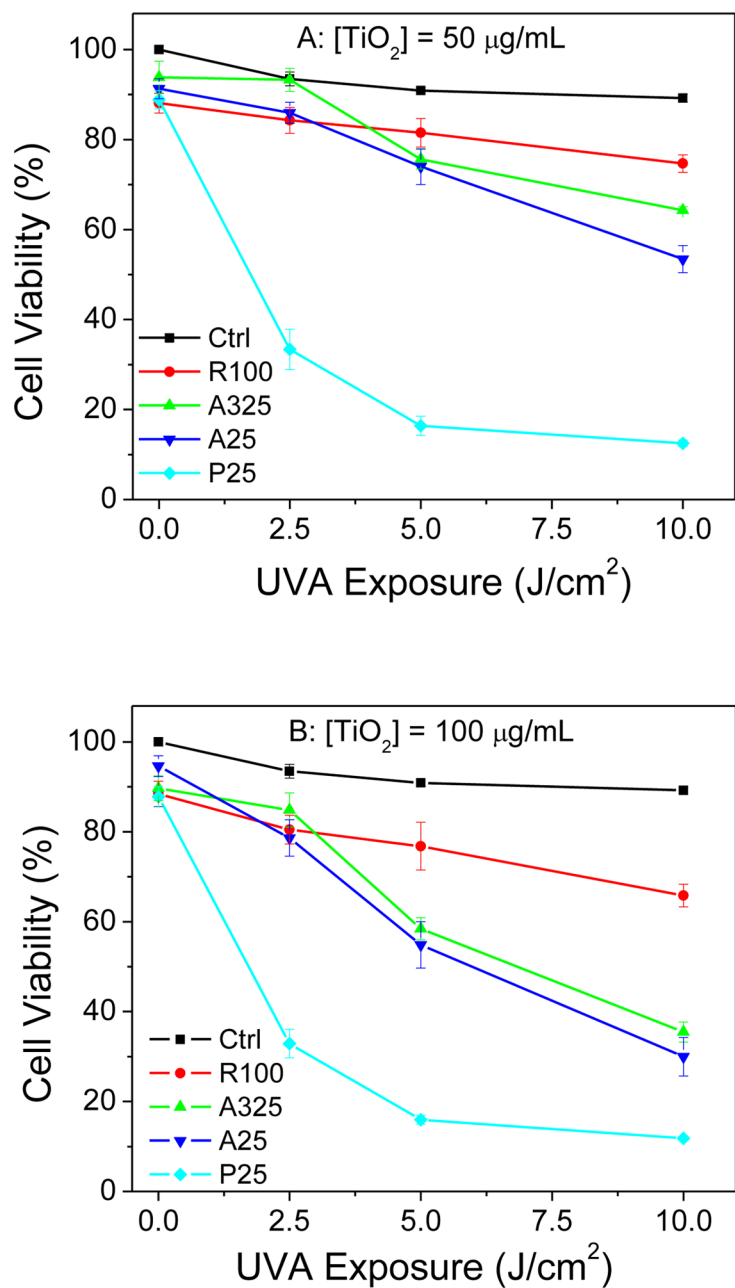


Figure 2. Effect of exposure to different TiO₂ samples on the metabolic activity of HaCaT cells at concentrations of (A) 50 µg/ml and (B) 100 µg/ml as a function of UVA irradiation dosage, as measured by the MTS assay. Values are the means ± SE (n = 4).

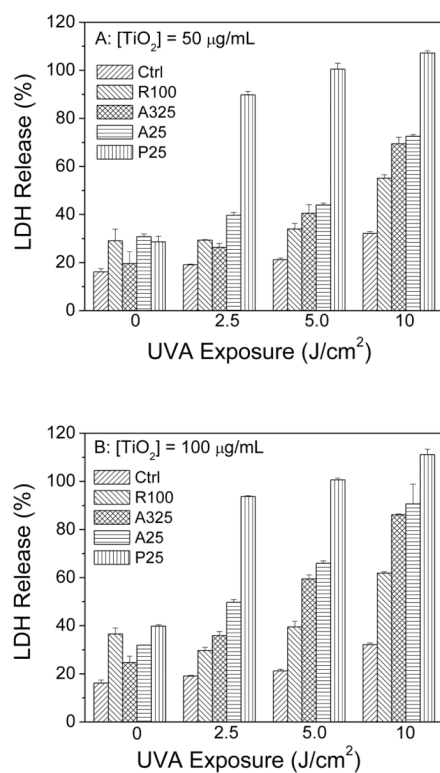


Figure 3. Effect of exposure to different TiO₂ samples on the metabolic activity of HaCaT cells at concentrations of (A) 50 µg/ml and (B) 100 µg/ml as a function of UVA irradiation dosage, as measured by the LDH assay. Values are the means ± SE (n = 4).

