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Does Impact Sport Activity Influence Total Hip Arthroplasty Durability?

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Abstract

Background Return to sport is a key patient demand after hip arthroplasty and some patients are even involved in high-impact sports. Although polyethylene wear is related to the number of cycles and the importance of the load, it is unclear whether high-impact sport per se influences THA durability.

Questions/purposes Therefore, we compared (1) function between the patients involved in high-impact sports and the patients with lower activities as measured by the Harris hip score (HHS) and the Hip Osteoarthritis Outcome Score (HOOS); (2) linear wear rates; and (3) survivorships

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considering revision for mechanical failure with radiographic signs of aseptic loosening as the end point.

Methods We retrospectively identified 70 patients who engaged in high-impact sports and 140 with low activity levels from among 843 THAs from a prospectively collected database performed between September 1, 1995, and December 31, 2000. Patients were evaluated at a minimum followup of 10 years (mean, 11 years; range, 10–15 years) by two independent observers. We obtained a HHS and HOOS at each followup.

Results The mean HOOS was higher in the high-impact group for three of the five subscales of the HOOS. Mean linear wear was higher in the high-impact group than in the low-activities group. We also found a higher number of revisions in the high-activity group.

Conclusions Our observations confirm concern about the risk of THA mechanical failures related to high-impact sport, and patient and surgeons alike should be aware of these risks of mechanical failures.

Level of Evidence Level III, therapeutic study. See the Guidelines for Authors for a complete description of levels of evidence.

Introduction

THA has been described as the procedure of the century and is probably the most effective modern orthopaedic procedure [\[21](#page-6-0)]. The population undergoing THA has changed during the last 30 years and many patients are now younger, more active, and with longer life expectancies at the time of surgery [[37\]](#page-6-0). As the clinical success of total joint arthroplasty has been documented and publicized, patients' expectations regarding the procedure have increased; returning to sport is now a major patient expectation after hip arthroplasty [\[34](#page-6-0)] and some patients are even involved in high-impact sports such as jogging, soccer, or martial arts practice [\[15](#page-6-0), [25,](#page-6-0) [33\]](#page-6-0). Several studies have shown a high percentage of participation in athletic activities after THA [[15\]](#page-6-0). Huch et al. [\[16](#page-6-0)] reported that 36% of patients were involved in athletic activities at the time of surgery and 52% 5 years after the surgery [\[6](#page-6-0)]. According to Wright and Bartel [[38\]](#page-6-0), return to athletic activity is the third concern after pain relief and ROM improvement among candidates for THA. One of the frequent questions of the patient before surgery is the potential ability to practice sport after surgery [\[34](#page-6-0)]. The surgeon naturally would wonder whether participation in sports has an adverse effect on THA durability [[19,](#page-6-0) [30](#page-6-0)]. A consensus survey based on individual surgeon opinion suggested some sports were generally recommended and others not [[24\]](#page-6-0). Many surgeons do not recommend highimpact sports because they may cause fracture [\[2](#page-5-0)] and because of excessive wear. Patients involved in such sports have high activity levels [[32\]](#page-6-0) with higher load magnitudes and generally higher numbers of activity cycles. Following the increasing number of patients involved in high-impact sport after THA, it is important to confirm these recommendations with studies similar to those after TKAs [\[27](#page-6-0)]. Based on the studies showing higher failure rates with higher activity levels and on expert opinion, we presumed involvement in high-impact sport would reduce the durability of the implant after THA.

Therefore, we compared patients involved in highimpact sports and those with lower activities to determine differences in: (1) function; (2) dislocation rate; (3) linear wear; and (4) survivorship considering revision for mechanical failure or radiographic signs of aseptic loosening as the end point. Finally we determined independent risk factors for failure.

