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# **New experimental evidence for mechanism of arrhythmogenic membrane potential alternans based on balance of electrogenic INCX / ICa currents**

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# **Abstract**

**Background—**Computer simulations have predicted that the balance of various electrogenic sarcolemmal ion currents may control the amplitude and phase of beat-to-beat alternans of membrane potential (Vm). However, experimental evidence for the mechanism by which alternans of calcium transients produces alternation of Vm (Vm-ALT) is lacking.

**Objective—**We sought to provide experimental evidence that Ca-to-Vm coupling during alternans is determined by the balanced influence of two Ca-sensitive electrogenic sarcolemmal ionic currents,  $I_{NCX}$  and  $I_{Ca}$ .

**Methods and Results—V<sub>m</sub>-ALT** and Ca-ALT were measured simultaneously from isolated guinea pig myocytes  $(n=41)$  using perforated patch and Indo- $1_{AM}$  fluorescence, respectively. There were three study groups: 1) Control, 2)  $I_{NCX}$  predominance created by adenoviral-induced NCX overexpression, and 3)  $I_{Ca}$  predominance created by  $I_{NCX}$  inhibition (SEA-0400) or enhanced  $I_{Ca}$  (As<sub>2</sub>O<sub>3</sub>). During alternans, 14 of 14 control myocytes demonstrated positive Ca-to-Vm coupling, consistent with  $I_{\text{NCX}}$ , but not  $I_{Ca}$  as the major electrogenic current in modulating action potential duration. Positive Ca-to-Vm coupling was maintained during  $I_{NCX}$  predominance in 8 of 8 experiments with concurrent increase in Ca-to-Vm gain ( $p<0.05$ ), reaffirming the role of increased forward mode electrogenic  $I_{NCX}$ . Conversely,  $I_{Ca}$  predominance produced negative Cato-Vm coupling in 14 of 19 myocytes ( $p<0.05$ ) and decreased Ca-to-Vm gain compared to control  $(p<0.05)$ . Furthermore, computer simulation demonstrated that Ca-to-Vm coupling changes from negative to positive was due to a shift from  $I_{Ca}$  to  $I_{NCX}$  predominance with increasing pacing rate.

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**Conclusion—**These data provide the first direct experimental evidence that coupling in phase and magnitude of Ca-ALT to Vm-ALT is strongly determined by relative balance of prominence of  $I_{NCX}$  versus  $I_{Ca}$  currents.

#### **Keywords**

alternans; repolarization; action potentials; intracellular calcium

# **INTRODUCTION**

Microvolt-level T wave alternans is a sensitive marker of vulnerability to ventricular arrhythmias in patients  $1, 2$ . T-wave alternans of the surface ECG arises from beat to beat alternation of action potential duration (Vm-ALT) at the single cell level. Under this paradigm beat-to-beat alternation of the calcium transient (Ca-ALT) causes beat-to-beat alternans in action potential shape and duration  $(Vm-ALT)^{3-5}$ . This concept was supported by our previous findings showing close correspondence between myocytes exhibiting depressed expression or function of calcium cycling proteins and their susceptibility to Vm- $ALT<sup>3</sup>$ . Therefore determining the mechanism by which electrogenic ionic currents transform Ca-ALT to Vm-ALT is critical to understanding how cardiac alternans promotes electrophysiological heterogeneities and cardiac arrhythmias. Previously computer simulations have predicted that the balance of various electrogenic sarcolemmal ion currents may control the amplitude and phase of beat-to-beat alternans of membrane potential <sup>5-8</sup>. However, to our knowledge these theoretical predictions have not been tested experimentally. We hypothesized that Ca-to-Vm coupling during alternans (i.e., the relationship between alternating calcium transients and the corresponding phase and amplitude of action potential alternans) is determined by the balanced influence of two Casensitive electrogenic sarcolemmal ionic currents,  $I_{NCX}$  and  $I_{Ca}$ . This hypothesis is based on established sensitivity of these currents to cytoplasmic calcium concentration. During Ca-ALT, a large calcium release is expected to promote forward mode  $I_{NCX}$ , hence prolonging APD, whereas this will be opposed by calcium induced inactivation of  $I_{Ca}$ , which shortens APD. Therefore, the relative predominance of each current would determine how Ca-ALT is coupled with respect to gain and phase to Vm-ALT. We used complementary and selective approaches to modify  $I_{NCX}$  or  $I_{Ca}$  function and hence to examine Ca-to-Vm coupling sign and Ca-to-Vm gain under conditions of  $I_{NCX}$  vs.  $I_{Ca}$  predominance. Our data supported the hypothesis that Ca-to-Vm coupling is determined by a competing balance of  $I_{NCX}$  (positive Ca-to-Vm coupling) and  $I_{Ca}$  (negative Ca-to-Vm coupling), and demonstrated that  $I_{NCX}$  is the major electrogenic mechanisms of Vm-ALT. These findings also have implications for disease states where the balance of ion channel expression is altered.