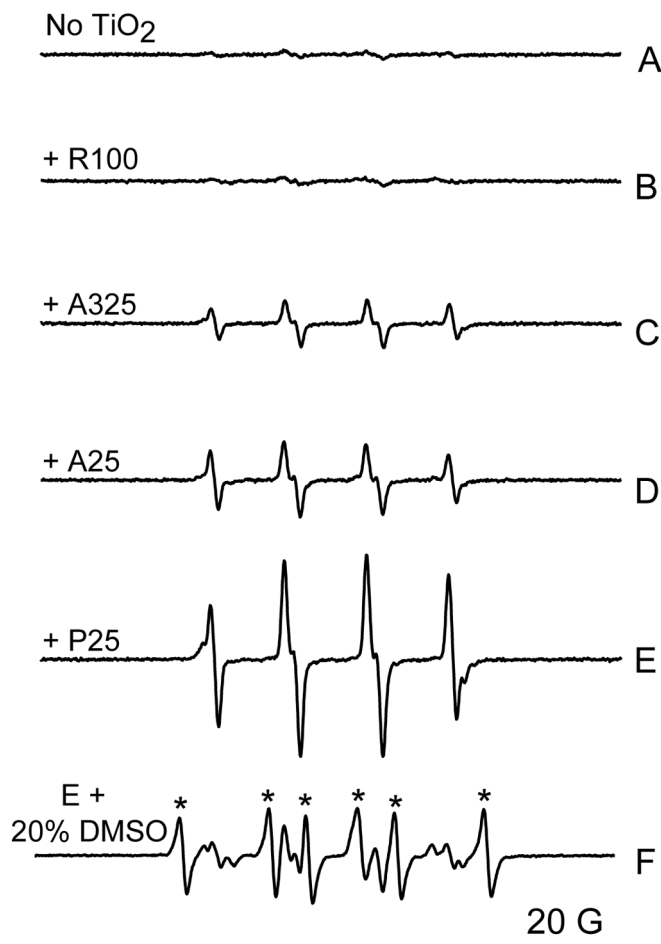


Figure 4.

Generation of hydroxyl radical from photoirradiation of TiO_2 samples under UVA light (340 nm). ESR spectra were recorded at room temperature 2 min after the UV light was turned on. Samples containing 25 mM BMPO and (A) without TiO_2 ; (B) with 0.1 mg/ml R100; (C) 0.1 mg/ml A325; (D) 0.1 mg/ml A25; (E) 0.1 mg/ml P25 and (F) same as E, but with the addition of 20% DMSO. Stars (*) indicate the ESR signal of the BMPO/ CH_3 adduct. Instrumental settings: microwave power, 10 mW; modulation frequency, 100 kHz; modulation amplitude, 1 G; scan range, 100 G.