Patients and Methods

From a prospectively collected database we retrospectively identified 70 patients who engaged in high-impact sports and 140 with low activity levels from among 843 patients who have had 843 THAs performed between September 1, 1995, and December 31, 2000. Patients were evaluated at a minimum followup of 10 years (mean, 11 years; range, 10–15 years) for Harris hip score (HHS) [[14\]](#page-6-0) and Hip Osteoarthritis Outcome Score (HOOS) [[28,](#page-6-0) [29\]](#page-6-0) radiographic analysis (wear rate) and aseptic loosening or need for revision. The indication for the procedure was primary or secondary arthritis of the hip. All patients received a cementless stem and a cementless cup and the bearing surface at that time was a ceramic head and a conventional polyethylene. The inclusion criteria were primary THA, age from 18 to 75 years at the time of surgery, patients with Charnley Grade A or B level [\[4](#page-6-0)], unilateral THA, primary arthritis, osteonecrosis or developmental dysplasia Stage 1, and a minimum followup greater than 10 years. We excluded patients with tumor, trauma and posttraumatic arthritis, congenital dislocation or developmental dysplasia Stage > 1 , history of surgery or infection on the index hip, and patients with early revision resulting from an early mechanical failure or an infection. Institutional review board approval was obtained.

Patients meeting the inclusion criteria were then allocated in each group using a specific sport and quality-oflife questionnaire. At a minimum followup of 10 years, patients were asked to fill out a questionnaire including three sections: the first section was related to the patient's characteristics (weight, height, age, professional occupation), the second included the University of California Los Angeles score (UCLA) [[40\]](#page-6-0) activity score and the Weiss et al. [\[36](#page-6-0)] scores, and the last section included the HOOS $[28, 29]$ $[28, 29]$ $[28, 29]$. We used the UCLA score $[40]$ $[40]$ to appreciate the level of activity. This score reflects only the frequency of the participation and the type of activity performed. To our knowledge, there is no technique to accurately and precisely determine the frequency and intensity of a sport activity. This questionnaire was sent to the patients with a letter from the two senior surgeons (JNA, JMA) requesting their participation. The same questionnaire was filled out by a telephone survey for the nonresponding patient (SF). Of the 843 patients screened, 70 patients reported a UCLA [\[40](#page-6-0)] activity score of 9 or 10 and were defined as the highimpact group. A group of patients considered as lowactivity patients (UCLA $[40]$ $[40]$ score from 1 to 4) was then identified from the survey. Patients of the high-impact group were then matched according to age at surgery $(\pm 5 \text{ years})$, sex, BMI $(\pm 3 \text{ kg/m}^2)$, American Society of Anesthesiology score, and followup $(\pm 2 \text{ years})$ with two patients in the low-activity group by a computerized matching process. After this matching process, 210 patients were included in our study, 70 in the high-impact group and 140 in the low-activity group (Table [1](#page-2-0)). Patient demographics were described using means and SDs or medians and ranges for continuous variables and counts (percent) for categorical variables. In the high-impact group, the mean UCLA score [[39\]](#page-6-0) was 9.3 ± 0.4 ; this score was 3.4 ± 0.6 in the low-activity group.

All patients were operated on by the two senior authors (JMA, JNA). An anatomical cementless hydroxyapatite (HA) -coated stem was used all cases (Symbios[®], Yverdon, Switzerland; FDA-approved). All the patients received a 28-mm ceramic femoral head implant. A cementless HA-coated titanium alloy acetabular cup was used in every case with a conventional UHMWPE (sterilization with gamma radiation under nitrogen).

Characteristic	High impact	Low activities	p value	
Age (years)	58.79 ± 9.4	58.57 ± 9.2	0.9	
American Society of Anesthesiologists score	1.43 ± 0.6	1.51 ± 0.8	0.7	
Body mass index $(kg/m2)$	25.03 ± 3.14	25.18 ± 3.16	0.8	
Harris hip score preoperatively	54 ± 12	57 ± 14	0.3	
Sex (male)	51.4\% (36)	51.4\% (72)	0.9	
Femoral head size 32	10% (7)	13 $\%$ (18)	0.3	
UCLA score	9.3 ± 0.4	3.37 ± 0.6	< 0.0001	

Table 1. Patient characteristics in the high-activity group and in the low-activity group

Mean values with standard deviation or percent with number of individuals.