#### **METHODS**

#### **Study Design**

Myocytes were divided into three groups to investigate the competing balanced influence of two Ca-sensitive electrogenic sarcolemmal ionic currents,  $I_{NCX}$  and  $I_{Ca}$  on Ca-to-Vm coupling during alternans: 1) Control, 2)  $I_{NCX}$  predominance, and 3)  $I_{Ca}$  predominance. I<sub>NCX</sub> predominance was achieved by In-vivo NCX gene transfer using a modified crossclamping method<sup>9</sup>. Western blot from in vitro NCX overexpression showed that NCX protein expression was indeed increased by  $3.8 \pm 2.9$  folds compared to control (n=3) and previously Ranu et al demonstrated that overexpression of NCX increases  $I_{NCX}$ , with no change in  $I_{Ca}$ .<sup>10</sup>  $I_{Ca}$  predominance was achieved by  $I_{NCX}$  inhibition or  $I_{Ca}$  enhancement. One uM of the selective I<sub>NCX</sub> inhibitor SEA0400 (Taisho Pharmaceutical Co, Ltd, Saitama, Japan) was used to achieve 80%  $I_{NCX}$  inhibition with no change in  $I_{Ca}$ <sup>11, 12</sup>.  $I_{Ca}$  was

increased with  $As_2O_3$  <sup>13</sup>. Myocytes were studied after 4 hours incubation with 3 uM of As<sub>2</sub>O<sub>3</sub>. The procedure increased  $I_{Ca}$  density by about 100% with no significant effect on I<sub>NCX</sub> under our experimental condition (see supplemental data).

#### **Vm-ALT and Ca-ALT recordings**

As described in supplementary material, Vm-ALT and Ca-ALT were measured simultaneously from isolated guinea pig myocytes (n=41) using perforated patch and Indo-1AM fluorescence, respectively. All experiments were performed at 32°C. Vm-ALT amplitude was measured by calculating the ratio of the difference in action potential duration (APD<sub>90</sub>) to the average APD<sub>90</sub> for two consecutive beats. Ca-ALT amplitude was measured by calculating the ratio of the difference in Ca transient amplitude to the average Ca transient amplitude for two consecutive beats. Ca-to-Vm coupling was determined from the coincident phase of Vm-ALT to Ca-ALT (i.e. positive vs. negative Ca-to-Vm coupling) and Ca-to-Vm gain was calculated as the ratio of Vm-ALT to Ca-ALT.

#### **ICa recordings**

ICa were elicited from a holding potential of −40 mV with depolarizing voltage pulses to 0 mV for 140 ms. Stimulation protocol, solutions, and temperature were the same as for V-ALT recordings.