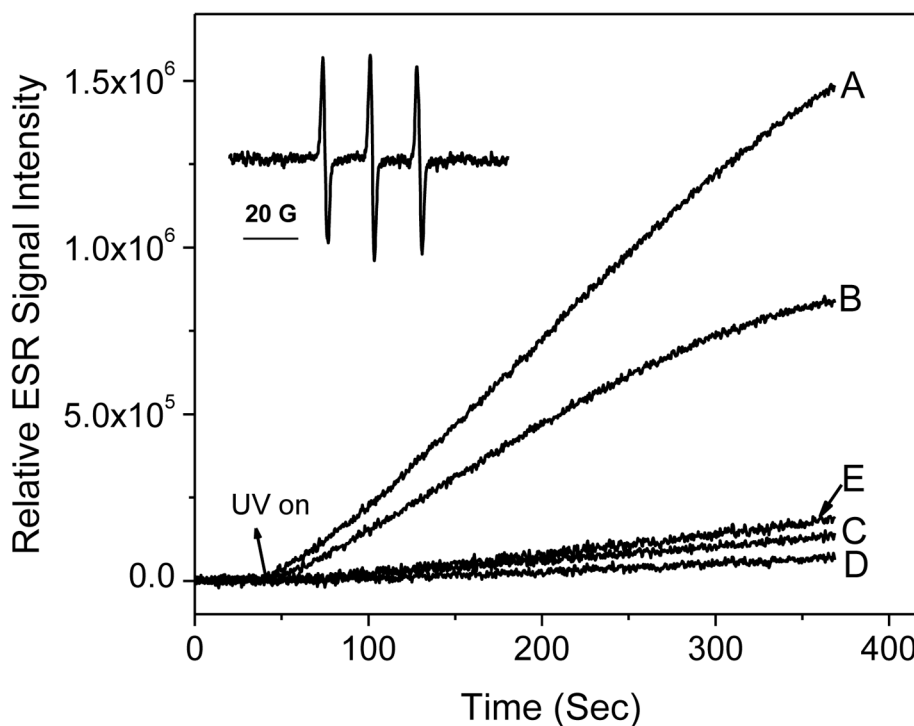


Figure 5. Generation of singlet oxygen from photoirradiation of TiO_2 samples under UVA light in a time- and crystal type-dependent manner. ESR spectra were recorded at room temperature. Samples containing 20 mM TEMP and (A) 0.1 mg/ml P25, (B) 0.1 mg/ml A25 (C) 0.1 mg/ml A325, (D) 0.1 mg/ml R100, and (E) 0.1 mg/ml P25 and 10 mM NaN_3 were irradiated with UVA light at 340 nm. Inset: ESR signal of **TEMPONE** ($a_N = 16.0$ G). The time scans of ESR signal intensity were obtained with a fixed field position (the peak position of the center line of the ESR spectrum), 15 mW microwave power and 1 G field modulation.

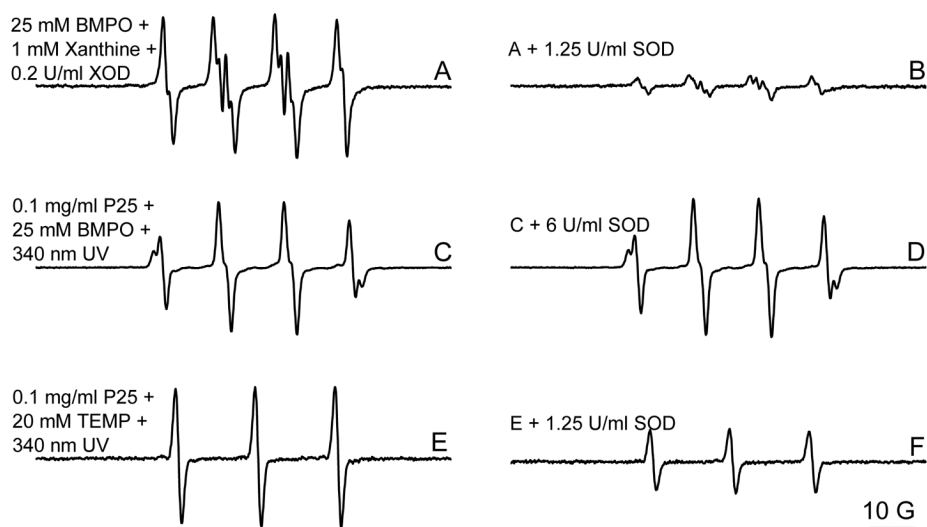


Figure 6. Effect of SOD on the generation of hydroxyl radicals and singlet oxygen by P25 during UVA irradiation. The same conditions were used as shown in Fig. 4 and Fig. 5.