Pre- and postoperatively we obtained a HHS to objectively determine the patient's functional level. To evaluate the patient's hip-related quality of life, patients were asked to fill out the HOOS [\[28](#page-6-0), [29](#page-6-0)] in the questionnaire. The HOOS [\[28](#page-6-0), [29](#page-6-0)] is a self-administered hip-related qualityof-life questionnaire corresponding to a validated and improved WOMAC $[2]$ $[2]$. The HOOS $[28, 29]$ $[28, 29]$ $[28, 29]$ includes five dimensions scored separately: pain (nine items); symptoms (seven items); activities of daily life function (17 items); sport and recreation function (five items); and quality of life (four items). Because it is desirable to analyze and interpret the five dimensions separately, an aggregate score was not calculated. All items are scored from 0 to 4, and each of the five scores is calculated as the sum of the items included. Scores are then transformed using free calculation software available online on the web site www.koos.nu to a 0 to 100 scale with zero representing extreme knee problems and 100 representing no knee problems. HOOS [\[28](#page-6-0), [29](#page-6-0)] score has not been calculated preoperatively because it was not yet available.

Radiographic postoperative evaluation consisted of AP and lateral views of the hip and pelvis and a true lateral view of the hip. The first postoperative radiograph was then used as a baseline from which subsequent radiographs were interpreted. At last followup, the radiographs were digitalized with a high-density scanner (SIERRA Advantage VIDAR Systems Corporation[®], Herndon, VA) and examined by two independent observers (SP, MO). Magnification correction factors were calculated for each film based on the known diameter of the prosthetic head. Polyethylene wear was measured using IMAGIKA $^{(8)}$ software (GSI Medical, Neuilly sur Seine, France); data processing procedures were based on the dual circle method to analyze digitalized radiographs. This software has already proved its reproducibility and accuracy [\[12](#page-6-0)]. The examiners analyzed each radiograph twice, once on each of 2 separate days. All data processing was performed independently from one another. Intra- and interobserver variability was calculated using the root mean square (RMS) error and coefficient of variation (COV) of all data. The differences of intraobserver values were 0.128 ± 0.031 mm with a coefficient of repeatability of 0.109 mm, an RMS error of 0.098 mm, and a COV of 2.3%. The difference in interobserver values was $0.107 \pm$ 0.027 mm with a coefficient of repeatability of 0.94 mm and an RMS error of 0.087 mm. Because not all patients had the same period of followup, the total wear was converted to a wear rate per year, and this linear wear was expressed as a mean \pm SD (millimeters per year). Osteolysis or loosening was analyzed using the following criteria for the femur and the acetabular cup. The femur was analyzed according to the seven zones described by Gruen et al. [[13\]](#page-6-0) and the corresponding seven zones on the lateral radiograph. Progressive radiolucencies, or radiolucencies greater than 2 mm in width, were recorded as well as signs of osteolysis. The femoral component stability was evaluated by the criteria of Engh et al. [\[9](#page-6-0)]. The stem was considered loose if a subsidence greater than 2 mm or a modification in the axis of more than 2° was recorded. Acetabular cup stability was evaluated with the Massin et al. [[24\]](#page-6-0) method analyzing the distance between femoral head center and landmark along a vertical axis (the distance between the center of the cup and the teardrop line) and horizontal axis (distance between the center of the cup and the vertical line through the teardrop). A difference between the postoperative value and at last followup greater than 3° was considered as a migration. The tilt of the acetabular component (alpha angle) was defined as the angle between the cup and the teardrop line. A variation greater than 3 between initial and followup alpha angle was interpreted as a migration. Radiolucent lines in the DeLee and Charnley zone [\[6](#page-6-0)] were analyzed and interpreted as important depending of their size, localization, and evolution. Patient demographic data, dislocation rate, and the radiographic data were expressed as the mean and the SD (Tables 1, [2](#page-3-0)).

Clinical improvement between the pre- and the last followup evaluation as described by the HHS [[14](#page-6-0)] was analyzed using a t-test for paired comparisons in each group. A comparison of the HOOS [\[28](#page-6-0), [29](#page-6-0)] at last followup in each group was performed.