#### **Computer simulations**

Computer simulations were performed using a guinea pig ventricular myocyte model that was constructed by combining mathematical formulations of selected sarcolemmal currents from  $14$  together with a mathematical model of Ca handling from  $15$  (see supplementary material for the detail) that produces CaT alternans. To study how the pacing rate and the balance of  $I_{NCX}$  and  $I_{Ca}$  influence Ca-to-Vm gain, we performed simulations for the control case and  $I_{Ca}$  predominance. The latter case was simulated by decreasing the maximum strength of  $I_{NCX}$  by 80%. Simulations were also carried out using the rabbit ventricular myocyte model of Mahajan et  $al<sup>15</sup>$  in order to demonstrate the robustness of electrogenic mechanisms underlying Ca-to-Vm coupling in different mammalian species (shown in the supplemental material).

#### **Statistical analysis**

Statistical analysis of data was performed using Sigmastat (SPSS Inc., Chicago, Illinois, USA). Statistical differences were assessed with One way ANOVA. A  $p<0.05$  was considered statistically significant. Results were expressed as mean  $\pm$  standard error of the mean (SEM).

## **RESULTS**

#### **Effect of INCX versus ICa predominance on calcium to voltage coupling during alternans**

To examine the influence of  $I_{NCX}$  and  $I_{Ca}$  on Ca-to-Vm coupling during alternans, action potentials (V) and calcium transients (Ca) alternans were simultaneously recorded as shown in Figure 1. In the control myocyte (top left) Ca-to-Vm coupling was positive; i.e., large Ca transient amplitude was coupled with long APD whereas small Ca transient amplitude was coupled with short APD on subsequent beat, consistent with  $I_{NCX}$ , but not  $I_{Ca}$  as the major electrogenic current. Consistent with this observation, with NCX overexpression (top right) positive Ca-to-Vm coupling was maintained with a concurrent increase in Ca-to-Vm gain, i.e. the ratio of Vm-ALT to Ca-ALT was larger than in control myocyte (0.62 vs 0.2 in these examples), confirming increased forward mode electrogenic  $I_{NCY}$ . In contrast,  $I_{Ca}$ predominance induced by inhibiting  $I_{NCX}$  with SEA0400 (1 uM) (bottom left) or increasing

 $I_{Ca}$  with As<sub>2</sub>O<sub>3</sub> (bottom right) produced negative Ca-to-Vm coupling at 240 bpm, i.e small Ca transient amplitude was coupled with long APD whereas large Ca transient amplitude was coupled with short APD on subsequent beat. The gain is small and negative (−0.13 and −0.09 respectively in these examples). These results are summarized in the Table. All control myocytes (14 of 14) demonstrated positive Ca-to-Vm coupling, consistent with  $I_{NCX}$ , but not  $I_{Ca}$  as the major electrogenic current. Positive Ca-to-Vm coupling was maintained with NCX overexpression in 8 of 8 myocytes with concurrent increase in Ca-to-Vm gain, confirming increased electrogenic  $I_{NCX}$ . Conversely,  $I_{Ca}$  predominance produced negative Ca-to-Vm coupling in 10 of 11 myocytes with inhibited NCX and 4 of 8 myocytes with increased  $I_{Ca}$ . The bottom panel in Figure 1 shows the negative Ca-to-Vm coupling examples. These data provide direct experimental support to our hypothesis that coupling in phase and magnitude of Ca-ALT to Vm-ALT is strongly determined by relative balance of prominence of  $I_{NCX}$  versus  $I_{Ca}$  currents.