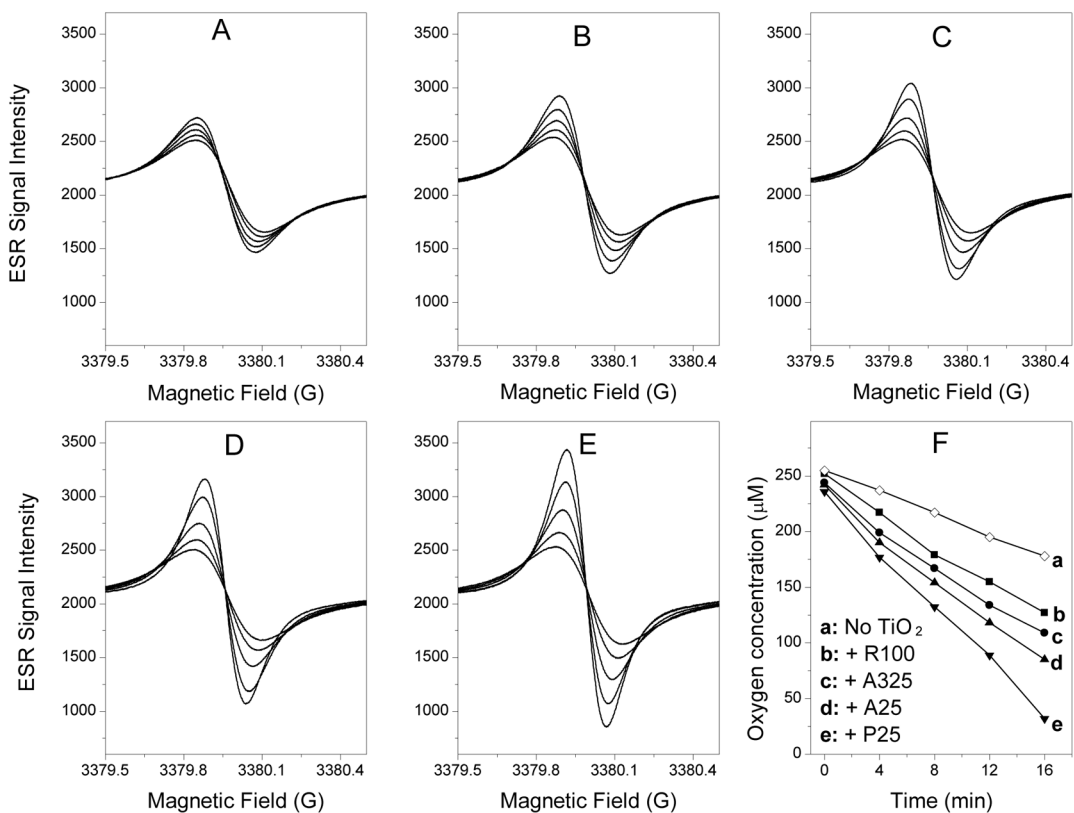


Figure 7.

Effect of TiO_2 samples on lipid peroxidation in liposomes. Oxygen consumption was measured in a closed chamber using liposome suspensions and the spin label ^{15}N -PDT. The liposome sample contained 30 mg/ml Egg PC and 0.1 μM ^{15}N -PDT spin label mixed with (A) no TiO_2 ; (B) 0.03 mg/ml of R100; (C) 0.03 mg/ml of A325; (D) 0.03 mg/ml of A25 and (E) 0.03 mg/ml of P25. Lipid peroxidation was initiated by UV (340 nm) irradiation. The ESR spectra were recorded with the low field line of the ^{15}N -PDT spin label every 4 min after the sample was sealed in a quartz capillary tube. The spectra were obtained with 0.5 mW incident microwave power and with 0.05 G field modulation at ambient temperature. The progressive increases in peak-to-peak signal intensity (and accompanying progressive narrowing of the linewidth) in each panel are due to time-dependent oxygen consumption resulting from lipid peroxidation, **as shown in panel F**. The enhancement effects of different TiO_2 nanoparticles on lipid peroxidation may be seen as bigger changes in the peak-to-peak signal intensities seen in panels B, C, D and E compared to panel A.

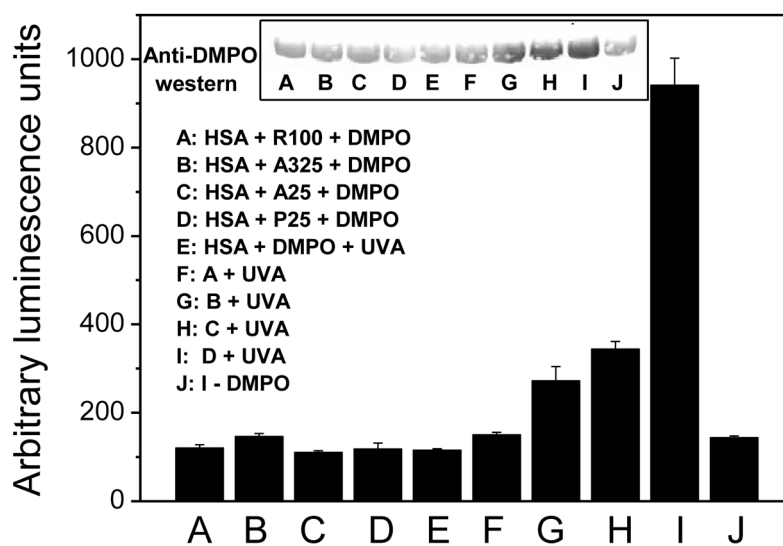


Figure 8. Effect of TiO₂ samples and UVA irradiation on the formation of DMPO-HAS-derived radical nitron adducts. Relative ELISA quantification and Western Blot analysis (inset).

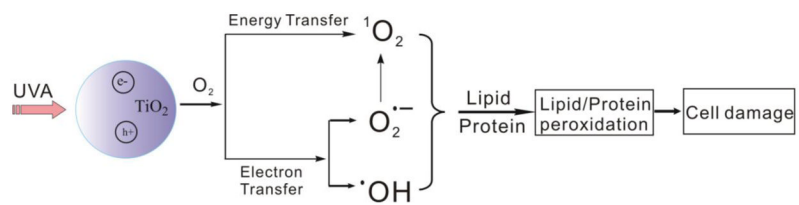


Figure 9. Proposed mechanism of TiO₂ nanoparticle-induced free radicals and lipid/protein peroxidation leading to cell damage.