Study	Number of hips	Number of design	Age	Male gender	Weight	Height	Activity
Charnley and Cupic $[5]$	106				N ₀		No
Livermore et al. [22]	385	3			Yes		
Xenos et al. $[39]$	100		Yes	N ₀	N ₀	N ₀	
Devane et al. [7]	80		Yes	N ₀	N ₀	$\overline{}$	Yes
Schmalzried et al. [31]	37	2	Yes	N ₀	Yes	Yes	Yes
Lübbeke et al. [23]	433		N ₀	No.		-	No
Current study	210		N ₀	Yes	No	N ₀	Yes

Table 2. Factors influencing wear in THA

To analyze the influence of activity on survival and polyethylene wear, we defined two groups of patients: (1) patients involved in high-impact sports (UCLA 9-10); and (2) patients only involved in low activities (UCLA 1-4). Sample size was calculated based on the estimated linear wear $[22]$ $[22]$ rate of 0.10 mm/year \pm 0.06 for the 32-mm femoral head size and 0.08 mm/year \pm 0.07 for the 28-mm femoral head size and, with an expected difference of wear rate between groups of 20%, a required level of statistical significance of $\alpha = 0.05$ and a power of $1-\beta = 0.95$; 50 subjects per group would be required to detect a difference of 0.025 mm/year. We tried to include all the patients with UCLA score > 8 from our database and including more patients with UCLA \lt 5 did not improve our power of calculation. The mean amount of wear was calculated for each of the two groups.

The analysis of polyethylene wear in the two groups was performed in two parts: (1) analysis of the risk factors that were selected for evaluation before the study was started (BMI, age, sex, femoral head size, activity, followup time) using linear regression analysis or Student's t-test; and (2) analysis of subsets of patients and risk factors that were statistically significant or clinically important in the primary hypothesis-driven risk-factor analysis (BMI, sex, femoral head size, activity) using a Pearson's Chi square test.

The prevalence of failure was calculated for each of the two groups excluding revisions related to septic loosening. Implant survival was estimated with use of the Kaplan-Meier method. Confidence intervals (CIs) at the 95% level were determined. The end point was defined by: revision for a mechanical failure of the components (one or both), or a fracture occurring during the athletic activities, or a mechanical failure defined as a migration of the components (one or both). Survivorships in the two groups were compared first in a univariate model according to a logrank method. Then an extended Cox model with use of a generalized estimating equation theory was used to compare survival by risk factor in the high- and low-activity groups and to perform a multivariate analysis of survival of implants. Odd ratios were reported with their 95% CIs and considered as significant if excluding the value 1. Analysis

Fig. 1 The mean postoperative HOOS scores were higher in the high-impact group for the symptoms, activities of daily living, and sport subscales and comparable between the two groups for the pain and quality-of-life subscales. $AdL =$ activities of daily living; Sports = sports and recreational function; $QoL =$ quality of life.

was performed using SPSS software (Version 12; SPSS Inc, Chicago, IL, USA). All calculations assumed twotailed tests.

Results

The mean HHS [[14](#page-6-0)] improved from 54 ± 12.8 preoperatively to 88.29 ± 12.5 points (range, 53–98) postoperatively in the high-impact group and from 55 ± 14.5 to 69.38 ± 19.4 points (range, 23–98) in the low-activity group. The mean HHS [[14\]](#page-6-0) improvement was greater $(p < 0.001)$ in the high-impact group with a mean improvement of 34 points in the high-impact group and 14 points in the low-activity group. The mean HOOS [\[28](#page-6-0), [29\]](#page-6-0) was higher in the high-impact group for the symptoms, activities of daily living, and sport subscales and comparable between the two groups for the pain and qualityof-life subscales (Fig. 1).

We observed no difference $(p = 0.5)$ in dislocation rate between the two groups. Four patients experienced hip

Fig. 2 Results of the Kaplan-Meier analysis showing a worse survivorship in the high-activity group at 15 years followup.

dislocation (1.9%) , one in the high-impact group (1.4%) and three in the low-activity group (2.14%).