#### **Effect of INCX versus ICa predominance on Ca-to-Vm gain during alternans**

To specifically examine the balanced influence of  $I_{NCX}$  and  $I_{Ca}$  on Ca-to-Vm gain during alternans, the ratio of Vm-ALT to Ca-ALT was calculated and plotted in Figure 2. The figure showed that increased  $I_{NCX}$  predominance by overexpressing NCX increased Ca-to-Vm gain (n=8, p< 0.05 compared to control n=14) indicating that relative availability of forward mode  $I_{NCX}$  is an important driving force for Vm-ALT. Conversely, at pacing rate of 240 bpm, enhancing  $I_{Ca}$  predominance by inhibiting  $I_{NCX}$  with SEA0400 decreased Ca-to-Vm gain significantly (n=11, p< 0.05 compared to control n=14). There was a trend towards increasing  $I_{Ca}$  with As<sub>2</sub>O<sub>3</sub> also decreased Ca-to-Vm gain, but not significantly (n=8, p=0.09 compared to control n=14). Therefore, Ca-to-Vm gain is strongly influenced by the balance of electrogenic  $I_{NCX}$  /  $I_{Ca}$  currents. However, at faster pacing rate (333 bpm) there was no difference in Ca-to-Vm gain between control and enhancing  $I_{Ca}$  predominance groups.

#### **Effect of pacing rate on Ca-to-Vm coupling during alternans**

Since current density of  $I_{Ca}$  but not  $I_{NCX}$  is influenced by recovery from time-dependent inactivation, increasing pacing rate is expected to reduce  $I_{Ca}$  current relative to  $I_{NCX}$ . Hence, we varied pacing rate to shift the relative contribution of  $I_{Ca}$  versus  $I_{NCX}$  as a means of further testing how the balance of these currents influences the transduction of Ca-ALT to Vm-ALT. Unlike control conditions, only under conditions of  $I_{Ca}$  preponderance (Figure 3, left panels) we observed negative Ca-to-Vm coupling. However, at faster pacing rates (Figure 3, right panels) Ca-to-Vm coupling became positive suggesting that the balance of  $I_{\text{NCX}}$  and  $I_{\text{Ca}}$  was shifted in such a way that  $I_{\text{Ca}}$  may no longer be the predominant electrogenic current in modulating action potential duration. This was further explored in the computer simulation shown in figure 4 where rate-dependence of Ca-to-Vm gain is plotted under control versus conditions of  $I_{Ca}$  preponderance (decreased  $I_{NCX}$ ). Consistent with our experimental results, Ca-to-Vm coupling was always positive in controls (Figure 4 filled rectangles), and Ca-to-Vm coupling increased as heart rate increased, consistent with ratedependent inactivation of  $I_{Ca}$  but not  $I_{NCX}$  (i.e. further enhancing  $I_{NCX}$  preponderance). Correspondingly, negative Ca-to-Vm coupling was observed only after shifting to conditions of  $I_{\text{Ca}}$  preponderance (Figure 4 open rectangles). However, as heart rate increased there was a reversion to positive Vm-to-Ca coupling, completely mirroring our experimental results (Figure 3).

To further explore the mechanism for dynamic shifts from negative to positive Vm-to-Ca coupling, we examined the traces of action potential, Ca transient,  $I_{Ca}$  and  $I_{NCX}$  at pacing rate of 240 bpm (left), 300 bpm (middle), and 333 bpm (right) in a condition where  $I_{NCX}$  is inhibited by 80%. The results of those computer simulations are shown in Figure 5 (a, b, c). Since action potential duration is influenced by the total amount of Ca influx through  $I_{Ca}$ 

and the peak  $I_{NCX}$  current density, we report for each current time trace numerical values for the time integrated value of  $I_{C<sub>0</sub>}$  during the action potential (in  $(pA/pF)^*$ ms), and the peak  $I_{NCX}$  value. Ca-to-Vm coupling was negative with inhibited  $I_{NCX}$  at a pacing rate of 240 bpm (left). As pacing rate increased to 333 bpm, Ca-to-Vm coupling became positive (right). However, at pacing rate of 300 bpm, there was large Ca-ALT but virtually no Vm-ALT. At a pacing rate of 240 bpm,  $I_{Ca}$  amplitude was large because of reduced Cadependent inactivation of this current when the Ca T amplitude is small, consistent with  $I_{Ca}$ predominance producing negative Ca-to-Vm coupling. As pacing rate increased to 333 bpm,  $I_{Ca}$  predominance was reduced due to shortening of APD but peak  $I_{NCX}$  magnitude increased due to increase Ca loading. Interestingly, at a pacing rate of 300 bpm, a smaller Ca T still corresponded to a larger  $I_{Ca}$ . However the difference of time-averaged  $I_{Ca}$  values between two beats were smaller than those at 240 bpm, thereby decreasing the contribution of  $I_{Ca}$  to Vm-ALT. In addition, average  $I_{NCX}$  was increased at 300 bpm compared to 240 bpm, thereby increasing the contribution of  $I_{NCX}$  to Vm-ALT. At 300 bpm, the effect of Ca-ALT on  $I_{\rm NCX}$  and  $I_{\rm Ca}$  was almost completely balanced so that Vm-ALT were absent despite the presence of Ca-ALT. In this situation, CaT-ALT are "hidden" insofar that their existence could not be inferred from electrical measurement alone. For pacing rate smaller (larger) than 300 bpm, Ca-to-Vm coupling was negative (positive). Therefore as pacing rate increased, the change of Ca-to-Vm coupling from negative to positive was due to a shift from  $I_{Ca}$  to  $I_{NCX}$  predominance. However, for control experiments shown in Figure 6, a small Ca T induced a small peak  $I_{NCX}$ . Thus APD shortened although  $I_{Ca}$  increased due to reduced Ca induced  $I_{Ca}$  inactivation at 240 bpm. As pacing rate increased to 444 bpm,  $I_{NCX}$ magnitude further increased due to its Ca dependence but APD was too short for  $I_{Ca}$  to dominate. Ca-to-Vm coupling was positive at all pacing rates, consistent with  $I_{NCX}$ , but not  $I_{Ca}$ , being the major electrogenic current producing Vm-ALT from Ca-ALT.

Checking the relationship between  $I_{Ca}$  and CaT for both control and during  $I_{NCX}$  inhibition we found that small CaT were associated with large  $I_{Ca}$  at slower pacing rates while at faster pacing rates, small CaT were associated with small I<sub>Ca</sub>. However, Ca-to-Vm coupling changes from negative to positive as pacing rate increased occurred only with  $I_{NCX}$ inhibition.

These two figures also demonstrated the rate dependence of  $I_{Ca}$  and  $I_{NCX}$ . At control condition, average  $I_{C<sub>a</sub>}$  between two consecutive beats decreased as pacing rate increased  $(417(pA/pF)*ms, 341(pA/pF)*ms, and 322(pA/pF)*ms at 240bpm, 333bpm, and 444bpm$ respectively) whereas average  $I<sub>NCX</sub>$  between two consecutive beats increased as pacing rate increased (−1.685pA/pF, −1.86pA/pF, and −2.115pA/pF at 240bpm, 333bpm, and 444bpm respectively). At inhibiting  $I_{NCX}$  (by 80%) condition, average  $I_{Ca}$  between two consecutive beats decreased as pacing rate increased (256(pA/pF)\*ms, 237(pA/pF)\*ms, and 173(pA/  $pF$ <sup>\*</sup>ms at 240bpm, 300bpm, and 330bpm respectively) whereas average  $I_{NCX}$  between two consecutive beats increased as pacing rate increased (−1.045pA/pF, −1.14pA/pF, and −1.245pA/pF at 240bpm, 300bpm, and 330bpm respectively). Figure 7 (top panel) shows representative traces of  $I_{Ca}$  at different pacing rate at patch-clamp experiments in real myocytes. As pacing rate increased  $I_{Ca}$  density decreased, confirming the results of computer simulations.

These data further support that as pacing rate increased the balance of  $I_{Ca}$  to  $I_{NCX}$  shift towards  $I_{NCX}$  predominance even under inhibiting  $I_{NCX}$  condition. Taken together, these finding reaffirmed that small shifts in the balance of  $I_{Ca}$  and  $I_{NCX}$  can influence Ca-to-Vm coupling during cardiac alternans.