Practicing a high-impact sport and being a male increased wear rate (both $p < 0.001$). At 10 to 15 years followup, the mean polyethylene wear rate was 1.62 ± 0.69 mm (range, 3.29–0.54 mm) and the linear wear was 0.14 ± 0.06 mm/year (range, 0.29–0.05 mm/ year) in the high-impact group. In the low-activity group, the mean wear was 0.74 ± 0.52 (range, 2.76–0.06) and the linear wear was 0.06 ± 0.04 (range, 0.2–0.06).

Survivorship was worse $(p < 0.001)$ in the high-impact group than in the low-activities group (Fig. 2). At last followup, 23 patients had been revised for mechanical failure or had implants that had radiographically migrated. Fourteen patients in the high-impact group reached the end point for the following reasons: two revisions for acetabular loosening, four revisions for femoral aseptic loosening, six with radiographic acetabular loosening, and two with radiographic loosening of both components. In the lowactivity group, nine patients reached the end point for the following reasons: one revision for acetabular loosening, four with radiographic femoral loosening, and four with radiographic acetabular loosening. One patient in the highactivity group (a skiing instructor) revised for aseptic loosening also had a femoral fracture during downhill skiing 2 years after acetabular revision. At 15 years followup, the survivorship in the high-impact sport group was 80% (range, 74%–86%) and 93.5% (range, 88.2%–97.6%) in the low-activity group.

Practicing a high-impact sport was a risk factor for failure with an odds ratio of 3.64 (95% CI, 1.49–8.9). Patients in the high-impact sport group had more mechanical failures ($p = 0.001$) than patients involved in low activity.

Discussion

One of the frequent questions of the patient before THA is the potential ability to practice sport after surgery and the potential risk related to sport practice [\[35](#page-6-0)]. We presumed long-term participation in high-impact sports would reduce function and durability of the implant after THA. Therefore, we compared patients involved in high-impact sports and those with lower activities to determine differences in: (1) function; (2) dislocation rate; (3) linear wear; and (4) survivorship considering revision for mechanical failure or radiographic signs of aseptic loosening as the end point; we then determined independent risk factors for failure.

Readers should understand the major limitations of our study. First, the duration of the followup is too limited to clearly show the potential long-term adverse effect of the sport practice. The followup of the two groups of patients should then be continued; one study [\[8](#page-6-0)] reported a correlation between the number of revisions at 20 years and polyethylene wear with a linear wear rate of 0.2 mm/year or greater. However, our study is relatively large and does have a relatively long minimum followup of 10 years. Second, we lacked data indicating the duration and the intensity of the patient's sportive activity. The only way to appreciate patient duration and intensity of athletic activity is pedometric analysis, but it reflects only a short period of patient activity (on pedometer) and is only available for prospective study. To minimize the effect of this limitation, we used the UCLA activity score [[40\]](#page-6-0), which includes the type of sport and also the frequency of practice particularly for the values 9 and 10. These values correspond to patients involved; frequently, in high-impact sport, much of these are nonrecommended activities after THA, but some of them are recommended sports like hiking.

The clinical outcomes and functional improvement were greater in the high-impact sport group compared with the low-activity group at 10 years. Sechriest et al. [[32\]](#page-6-0) found a UCLA score [[40\]](#page-6-0) positively correlated with postoperative HHS $[14]$ $[14]$. Lübbeke et al. $[23]$ $[23]$ recently noticed that patients with the highest activity (evaluated by UCLA score) had the best outcome and highest satisfaction after surgery. These findings are also consistent with those reporting THA in the younger and active patient [\[10](#page-6-0)] or in the younger patient with a resurfacing hip [\[1](#page-5-0)]. Our observations demonstrated high functional score and high hiprelated quality-of-life scores can also be obtained for older patients involved in high-impact sport.