## **DISCUSSION**

In the present report, we provide new experimental evidence supporting an important role for a fine balance between electrogenic  $I_{NCX}/I_{Ca}$  currents in cardiac alternans. In particular, we find that  $I_{NCX}$  predominance produces positive Ca-to-Vm coupling whereas  $I_{Ca}$ predominance produces negative Ca-to-Vm coupling. When the effect of CaT-ALT on these two currents is perfectly balanced, CaT-ALT does not produce Vm-ALT (zero gain). In addition, the sign of Ca-to-Vm coupling can change with pacing rate due to the fact that  $I_{Ca}$ and  $I<sub>NCX</sub>$  have different dependences. Combined with the theoretical framework provided by the computer simulations, our findings help to shed light on complex mechanisms controlling the relationship between cytosolic calcium and membrane voltage under highly dynamic conditions such as alternans which ultimately influence the spatial organization of repolarization in the heart.

#### **Electrogenic mechanisms for transducing Ca-ALT to Vm-ALT**

The central aim of this work was to establish experimental evidence for the mechanism by which the myocyte generates Vm-ALT from Ca-ALT. Elucidating this relationship is critical to understanding how arrhythmogenic Vm-ALT arises under normal and pathological conditions. There are several important electrogenic feedback mechanisms by which Ca-ALT can be transduced to Vm-ALT including; 1. SR calcium release enhances inactivation of sarcolemmal  $I_{Ca}$ , shown as negative feedback because it results in lowering membrane voltage (shortening APD), and 2. SR calcium release enhances calcium extrusion by  $I_{NCX}$ , shown as positive feedback because it increases membrane voltage (lengthens APD because electrogenic  $I_{NCX}$  drives 3 sodium into the cell for every one calcium extruded). It has been observed that the large Ca transient during beat-to-beat (large-small) Ca-ALT is accompanied by a short APD in some species (or certain experimental conditions)  $^{16, 17}$ , while in other species by a prolonged APD  $^{18, 19}$ . It was suggested that the  $I_{NCX}$  is responsible for prolongation of APD during large Ca transient, while Ca-dependent inactivation of  $I_{Ca}$  is the mechanism of APD shortening <sup>7, 18</sup>.

Our data suggest that  $I_{NCX}$  is the most preponderant electrogenic mechanism for Vm-ALT, based on the fact that we consistently observed positive Ca-to-Vm coupling in normal myocytes in this (Figure 1) and prior studies.  $4, \overline{20}$  In other words, under normal conditions, Ca-ALT and  $V_m$ -ALT are in phase. The opposite would be expected if  $I_{Ca}$  was the electrogenic mechanism. However, we also hypothesize that any condition (drugs, disease, heart rate, etc), which shifts the balance of sarcolemal currents away from  $I_{NCX}$ preponderance, will also change the electrogenic currents that govern alternans, and hence the magnitude and phase of cellular alternans.

#### **The balance of INCX and ICa determines the phase and gain of Ca-to-Vm coupling**

The advantage of manipulating  $I_{NCX}$  and  $I_{Ca}$  predominances in the present study stems from the ability to demonstrate a causal relationship between a single current and the development of cellular alternans and Ca-to-Vm coupling. As shown in figure 1,  $I_{NCX}$  predominance produces positive Ca-to-Vm coupling whereas  $I_{Ca}$  predominance produces negative Ca-to-Vm coupling. Selective enhancement or reduction of INCX increased or decreased Ca-to-Vm gain, respectively as demonstrated in Figure 2. This finding supports the hypothesis that  $I_{NCX}$  is the principle electrogenic current for  $V_m$ -ALT. Conversely, when  $I_{NCX}$  was inhibited,  $I_{Ca}$  becomes the predominant electrogenic carrier transducing Ca-ALT to  $V_{m}$ -ALT. In this case, negative Ca-to-Vm coupling is observed to produce electromechanical discordance, where Ca transient and APD alternate in opposite phase (figure 1).

To check the importance of Ca-dependence of  $I_{Ks}$ , we repeated the simulations of Figure 4 after removing the Ca-dependence of  $I_{Ks}$  by replacing Ca<sub>i</sub> by a constant value of 0.1  $\mu$ M in the formula for  $g_{Ks}$  given in the supplementary material. The results were unchanged, showing that the Ca-dependence of  $I_{Ks}$  has a negligible role in determining the sign of Cato-Vm coupling.

The balance of  $I_{NCX}$  and  $I_{Ca}$  determining the gain of Ca-to-Vm coupling may also explain the differences of Ca-to-Vm gain between canine and guinea pig. It has been reported that the larger Ca-to-Vm gain in the canine compared with guinea pig is due to differences in ion channel expression levels and kinetic properties  $^{21}$ . On the background of smaller  $I_{Kr}$  and  $I_{Ks}$  in the canine<sup>22</sup>, in conjunction with a much smaller  $I_{Ca}$  during the late AP plateau <sup>23</sup>, Ca transient-induced changes in  $I_{NCX}$  have a much greater modulatory effect on AP repolarization, identifying  $I_{NCX}$  as the predominant Ca-to-Vm coupler during alternans. The other Ca-dependent currents,  $I_{Ca}$  and  $I_{to}$ , play a role in shaping the AP during its initial plateau phase, causing crossover between consecutive APs during alternans, but have a minimal effect on APD. The situation can be different, with  $I_{Ca}$  playing a role in Vm-ALT, in species, where  $I_{Ca}$  persists into the late phase of the AP (e.g., guinea pig) and the Cadependent  $I_{Ks}$  repolarizing current has a large conductance<sup>24, 25</sup>. Under such conditions, a large Ca transient can lead to APD shortening during alternans, due to increased Cadependent inactivation of  $I_{Ca}$ . Therefore, the Ca-to-Vm coupling gain in the guinea pig is smaller compared with canine<sup>21</sup> and the balance of  $I_{NCX}$  and  $I_{Ca}$  determines the gain of Cato-Vm coupling.

Our data also suggest that small shifts in the balance of activity between  $I_{NCX}$  and  $I_{Ca}$  can dynamically influence Ca-to-Vm coupling. Under conditions of  $I_{C<sub>a</sub>}$  preponderance, negative coupling between Ca-ALT and Vm-ALT was transformed to positive coupling at increased heart rates (Figure 4). To explain the rate dependent shift we determined the rate dependence of  $I_{Ca}$  and  $I_{NCX}$ .  $I_{Ca}$  at different pacing rate were measured and shown in Figure 7. As pacing rate increased  $I_{Ca}$  density decreased. Since we used same square waveform to initiate  $I_{Ca}$  faster pacing rate means shorter diastolic interval for  $I_{Ca}$  to recover from inactivation and less channel available for the activation. Faster pacing also increases diastolic calcium. The rise in calcium at high rates depends primarily on the corresponding accumulation of sodium, due to the activity of  $I_{NCX}$  <sup>26</sup>. Another mechanism that promotes calcium loading at high rates is that the action potential waveform spends more time per period at plateau potentials, and so the time spent in the calcium efflux mode is reduced. Therefore, with increasing pacing rate,  $I_{NCX}$  increases and  $I_{Ca}$  decreases in normal myocytes. Pharmacological inhibition of  $I_{NCX}$  affects the rate dependences of both  $I_{Ca}$  decrease and  $I_{\text{NCX}}$  increase as shown in Figure 5&6, thereby shifting the balance of  $I_{\text{NCX}}$  and  $I_{\text{Ca}}$  in a rate-dependent fashion. For intermediate pacing rate (240 bpm),  $I_{Ca}$  dominates due to  $I_{NCX}$ inhibition, thereby giving rise to negative coupling. In contrast, for even faster pacing rate (333 bpm), the  $I_{Ca}$  decrease and  $I_{NCX}$  increase are sufficient to produce a positive coupling despite pharmacological  $I_{NCX}$  inhibition.