Our series is consistent with literature showing increased polyethylene wear in patients with higher activities. Many factors seem to influence polyethylene wear; some of them may be confusing factors correlated to the degree of activity of the patient such as age, weight, and height of the patient (Table [2](#page-3-0)). The observations show participation in high-impact sports and being a male increased the wear rate. Why males have a higher rate of wear remains unclear [\[32](#page-6-0)]. Sex-specific differences have been mentioned to explain these differences including body

Study	Number of hips	Mean age	Mean followup	Couple	Mechanical failure	Femoral osteolysis	Linear PE wear
Migaud et al. $[26]$	39	41 years	13 years	Metal/metal	0/39		
	39			Ceramic/PE	11/39		
Lübbeke et al. [23]	58	67.7 years	10 years	Ceramic/PE	-	14/58	
Bedigrew et al. $[1]$	52	50 years	2 years	Metal/metal	0/52	0/52	
Flugsrud et al. $[11]$	188	63 years	16 years	All types	32/188		
Calvert et al. [3]	60	59 years	4 years	Ceramic/chromium linked	$\overline{0}$		0.02 mm/year
	59	-	-	Ceramic/PE	$\overline{0}$	$\qquad \qquad \longleftarrow$	0.11 mm/year
Current study	70	58.3 years	11 years	Ceramic/PE	14/70	11/70	0.145 mm/year

Table 3. Number of revision and THA radiological outcomes of high-activity patients

 $PE = polyethylene$.

anatomy such as weight distribution, gait pattern, or body composition as well as physiological considerations such as the lubricating properties of synovial fluid. Patient activity remains, however, the most important patient-related factor influencing prosthetic wear [[31\]](#page-6-0) depending on the applied load and the number of cycles the load is applied across the articulating surfaces [\[38\]](#page-6-0). Recent literature reported improved function and higher midterm survivorship for highly active patients using metal-on-metal bearing surfaces [\[26](#page-6-0)]. Better function and higher survivorship have also been reported after hip resurfacing in highly active men but with limited followup [1] and unanswered questions related to the potential adverse effect of resurfacing and metal-on-metal bearing surfaces such as corrosion, pseudotumor, or cytotoxicity [\[18](#page-6-0)]. Ceramic-on-ceramic bearing surfaces showed limited wear [[17\]](#page-6-0), but fractures and squeaking may adversely balance the potential benefit in terms of wear in highly active patients. One interesting solution to limit the osteolysis without having each potential drawback of the hard-on-hard bearing surfaces may be the use of highly crosslinked polyethylene showing lower wear rates at 5 and now 10 years [3].

We found a lower survivorship in the high-impact group with more mechanical failures. Our findings were consistent with those in the literature (Table 3). Flugsrud et al. [\[11](#page-6-0)] reported a comparable revision rate from the Norwegian database with a 17% revision rate after 13 years for patients involved in intermediate to intense sport activity during leisure and 13% for patients involved in lower activities. Lübbeke et al. $[23]$ $[23]$ first used the UCLA scale to differentiate patient activity groups for clinical and radiographic femoral osteolysis showing a greater amount of osteolysis around the femoral component in the highactivity group without any difference in terms of wear rate between the moderate- and the high-activity groups. This is in accordance with the experts' recommendations concerning the practice of high-impact activities at least when using conventional polyethylene $[20]$ $[20]$ $[20]$. Most of the very

active patients may however not follow their surgeon's recommendations, as suggested by Seyler et al. [\[33](#page-6-0)]. On the other hand, nonimpact sports reportedly promote bone growth [\[8](#page-6-0)], reduce obesity, and improve psychological health [\[15](#page-6-0)] and are therefore important after total joint arthroplasties.

Our findings suggest patients with cementless THA, practicing a high-impact sport such as football, skiing, tennis, or martial arts, have better function than patients involved in low activities. However, involvement in athletic activities increased the wear rate and adversely affected implant survivorship. Our observations therefore confirm experts' concerns about the potential risk related to the high-impact sport and both patients and surgeons should be aware of these risks. The potential adverse effect related to the hard-on-hard bearing surfaces and the potential benefit related to the highly crosslinked polyethylene should be evaluated in prospective comparative studies including active patients to enhance the surgeon's bearing surface choices because sport is now a reality after THA.

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