#### **Supplementary Material**

Refer to Web version on PubMed Central for supplementary material.

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Wan et al. Page 10





Wan et al. Page 11



**Figure 2. Increasing INCX predominance increases Ca-to-Vm gain whereas increasing ICa predominance decreases Ca-to-Vm gain**

Ca-to-Vm gain was calculated as the ratio of Vm-ALT to Ca-ALT. The bar graph showed that increasing  $I_{NCX}$  predominance by overexpressing NCX increased Ca-to-Vm gain significantly (n=8, p< 0.05 compared to control n=14). At pacing rate of 240 bpm increasing  $I_{Ca}$  predominance by inhibiting  $I_{NCX}$  with SEA0400 decreased Ca-to-Vm gain significantly  $(n=11, p< 0.05$  compared to control n=14). There was a trend that increasing  $I_{Ca}$  with As<sub>2</sub>O<sub>3</sub> also decreased Ca-to-Vm gain, but not significantly (n=8, p=0.09 compared to control). However, at faster pacing rate (333 bpm) there was no difference in Ca-to-Vm gain between control and enhancing  $I_{Ca}$  predominance groups.



**Figure 3. As pacing rate further increased Ca-to-Vm coupling changed from negative coupling to positive coupling in ICa predominant myocytes**

With SEA0400 inhibiting  $I_{NCX}$  (top panel) or with  $As_2O_3$  increasing  $I_{Ca}$  (bottom panel) Cato-Vm coupling was negative at pacing rate of 240 bpm (left). However, as pacing rate increased to 333 bpm Ca-to-Vm coupling changed to positive (right).

Wan et al. Page 13



#### **Figure 4. Computer simulations showing that the gain of Ca-to-Vm coupling changed from negative to positive as pacing rate increased**

In control alternans occurred when pacing rate reached 180 bpm or faster. Ca-to-Vm coupling was positive. Inhibiting  $I_{NCX}$  (by 80%) Ca-to-Vm coupling was negative at pacing rate between 220 and 290 bpm. As pacing rate increased to >300 bpm, Ca-to-Vm coupling changed to positive.



#### **Figure 5. Balanced influence of INCX and ICa on Ca-to-Vm coupling in inhibiting INCX condition**

The figure illustrated the traces of action potential, Ca transient,  $I_{Ca}$  and  $I_{NCX}$  at pacing rate of 240 bpm (left), 300 bpm (middle), and 333 bpm (right) in inhibiting  $I_{NCX}$  (by 80%) as shown in Figure 4 (a, b, c) in computer simulation. The numbers under  $I_{Ca}$  curves came from the time integration of currents ((pA/pF)\*ms), and the numbers under  $I_{NCX}$  was the peak current density. Ca-to-Vm coupling was negative with inhibited  $I_{NCX}$  at pacing rate of 240 bpm (left). As pacing rate increased to 333 bpm, Ca-to-Vm coupling was positive (right). However, at pacing rate of 300 bpm, there was large Ca-ALT but virtually no Vm-ALT.

Wan et al. Page 15



**Figure 6. Relationship between Ca-to-Vm coupling and electrogenic currents in control** The figure illustrated the traces of action potential, Ca transient,  $I_{Ca}$  and  $I_{NCX}$  at pacing rate of 240 bpm (left), 333 bpm (middle), and 444 bpm (right) in a control as shown in Figure 4 (d, e, f) in computer simulation. Ca-to-Vm coupling were positive at all pacing rate.

Wan et al. Page 16



#### **Figure 7. ICa density decreased as pacing rate increased at fast pacing rate** Top panel illustrated representative traces of  $I_{Ca}$  at different pacing rate. As pacing rate increased ICa density decreased. Summary data from 10 myocytes was shown in bottom panel.

#### **Table**

Effect of  $I_{NCX}$  vs  $I_{Ca}$  predominance on Ca-to-Vm coupling.

